1 Reproducible Coactivation Patterns of Functional Brain Networks Reveal the Aberrant

2 Dynamic State Transition in Schizophrenia

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27 Highlights:

28 1. Three coactivation patterns (CAPs) pairs with opposite coactivation profiles were

identified, and the between-state transition probability was positively correlated with theirspatial similarity.

31 2. Good spatial and temporal reproducibility and generalizability of CAPs were achieved

32 under varied analytic methods and independent cohorts.

33 3. Schizophrenia patients showed altered temporal dynamics not only within the triple-

34 network but also other primary and higher-order networks.

35

36 Abstract

37 It is well documented that massive dynamic information is contained in the resting-state

38 fMRI. Recent studies have identified recurring states dominated by similar coactivation

39 patterns (CAP) and revealed their temporal dynamics. However, the reproducibility and

40 generalizability of the CAP analysis is unclear. To address this question, the effects of

41 methodological pipelines on CAP are comprehensively evaluated in this study, including

42 preprocessing, network construction, cluster number and three independent cohorts. The CAP

43 state dynamics are characterized by fraction of time, persistence, counts, and transition

44 probability. Results demonstrate six reliable CAP states and their dynamic characteristics are

45 also reproducible. The state transition probability is found to be positively associated with the

46 spatial similarity. Furthermore, the aberrant CAP in schizophrenia has been investigated by

47 using the reproducible method on three cohorts. Schizophrenia patients spend less time in

48 CAP states that involve the fronto-parietal network, but more time in CAP states that involve

49 the default mode and salience network. The aberrant dynamic characteristics of CAP are

50 correlated with the symptom severity. These results reveal the reproducibility and

51 generalizability of the CAP analysis, which can provide novel insights into the

52 neuropathological mechanism associated with aberrant brain network dynamics of

53 schizophrenia.

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Keywords: coactivation patterns, dynamics, reproducibility, schizophrenia, triple-network

57 **1. Introduction**

Since the resting-state fMRI was confirmed to be physiologically meaningful, (B. Biswal 58 et al., 1995) a number of resting-state fMRI studies have emerged, of which functional 59 connectivity (FC) is one popular method to detect the remote functional co-fluctuations (B. B. 60 Biswal et al., 2010; Friston, 2011). Previous functional connectivity methods have typically 61 assumed stationarity that the time series do not change their characteristics over time. 62 However, the brain is indeed a complex system featured by the dynamic functional brain 63 connectome (Zalesky et al., 2014). Recent evidence suggests that functional interactions 64 65 between different brain regions and networks vary with time. The sliding-window based dynamic functional connectivity (dFC) is intensively used to measure the dynamic interaction 66 between two regions (Hutchison et al., 2013; Preti et al., 2017), which has been shown to link 67 with individual differences (Fong et al., 2019), task performances and disease alterations 68 69 (Gonzalez-Castillo & Bandettini, 2018).

Despite the limitation of the sliding-window approach, the dynamic characteristics of the 70 71 functional brain connectome at the macroscopic level support that the brain has multiple functional recurring states (Zalesky et al., 2014). There are several methods for dynamic brain 72 73 state detection. Combining the sliding-window dFC with the clustering method, Allen and colleagues identified several FC states, as an intermediate scale between static and instant FC 74 underlying small short-time tasks, which can reallocate and integrate attentional and executive 75 resources (Allen et al., 2014). Besides, based on the assumption of temporal independence, 76 Smith and colleagues used temporal ICA to identify temporal function modes (TFM), which 77 represent unique brain activation patterns (Smith et al., 2012). Different from the dFC-78 clustering and TFM which assign each time point to one single state, the approach of the 79 hidden Markov model (HMM) could identify a mixture of the brain states with a given 80 probability at each time point, by assuming the transitions between states should follow a 81 Markov process (Vidaurre et al., 2016). Vidaurre et al. used HMM in resting-state fMRI, and 82 they found two hierarchical metastates that represent higher-order cognition and sensorimotor 83 84 systems (Vidaurre et al., 2017).

The coactivation pattern (CAP) analysis is a data-driven method to detect the functional brain states in a single volume level (Liu et al., 2013; Liu & Duyn, 2013), which originates from the point process analysis (Tagliazucchi et al., 2012). Rather than capturing the dFC configurations as brain states, it is simple and straightforward that, for each frame of the data, the spatial coactivation patterns represent a specific whole-brain activation configuration to deal with the real-time task at that time, and that different frames which share the same spatial

91 patterns are regarded as the same CAP state (Figure 1A). As a data-driven method, CAP

- analysis relies on very few mathematical presumptions, and is free of the confounding
- 93 influence from the sliding window length. Therefore, CAP analysis has increasingly been
- 94 used to study the abnormal network dynamics in depression (Kaiser et al., 2019), Alzheimer's
- disease (Kaiser et al., 2019; Ma et al., 2020) and task fMRI (Freitas et al., 2020).

The reproducibility is crucial for analytical methods in fMRI studies (Botvinik-Nezer et al., 2020; Eklund et al., 2016; Zuo et al., 2019). A lot of analytic flexibility exists in fMRI studies (Vergara et al., 2017), such as different preprocessing pipelines (Shirer et al., 2015), different software and toolboxes (Bowring et al., 2019). It is necessary to clarify the effects of varied settings in neuroimaging analyses (Aurich et al., 2015; Strother, 2006; Vergara et al.,

101 2017) and to establish a standard and robust methodological pipeline (Esteban et al., 2019).

102 However, it still remains unknown about the analytic flexibility and reproducibility for CAP

103 analysis.

Schizophrenia is a psychiatric disorder with complex structural and functional brain 104 105 alterations, characterized by abnormal connectome and functional dynamics (Collin et al., 2016; Fornito et al., 2012; Hunt et al., 2017). Particularly, the triple-network (V. Menon, 106 107 2011), including the default-mode network (DMN), fronto-parietal network central (FPN) or executive network (CEN), and salience network (SN), is postulated as a critical core of 108 network dysfunction for understanding the neuropathological mechanism of psychiatric 109 disorders including schizophrenia (Manoliu et al., 2014; V. Menon, 2011). Recently, Supekar 110 and colleagues found that reduced dynamic interactions among the SN, CEN and DMN may 111 substrate neurobiological signatures of schizophrenia (Supekar et al., 2019). However, little is 112 known about the aberrant dynamic characteristics in schizophrenia concerning triple networks 113 as well as other parts of the whole brain. 114

This study aimed to first investigate the reproducibility and generalizability of the CAP, 115 and then utilize the robust analytical approach to study the aberrant dynamic state transition in 116 schizophrenia. To achieve this goal, key methodological aspects were carefully evaluated for 117 118 the robustness of CAP, including different preprocessing pipelines, ROI numbers for network construction, cluster numbers, and cohorts. Then, reliable dynamic states in the functional 119 120 brain coactivation patterns were identified and further employed to compare the temporal dynamic characteristics between schizophrenia patients (SZ) and healthy controls (HC) in 121 three independent data cohorts. Next, the associations between aberrant dynamic state 122 123 transition and clinical symptom severity were explored.

125 2. Materials and Methods

126 **2.1 Participants**

127 To explore the reproducibility and generalizability of this study, three cohorts (WuXi, 128 COBRE and UCLA) were analyzed. The WuXi cohort was used as the primary cohort, the 129 other two open-access cohorts were treated as verification and their detailed participant 130 information was described in the Supplementary material.

For the primary cohort (WuXi), all subjects were scanned by a structural MRI and 131 resting-state functional MRI on a 3.0-Tesla Magnetom TIM Trio (Siemens Medical System) at 132 133 the Department of Medical Imaging, Wuxi People's Hospital, Nanjing Medical University. Foam pads were used to reduce head motion and scanner noise. Before the scan, the subjects 134 were instructed to keep their eyes closed, relax but not fall asleep, and move as little as 135 possible during data acquisition. After excluding subjects with large head motion, 69 SZ 136 137 subjects and 97 HC subjects remained for the current study. Positive and Negative Syndrome Scale (PANSS) was used to measure the psychiatric symptoms of SZ patients. 138 Framewise displacement (FD) was calculated from the resting-state fMRI data to 139

measure head motion (Di & Biswal, 2015). Subjects were excluded if their maximum
translation or rotation FD were greater than 2 mm or 2°. The k-means clustering was
performed in all 97 HC subjects. For the group comparisons between SZ and HC, only ageand gender-matched HC subjects were analyzed. The age- and gender-matched demographic
information for the three cohorts were provided in Table 1. The information for all HC
subjects used in the coactivation patterns generation can be found in the Supplementary
material.

