

The proportional recovery rule redux

Arguments for its biological and predictive relevance

Jeff Goldsmith^{1,*}, Tomoko Kitago^{2,3}, Angel Garcia de la Garza¹, Robinson Kundert⁴,
Andreas Luft^{4,5}, Cathy Stinear⁶, Winston D. Byblow⁷, Geert Kwakkel^{8,9}, John W.
Krakauer^{10,11}

¹. Department of Biostatistics, Columbia Mailman School of Public Health, New York, New York, USA

². Burke Neurological Institute, White Plains, New York, USA

³. Weill Cornell Medicine, New York, New York, USA

⁴. Cereneo, Center for Neurology and Rehabilitation, Vitznau, Switzerland

⁵. Vascular Neurology and Neurorehabilitation, Department of Neurology, University Hospital Zurich, University of Zurich, Zurich, Switzerland

⁶. Department of Medicine, University of Auckland, Auckland, New Zealand

⁷. Department of Exercise Sciences, University of Auckland, New Zealand

⁸. Rehabilitation Research Centre, Reade, Amsterdam, Netherlands

⁹. Rehabilitation Medicine, Amsterdam UMC - Location VUMC, Amsterdam Movement Sciences, Amsterdam, Netherlands

¹⁰. Department of Neurology, Johns Hopkins University, Baltimore, MD, USA

¹¹. Department of Neuroscience, Johns Hopkins University, Baltimore, MD, USA

* ajg2202@cumc.columbia.edu

Abstract

The proportional recovery rule (PRR) posits that most stroke survivors can expect to reverse a fixed proportion of motor impairment. As a statistical model, the PRR explicitly relates change scores to baseline values – an approach that has the potential to introduce artifacts and flawed conclusions. We describe approaches that can assess associations between baseline and changes from baseline while avoiding artifacts either due to mathematical coupling or regression to the mean due to measurement error. We also describe methods that can compare different biological models of recovery. Across several real datasets, we find evidence for non-artifactual associations between baseline and change, and support for the PRR compared to alternative models. We conclude that the PRR remains a biologically-relevant model of recovery, and also introduce a statistical perspective that can be used to assess future models.

Intuition, experience, and data suggest that patients with worse motor impairment in the immediate post-stroke period will also typically see the largest absolute reductions in impairment during the first three to six months of recovery. However, rigorously quantifying this observation has proved challenging. The proportional recovery rule (PRR) was an early attempt to describe the relationship between initial impairment and recovery through the investigation of upper-extremity Fugl-Meyer assessments (FMA-UE) at baseline and at subsequent follow-up visits, with recovery defined as the change over time (Prabhakaran et al. 2008; Krakauer and Marshall 2015). This work indicated that, on average, a large subset of patients recovered roughly 70% of the maximal potential recovery from impairment, but a biologically distinct and smaller subgroup recovered much less (“non-recoverers”). Since its introduction, the PRR has been applied across several neurological domains, implemented in various ways across studies, and evaluated using several different statistical metrics (Lazar et al. 2010; Winters et al. 2015; Winters et al. 2017; Veerbeek et al. 2018; Byblow et al. 2015). In a recent article, we sought to reestablish the original conceptualization of the PRR as a regression model for describing of recovery from upper limb impairment (Kundert et al. 2019).

The PRR has, in recent years, come under fire. Many of the criticisms hinge on statistical questions about the relationship between baseline values and change scores; a relationship that is often fraught, counterintuitive, and has confounded researchers and statisticians for decades. Bringing these issues to the fore and illustrating the ways they affect analyses of stroke recovery has spurred an important and informative debate. Specifically, there are questions about the usefulness of correlations in the case when there is mathematical coupling from inclusion of the baseline value in the change score, the distinction between population-level descriptions and patient-level predictions; the usefulness of the PRR in functional domains other than upper-extremity motor control; the identification of “non-recoverers”, both prospectively and retrospectively; and the possibility that ceiling effects exaggerate associations or introduce non-linearity not accounted for by the PRR (Hope et al. 2018; Hawe, Scott, and Dukelow 2019; Bonkhoff et al. 2020; Bowman et al. 2021).

The growing meta-literature discusses the PRR in an abstract way, focusing on a baseline x , a single follow-up y , the change $\delta = y - x$, and all the various correlations among them. Readers could be forgiven for asking how an intuitive formula for expected recovery spawned its own cottage industry, and why arguments about the PRR have become so esoteric. We suspect that many, by now, would prefer a simple judgment on the truth of the PRR without a winding statistical detour. We’re sympathetic to this perspective, but find the detour necessary as the nuanced and sometimes counterintuitive statistical arguments are critical to get right for the sake of furthering our understanding of the biological mechanisms of recovery.

Our goals are to discuss the statistical issues relevant to the PRR clearly, to describe appropriate analysis techniques, and to resolve arguments where possible. We discuss valid but non-standard hypothesis tests for correlations, framed to distinguish true signal from artifact. This is not necessarily the same as distinguishing between the PRR and other models of recovery; we therefore evaluate competing models based on their ability to predict outcomes. Much of this discussion assumes that “recoverers” and “non-recoverers” can be differentiated,

and mainly focuses on models for recoverers. That said, the existence of distinct recovery groups complicates the quantification of recovery. We discuss the hazards of applying advanced statistical methods in settings where they aren't justified by the data, and discuss ways of testing whether observed data are consistent with a hypothesized generating mechanism. Throughout, we use simulated datasets and data taken from several published studies of recovery to illustrate our statistical points. In some places, the discussion is unavoidably technical, but the aim is to focus on the details that are pertinent to the core question: Is there is a true systematic relationship between impairment and change in impairment after stroke? If the answer is yes, then this would imply that there is important biological work to be done to explain the mechanism for this phenomenological regularity.

Results

Limitations of the correlation between baseline and change as a measure of association

Although the PRR is best understood as a regression model (Kundert et al. 2019), correlations between baseline and follow-up, and between baseline and change have often been used to summarize data and are presented as evidence for the rule. A focus on $\text{cor}(x, \delta)$, where $\delta = y - x$ is the change between follow-up (y) and baseline (x), is intuitive in the context of recovery. The value of this correlation can be effected in unexpected ways due to mathematical coupling, most broadly defined as the setting where one value (x) is also included in the definition of the second (δ). The following relationship is known to hold:

$$\text{cor}(x, \delta) = \frac{\sigma_y \text{cor}(x, y) - \sigma_x}{\sqrt{\sigma_y^2 + \sigma_x^2 - 2\sigma_x \sigma_y \text{cor}(x, y)}} = \frac{\sqrt{k} \text{cor}(x, y) - 1}{\sqrt{1 + k - 2\sqrt{k} \text{cor}(x, y)}} \quad (1)$$

This equation shows the dependence of $\text{cor}(x, \delta)$ on $\text{cor}(x, y)$ and the variance ratio $k = \frac{\sigma_y^2}{\sigma_x^2}$. The relationship between these quantities, visualized as a three-dimensional surface by Hope and colleagues (Hope et al. 2018), is shown as a contour plot in Figure 1. For reasons that will become clear shortly, we highlight the contour corresponding to $k = 1$, where baseline and follow-up have equal variance. Other contour lines in this figure correspond to fixed values of k ranging between 0.01 and 4.

An immediate observation from this plot is that the range of possible values for $\text{cor}(x, \delta)$ depends on $\text{cor}(x, y)$. When $\text{cor}(x, y) = 0$, for example, $\text{cor}(x, \delta)$ is restricted to lie in $[-1, 0]$ rather than $[-1, 1]$. By itself, this suggests that usual tests for the significance of a correlation in which the null value is assumed to be 0 are inappropriate for investigations of recovery. However, as we'll see shortly, this does not suggest that hypothesis tests are impossible – only that more appropriate ones are necessary.

The dependence of $\text{cor}(x, \delta)$ on $\text{cor}(x, y)$ and $k = \frac{\sigma_y^2}{\sigma_x^2}$ is the basis for two related criticisms of using the correlation between baseline and change as a statistical measure of recovery. First, the canonical example of coupling is the setting in which when baseline (x) and follow-up (y) are uncorrelated and have the same variance. This situation is represented by the point on the surface where $\text{cor}(x, y) = 0$ and the variance ratio $k = \frac{\sigma_y^2}{\sigma_x^2} = 1$. In this setting $\text{cor}(x, \delta) = -0.71$ – a value that, for some, is unexpectedly high and casts doubt on any large correlation between baseline and change (Hope et al. 2018; Hawe, Scott, and Dukelow 2019).

A broader argument relates to settings where measurements at follow-up have much lower variance than initial values, as is typically the case for studies of recovery. In cases where k is small, $\text{cor}(x, \delta)$ may be “(non-trivially) stronger than $\text{cor}(x, y)$ ” and therefore spurious or misleading (Hope et al. 2018). Settings with small values of k have been described as “degenerate” in that $\text{cor}(x, \delta)$ will approach -1 (Bonkhoff et al. 2020); as Figure 1 makes clear, this is a concern for any value of $\text{cor}(x, y)$.

