

1 **3D models of Alzheimer's disease patient microglia recapitulate disease phenotype** 2 **and show differential drug responses compared to 2D**

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12 **Abstract**

13 Alzheimer's disease (AD) is an incurable neurodegenerative disorder with a rapidly increasing
14 prevalence worldwide. Current approaches targeting hallmark pathological features of AD have had
15 no consistent clinical benefit. Neuroinflammation is a major contributor to neurodegeneration and
16 hence, microglia, the brain's resident immune cells, are an attractive target for potentially more
17 effective therapeutic strategies. However, there is no current *in vitro* model system that faithfully
18 recapitulates patient-specific microglial characteristics. To address this shortcoming, we developed
19 novel 3D models of monocyte-derived microglia-like cells (MDMi) from AD patients. MDMi in 3D
20 exhibited mature microglial features, including a highly branched morphology and enhanced bonafide
21 microglial marker expression compared to 2D. Moreover, AD MDMi in 3D co-cultures with neuro-
22 glial cells showed altered cell-to-cell interactions, growth factor and cytokine secretion profiles and
23 responses to amyloid- β . Drug screening assays in 3D AD MDMi revealed different cytokine responses
24 compared to 2D. Our study demonstrates disease- and drug-specific responses in 3D MDMi models
25 that are not apparent in 2D and presents a new 3D platform for more effective and personalised drug
26 testing.

27 **Introduction**

28 Alzheimer's disease (AD) is a complex age-related neurodegenerative disorder involving progressive
29 impairment of cognitive functions, with distinct pathogenicity and clinical phenotypes among patients.
30 Predictions estimate that AD, together with other neurodegenerative diseases, will become the second
31 leading cause of death in the next 20 years (1). Nevertheless, no prevention strategies or cure exist
32 despite major advances in deciphering the molecular basis of AD. The most characteristic
33 neuropathological hallmarks of AD brains are the presence of extracellular senile plaques, consisting
34 primarily of misfolded amyloid- β (A β) protein, and intracellular neurofibrillary tangles, composed of
35 hyperphosphorylated tau protein. Accumulation of protein aggregates in the brain parenchyma triggers
36 multiple deleterious processes, including oxidative stress and mitochondrial dysfunction (2), which
37 alter brain homeostasis. For decades, reducing the protein aggregate burden in AD brains has been the
38 main goal of candidate therapeutics, but these strategies have yielded poor outcomes in clinical trials.
39 The field is therefore in desperate need for more effective drug targets.

40 Chronic neuroinflammation and sustained activation of pro-inflammatory pathways are critical
41 components of many neurodegenerative diseases, including AD. Recent reports have shown that
42 neuroinflammation plays a major role in the pathogenesis and progression of AD (3, 4). Microglia, the
43 resident immune modulators of the brain, are key effectors of neuroinflammation and hence represent
44 a promising candidate for targeted therapeutics for AD and other neurodegenerative diseases.
45 Microglia develop aberrant phenotypes under non-homeostatic brain conditions and consequently
46 mediate multiple pathogenic mechanisms, including neuron and synapse degeneration, that are critical
47 to the cognitive decline characteristic of AD (5, 6). Moreover, most AD risk gene variants (for example
48 *TREM2*, *APOE*, *CLU*, *CD33*, *PILRB*, *BINI*, *PLCG2* and *MEF2C*) converge on biological pathways
49 linked to microglial function (7-12). Recent studies have correlated the responses of diseased microglia
50 in AD brains with the varied clinical presentations seen among patients. Indeed, the individual's
51 genetic makeup determines whether diseased microglia will prevent or exacerbate the pathogenic
52 processes underlying disease in that particular patient's brain (13-15). As such, microglia not only
53 contribute to the pathology of AD but also show patient-specific characteristics, thus being essential
54 players in the patient heterogeneity observed in AD.

55 Current *in vitro* model systems used to study the role of microglia in AD (reviewed in (16, 17)) lack
56 either clinical relevance or physiological complexity, thereby affecting translatability of drug
57 outcomes into the clinic. Murine microglia lack the ability to fully recapitulate disease phenotypes of
58 AD patients due to the little resemblance of immune functions and ageing processes between mice and
59 humans (18-21). Human immortalised microglia cell lines are genetically and functionally very

60 different from *in vivo* microglia (22-24). Freshly isolated primary microglia from AD patients are
61 normally obtained from post-mortem brains in low yields and rapidly lose microglial phenotypic
62 signatures upon removal from the brain environment (22). Lastly, human induced pluripotent stem cell
63 (hiPSC)-derived microglia allow for the generation of a clinically relevant, patient-specific microglia
64 platform. However, establishing hiPSC-derived microglia requires costly, long and technically
65 challenging protocols that result in variable differentiation efficiencies (25), and the cells lose patient-
66 specific traits, including ageing markers, upon reprogramming (26).