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148 2.2 fMRI Data Acquisition

149 for the primary cohort (WuXi), the resting-state scans were acquired using a single-shot

150 gradient-echo echo-planar-imaging sequence (Tian et al., 2016) with the following

parameters: TR = 2000 ms, TE = 30 ms, slice number = 33, slice thickness = 4 mm, flip

angle = 90°, matrix size = 64×64 , FOV = 220 mm, voxel size = $3.4 \times 3.4 \times 4$ mm³, and volume

153 number = 240. Three-dimensional T1-weighted images were acquired by employing a 3D-

154 MPRAGE sequence with the following parameters: TR = 2530 ms, TE = 3.44 ms, flip

angle = 7° , matrix size = 256×256 , slice number = 192, slice thickness = 1 mm,

156 FOV = 256 mm, and voxel size = $1 \times 1 \times 1$ mm³. The fMRI data acquisition parameters for the

157 other two cohorts were described in the Supplementary material.

159 2.3 fMRI Data Preprocessing

160	The resting-state fMRI data were preprocessed using DPABI (http://rfmri.org/dpabi), and
161	the preprocessing steps were followed: 1) Remove the first 2 time points for the UCLA and
162	COBRE dataset, and remove the first 5 time points for the WuXi cohort; 2) Realignment; 3)
163	Coregisteration of T1 image to functional image; 4) T1 segmentation by DARTEL; 5)
164	Normalization of the functional images by T1 DARTEL; 6) Nuisance regression, including 24
165	head motion parameters, mean white matter (WM) and mean cerebrospinal fluid (CSF) signal,
166	both with and without global signal regression (GSR); 7) Detrend; 8) Band-pass filtering,
167	from $0.01 \sim 0.08$ Hz; 9) Smoothing with an 8 mm FWHM kernel.
168	To evaluate the effect of preprocessing steps, the resting-state fMRI data was also
169	preprocessed using a standard task fMRI data preprocessing pipeline, which is similar to the
170	above steps but without nuisance regression and filtering.
171	The BOLD signal for the preprocessed resting-state fMRI data was extracted from 408
172	ROIs separately. The 408 ROIs were consist of 400 cortical regions from Yeo's 7 network
173	parcellation (Schaefer et al., 2018) and 8 subcortical regions (bilateral caudate nucleus,
174	putamen, globus pallidus and amygdala) from the AAL template (Tzourio-Mazoyer et al.,
175	2002). The 400 cortical regions are allocated to 7 networks including the visual network
176	(VN), somatomotor network (SMN), dorsal attention network (DAN), ventral attention
177	network (VAN), limbic network, fronto-parietal network (FPN) and default mode network
178	(DMN) (Yeo et al., 2011). The 7 networks have parcellations with different spatial scales from
179	100 to 1000, and 400 was mainly used in this study because the average voxel size for the 400
180	ROIs is comparable to the average voxel size of the 8 subcortical regions from the AAL
181	template.

182

183 **2.4 Coactivation Pattern Analysis**

184 Coactivation pattern (CAP) analysis is a data-driven method that identifies recurring 185 states across time points with similar whole-brain coactivation patterns. In this study, the CAP

186 analysis was performed using home-made scripts in MATLAB

187 (<u>https://www.mathworks.com/</u>).

188 First, to represent the relative activation magnitude changes in the 408 ROIs, each time

189 series were normalized using a z-score. For each subject *i*, a two-dimensional normalized

BOLD matrix $X_i(T \times 408)$ was obtained, where T is the number of time points and 408 is the

191 ROI number.

Next, all HC subjects' normalized BOLD metrics X_{HC} ($T \times 408$) were concatenated to 192 obtain the X_{HC} ($T_{HC} \times 408$, $T_{HC} = T \times N$), where N is the sample size of all HC subjects. Then, 193 k-means clustering was performed to identify similar coactivation patterns across all volumes 194 from all HC subjects, and the distance between two volumes was calculated by subtracting 195 their Pearson correlation coefficient from one. The cluster number K was selected from 2 to 196 21 with a step length of 1. The clustering algorithm was repeated 100 times with a new initial 197 cluster centroid for each K value, and the results with the lowest within-cluster sums of point-198 to-centroid distances were used. Frames assigned to the same CAP state were averaged and 199 divided by the within-cluster standard deviation to generate the normalized CAP maps (Z-200 maps) at the group level (Figure 1A). 201

The clustering patterns obtained from all HC subjects were then applied to each SZ subject. Specifically, each frame from the $X_{SZ_i}(T \times 408)$ was extracted, which is a 1 × 408 vector representing the whole-brain coactivation level at that time point. Then, the spatial similarity between each frame and each normalized CAP map was calculated using the Pearson correlation, and the frame was assigned to the CAP with the largest spatial similarity.

The silhouette score (Rousseeuw, 1987) was calculated to evaluate the clustering results 207 for different K values. As shown in Figure S1, Supplementary material, the silhouette score 208 was monotonically decreasing with the increase of K. Then, the elbow criterion was 209 considered to determine the number of clusters. While one issue is that the time points of the 210 three cohorts are limited, if the cluster number is too large, then each CAP state would only 211 account for a few seconds through the entire scan. Therefore, 6 clusters were mainly analyzed 212 and reported in the manuscript as a trade-off, and one recent paper also used 6 clusters for the 213 214 CAP analysis (Zhang et al., 2020).

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216 **2.5 State Temporal Dynamics Measures / CAP Metrics:**

To evaluate the dynamic properties within and between CAP states, four dynamic 217 measures (CAP metrics) were calculated at the individual level: 1) Fraction of time is 218 219 defined as the proportion of total volumes spent in one CAP state over the whole time series; 2) **Persistence** is the average time spent in one state before transferring to another state, and it 220 221 describes the mean volume-to-volume maintenance of one CAP state; 3) Number of states 222 (Counts) is how many times one state occurred during the whole scan; and 4) Transition probability matrix is the probability that one volume within State A transfers to the next 223 volume belonging to State B, with a non-zero diagonal as the volume within State A could 224 225 still stay within State A for the next volume.

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227 **2.6 Transition Probability and Spatial Similarity between States**

The relationship between the spatial similarity and transition probability between two 228 229 states was measured in all HC subjects. The spatial similarity between different brain states was calculated using the Pearson correlation. Before measuring the relationship between the 230 two metrics, the symmetry of the transition probability was first examined. In detail, the 231 transition probability from State A to State B was paired with the transition probability from 232 State B to State A, and the Pearson correlation was calculated between all pairs to test the 233 234 symmetry level. The transition probability metrics were then averaged on the group level and symmetrized. Finally, the relationship between the spatial similarity and transition probability 235 236 was measured using the Pearson correlation. The diagonal values were not analyzed in this 237 part.

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239 2.7 Reproducibility Analysis

240 Recently, neuroimaging studies have drawn more attention to reproducibility. In this study, the CAPs' spatial and temporal reproducibility were considered from four aspects. The 241 242 first aspect is to consider the effects of different data preprocessing steps, including two standard resting-state fMRI preprocessing pipelines (with and without GSR) and one classic 243 task fMRI preprocessing pipeline. Then, the effects of different spatial resolutions of the 244 template were assessed. In detail, 100, 200, 400 and 1000 ROIs from Yeo's 7 network 245 parcellations (Schaefer et al., 2018) plus the 8 subcortical regions from the AAL atlas 246 (Tzourio-Mazoyer et al., 2002) were tested. Different K values were also compared to see 247 whether the CAP states gradually change with the increase of cluster number. Finally, the 248 CAP analysis was performed in three independent cohorts separately to detect the site effect. 249 Furthermore, to verify the generalizability of this study, whether the results obtained by 250 one cohort can be directly replicated in other cohorts, we applied the CAPs generated from 251 the WuXi cohort to the other two cohorts, then the spatial maps and temporal dynamics 252 253 among CAP states were compared. The spatial reproducibility was assessed by calculating the Pearson correlations between 254

CAPs' spatial maps under different conditions, and the temporal dynamics were then

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258 2.8 Statistical Analysis

compared between spatial matched CAPs.

259	For group comparisons, only age- and gender-matched HC and SZ subjects were
260	analyzed. Age was compared between SZ and HC by a two-sample t-test, and a chi-square
261	cross-table test was used to test the gender difference. As for the CAP metrics, two-sample t-
262	tests were performed with age and gender as covariates. FDR correction ($q = 0.05$) was used
263	to correct for the multiple comparisons.
264	The relationship between CAP metrics and behavioral measures, such as disease
265	symptoms and disease duration, were tested using partial correlation with age and gender as
266	covariates. The state temporal dynamics and behavioral measures were first normalized using
267	z-score, and subjects with large deviation $(Z > 3)$ were excluded in the correlation analysis as
268	the outlier. FDR correction ($q = 0.05$) was used to correct for the multiple comparisons.

