

# 3D printed pacifier-shaped mouthpiece for fMRI-compatible gustometers

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## Abstract

Gustometers have allowed the delivery of liquids in fMRI settings for decades and mouthpieces are a critical part of those taste delivery systems. Here we propose an innovative 3D printed mouthpiece inspired by children's pacifiers that allow participants to swallow while lying down in an MRI scanner. Our results validate the effectiveness of our method by showing significant clusters of activation in the insular and piriform cortex which are regions that have been consistently identified to compute taste processing. We used a large sample (n=85) to validate our method. Our mouthpiece fulfills several criteria guaranteeing a gustatory stimulus of quality, making the delivery more precise and reliable. Moreover, this new pacifier-shaped design is: simple and cheap to manufacture, hygienic, comfortable to keep in mouth, and flexible to diverse use cases. We hope that this new method will promote and facilitate the study of taste and flavor perception in the context of reward processing in affective neuroscience and thus help provide an integrative approach to the study of the emotional nature of rewards.

*Keywords:* Mouthpiece, gustometer, fMRI, taste, flavor

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# 1 Introduction

2 Studying the neuronal pathways of chemical senses (i.e., olfaction and  
3 gustation) requires special equipment. However, it is relatively easy to make  
4 olfactometers (e.g. Coppin, 2020), and the same statement may be even more  
5 true for gustometers (e.g. Canna et al., 2019).

6 The gustometer is a tool specifically designed to deliver liquids. Some  
7 gustometers have been used for almost 20 years (e.g. O’Doherty et al., 2002;  
8 Small et al., 2003). However, mouthpieces, which are a critical part of the  
9 gustatory delivery system (Andersen et al., 2019; Canna et al., 2019), have  
10 not been much updated, whereas the number of publications on the topic  
11 have kept increasing over the years (see Fig. 1).

12

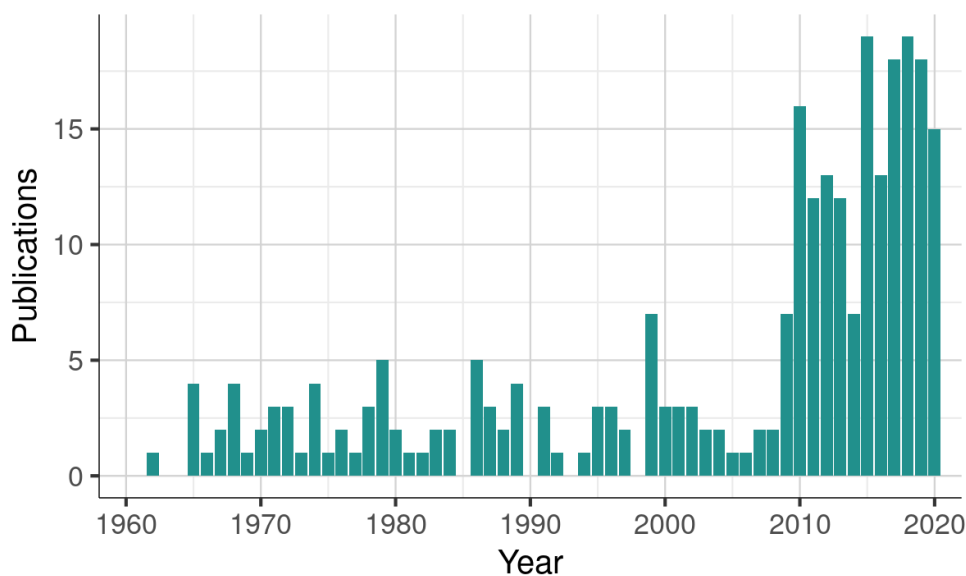


Figure 1: **Publications listed on Google Scholar.** Results returned when queried with the search terms involving a ‘gustometer’. Results show a clear increase of the number of publication over the years, culminating with over 300 publications on 2020.

