

1 **TITLE PAGE**

2 Inter-laboratory automation of the *in vitro* micronucleus assay using imaging flow cytometry and  
3 deep learning

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## 27 **DECLARATIONS**

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## 40 **Conflicts of interest/competing interests**

41 M. A. R., is an employee of Luminex Corporation which manufactures the Amnis ImageStream  
42 imaging flow cytometers used in this research study.

43

## 44 **Availability of data and materials**

45 Imaging flow cytometry test images alongside the final DeepFlow neural network are provided for  
46 download from the BioStudies database (<http://www.ebi.ac.uk/biostudies>) under accession number  
47 S-BSST641.

48

## 49 **Code availability**

50 The presented deep learning image analysis pipeline is available for download at the BioStudies  
51 database (<http://www.ebi.ac.uk/biostudies>) in MATLAB and Python programming languages under  
52 accession number S-BSST641.

53

54 **Ethics approval**

55 This study uses *in vitro* cell lines only. No ethical approval was required.

56

57 **Consent to participate**

58 Not applicable

59

60 **Consent for publication**

61 Not applicable

62 **ABSTRACT**

63 The *in vitro* micronucleus assay is a globally significant method for DNA damage quantification  
64 used for regulatory compound safety testing in addition to inter-individual monitoring of  
65 environmental, lifestyle and occupational factors. However it relies on time-consuming and user-  
66 subjective manual scoring. Here we show that imaging flow cytometry and deep learning image  
67 classification represents a capable platform for automated, inter-laboratory operation. Images were  
68 captured for the cytokinesis-block micronucleus (CBMN) assay across three laboratories using  
69 methyl methanesulphonate (1.25 – 5.0 µg/mL) and/or carbendazim (0.8 – 1.6 µg/mL) exposures to  
70 TK6 cells. Human-scored image sets were assembled and used to train and test the classification  
71 abilities of the “DeepFlow” neural network in both intra- and inter-laboratory contexts. Harnessing  
72 image diversity across laboratories yielded a network able to score unseen data from an entirely new  
73 laboratory without any user configuration. Image classification accuracies of 98%, 95%, 82% and  
74 85% were achieved for ‘mononucleates’, ‘binucleates’, ‘mononucleates with MN’ and ‘binucleates  
75 with MN’, respectively. Successful classifications of ‘trinucleates’ (90%) and ‘tetranucleates’ (88%)  
76 in addition to ‘other or unscorable’ phenotypes (96%) were also achieved. Attempts to classify  
77 extremely rare, tri- and tetranucleated cells with micronuclei into their own categories were less  
78 successful ( $\leq 57\%$ ). Benchmark dose analyses of human or automatically scored micronucleus  
79 frequency data yielded quantitation of the same equipotent dose regardless of scoring method. We  
80 conclude that this automated approach offers significant potential to broaden the practical utility of  
81 the CBMN method across industry, research and clinical domains. We share our strategy using  
82 openly-accessible frameworks.

83

84 **Keywords**

85 Micronucleus test, genetic toxicology, compound screening, machine learning, high throughput,  
86 image analysis.

87

## 88 INTRODUCTION

89 Across industry, government and academic research institutions the *in vitro* micronucleus test is one  
90 of the most widely used bioassays for the identification and quantification of chromosomal damage  
91 (Decordier and Kirsch-Volders 2006; Fenech 2000; Fenech 2020; Kirsch-Volders et al. 2011).  
92 Because DNA damage at the chromosome level is recognised as a key event in the initiation of  
93 carcinogenesis, the assay has become an essential component of genetic toxicity screening  
94 programmes worldwide (Fenech 2000). Harmonised assay protocols and scoring approaches have  
95 been detailed by Organisation for Economic Cooperation and Development (OECD)-Test Guideline  
96 487 (OECD 2016). In addition to regulatory compound screening, the assay is also widely used for  
97 more specific research and clinical purposes including compound mode-of-action determinations,  
98 tumour radiosensitivity prediction and inter-individual monitoring of lifestyle, occupational and  
99 environmental factors including radiation biodosimetry assessments (Decordier and Kirsch-Volders  
100 2006; Fenech 2000; Fenech 2020; Kirsch-Volders et al. 2011; Wang et al. 2019).

101 The micronucleus assay operates through the detection of whole chromosomes or chromosome  
102 fragments expressed by cells after nuclear division as satellite ‘micronucleus’ (MN) events. Because  
103 complete nuclear division is required to enable expression of these events, the ‘cytokinesis-block’  
104 version of the assay was developed. This method inhibits cell division into daughter entities  
105 (cytokinesis) using the microfilament assembly inhibitor cytochalasin-B. This yields cells that have  
106 successfully undergone division easily identifiable by their binucleated appearance. In this way, the  
107 cytokinesis-block micronucleus (CBMN) assay allows scoring of micronucleus events in cells  
108 known to have undergone division during the treatment period. This avoids misleading results  
109 otherwise present due to pre-existing damage, sub-optimal cell culture conditions or from the  
110 selection of overly cytotoxic compound doses that retard or inhibit cell division and concomitant  
111 micronucleus expression (Decordier and Kirsch-Volders 2006; Fenech 2000; Kirsch-Volders et al.  
112 2011).

113

114 Despite almost global utilisation, CBMN assay scoring still often relies upon manual observation and  
115 recording using light microscopy. Whilst manual scoring is the ‘gold standard’, it suffers from user  
116 subjectivity and scorer variability in addition to being extremely time and labour-intensive  
117 (Rodrigues et al. 2014a; Rodrigues et al. 2014b; Rodrigues et al. 2018). For these reasons, over the  
118 last two decades significant efforts have been directed towards automated approaches for both image  
119 collection and subsequent scoring. As recently reviewed (Rodrigues et al. 2018), these largely  
120 involve slide and laser scanning microscopy systems that automate image collection in conjunction  
121 with traditional, threshold-based image classification techniques (Darzynkiewicz et al. 2011;  
122 Decordier et al. 2009; Decordier et al. 2011; François et al. 2014; Maertens and White 2015;  
123 Rossnerova et al. 2011; Schunck et al. 2004; Seager et al. 2014; Smolewski et al. 2001; Varga et al.  
124 2004; Verhaegen et al. 1994; Willems et al. 2010). Conventional flow cytometry methods have also  
125 been developed that aim to identify isolated micronuclei using fluorescence intensity measurements  
126 in the absence of image-based validation (Avlasevich et al. 2006; Bryce et al. 2008; Bryce et al.  
127 2010; Bryce et al. 2013; Bryce et al. 2007).

128

129 More recently, imaging flow cytometry unites the acquisition approach of flow cytometry with  
130 microscopical observation (Allemang et al. 2021; Rodrigues 2018; Rodrigues 2019; Rodrigues et al.  
131 2014a; Rodrigues et al. 2014b; Rodrigues et al. 2016a; Rodrigues et al. 2018; Rodrigues et al. 2016b;  
132 Wang et al. 2019; Wilkins et al. 2017). This fluidics-based approach is well suited for processing cell  
133 suspension cultures (*e.g.*, TK6 B-lymphocytes commonly used for the CBMN assay) enabling rapid  
134 collection of transmitted light brightfield, darkfield laser scatter and fluorescence images for  
135 populations of tens of thousands of single cells. Simple inclusion of a single nuclear fluorescent stain  
136 (*e.g.*, Hoechst 33342, propidium iodide or DRAQ5 *etc.*) allows detection of parent nuclei and  
137 micronucleus events (Rodrigues 2018; Rodrigues 2019; Rodrigues et al. 2018; Rodrigues et al.  
138 2016b). Without need of further labels, the brightfield images provide essential context for detecting

139 micronuclei associated with parent cells (Rodrigues et al. 2014a; Verma et al. 2018). The ‘Amnis  
140 ImageStream<sup>X</sup>’ series cytometers (Luminex Corporation) further support unassisted data acquisition  
141 for multiple samples via a 96-well plate sampling attachment. Images are stored to sample-specific  
142 data files enabling archiving should human validation or reevaluation be required (Rodrigues et al.  
143 2018). Traditional image classification approaches deployed within the manufacturer-supplied  
144 analysis software have shown utility for CBMN scoring automation (Rodrigues 2018; Rodrigues  
145 2019; Rodrigues et al. 2014a; Rodrigues et al. 2014b; Rodrigues et al. 2016a; Rodrigues et al. 2018;  
146 Rodrigues et al. 2016b; Wang et al. 2019; Wilkins et al. 2017). However, in our experience these  
147 strategies require significant expertise to set up, in addition to frequent tuning to maintain acceptable  
148 performance, even within a single laboratory (Verma et al. 2018). Deviations of around 30% from  
149 the results obtained by manual microscopy scoring have also been reported in experiments utilising  
150 this approach to study irradiated peripheral blood lymphocytes (Rodrigues et al. 2016b). This  
151 outcome was in part attributed to the lack of flexibility of the implemented image analysis algorithms  
152 relative to the expertise of human judgement (Rodrigues et al. 2018; Rodrigues et al. 2016b).

153  
154 Building image classification strategies that *generalise* well enough to permit robust, entirely  
155 automated image classifications without need of human intervention or configuration is a difficult  
156 task. This is because, even when protocols are harmonised, there will always be variability (*e.g.*,  
157 illumination, focus and fluorescence staining heterogeneity *etc.*) in the input image data. This  
158 variation is even more extreme across laboratories due to the inevitable use of different imaging  
159 equipment, calibration settings, personnel, cell culture and bioassay regimens. Recently, artificial  
160 intelligence approaches have been achieving increasing success in providing generalised automation  
161 of image classification tasks (Caicedo et al. 2019; Moen et al. 2019). These approaches can use  
162 handcrafted features extracted from images in conjunction with machine learning algorithms, but  
163 increasingly, the availability of computational power is enabling the application of deep learning on  
164 image pixel data (Blasi et al. 2016; Eulenberg et al. 2017). This approach uses so-called deep

165 convolutional neural networks in a manner inspired by neural connectivity in the brain. A typical  
166 image classification workflow involves assigning ‘ground truth’ class annotations to a large set of  
167 images before subdividing them into ‘train’ and ‘test’ datasets. The weights connecting the nodes of  
168 the neural network are then optimised during a training phase that attempts to match the input images  
169 to the annotated classifications. A potential issue due to the flexibility of neural networks as non-  
170 linear function approximators is that ‘memorisation’ due to over-fitting of training data can emerge  
171 (Zhang et al. 2017). For this reason, final network accuracy is assessed by cross validation against a  
172 test set that importantly was entirely ‘unseen’ during the training phase. Subsequently, the trained  
173 neural net can be deployed for the classification of new images.