269

270 **3. Results**

271 **3.1. Demographics and Questionnaires**

No group differences of age or gender were found between the SZ and HC in all three cohorts, and the detailed group characteristics are given in Table 1.

274

275 **Table 1.** The demographic information for the three cohorts

	HC	SZ	P value	
WuXi cohort (<i>n</i> = 138)				
Num of subjects	69	69		
Age [years]	45.84 ± 11.89	46.06 ± 10.96	0.9112 ^{a)}	
Gender (Male / Female)	35 / 34	35 / 34	1 ^{b)}	
Disease duration	-	19.84 ± 10.96	-	
PANSS positive	-	20.06 ± 4.59	-	
PANSS negative	-	23.78 ± 3.84	-	
PNASS general	-	41.67 ± 5.27	-	
PNASS total	-	85.51 ± 9.50	-	
COBRE cohort (<i>n</i> = 108)				
Num of subjects	54	54		
Age [years]	37.22 ± 12.48	37.80 ± 14.13	0.8234 ^{a)}	
Gender (Male / Female)	43 / 11	43 / 11	1 ^{b)}	
Disease duration	-	15.19 ± 12.46	-	
PANSS positive	-	14.13 ± 4.29	-	
PANSS negative	-	14.46 ± 5.10	-	
PNASS general	-	28.57 ± 8.40	-	
PNASS total	-	57.17 ± 13.52	-	
UCLA cohort ($n = 90$)				
Num of subjects	45	45		
Age [years]	36.73 ± 8.65	37.00 ± 8.75	0.8973 ^{a)}	
Gender (Male / Female)	33 / 12	33 / 12	1 ^{b)}	
BPRS	-	50.40 ± 14.08	-	
SAPS	-	28.89 ± 18.49	-	
SANS	-	35.09 ± 18.55	-	

276 Data are expressed as mean \pm SD (SD: standard deviation).

- 277 Abbreviations: BPRS, Brief Psychiatric Rating Scale; SANS, Scale for the Assessment of
- 278 Negative Symptoms; SAPS, Scale for the Assessment of Positive Symptoms; PANSS,
- 279 Positive and Negative Syndrome Scale.
- ^{a)} two-sample t-test; ^{b)} chi-square cross-table test.
- 281

282 **3.2. Reliable CAP identification and Dynamic Characteristics**

This study tested different methodological combinations on three independent data cohorts, such as preprocessing pipelines, ROI numbers and cluster numbers. Below we reported the primary results of six reliable CAP states, which are based on the WuXi cohort, using the resting-state preprocessing with global signal regression (GSR) and 408 ROIs. The other validation results are provided in the Supplementary material.

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289 *3.2.1. Coactivation Patterns and Brain States*

The coactivation patterns were generated from all HC subjects using temporal k-means 290 291 clustering, and six CAP states were finally identified (Figure 1B), after the search for optimal cluster number (see details in the Supplementary material). Among the six CAP states, brain 292 293 regions that belong to the same functional network, such as the default mode network (DMN), fronto-parietal network (FPN), and salience network (SN), tend to be activated or deactivated 294 simultaneously. One interesting phenomenon is that the six CAP states were grouped into 295 three pairs with opposite spatial coactivation patterns. For example, State 1 and 2 grouped 296 together - State 2 was mainly related with the activated FPN, DMN (without posterior 297 cingulate cortex and precuneus) and deactivated visual network (VN), while State 1 had the 298 opposite spatial pattern. Since each CAP state had certain brain networks with relatively 299 stronger activation or deactivation than the other networks of the whole brain, we found that 300 not only triple networks but also primary (VN, SMN) and higher-order networks (DAN) were 301 identified in the dominant CAP states. 302





Figure 1 A) An illustration for the CAP analysis. The normalized spatial map for each 305 volume was input for the k-means clustering, to identify volumes with similar coactivation 306 307 patterns, and then average them to generate the CAPs. B) Six CAP states were identified by CAP analysis based on the primary configuration (WuXi cohort, resting-state fMRI 308 preprocessing with GSR and 408 ROIs for the network construction). These brain states were 309 normalized at the group level, and the value is the z-statistic value. Red color indicates a 310 311 relatively stronger activation, while blue color indicates a relatively stronger deactivation. State 1 was mainly related to deactivated FPN, DMN and activated VN, and the opposite is 312 313 true for State 2; State 3 was mainly characterized by activated DMN and deactivated FPN and DAN, and the opposite is true for State 6; State 4 was mainly characterized by deactivated 314 315 DMN and activated SN and SMN, and the opposite is true for State 5.

Abbreviations: DAN, dorsal attention network; DMN, default mode network; FPN, frontoparietal network; SN, salience network; SMN, somatomotor network; VN, visual network.

319 *3.2.2. Transition Probability and Spatial Similarity between States*

As shown in the diagonal of the transition probability matrix (Figure 2A), the temporal 320 activity was dominated by the identified CAP states (more than 60% of the time), and the 321 between-state alteration remained low transition probability (1% to 11% of the time). 322 Comparing Figure 2A and Figure 2B, it is clear that the transition probability between brain 323 324 states with strong anti-correlated spatial coactivation was close to zero. Taking State 4 and State 5 for an example (Figure 2C), their coactivation patterns were opposite (spatial 325 similarity r = -0.99), their transition probability from State 4 to State 5 was 0.0081, and from 326 State 5 to State 4 was 0.0103. Despite the small discrepancy in bi-directional transition 327 328 probability, the symmetry in the transition probability matrix is pronounced. Figure 2D showed a significant positive correlation (r = 0.8479, p < 0.0001) between the transition 329 330 probability from State A to State B and transition probability from State B to State A. Finally, the relationship between the transition probability and spatial similarity metrics was 331 332 evaluated. As shown in Figure 2E, the transition probability between two CAP states was highly correlated with their spatial similarity (r = 0.9817, p < 0.0001). 333 334



335

336 Figure 2. The relationship between CAP state transition probability and their spatial similarity. A) The group average transition probability matrix in all HC subjects. B) The 337 spatial similarity between six CAP states, measured by the Pearson correlation. C) The 338 transition probability between State 4 and State 5, and their spatial similarity, the values were 339 shown in the white dashed circles in Figure 2A and Figure 2B. D) The correlation between 340 transition probability from State A to State B and transition probability from State B to State 341 A. The shadow represents the 95% confidence interval. E) The correlation between the 342 symmetrized transition probability between State A and State B and their spatial similarity. 343 The shadow represents the 95% confidence interval. 344

345

346 *3.2.3. Spatial Reproducibility Evaluation*

As shown in Figure 3, each row or column showed two pairs with high spatial similarity,
which suggest reproducible CAP states and their groups. It indicated that good spatial
reproducibility within the HC group remained across different preprocessing pipelines and
ROI numbers for network construction.

Moreover, the validation analysis for different cluster number K also demonstrated good spatial reproducibility, although more CAP states were separated with the increase of K. For example, as shown in Figure 6, when K increased from 6 to 8, four states (State 3 to State 6) remained unchanged, their one-to-one correspondence spatial similarity was larger than 0.9, and the other two states (State 1 and State 2) were subdivided into four states.

To evaluate the reproducibility and generalizability of identified CAP states, the clustering results from the WuXi cohort were applied to all subjects from the COBRE cohort and UCLA cohort. The diagonal of metrics in Figure 7A showed the high spatial similarity of each CAP state between the WuXi cohort and the other two cohorts.





361

362 **Figure 3.** The CAP spatial similarity between states under A) different preprocessing

pipelines and B) different ROI numbers. The spatial similarity was measured by the Pearsoncorrection.

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366 *3.2.4. Temporal Reproducibility Evaluation*

To verify the temporal reproducibility within the HC group more straightforwardly, all states were relabeled to group corresponding states together. As shown in Figure 4, the absolute values for the CAP metrics across different preprocessing pipelines, ROI numbers

and cohorts were evaluated in HC. As for the preprocessing pipeline, rest preprocessing with

- and without GSR showed consistent results across all the three CAP metrics, while task
- 372 preprocessing showed shorter persistence and more counts. All three CAP metrics were not

373 sensitive to the ROI number. Different cohorts showed a consistent fraction of time and

- 374 persistence, and the WuXi cohort exhibited more counts than the other two cohorts.
- 375



Figure 4. The CAP metrics reproducibility within the HC group under different A)
preprocessing pipelines, B) ROI numbers and C) cohorts.