The recognition of these statistical issues, and the role they have played in understanding recovery, reveals some limitations of using correlation to measure the association between baseline and change and produce evidence for the significance of this association. By itself, $\text{cor}(x, \delta)$ will give at best an incomplete understanding of recovery, and traditional hypothesis tests (focusing on 0 as a null value) are inappropriate. That said, these criticisms don’t invalidate the PRR – they aren’t even directly relevant to the PRR. Instead, they clarify the importance of understanding the relationship between $\text{cor}(x, \delta)$, $\text{cor}(x, y)$ and the variance ratio $k = \frac{\sigma_y^2}{\sigma_x^2}$; the importance of each these in the studies of recovery; and the use of appropriate summaries of the data.

Distinguishing true and artifactual signals

To paraphrase the previous section, when the variance ratio is small, large values of $\text{cor}(x, \delta)$ can arise from a wide range of $\text{cor}(x, y)$. It has been argued that high correlations between baseline and change are invalid unless they are accompanied by high correlations between baseline and follow-up.

Refutation of this view has a long history in the statistical literature. Oldham (Oldham 1962) argues that a variance ratio other than 1 is evidence for some real effect or process: “Unless some agent has caused a change of standard deviation between the two occasions, σ_x^2 will equal σ_y^2 ”. This argument is slightly more complicated when the outcome measure is bounded, a setting Oldham did not consider but that arises in stroke recovery. Heterogeneous recovery that depends on initial impairment could be the agent that causes a reduction in variance; alternatively, variance may be reduced because recovery is homogeneous but subject to ceiling effects or because the impairment scale is nonlinear. In any case, when $k < 1$ the amount of recovery is related to the baseline value in a way that is not attributable to mathematical coupling, and differentiating between explanations is necessary after ruling out coupling. Oldham’s method, which derives from the role of the variance ratio in studies where

baseline and change are important, formalizes this concept and is a commonly-used approach for understanding the relationship between baseline and change; it will be presented in the next section.

The value of $\text{cor}(x, \delta)$ depends on the variance ratio k and on $\text{cor}(x, y)$. The variance ratio can be used as a measure of the extent to which recovery depends on baseline values, regardless of the value of $\text{cor}(x, y)$. Meanwhile, $\text{cor}(x, y)$ indicates whether follow-up values are related to baseline, regardless of k . Thus $\text{cor}(x, y)$ is relevant for questions of patient-level prediction although, as we'll argue later, correlations are less useful than direct measures of prediction accuracy.

We simulate four datasets with different values of $\text{cor}(x, y)$ and k :

- A: $\text{cor}(x, y) = 0$ and $k = 1$
- B: $\text{cor}(x, y) = .9$ and $k = 1$
- C: $\text{cor}(x, y) = 0$ and $k = .16$
- D: $\text{cor}(x, y) = .9$ and $k = .16$

All datasets have x values generated from a Normal distribution with mean 30 and standard deviation 14, and consist of 30 simulated subjects. Datasets A and B have follow-up values (y) with mean 30, while datasets C and D have follow-up values with mean 53 (variances at follow-up are determined by the variance ratio). The left panels in Figure 1 show baseline and follow-up values (top row) and scatterplots of δ against initial impairment (bottom row), with initial impairment defined as $FM_{max} - x = 66 - x$. The right panel indicates the placement of these datasets on the contour plot of $\text{cor}(x, \delta)$.

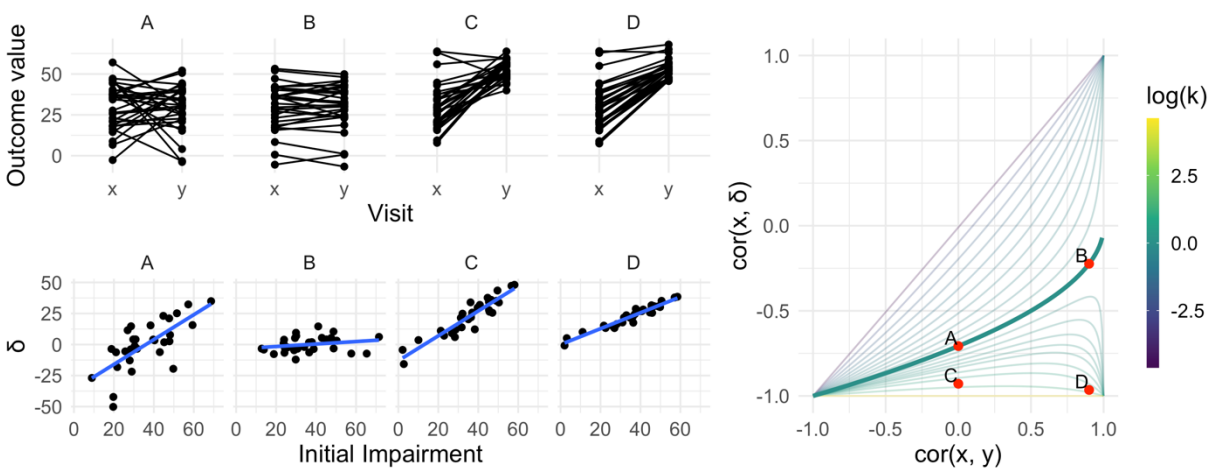


Figure 1: The left panels show four simulated datasets, labeled A, B, C, and D. In the top row, panels show outcome values and baseline (x) and follow-up (y). In the bottom row, panels show change (δ) against initial impairment ($66 - x$). The right panel shows a contour plot of Equation 1, with contours corresponding to values of the variance ratio k and the contour for $k = 1$ highlighted. Points on this surface show correlation values obtained for Dataset A through D.

Dataset A is a canonical example of mathematical coupling, a setting that results in $\text{cor}(x, \delta) = -0.71$. Like Dataset A, Dataset C has $\text{cor}(x, y) = 0$, but the variance ratio is lower. Given our emphasis on k and on $\text{cor}(x, y)$, any debate about whether $\text{cor}(x, \delta)$ for this dataset might be called “spurious” is less relevant than (i) the true reduction in variance that results from recovery; and (ii) the true association between the baseline value and the magnitude of change. Indeed, despite the inability of the baseline value to usefully predict follow-up in Dataset C, these data represent in which baseline values can be used to predict change in a non-artifactual way, which is a setting that Oldham and many others since have argued is important (Oldham 1962; Tu and Gilthorpe 2007).

In contrast, Datasets B and D have large $\text{cor}(x, y)$, which suggests an ability to predict follow-up using baseline with some degree of accuracy. In Dataset B, change from baseline to follow-up is constant with some patient-level noise, and accurate predictions at follow-up are a simple byproduct of that constancy. Dataset B is also, arguably, irrelevant: whether due to measurements that are truly nonlinear, ceiling effects, or proportionality, motor impairment recovery is marked by heterogenous recovery across subjects.

Dataset D represents the least controversial scenario. There is recovery heterogeneity that is predictable based on initial values and results in a variance ratio that is less than one, and the initial values meaningfully predict outcomes at follow-up. This isn’t artifactual: the variance ratio and correlations don’t arise either from coupling or regression to the mean due to measurement error. Real data that are similar to these are suggestive of an underlying biological recovery process in which baseline values predict change and final outcomes.

Taken together, the simulated datasets in this section illustrate the relationship between $\text{cor}(x, y)$, k , and $\text{cor}(x, \delta)$, as well as the kinds of observed data that can give rise to various combinations of these values. The examples highlight discrepancies between $\text{cor}(x, y)$ and $\text{cor}(x, \delta)$ to illustrate their shortcomings when viewed individually. We also identify a setting, typified by Dataset D, in which each measure suggests the presence of a relevant association. It is not the case that data like these necessarily imply that recovery follows the PRR. Other biological models could produce data similar to Dataset D, and how to compare competing models will be considered in later sections.

Recasting Oldham’s method

Equation (1) and Figure 1 show that $\text{cor}(x, y)$ and k determine the value of $\text{cor}(x, \delta)$ in ways that can be counterintuitive. When $\text{cor}(x, y) = 0$, for example, an appropriate null value for a hypothesis test of $\text{cor}(x, \delta)$ is -0.71 rather than 0, because this corresponds to “no recovery” or $k = 1$; a table in the appendix provides null values for hypothesis tests of $\text{cor}(x, \delta)$ under a range of values of $\text{cor}(x, y)$. However, like others, we think the possible confusion around $\text{cor}(x, \delta)$ as a measure of evidence make it less suitable than other approaches.

Oldham’s method suggests to use $\text{cor}(\frac{x+y}{2}, x - y)$, or simply $\text{cor}(x + y, x - y)$, in place of $\text{cor}(x, \delta)$. This correlation is zero, rather than -0.71 , in the canonical example of mathematical

coupling. Indeed, this correlation is zero if and only if $k = 1$ – regardless of $\text{cor}(x, y)$, and even in many cases where measurement error or other processes might affect the ability to reliably measure outcomes at baseline and follow-up. Thus, Oldham’s method often guards against false conclusions due to mathematical coupling and regression to the mean due to measurement error.