174  
175 In the context of the CBMN assay, deep learning approaches were recently used on imaging flow  
176 cytometry data using the cytometer manufacturer’s ‘Amnis Artificial Intelligence’ software to  
177 identify binucleated cells in the 3-D reconstructed skin micronucleus assay. This binucleated cell  
178 population was then used as a refined start point from which to expedite manual identification of  
179 micronucleus events (Allemang et al. 2021). However, there would be considerable value in openly  
180 accessible frameworks for accessibility and for adaptability: the modular nature of modern, open  
181 source deep learning interfaces allows new network architectures to be easily switched or  
182 specifically tailored as they emerge. This flexibility provides complete ability to build bespoke  
183 solutions using the latest tools to pursue maximal accuracy and the accommodation of diverse  
184 research objectives.

185  
186 Here, we used imaging flow cytometry to automate image capture for the CBMN assay across three  
187 laboratories using differing local protocols for cell culture, bioassay procedure, DNA staining,  
188 cytometer calibration and image collection. Given the inherent variability in the captured images, we  
189 investigate the ability of deep learning to enable robust, inter-laboratory scoring automation. To do  
190 this, we provide an open framework that utilises the powerful, yet lightweight DeepFlow neural



191 network architecture that has been previously optimised to achieve rapid training and classification  
192 of imaging flow cytometry data (Eulenberg et al. 2017).

193

194

## 195 **MATERIALS & METHODS**

### 196 **Multi-centre image collection**

197 Image data was collected using three different Amnis ImageStream<sup>X</sup> imaging flow cytometers  
198 (Luminex Corporation, USA) across three locations: Central Biotechnology Services, Cardiff  
199 University School of Medicine (hereafter, Cardiff), the Department of Veterinary Medicine's  
200 Imaging Facility, University of Cambridge, UK (Cambridge) and at GlaxoSmithKline Research and  
201 Development, Stevenage, UK (GSK).

202

### 203 **Chemicals**

204 Methyl methanesulphonate (MMS) (#129925) (CAS registry number 66-27-3) and carbendazim  
205 (#378674) (CAS no. 10605-21-7) were purchased from Sigma-Aldrich (Merck), UK.

206

### 207 **Cardiff and Cambridge: Cell culture and cytokinesis-block micronucleus assay**

208 P53 competent, virally transformed human B lymphoblastoid (TK6) cells were purchased from the  
209 Health Protection Agency Culture Collections (Wiltshire, UK). The cells were cultured in RPMI  
210 1640 media (#A1049101, ThermoFisher) supplemented with 100 U/mL penicillin and 100 µg/mL  
211 streptomycin and containing 10% (v/v) heat-inactivated horse serum (#26050088, ThermoFisher).  
212 Cells were seeded at  $2 \times 10^5$  cells/mL in 25 cm<sup>2</sup> flasks (ThermoFisher) and incubated at 37 °C for ~  
213 1.5 cell cycles (24-30 h) in the presence of MMS (0 / 1.25 / 2.5 / 5.0 µg/mL doses) or carbendazim (0  
214 / 0.8 / 1.0 / 1.6 µg/mL doses) with co-exposed cytochalasin-B (#C6762, Sigma) added to a final  
215 concentration of 3 µg/mL as a cytokinesis-block. Following exposure, cells were pelleted by  
216 centrifugation (200xg, 10 min) and washed once with 10 mL phosphate buffered saline (PBS). Cells

217 were then pelleted and resuspended in 2 mL 1X BD FACS lysing solution (#349202, BD) for 12 min  
218 to achieve fixation and permeabilisation.

219

### 220 **GSK: Cell culture and cytokinesis-block micronucleus assay**

221 TK6 (IVGT) cells (#13051501) purchased from ECACC, operated by Public Health England  
222 (Wiltshire, UK). The cells were cultured in RPMI 1640 media with 2 mM glutamine (#52400-025,  
223 ThermoFisher) supplemented with 100 U/mL penicillin and 100 µg/mL streptomycin (#15140-122,  
224 ThermoFisher), 1.8 mM sodium pyruvate (#11360-039, ThermoFisher) and containing 10% (v/v)  
225 heat-inactivated horse serum (#26050-088, BioSera, Labtech, UK). Cells were seeded at  $2 \times 10^5$   
226 cells/mL in 25 cm<sup>2</sup> flasks (ThermoFisher) and incubated at 37 °C for 24 h in the presence of  
227 carbendazim (0 / 0.8 / 1.2 / 1.6 µg/mL doses) with co-exposed cytochalasin-B (#C6762, Sigma)  
228 added to a final concentration of 6 µg/mL as a cytokinesis-block. Following exposure, cells were  
229 pelleted by centrifugation (200xg, 10 min) and washed once with 10 mL PBS (#10010-015,  
230 ThermoFisher). Cells were then pelleted and resuspended in 2 mL 1X BD FACS lysing solution  
231 (#349202, BD) for 12 min to achieve fixation and permeabilisation.

232

### 233 **Nuclear labelling**

234 Fixed, permeabilised cells were incubated with nuclear stains in PBS at room temperature. Nuclei  
235 and micronuclei were stained at the Cardiff and GSK laboratories by 30 min incubation with 0.05  
236 mM DRAQ5 (peak excitation: 647 nm, peak emission: 681 nm) (#564902, BD). Samples at the  
237 Cambridge laboratory were stained with a 1:2500 dilution (8 µM) of Hoechst 33342 (peak excitation:  
238 351 nm, peak emission: 461 nm) (#62249, ThermoFisher) for 30 mins. After labelling, cells were  
239 pelleted, resuspended and final cell concentrations adjusted through addition of PBS towards an  
240 optimal cell concentration for imaging flow cytometry (typically ~100 µL sample volumes at ~ $10^7$   
241 cells/mL).

242

## 243 **Imaging flow cytometry**

244 Brightfield and nuclear fluorescence images (20,000 images / sample) were collected using Amnis  
245 ImageStream<sup>X</sup> (Luminex) flow cytometers using the 40X objective lens via the manufacturer's  
246 INSPIRE software at the Cardiff, Cambridge and GSK laboratories (described above). At Cardiff  
247 and GSK, DRAQ5-labelled cells were excited using 488 nm or 642 nm lasers (respectively) with the  
248 brightfield collected in channel 1 and DRAQ5 in channel 11. At Cambridge, Hoechst 33342-labelled  
249 cells were excited using a 405 nm laser with brightfield collection in channel 4 and nuclear  
250 fluorescence collection in channel 1. At all locations, a brightfield area range of 100-900  $\mu\text{m}^2$  was  
251 used to avoid debris, speed bead and large aggregate image collection. Full details of image  
252 acquisition settings including the laser excitation powers the exact cytometer models utilised at each  
253 location are provided in **Supp. Table S1**.

254

## 255 **Compensated image file generation using IDEAS**

256 Prior to image extraction, raw image files (.rif) acquired by the INSPIRE software were converted to  
257 compensated image files (.cif) using identical settings via batch processing with a template using the  
258 IDEAS (version 6.2) software (Luminex). During the process, populations of cell images suitable for  
259 scoring were refined by gating out (brightfield area, 200 – 500  $\mu\text{m}^2$  versus aspect ratio, 0.75 – 1.0)  
260 debris and identifying a single cell population that was also suitably in focus. This was achieved by  
261 linescan gradient via the root mean square of the brightfield images ranging from 55 – 80.

262

## 263 **Image data pre-processing: CIF to TIF extraction**

264 Single, in-focus cell populations were exported from the IDEAS software in compensated image file  
265 format (.cif). The individual cell images within these files were then extracted to 16-bit grayscale,  
266 two-channel (nuclear fluorescence / brightfield) multipage TIF files using a custom script (code and  
267 example available for download from the BioStudies database (<http://www.ebi.ac.uk/biostudies>) in  
268 MATLAB and Python programming languages under accession number S-BSST641). During this

269 TIF extraction process, each channel image was also max/min rescaled to normalise illumination.  
270 Images were also cropped and zero-padded to a standard 64x64 pixel-square size for input into the  
271 DeepFlow network.

272

### 273 **Deep learning image classification**

274 Automated scoring was achieved using a nine-class, feed-forward, image classification deep neural  
275 network built using our previously described “DeepFlow” architecture (Eulenberg et al. 2017). This  
276 network is optimised for the relatively small input dimensions of imaging flow cytometry data, and  
277 in itself utilises dual-path convolution / batch normalisation / nonlinearity subunits interspersed by  
278 max pooling from the popular “Inception” architecture (Szegedy et al. 2015). These subunit layers  
279 process and aggregate visual information at increasing scale before average pooling, the fully  
280 connected layer and softmax classification (full network architecture shown, **Supp. Figure 1**).  
281 Images were passed to the network with an input size of 64x64x2 (x, y, channels), with augmentation  
282 by random x/y reflection, rotation, translation, 90%-110% image scaling and zero-center batch  
283 normalisation. Training lasted for 30 epochs using a batch size of 88 with optimisation under ADAM  
284 using cross-entropy loss. The initial learn rate was  $5 \times 10^{-3}$ , dropping every five epochs by 0.9, with  
285 L2 regularisation  $1 \times 10^{-4}$  and epsilon  $1 \times 10^{-8}$ . Images were shuffled every epoch. The final pre-trained  
286 network alongside test images and all code detailing training hyper-parameters and final layer  
287 weightings are available for download in MATLAB (using the Deep Learning Toolbox) or Python  
288 (using TensorFlow / keras) languages at the BioStudies database (<http://www.ebi.ac.uk/biostudies>)  
289 under accession number S-BSST641.