13 Here, we propose an innovative 3D printed MRI-compatible mouthpiece  
14 which fulfills several criteria guarantying a gustatory stimulus of quality.  
15 First, this new mouthpiece (see Fig. 2) allow participants to swallow while  
16 lying down in a scanner, with their heads immobilized in a given position

17 and can remain comfortably in the mouth for an considerable amount of  
18 time without requiring any particular effort. Indeed this design –inspired by  
19 children’s pacifiers– removes the need for the participant to apply pressure  
20 on a 'biting stick 'with their teeth and to have to take into account individual  
21 dental impressions (e.g. Goto et al., 2015). Second, the mouthpiece permits  
22 to deliver up to 8 different liquids in a precise and consistent manner in the  
23 center of the tongue. This make it possible to control location delivery, thus  
24 minimizing somatosensory variations.

25  
26 The mouthpiece can be available to any laboratory having access to a 3D  
27 printer or could otherwise get them from any 3D printing service company  
28 since our plans are made freely available. It can be manufactured in quantity  
29 for a very low price (0.5 USD\$ of material per piece). This makes it intrinsi-  
30 cally hygienic since each participant uses a mouthpiece specially printed for  
31 them. Moreover, the printing material can easily be adapted to match differ-  
32 ent countries’ sanitary regulations. Ours were made out of natural polylactic  
33 acid (PLA) compatible with use in contact with food (Conn et al., 1995).  
34 Finally, it does not require to modify any pre-existing apparatus and will fit  
35 to most gustometer setups seamlessly.

## 36 1.1 Mouthpiece description

37 The mouthpiece inspired by children’s pacifier consists of three parts: a  
38 mouth shield, an elongated teat and a tube guide. These three pieces are  
39 printed separately in natural PLA, a biodegradable plastic made from corn.  
40 Other plastics can be used but it remains the responsibility of the researcher  
41 to comply with the health standards of the country in which he or she is  
42 conducting the experiments with this mouthpiece.

43  
44 An oval mouth shield (Fig. 2A) holds the mouthpiece comfortably on  
45 the lips thanks to its curvature adapted to the morphology of the face. A  
46 cylindrical teat (40 mm long x 22 mm diameter) is inserted and clipped  
47 on the centre of the mouth shield. This teat receives the tubes at one ex-  
48 tremity and directs the liquids to the tongue (Fig. 2B). The part that goes  
49 into the mouth and is intended to come into contact with the tongue is  
50 bevelled on one side and rounded on the other. This allows for easy con-  
51 tact of the tongue on the teat to deliver drops of liquid comfortably and

52 accurately. Depending on research needs, up to 8 tubes with an external  
53 diameter of 2.5 mm ( $\pm 0.3$  mm) can be inserted into the teat. The last  
54 piece is a tube guide (Fig. 2C) that is clipped onto the mouth shield and  
55 allows the tubes to be at a 90° angle so that they run along the body of the  
56 participant lying on the MRI bed (Fig. 2D). The 3D printing files (stl) that  
57 we supply ([https://github.com/munoztd0/Mouthpiece\\_gusto](https://github.com/munoztd0/Mouthpiece_gusto)) include seven  
58 versions with a diameter of 2.5 mm  $\pm 0.3$  mm in steps of 0.1 mm. All these  
59 versions make it possible to choose the parts that fit together best according  
60 to the 2.5 mm tubes used by the researchers and allows to adjust for different  
61 types of liquid or viscosity levels.