Instead of $\text{cor}(x + y, x - y)$, we prefer to focus on the variance ratio k . Values of k that differ from 1 suggest non-artifactual associations between baseline and change. In parallel, we examine the correlation $\text{cor}(x, y)$, which is equal to zero under the null hypothesis that follow-up values are uncorrelated with baseline. These are important but distinct; erroneous suggestions that very small values of k produce spurious correlations seem to stem from conflating the two. We again emphasize that these tests are intended to assess whether correlations are “artifactual”, but not to evaluate support for the PRR in comparison to competing models. For instance, as noted by both (Hope et al. 2018) and (Hawe, Scott, and Dukelow 2019), Oldham’s method does not address the possibility of ceiling effects; in our view, determining which process gives rise to observed correlations comes after assessing whether those correlations are artifacts driven by coupling.

Parametric hypothesis tests are available for both k and $\text{cor}(x, y)$, but depend on assumptions that may be unmet in the context of stroke recovery. We also argue for specific null values of both k and $\text{cor}(x, y)$, although other choices are possible; one might instead choose “random recovery” described in Lohse et al (2021) as a null distribution and identify corresponding values. Instead of a parametric approach, we suggest a resampling-based one that can compare to the null values we suggest, and we describe how this method can be used for other null distributions. See Methods for details. A web-based app is available to carry out this analysis (https://jeff-goldsmith.shinyapps.io/prr_dashboard/).

Correlations, variance ratios, and regression

Correlations have often been taken as evidence for the PRR. These are imperfect – $\text{cor}(x, \delta)$ can be counterintuitive even if, as we’ve seen, viable and appropriate analyses using k and $\text{cor}(x, y)$ are available. More importantly, the PRR is best understood as a regression model in which initial impairment is used as a predictor of change. Null-value hypothesis testing in a regression-based view of the PRR can be difficult for reasons that are analogous to those for correlations; appropriate null values are non-standard. Here we suggest null value tests for regression coefficients and R^2 based on the understanding developed for correlations. As with correlations, other null values (such as those observed for “random recovery”) are also possible. In later sections, we consider alternative ways to evaluate the PRR as a regression model.

A simple linear regression of δ on $ii = \text{max} - x$, where max is the maximum possible value of the scale and $\text{max} - x$ is initial impairment, can be written

$$\delta = \beta_0 + \beta_1 ii + \epsilon.$$

The following expressions relate regression parameters and diagnostics to $\text{cor}(x, y)$ and k :

- $\widehat{\beta}_1 = 1 - \text{cor}(x, y)\sqrt{k}$
- $R^2 = \text{cor}(x, \delta)^2 = \left(\frac{\widehat{\beta}_1}{\sqrt{k - 2\widehat{\beta}_1 - 1}} \right)^2$

From these, we conclude first that $\text{cor}(x, y) = 0$ implies $\widehat{\beta}_1 = 1$. This suggests that usual hypothesis tests of the slope which assume a null value of 0 should instead assume a null value of 1. Moreover, this test measures the association between baseline and follow-up, and slopes that differ significantly from one suggest that baselines can be used to predict follow-up values. Second, we see that the amount of variation explained depends on both $\text{cor}(x, y)$, through the estimated slope, and on the variance ratio; for example, in the canonical example of mathematical coupling, $R^2 = 0.5$. Resampling-based tests for the slope and R^2 can be performed analogously to those for k and $\text{cor}(x, y)$ using these (or other) null values.

Like $\text{cor}(x, \delta)$, R^2 should be interpreted with caution: the preceding expression provides a way to determine the expected or null R^2 for a given slope and $k = 1$, which can be used as a frame of reference for observed R^2 values. R^2 values that depart from the null value may suggest $k \neq 1$ and, by extension, changes that are related to baseline in a way that systematically reduces the variance ratio. As in the previous section, based on this analysis it will remain unclear whether a statistically significant difference is attributable to proportional recovery, ceiling effects, or some other process; distinguishing between models is the subject of later sections.

The above expression for R^2 is in the context of a regression of change on initial impairment, which will differ from the R^2 arising from a regression of the follow-up value on the baseline observation. Because these R^2 values are the square of $\text{cor}(x, \delta)$ and of $\text{cor}(x, y)$, respectively, much of our previous discussion applies here. The initial value x may explain a higher proportion of variation in δ than in y ; this setting is not necessarily artificial, and high R^2 in the regression of change on baseline can be important even when R^2 in the regression of follow-up on baseline is low, just as high $\text{cor}(x, \delta)$ can be important even when $\text{cor}(x, y)$ is low.

The inclusion of the intercept β_0 in the simple linear regression differs from the usual formulation of the PRR and helps to establish clear connections between a correlation-based and a regression-based perspective. This is helpful for evaluating the results of past studies, especially results expressed in terms of percent variation explained, and refines the use of both correlations and regressions as evidence for the PRR.

Similar to correlations and variance ratios, results from a regression-based analysis can, when understood correctly, help assess evidence for the PRR in a given dataset: establishing statistical significance using appropriate tests, along with evaluation of regression diagnostics, will suggest whether data are consistent with the PRR. However, all these approaches measure only linear associations, and neither compare the PRR to alternative models for recovery nor evaluate the ability of the PRR to make accurate predictions about patient outcomes.

Comparing distinct biological models for recovery

The PRR was developed as a model to explain recovery from motor impairment after stroke. Quantitative results, illustrated in Dataset C, show it's possible for recovery, defined as the change from baseline to follow-up, to be related to baseline values even when follow-up is not predicted well by baseline. But the ability to predict patient outcomes at follow-up is important in itself, and predictive performance can form a basis for comparing the PRR to alternative biological models for recovery. We suggest cross validation (CV) as a means to compare models, using median absolute prediction error (MAPE) in held-out data to measure predictive accuracy (lower MAPE values reflect higher prediction accuracy). Details are available in Methods.

To illustrate how prediction accuracy might be used to distinguish between competing models for recovery, we generate three datasets under different recovery mechanisms and use CV to evaluate candidate models. The first two Datasets, which we'll label C_{200} and D_{200} , are generated using the same process as Datasets C and D above but consist of 200 patients. Dataset E_{200} is similar to Dataset B, but has a latent follow-up mean of 70 rather than 30. Follow-up values greater than 66 are subject to threshold, with randomness added to reflect small deviations from the maximum attainable value. That is, Dataset E_{200} implements large, constant recovery (with some noise) and imposes a ceiling.

We consider three models for the association between y and x . First, we assume that y values are randomly distributed around a common mean value, and do not depend on x ; this is an intercept-only regression model, and the mean of observed y values is used to predict future outcomes. Second, we implement the PRR (without intercept) to estimate δ given x , with y taken to be $x + \delta$. Third, we assume that y depends on x , but allow the association to be smooth and nonlinear using a generalized additive model; in contrast to the PRR, this does not assume a constant recovery proportion, and focuses on predicting the follow-up value directly. These models are most appropriate for Datasets C_{200} , D_{200} , and E_{200} , respectively, although the additive model also includes the intercept-only model and the PRR as special cases.