290

### 291 **Ground truth curation by human scoring**

292 For the Cardiff / Cambridge analyses, cell image data across compounds (carbendazim and MMS)  
293 and doses (0 – 5  $\mu\text{g}/\text{mL}$ ) were merged to create diverse ground truth training sets that contained the  
294 wide representation of different cell phenotypes essential for effective network training. Ground truth

295 classifications for each image were assigned by biologists with extensive experience manually  
296 scoring the *in vitro* micronucleus assay, with phenotypes assigned through consideration of both the  
297 nuclear fluorescence and the brightfield image (*i.e.*, ensuring nuclear events belonged to one cell  
298 *etc.*). As per micronucleus assay test guidance, the aim was to only score cells positive for  
299 micronucleus events where the micronuclei were fluorescently-labelled, were circular/oval in shape,  
300 were within the size range of  $1/3 - 1/16^{\text{th}}$  that of the parent nuclei, and that were clearly inside the  
301 cell boundary of the parent cell (Fenech 2000; OECD 2016). At the GSK laboratory, TK6 cells were  
302 exposed to just the carbendazim compound (0 / 0.8 / 1.2 / 1.6  $\mu\text{g/mL}$  doses) with the experiment  
303 conducted in triplicate. For the initial network cross validation with the GSK data, five thousand  
304 human-scored cell images were used with these events equally accumulated from across all  
305 carbendazim exposures. For the dose-response analysis, cell populations of two thousand events  
306 were scored per dose in triplicate by either human-scoring or by the neural network.

307

### 308 **Statistical significance of micronucleus responses relative to control**

309 Assessment of micronucleus response significance was conducted according to the framework  
310 described in Johnson et al., (Johnson et al. 2014). Response data was  $\log_{10}$  transformed and assessed  
311 for normality and variance homogeneity by Shapiro-Wilk and Bartlett tests respectively. Where the  
312 transformed data passed these tests ( $p > 0.05$ ), comparisons of micronucleus responses relative to  
313 untreated negative controls employed one sided *post hoc* Dunnett's test with alpha 0.05. Datasets  
314 that failed these tests ( $p < 0.05$ ) were analysed using the non-parametric *post hoc* Dunn's test.

315

### 316 **Benchmark dose analysis**

317 To compare the dose-response relationships obtained from human expert scoring relative to those  
318 obtained from automatic scoring using the trained neural network, nonlinear regression analysis  
319 using the Benchmark Dose (BMD) framework was used. Using the freely available PROAST  
320 software, dose-response data were analysed using both the exponential and the Hill model family

321 recommended for the assessment of continuous toxicity data by the European Food Safety Authority  
322 (EFSA) (Hardy et al. 2017). In each analysis, combined datasets (*i.e.*, across scoring methods) were  
323 analysed together with ‘scoring method’ specified as a potential covariate (Wills et al. 2016). More  
324 complex models with additional parameters were accepted if the fit significantly ( $p < 0.05$ ; log-  
325 likelihood) improved. Here, as in previous work, we found that the log-steepness (*parameter d*) and  
326 maximum response (*parameter c*) could reasonably be held equal across dose-response curves,  
327 whereas the parameters for background response (*parameter a*), potency (*parameter b*), and within-  
328 group variance (*var*) were found to be covariate-dependent (Slob and Setzer 2014). The BMD output  
329 describes the ‘equipotent dose’ of the modelled dose-response relationships in addition to the  
330 bounding, two-sided 90% confidence interval for each level of the covariate. The benchmark  
331 response (BMR) size (also termed the critical effect size) used was 50%, which represents a 50%  
332 increase in response relative to the background established in the vehicle (zero-dose) control.

333

334

## 335 RESULTS

336 Here, we investigate the ability of deep learning to provide generalised automation of CBMN assay  
337 scoring using imaging flow cytometry data acquired according to local protocols across three  
338 different laboratories (Cardiff, Cambridge and GSK). **Fig. 1a** demonstrates our workflow. At the end  
339 of the assay, cells were fixed and permeabilised before fluorescent nuclear staining. The choice of  
340 nuclear stain varied across the different laboratories according to compatibility with the laser  
341 configuration of the local imaging cytometer. At Cambridge, cells were labelled with the blue-  
342 fluorescent dye Hoechst 33342 which was stimulated by a 405 nm laser with image capture using a  
343 ImageStream<sup>X</sup> cytometer. At Cardiff and GSK, ImageStream<sup>X</sup> MKII cytometers were used in  
344 conjunction with the red-emitting DRAQ5 nuclear stain and excitation by either a 488 nm or 642 nm  
345 laser (respectively). Full details of image acquisition settings at each laboratory are shown in **Supp.**  
346 **Table 1**. Image acquisition speeds depended on cell concentrations, in addition to the time taken to

347 purge the flow stream and load each new sample; approximately ~ 2000 – 5000 cell-images / minute  
348 was typical.

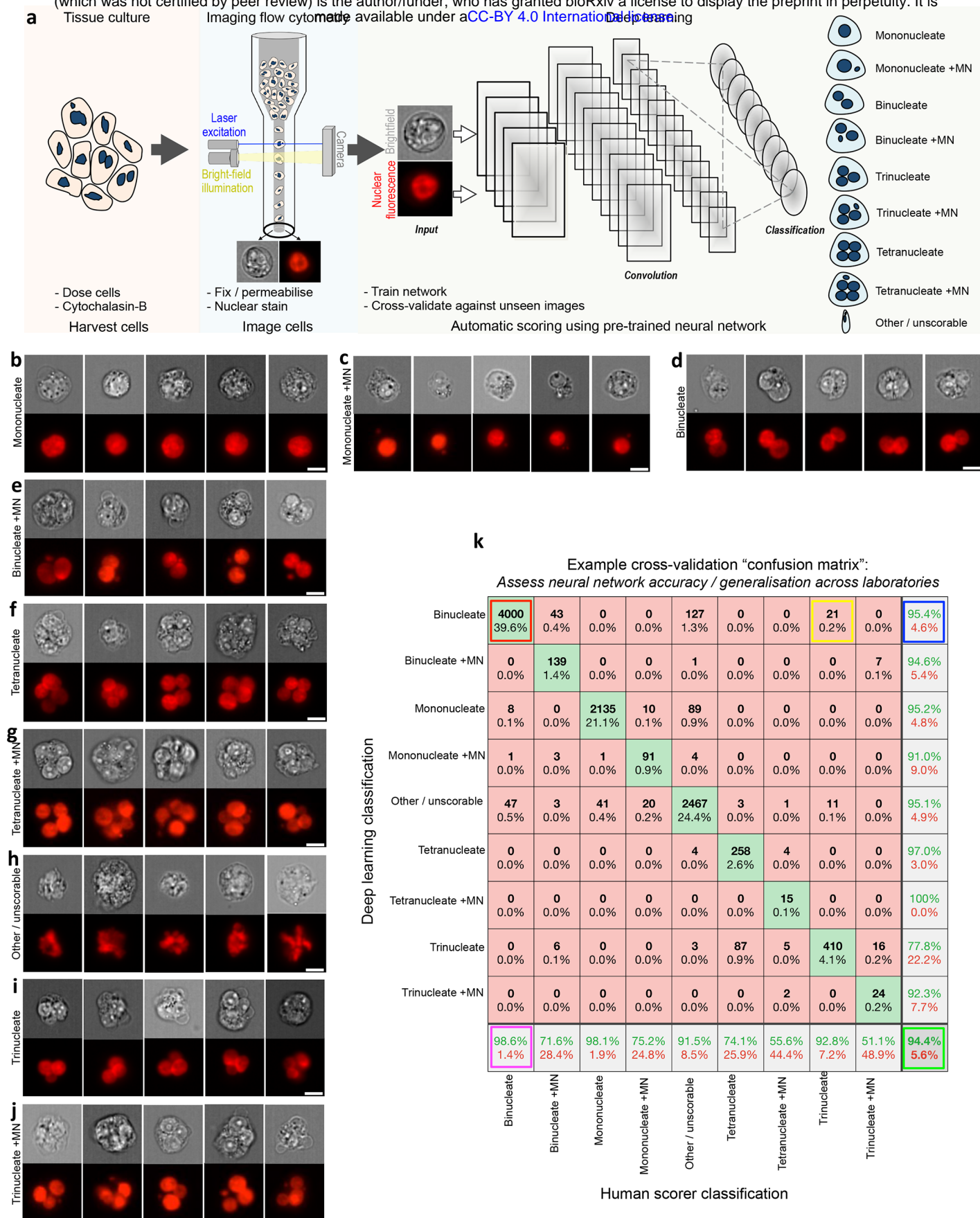
349

350 After image collection, a template file created in the cytometer manufacturer's IDEAS software was  
351 used to automatically batch-save populations of single cells that additionally met acceptable focus  
352 criteria (see Methods). These cell populations served as the input into the deep learning scoring  
353 pipeline. This workflow is provided for download in both MATLAB and Python programming  
354 languages at the Biostudies database (accession no. S-BSST641). In brief – the download  
355 demonstrates initial image pre-processing to normalise image illumination across cytometers in  
356 addition to how to build and train the DeepFlow neural network using a human-scored training  
357 image set. After successful training, the saved network can subsequently be used to automate the  
358 scoring of new images. For example, **Fig. 1b-j** shows typical events classified by a pretrained, nine-  
359 class network with cell classes for mononucleates, binucleates, trinucleates and quadrinucleates with  
360 or without micronucleus events in addition to a final class for 'other or unscorable' phenotypes.

361

362 As introduced above, an essential component of network testing involves cross validation with  
363 human-scored test images unseen during the training phase. We display this evaluation as a  
364 confusion matrix, which compares network outputs to the human scores for every image in the test  
365 set (explained, **Fig. 1k**). In the subsequently presented results, we use this strategy to rigorously test  
366 the ability of a range of trained networks to enable automated CBMN assay scoring in both intra- and  
367 inter-laboratory contexts. In each instance, human-scored image sets were built from cell events  
368 pooled across the available compounds and exposures. This strategy was chosen to maximise the  
369 diversity of cellular phenotypes present, as well as to ensure that the rarer, micronucleated  
370 phenotypes that predominately manifested at higher exposures were well represented.