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380 **3.3. Aberrant and Reproducible State Dynamics in Schizophrenia**

381 *3.3.1. State Temporal Dynamic Differences between SZ and HC*

The robust CAP analysis was applied to investigate the schizophrenia-related abnormalities in the CAP dynamic state transition across three independent data cohorts. The state temporal dynamics (CAP metrics) were compared between SZ patients and wellmatched HC controls by using a two-sample t-test, with age and gender as covariates. The results of group comparisons were presented in Figure 5. As mentioned above, the six CAP states could be grouped into three pairs (State 1 and 2, State 3 and 6, State 4 and 5). The mean fraction of time of each state for SZ and HC groups was around 15% to 20%, and each state

persisted for 5 to 6 seconds. For example, the pair of State 4 and State 5 occupied the highest

fraction of time in both the SZ and HC groups, which shared opposite spatial coactivation 390 patterns dominated by SN, SMN and DMN. Almost every state except State 6 showed 391 significant temporal dynamic differences (P<0.05, FDR corrected). The group differences 392 were similar within each pair. For instance, SZ patients showed less fraction of time in states 393 characterized by FPN and DMN (State 1 and State 2), and more fraction of time in states 394 characterized by SN and DMN (State 4 and State 5). 395 Specifically, SZ patients showed a significantly reduced fraction of time and persistence 396 in State 1 and 2, as well as reduced counts in State 2, compared with the HC group (Figure 397

- 5A). In State 4 and 5, SZ patients had significantly increased fraction of time and counts.
- 399 Moreover, SZ patients showed a significantly increased fraction of time and counts in State 3,
- 400 but not in State 6. As for the transition probability between CAP states, SZ patients showed
- 401 lower transition probability from State 4 to State 2, and lower transition probability within
- 402 State 1 and State 2 (Figure 5B). On the other hand, SZ patients showed higher transition
- 403 probability from State 1 to State 5, State 2 to State 3, State 3 to State 5 and State 6 to State 4.
- 404 The detailed statistic values for these CAP metrics were described in Table S2, Supplementary405 material.



408 Figure 5. State temporal dynamic differences between SZ and HC. The group differences in A) fraction of time, persistence, counts and B) transition probability. Red bins are the SZ 409 group and blue bins are the HC group. Two-sample t-tests were performed with age and 410 gender as covariates. Error-bar is the standard error. * indicates p < 0.05, and ** indicates p < 0.05411 0.005, and *** indicates p < 0.0005 with FDR correction. For the transition probability, the 412 red arrow means higher transition probability in the SZ group, and vice versa for the blue 413 arrow. C) Behavioral relevance with state temporal dynamics in SZ. The fraction of time of 414 State 6 was negatively correlated with the positive PANSS score, r = -0.4406, p = 0.0013; The 415 counts of State 6 was negatively correlated with the positive PANSS score, r = -0.4657, p =416 0.0005; The transition probability from State 5 to State 6 was negatively correlated with the 417 positive PANSS score, r = -0.3953, p = 0.0316 (all the p values were FDR adjusted). The 418 419 shadow represents the 95% confidence interval. Abbreviations: PANSS, Positive and Negative Syndrome Scale. 420

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422 *3.3.2.* The relationships between State Temporal Dynamics and Clinical Data

The clinical relevance with state temporal dynamics was evaluated in the SZ group, 423 using partial correlation with age and gender controlled. As shown in Figure 5C, after FDR 424 correction, the following negative correlations between CAP metrics and positive PANSS 425 score were found: the fraction of time of State 6 (r = -0.4406, p = 0.0013), the counts of State 426 6 (r = -0.4657, p = 0.0005), and the transition probability from State 5 to State 6 (r = -0.3953, 427 p = 0.0316). In addition, the persistence of State 3 (r = -0.3388, p = 0.0323) was negatively 428 correlated with the disease duration, the fraction of time of State 4 (r = 0.3556, p = 0.0203), 429 and the persistence of State 5 (r = 0.3653, p = 0.0154) was positively correlated with the 430 431 PANSS total score.

432

433 **3.3.3. Reproducible Group Differences between SZ and HC**

The reproducibility of SZ patients' dynamic alterations was also validated in this study, which confirmed good temporal reproducibility for the group differences. For instance, SZ showed more fraction of time in State 4 and State 5 and less fraction of time in State 1 and State 2. These results were consistent across different methodological pipelines (Figure S5 and Figure S8, Supplementary material). And for the unchanged states under K = 6 (State 5) and K = 8 (State 1), their temporal dynamic differences that SZ showed more fraction of time than HC were consistent as well (Figure 6B).

Figure 7B showed the fraction of time differences between SZ and HC across the three cohorts. Their overall trend among the six CAP states was similar, particularly State 2, State 3 and State 5 showed consistent significant group differences in the WuXi cohort and COBRE cohort. Although the temporal dynamic differences obtained from the UCLA cohort were less similar compared with the other two cohorts, the absolute values still showed a consistent trend as presented in Figure 5C.

In addition, the repeatability for different cohorts was validated. Rather than using the
CAP maps from one cohort to the other cohorts, the CAP analysis was independently
performed for the COBRE and UCLA cohort, and the spatial and temporal results were
compared. Although the repeatability for different cohorts was relatively weaker, considerable
spatial overlaps were identified across the three cohorts. More details were described in
Figure S11 to Figure S13, Supplementary material.

453



Figure 6. CAP analysis reproducibility with different cluster numbers. In this case, the configuration was WuXi cohort, rest preprocessing with GSR and 408 ROIs. A) The CAP spatial similarity between K = 6 and K = 8. B) The State 1 in K = 6 was divided into two states in K = 8, State 2 and State 3. State 5 in K = 6 remained in K = 8, which corresponds to State 1, and the SZ group also showed a consistent more fraction of time than the HC group. The error bar is the standard error.



463Figure 7. The generalizability of network dynamic measure differences between SZ and HC464across the three independent cohorts. A) Applying the clustering results based on the WuXi465cohort to the other two cohorts, their spatial similarity was measured by the Pearson466correlation. B) The fraction of time differences between SZ and HC across the three cohorts. *467indicates p < 0.05, ** indicates p < 0.005 and *** indicates p < 0.005 (FDR adjusted). The468error bar is the standard error.

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462

470 4. Discussion

In this study, we first identified the characteristic and reliable states and transitions of 471 functional brain networks in the healthy adults, and then investigated the schizophrenia-472 related aberrant state dynamics, based on the coactivation pattern analysis and three 473 independent cohorts. Healthy and patient cohorts achieved robust results across different 474 methodological pipelines. Our results revealed six reliable coactivation states of functional 475 brain networks, which were constituted by typical resting-state networks including triple 476 477 networks as well as primary and other higher-order networks. The principle of spontaneous state transitions inferred the higher spatial similarity, the higher transferring probability 478 between the separable coactivation states. Patients with schizophrenia showed reproducible 479 evidence of aberrant coactivation patterns dynamics, particularly the state dominance such as 480 the fraction of time was altered and associated with positive symptoms in the patients. 481 Together, our study confirms the reproducibility and generalizability of CAP analysis, which 482 483 could provide meaningful information about the network dysfunction and neuropathological mechanisms in psychiatric disorders. 484

485

486 **4.1. Coactivation Patterns for Brain States**

The CAP analysis is based on the temporal k-means clustering of whole-brain functional 487 activities, which identifies a group of spatial maps with similar whole-brain coactivation 488 patterns across the whole scan. Motivated by the idea of PPA (Tagliazucchi et al., 2012), Liu 489 et al. found that the DMN can be simply identified by averaging multiple distinct 490 coactivations or co-deactivation patterns at different time points (Liu & Duyn, 2013). Yeo's 7 491 network parcellation was used in this study, and brain regions belonging to the same network 492 tended to be activated or deactivated together (Figure 2). This result supports the intrinsic 493 relationship between brain regions within the same functional network (B. B. Biswal et al., 494 495 2010; Calhoun & Adali, 2012), and these intrinsic networks can be simply extracted by averaging a few time points rather than using a more complex mathematical method such as 496 497 ICA. Thus, while CAP states are derived from resting-state fMRI signals by using not pairwise functional connectivity but temporal clustering, which we feel at least partly 498 499 represents the temporal dynamic characteristics of the whole-brain functional connectome (Zuo et al., 2012). 500

Previous ICA analyses used to divide the DMN network into anterior part and posterior 501 part (B. B. Biswal et al., 2010; Zuo et al., 2010). Our results also found the posterior DMN 502 (mainly includes the precuneus/posterior cingulate cortex and angular gyrus) and the anterior 503 DMN (mainly includes the medial prefrontal cortex) were activated at different level across 504 states. The posterior DMN tends to be related to the SN and SMN (State 4 and 5), while the 505 anterior DMN was associated with FPN and DAN (State 3 and 6). Besides, three pairs of 506 507 states were identified with opposite coactivation patterns. For instance, when DMN was activated, the FPN and DAN were deactivated (State 3), and vice versa is true for State 6. The 508 phenomenon of opposite CAP pairs has also been found in previous studies (Huang et al., 509 2020; Janes et al., 2020; Zhang et al., 2020), suggesting these regions tend to be activated in 510 an opposite manner that the activation of region A would suppress the activity of another 511 512 region B, and vice versa.