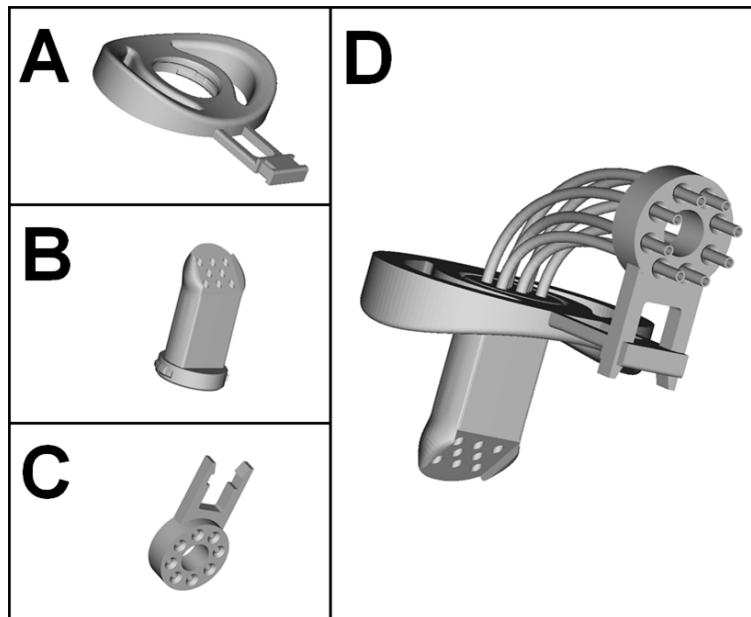


Figure 2: **3D representation of the fMRI compatible mouthpiece.** Detailed 3D representation of (A) the mouth shield , (B) the mouthpiece, (C) the tube guide and (D) the complete mouthpiece assembled with 8 tubes.

## 62 **2 Method**

### 63 **2.1 Participants**

64 This study was part of a larger experiment that was related to a differ-  
65 ent study question (reward processing) in which 97 right-handed participants  
66 were recruited. The study was approved by the Swissmedic ethical commit-  
67 tee. All participants gave written informed consent and received 200 Swiss  
68 francs for their participation to the whole session. In total, 12 participant  
69 were discarded from the analysis because of missing or incomplete data (5  
70 MRI and 7 behavioral).

71  
72 We report data on the 85 remaining participants (55 female; mean age,  
73  $37.3 \pm 12.4$ ; min–max, 18–67 years). No predetermined sample size was esti-  
74 mated via statistical methods. None of the participants have reported having  
75 any kind of olfactory disorder. All participants were asked to have fasted  
76 overnight to our experiment that happened in the morning.

### 77 **2.2 Preparations**

78 Milkshake preparations were made from a mix of milk (300 g) and ice  
79 cream (60 g) for a total of 71 kcal/100 g. Potassium chloride (KCl, 1.8 g)  
80 and sodium bicarbonate (NaHCO<sub>3</sub>, 0.21 g) were diluted in 1L of distilled  
81 water to recreate an artificial tasteless saliva solution. This main solution  
82 was then used to create less concentrated preparations to be able to further  
83 match each individual’s perception of a tasteless solution. In total, there were  
84 4 different tasteless concentrations (1/1, 3/4, 1/2 and 1/4) and 3 flavors of  
85 milkshake (strawberry, chocolate or vanilla). Each participant was asked  
86 which flavor of milkshake they preferred as well as which saliva solution they  
87 found more neutral. This two solution where then used as the main two  
88 stimuli for the rest of the experiment.

### 89 **2.3 Gustometer**

90 Single channel syringe pumps (Chemyx OEM) were used to achieve high  
91 flow control. Two syringes of up to 60 mL were connected via 8 meters

92 length polyurethane food grade tubing (external diameter = 4 mm, inner  
93 diameter = 2.5 mm) to 1 meter length food grade PTFE tubing (external  
94 diameter = 2.5 mm, inner diameter = 1.9 mm) and then to the mouthpiece  
95 at a delivery rate of 1 mL/s. The syringe pumps were connected to a 16-port  
96 RS-232 rackmount device server (Moxa, Nport 5610) and then controlled via  
97 TCP/IP using specific C libraries designed for stimulus presentation software  
98 (E-prime, Matlab or python). While it is out of the scope of this paper but  
99 readers can refer to (Andersen et al., 2019; Canna et al., 2019; Haase et al.,  
100 2007) for detailed instructions on how to setup a MRI-compatible gustometer.

## 101 **2.4 Taste Reactivity Task**

102 An taste reactivity test was administered while participants were lying  
103 in the scanner. The task consisted in the evaluation of the perceived pleas-  
104 antness and intensity of two different stimuli: a milkshake and a tasteless  
105 solution. We chose individually adjusted tasteless solution as control stimu-  
106 lus instead of plain water because water has been shown to have an inherent  
107 taste (Bartoshuk et al., 1964). Each trial consisted on the administration  
108 of 1 mL of the solution and the delivery order of the two conditions were  
109 randomized within each participant. Participants were asked to keep the  
110 solution on their tongue for 4s before swallowing to avoid adding movement  
111 noise to the fMRI response. The experimental trials were intertwined with  
112 rinse trials to cleanse the participants' palate with 1 mL of water.