371



**Fig. 1 Automating the *in vitro* micronucleus assay using imaging flow cytometry and deep learning image classification.** **a** Workflow: harvested cells were fixed and permeabilised before counterstaining the nuclei with a fluorescent DNA stain. Transmitted light brightfield (grey) and nuclear fluorescence (red) images were then automatically captured by high-throughput imaging flow cytometry. After initial training using a human-annotated image set, single cell images from the cytometer can be automatically classified using the neural network image classification algorithm. **b-j** Example image classifications according to a nine-class network developed to score the cytokinesis-block *in vitro* micronucleus assay in human lymphoblastoid TK6 cells. **k** An example cross-validation 'confusion matrix' obtained during preliminary network optimisations and presented here to demonstrate confusion matrix interpretation. The matrix represents an image set scored by humans that is 'unseen' during network training. The horizontal direction represents the human scorer classifications, whilst the vertical direction shows the automated output classifications from the network. The green diagonal represents correct, matching classifications: for example (indicated, red box) 4,000 'binucleate' images, representing 39.6% of the total test image set, were classified correctly. Away from this diagonal, misclassifications are shown e.g., (yellow box) 21 images (0.2%) labelled as 'trinucleates' by human scoring were incorrectly classified as 'binucleates' by the network. In the bottom-right corner (green box) the overall network accuracy and overall misclassification rate are shown for all nine classes (94.4% and 5.6%, respectively). In the white squares down the right-hand side of the matrix, the network precision *i.e.*, true positive / (true positive plus false positive) (green percentages) and the false discovery rate *i.e.*, 100-precision (red percentages) are shown for each classification. The horizontal bottom white row shows the network sensitivity *i.e.*, true positive / (true positive plus false negatives) (green percentages) and false negative rates (red percentages), respectively. Therefore – by example – 95.4% of the images classified as binucleates by the network were binucleates by human-scoring (blue box) whereas the trained model can be expected to correctly assign the binucleate class 98.6% of the time (magenta box). Scale bars equal 5 microns



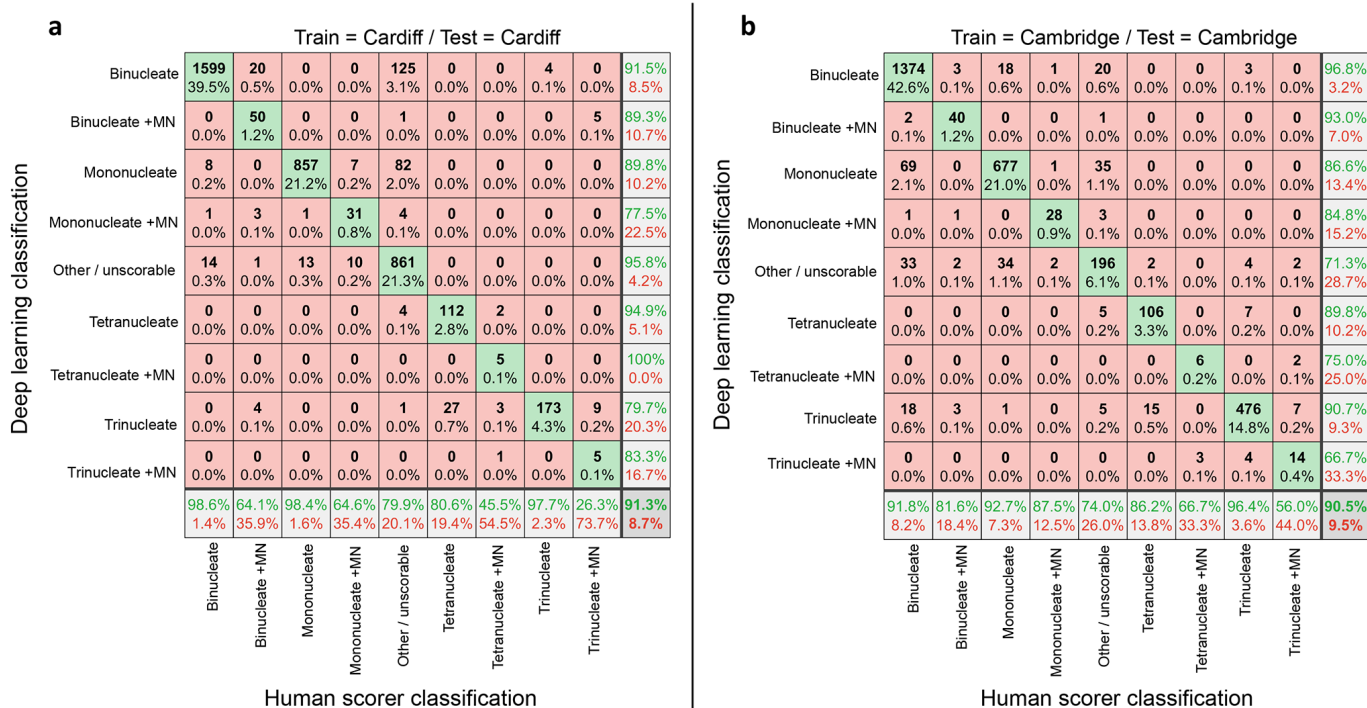
372 First, we tested the ability of a network trained on one laboratory's data to work well for unseen data  
373 from that same laboratory (*i.e.*, 'single-laboratory testing') using imaging flow cytometry data  
374 collected at either Cardiff or Cambridge (**Fig. 2**). In this single laboratory context, images were  
375 randomly assigned to training (60%) and unseen testing (40%) groups. In both instances, the overall  
376 accuracies within this single-laboratory context were very high (91.3% and 90.5% for Cardiff and  
377 Cambridge, respectively). However, the compiled test sets were quite imbalanced in terms of the  
378 numbers of images per class, with network performance with some of the sparser classifications less  
379 well represented by the metric of overall accuracy.

380

381 For Cardiff (**Fig. 2a**), whereas accuracy in classification of the common parent nuclei classes (*i.e.*,  
382 mononucleates, binucleates, trinucleates) was generally very good (> 97 %), 20 out of a total of 78  
383 events (~ 25%) human-scored as 'binucleate + MN' were misclassified as 'binucleates' by the  
384 network. Similarly, around 35% of the human-scored 'mononucleate + MN' events were outputted  
385 into the 'mononucleate' or 'other/unscorable' classes, with a further ~ 20% of 'tetranucleated' test  
386 images misclassified as 'trinucleates'. Despite scoring ~10,000 total events from the Cardiff  
387 cytometer, the very rarest cell phenotypes represented by the 'tetranucleate with MN' and  
388 'trinucleate with MN' classes presented at very low frequency (~ 0.27 % and 0.47 %, respectively).  
389 This led to sparsity in the training set which appeared associated with the network missing  
390 micronucleus events, as the 'trinucleate + MN' images were often misclassified into the 'trinucleate'  
391 or 'tetranucleate' classes. In a similar manner, 'tetranucleate + MN' images were often misclassified  
392 into the 'trinucleate' or 'binucleate + MN' categories.

393

394 Similar results were observed within the Cambridge laboratory (**Fig. 2b**). Whereas accuracies with  
395 the 'mononucleate plus MN' and 'binucleate plus MN' classes showed slight improvement when  
396 compared against Cardiff, accuracies with the sparser, micronucleated tri- and tetranucleated cells  
397 again suffered (~ 44 and ~ 33% error rates, respectively).



**Fig. 2 Assessing automated scoring accuracies using intra-laboratory train and test data.** a/b Confusion matrices comparing human scoring versus deep learning image classifications for test image sets of approximately four thousand unseen images. In each instance, the results reflect the outputs from nine-class networks trained and tested exclusively on image-data from one imaging cytometer at either the **a** Cardiff or **b** Cambridge laboratories

398

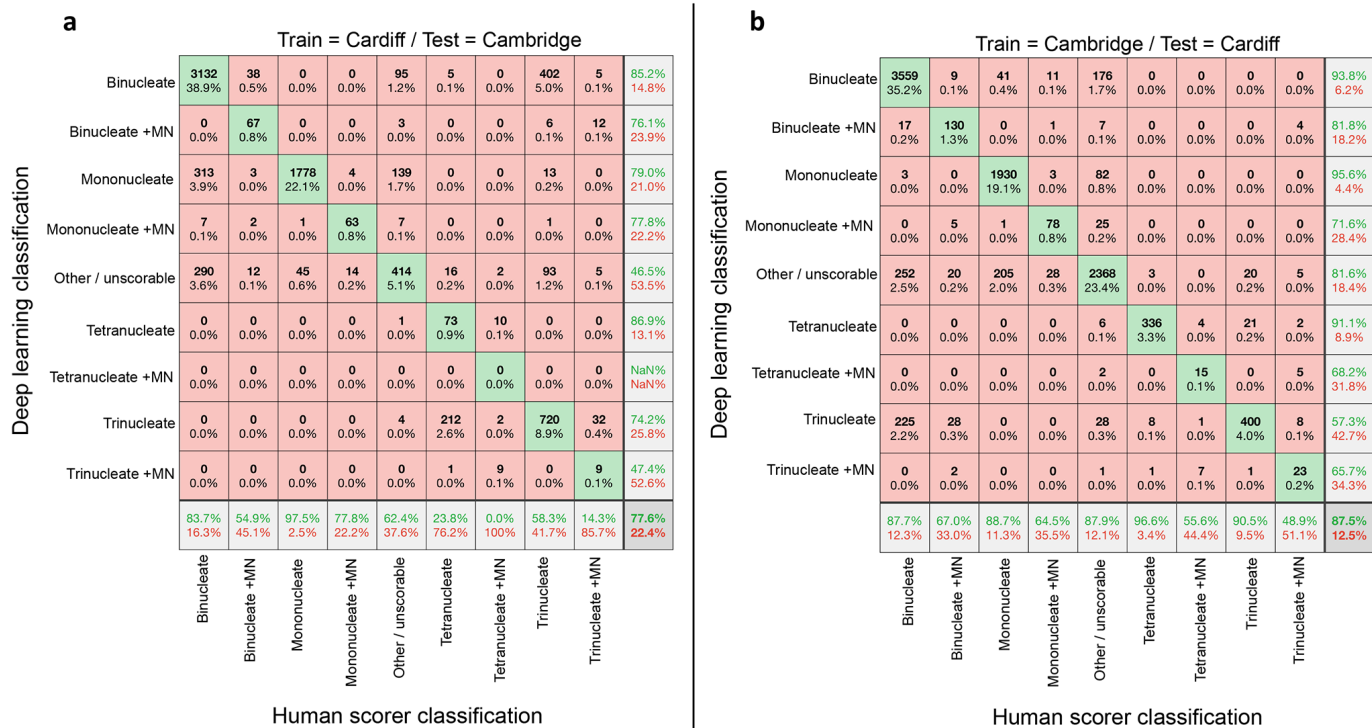
399 We next considered the ability of the networks trained on single-laboratory data to generalise to the  
400 task of scoring the image data collected from the opposite Centre (**Fig. 3**). This was expected to be a  
401 difficult task given that the networks had been trained initially with fairly small numbers of images  
402 and because the two laboratories had utilised different cytometer models (IS<sup>X</sup> vs. IS<sup>X</sup> Mk II) and  
403 nuclear stains (Hoechst at Cambridge or DRAQ5 at Cardiff). This presented the likelihood of  
404 overfitting during training – yielding networks highly adapted to the task of scoring data from that  
405 particular laboratory.