513 The DMN is known as the task-negative network. For State 3 to State 6, when DMN was 514 activated, other task-positive networks such as FPN and SN were either not activated or 515 deactivated. These results verified the anti-correlation between the task-positive network and 516 the task-negative network (Fox et al., 2005; Power et al., 2011). Based on CAPs, Li and 517 colleagues concatenated a set of task activation maps from the Human Connectome Project, 518 and validated the robust anti-correlated functional network (DMN) across multiple tasks (Li et

al., 2020). However, we found that the DMN was not always activated conversely compared

520 with FPN. Specifically, the medial-prefrontal subsystem and temporal subsystem of DMN

521 were co-deactivated with FPN when the visual network was activated, and vice versa is true

522 (State 1 and State 2). This is consistent with recent findings that the DMN and FPN are

- 523 coactivated when evaluating internal information (Beaty et al., 2016; Zhu et al., 2017) and
- 524 involved in task preparation (Koshino et al., 2011).
- 525

526 **4.2. Transition Probability and Spatial Similarity**

527 Unlike the Pearson correlation matrix which is mathematically symmetric, the transition probability between State A and State B is not equal. Nevertheless, a significant positive 528 529 correlation was obtained (r = 0.8479, p < 0.0001) between the transition probability pairs, suggesting the transition probability between two states is an approximation (Figure 4A). In 530 531 addition, the transition probability between two states was significantly correlated with their spatial similarity (r = 0.9817, p < 0.0001), which suggests that one state would transfer to the 532 533 other state with a higher probability. This positive association was also found by a previous study based on the hidden Markov model (Vidaurre et al., 2017), as the brain should activate 534 535 continuously, it is less likely that one CAP state would directly change to another state with opposite whole-brain coactivation configuration without any intermediate state. 536

537

538 4.3. Reproducibility in CAPs Analysis and Results

539 In this study, we considered the reproducibility of our analyses from several aspects, 540 including preprocessing pipeline, ROI number, cluster number and cohort, and they showed 541 consistent results.

For CAP analysis based on resting-state fMRI data, currently there is no standard 542 preprocessing pipeline. Some studies used the common task preprocessing pipeline, which 543 mainly includes realignment, spatial normalization and smoothing (Kaiser et al., 2019; 544 Karahanoglu & Van De Ville, 2015). More studies used the standard resting-state 545 546 preprocessing pipeline, which has additional steps such as nuisance signal regression (WM, CSF) and temporal filtering, with and without GSR (Karahanoglu & Van De Ville, 2015; Liu 547 et al., 2013; Liu & Duyn, 2013; Ma et al., 2020). We used both the task and resting-state 548 preprocessing pipelines (with and without GSR) in this study. As shown in Figure 3 and 549 550 Figure 4, similar coactivation patterns and temporal dynamics were obtained for different 551 preprocessing pipelines, which suggests the preprocessing has little effect on the whole-brain coactivation patterns. Besides, as Figure 4A showed, task preprocessing has shorter 552

persistence and more counts. The reason could be that the high-frequency noise (Chen &
Glover, 2015) was not filtered during the task preprocessing, which causes frequent
fluctuations and shorter persistence.

Both voxel-level (Liu et al., 2013) and ROI-level (Janes et al., 2020) were studied in previous CAP analysis studies. Using ROI could reduce the dimension and save a lot of time and computational resources (Chen et al., 2015), while it could also decrease the spatial resolution and ignore spatial details. We chose different ROI numbers from 100, 200, 400 to 1000 to represent multiple levels of ROI size. As shown in Figure 3 and Figure 4, the coactivation patterns showed highly spatial and temporal dynamics consistency, suggesting that the CAP analysis is not sensitive to the spatial resolution.

As for the cluster number, when increasing the cluster number, the spatial and temporal properties change continuously. For instance, when K increased from 6 to 8, four states remained the overall spatial coactivation patterns, and their temporal dynamics were also unchanged (Figure 6).

567 Besides the analytic variations, we also validated the results obtained from the three independent cohorts. Although the spatial consistency of coactivation patterns between 568 569 cohorts was less than that of different preprocessing steps, there were still considerable spatial overlaps. To further verify the generalizability of our findings, we mapped the CAP maps 570 obtained by the WuXi cohort to the other two cohorts, and the group temporal dynamic 571 differences between SZ and HC were similar across cohorts (Figure 7B). In conclusion, our 572 study suggested there was considerable reproducibility across different analytic variations and 573 cohorts. 574

575

576 4.4. State Temporal Dynamics Abnormalities in Schizophrenia and Their

577 **Reproducibility**

Using the robust CAP spatial maps, the state temporal dynamics in terms of fraction of 578 time, persistence, counts, and transition probability were calculated and compared between 579 580 SZ and HC groups. Reproducible and aberrant state temporal dynamic was found in schizphrenia patients concerning different methodological pipelines or cohorts (Figure 5 - 7). 581 582 Most CAP states demonstrated aberrant dynamic characteristics, suggesting schizophrenia-583 related network dysfunction is widespread over the whole brain, which is consistent with the 584 accumulating evidence that schizophrenia is characterized by whole-brain network dysfunction (Adhikari et al., 2019; Collin et al., 2016; Fornito et al., 2012; Kambeitz et al., 585 586 2016; Venkataraman et al., 2012). Previous fMRI studies reported that schizophrenia patients

showed distributed alterations in the dynamic functional connectivity (Du et al., 2018), 587 dynamic brain activity (Fu et al., 2018) and dynamic state (Allen et al., 2014; Damaraju et al., 588 2014; Fu et al., 2020; Mennigen et al., 2018; Rashid et al., 2014). A recent resting-state fMRI 589 study revealed dysregulated brain dynamics, i.e., reduced, less persistent, and more variable 590 between-network interactions among SN, FPN and DMN in schizophrenia (Supekar et al., 591 2019), which proves aberrant triple network saliency model of psychosis (V. J. W. P. Menon, 592 2020). Our findings extend the current understanding about schizophrenia-related dynamic 593 594 abnormalities in such manner that aberrant state temporal dynamics in schizophrenia is 595 associated with not only triple networks but also part of primary (VN, SMN) and higher-order networks (DAN). 596

597 First, we found that SZ patients had insufficiently intensified activation and less inhibited deactivation in FPN-DMN state, but on the contrary for SN-DMN state, of which the 598 599 transition probability changed significantly. It has been well documented that, the triple networks, involving FPN, SN and DMN, are the cores for higher cognition. Specifically, FPN 600 601 is engaged in externally oriented attention during demanding cognitive tasks, SN is crucial in the process of salience mapping, and DMN is related to self-referential processes (V. Menon, 602 603 2011). Imaging findings based on triple network alterations have enhanced our understanding of the psychopathology in schizophrenia, depression and autism (Krishnadas et al., 2014; 604 Manoliu et al., 2014; Nekovarova et al., 2014; Supekar et al., 2019; J. Wang et al., 2020). 605 Recent meta-analysis confirms that the triple network might underlie the common network 606 dysfunction across psychiatric disorders including schizophrenia (Sha et al., 2019). Although 607 our findings highlight schizophrenia-related dynamic abnormalities centered in the triple 608 network, in line with an earlier study (Supekar et al., 2019), our results further point out that 609 the DMN was continuously activated across all states while SN and FPN were only involved 610 with specific states, which may suggest the DMN play a crucial role in the state transitions 611 and cross-network interactions within the triple networks. 612

Second, we found that the robust CAP states were also centered in the primary networks 613 614 such as VN and SMN, and higher-order network such as DAN, which had substantially altered temporal state dynamics in schizophrenia patients. Interestingly, the VN, SMN, and 615 616 DAN were recently identified across psychiatric disorders, by partial least squares which is a 617 different data-driven approach from CAP analysis, as key parts underlying the general 618 psychopathology, cognitive dysfunction, and impulsivity (Kebets et al., 2019). In this study, Kebets and colleagues found the latent components of whole-brain resting-state functional 619 620 connectivity were robust, and particularly, SMN showed featured alterations in the static

resting-state functional connectivity within and between networks. Our study provides 621 consistent evidence for schizophrenia-related network dysfunction from a new perspective of 622 CAP states and state transition. Furthermore, we reported that the dynamic characteristics of 623 the FPN-DAN state (State 6) were negatively correlated with the PANSS positive scores, and 624 those of SN-DMN state (State 4 and 5) were positively correlated with the PANSS total 625 scores, consistent with previous evidence (Kindler et al., 2015; Manoliu et al., 2013; Pang et 626 al., 2017; Rotarska-Jagiela et al., 2010; D. H. Wang et al., 2018). Importantly, the transition 627 probability from the SN-DMN state (State 5) to the FPN-DAN state (State 6) was also 628 629 negatively correlated with the positive PANSS scores. Notably, the group difference was not significant for State 6 (Figure 5A). This finding may suggest that the state transition is likely 630 631 to alleviate the disease severity from the symptom positively-related state to the symptom negatively-related state, which might provide a potential intervention target for schizophrenia 632 633 patients. Taken together, the reproducible abnormalities of state temporal dynamics identified in this study implicate that schizophrenia is associated with whole-brain functional network 634 635 dysregulation and dynamic alterations.