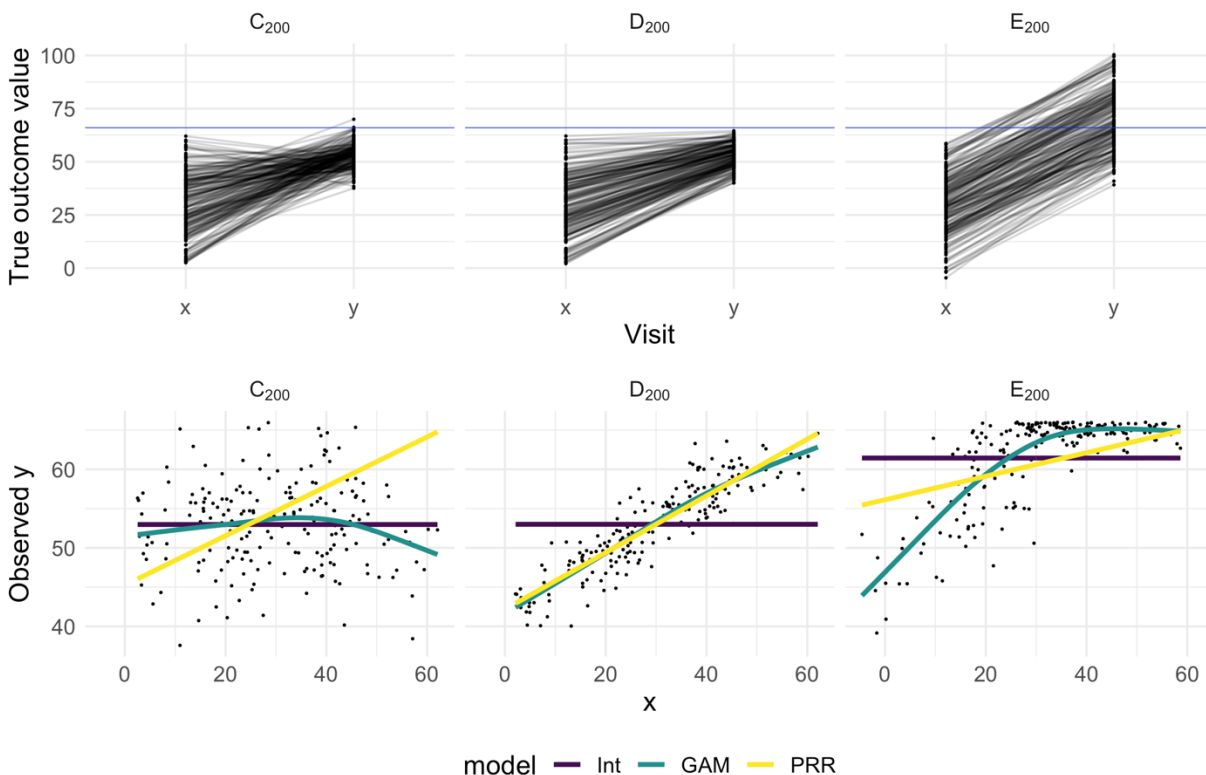


Figure 2: The top panels show three simulated datasets with true outcome values and baseline (x) and follow-up (y); a horizontal line indicates a ceiling on observed values. In the bottom row, panels show the observed (ceiled) value at follow-up against the baseline value. Fitted values from an intercept-only model (Int), a generalized additive model (GAM), and the PRR are shown in the bottom row.

The top row in Figure 2 shows baseline and follow-up values and scatterplots of observed (ceiled) y against x (bottom row). The panels in the bottom row of Figure 2 clarify the relationship between the data generating mechanism and the ability of x to predict y ; in each panel, fitted values from each of the three candidate models are overlaid. Unsurprisingly, for Dataset C₂₀₀, there is no apparent relationship between x and y – these data are generated under $\text{cor}(x, y) = 0$. Dataset D₂₀₀ is a case when baseline values are predictive of change and outcomes. In Dataset E₂₀₀, the expected y increases linearly with x until reaching a plateau, and then is uniformly near the maximum value.

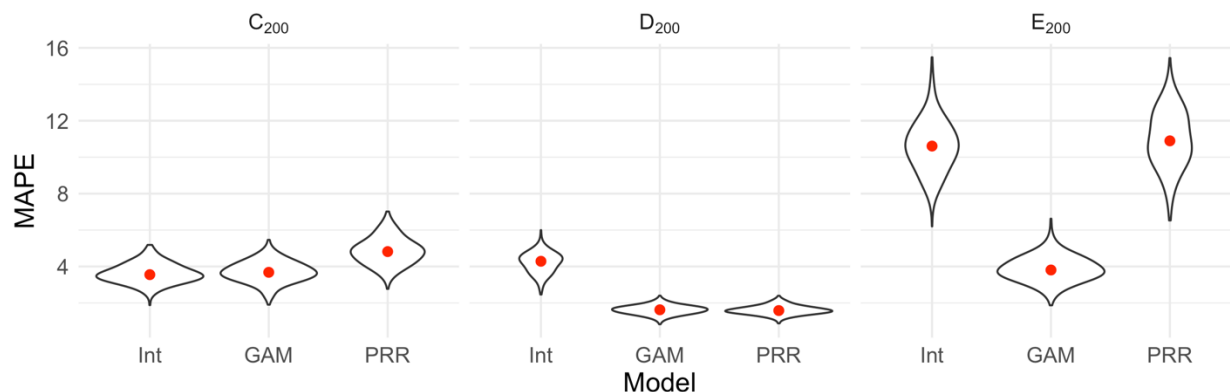


Figure 3: Each panel shows the distribution of median absolute prediction errors (MAPE) obtained using cross validation for each of three models. Panels correspond to the simulated datasets shown in Figure 2. Models compared are an intercept-only model (Int), a generalized additive model (GAM), and the PRR.

Figure 3 shows the result of our cross-validation procedure applied to Datasets C₂₀₀, D₂₀₀, and E₂₀₀; panels show the distribution of MAPE across repeated training / testing splits. For Dataset C₂₀₀, the intercept-only model is the best performer; the PRR suffers from the lack of an intercept, which produces a bias in the predictions. The additive model, meanwhile, is comparable to the intercept-only model, with a very slight increase in MAPE due to the flexibility of the model. For Dataset D₂₀₀, the intercept-only model is the worst performer, while the (true) PRR and additive models are similar. Finally, for Dataset E₂₀₀, only the additive model is flexible enough to capture the underlying non-linear association between y and x .

These results suggest that cross validation can effectively identify a best (or worst) model on the basis of prediction accuracy. When two or more models are similarly accurate, other considerations may be relevant. In Datasets C₂₀₀ and D₂₀₀, for example, the additive model contains the true, simpler model as a special case and is needlessly complex. We also emphasize a limitation of cross validation, which is the exclusive focus on prediction accuracy. This is analogous to using only $\text{cor}(x, y)$ to understand recovery, rather than $\text{cor}(x, y)$ and k together. As we have discussed elsewhere, dismissing observations like those in Dataset C₂₀₀ as uninteresting because baseline does not predict follow-up would be a mistake: the correlation between baseline and change does not arise from mathematical coupling and may reflect important recovery mechanisms. We therefore suggest CV as one component of a careful analysis.

Results for reported datasets

We now evaluate three previously reported datasets in light of the preceding; see Methods for descriptions.

Figure 4 illustrates each of these example datasets. In the left panels, we show observed FM values for patients at baseline and follow-up (top row), and scatterplots of change against baseline (bottom row). Throughout, we differentiate recoverers and non-recoverers as specified

in the original analyses. The right panel shows the contour plot of $\text{cor}(x, \delta)$, with points corresponding to observed values among recoverers for each dataset. These values cluster in the bottom right corner, with reasonably large values of $\text{cor}(x, y)$ and $k < 1$.

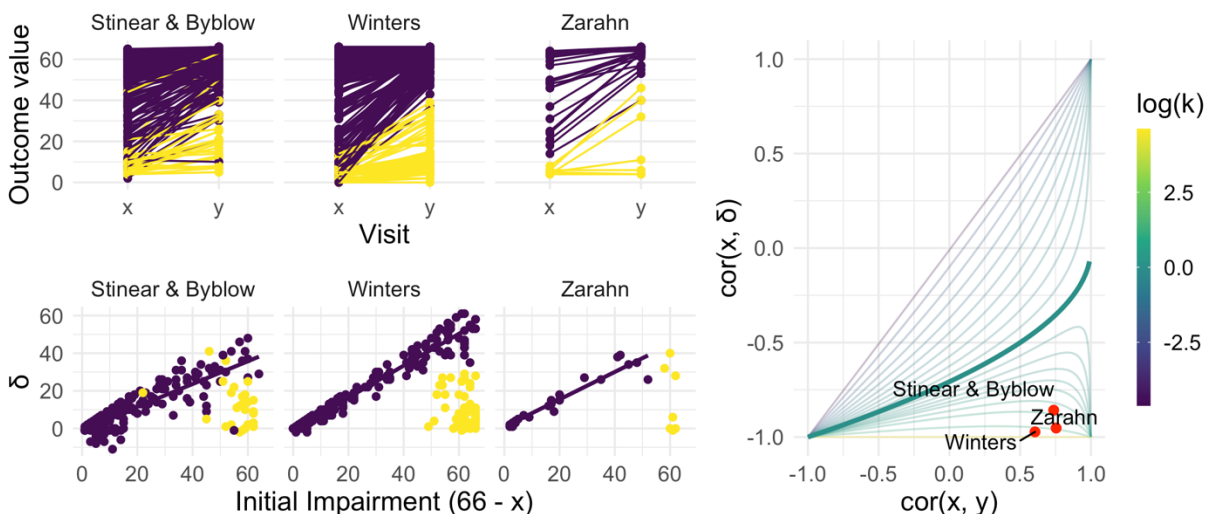


Figure 4: The left panels show three real datasets. In the top row, panels show outcome values and baseline (x) and follow-up (y); points are colored to indicate recoverers (purple) and non-recoverers (yellow) using the definitions from each paper describing the data. In the bottom row, panels show change (δ) against initial impairment ($66 - x$), again separating recoverers and non-recoverers. The right panel shows a contour plot of Equation 1, with contours corresponding to values of the variance ratio k and the contour for $k = 1$ highlighted. Points on this surface show correlation values obtained for the real datasets.

We next conducted the bootstrap analysis on the subsample of recoverers to obtain inference for k and $\text{cor}(x, y)$. We display the results using 1000 bootstrap samples for each dataset in the contour plot in Figure 5, showing the null value corresponding to random recovery for reference, and summarize the results using 95% confidence intervals in the Table 1. For each dataset, there is strong evidence that k and $\text{cor}(x, y)$ differ from our suggested null values (1 and 0, respectively), and from those corresponding to random recovery. That is, we have evidence both that recovery is related to baseline values in a way that reduces variance at follow-up, and also that baseline values are predictive of follow-up.