406

407 Despite these factors, at first-glance the overall accuracies appeared quite encouraging at 77.6% for  
408 the Cardiff-trained network classifying the Cambridge images (**Fig. 3a**) and 87.5% for the  
409 Cambridge network classifying Cardiff images (**Fig. 3b**). Comparing across the individual classes, it  
410 was apparent that the Cambridge-trained model generalised slightly better to the task of scoring the  
411 Cardiff data than was observed *vice-versa*. Closer examination however showed that the metric of  
412 overall accuracy was weighted by the prevalence of the easily identified ‘mononucleate’ and  
413 ‘binucleate’ phenotypes, which masked assessment of the ability of the networks to identify the  
414 micronucleated classes representing DNA-damage events (**Fig. 3a/b**). In this regard, in almost all  
415 instances, the accuracy of micronucleated event detection suffered considerably compared to the  
416 results achieved with laboratory-matched test data (**Fig. 2**).

417

418 With these single-laboratory results established, the images from Cambridge and Cardiff were  
419 combined together. This increased the diversity of training exemplifications considerably given the  
420 use of two different nuclear stains, two compounds, different imaging cytometers and no ‘hold out’  
421 requirement for cross validation testing. Training a new DeepFlow neural network on this combined  
422 training set (~ 19,000 images) took approximately one hour using modest hardware (single RTX  
423 2080 GPU). The resulting network was then cross validated using a test set where both the bioassay

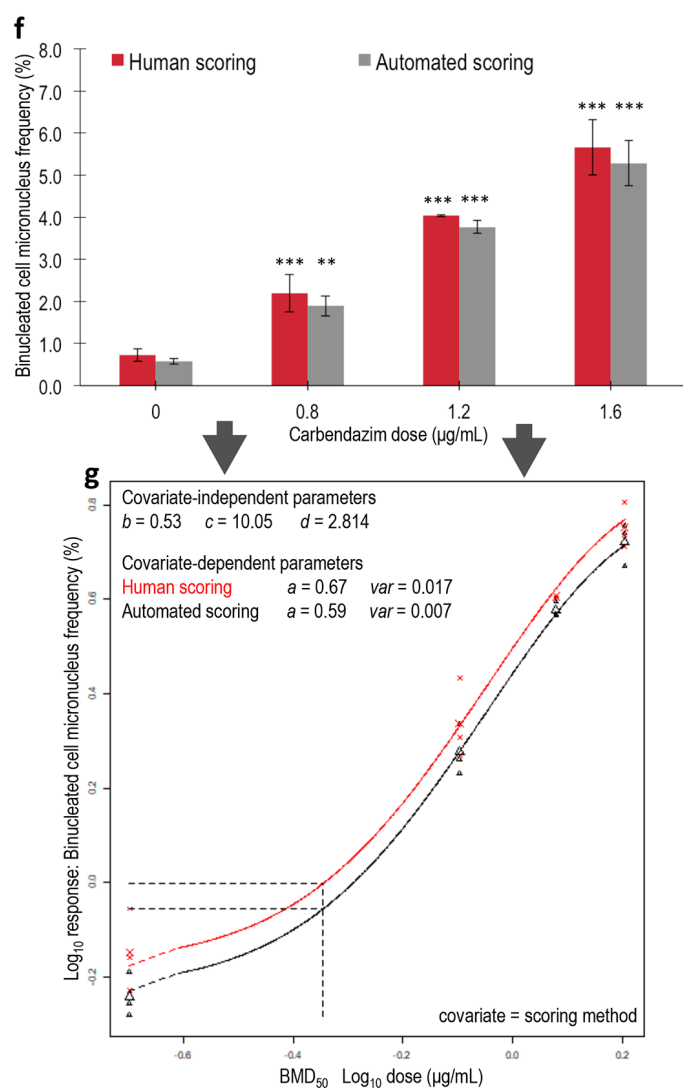
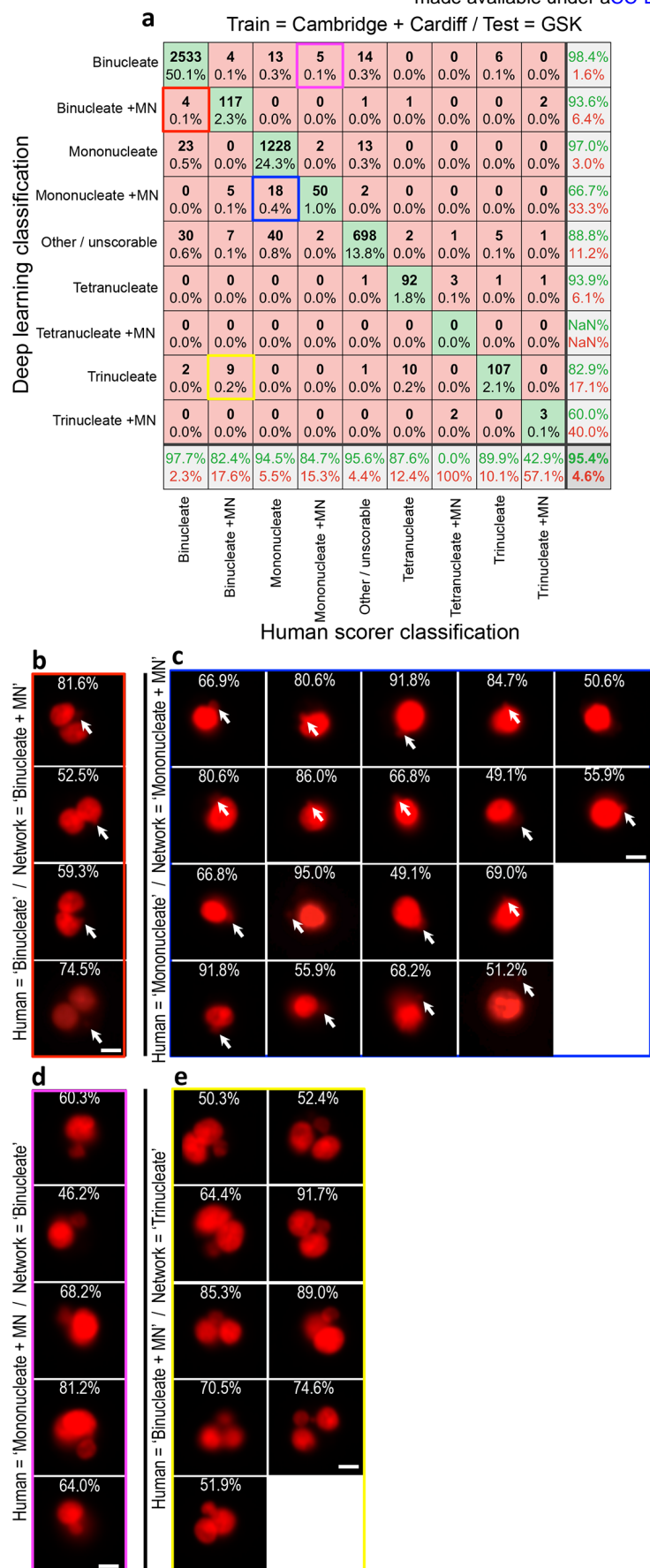


**Fig. 3 Assessment of automated network scoring accuracies using inter-laboratory test data.** **a/b** Confusion matrices comparing human scoring versus deep learning image classifications for test image sets of approximately ten thousand unseen images. In each instance, the results reflect the outputs from nine-class networks trained exclusively on image data from one laboratory's imaging cytometer before cross-validation testing against image data collected at a different laboratory. **a** Network accuracies after training using Cardiff data before testing on unseen Cambridge data. **b** Network accuracies after training on Cambridge data then testing on unseen Cardiff data

424 and imaging cytometry were conducted at an entirely new, third laboratory (GSK). Scoring ~ 5,000  
425 test-images took around six seconds on the RTX 2080 hardware or ~ 82 seconds on a single CPU.  
426 This time, the network showed much better ability to generalise to the task of successfully scoring  
427 the images from the new laboratory (**Fig. 4a**). Across the four core classes central to utilisation of  
428 CBMN assay (*i.e.*, ‘mononucleate’, ‘mononucleate plus MN’, ‘binucleate’ and ‘binucleate plus  
429 MN’), and with no user input or configuration required, the network achieved 98%, 82%, 94%, and  
430 85% accuracies, respectively.

431  
432 We then examined failure cases, starting with 22 instances where the network detected micronucleus  
433 events in cells scored by humans as just mono- or binucleated (**Fig. 4a**). Surprisingly, many did, in  
434 fact, appear to have faint or partially occluded potential micronucleus or nuclear bud events that  
435 would have been extremely difficult for the human scorer to detect (**Fig. 4b/c**). Similarly,  
436 visualisation of cell events scored by humans as either ‘mononucleate with MN’ or ‘binucleate with  
437 MN’, but outputted by the network as ‘binucleate’ or ‘trinucleate’ showed that these images often  
438 contained very large micronucleus events (**Fig. 4d/e**). Indeed, some of these likely exceeded the  
439 upper size limitation typically imposed on micronucleus classifications (*i.e.*,  $\leq 1/3$  diameter of the  
440 parent-nuclei) suggesting additional validity to the network’s outputs.