636

637 **4.5. Limitations**

Although the k-means clustering has been widely used in fMRI data, currently there is no 638 optimal criterion to determine the cluster number (Vergara et al., 2020). In this study, the 639 volume numbers for the WuXi, COBRE and UCLA cohort are 240, 150 and 152 respectively, 640 with the same TR. When we increased the cluster number in the CAP analysis, the average 641 volumes allocated to each cluster (state) decreased, which might cause more variability for 642 each cluster and reduce the clustering stability. In the COBRE and UCLA cohort, we tested 643 the k-means clustering from 2 to 21, and for K = 21 there are only average 7 volumes for a 644 single state, which had too limited temporal information. Therefore, we chose the K = 6645 following the qualitative but arbitrary criteria in line with the prior study (Liu & Duyn, 2013). 646 647

648 **5. Conclusion**

In summary, functional brain states involved with specific coactivation patterns at different time points were obtained using coactivation pattern analysis. The spatial and temporal reproducibility of these CAPs was verified from multiple aspects, such as different preprocessing pipelines and independent cohorts. Moreover, the robust and aberrant temporal dynamics were identified in schizophrenia, associated with the severity of clinical symptoms. This study proved that the CAP analysis has good reproducibility and generalizability, which

- 655 is useful to provide novel and robust information about aberrant brain dynamic configurations656 for understanding the psychopathological mechanisms in schizophrenia.
- 657

658 Ethics Statement

All participants provided informed written consent. This research was approved by the
respective Universities/Hospitals depending on the origin of the dataset (Medical Ethics
Committee of Wuxi Mental Health Center, Nanjing Medical University for the WuXi cohort,
Institutional Review Boards at UCLA and the Los Angeles County for the UCLA cohort, and
institutional review board protocols of the University of New Mexico for the COBRE cohort).

- 664 This study was conducted in accordance with the Declaration of Helsinki guidelines.
- 665

666 **Conflict of Interest**

- 667
- 668

669 Data and Code Availability Statements

670 The two open cohorts were obtained from UCLA Consortium for Neuropsychiatric

671 Phenomics LA5c Study (<u>https://openneuro.org/datasets/ds000030/versions/1.0.0</u>) and The

672 Center for Biomedical Research Excellence (COBRE)

The authors declare no conflict of interest.

- 673 (<u>http://fcon_1000.projects.nitrc.org/indi/retro/cobre.html</u>). The WuXi cohort is not publicly
- available due to privacy or ethical restrictions. The code that supports the findings of this
- 675 study will be made available upon request from the corresponding author.
- 676

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685 **References**

- Adhikari, B. M., Hong, L. E., Sampath, H., Chiappelli, J., Jahanshad, N., Thompson, P. M., et
 al. (2019). Functional network connectivity impairments and core cognitive deficits in
 schizophrenia. *Hum Brain Mapp*, 40(16), 4593-4605. doi:10.1002/hbm.24723
- Allen, E. A., Damaraju, E., Plis, S. M., Erhardt, E. B., Eichele, T., & Calhoun, V. D. (2014).
 Tracking Whole-Brain Connectivity Dynamics in the Resting State. *Cerebral Cortex*, 24(3), 663-676. doi:10.1093/cercor/bhs352
- Aurich, N. K., Alves Filho, J. O., Marques da Silva, A. M., & Franco, A. R. (2015).
 Evaluating the reliability of different preprocessing steps to estimate graph theoretical
 measures in resting state fMRI data. *Front Neurosci*, *9*, 48.
 doi:10.3389/fnins.2015.00048
- Beaty, R. E., Benedek, M., Silvia, P. J., & Schacter, D. L. (2016). Creative Cognition and
 Brain Network Dynamics. *Trends Cogn Sci*, 20(2), 87-95.
 doi:10.1016/j.tics.2015.10.004
- Biswal, B., Yetkin, F. Z., Haughton, V. M., & Hyde, J. S. (1995). Functional Connectivity in
 the Motor Cortex of Resting Human Brain Using Echo-Planar Mri. *Magnetic Resonance in Medicine*, 34(4), 537-541. doi:DOI 10.1002/mrm.1910340409
- Biswal, B. B., Mennes, M., Zuo, X. N., Gohel, S., Kelly, C., Smith, S. M., et al. (2010).
 Toward discovery science of human brain function. *Proc Natl Acad Sci U S A*, 107(10), 4734-4739. doi:10.1073/pnas.0911855107
- Botvinik-Nezer, R., Holzmeister, F., Camerer, C. F., Dreber, A., Huber, J., Johannesson, M., et
 al. (2020). Variability in the analysis of a single neuroimaging dataset by many teams.
 Nature, 582(7810), 84-88. doi:10.1038/s41586-020-2314-9
- Bowring, A., Maumet, C., & Nichols, T. E. (2019). Exploring the impact of analysis software
 on task fMRI results. *Hum Brain Mapp*, 40(11), 3362-3384. doi:10.1002/hbm.24603
- Calhoun, V. D., & Adali, T. (2012). Multisubject independent component analysis of fMRI: a
 decade of intrinsic networks, default mode, and neurodiagnostic discovery. *IEEE Rev Biomed Eng*, 5, 60-73. doi:10.1109/RBME.2012.2211076
- Chen, J. E., Chang, C., Greicius, M. D., & Glover, G. H. (2015). Introducing co-activation
 pattern metrics to quantify spontaneous brain network dynamics. *Neuroimage*, 111,
 476-488. doi:10.1016/j.neuroimage.2015.01.057
- Chen, J. E., & Glover, G. H. (2015). BOLD fractional contribution to resting-state functional
 connectivity above 0.1 Hz. *Neuroimage*, 107, 207-218.
 doi:10.1016/j.neuroimage.2014.12.012
- Collin, G., Turk, E., & van den Heuvel, M. P. (2016). Connectomics in Schizophrenia: From
 Early Pioneers to Recent Brain Network Findings. *Biol Psychiatry Cogn Neurosci Neuroimaging*, 1(3), 199-208. doi:10.1016/j.bpsc.2016.01.002
- Damaraju, E., Allen, E. A., Belger, A., Ford, J. M., McEwen, S., Mathalon, D. H., et al.
 (2014). Dynamic functional connectivity analysis reveals transient states of
 dysconnectivity in schizophrenia. *Neuroimage Clin, 5*, 298-308.
 doi:10.1016/j.nicl.2014.07.003
- Di, X., & Biswal, B. B. (2015). Characterizations of resting-state modulatory interactions in the human brain. *J Neurophysiol*, 114(5), 2785-2796. doi:10.1152/jn.00893.2014
- Du, Y., Fryer, S. L., Fu, Z., Lin, D., Sui, J., Chen, J., et al. (2018). Dynamic functional
 connectivity impairments in early schizophrenia and clinical high-risk for psychosis.
 Neuroimage, 180(Pt B), 632-645. doi:10.1016/j.neuroimage.2017.10.022
- Eklund, A., Nichols, T. E., & Knutsson, H. (2016). Cluster failure: Why fMRI inferences for
 spatial extent have inflated false-positive rates. *Proceedings of the National Academy*of Sciences of the United States of America, 113(28), 7900-7905.
 doi:10.1073/pnas.1602413113

