

# Spatial redistribution of neurosecretory vesicles upon stimulation accelerates their directed transport to the plasma membrane.

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## Abstract

Through the integration of results from an imaging analysis of intracellular trafficking of labelled neurosecretory vesicles in chromaffin cells, we develop a Markov state model to describe their transport and binding kinetics. Our simulation results indicate that a spatial redistribution of neurosecretory vesicles occurs upon secretagogue stimulation leading vesicles to the plasma membrane where they undergo fusion thereby releasing adrenaline and noradrenaline. Furthermore, we find that this redistribution alone can explain the observed up-regulation of vesicle transport upon stimulation and its directional bias towards the plasma membrane. Parameter fitting indicates that in the deeper compartment within the cell, vesicle transport is asymmetric and characterised by a bias towards the plasma membrane. We also find that crowding of neurosecretory vesicles undergoing directed transport explains the observed accelerated recruitment of freely diffusing vesicles into directed transport upon stimulation.

*Keywords:* intracellular transport, secretion, neurosecretory vesicles, regulated exocytosis, cytoskeleton

## Introduction

Neuroendocrine chromaffin cells in the adrenal medulla are a model system to study the exocytosis of secretory vesicles (SVs) which is preceded by their transport from the Golgi apparatus to their site of exocytosis on the plasma membrane [1]. Defects in this process have been tied to a range of neurodegenerative diseases [2] by mechanism that are not yet fully elucidated [3]. The highly crowded and stochastic nature of the cytoplasm, however, represents a major difficulty in exploring intracellular transport systems and as a result many of the mechanisms involved in bringing vesicles towards the plasma membrane remain elusive [1].

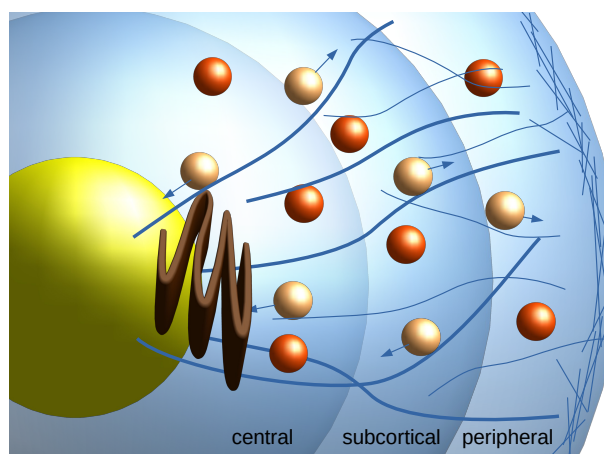
Microtubules and actin filaments perform a vital role in the transport of secretory vesicles and can be considered the tracks of the intracellular transport network [4]. They are semi-flexible and some of them can be several  $\mu\text{m}$  in length.

In the central region of the cytoplasm both systems of cytoskeleton filaments, F-actin and microtubules, are involved in the cytoplasmic transport of secretory granules [5–7] through molecular motor proteins. In this cellular region microtubules are

mostly aligned radially while close to the cortex their density is lower and they align tangentially with the cortex [6]. In the periphery of the cell, transport along the actin filament network occurs through processive molecular motors such as myosin-V [8,9] [1,10] and non-processive such as Myosin-II [11]. Recruitment of SVs to the cortical actin network occurs via the action of Myosin-VI short-insert isoform which has both a processive and a non-processive function [12].

The sketch shown in Fig 1 shows the cytoplasm of chromaffin cells with neurosecretory vesicles immersed in and occasionally transported along microtubules (thick lines) or actin filaments (thin lines). In addition to its role as a barrier between the cytoplasm and the active sites [13,14] the cortical actin network has an active role in exocytosis. It contributes to the transport of SVs in the periphery of the cell [15], facilitates the transport of SVs through the cellular cortex towards the sites of exocytosis and it also contributes mechanically to the exocytosis [16,17].

Vesicles undergoing directed motion along microtubules often cover relatively large distances [18]. Some vesicles exhibit a restricted behaviour [19] termed "caged", which is generally associated to anchoring to the actin meshwork [12]. It has also been suggested that within the dense actin meshwork, secretory vesicles can become effectively trapped and hence also display caged behaviour [18].



**Fig 1.** Sketch of secretory vesicle transport between the Golgi apparatus (brown) and the cortical actomyosin network in chromaffin cells. Microtubules are shown as thick blue curves, actin filaments as thinner fibres. Secretory vesicle currently undergoing transport are represented by the lighter coloured spheres with arrows denoting the direction of transport whereas the darker orange spheres represent vesicles that are freely diffusing in the cytoplasm.

In [19] Live-cell imaging of nicotine stimulated bovine adrenal chromaffin cells was used to track the motion of secretory vesicles in 3-dimensions by confocal microscopy. Vesicles were categorised as undergoing either directed, free or caged motion and according to their distance from the plasma membrane. The measured transition rates implied that upon nicotine stimulation, cells spatially adjust their secretory vesicle pools and that upon stimulation both the fraction of vesicles undergoing directed transport increases as well as the rate by which vesicles enter directed transport – both contributing to the efficient replenishment of the pools of releasable vesicles. What feedback mechanisms, however, trigger those adjustments is not currently known.

The aim of this study is to introduce a quantitative description of secretory vesicle transport in chromaffin cells that is well adapted to the available data. Our goal is to show that spatial redistribution of vesicles can trigger the observed up-regulation of

directed transported upon stimulation. 48

Modelling studies of intracellular transport have so far focused on transport along 49  
and within bundles of fibres [20–23]. On the other hand cytoplasmic vesicle transport as 50  
part of the secretory pathway has not received much attention from modellers so far: 51  
In [24] the biochemical reaction network underlying exocytosis has been modelled 52  
through a system of rate equations. Agent based models have been considered in 53  
various studies such as in [25] which focuses on simulation methods, as well as in [26] on 54  
spatial aspects of vesicular sorting into different compartments and in [27] on aspects of 55  
pattern formation. 56

Mathematical modelling of the transport of secretory vesicles in chromaffin cells has 57  
so far been focusing on arrival and release statistics. Amperometric techniques make it 58  
possible to record the discrete arrival times of newly trafficked vesicles at the plasma 59  
membrane and hence provide insight into the underlying nature of the secretory 60  
pathway. In [28] it was shown that these arrival times follow a non-Poissonian 61  
probability distribution suggesting that there is an active recruitment process 62  
underlying the replenishment of releasable vesicles upon stimulation. More specifically, 63  
through the coupling of an attractive harmonic potential to a random process modelling 64  
vesicle migration, key aspects of arrival time statistics could be explained. Nevertheless, 65  
such a phenomenological model does not have the potential to link this effect to 66  
structural properties of the intracellular environment. 67

In order to address this issue, a recent study [29] suggested a system of 68  
advection-diffusion equations [30] as a tool to explore the various features of 69  
up-regulation of directed vesicle transport reported in [19]. It was found that spatial 70  
redistribution triggered by nicotine stimulation explains the observed bias toward 71  
*outward transport as compared to inward* transport upon stimulation. The parameter 72  
space for this class of models, however, turned out to be too high-dimensional 73  
prohibiting meaningful parameter fitting given the limited amount of available data [19]. 74  
As a consequence, this study could not address the question whether and under which 75  
additional assumptions the spatial redistribution that occurs upon stimulation can 76  
explain other more intricate aspects of up-regulation such as the much larger overall 77  
fraction of vesicles undergoing directed transport and the accelerated recruitment into 78  
directed transport. 79

In our study we construct a conceptually simpler Markov state model to address 80  
these questions. This allows for a direct incorporation of the transition rates which are 81  
reported in [19] individually for each of the three spatial compartments: central, 82  
subcortical and peripheral. 83

We indeed find that the Markov chain based on the reported transition rates 84  
predicts spatial redistribution upon stimulation. Adding the additional assumption 85  
obtained through parameter fitting that the transport network in the central part of the 86  
cell has an outward bias, we find that this amplifies the overall fraction of vesicles 87  
undergoing directed transport in agreement with observations. We illustrate the 88  
underlying mechanism using an even simpler minimal Markov state model. 89

We also find that spatial redistribution accelerates the transition rates into directed 90  
transport as reported in [19] provided that the capacity of transport fibres is limited. 91