441  
442 Progressing towards the less frequent cell phenotypes, the accuracies achieved with the ‘trinucleate’  
443 and ‘tetranucleate’ cell classes were also good at 90% and 88% respectively. However, detection of  
444 these cell types with micronucleus events was either quite poor or failed entirely. Again, this  
445 outcome was likely related to extreme sparsity in occurrence ( $< 0.25$  % frequency in the training  
446 data). In an attempt to improve accuracies with these classes, we tried both class weighting the  
447 classification layer and combining tri- and tetranucleated events with and without micronucleus  
448 events into a single, ‘polynucleated’ class (**Supp. Figure 2**). Whereas both strategies somewhat  
449 improved the classification accuracies with these rare events, they were also found to compromise



**Fig. 4 Network accuracy and dose-response assessment using unseen test data from a new laboratory.** **a** Confusion matrix showing human versus deep learning image classifications for a test image set of approximately five thousand unseen images. Here, the neural network was trained using image data from both the Cambridge and Cardiff laboratories before testing on new, unseen imaging cytometry data acquired at a third laboratory (GSK). **b** Cell events human scored as 'binucleates' but classified as 'binucleate plus MN' by the neural network (*i.e.*, red square in **A**). **c** Cell events human scored as 'mononucleates' but classified as 'mononucleate with MN' by the neural network (*i.e.*, blue square in **a**). **b/c**, Close examination of the purportedly misclassified cells shows that many display indistinct events that might be micronucleus or nuclear buds missed by the human scorer (indicated, white arrows). **d** Cell events human scored as 'mononucleate with MN' but classified as 'binucleate' by the neural network (*i.e.*, magenta square in **a**). **e** Events human scored as 'binucleate with MN' classified as 'trinucleate' by the neural network (*i.e.*, yellow square in **a**). **d/e** In both instances, some of the human-scored micronucleus events encroach upon the 1/3 parent nuclei upper-size limitation typically imposed on micronucleus classifications. **b-e** For each event, the white percentages represent neural network confidence in the outputted classification. **f** Binucleated-cell micronucleus frequencies for a three dose plus control dose-response experiment performed in triplicate for carbenzimidazole exposure to TK6 cells. Scores were established from image sets of 2,000 events per replicate by human scoring or by the cross-validated network established in (**a**). (\*) (\*\*) (\*\*\*) indicate statistical significance relative to control at  $p < 0.05$ ,  $p < 0.01$  and  $p < 0.001$  respectively. **g** Covariate benchmark (BMD) dose modelling using dose-response data from either the human (black) or automated neural network (red) scores established in (**f**). The horizontal and vertical dashed lines represent interpolation to determine the equipotent, benchmark dose for a benchmark response size of 50%. Regardless of human or automated scoring, the model predicts the same benchmark dose. Scale bars equal 5 microns

450 the accuracies achieved with one or more of the four core phenotypes more central to successful  
451 CBMN assay scoring.

452

453 Given that the frequency of binucleated cells with or without micronucleus events represents the core  
454 readout for successful DNA damage assessment by the CBMN assay, after validating the network we  
455 proceeded to assess the binucleated-cell micronucleus frequency for a three dose plus control  
456 experiment conducted in triplicate with carbendazim at the GSK laboratory. For each dose and  
457 replicate, 2000 cell images were scored both manually and automatically. Visually, the resultant  
458 dose-response relationships appeared similar across the human and neural network scoring  
459 approaches, with the human scores consistently fractionally higher for each dose-group (**Fig. 4f**). To  
460 better understand the consequences of this using a recognised, quantitative framework for genotoxic  
461 potency estimation, the dose-response relationships were fitted using both the exponential and the  
462 Hill model families recommended for the assessment of continuous toxicity data using Benchmark  
463 Dose (BMD) analysis (Hardy et al. 2017). With scoring method specified as a potential covariate,  
464 model fitting with the PROAST package resulted in covariate-dependent parameterisation for the  
465 background response (parameter  $a$ ) and for within-group variation ( $var$ ). For both model families,  
466 this parameterisation subsequently allowed rejection of scoring method as covariate, yielding the  
467 *same* estimation for the equipotent, benchmark dose from both manual and automated methods (**Fig.**  
468 **4g**). Model fits to the data are presented in **Supp. Figure 3**.

469

470

## 471 **DISCUSSION**

472 The CBMN assay represents a globally significant method for the identification and quantification of  
473 chromosomal damage (Fenech 2000; Fenech 2020; OECD 2016). Its utility reaches beyond  
474 regulatory compound screening to encompass inter-individual monitoring of wide-ranging lifestyle,  
475 occupational and environmental factors (Fenech 2020; Kirsch-Volders et al. 2011; Wang et al.

476 2019). Despite this, continued reliance upon time-consuming and user-subjective manual scoring  
477 represents a bottleneck to broadening practical utilisation (Seager et al. 2014; Verma et al. 2018;  
478 Verma et al. 2017). In this pilot study, we show that rapid image acquisition by imaging flow  
479 cytometry in conjunction with deep learning image classification represents a capable platform for  
480 automated, inter-laboratory operation. We share our strategy via openly accessible frameworks.

481  
482 As an image acquisition method, imaging flow cytometry is now well established as a means for  
483 high-throughput CBMN data capture with concomitant image archiving potential (Rodrigues et al.  
484 2014a; Rodrigues et al. 2016a; Rodrigues et al. 2018). Moreover, this is achieved with simple sample  
485 preparation involving a single nuclear stain and brightfield to provide the context that events lie  
486 inside parent cells (Rodrigues et al. 2018). Comparison studies have shown that the captured images  
487 contain dose-response information that aligns to results obtained from ‘gold standard’ manual  
488 microscopy scoring (Verma et al. 2018). Whereas conventional flow cytometry offers faster  
489 throughput, it lacks this image-based validation whilst additionally requiring cell lysis. This prevents  
490 utilisation of the cytokinesis-block version of the assay with its associated advantages such as robust  
491 utilisation of primary human cell lines, knowledge that cells have divided during the test period and  
492 quantitation of mononucleated, binucleated and different classes of multinucleated cells. This  
493 information is useful in the avoidance of misleading negative results and additionally enables  
494 calculation of division and replication indexes that contribute to assessments of mitogen response  
495 and cytostatic impact (Rodrigues et al. 2018).

496  
497 Beyond image collection, automated scoring of imaging flow cytometry data – as with other  
498 automated microscopy strategies – has thus far largely relied upon traditional, threshold-based image  
499 classification techniques. These require image analysis expertise to implement, alongside user-  
500 configuration and tuning to maintain performance (Rodrigues et al. 2018; Seager et al. 2014; Verma



501 et al. 2017). Unfortunately, much as with traditional manual scoring, this is time-consuming and  
502 subjective.

503  
504 In contrast, once successfully trained, the results achieved here suggest that deep learning image  
505 classification has the potential to eliminate these expertise and user-input requirements, dramatically  
506 reducing the time to results. This comes from encompassing image diversity during network training  
507 and harnessing it to improve the consistency and robustness of subsequent classifications. To this  
508 end, here we show that utilisation of diverse training data curated across two laboratories utilising  
509 different nuclear stains, multiple compounds and two different cytometer models yielded a capable  
510 neural network for scoring automation. Without user configuration, the network was able to classify  
511 data collected from an entirely new laboratory with > 82% accuracy for each of the four cell  
512 phenotypes central to CBMN performance (*i.e.*, mononucleate and binucleate cells with or without  
513 micronucleus events) in addition to successfully classifying tri- and tetranucleated cells (> 88%  
514 accuracy) and unscorable events (96% accuracy). Importantly, these seven classes encompassed  
515 virtually all of the cell images encountered (>99%). Success at micronucleus detection in both  
516 mononucleate and binucleate cell classes further suggests that this single network could be used to  
517 automate scoring of both mononuclear and cytokinesis-block versions of the assay.

518  
519 Despite this success with the assay classes central to CBMN scoring, the scarce, tri- and  
520 tetranucleated phenotypes with micronucleus events proved more challenging. Commonly employed  
521 methods such as class weighting or class combination offered little in the way of accuracy  
522 improvements, and often compromised accuracy with the other classes. These findings suggest that  
523 significant increases in the representation of these sparse events during training will likely be  
524 required to improve success. In this context, imaging flow cytometry is well suited to examine  
525 whether an improved image bank leads to enhanced accuracy in scoring given the high rates of  
526 image capture achievable. Our results also suggests that class reduction does not necessarily simplify

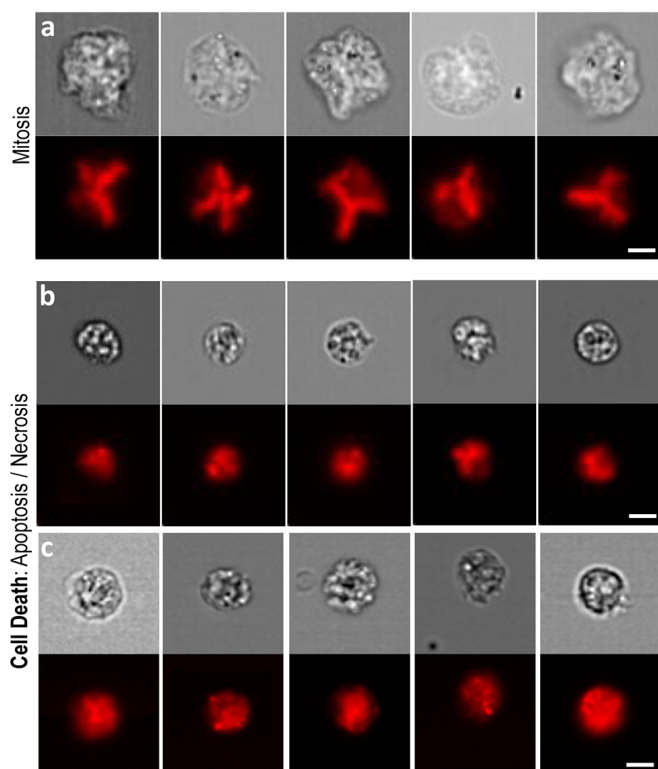
527 the classification problem and may instead cause ambiguities. In this way, future expansions to the  
528 number of classes to encompass all distinctive cellular phenotypes may represent a route to  
529 improving overall network performance.