113  
114 All 40 evaluations (20 per solution) were done on visual analog scales dis-  
115 played on a computer screen. Participants had to answer through a button-  
116 box placed in their hand. The visual scales for the intensity report ranged  
117 from “not perceived” to “extremely intense”; and from “extremely unpleas-  
118 ant” to “extremely pleasant” for liking ratings.

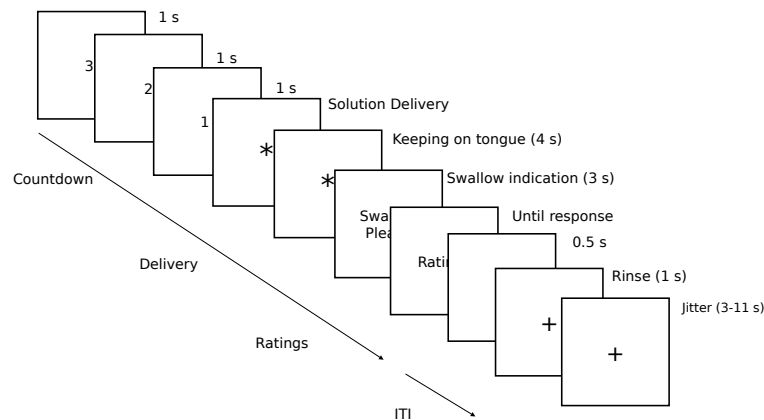


Figure 3: **Task procedure.** The sequence of the taste reactivity test administered while participants were lying in the scanner. After a brief countdown, the participants were shown an fixation cross followed by the delivery of either a milkshake or a tasteless solution. They were asked to keep the solution on their tongue for 4s and then indicated to swallow it. At this moment they were asked their perceived pleasantness and intensity of the solution. The experimental trials were intertwined with rinse trials to cleanse their palate.

## 119 2.5 Data Acquisition

120 The collection of the responses were controlled by a computer running  
121 MATLAB (version R2015a; MathWorks, Natick, USA). The presentation  
122 of the stimuli was implemented using Psychtoolbox (version 3.0). The ac-  
123 quisition of the neuroimaging data was performed via a 3 Tesla Magnetom  
124 TrioTrim scanner (Siemens Medical Solutions, Erlangen, Germany) supplied  
125 with a 32-channel head coil following a gradient echo (GRE) sequence to  
126 record Blood-Oxygen-Level-Dependent (BOLD) signal. We recorded forty  
127 echo-planar imaging (EPI) slices per scan with a isotropic voxel size of 3  
128 mm. Our scanner parameters were set at: echo time (TE) = 20 ms, repeti-  
129 tion time (TR) = 2000 ms, field of view (FOV) = 210×210×144 mm, matrix  
130 size = 70×70 voxels, flip angle = 85°, 0.6 mm gap between slices.

131 Besides structural whole brain T1-weighted ( $T1_w$ ) images (isotropic voxel  
132 size = 1.0 mm), dual gradient  $B_0$  field maps (Fmaps) were also acquired for  
133 each participant to deal with distortions caused by inhomogeneity in the  
134 static-field.

## 135 2.6 Preprocessing

136 We combined the Oxford Centre’s *FMRIB* Software Library (FSL, version  
137 4.1; Jenkinson et al., 2012) with the Advanced Normalization Tools (ANTs,  
138 version 2.1; Avants et al., 2011) to create a pipeline optimized for the pre-  
139 processing of our neuroimaging data (see Suppl. Fig. S1).