Esteban, O., Markiewicz, C. J., Blair, R. W., Moodie, C. A., Isik, A. I., Erramuzpe, A., et al. 735 736 (2019). fMRIPrep: a robust preprocessing pipeline for functional MRI. Nat Methods, 737 16(1), 111-116. doi:10.1038/s41592-018-0235-4 Fong, A. H. C., Yoo, K., Rosenberg, M. D., Zhang, S., Li, C. S. R., Scheinost, D., et al. 738 739 (2019). Dynamic functional connectivity during task performance and rest predicts 740 individual differences in attention across studies. Neuroimage, 188, 14-25. doi:10.1016/j.neuroimage.2018.11.057 741 Fornito, A., Zalesky, A., Pantelis, C., & Bullmore, E. T. (2012). Schizophrenia, neuroimaging 742 and connectomics. Neuroimage, 62(4), 2296-2314. 743 doi:10.1016/j.neuroimage.2011.12.090 744 Fox, M. D., Snyder, A. Z., Vincent, J. L., Corbetta, M., Van Essen, D. C., & Raichle, M. E. 745 (2005). The human brain is intrinsically organized into dynamic, anticorrelated 746 747 functional networks. Proceedings of the National Academy of Sciences of the United States of America, 102(27), 9673-9678. doi:10.1073/pnas.0504136102 748 Freitas, L. G. A., Bolton, T. A. W., Krikler, B. E., Jochaut, D., Giraud, A. L., Huppi, P. S., et 749 750 al. (2020). Time-resolved effective connectivity in task fMRI: Psychophysiological interactions of Co-Activation patterns. Neuroimage, 212, 116635. 751 doi:10.1016/j.neuroimage.2020.116635 752 Friston, K. J. (2011). Functional and effective connectivity: a review. Brain Connect, 1(1), 13-753 36. doi:10.1089/brain.2011.0008 754 Fu, Z., Iraji, A., Turner, J. A., Sui, J., Miller, R., Pearlson, G. D., et al. (2020). Dynamic state 755 756 with covarying brain activity-connectivity: On the pathophysiology of schizophrenia. Neuroimage, 224, 117385. doi:10.1016/j.neuroimage.2020.117385 757 Fu, Z., Tu, Y., Di, X., Du, Y., Pearlson, G. D., Turner, J. A., et al. (2018). Characterizing 758 759 dynamic amplitude of low-frequency fluctuation and its relationship with dynamic functional connectivity: An application to schizophrenia. Neuroimage, 180(Pt B), 619-760 631. doi:10.1016/j.neuroimage.2017.09.035 761 Gonzalez-Castillo, J., & Bandettini, P. A. (2018). Task-based dynamic functional connectivity: 762 763 Recent findings and open questions. Neuroimage, 180(Pt B), 526-533. doi:10.1016/j.neuroimage.2017.08.006 764 Huang, Z., Zhang, J., Wu, J., Mashour, G. A., & Hudetz, A. G. (2020). Temporal circuit of 765 766 macroscale dynamic brain activity supports human consciousness. Sci Adv, 6(11), eaaz0087. doi:10.1126/sciadv.aaz0087 767 Hunt, M. J., Kopell, N. J., Traub, R. D., & Whittington, M. A. (2017). Aberrant Network 768 769 Activity in Schizophrenia. Trends Neurosci, 40(6), 371-382. doi:10.1016/j.tins.2017.04.003 770 Hutchison, R. M., Womelsdorf, T., Allen, E. A., Bandettini, P. A., Calhoun, V. D., Corbetta, 771 772 M., et al. (2013). Dynamic functional connectivity: Promise, issues, and interpretations. Neuroimage, 80, 360-378. doi:10.1016/j.neuroimage.2013.05.079 773 774 Janes, A. C., Peechatka, A. L., Frederick, B. B., & Kaiser, R. H. (2020). Dynamic functioning 775 of transient resting-state coactivation networks in the Human Connectome Project. Hum Brain Mapp, 41(2), 373-387. doi:10.1002/hbm.24808 776 Kaiser, R. H., Kang, M. S., Lew, Y., Van Der Feen, J., Aguirre, B., Clegg, R., et al. (2019). 777 778 Abnormal frontoinsular-default network dynamics in adolescent depression and 779 rumination: a preliminary resting-state co-activation pattern analysis. Neuropsychopharmacology, 44(9), 1604-1612. doi:10.1038/s41386-019-0399-3 780 Kambeitz, J., Kambeitz-Ilankovic, L., Cabral, C., Dwyer, D. B., Calhoun, V. D., van den 781 Heuvel, M. P., et al. (2016). Aberrant Functional Whole-Brain Network Architecture in 782 Patients With Schizophrenia: A Meta-analysis. Schizophr Bull, 42 Suppl 1, S13-21. 783 doi:10.1093/schbul/sbv174 784

785	Karahanoglu, F. I., & Van De Ville, D. (2015). Transient brain activity disentangles fMRI
786	resting-state dynamics in terms of spatially and temporally overlapping networks.
787	Nature Communications, 6, 7751. doi:10.1038/ncomms8751
788	Kebets, V., Holmes, A. J., Orban, C., Tang, S., Li, J., Sun, N., et al. (2019). Somatosensory-
789	Motor Dysconnectivity Spans Multiple Transdiagnostic Dimensions of
790	Psychopathology, <i>Biol Psychiatry</i> , 86(10), 779-791.
791	doi:10.1016/i.biopsych.2019.06.013
792	Kindler, J., Jann, K., Homan, P., Hauf, M., Walther, S., Strik, W., et al. (2015). Static and
793	Dynamic Characteristics of Cerebral Blood Flow During the Resting State in
794	Schizophrenia Schizophrenia Bulletin 41(1), 163-170, doi:10.1093/schbul/sbt180
795	Koshino, H., Minamoto, T., Ikeda, T., Osaka, M., Otsuka, Y., & Osaka, N. (2011). Anterior
796	medial prefrontal cortex exhibits activation during task preparation but deactivation
797	during task execution. <i>Plos One</i> , 6(8), e22909, doi:10.1371/journal.pone.0022909
798	Krishnadas R Rvali S Chen T Uddin L Supekar K Palaniyappan L et al (2014)
790	Resting state functional hyperconnectivity within a triple network model in paranoid
800	schizophrenia Lancet 383 65-65
801	Li M Dahmani I Wang D Ren I Stocklein S Lin V et al (2020) Co-activation
802	natterns across multiple tasks reveal robust anti-correlated functional networks
802	Neuroimage 227 117680 doi:10.1016/i.neuroimage 2020.117680
804	Liu X Chang C & Duyn I H (2013) Decomposition of spontaneous brain activity into
805	distinct fMRI co-activation natterns <i>Eront Syst Neurosci</i> 7 101
806	doi:10.3389/fnsvs 2013.00101
807	Liu X & Duyn I H (2013) Time-varying functional network information extracted from
808	brief instances of spontaneous brain activity. Proc Natl Acad Sci US A 110(11) 4392-
800	4397 doi:10.1073/nnas.1216856110
009 010	Ma X Zhuo Z Wei I Ma Z Li Z Li H et al (2020) Altered Temporal Organization
010	of Brief Spontaneous Brain Activities in Patients with Alzheimer's Disease
011 012	Neuroscience 425, 1, 11, doi:10.1016/j.neuroscience.2010.11.025
012	Manoliu A Riedl V Doll A Bauml I G Muhlau M Schwerthoffer D et al (2013)
013 81 <i>1</i>	Insular Dysfunction Reflects Altered Between-Network Connectivity and Severity of
014 Q15	Negative Symptoms in Schizophrenia during Psychotic Remission Front Hum
01J 816	Neurosci 7 216 doi:10 3389/fnhum 2013 00216
010 917	Manoliu & Riedl V Zherdin & Muhlau M Schwerthoffer D Scherr M et al (2014)
017 Q1Q	Aberrant dependence of default mode/central executive network interactions on
010 910	anterior insular salience network activity in schizonbrenia. Schizonbr Bull 40(2), 428-
820	437 doi:10.1093/schbul/sbt037
020 921	Mennigen F Miller R I Rashid B Fryer S I Loewy R I Stuart B K et al (2018)
021	Reduced higher-dimensional resting state fMRI dynamism in clinical high-risk
022	individuals for schizonbrenia identified by meta-state analysis. Schizonbrania
023	Research 201 217-223 doi:10.1016/j.schres.2018.06.007
024 025	Menon V (2011) Large-scale brain networks and psychonathology: a unifying triple network
020	model Trands Coan Sci 15(10) 483 506 doi:10 1016/i tics 2011 08 003
020 027	Menon V I W P (2020) Brain networks and cognitive impairment in psychiatric disorders
021	10(2) 200
020 020	19(5), 509. Nekovarova T. Eginerova I. Horacek I. & Spaniel F. (2014). Bridging disparate symptoms
029	of schizonbronia: a triple network dusfunction theory. <i>Event Bahay Neurosci</i> 8, 171
030	doi:10.2280/fmbab.2014.00171
031	Dang I I Kannady D Wai O I IV I Y Gao I S Li H at al (2017) Decreased
032 022	Functional Connectivity of Insular Contax in Drug Naive First Enizode Schizerheenie.
033 024	In Polotion to Symptom Soverity <i>Play One</i> 12(1) doi: A DTM 20167242
034 025	In Relation to Symptom Seventy. <i>Filos One</i> , $12(1)$. doi:ARTN e010/242 10.1371/journal.none.0167242
030	10.15/1/journal.polic.010/242
	29