## Preliminary experimental results 92

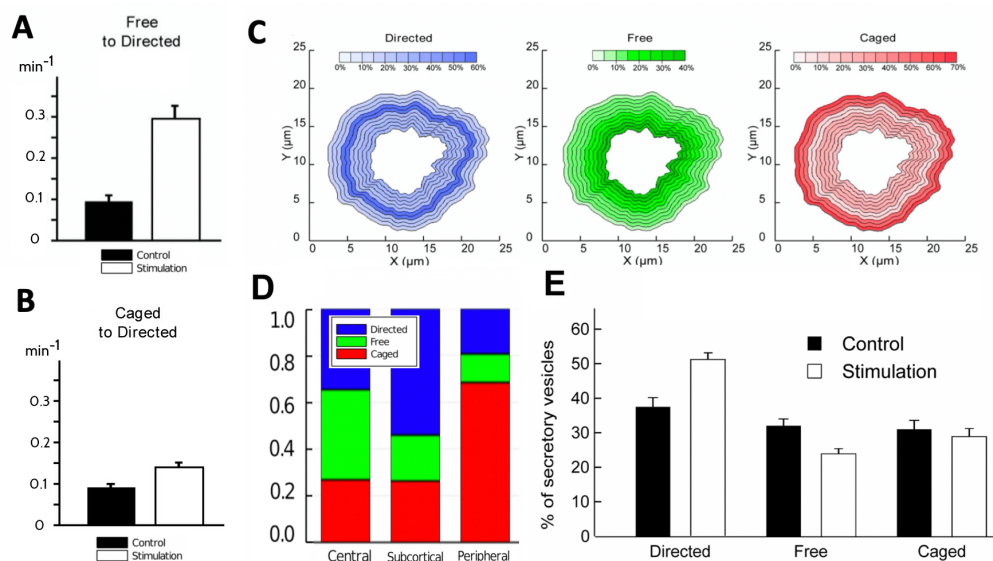
In [19] bovine adrenal chromaffin cells were imaged using time-lapse z-stack confocal 93  
imaging. A number of equatorial slices in the x-y plane of chromaffin cells were imaged 94  
so that 20% of the cell's latitudinal range was covered. As a consequence, most of the 95  
secretory vesicle activity occurred within the imaged region. Individual vesicles were 96  
then tracked and the growth of each trajectory's mean square displacement as a 97  
function of time - sub-linear, linear or supra-linear - was used to categorize them as 98

either *caged*, *free* or *directed*. Comparing vesicles in control and in nicotine stimulated cells, the following key findings were reported:

1. *Up-regulation of directed transport*: Upon stimulation the fraction of vesicles undergoing directed motion grows from roughly 38% to 52% (Fig 1E in [19] which is reproduced in Fig 2E).
2. *Bias towards outward transport*: While vesicle transport is unbiased in control cells, in stimulated cells the ratio of outward vs. inward transport is roughly 2:1 (Fig 3S and 3T in [19]).

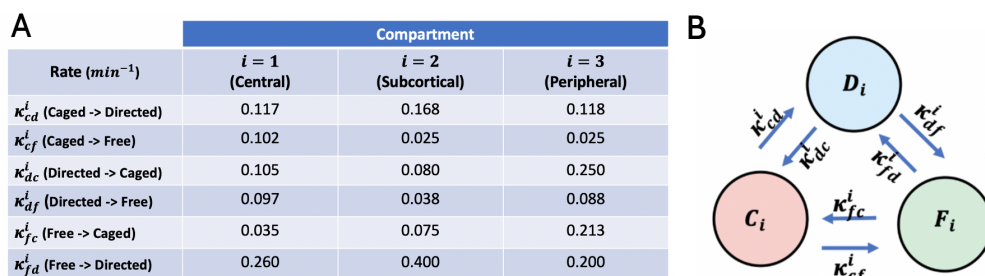
In addition to categorising vesicle trajectories, the transitions of vesicles from one motile state to another were recorded in trajectories spanning periods of 2 minutes. One of the key observations was that

3. stimulation leads to a *three-fold increase of the rate by which vesicles transition from free (unbiased random walk) motion to directed motion* (Fig 3H in [19] reproduced in Fig 2A).



**Fig 2. Statistics of tracked vesicles reported in [19].** (A) Figures 3H (with rates per 2 min) in [19]: average transition rates from free to directed motile state in control and stimulation. (B) Figures 3B (with rates per 2 min) in [19]: average transition rates from caged to directed motile state in control and stimulation. (C) Figure 2C in [19]: Proportions of vesicle motile behaviour in spatial bands of radial width 0.5  $\mu\text{m}$ . (D) Data in Fig 2C from [19] averaged within the three spatial compartments. (E) Figure 1E in [19]: Percentages of secretory vesicles in each motile state in control and stimulation.

Moreover, determining the transition rates within spatial bands of radial width 0.5  $\mu\text{m}$  revealed three functionally distinct ring-shaped spatial compartments (visualised in Figure 1): the *peripheral* (0.5-1.5  $\mu\text{m}$  distance from cell membrane), *subcortical* (1.5-2.5  $\mu\text{m}$ ) and *central* (2.5 - 5.0  $\mu\text{m}$ ). Note that when determining the average transition rates for these compartments we omit the outermost radial band right at the cortex which is mostly populated by caged vesicles. Fig 3 provides the transition rates reported in Fig.3J-R in [19] (per 2 minutes) converted to numerical values per 1 minute as well as a sketch of the underlying 3-motile-states model.



**Fig 3. (A) Experimentally observed transition rates.** Table of transition rates reported in [19]. **(B)** Graphical sketch of 3-state Markov chain model ( $C_i$ (aged),  $D_i$ (irected),  $F_i$ (ree)) for single spatial compartments  $i = 1, 2, 3$ .

They provide at least speculative insight into the underlying architecture of the intracellular transport network: The higher free-to-directed transition rate in the subcortical compartment suggests the presence of a higher density of cytoskeleton fibres in this region. Another observation is that the free-to-caged transition rate is significantly elevated in the peripheral region which might reflect a relatively higher density of the peripheral actin meshwork [31]. The higher caged-to-directed transition rate in the subcortical compartment as compared to the practically identical rates in the central and peripheral ones suggests that the microtubules and actin meshwork are both dense in this compartment or that they achieve significant overlap.

The directed-to-free transition rates are relatively higher in the central and peripheral compartments in comparison to the subcortical rate. We hypothesise that this is due to the higher number of microtubules terminating within these regions by which the faster off-rates there might also reflect the detachment of vesicles after reaching the "end of the track". Another interesting observation from Fig 3 is that the caged-to-free transition rate is relatively higher in the central compartment, whereas free-to-caged rate is the lowest in the central compartment. This might be evidence that recently synthesised vesicles might enter the transport network as initially caged vesicles which is supported by the literature [32].

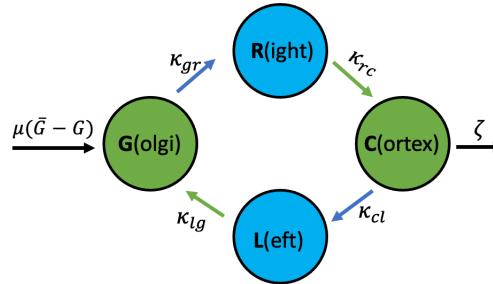
## Materials and methods

Our goal is to develop a Markov state model based on the transition rates listed in Fig 3. In [19] these have been published for stimulated cells, but not for control cells. We will therefore assume that the transition rates listed in Fig 3 in principle are valid irrespective of stimulation vs non-stimulation. Note that in the context of our model, this implies that stimulation does not structurally alter the characteristics of how secretory vesicles behave in the cytoplasm, and especially interact with the cytoskeleton.

We will show that such a model is able to explain the key experimental observations listed above. Spatial inhomogeneity of the cytoskeleton, specifically the non-uniform spatial distribution of outward vs inwards directed vesicle transport, coupled with the spatial redistribution of vesicles upon stimulation, will trigger up-regulation of outward transport and of overall transport as listed above. We refer to this mechanism as the "acceleration through spatial redistribution" hypothesis. We will start by introducing a minimal ("toy") model in order to provide an intuitive initial illustration of the mechanism.

## Minimal 4-state model

The following 4-state continuous time Markov chain visualised in Fig 4 provides a proof of concept for the "acceleration through spatial redistribution" hypothesis.



**Fig 4. Graphical sketch of the minimal 4-state model.**

In this simple model vesicles exist in one of four states, respectively spatial compartments: They are generated at the Golgi apparatus (G), from where they might engage in outward – visualised as right-directed – transport (R) towards the cell cortex (C). Vesicles at the cortex engage in in-ward – shown as left-directed (L) – transport and ultimately arrive back at the Golgi. Alternatively, vesicle at the cortex may enter the pathway towards exocytosis with rate  $\zeta$ . This pathway acts as a sink whereas the cell's synthesis of vesicles near the Golgi represents a source of new secretory vesicles. We assume that vesicle synthesis is regulated by feedback mechanisms which aim at maintaining a given number of  $\bar{G}$  vesicles at the Golgi apparatus.