140  
141 A challenge of fMRI gustometry is that BOLD signal is highly prone to  
142 movement artifacts and thus the swallowing of liquid solutions while lying  
143 down produces significant deglutition artifacts. To offset this loss of signal we  
144 followed (Griffanti et al., 2017) rigorous protocol for fMRI ICA-based artifact  
145 removal (e.g. motion, susceptibility or blood flow in arteries). Field maps  
146 were then applied to correct geometric distortion and ANTs was used to dif-  
147 feomorphically co-register the preprocessed functional and structural images  
148 to the Montreal Neurological Institute (MNI) space, using nearest-neighbor  
149 interpolation and leaving the functional images in their native resolution.  
150 Finally, we applied a spatial smoothing of 8 mm full width half maximum.

## 151 2.7 Data Analysis

152 Statistical analyses of the behavioral data were performed with R (ver-  
153 sion 4.0; R Core Team, 2019). We report Cohen’s  $d_z$  and their 95%*CI* as  
154 estimates of effect sizes for the paired  $t$  tests (Lakens, 2013) together with a  
155 Bayes factor ( $BF_{10}$ ) quantifying the likelihood of the data under the alter-  
156 native hypothesis relative to the null hypothesis Morey et al. (2015).

157  
158 The Statistical Parametric Mapping software (SPM, version 12; Penny  
159 et al., 2011) was used to perform a random-effects univariate analysis on the  
160 voxels of the image times series following a two-stage approach to partition  
161 model residuals to take into account within- and between-participant vari-  
162 ance (Holmes and Friston, 1988; Mumford and Poldrack, 2007).

163  
164 We specified a subject-level general linear model (GLM) for each partic-  
165 ipant and added a high-pass filter cutoff of 1/128 Hz to eliminate possible  
166 low-frequency confounds (Talmi et al., 2008). Each regressor of interest was  
167 derived from the onsets and duration of the stimuli and convoluted using  
168 a canonical hemodynamic response function (HRF) into the GLM to ob-



tain weighted parameter estimates ( $\beta$ ). The subject-level GLM consisted of six regressors: (1) the trial, (2) the reception of the milkshake solution, (3) the reception of the tasteless solution, (4) water rinsing, (5) question about solution pleasantness and, (6) intensity. Group-level statistical  $t$ -maps were then created by combining subject-level estimated beta weights (Milkshake > Tasteless) and residuals.

We used the AFNI's *3dFWHMx* function to estimate the intrinsic spatial smoothness of our xyz dimensions that we inputted in the new *3dClustSim* function (Cox et al., 2017) to create—via Monte Carlo simulation—a cluster extent threshold corrected for multiple comparisons over the whole brain at  $p < 0.05$  for a height threshold of  $p < 0.001$ . We report the minimum extent threshold, the peak MNI coordinates, and the number of consecutive significant voxels at  $p < 0.005$  within the cluster ( $k$ ). Finally, we display the statistical  $t$ -maps of our group results of the Milkshake > Tasteless contrast surviving cluster-level correction overlaid on a high-resolution template in MNI space.

### 3 Results

We analyzed the taste intensity ratings during our task using a paired  $t$  tests with two conditions (milkshake or tasteless). As expected, participants rated the milkshake solution as more intense than the tasteless solution ( $F_{(1,84)} = 153.81$ ,  $p < 0.001$ ,  $\eta_p^2 = 0.65$ , 90% CI = [0.54, 0.72],  $BF_{10} = 2.35 \times 10^{23}$ , see Fig. 4A).

We report the results from our group-level analysis using a height threshold of  $p < 0.005$ , with a minimum cluster extent threshold corrected for multiple comparisons at  $p < 0.05$  of 123 voxels. For the taste reactivity task, the pleasant solution (Milkshake > Tasteless) activated the primary olfactory (piriform) cortex bilaterally (right: MNI  $[xyz] = [-22 -3 -14]$ ,  $k = 282$ ; left: MNI  $[xyz] = [21 -6 -14]$ ,  $k = 149$ ), the primary gustatory (insular) cortex (left: MNI  $[xyz] = [21 -6 -14]$ ,  $k = 149$ ), and the primary somatosensory (parietal operculum/postcentral gyrus, see Fig. 5 and Suppl. Table S1 for more details).