530

531 In this regard, we identified additional, potentially-scorable cell phenotypes (**Fig. 5**). In particular,  
532 cell death events (*i.e.*, due to apoptosis and necrosis) were visually apparent, but we were unable to  
533 determine apoptotic from necrotic events using just the brightfield and nuclear fluorescence images  
534 alone. Cells caught during mitosis also represented distinctive events. At the same time, we were less  
535 convinced that more subtle phenotypes relevant to the expanded, CBMN cytome assay such as  
536 nuclear buds and bridges could reliably and consistently be detected – given the relatively low  
537 resolution of the image data (Fenech 2007). However, it is important to note that previous studies  
538 demonstrating capture of these phenotypes by imaging flow cytometry have utilised both the 60X  
539 ImageStream objective lens in addition to hypotonic treatments to swell cell volumes prior to  
540 imaging (Rodrigues 2019; Rodrigues et al. 2018). Hypotonic treatments were not used here but may  
541 improve image capture of these more subtle phenotypes. With regards to network class expansion to  
542 encompass these events – or, indeed for simultaneous measurement of other endpoints – the  
543 ImageStream platform is capable of multiplexed imaging. Additional channels might therefore be  
544 used to simultaneously measure other DNA-damage pathways (*e.g.*, YH2AX for DNA double-strand  
545 breaks (Smart et al. 2011)), or to improve the reliability of ground truth image curations through use  
546 of additional fluorescent markers to differentiate events such as apoptotic from necrotic cells.

547

548 Manual scoring of the images for this experiment was more challenging than the exemplar images  
549 shown might suggest. Fundamentally, the acquired images are relatively low resolution (*i.e.*, cells  
550 occupy ~ 64x64 pixels) and further image degradation is always present as a result of the capture of  
551 moving objects by time delay integration. The acquired images also represent a central, 2-D  
552 projection of a 3-D cell-object. This means that nuclei and micronucleus events may overlap each



**Fig. 5 Other scorable cell phenotypes captured by imaging flow cytometry.** **a** Cells undergoing mitosis were visually apparent according to metaphase spread-type nuclear fluorescence imagery (red) alongside large, brightfield-delineated cell sizes (grey). **b/c** Cell death events displayed shrunken cell sizes in conjunction with granular brightfield and fluorescence imagery. In the case of cell death, two distinctive cell phenotypes appeared visually separable according to cell size and the number, size and extent of nuclear foci formation (**b** versus **c**). Whether these observations represented distinct apoptotic versus necrotic events was unclear from the nuclear fluorescence and brightfield information alone. Scale bars equal 5 microns

553 other, or they may lie outside of the plane of optimal focus (Rodrigues et al. 2018). These factors all  
554 served to make ground truth assignments more complicated, even for experienced CBMN scorers.  
555 Whereas network accuracy assessments by confusion matrix provided a more representative  
556 breakdown of outputs when compared to simplistic overall accuracy measures, it is a relatively  
557 stringent success measure because any ambiguity in human score assignment is not captured. A  
558 potential advantage of automated network classification approach is therefore likely greater  
559 consistency – even in error – than arises from manual scoring.

560  
561 Regarding image focussing, the ImageStream platform offers ‘extended depth of field’ (EDF)  
562 technology, whereby image deconvolution is used to improve the utility of out of focus events  
563 through projection onto a single plane (Ortyn et al.). Whereas previous studies have shown this  
564 technique can improve accuracy in ‘spot counting’ applications, the strategy has been reported less  
565 helpful for the provision of improved CBMN data (Parris et al. ; Rodrigues 2018; Rodrigues et al.  
566 2014a). This was attributed to a slight degradation in overall image resolution, compromising  
567 differentiation of micronucleus events from parent nuclei (Rodrigues 2018). On a similar theme, the  
568 ImageStream platform is also configurable with 20X, 40X or 60X objective lenses. Here, image  
569 collection was via the ‘standard’, 40X objective across all laboratories. This approach was chosen as  
570 previous work has shown that whilst greater resolution is achievable with the 60X objective, focus  
571 depth also decreases, reinforcing the out of plane difficulties described above (Rodrigues et al.  
572 2018).

573  
574 Whilst considering the nature and utility of imaging flow cytometry data, a relevant comparison is to  
575 that provided by other automated imaging methods such as slide scanning platforms. In addition to  
576 the potential for higher resolution imaging, here an overlooked advantage comes from the ability to  
577 use slide-based preparations created by cytocentrifugation. This technique causes the flattening and  
578 spreading of cellular content, presenting nuclear objects on a more two dimensional plane (Fitzgerald

579 and Hosking 1982; Shanholtzer et al. 1982). From a practical perspective however, this also  
580 necessitates the consistent preparation of high-quality slides with optimal cell densities (Rodrigues et  
581 al. 2018). Meanwhile, a major advantage of the imaging flow cytometry approach is that single cell  
582 image data is inherently acquired by the fluidics-based processing of individualised cells.

583

## 584 **CONCLUSIONS**

585 As a platform for the CBMN assay, imaging flow cytometry combines the high throughput and  
586 multiplexing potential of flow cytometry with the image-based validation and archiving attributes of  
587 automated microscopy. Here we demonstrate accurate, automated assay scoring using a neural  
588 network for data collected in a laboratory wholly separate to that in which the algorithm was trained.  
589 This proves that without any human configuration, the machine is able to correctly anticipate the  
590 decisions of the expert human on unseen images in a new setting. For the first time, this suggests the  
591 possibility for generalised scoring automation through dissemination of a pretrained network for the  
592 ImageStream platform established from ground truth agreed by a single, expert group. Such an  
593 approach would provide the ultimate in terms of standardisation and result reliability, but more  
594 importantly could enable adoption of the assay beyond current practitioners as local expertise in  
595 scoring and/or image analysis would no longer be required. For these reasons, we believe that full  
596 development of this automated, accessible, inter-laboratory approach would represent a truly twenty-  
597 first century method with significant potential to transform CBMN utility across industry, research  
598 and clinical domains.

599

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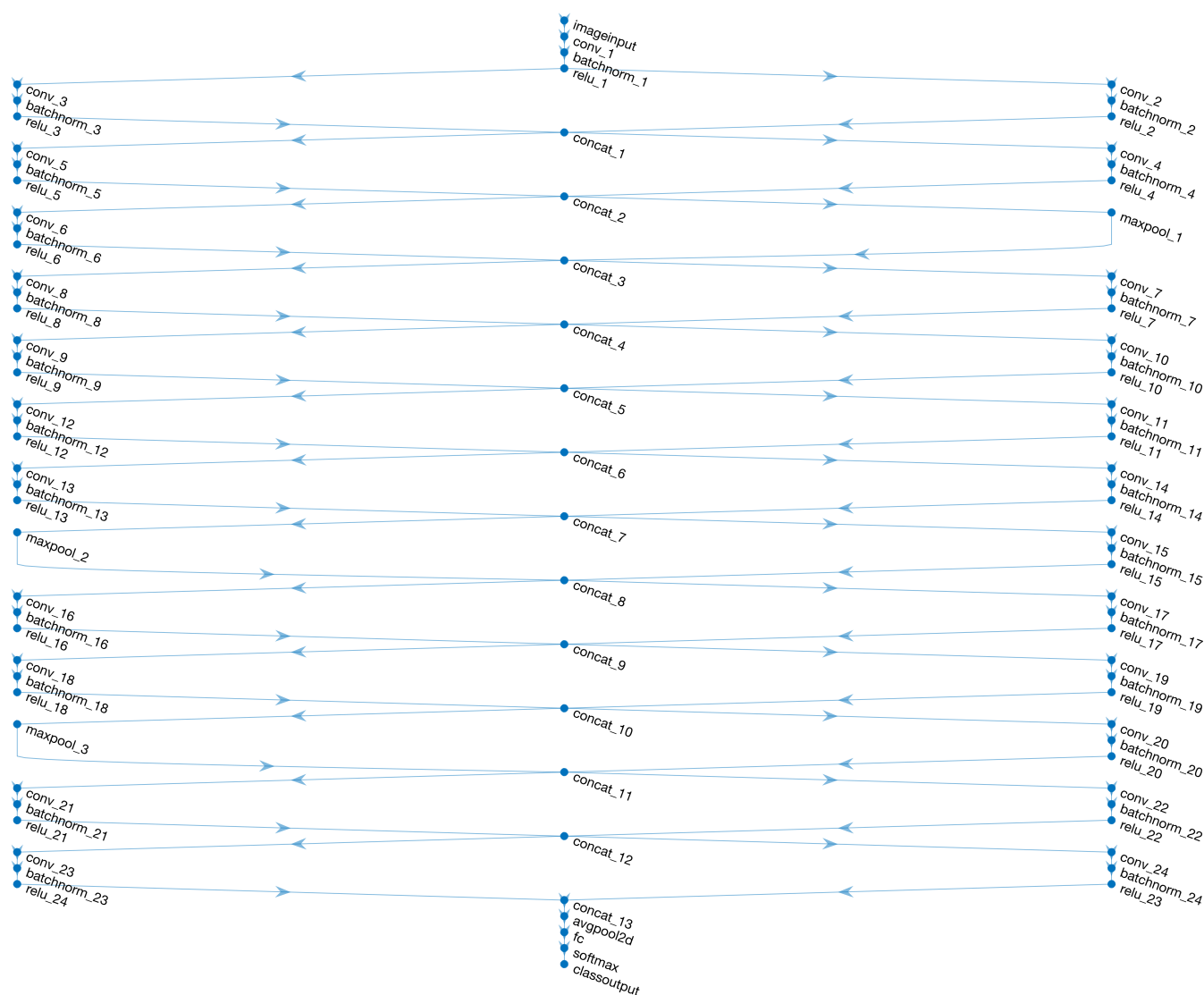
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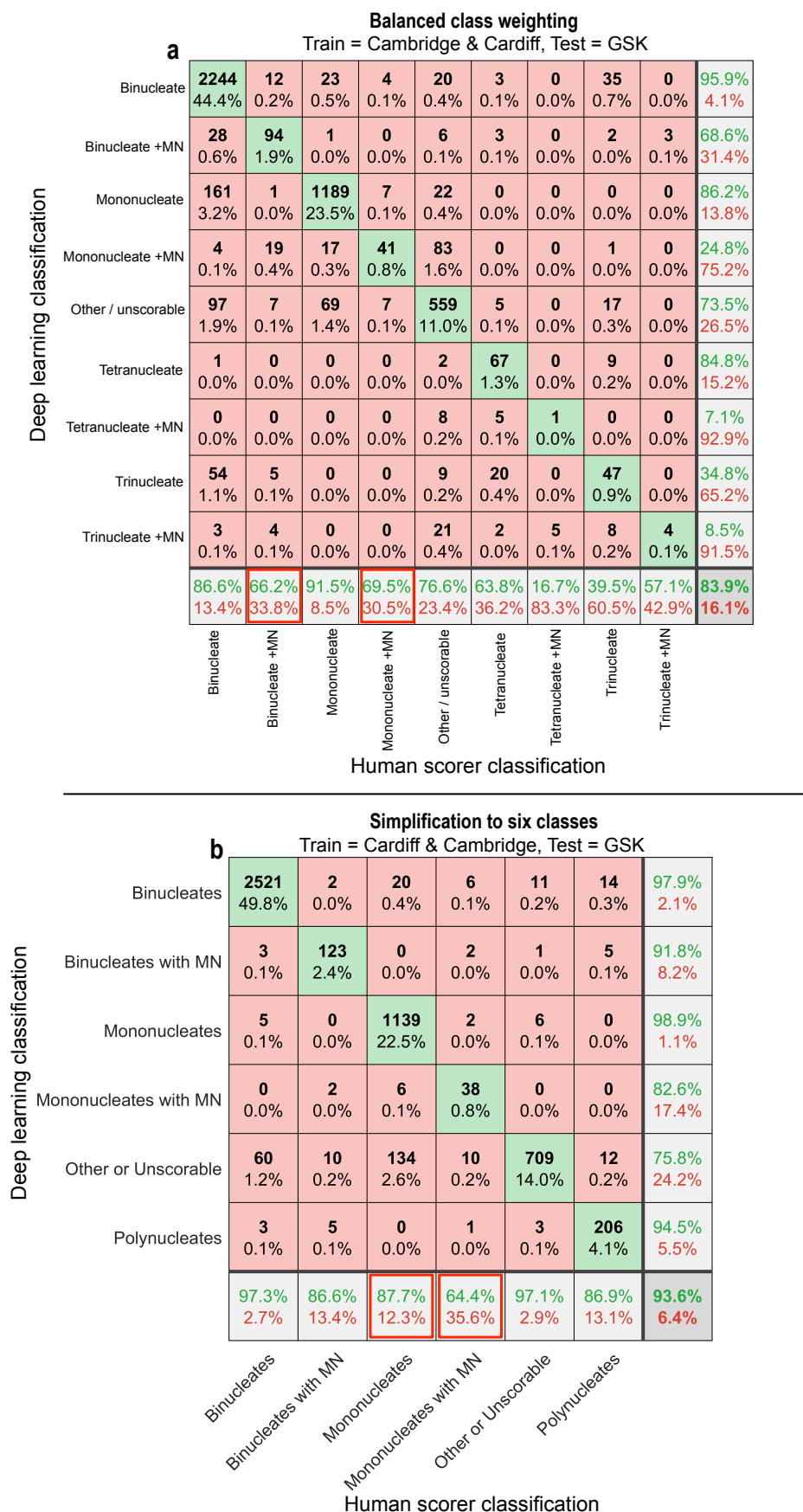
**Supp. Table 1 – Imaging flow cytometry data acquisition information**