This gives rise to the system of rate equations

$$\begin{aligned}\dot{G}(t) &= \mu(\bar{G} - G) - \kappa_{gr} G(t) + \kappa_{lg} L(t), \\ \dot{C}(t) &= \kappa_{rc} R(t) - \kappa_{cl} C(t) - \zeta C(t), \\ \dot{R}(t) &= \kappa_{gr} G(t) - \kappa_{rc} R(t), \\ \dot{L}(t) &= \kappa_{cl} C(t) - \kappa_{lg} L(t).\end{aligned}\tag{1}$$

In order to verify the up-regulation through spatial redistribution hypothesis, we take  $\zeta$  as zero in a control cell and assume that stimulated cells are characterised by  $\zeta > 0$ . In our assessment we only consider the steady state solution (for details see supplementary section S1 Steady state solution of the minimal 4-state model) where  $\mu$  is large, i.e. where  $G = \bar{G}$  and

$$C = \frac{\kappa_{gr}}{\zeta + \kappa_{cl}} G, \quad R = \frac{\kappa_{gr}}{\kappa_{rc}} G, \quad L = \frac{\kappa_{gr} \kappa_{cl}}{\kappa_{lg} (\zeta + \kappa_{cl})} G.\tag{2}$$

In the context of this minimal model up-regulation of outward transport is characterised by how  $\frac{R}{L}$  depends on  $\zeta$ , namely

$$\frac{R}{L} = \frac{\kappa_{lg}}{\kappa_{rc}} \left( 1 + \frac{\zeta}{\kappa_{cl}} \right),\tag{3}$$

which increases monotonically as a function of  $\zeta$  since all transition rates are positive. This shows that the minimal model predicts a bias towards outward transport in response to stimulation. Note that the decrease of the number of vesicles in  $L$  is triggered by a preceding decrease in the compartment  $C$  (see (2)). In this sense the observed up-regulation is a consequence of the adjustment of the spatial distribution upon stimulation.

Note that to mimic a ratio of  $R : L \sim 1$  which is observed in control cells ( $\zeta$  small) the rates  $\kappa_{lg}$  and  $\kappa_{rc}$ , which both represent off-rates from vesicle transport, are required to be approximately equal as a consequence of (3).

Up-regulation of directed transport upon stimulation, on the other hand, is characterised by the ratio  $\frac{R+L}{G+C}$ , which – at steady state – is given by

$$\frac{R+L}{G+C} = \frac{\kappa_{gr}}{\kappa_{rc}} \left( 1 + \frac{1}{\kappa_{lg}} \frac{\alpha\gamma - \beta\nu}{\alpha + \zeta} \right), \quad (4)$$

where  $\nu = \kappa_{gr} - \kappa_{cl}$ ,  $\beta = \frac{1}{2}(\kappa_{rc} + \kappa_{lg})$ ,  $\alpha = \kappa_{gr} + \kappa_{cl}$ ,  $\gamma = \frac{1}{2}(\kappa_{rc} - \kappa_{lg})$ . Note that  $\alpha$  and  $\beta$  are both positive. Therefore, the minimal model predicts up-regulation of directed transport only if  $\nu > 0$  and/or  $\gamma < 0$ . The fact that we need  $\kappa_{rc} \sim \kappa_{lg}$  for an 1:1 ratio of right and left moving vesicles in control suggests  $\gamma \sim 0$  and therefore we require  $\nu > 0$ .

Interpreting the on-rates  $\kappa_{gr}$  and  $\kappa_{cl}$  as representatives of effective fibre densities – the more cytoskeleton fibres and motor proteins moving in the right direction are available, the larger the respective on-rates – the result that  $\nu > 0$  indicates that there should be a higher net density of fibres triggering outward transport as compared to fibres resulting in transport away from the cortex. It is worth noticing that small  $\kappa_{cl}$  favours both, up-regulation of directed transport in (4) and a strong bias towards outward transport ( $R/L$ , see (3)) upon stimulation.

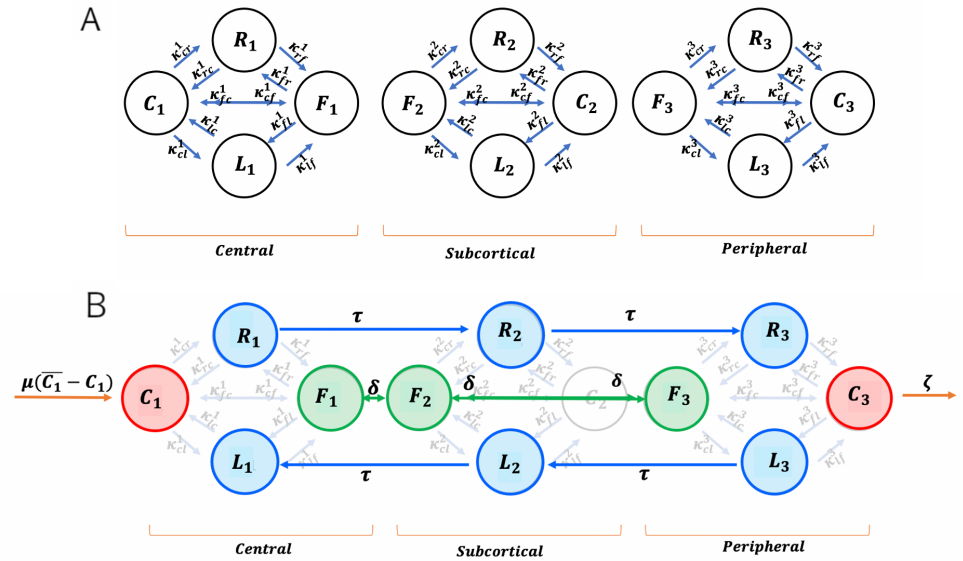
Finally, it is important to note that there is an inherent asymmetry in this minimal model. Specifically, only transitions from the spatially interior state G to right directed motion are considered and not vice versa. Similarly, we only consider transitions from the spatially outward state C to left directed motion and not vice versa. This restriction makes sense for a simplified model thought to be coarse-graining a more intricate underlying system. In the following development of the full Markov state model we consider three spatial compartments with bi-directional transitions modelling vesicle attachment and detachment from cytoskeleton fibres and molecular motors. The asymmetry of the minimal model will be replaced by transitions between spatial compartments modelling directed transport.

## Markov state model

Our goal is to formulate a mathematical model which explains the key experimental observations reported in [19]. To this end we refine the minimal model visualised in figure 4 by adding spatial compartments building on the measured rates listed in Fig 3.

We represent the spatial distribution of vesicles by assigning them to one of the three compartments *central* ( $i=1$ ), *subcortical* ( $i=2$ ) and *peripheral* ( $i=3$ ), which mimics the terminology used in [19].

In each spatial compartment vesicles are either in state  $F_i$  (diffusing *freely* in the cytoplasm),  $C_i$  (*caged*, i.e. undergoing random, though spatially restricted motion) or undergoing directed motion in state  $R_i$  (towards the cell periphery usually visualised on the *right*) or  $L_i$  (towards the cell centre usually visualised on the *left*).



**Fig 5. Visualisation of Markov states with intra-compartmental transitions (A) and inter-compartmental transitions (B).**

Figure 5A provides a visualisation of the transitions occurring within the individual spatial compartments of the model. Note that the experimental study only provides information about the rates by which either free or caged vesicles engage in directed transport, but not about the direction of transport (Fig 3).

For this reason we introduce the structural parameter  $0 \leq \rho_i \leq 1$  for each of the three spatial compartments  $i = 1, 2, 3$ . The role of this parameter is to determine how the experimentally recorded on-rates into directed transport  $\kappa_{fd}^i$  and  $\kappa_{cd}^i$  from figure 3 distribute into outward (right) and inward (left) transport. Using the structural parameters we write the transition rates from the free and caged states into either left or right transport shown in Fig 5A as

$$\begin{aligned} \bar{\kappa}_{fr}^i &= \rho_i \kappa_{fd}^i, & \bar{\kappa}_{cr}^i &= \rho_i \kappa_{cd}^i, \\ \bar{\kappa}_{fl}^i &= (1 - \rho_i) \kappa_{fd}^i, & \bar{\kappa}_{cl}^i &= (1 - \rho_i) \kappa_{cd}^i. \end{aligned} \quad (5)$$

Here we use the overbar notation to indicate that these rates will be further modified below. One way of interpreting the factors  $\rho_i$  is as the fraction of fibres within one of the spatial compartments along which vesicles will be transported outwards vs inwards. This implies that  $\rho_i$  does not reflect the concentration of fibres within the respective spatial compartment. Instead the rates  $\kappa_{fd}^i$  are likely to reflect the net fibre densities in any given compartment.