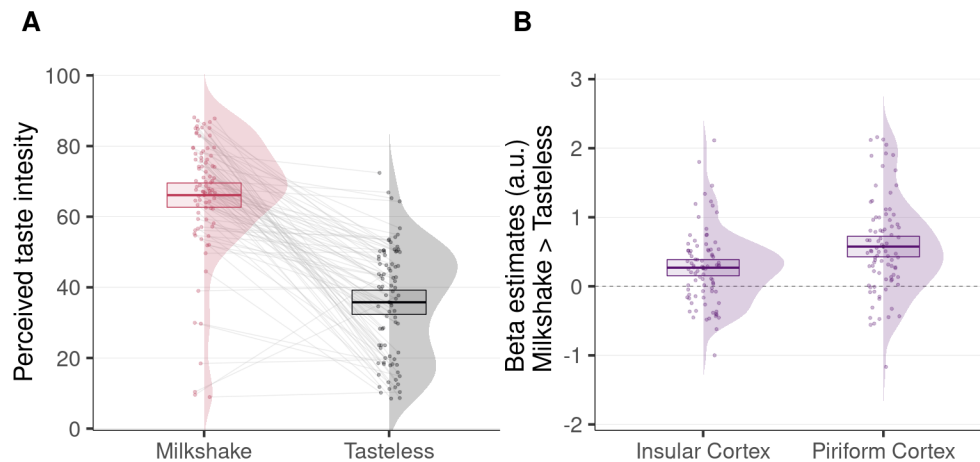


Figure 4: **Behavioral and fMRI results.** (A) Individual estimates, densities and overall mean of perceived taste intensity of the milkshake and the tasteless solutions. (B) Individual beta estimates, densities and overall means of the Milkshake > Tasteless contrast across participants during taste delivery extracted from voxel clusters within the insular and piriform cortex. Error bars represent 95% CI ( $n = 85$ ).

202 We also computed observed power calculations within two regions, namely  
203 the insular and piriform cortex. To achieve that we extracted the averaged  
204 betas values from within these two regions and calculated their standardized  
205 effect size ( $d_z$ ). We report a  $d_z = 0.41$  for the insula and  $d_z = 0.56$  for the  
206 piriform, this allowed us to estimate that to achieve a 90% power at  $\alpha =$   
207 0.05 one would need 53 or 29 participants, for the insula or the piriform  
208 respectively, to reproduce these results (see Suppl. Fig. S2).

## 209 4 Discussion

210 In this paper, we presented a 3D printed MRI compatible mouthpiece for  
211 the study of human taste and flavor perception in fMRI settings. After de-  
212 scribing this mouthpiece, we reported the results of 3 Tesla fMRI study and,  
213 as illustrated by our findings, this mouthpiece allows to obtain an effective  
214 measure of brain related activity during the consumption of gustatory stimuli.  
215

216 We provide results from a large sample that both demonstrate the ef-  
217 fectiveness and validity of our procedure by showing significant clusters of

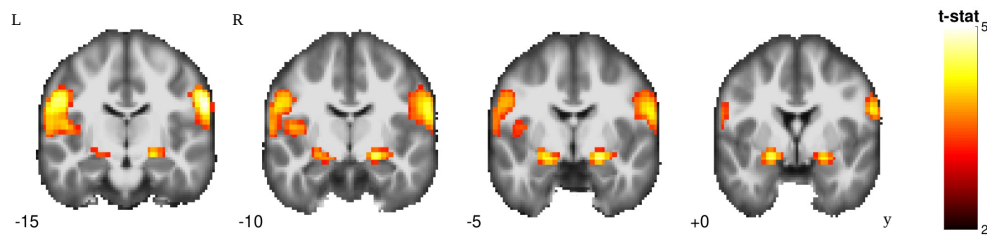


Figure 5: **Neural correlates of taste.** Regions which the BOLD signal positively correlates with the magnitude of the contrast Milkshake > Tasteless ( $n = 85$ ). Statistical  $t$ -maps are shown with a threshold of  $p < 0.001$  and a minimum cluster extent threshold (corrected for multiple comparisons) of 123 voxels.