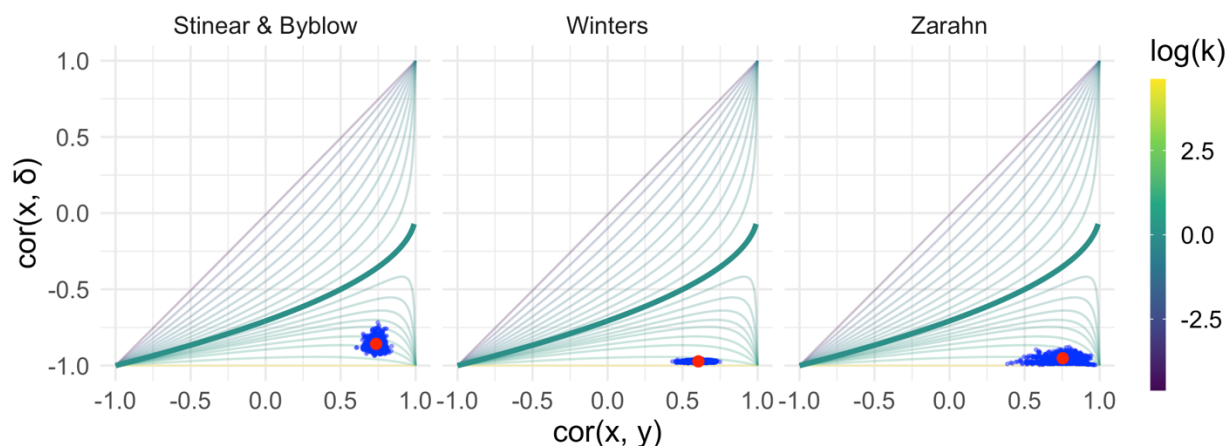


Figure 5: Each panel shows the results of the bootstrap procedure used to obtain inferences about the value of correlations and variance ratio. Red points are the values obtained for the full dataset, and blue points are values obtained in each of 1000 bootstrap samples; points are overlaid on the contour plot of Equation 1.

| Dataset Name | k | $\text{cor}(x, y)$ |
|------------------|-------------------|--------------------|
| Stinear & Byblow | 0.39 [0.27, 0.54] | 0.73 [0.66, 0.79] |
| Winters | 0.07 [0.05, 0.09] | 0.59 [0.49, 0.69] |
| Zarahn | 0.13 [0.03, 0.24] | 0.75 [0.55, 0.92] |

Table 1: Values and 95% confidence intervals for k and $\text{cor}(x, y)$ for each of three datasets. Confidence intervals are obtained through a bootstrap procedure with 1000 bootstrap samples.

We compared the performance of three models in terms of predictive accuracy using cross validation. As for simulated data, we considered an intercept-only model, the PRR, and an additive model. For each dataset, we generated 1000 training / testing splits and summarize prediction accuracy using MAPEs. The plots below show the distribution of MAPE across splits for each model and dataset. Although it was not originally intended for prediction, the PRR consistently outperforms both competitors in terms of prediction accuracy.

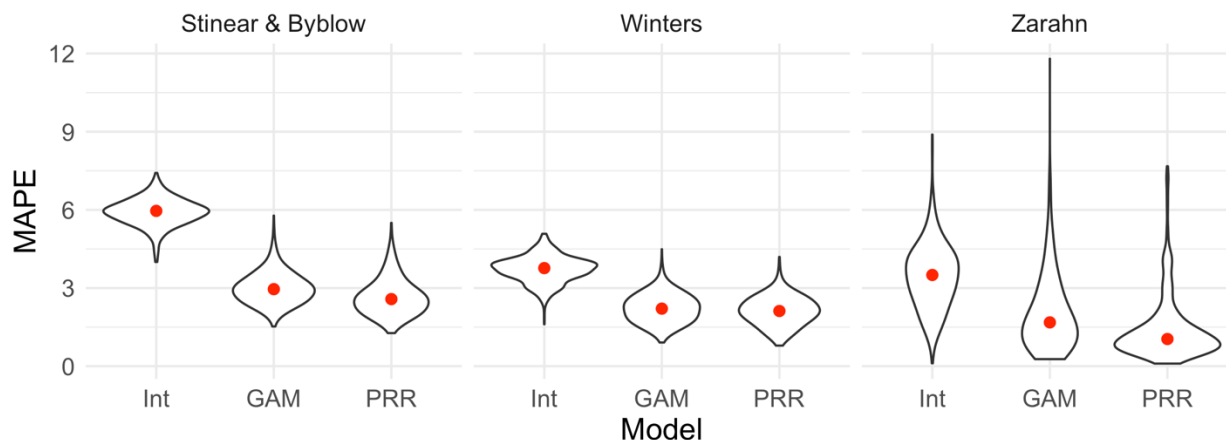


Figure 6: Each panel shows the distribution of median absolute prediction errors (MAPE) obtained using cross validation for each of three models. Panels correspond to the datasets shown in Figure 4. Models compared are an intercept-only model, a generalized additive model, and the PRR.

To provide some frame of reference for the MAPEs reported in Figure 6, in Table 2 we provide values for the percent of outcome variation explained by the PRR for each dataset.

| Dataset Name | R^2 |
|------------------|-------|
| Stinear & Byblow | 0.55 |
| Winters | 0.35 |
| Zarahn | 0.56 |

Table 2: R^2 values reflecting the proportion of follow-up (y) variation explained by the PRR for each of three datasets. Follow-up values are obtained by adding predicted change from the PRR to observed baseline values.

The preceding results for k , $\text{cor}(x, y)$, and cross-validated MAPE suggest that data among recoverers is consistent with the PRR for each study. These results are not driven by coupling or regression to the mean, and a competing model for recovery, specifically, a non-linear association between baseline and follow-up, which might arise from near-constant recovery in the presence of a ceiling effect, does not produce more accurate predictions than the PRR.

Distinguishing between recoverers and non-recoverers

To this point, we have focused on recoverers under the implicit assumption that a biologically distinct group of non-recoverers exists and can be identified. This assumption is supported by prior studies of upper limb motor control and deficits in other domains (Prabhakaran et al 2008, Byblow et al. 2015, Winters et al. 2016, Zandvliet et al. 2020), and promising work suggests it is

possible to identify non-recoverers using baseline characteristics (Byblow et al. 2015). However, the identification of non-recoverers has not been approached in the same way across studies, and there is concern that data-driven methods can produce misleading results in some circumstances (Hawe, Scott, and Dukelow 2019; Lhose et al 2021). It is necessary to understand the limitations of some methods for data-driven subgroup identification before assessing related arguments about recovery and the PRR.

Clustering refers to a collection of methods for unsupervised learning that has several weaknesses in the context of recovery. It is unclear what clustering approach is best, and results can be sensitive to this choice. Perhaps more critically, determining the “true” number of clusters present is imprecise and open to interpretation. Although tools like the Gap statistic (Tibshirani, Walther, and Hastie 2001; James et al. 2013) can provide guidance, the choice between one, two, or more clusters is not supported by hypothesis tests, confidence intervals, or other methods for statistical inference. Practitioners are encouraged to try several numbers of clusters and cautioned to be aware that there is rarely a single best selection (James et al. 2013). Results are typically considered exploratory, and assessed for validity based on visual inspection or additional supporting information. As such, clustering can provide only limited evidence for or against the existence of recoverers and non-recoverers (or finer partitions of patients) when examining a specific dataset. At worst, one might simply assume that distinct recoverer and non-recoverer clusters exist and can be separated using clustering. Failure to critically examine this assumption using visual and quantitative data checks can yield misleading results.

The weaknesses inherent to cluster identification can lead to flawed scientific conclusions. Hawe, Scott, and Dukelow (2019) and Lohse et al (2021) show how errors can arise using “random” recovery. Put briefly, random recovery assumes follow-up values y are uniformly distributed between the baseline x and the maximum possible value. If data arise via this mechanism and it is assumed that two groups exist, the use of clustering will often uncover one cluster that appears to follow the PRR with a recovery proportion of roughly 0.75. A dataset generated under random recovery and analyzed in this way is shown in the left panel of Figure 7.

Based on this, Lohse et al (2021) propose an approach for comparing the PRR to random recovery for an observed sample. Data under random recovery can be generated by drawing baseline values x from the observed values with replacement (to mimic the distribution of baseline values in the sample) and then drawing follow-up values y from a uniform distribution between the baseline x and the maximum possible value. This simulated data can be analyzed through clustering followed by regression to obtain an observed slope in the “recoverer” cluster. By repeating this process many times, one can obtain the distribution of slopes in the “recoverer” cluster under random recovery. Treating this as a null distribution, Lohse et al (2021) argue, provides a way to quantify whether a slope obtained through the same analysis of real data is consistent with random recovery.