Similar considerations for off-rates are not necessary, so we assume that

$$\kappa_{rf}^i = \kappa_{lf}^i = \kappa_{df}^i \quad \text{and} \quad \kappa_{rc}^i = \kappa_{lc}^i = \kappa_{dc}^i \quad (6)$$

for all three spatial compartments  $i = 1, 2, 3$ , i.e. the experimentally observed off-rates from directed transport reported in figure 3 taken from [19] are used irrespective of the direction of transport.

In order to connect the so-far isolated spatial compartments sketched in Fig 5A, we introduce additional transitions accounting for the random and directed motion of vesicles. The mean square displacement per time of free vesicle trajectories in 3D has been determined in [19] (Fig S1) as  $0.75 \mu\text{m}^2/\text{min}$ . Assuming an average distance of  $1.7 \mu\text{m}$  between our three, linearly aligned, spatial compartments this suggests a



inter-compartment transition rate of  $\delta = (0.75/6)/1.7^2 \text{ min}^{-1} \approx 0.04 \text{ min}^{-1}$  to account for random motion of free vesicles. The corresponding transitions between the states of free vesicles in neighbouring compartments are visualised in Fig 5B as bidirectional arrows.

We also include uni-directional transitions between the directed states in order to represent directed transport of secretory vesicles. In Fig 5B these are shown as blue arrows. Instantaneous maximal vesicle speeds of up to  $0.05 \mu\text{m s}^{-1}$  have been reported in [19]. This would suggest transition rates of  $0.05 \times 60/1.7 \approx 1.8 \text{ min}^{-1}$ . In steady state solutions of the Markov state model, however, these fast transition rates would result in vesicles pooling at the states  $R_3$  and  $L_1$  which is not supported by observations [19]. Instead, we assume that vesicles achieve maximal speeds only intermittently and estimate the transition rate of vesicles undergoing directed transport as  $\tau = 0.15 \text{ min}^{-1}$ .

Description	Symbol	Value	Reference
Inter-compartmental transition of free vesicles	$\delta$	$0.04 \text{ min}^{-1}$	Figure S1 in [19].
Transition into exocytosis pathway (control)	$\zeta_{\text{ctr}}$	$0.0 \text{ min}^{-1}$	Estimated
Transition into exocytosis pathway (stimulated cells)	$\zeta_{\text{stim}}$	$0.15 \text{ min}^{-1}$	Estimated
Directed spatial transition	$\tau$	$0.15 \text{ min}^{-1}$	Estimated
Outward vs inward transport	$\rho_1, \rho_2, \rho_3$	0.75, 0.6, 0.4	Estimated (see supplementary section Fitting of structural parameters)
Repression (crowding) coefficients	$\hat{R}_i, \hat{L}_i$ ( $i = 1, 2, 3$ )	0.2	Estimated

**Table 1. Parameter values**

Additional transitions embed the Markov State model (visualised in Fig 5B within the life-cycle of secretory vesicles. We model vesicle synthesis as an in-flux of vesicles into  $C_1$  (the caged pool close to the Golgi apparatus) with rate  $\mu(\bar{C}_1 - C_1)$ . At steady state this term effectively imposes the constant value  $\bar{C}_1$  on the number of vesicles in  $C_1$ , so for our purposes  $\mu$  is an arbitrary large value which has no effect on the steady state solutions and  $\bar{C}_1$  is an arbitrary constant which factors out of the steady state solution after we normalise either by the total number of vesicles in the system or in the respective spatial compartment. Having vesicles enter the system through the caged node  $C_1$  as opposed to the central node of free vesicles  $F_1$  reflects our hypothesis (supported by [32]) that vesicles travel through an actin meshwork adjacent to the Golgi upon entering the system.

Finally, as in the minimal 4 state model, we model the onset of the pathway through which vesicles undergo exocytosis by an outgoing-transition (rate) from the pool of caged vesicles in compartment  $i = 3$  (peripheral) denoted by  $\zeta$ . This reflects the role the actin cortex plays in the exocytosis pathway [31]. With these parameter values, especially with the estimated values for  $\tau$  and  $\zeta$  steady state simulations of stimulated cells exhibit relative shares of vesicles (free, caged and undergoing directed motion) Fig 7A which coincide well with measured values from [19] visualised in Fig 2C and D. Note that the full system of rate equations corresponding to the Markov chain shown in

Fig 5 is shown in supplementary section S2 Governing Equations. 275

## Fitting of structural parameters 276

We determine the structural parameters  $\rho_1$ ,  $\rho_2$  and  $\rho_3$  (see Table 1) by fitting (least-squares) the predicted ratios of right vs left moving vesicles denoted by  $\Phi_\zeta$  and the predicted ratio of directed motion vs random motion denoted by  $\Psi_\zeta$ . These quantities are given by

$$\Phi_\zeta = \frac{\sum_{i=1}^3 (R_i^\zeta + L_i^\zeta)}{\sum_{i=1}^3 (F_i^\zeta + C_i^\zeta)} \quad \text{and} \quad \Psi_\zeta = \frac{\sum_{i=1}^3 R_i^\zeta}{\sum_{i=1}^3 L_i^\zeta},$$

where  $i$  is the spatial compartment index and  $R_i^\zeta$ ,  $L_i^\zeta$ ,  $F_i^\zeta$  and  $C_i^\zeta$  are the steady state abundances for a given exocytosis rate  $\zeta$ . 277

We take into account the deviations of those quantities from the observed ones for both, stimulated cells and control cells. The error functional which we minimise is therefore given by 278  
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$$\mathcal{E} = (\Phi_{\zeta_{\text{stim}}} - \Phi_{\text{stim}}^{\text{obs}})^2 + (\Phi_{\zeta_{\text{ctr}}} - \Phi_{\text{ctr}}^{\text{obs}})^2 + (\Psi_{\zeta_{\text{stim}}} - \Psi_{\text{stim}}^{\text{obs}})^2 + (\Psi_{\zeta_{\text{ctr}}} - \Psi_{\text{ctr}}^{\text{obs}})^2, \quad (7)$$

where the experimentally observed values are given by  $\Phi_{\text{ctr}}^{\text{obs}} = 0.38/0.62 \approx 0.6$ , 282  
 $\Phi_{\text{stimu}}^{\text{obs}} = 0.52/0.48 \approx 1.1$  (see Fig 2E) as well as  $\Psi_{\text{ctr}}^{\text{obs}} = 1.0$ ,  $\Psi_{\text{stimu}}^{\text{obs}} = 2.0$ . 283

## Modelling of carrying capacities 284

Steady state simulation results with the constant transition rates (5), however, are not consistent with the threefold increase in the average free-to-directed transition rate observed upon stimulation (Fig 2A). Spatial redistribution alone cannot account for this since the slowest - among all spatial compartments - reported transition rate  $\kappa_{fd}^i$  in stimulation is  $0.2 \text{ min}^{-1}$  (Fig 3), whereas the average rate reported in control is  $0.1 \text{ min}^{-1}$  (Fig 2A, which reports rates *per 2 min*). 285  
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We hypothesise that the observed increase in the average free-to-directed transition rate upon stimulation is a consequence of the global decrease in vesicle abundance occurring at stimulation. We therefore suggest that in control transitions are slowed down by crowding of vesicles undergoing directed transport. 291  
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We use Hill functions (for a repressor [33]) to model the limiting effect of carrying capacities on all other transition rates into directed transport by the following correction factors 295  
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$$\alpha_i(R_i) = \frac{1}{1 + \frac{(R_i - R_i^{\zeta_{\text{stim}}})_+}{\hat{R}_i}} \quad \text{and} \quad \beta_i(L_i) = \frac{1}{1 + \frac{(L_i - L_i^{\zeta_{\text{stim}}})_+}{\hat{L}_i}} \quad \text{for } i = 1, 2, 3. \quad (8)$$

The Hill functions are parametrised by the repression coefficients  $\hat{R}_i$  and  $\hat{L}_i$  ( $i = 1, 2, 3$ ). To ensure that this modification does not alter the steady state population sizes in stimulation,  $R_i^{\zeta_{\text{stim}}}$  and  $L_i^{\zeta_{\text{stim}}}$ , we include these values in the correction factors (8) taking only the positive part of  $R_i - R_i^{\zeta_{\text{stim}}}$  and  $L_i - L_i^{\zeta_{\text{stim}}}$ , respectively. 298  
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It obviously appears problematic to include steady state abundances in stimulation in the correction factors. To remove these dependencies one might rewrite the correction factors as a classical Hill function with two constants, namely  $\alpha_i(R_i) = \mu_i / (1 + R_i / \nu_i)$  (for  $R_i > R_i^{\zeta_{\text{stim}}}$ ) and analogous expressions for  $\beta_i$ . Nevertheless, such rewriting of the correction is not required to run the simulations and it would render our choice of parameters less transparent. We therefore keep the notation used in (8). 302  
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Note that applying the correction factors (8) to the transition rates (5) would also slow down transitions from the pool of caged vesicles into transport states. Reported transition rates from caged into directed motion (averaged among spatial compartments), however, only exhibit minor variation between control and stimulation (Fig 2A). We argue that for caged vesicles the speed-up in response to less crowding along transport fibres upon stimulation might be compensated by faster turnover of the actomyosin cortex upon stimulation [31] which could prevent a large fraction of caged vesicles from binding to fibre-motor-protein complexes.