836 837	Power, J. D., Cohen, A. L., Nelson, S. M., Wig, G. S., Barnes, K. A., Church, J. A., et al. (2011). Functional Network Organization of the Human Brain. <i>Neuron</i> , 72(4), 665-
838	6/8. doi:10.1016/j.neuron.2011.09.006
839	Preti, M. G., Bolton, I. A. W., & Van De Ville, D. (2017). The dynamic functional
840	connectome: State-of-the-art and perspectives. <i>Neuroimage</i> , 100, 41-54.
841	doi:10.1016/j.neuroimage.2016.12.061
842	Rashid, B., Damaraju, E., Pearlson, G. D., & Calhoun, V. D. (2014). Dynamic connectivity
843	states estimated from resting IMRI Identify differences among Schizophrenia, bipolar
844	disorder, and healthy control subjects. Frontiers in Human Neuroscience, 8. doi:ARIN
845	89/ 10.2220/5.1
846	10.3389/Innum.2014.0089/ Determine Legisle A year de Ver V Oertel Kreekel V Uhlheer D L Vereley K &
847	Kotarska-Jagtela, A., van de ven, v., Oertel-Knochel, v., Oninaas, P. J., vogeley, K., &
848	Linden, D. E. J. (2010). Resting-state functional network correlates of psychotic
849	symptoms in schizophrenia. Schizophrenia Research, 11/(1), 21-30.
850	doi:10.1010/J.scnres.2010.01.001
851	Rousseeuw, P. J. (1987). Sinouettes: a graphical and to the interpretation and validation of
852	cluster analysis. Journal of Computational and Applied Mathematics, 20(1), 53-65.
853	(2018) Level Clabel Dependentian of the Hymon Combrel Contex from Intrinsio
854	(2018). Local-Global Parcentation of the Human Cerebral Cortex from mirrinsic
855	Functional Connectivity MRI. Cereb Cortex, 28(9), 3095-3114.
850	doi:10.1095/cercor/bhx1/9 Sha Z. Wagan T. D. Maghalli A. & Ha V. (2010). Common Dysfunction of Langa Socia
857	Sna, Z., Wager, T. D., Mechelli, A., & He, Y. (2019). Common Dystunction of Large-Scale
858	289. doi:10.1016/i biorgych 2019.11.011
009	Shiror W. P. Jiang H. Price C. M. Ng. P. & Creating M. D. (2015) Optimization of re-
000	fMPL Pre processing for Enhanced Signal Noise Separation. Test Retect Reliability
001	and Group Discrimination Neuroimage 117, 67,79
002	doi:10.1016/i.neuroimage 2015.05.015
864	Smith S M Miller K I Moeller S Xu I Auerbach F I Woolrich M W et al (2012)
004 965	Temporally_independent functional modes of spontaneous brain activity. Proc Natl
866	Acad Sci US A $100(8)$ 3131-3136 doi:10.1073/pnas.1121320109
867	Strother S C (2006) Evaluating fMRI preprocessing pipelines - Review of preprocessing
868	steps for BOLD fMRL <i>Ippe Engineering in Medicine and Riology Magazine</i> 25(2)
860	27-41 doi: Doi 10 1109/Memb 2006 1607667
870	Supekar K Cai W Krishnadas R Palaniyannan L & Menon V (2019) Dysregulated
871	Brain Dynamics in a Triple-Network Saliency Model of Schizophrenia and Its
872	Relation to Psychosis <i>Biol Psychiatry</i> 85(1), 60-69
873	doi:10.1016/i bionsych 2018.07.020
874	Tagliazucchi F Balenzuela P Fraiman D & Chialvo D R (2012) Criticality in large-
875	scale brain FMRI dynamics unveiled by a novel point process analysis. <i>Front Physiol</i>
876	3. 15. doi:10.3389/fphys.2012.00015
877	Tian, L., Meng, C., Jiang, Y., Tang, O., Wang, S., Xie, X., et al. (2016). Abnormal functional
878	connectivity of brain network hubs associated with symptom severity in treatment-
879	naive patients with obsessive-compulsive disorder: A resting-state functional MRI
880	study. 66, 104-111.
881	Tzourio-Mazoyer, N., Landeau, B., Papathanassiou, D., Crivello, F., Etard, O., Delcroix, N.,
882	et al. (2002). Automated anatomical labeling of activations in SPM using a
883	macroscopic anatomical parcellation of the MNI MRI single-subject brain.
884	Neuroimage, 15(1), 273-289. doi:10.1006/nimg.2001.0978

- Venkataraman, A., Whitford, T. J., Westin, C. F., Golland, P., & Kubicki, M. (2012). Whole
 brain resting state functional connectivity abnormalities in schizophrenia. *Schizophrenia Research*, 139(1-3), 7-12. doi:10.1016/j.schres.2012.04.021
- Vergara, V. M., Mayer, A. R., Damaraju, E., Hutchison, K., & Calhoun, V. D. (2017). The
 effect of preprocessing pipelines in subject classification and detection of abnormal
 resting state functional network connectivity using group ICA. *Neuroimage*, 145, 365376. doi:10.1016/j.neuroimage.2016.03.038
- Vergara, V. M., Salman, M., Abrol, A., Espinoza, F. A., & Calhoun, V. D. (2020). Determining
 the number of states in dynamic functional connectivity using cluster validity indexes.
 Journal of Neuroscience Methods, 337. doi:ARTN 108651
- 895 10.1016/j.jneumeth.2020.108651
- Vidaurre, D., Quinn, A. J., Baker, A. P., Dupret, D., Tejero-Cantero, A., & Woolrich, M. W.
 (2016). Spectrally resolved fast transient brain states in electrophysiological data. *Neuroimage*, 126, 81-95. doi:10.1016/j.neuroimage.2015.11.047
- Vidaurre, D., Smith, S. M., & Woolrich, M. W. (2017). Brain network dynamics are
 hierarchically organized in time. *Proc Natl Acad Sci U S A*, *114*(48), 12827-12832.
 doi:10.1073/pnas.1705120114
- Wang, D. H., Li, M. L., Wang, M. Y., Schoeppe, F., Ren, J. X., Chen, H. F., et al. (2018).
 Individual-specific functional connectivity markers track dimensional and categorical features of psychotic illness (vol 25, 2119, 2020). *Molecular Psychiatry*, 25(9), 2200-2200. doi:10.1038/s41380-018-0340-x
- Wang, J., Wang, Y., Huang, H., Jia, Y., Zheng, S., Zhong, S., et al. (2020). Abnormal dynamic
 functional network connectivity in unmedicated bipolar and major depressive
 disorders based on the triple-network model. *Psychol Med*, 50(3), 465-474.
 doi:10.1017/S003329171900028X
- Yeo, B. T., Krienen, F. M., Sepulcre, J., Sabuncu, M. R., Lashkari, D., Hollinshead, M., et al.
 (2011). The organization of the human cerebral cortex estimated by intrinsic
 functional connectivity. *J Neurophysiol*, *106*(3), 1125-1165.
 doi:10.1152/jn.00338.2011
- Zalesky, A., Fornito, A., Cocchi, L., Gollo, L. L., & Breakspear, M. (2014). Time-resolved
 resting-state brain networks. *Proc Natl Acad Sci U S A*, *111*(28), 10341-10346.
 doi:10.1073/pnas.1400181111
- 217 Zhang, J., Huang, Z., Tumati, S., & Northoff, G. (2020). Rest-task modulation of fMRI218 derived global signal topography is mediated by transient coactivation patterns. *PLoS*219 *Biol, 18*(7), e3000733. doi:10.1371/journal.pbio.3000733
- Zhu, W., Chen, Q., Xia, L., Beaty, R. E., Yang, W., Tian, F., et al. (2017). Common and
 distinct brain networks underlying verbal and visual creativity. *Hum Brain Mapp*,
 38(4), 2094-2111. doi:10.1002/hbm.23507
- Zuo, X. N., Biswal, B. B., & Poldrack, R. A. (2019). Editorial: Reliability and Reproducibility
 in Functional Connectomics. *Front Neurosci, 13*, 117. doi:10.3389/fnins.2019.00117
- Zuo, X. N., Ehmke, R., Mennes, M., Imperati, D., Castellanos, F. X., Sporns, O., et al. (2012).
 Network centrality in the human functional connectome. *Cereb Cortex*, 22(8), 18621875. doi:10.1093/cercor/bhr269
- Zuo, X. N., Kelly, C., Adelstein, J. S., Klein, D. F., Castellanos, F. X., & Milham, M. P.
 (2010). Reliable intrinsic connectivity networks: Test-retest evaluation using ICA and dual regression approach. *Neuroimage*, 49(3), 2163-2177.
 doi:10.1016/j.neuroimage.2009.10.080
- 932