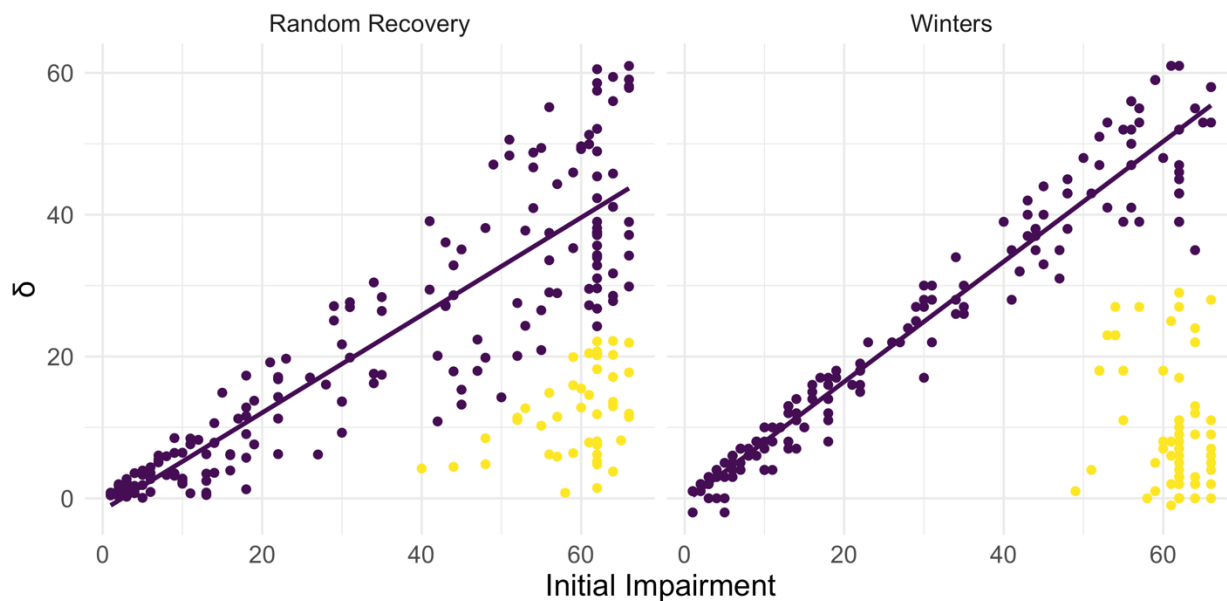


Figure 7: Both panels show change between baseline and follow-up against initial impairment ($66 - \text{baseline}$). Left panel shows data simulated under a ‘random recovery’ process, in which outcome values are drawn from a uniform distribution over the baseline value and ceiling. Right panel presents again data from Winters et al. 2015.

However, a narrow focus on the distribution of slopes that arises from random recovery bypasses a critical question – whether the results of the clustering analysis themselves are consistent with random recovery. Put differently, one must first ask whether there is evidence for the existence of distinct clusters in observed data using random recovery to generate a null distribution. Viewing data generated under random recovery alongside data obtained in a study of upper limb motor control recovery, as in Figure 7, emphasizes this difference. While clustering can misleadingly identify a “recoverer” group when data actually follow random recovery, visual inspection suggests that an obviously different mechanism underlies the Winters dataset. The null distribution of within-cluster dispersion, rather than slopes, provides a way to quantify this difference; see Methods for details. Given the contrast between panels in Figures 7, it is not surprising that this approach rejects the null of random recovery for these data ($p < 0.001$).

From this, we conclude that an inappropriate application of unsupervised learning (i.e. one that presumes two clusters exists) can produce misleading results. This problem is exacerbated by the lack of concrete statistical guidance for determining the number of clusters in a sample. (Similar issues can arise in other ways, for example from a definition of non-recoverers as those who recover less than expected under the PRR.) Simulations of random recovery, like those in Hawe, Scott, and Dukelow (2019) and Lohse et al (2021), are useful for illustrating these issues but should not be misinterpreted: the ability to produce slopes like the PRR through analyses of simulated data does not refute the PRR (or any other model of recovery). Nor does it argue against the existence of meaningful recoverer and non-recoverer groups. In many studies of upper limb motor control recovery, a distinct group of non-recoverers is clear from a

visualization of the data (and supported through appropriate hypothesis tests) or can be identified through a distinct biomarker, and does not artifactually arise through clustering.

Discussion

The PRR was discovered while examining for a possible regularity in the relationship between initial impairment, as measured by the FM-UE, and recovery in the context of upper limb paresis in the time shortly after stroke (Krakauer and Marshall 2015). It was understood as a description of the biological change process that underlies observed recovery, and subsequently evaluated in other recovery settings. Although it was not intended to form the basis for patient-level predictions, the strong correlations between initial impairment and recovery has suggested that accurate predictions are possible. At its core, the PRR models the association between baseline and change; this is always a fraught statistical problem, and recent publications on the PRR have revived longstanding concerns in the context of stroke recovery (Hope et al. 2018; Hawe, Scott, and Dukelow 2019; Bonkhoff et al. 2020).

We have revisited the arguments for the PRR as a descriptive and predictive model, focusing on key statistical questions at each step. We identified scenarios in which observed correlations are “artificial” – induced either by mathematical coupling or regression to the mean due to measurement error – versus those when they are real signals, emphasizing the variance ratio and tests similar to Oldham’s method. For non-artificial signals, we used cross validation to compare models for recovery (e.g. PRR versus constant recovery with a ceiling); this also provides a concrete metric for the clinical usefulness of predictions made by each method. Finally, we considered the problem of distinguishing recoverers from non-recoverers, and the limitations of unsupervised learning for this problem.

Our findings in these datasets suggest that the association between initial impairment and change is non-artificial, and the PRR is better as a biological and predictive model than a non-linear model that is able to capture associations that arise from constant recovery across patients with a ceiling on the outcome. These data also suggest that a biologically distinct group of non-recoverers exists. We distinguish between the usefulness of the PRR as a biological and a predictive model deliberately: biological models are important for understanding the recovery process itself, and accurate predictions are important in clinical care. Although the PRR is useful for both, it isn’t necessary that a single model address both considerations simultaneously.

We acknowledge several limitations and caveats. The statistical considerations for recovery are nuanced and often counterintuitive. Our arguments deviate from usual null-value hypothesis testing, and recognize that zero is often not the appropriate null value. This is related to the important observation that “large” correlation values can arise in a variety of settings, which complicates but does not invalidate statistical approaches. While we distinguish between the usefulness of a model as either biological or predictive, our preferred method for comparing models is based only on their predictive accuracy. Cross validation can identify models that have better or worse predictive performance, but in itself does not examine the validity of

underlying model assumptions or ensure that better-performing models are accurate enough to make meaningful clinical predictions. Recoverers and non-recoverers should be identified in a way that is not artificial, and that does not serve to introduce evidence for a model of recovery that would not otherwise exist. Lastly, we recognize that not every dataset will be similar to those we presented; in those cases, we hope the tools we suggest will be used to evaluate the PRR against other models.

The PRR provides an appealingly simple model for understanding recovery, even if the statistical approaches for evaluating it are not direct. We argue that the PRR is and will continue to be relevant as a model for recovery, but we agree with others that more complex analytic strategies are necessary to move beyond it. Recovery depends on factors other than initial impairment. The PRR estimates an average recovery proportion, but individuals will recover more or less than that average; determining whether this is “noise” or heterogeneity that can be predicted using other forms of measure at baseline is an important next step. Similarly, reliable techniques to identify non-recoverers at baseline are needed. Different outcome measures and different recovery settings may not be well described by the PRR. A specific focus on predicting long-term outcomes is an important goal; supervised learning methods may be helpful in this, although many of these methods have unclear interpretations.

More complex models than the PRR do not inherently resolve the statistical issues we’ve raised and may in fact make them harder to identify. For example, it’s been suggested that mixed models could account for differences in baseline values and change across subjects in a way that avoids mathematical coupling by modeling baseline and follow-up values directly (Lohse et al. 2021; Bowman et al. 2021). This is true for a specific, non-standard numeric coding of visit times, but a more standard mixed model does not avoid coupling. Consider a model for outcome values at baseline (time = 0) and a single follow-up (time = 1) that includes both random intercepts and random slopes. When such a model is applied to Datasets A, C, and D, the random intercepts and slopes will be correlated; low random intercepts will suggest steeper random slopes in a way that mimics baseline and change scores. Put differently, to predict a follow-up value from baseline, one must use the baseline value to predict a random slope using the correlation between random effects. Distinguishing between mathematical coupling and recovery that changes the variance ratio remains a problem, but now one that involves the correlation of random effects. Alternatively, coding baseline as time = -0.5 and follow-up as time = 0.5 induces a model that mimics Oldham’s method, and avoids coupling based on similar arguments (Blance, Tu, and Gilthorpe 2005).