As a consequence we keep the peripheral caged-to-directed transition rates unmodified, while rescaling all rates listed in (5) as follows

$$\begin{aligned} \kappa_{fr}^1 &= \bar{\kappa}_{fr}^1 \alpha_1, & \kappa_{fl}^1 &= \bar{\kappa}_{fl}^1 \beta_1, & \kappa_{cr}^1 &= \bar{\kappa}_{cr}^1 \alpha_1, & \kappa_{cl}^1 &= \bar{\kappa}_{cl}^1 \beta_1, \\ \kappa_{fr}^2 &= \bar{\kappa}_{fr}^2 \alpha_2, & \kappa_{fl}^2 &= \bar{\kappa}_{fl}^2 \beta_2, & \kappa_{cr}^2 &= \bar{\kappa}_{cr}^2 \alpha_2, & \kappa_{cl}^2 &= \bar{\kappa}_{cl}^2 \beta_2, \\ \kappa_{fr}^3 &= \bar{\kappa}_{fr}^3 \alpha_3, & \kappa_{fl}^3 &= \bar{\kappa}_{fl}^3 \beta_3, & \kappa_{cr}^3 &= \bar{\kappa}_{cr}^3, & \kappa_{cl}^3 &= \bar{\kappa}_{cl}^3. \end{aligned} \quad (9)$$

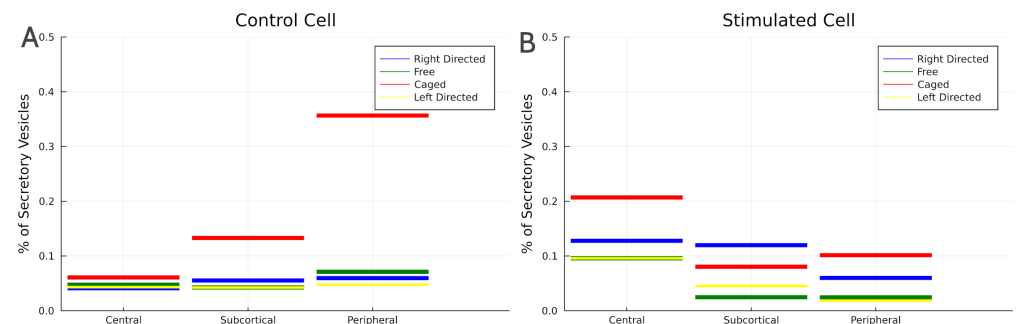
In the absence of more detailed data, and since we only seek to provide a preliminary proof of concept for the idea that crowding can explain the 3-fold speed-up of transitions from free to directed (Fig 2A) we choose a single constant for the repression coefficients (see Table 1).

Also note that to keep the fitting procedure simple we do not reassess the structural parameters  $\rho_i$ ,  $i = 1, 2, 3$  with the modified transition rates. Indeed they only have a minor effect on the capacity of the model to correctly predict up-regulation of outward and total transport as shown below in section Spatial redistribution can explain both, up-regulation of directed transport and bias towards the plasma membrane.

## Results

### Stimulated exocytosis triggers spatial rearrangement of chromaffin vesicles.

We numerically compute the steady state solutions of the Markov state model visualised in Fig 5 with the rates (9) and (6).

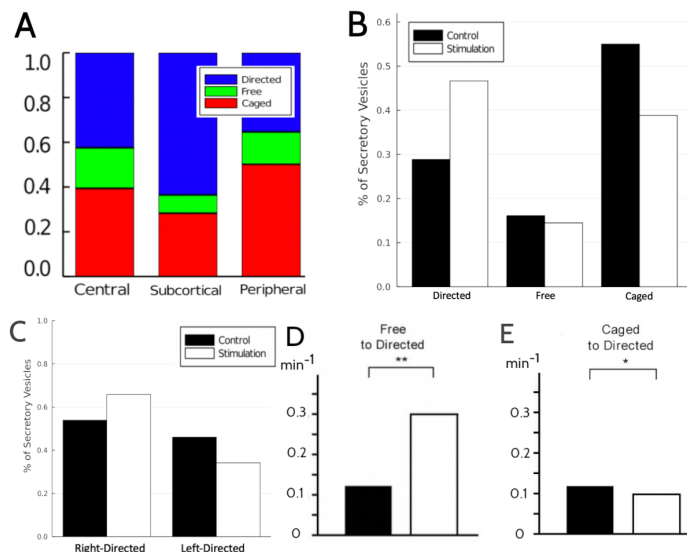


**Fig 6.** Simulated steady state probability distributions of vesicles in control (A) and upon stimulation (B), both normalised so they admit a probabilistic interpretation.

In simulated control cells, the steady state distribution of vesicles (Fig 6A) is characterised by a large portion of vesicles (of about 38%) being pooled in the caged state at the cortex. In the corresponding steady state distribution for a stimulated cell (Fig 6), this pool of vesicles ready to enter the pathway leading to exocytosis is largely reduced. This results in caged vesicles being distributed more evenly between the three spatial compartments upon stimulation with most of them now being located in the

central region of the cell. All together this accounts for a significant shift in the spatial distribution of vesicles from the cell periphery to the cell centre as a consequence of the permanent out-flux of vesicles at the cortex in response to secretagogue stimulation.

From the results of Fig 6 we extract the intra-compartmental proportions for a stimulated cell which are visualised in Fig 7A and qualitatively agree with the experimentally recorded intra-compartmental proportions shown Fig 2C and D.



**Fig 7.** Steady state simulation results: **A** Percentages of secretory vesicles in each motile state (stimulation). **B** Percentages of secretory vesicles in each directed (right vs left). **C** Intra-compartmental proportions in stimulated cells. **D** Aggregated transition rates from free to directed motion. **E** Aggregated transition rates from caged to directed motion.

## Spatial redistribution can explain both, up-regulation of directed transport and bias towards the plasma membrane

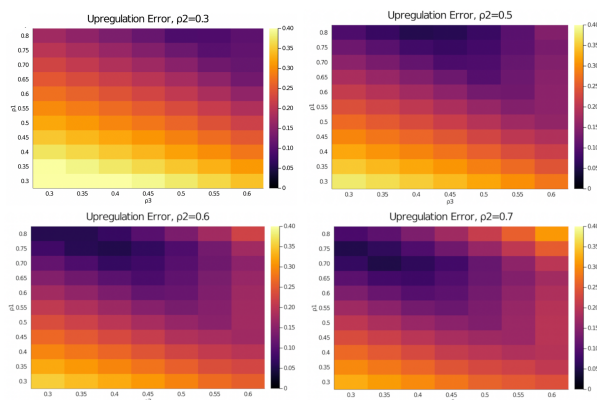
Our model predicts an increase from 29% to 47% in the share of vesicles undergoing directed transport in stimulated cells vs control (Fig 7B). This compares well with the experimental data reproduced in Fig 2E. Likewise the rate of outward moving vesicles vs. inward moving vesicles increases from about 1:1 in control to about 2:1 in stimulated cells (Fig 7C) which also coincides with the data reported in [19].

The vesicle distributions in Fig 6 reveal that upon stimulation the relative abundance of vesicles moving outwards (blue) increases in the central and subcortical compartment. On the other hand the relative abundance of vesicles moving inwards (yellow) decreases in the peripheral compartment, though to a lesser extent. Both effects contribute to the up-regulation of total and outward directed transport. They are both triggered by spatial redistribution of vesicles upon stimulation since the states in which most of the redistribution takes place are those which precede states of direct motion: from  $C_1$  and  $F_1$  vesicles transition into  $R_1$  – and later  $R_2$  and  $R_3$ , from  $C_3$  they transition into  $L_3$  – and later back into  $L_2$  and  $L_1$ .