<b>Centre</b>	<b>Excitation laser (nm)</b>	<b>Intensity (mW)</b>	<b>Brightfield channel</b>	<b>Nuclear fluorescence channel</b>	<b>Nuclear stain</b>	<b>Objective lens</b>	<b>Cytometer Model</b>
Cambridge	405	50	Ch04	Ch01	Hoechst 33342	40X	Amnis ImageStream <sup>x</sup>
Cardiff	488	100	Ch01	Ch11	DRAQ5	40X	Amnis ImageStream <sup>x</sup> MkII
GSK	642	55	Ch01	Ch11	DRAQ5	40X	Amnis ImageStream <sup>x</sup> MkII

Image data were collected using three different imaging flow cytometers located across three laboratories (Cambridge, Cardiff and GSK). At each laboratory, the choice of fluorescent nuclear stain depended upon local protocols and compatibility with the cytometer's laser configuration.

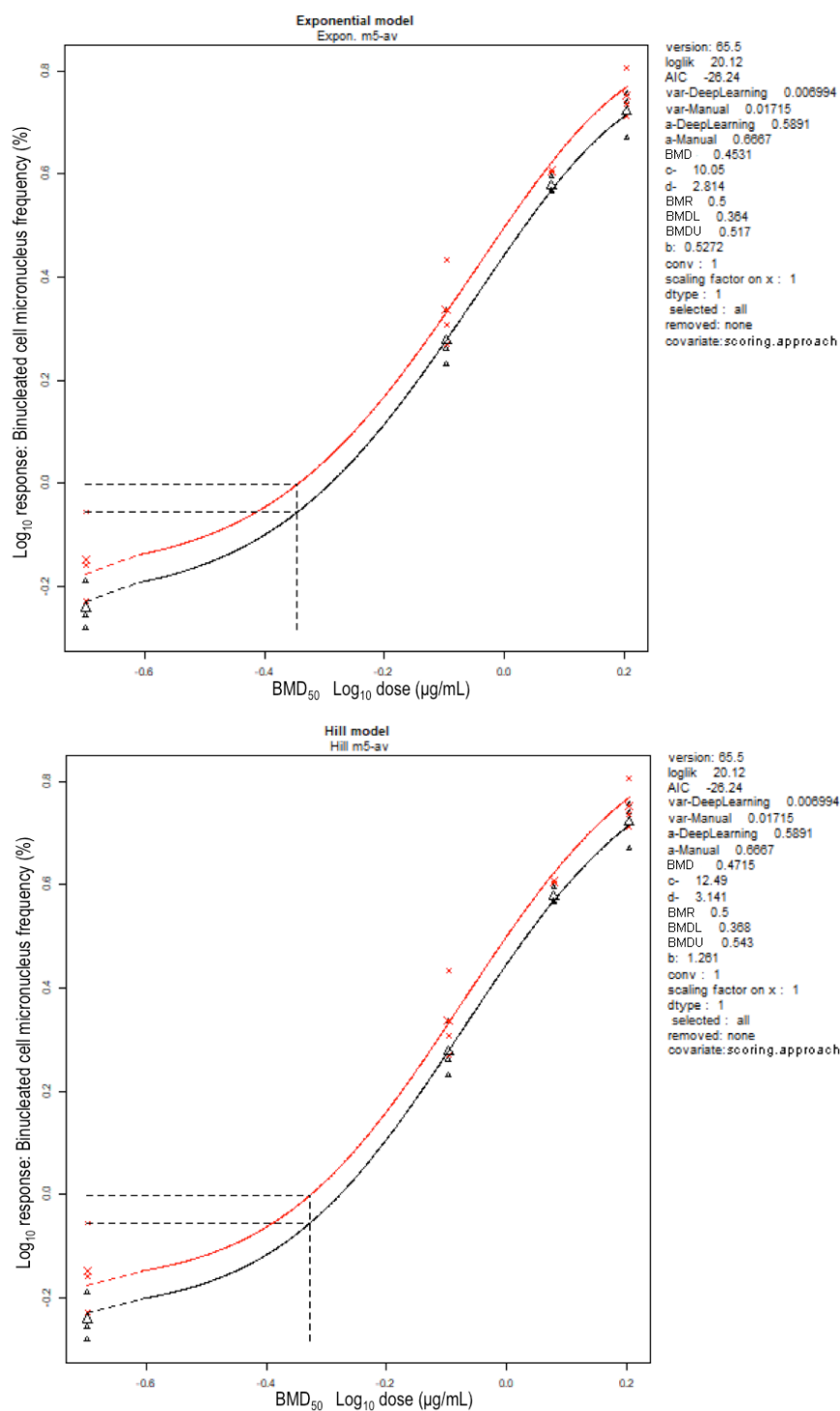


**Supp. Figure 1** DeepFlow neural network architecture schematic. The DeepFlow network utilises a 64x64x2 input layer (x, y, channels) followed by repeating dual-path subunits from the “Inception” architecture to aggregate visual information over increasing scales. The number of kernels used increases at each layer, yielding 336 features maps with size 8 x 8 before average pooling, the fully connected (fc) layer and softmax classification using cross-entropy loss.



**Supp. Figure 2** Cross validation testing using class weighting or class simplification strategies. **a/b** Confusion matrices comparing human scoring versus deep learning image classifications for a test set of ~ 5000 unseen images. In each instance, the results reflect the outputs after training using image data from both the Cambridge and Cardiff laboratories before cross validation on new imaging cytometry data acquired at a third laboratory (GSK). In **a** class weighted cross entropy loss was used at the classification layer in an attempt to improve performance with the sparsely-represented phenotypes (*i.e.*, tri and tetranucleates with or without micronucleus (MN) events). In **b** these sparse, multinucleated categories were combined together into a single 'polynucleated' class. Whilst some improvements were realised using these strategies, they both reduced achieved accuracies (indicated, red squares) with one or more of the four, core phenotypes central to successful CBMN scoring (*i.e.*, mono or binucleated cells with or without MN events).





**Supp. Figure 3** Benchmark dose (BMD) analysis using exponential and Hill model families. The curves represent fits to micronucleus dose-response data obtained either by human (red) or neural network (black) scoring using either the exponential (top) or the Hill (bottom) model families. Both models were fitted with covariate (scoring method) dependent parameters for the background (parameter  $a$ ) and within-group variance ( $var$ ), whilst constant parameters could be used for potency, shape and steepness (parameters  $b$ ,  $c$  and  $d$ ). Horizontal and vertical dashed lines represent interpolation at a benchmark response (BMR) size of 50% to determine the  $BMD_{50}$  (respectively).