Our point is not that mixed models are a wrong choice – in fact, we are enthusiastic about recent work that combines serial measurement, nonlinear trends, random effects, and mixture models (van der Vliet et al. 2020). Taken together, these elements can overcome many of the limitations introduced by studies that include only baseline and single follow-up observations. Serial measurements and careful modeling provide insight into patients’ recovery trajectory, reduce effects of measurement error, and identify non-recoverers early in the recovery process. Nonetheless, non-linear mixed models fit to serial measurements are not a panacea, and do not avoid the challenges described in this paper. The same fundamental issues that arise from

within-subject correlation and changing variances over time due to recovery and measurement ceilings should be considered when using this or any other model framework. Indeed, more complex models may serve to mask these basic issues by making them implicit rather than explicit.

Allowing for differences in datasets, implementations, and performance criteria, our results are consistent with those reported in recent papers examining the PRR as a predictive model. Bonkhoff et al. 2020 fit several models to a subset of patients selected to mitigate ceiling effects and avoid including non-recoverers, and found that that PRR was among the best performing models in terms of out-of-sample prediction accuracy. The percent of outcome variation explained was lower in their work than in our analyses (21% vs 35-56%), leading the authors to suggest that the PRR may be better than other models but insufficient for making clinical predictions in the context of precision neurology. Our view is a less pessimistic take on the same information: that the PRR outperforms competing models (including those intended to account for ceiling effects) attests to its value, and the percent of outcome variation explained is suggestive of an important biological mechanism that should be investigated and understood— even if R^2 values are not as high as has been suggested. After all, if it were found that a risk factor accounted for greater than 20% of the variance in the chance of getting a disease it would immediately be investigated and prevention attempted. From the standpoint of clinical prediction, it seems likely that accurate models developed in the future will include initial impairment as a covariate, and may include a term that reflects proportional recovery.

In light of this, we stress again that the PRR is intended as a model for recovery from a specific form of impairment as measured by the FM, and is best understood as an attempt to mathematically capture a component of the recovery process. The emphasis on change between baseline and follow-up is deliberate: biological recovery is a process that causes a change, which then leads to the final value. Understanding whether recovery varies across patients and what mechanism might drive such variability is a fundamental scientific question. That the PRR also has some value for predicting final outcomes is to be welcomed but not necessary for its biological importance.

Applications of the PRR in studies of upper limb motor control recovery have often found that, averaging across recoverers, roughly 70% of lost function is regained in the time shortly after stroke. We've argued that this is attributable to spontaneous biological recovery (Cramer 2008; Zeiler and Krakauer 2013; Cassidy and Cramer 2017). The existence of such a mechanism does not imply that behavioral interventions are unable to improve patient outcomes. Instead, future clinical trials should seek to improve on the proportion of impairment reduction, reduce the proportion of non-recoverers, or induce changes that are distinct from (and better than) those expected under the PRR.

Conclusions

Consideration of associations between baseline, follow-up, and change continues across domains despite the statistical challenges, and for good reason: these can be and often are related in ways that are not due to artifacts. Our goal here was to clarify statistical reasoning concerning the problem of relating baseline to change in the context of stroke recovery. It is for the reader to decide whether the work presented here is either a bumpy statistical detour or an interesting scenic route. In either case, rigor about this issue is essential for continued biological and clinical progress, and it would be unfortunate if the recent spate of papers leads to dismissal of the PRR out of either confusion or exhaustion.

As a model that relates baseline values to change, the PRR requires the application of careful, and sometimes counterintuitive, statistical techniques. We have described well-established but non-standard approaches to distinguish between artifacts due to coupling from signals that arise from true associations, introduced tools to compare competing models for recovery based on their predictive accuracy, and elaborated on issues that can arise when using some data-driven methods to distinguish recoverers and non-recoverers. In our analyses of real data, we found evidence for signals not attributable to coupling and obtained better predictions using the PRR than a model that assumes constant recovery (with some noise) up to a ceiling. This suggests that the PRR is non-artifactual and remains relevant, at the very least, as a model for recovery. Future work should seek to both explain the mechanistic basis for PRR and improve upon it as a predictive model.

Methods

Reported Datasets

Details of inclusion and exclusion criteria are available in the referenced literature. All patients received usual care according to evidence-based stroke guidelines for physical therapists, but no systematic interventions.

- **Stinear & Byblow:** combined data from two studies. First, Byblow et al 2015 assessed an *a priori* prediction of proportional recovery based on corticospinal tract integrity using transcranial magnetic stimulation to determined motor evoked potential status (MEP+, MEP-) for 93 patients within 1 week of first-ever ischemic stroke. FMA-UE were obtained at 2, 6, 12, and 26 weeks. Second, Stinear et al 2017 added data from recurrent ischemic stroke and intracerebral hemorrhage patients with new upper-limb weakness to form a larger dataset of 157 patients, all with known MEP status. Following this work, we define recoverers and non-recoverers as MEP+ and MEP-, respectively.
- **Winters:** first ever ischemic stroke patients were recruited for the prospective cohort study entitled Early Prediction of functional Outcome after Stroke (EPOS) (Nijland et al 2010; Veerbeek et al 2011). Data comprise baseline (day 2 post-stroke) and follow-up (day 187 post-stroke) FMA-UE observations for 223 patients; 211 were originally reported in Winters

et al 2015, with recoverers and non-recoverers identified using a hierarchical clustering based on average pairwise Mahalanobis distances.

- **Zarahn:** data consist of patients with first time ischemic stroke with some degree of clinical hemiparesis (NIH stroke scale for the arm ≥ 1). FMA-UE was assessed both at ~ 2 days post-stroke and ~ 3 months post-stroke and were originally reported in Zarahn et al 2011. We focus on the 30 patients in the imaged subsample with publicly available FMA-UE values. Recoverers and non-recoverers are determined using baseline FMA-UE > 10 .

Resampling approach for inference on $\text{cor}(x, y)$ and k

We suggest a bootstrap procedure to obtain confidence intervals for $\text{cor}(x, y)$ and k . A single bootstrap sample can be constructed by selecting subjects (pairs of both x and y values) from a full dataset with replacement. Next, we compute the values k and $\text{cor}(x, y)$ for the bootstrap sample. This is repeated a large number of times (e.g. 1000) to produce an empirical distribution for the quantities of interest, which can be used to derive corresponding confidence intervals. Simulations evaluating this approach suggest that coverage of 95% CIs is roughly 0.95 for moderate sample sizes.

Our suggested null values for k and $\text{cor}(x, y)$ are 1 and 0, respectively, but other values can be used. For null hypotheses framed in terms of data generating mechanisms rather than parameter values, such as the “random” recovery null hypothesis (Lohse et al 2021), it can be difficult to derive the corresponding null values. In these cases, we suggest to obtain empirical values by generating a large dataset under the null and computing the k and $\text{cor}(x, y)$ directly.

Cross validation to compare models

Data are divided into training and testing sets; training data are used to fit models, and these models are applied to data in the testing set to obtain predicted outcomes. The difference between predicted and observed outcomes in the testing data reflects each model’s ability to make accurate predictions of data not used in model development. Comparing models in terms of their median absolute prediction error (MAPE) is an established technique for choosing among candidate models, and the MAPE provides a measure of the anticipated prediction error for a given model.

Cross validation has several possible implementations; here random training and testing splits are comprised of 80% and 20% of the data, respectively, and the training data is used to fit each model. Given model fits, predictions are made for the testing dataset and compared to actual outcomes, and the difference is summarized using the MAPE. This process is then repeated 1000 times, so that the distribution of MAPE across training and testing splits is obtained.

Defining a null distribution for within-cluster dispersion

Although the Gap statistic does not allow for inference to determine the number of clusters within a sample, it provides a useful metric for comparing observed data to a null hypothesis of random recovery. Intuitively, for a given number of clusters k , the Gap statistic $Gap(k)$ compares the observed degree of within-cluster similarity to the expected degree of within-cluster similarity under a reference distribution. Suppose a clustering analysis has produced clusters C_1, C_2, \dots, C_k . Assuming the Euclidean distance is used to measure distance between observations in the same cluster, we measure overall within-cluster dispersion using the pooled within cluster sum of squares around the cluster mean:

$$W_k = \sum_{r=1}^k \sum_{z_i \in C_r} \|z_i - \mu_r\|^2.$$

Here, μ_r is the within-cluster mean and z_i is the vector of observed values for subject $1 \leq i \leq n$ (e.g. $z_i = (x_i, y_i)$).

The value of W_k decreases as k increases, regardless of whether additional true clusters are identified. The Gap statistic therefore standardizes $\log(W_k)$ to provide guidance on the choice of k within a dataset. To standardize $\log(W_k)$, one compares the observed value to its expectation under a reference distribution:

$$Gap_n(k) = E_n^*\{\log(W_k)\} - \log(W_k).$$

The expectation $E_n^*\{\log(W_k)\}$ is approximated through the analysis of multiple datasets simulated under the reference distribution. For each dataset one computes $\log(W_k^*)$, and the expected value is taken as the average across these. The reference distribution in the calculation of the Gap statistic is often uniform over the range of each feature in the clustering analysis. In the context of recovery, this suggests a square over all possible values of x and y rather than the triangular region defined by random recovery, but the spirit is similar.