This mechanism is overshadowed by the dense network of potential transitions in the Markov State model Fig 5 and so it is easier to understand it in the context of the minimal model Fig 4. This simpler model also features redistribution of non-moving vesicles upon stimulation, namely through the number of vesicles in state C(ortex) which decreases upon stimulation ( $\zeta$  large) according to Eq (2). As a consequence, upon

stimulation the number of vesicles in the state L(ef) also decreases, since C is the only state from which vesicles transition into L. This readily explains the increase of the ratio R:L under stimulation (see Eq (3)) in the minimal model. It also indicates that in the full Markov state model the mechanism which drives the increase of the ratio of outward vs inward transport upon stimulation is the redistribution of caged and free vesicles upon stimulation.

The mechanism which drives the up-regulation of the total share of vesicles undergoing directed transport is more obscure. For the minimal model we have concluded that up-regulation of total directed transport requires  $\nu = \kappa_{gr} - \kappa_{cl} > 0$  in Eq (4) (or alternatively  $\gamma < 0$  which we ruled out assuming that  $2\gamma = \kappa_{rc} - \kappa_{lg} = 0$ ). In other words, the rate by which vesicles enter the state representing transport to the R(ight) should be faster than the corresponding rate by which vesicles enter the state L(ef). Again the underlying mechanism is triggered by the redistribution of non-moving cells upon stimulation which decreases the number of vesicles in C(ortex). If the rates,  $\kappa_{gr}$  and  $\kappa_{cl}$ , were equal (i.e.  $\nu = 0$ ), then the ratio of L:C (Eq 12) and R:G (Eq 11) would be same before and after stimulation prohibiting upregulation of total transport represented by  $(R + L)/(G + C)$  (Eq (4)). However, with the rate to enter L being smaller than the one to enter R, the decrease in C has a relatively smaller effect on R+L than on G+C and the share of vesicles undergoing directed transport increases.



**Fig 8.** Heatmap plots of the predictive error (7) with respect to up-regulation of total and right vs left transport for different values of the structural parameters  $\rho_1$ ,  $\rho_2$  and  $\rho_3$ .

### Outward directed structural bias of the central transport network promotes overall up-regulation of directed transport upon stimulation.

Least squares fitting of the three structural parameters  $\rho_1$ ,  $\rho_2$  and  $\rho_3$  (Fig 8) by minimising the error functional (7) shows that in order for the model to correctly predict the observed up-regulation of both, outward and total directed transport, the structural parameters  $\rho_1$  and/or  $\rho_2$  are required to have an outward bias ( $> 0.6$ ). This observation is reminiscent of the requirement that  $\kappa_{gr} > \kappa_{cl}$  in the minimal model. It indicates that in the central and sup-peripheral part of the cell the vesicles' propensity to engage in outward directed transport is higher than to engage in in-ward transport. Note that these parameters are phenomenological, they do not indicate whether this effect is caused by the density of outward-transport fibres in the central and subcortical regions being relatively higher than the density of inward-transport fibres, or – alternatively – by faster rates of attachment to outward directed fibre-motor combinations.

What we conclude is that a cytoskeleton with a bias towards outward transport in the central and subcortical regions will trigger an up-regulation of total and outward vesicle transport in response to their spatial redistribution at stimulation.

## Crowding limits entry into the vesicular transport network towards the plasma membrane

We modelled crowding of cytoskeleton fibres through Hill-functions (8) in the on-rates (9) since a straightforward Markov state model with constant transition rates according to (5) would not be consistent with the reported 3-fold acceleration of transitions of free vesicles into directed motion [19] (reprinted in Fig 2A) upon stimulation.

We fit a single, spatially uniform, repressor coefficient (Table 1) in a way such that - at steady state - the average free-to-directed transition rate is  $0.126 \text{ min}^{-1}$  in control ( $0.29 \text{ min}^{-1}$  in stimulation) as compared to  $0.27 \text{ min}^{-1}$  (control) ( $0.3 \text{ min}^{-1}$  in stimulation) for the model with constant transition rates. The model with non-linear transition rates modelling crowding therefore allows to reproduce the 3-fold speed-up of transitions from free into directed motion (Fig 7D) observed experimentally (Fig 2A).

In agreement with the available data (Fig 2B) it predicts that the overall rate of transitions from caged behavior into direction motion does not increase upon stimulation (see Fig 7E). Note that this was only possible through the assumption that crowding doesn't affect the transitions from caged vesicles in the periphery into directed (see (9)) motion which we believe could reflect the specific structure of the rapidly turning over actomyosin cortex in stimulated cells.

The correction factors with the uniform repressor coefficients listed in Table 1 are close to one in the central compartment, indicating that crowding in control is stronger in the periphery of the cell. (the exact correction factors are visualised in supplementary figure 10). Arguably our choice of the repressor coefficients is simplistic since we lack sufficient data to perform more detailed parameter fitting. It is also for this reason that we don't perform a detailed sensitivity analysis of the repressor coefficients. Indeed variations in the choice of the repressor coefficients change the magnitude of the correction factors, the only robust feature being that the correction factors are closer to one in the cell centre, whereas crowding is stronger in the periphery. The reason is that most variation of vesicle abundance between control and stimulation is in the periphery of the cell. In the cell centre, however, the model assumes the presence of feedback mechanisms which regulate vesicle synthesis in a way such that vesicle abundance in the cell centre hardly varies between control and stimulation.

## Discussion

In this study we formulate a Markov transition state model which is closely aligned to the data obtained from tracking secretory vesicles in chromaffin cells reported in [19].

We model the asymmetry of directed transport due to the topological constraints of the intracellular space: directed transport originating in the central compartment is biased towards the cell periphery, transport of vesicles originating in the peripheral compartment is towards the cell centre. In the Markov state model Fig 5B this is implemented by the central compartment having only a single transport transition ( $R_1 \rightarrow R_2$ ) directed towards the periphery, and by the peripheral compartment having only one transport transition  $L_3 \rightarrow L_2$  directed towards the cell centre.

Steady state simulations of control and stimulated cells show that secretagogue stimulation shifts the spatial distribution of secretory vesicles from the cell periphery towards the central region of the cell. The spatial redistribution upon stimulation leads

to a significant increase of the overall share of vesicles undergoing outward transport. This agrees with observations [19] and with an earlier modelling study [29].

In addition our study suggests that the spatial redistribution also triggers the up-regulation of overall directed transport, i.e. irrespective of direction, observed in [19]. The mechanism relies on the (on-)rates by which vesicles enter the states representing outward transport being faster than the corresponding (on-)rates by which vesicles enter the states associated to inward transport. (Alternatively the (off-)rates by which vesicles leave the states representing outward transport could also be slower than the corresponding rates by which vesicles leave the inward transport states). In this study we illustrate this mechanism using the minimal model visualised in Fig 4.

For the full Markov state model Fig 5 parameter fitting shows that the required asymmetry originates from the central (and - to a lesser extent - the subcortical) compartment having a bias towards outward transport ( $\rho_1 = 0.75 > 0.5$ , see Table 1). This indicates that the up-regulation at stimulation is an in-built property of the cell's cytoskeleton architecture – fibre-motor assemblies in the central region of the cell having a bias towards outward transport – and not necessarily triggered by molecular feedback mechanisms.

Under the additional modelling assumption that the capacity of the cytoskeleton fibres serving as transport tracks is limited in control through crowding, our model also explains the observed accelerated recruitment of free vesicles (vesicles undergoing unconstrained random walks) into directed transport. In which spatial compartment, however, crowding is effective, is difficult to determine based on the published data. The only conclusion we draw is that crowding has a significantly stronger effect in the periphery of the cell as compared to the cell centre, since the steady state distribution of vesicles in control is predominantly characterised by an accumulation of vesicles in the periphery of the cell (see steady state distributions in absolute numbers shown in supplementary Fig 9).

## Conclusion

In this study we show that a mathematical model based on experimentally observed transition rates [19] between motile states of secretory vesicles in chromaffin cells predicts a spatial redistribution of vesicles and up-regulation of outward transport in response to secretagogue stimulation.

We show that this spatial redistribution combined with spatial inhomogeneity of the cellular transport network – a bias towards outward transport in the central region of the cell – explains that upon stimulation a relatively larger share of vesicles undergoes directed transport in agreement with experimental data. This indicates that the up-regulation at stimulation is an in-built property of the cell's cytoskeleton architecture, and not necessarily triggered by molecular feedback mechanisms.

We also show that crowding of vesicle transport in control, i.e. in non-stimulated cells, is sufficient to explain that the rate by which free vesicles engage in directed transport is three-fold accelerated in stimulated cells [19].

The mathematical model makes a series of testable predictions. While it does not appear feasible to alternate the structure of the cytoskeleton in a way which changes the directional bias of the transport network, manipulation of either plus end or minus end directed molecular motors involved in vesicle transport could have a similar effect. Our model predicts that if the cellular transport network has an inward bias, then the fraction of vesicles undergoing directed transport will be reduced in stimulated cells.