218 activation within the same regions that have been reported throughout differ-  
219 ent meta-analyses on taste (Yeung et al., 2017) and olfaction (Seubert et al.,  
220 2013).

221

222 We found clear activations of: (i) the middle insular cortex which was no  
223 surprise since this region has consistently been identified as the the human  
224 primary gustatory cortex (Buck and Bargmann, 2000; Small and Faurion,  
225 2015), (ii) the parietal operculum/postcentral gyrus which has been reported  
226 to be the primary cortex for oral somatosensory representation in humans  
227 (Boling et al., 2002) and, (iii) the anterior medial temporal lobes –including  
228 the hippocampal formation and the amygdaloid complex– which have also  
229 both been revealed to play a crucial role in food intake (Coppin, 2016; David-  
230 son et al., 2009; Petrovich, 2011).

231

232 We however encountered some limitations that should be addressed. First,  
233 some participants reported that a 40 mm long mouthpiece was a bit too long  
234 and thus uncomfortable. This can easily be alleviated by printing a shorter  
235 mouthpiece in those cases. We also tried to extend our setup to a non-MRI  
236 contexts where participants would be seated in an upright position. It appeared  
237 that the liquids would not flow as consistently and precisely that they did  
238 in a lying position and would suggest that the prototype would have to be  
239 modified for such contexts.

240

241 In a few cases and during intensive use, we also noticed that the plas-  
242 tic could become porous, so that the joints between the tubes and the teat  
243 were no longer perfectly sealed. As a result, some participants reported that

244 rinsing liquid had run down their cheeks. However, this did not prevent the  
245 stimuli from being sent, but it is something that the researchers could mon-  
246 itor. One option might be to choose a less porous plastic that is still within  
247 the country’s legislative constraints on plastics permitted for food contact.

248

249 Moreover we think it is important to tell the participants to place their  
250 tongue in such a way as to let the solutions flow without blocking the teat  
251 to deliver drops of liquid comfortably and accurately.

## 252 5 Conclusion

253 The main advantages of this mouthpiece are its low cost, flexibility, ease to  
254 produce and fMRI-compatible design. Any lab with access to an 3D printer  
255 can make one or could otherwise get them from any 3D printing service com-  
256 pany since our plans are made freely available. But most importantly, it  
257 is flexible and can be modified to any particular case. It can easily match  
258 different countries’ sanitary regulations or be adjusted for different types of  
259 liquid or viscosity levels. It also does not require to modify any pre-existing  
260 apparatus and will integrate to most gustometer setups without any addi-  
261 tional work.

262

263 We think that this new method will promote the use of primary rewards  
264 (i.e. milkshakes) instead of more widely used secondary rewards (e.g. food  
265 pictures) to measure hedonicity. This is extremely important because, for one  
266 part, it allows comparison with the animal literature on innate food rewards;  
267 but also avoids reward type-dependent neural circuits of secondary rewards  
268 (Nakamura et al., 2020; Sescousse et al., 2013). Moreover, taste consumption  
269 can induce an affective experience by itself rather than a representation of  
270 the affective experience (i.e. pictures of food) which is a crucial property for  
271 the proper study of processing rewards (Pool et al., 2016, 2021).

272

273 Affective neuroscience would benefit from the inclusion of more studies  
274 in olfaction and taste using primary rewards. This would provide the means  
275 for an integrative approach to study the emotional nature of reward (Num-  
276 menmaa and Sander, 2020).

277

278 **Data and materials availability:** Unthresholded statistical  $t$ -maps are  
279 available at the Neurovault platform ([neurovault.org/images/442236/](https://neurovault.org/images/442236/)). Com-  
280 puter code used for producing the mouthpiece as well as preprocessing and  
281 analyzing the data is available in a publicly hosted software repository ([github.com/munoztd0/Mouthpiece\\_gusto](https://github.com/munoztd0/Mouthpiece_gusto)).  
282

283 **Credits:** DMT analyzed the data. ERP help with the validation. CM  
284 designed the apparatus. ZP provided the participants. GC and DS designed  
285 the experiments and SD managed the project. DMT, GC and SD wrote the  
286 first draft. All authors reviewed and approved the final manuscript.

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