We use the Gap statistic to measure the strength within-cluster dispersion against that expected under a reference distribution. To compare observed data to a null distribution, we suggest a resampling-based approach to construct a null distribution for $Gap_n(k)$. For random recovery, to construct a single resampled dataset, we suggest to sample observed x values with replacement; generate corresponding y values under random recovery; and obtain $Gap_n^*(k)$. This process is repeated many times, and the observed value $Gap_n(k)$ is compared to the distribution of $Gap_n^*(k)$. This process is very similar to one suggested by Lohse et al 2021, with the exception that we focus on evidence for clustering through $Gap_n(k)$ rather than the distribution of slope values obtained in analyses of resulting clusters.

The Gap statistic can be computed for any clustering method. By extension, our method for comparing the observed amount of within-cluster dispersion to that expected under a null distribution, can as well. In our analyses we follow recent literature, and use hierarchical clustering based on Mahalanobis distances between points. Simulations suggest that our testing approach achieves nominal size: when data are in fact generated under random recovery, we reject the null hypothesis 5% of the time under $\alpha = 0.05$.

Acknowledgements

We acknowledge the EXPLICIT-stroke consortium for collecting data. This data collection was supported by funding from the Royal Dutch Society of Physical Therapy and the Netherlands Organization for Health Research and Development (ZonMw; Grant No. 89000001). JG's work was supported in part by NIH-funded R01NS097423.

References

- Blance, Andrew, Yu-Kang Tu, and Mark S Gilthorpe. 2005. "A Multilevel Modelling Solution to Mathematical Coupling." *Statistical Methods in Medical Research* 14 (6): 553–65.
- Bonkhoff, Anna K, Thomas Hope, Danilo Bzdok, Adrian G Guggisberg, Rachel L Hawe, Sean P Dukelow, Anne K Rehme, Gereon R Fink, Christian Grefkes, and Howard Bowman. 2020. "Bringing proportional recovery into proportion: Bayesian modelling of post-stroke motor impairment." *Brain*.
- Bowman, Howard, et al. "Inflated Estimates of Proportional Recovery From Stroke: The Dangers of Mathematical Coupling and Compression to Ceiling." *Stroke* (2021): STROKEAHA-120.
- Byblow, Winston D, Cathy M Stinear, P Alan Barber, Matthew A Petoe, and Suzanne J Ackerley. 2015. "Proportional Recovery After Stroke Depends on Corticomotor Integrity." *Annals of Neurology* 78 (6): 848–59.
- Cassidy, Jessica M, and Steven C Cramer. 2017. "Spontaneous and Therapeutic-Induced Mechanisms of Functional Recovery After Stroke." *Translational Stroke Research* 8 (1): 33–46.
- Cramer, Steven C. 2008. "Repairing the Human Brain After Stroke: I. Mechanisms of Spontaneous Recovery." *Annals of Neurology* 63 (3): 272–87.
- Hawe, Rachel L, Stephen H Scott, and Sean P Dukelow. 2019. "Taking Proportional Out of Stroke Recovery." *Stroke* 50 (1): 204–11.
- Hope, Thomas M H, Karl Friston, Cathy J Price, Alex P Leff, Pia Rotshtein, and Howard Bowman. 2018. "Recovery after stroke: not so proportional after all?" *Brain* 142 (1): 15–22.
- James, Gareth, Daniela Witten, Trevor Hastie, and Robert Tibshirani. 2013. *An Introduction to Statistical Learning*. Vol. 112. Springer.
- Krakauer, John W, and Randolph S Marshall. 2015. "The Proportional Recovery Rule for Stroke Revisited." *Annals of Neurology* 78 (6): 845–47.
- Kundert, Robinson, Jeff Goldsmith, Janne M Veerbeek, John W Krakauer, and Andreas R Luft. 2019. "What the Proportional Recovery Rule Is (and Is Not): Methodological and Statistical Considerations." *Neurorehabilitation and Neural Repair* 33 (11): 876–87.
- Lazar, Ronald M, Brandon Minzer, Daniel Antonello, Joanne R Festa, John W Krakauer, and Randolph S Marshall. 2010. "Improvement in Aphasia Scores After Stroke Is Well Predicted by Initial Severity." *Stroke* 41 (7): 1485–8.
- Lohse, Keith, Rachel Hawe, Sean Dukelow, and Stephen Scott. 2021. "Statistical Limitations on Drawing Inferences About Proportional Recovery." *Neurorehabilitation and Neural Repair* 35 (1): 10–22.

Oldham, PD. 1962. "A Note on the Analysis of Repeated Measurements of the Same Subjects." *Journal of Chronic Diseases* 15 (10): 969–77.

Prabhakaran, Shyam, Eric Zarahn, Claire Riley, Allison Speizer, Ji Y Chong, Ronald M Lazar, Randolph S Marshall, and John W Krakauer. 2008. "Inter-Individual Variability in the Capacity for Motor Recovery After Ischemic Stroke." *Neurorehabilitation and Neural Repair* 22 (1): 64–71.

Stinear, C. M., Byblow, W. D., Ackerley, S. J., Smith, M. C., Borges, V. M., & Barber, P. A. (2017). PREP2: A biomarker-based algorithm for predicting upper limb function after stroke. *Annals of clinical and translational neurology*, 4(11), 811-820.

Tibshirani, Robert, Guenther Walther, and Trevor Hastie. 2001. "Estimating the Number of Clusters in a Data Set via the Gap Statistic." *Journal of the Royal Statistical Society: Series B (Statistical Methodology)* 63 (2): 411–23.

Tu, Yu-Kang, and Mark S Gilthorpe. 2007. "Revisiting the Relation Between Change and Initial Value: A Review and Evaluation." *Statistics in Medicine* 26 (2): 443–57.

Veerbeek, Janne M, Caroline Winters, Erwin EH van Wegen, and Gert Kwakkel. 2018. "Is the Proportional Recovery Rule Applicable to the Lower Limb After a First-Ever Ischemic Stroke?" *PloS One* 13 (1): e0189279.

van der Vliet, Rick, Ruud W Selles, Eleni-Rosalina Andrinopoulou, Rinske Nijland, Gerard M Ribbers, Maarten A Frens, Carel Meskers, and Gert Kwakkel. 2020. "Predicting Upper Limb Motor Impairment Recovery After Stroke: A Mixture Model." *Annals of Neurology* 87 (3): 383–93.

Winters C, van Wegen EE, Daffertshofer A, Kwakkel G. Generalizability of the Proportional Recovery Model for the Upper Extremity After an Ischemic Stroke. *Neurorehabil Neural Repair*. 2015 Aug;29(7):614-22. doi: 10.1177/1545968314562115. Epub 2014 Dec 11. PMID: 25505223.

Winters C, Kwakkel G, Nijland R, van Wegen E; EXPLICIT-stroke consortium. When Does Return of Voluntary Finger Extension Occur Post-Stroke? A Prospective Cohort Study. *PLoS One*. 2016 Aug 5;11(8):e0160528. doi: 10.1371/journal.pone.0160528. PMID: 27494257; PMCID: PMC4975498.

Winters, Caroline, Erwin EH Van Wegen, Andreas Daffertshofer, and Gert Kwakkel. 2017. "Generalizability of the Maximum Proportional Recovery Rule to Visuospatial Neglect Early Poststroke." *Neurorehabilitation and Neural Repair* 31 (4): 334–42.

Zandvliet SB, Kwakkel G, Nijland RHM, van Wegen EEH, Meskers CGM. Is Recovery of Somatosensory Impairment Conditional for Upper-Limb Motor Recovery Early After Stroke? *Neurorehabil Neural Repair*. 2020 May;34(5):403-416. doi: 10.1177/1545968320907075. PMID: 32391744; PMCID: PMC7222963.

Zeiler, Steven R, and John W Krakauer. 2013. "The Interaction Between Training and Plasticity in the Post-Stroke Brain." *Current Opinion in Neurology* 26 (6): 609.

Supplementary materials

In the table below, we provide values of $\text{cor}(x, \delta)$ for a range of input values $\text{cor}(x, y)$, keeping k fixed at 1. These are a result of equation (1) in the manuscript, and are intended to provide context for correlations between baseline and change that arise through coupling rather than as a result of a recovery process that affects the variance ratio.

| k | $\text{cor}(x, y)$ | $\text{cor}(x, \delta)$ |
|-----|--------------------|-------------------------|
| 1 | 0 | -0.707 |
| 1 | 0.1 | -0.671 |
| 1 | 0.2 | -0.632 |
| 1 | 0.3 | -0.592 |
| 1 | 0.4 | -0.548 |
| 1 | 0.5 | -0.5 |
| 1 | 0.6 | -0.447 |
| 1 | 0.7 | -0.387 |
| 1 | 0.8 | -0.316 |
| 1 | 0.9 | -0.224 |