What could be simpler is to limit the rate by which vesicles in stimulated cells progress through the cortical actomyosin network to the site of exocytosis, e.g. through cytoskeleton drugs or genetic manipulation. In this case the Markov state model

predicts that the spatial redistribution is reduced and that the up-regulation of both total and outward transport will be limited.

Finally our model also predicts that chromaffin cells with a reduced rate of secretory vesicle biosynthesis will be less affected by crowding in the absence of secretagogue stimulation because of a lower overall vesicle population. Therefore such non-stimulated cells should exhibit the same fast vesicle transition rates from free motion into directed motion as stimulated cells.

One limitation of this study is that it does not consider the details of the pathway by which the actomyosin cortex recruits secretory vesicles and supports their progress towards the active sites. Future research will address this question. Indeed not much is known about the regulation mechanisms that couple cytoplasmic transport of chromaffin vesicles and the regulation of exocytosis through the actin cytoskeleton [11,18]. We believe that dynamic solutions of mathematical models such as the one introduced in this study have the potential to give insight into those regulation mechanisms, especially when combined with data on vesicle release statistics. Further, they will provide insights for futures studies on other trafficking events including that of autophagosomes [34] and synaptic vesicles in neurons [35].

## Supporting information

### S1 Steady state solution of the minimal 4-state model.

The steady state solution of the system (1) satisfies the following equations,

$$G = \frac{\mu \bar{G}}{\kappa_{gr} + \mu} + \frac{\kappa_{lg}}{\kappa_{gr} + \mu} L, \quad (10)$$

$$R = \frac{\kappa_{gr}}{\kappa_{rc}} G, \quad (11)$$

$$L = \frac{\kappa_{cl}}{\kappa_{lg}} C, \quad (12)$$

$$C = \frac{\kappa_{rc}}{\kappa_{cl} + \zeta} R. \quad (13)$$

We can now express C and L in terms of G as follows,

$$C = \frac{\kappa_{gr}}{\kappa_{cl} + \zeta} G, \quad (14)$$

$$L = \frac{\kappa_{gr} \kappa_{cl}}{\kappa_{lg} (\kappa_{cl} + \zeta)} G. \quad (15)$$

Now we can combine (10), (15) to get the steady state solution for G in terms of  $\bar{G}$ ,

$$G = \bar{G} \frac{1}{1 + \frac{\kappa_{gr}}{\mu} \cdot \frac{1}{1 + \frac{\kappa_{cl}}{\zeta}}}.$$

This is the steady state for the population size in state G. As mentioned in section Minimal 4-state model it converges to  $\bar{G}$  in the limit when the rate  $\mu$  is large. This complements the steady state abundances (11),(14) and (15).

### S2 Governing Equations.

We provide below the full system of coupled differential equations describing the Markov state model visualised in Figures (5)A and (5)B above using the modified rates

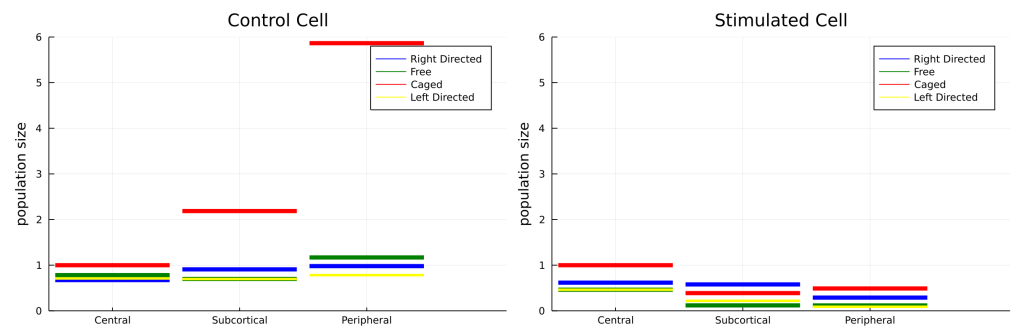


from section Modelling of carrying capacities.

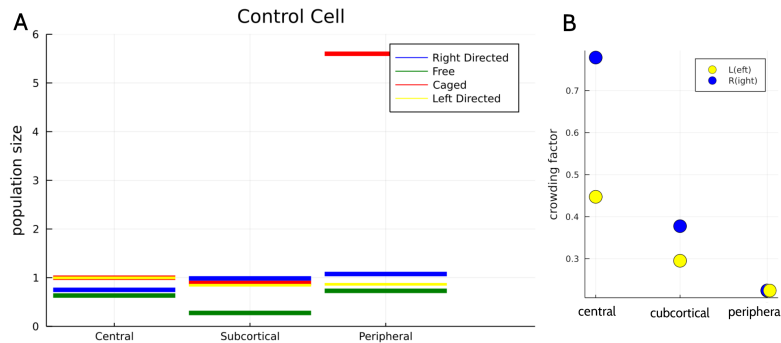
$$\begin{aligned}
 \dot{R}_1(t) &= \kappa_{fr}^1 F_1 + \kappa_{cr}^1 C_1 - (\tau + \kappa_{rf}^1 + \kappa_{dc}^1) R_1 \\
 \dot{R}_2(t) &= \kappa_{fr}^2 F_2 + \kappa_{cr}^2 C_2 + \tau R_1 - (\tau + \kappa_{rf}^2 + \kappa_{dc}^2) R_2 \\
 \dot{R}_3(t) &= \kappa_{fr}^3 F_3 + \kappa_{cr}^3 C_3 + \tau R_2 - (\kappa_{rf}^3 + \kappa_{dc}^3) R_3 \\
 \dot{C}_1(t) &= \kappa_{fc}^1 F_1 + \kappa_{dc}^1 (R_1 + L_1) - (\kappa_{cf}^1 + \kappa_{cd}^1) C_1 \\
 \dot{C}_2(t) &= \kappa_{fc}^2 F_2 + \kappa_{dc}^2 (R_2 + L_2) - (\kappa_{cf}^2 + \kappa_{cd}^2) C_2 \\
 \dot{C}_3(t) &= \kappa_{fc}^3 F_3 + \kappa_{dc}^3 (R_3 + L_3) - (\kappa_{cf}^3 + \kappa_{cd}^3 + \zeta) C_3 \\
 \dot{F}_1(t) &= \kappa_{df}^1 (R_1 + L_1) + \kappa_{cf}^1 C_1 - (\kappa_{fc}^1 + \kappa_{fd}^1) F_1 + \delta(F_2 - F_1) \\
 \dot{F}_2(t) &= \kappa_{df}^2 (R_2 + L_2) + \kappa_{cf}^2 C_2 - (\kappa_{fc}^2 + \kappa_{fd}^2) F_2 + \delta(F_3 - F_2) + \delta(F_1 - F_2) \\
 \dot{F}_3(t) &= \kappa_{df}^3 (R_3 + L_3) + \kappa_{cf}^3 C_3 - (\kappa_{fc}^3 + \kappa_{fd}^3) F_3 + \delta(F_2 - F_3) \\
 \dot{L}_1(t) &= \kappa_{fl}^1 F_1 + \kappa_{cl}^1 C_1 + \tau L_2 - (\kappa_{lf}^1 + \kappa_{dc}^1) L_1 \\
 \dot{L}_2(t) &= \kappa_{fl}^2 F_2 + \kappa_{cl}^2 C_2 + \tau L_3 - (\tau + \kappa_{lf}^2 + \kappa_{dc}^2) L_2 \\
 \dot{L}_3(t) &= \kappa_{fl}^3 F_3 + \kappa_{cl}^3 C_3 - (\tau + \kappa_{lf}^3 + \kappa_{dc}^3) L_3
 \end{aligned}$$

### S3 Steady state distributions, absolute values

518



**Fig 9.** Simulated steady state probability distribution of vesicles in control (A) and upon stimulation (B), visualised with absolute values and  $C1 = 1$ .



**Fig 10.** (A) Control steady state distribution of vesicles in control with constant transition rates (5) and visualised using absolute values (normalised such that  $C1 = 1$ ). (B) Crowding correction factors (8) in control.

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## References

1. Gimenez-Molina Y, Villanueva J, Francés MdM, Viniegra S, Gutiérrez LM. Multiple Mechanisms Driving F-actin-Dependent Transport of Organelles to and From Secretory Sites in Bovine Chromaffin Cells. *Frontiers in Cellular Neuroscience*. 2018;12:344. doi:10.3389/fncel.2018.00344.
2. McMurray CT. Neurodegeneration: diseases of the cytoskeleton? *Cell Death Differ*. 2000;7(10):861–865.
3. Wang T, Martin S, Nguyen TH, Harper CB, Gormal RS, Martínez-Mármol R, et al. Flux of signalling endosomes undergoing axonal retrograde transport is encoded by presynaptic activity and TrkB. *Nature Communications*. 2016;7. doi:10.1038/ncomms12976.
4. Barlan K, Gelfand VI. Microtubule-Based Transport and the Distribution, Tethering, and Organization of Organelles. *Cold Spring Harbor Perspectives in Biology*. 2017;9(5). doi:10.1101/cshperspect.a025817.
5. Caviston JP, Holzbaur ELF. Microtubule motors at the intersection of trafficking and transport. *Trends in Cell Biology*. 2006;16(10):530 – 537. doi:https://doi.org/10.1016/j.tcb.2006.08.002.
6. Trifaró JM, Gasman S, Gutiérrez LM. Cytoskeletal control of vesicle transport and exocytosis in chromaffin cells. *Acta Physiologica*. 2008;192(2):165–172. doi:10.1111/j.1748-1716.2007.01808.x.
7. Brown SS. Cooperation Between Microtubule- and Actin-Based Motor Proteins. *Annual Review of Cell and Developmental Biology*. 1999;15(1):63–80. doi:10.1146/annurev.cellbio.15.1.63.
8. Rosé SD, Lejen T, Casaletti L, Larson RE, Pene TD, Trifaró JM. Myosins II and V in chromaffin cells: myosin V is a chromaffin vesicle molecular motor involved in secretion. *Journal of Neurochemistry*. 2003;85(2):287–298. doi:10.1046/j.1471-4159.2003.01649.x.
9. Rudolf R, Kögel T, Kuznetsov SA, Salm T, Schlicker O, Hellwig A, et al. Myosin Va facilitates the distribution of secretory granules in the F-actin rich cortex of PC12 cells. *Journal of Cell Science*. 2003;116(7):1339–1348. doi:10.1242/jcs.00317.
10. Ñeco P, Giner D, Del Mar Francés M, Viniegra S, Gutiérrez LM. Differential participation of actin- and tubulin-based vesicle transport systems during secretion in bovine chromaffin cells. *European Journal of Neuroscience*. 2003;18(4):733–742. doi:10.1046/j.1460-9568.2003.02801.x.

11. Papadopulos A, Gomez GA, Martin S, Jackson J, Gormal RS, Keating DJ, et al. Activity-driven relaxation of the cortical actomyosin II network synchronizes Munc18-1-dependent neurosecretory vesicle docking. *Nature Communications*. 2015;6. doi:10.1038/ncomms7297.
12. Tomatis VM, Papadopulos A, Malintan NT, Martin S, Wallis T, Gormal RS, et al. Myosin VI small insert isoform maintains exocytosis by tethering secretory granules to the cortical actin. *Journal of Cell Biology*. 2013;200(3):301–320. doi:10.1083/jcb.201204092.
13. Trifaró JM, Bader MF, Doucet JP. Chromaffin cell cytoskeleton: its possible role in secretion. *Canadian Journal of Biochemistry and Cell Biology*. 1985;63(6):661–679. doi:10.1139/o85-084.
14. Gutiérrez LM, Villanueva J. The role of F-actin in the transport and secretion of chromaffin granules: an historic perspective. *Pflügers Archiv - European Journal of Physiology*. 2018;470(1):181–186.
15. Oheim M, Stühmer W. Tracking chromaffin granules on their way through the actin cortex. *European Biophysics Journal*. 2000;29(2):67–89.
16. Giner D, López I, Villanueva J, Torres V, Viniegra S, Gutiérrez LM. Vesicle movements are governed by the size and dynamics of F-actin cytoskeletal structures in bovine chromaffin cells. *Neuroscience*. 2007;146(2):659 – 669. doi:<https://doi.org/10.1016/j.neuroscience.2007.02.039>.
17. Meunier FA, Gutiérrez LM. Captivating New Roles of F-Actin Cortex in Exocytosis and Bulk Endocytosis in Neurosecretory Cells. *Trends in Neurosciences*. 2016;39(9):605–613. doi:10.1016/j.tins.2016.07.003.
18. Porat-Shliom N, Porat-Shliom N, Milberg O, Milberg O, Masedunskas A, Masedunskas A, et al. Multiple roles for the actin cytoskeleton during regulated exocytosis. *Cellular and molecular life sciences : CMLS*. 2013;70(12):2099–2121.
19. Maucort G, Kasula R, Papadopulos A, Nieminen TA, Rubinsztein-Dunlop H, Meunier FA. Mapping Organelle Motion Reveals a Vesicular Conveyor Belt Spatially Replenishing Secretory Vesicles in Stimulated Chromaffin Cells. *PLOS ONE*. 2014;9(1):1–9. doi:10.1371/journal.pone.0087242.
20. Smith DA, Simmons RM. Models of Motor-Assisted Transport of Intracellular Particles. *Biophysical Journal*. 2001;80(1):45 – 68. doi:[https://doi.org/10.1016/S0006-3495\(01\)75994-2](https://doi.org/10.1016/S0006-3495(01)75994-2).
21. Bressloff PC. *Stochastic processes in cell biology*. vol. 41. Springer; 2014.
22. Haderer KP. *Topics in Mathematical Biology by Karl Peter Haderer. Lecture Notes on Mathematical Modelling in the Life Sciences*. Cham: Springer International Publishing : Imprint: Springer; 2017.
23. White D, de Vries G, Dawes A. Microtubule Patterning in the Presence of Stationary Motor Distributions. *Bulletin of mathematical biology*. 2014;76(8):1917–1940.
24. Chen W, Zhou W, Xia T, Gu X. A Computational Analysis Framework for Molecular Cell Dynamics: Case-Study of Exocytosis. *PLOS ONE*. 2012;7(7):1–10. doi:10.1371/journal.pone.0038699.

25. Mayorga LS, Verma M, Hontecillas R, Hoops S, Bassaganya-Riera J. Agents and networks to model the dynamic interactions of intracellular transport. *Cellular Logistics*. 2017;7(4):e1392401. doi:10.1080/21592799.2017.1392401.
26. Klann M, Koepl H, Reuss M. Spatial Modeling of Vesicle Transport and the Cytoskeleton: The Challenge of Hitting the Right Road. *PLOS ONE*. 2012;7(1):1–15. doi:10.1371/journal.pone.0029645.
27. Birbaumer M, Schweitzer F. Agent-based modeling of intracellular transport. *The European Physical Journal B*. 2011;82(245).
28. Jarukanont D, Bonifas Arredondo I, Femat R, Garcia ME. Vesicle Motion during Sustained Exocytosis in Chromaffin Cells: Numerical Model Based on Amperometric Measurements. *PloS one*. 2015;10(12):e0144045–e0144045.
29. Oelz DB. Quasi-steady-state reduction of a model for cytoplasmic transport of secretory vesicles in stimulated chromaffin cells. *Journal of Mathematical Biology*. 2021;82(4):29. doi:10.1007/s00285-021-01583-5.
30. Bressloff PC. *Stochastic Processes in Cell Biology* by Paul C. Bressloff. 1st ed. *Interdisciplinary Applied Mathematics*, 41. Cham: Springer International Publishing : Imprint: Springer; 2014.
31. Papadopulos A. Membrane shaping by actin and myosin during regulated exocytosis. *Molecular and Cellular Neuroscience*. 2017;84:93–99. doi:<https://doi.org/10.1016/j.mcn.2017.05.006>.
32. Gurel P, Hatch A, Higgs H. Connecting the Cytoskeleton to the Endoplasmic Reticulum and Golgi. *Current Biology*. 2014;24(14):R660–R672. doi:<https://doi.org/10.1016/j.cub.2014.05.033>.
33. Alon U. *An introduction to systems biology: design principles of biological circuits*. CRC press; 2019.
34. Wang T, Martin S, Papadopulos A, Harper CB, Mavlyutov TA, Niranjana D, et al. Control of Autophagosomal Axonal Retrograde Flux by Presynaptic Activity Unveiled Using Botulinum Neurotoxin Type A. *Journal of Neuroscience*. 2015;35(15):6179–6194. doi:10.1523/JNEUROSCI.3757-14.2015.
35. Joensuu M, Padmanabhan P, Durisic N, Bademosi ATD, Cooper-Williams E, Morrow IC, et al. Subdiffractional tracking of internalized molecules reveals heterogeneous motion states of synaptic vesicles. *Journal of Cell Biology*. 2016;215(2):277–292. doi:10.1083/jcb.201604001.
36. Bezanson J, Edelman A, Karpinski S, Shah VB. Julia: A Fresh Approach to Numerical Computing. *SIAM Review*. 2017;59(1):65–98. doi:10.1137/141000671.