67 The monocyte-derived microglia-like cell (MDMi) model system addresses the shortcoming of the
68 above models and provides a novel, cost-effective approach for the rapid generation of personalised
69 microglia cultures from living patients. This method has been previously applied by us and others
70 using *ex vivo* blood-derived monocytes from schizophrenia (27, 28), Nasu-Hakola disease (29) and
71 amyotrophic lateral sclerosis (ALS) (30) patients, demonstrating disease-associated phenotypes in the
72 patient-derived MDMi. In addition to their controlled genetic background, MDMi are readily available
73 and yield mature microglia in a short time frame, thus allowing for the study of mature microglia from
74 large patient cohorts (31, 32).

75 Microglial identity is driven by the multicellular milieu and three-dimensional (3D) network of
76 macromolecules present in the brain. Therefore, the traditional two dimensional (2D) culture
77 conditions of microglia *in vitro* systems greatly abrogate their ability to replicate mature microglial
78 function (33). The physiological relevance of the MDMi model can be increased by using 3D *in vitro*
79 culture techniques and co-cultures with neuro-glial cells to incorporate the cues supporting microglial
80 development *in vivo*. The development of a complete AD pathological cascade in 3D, but not in 2D,
81 shows an improved *in vitro* disease modelling capacity of 3D culture systems compared to 2D (34,
82 35). However, no 3D *in vitro* model of AD has yet incorporated patient-derived microglial cells in a
83 highly reproducible and experimentally flexible 3D cell culture system (36).

84 In this study, we generated for the first time 3D patient-specific MDMi models from multiple living
85 AD patients. These 3D hydrogel-based MDMi models are consistent and easy to generate and allow
86 for the establishment of 3D MDMi co-cultures with human neuro-glial cells, which provide a more
87 complex and physiologically relevant culture environment. We characterised 3D MDMi models at
88 different levels. Firstly, we examined whether a 3D hydrogel scaffold enhances microglia-like features
89 (*i.e.*, morphology and marker expression) in MDMi compared to a 2D platform using cells from
90 healthy controls. Secondly, we demonstrated the feasibility to generate 3D MDMi models in 3D co-
91 culture. Thirdly, we studied AD-specific changes in the 3D cultures, including morphology, expression
92 of AD risk genes, cell-to-cell interaction with neuro-glial cells and functional responses against A β

93 aggregates. Finally, to test the potential applicability of 3D MDMi platforms in a drug screening setting,
94 we compared drug responses in MDMi between the 2D, 3D and 3D co-culture models. Together, the
95 utility of the 3D MDMi models presented here opens new avenues for more predictable and
96 personalised *in vitro* microglia models to test candidate therapeutics.

97 **Methods**

98 **Study cohort**

99 This study involved the recruitment of Alzheimer's disease (AD) and Healthy control (HC)
100 participants through the *Prospective Imaging Studying of Aging: Genes, Brain and Behaviour study*
101 (PISA) at QIMR Berghofer Medical Research Institute, Queensland, Australia (37). All research
102 adhered to the ethical guidelines on human research outlined by the National Health and Medical
103 Research Council of Australia (NHMRC). Ethical approval was obtained from QIMR Berghofer
104 Medical Research Institute. All participants provided informed consent before participating in the
105 study. The number of samples varied in each assay due to the limited proliferative capacity of MDMi
106 in culture, and the quantity of blood samples available from each donor. Further, repeated longitudinal
107 sampling of peripheral blood from patients was not within the scope of this study. All samples used
108 for assays were randomly selected, with matching age, gender and apolipoprotein E (APOE) status for
109 each assay. APOE genotyping was performed in the Sample Processing Facility at QIMR Berghofer
110 Medical Research Institute, Queensland, Australia, as previously described (37).

111 **Table 1. Summary of donor information.**

Study cohorts		Healthy Control (HC)	Alzheimer's disease (AD)
N° of participants		<i>n</i> = 12	<i>n</i> = 13
Sex of participants	Females (%)	58.3% (7/12)	53.8% (7/13)
	Males (%)	41.7% (5/12)	46.2% (6/13)
Age of participants (mean ± SD)		68.5 ± 2.7	69.3 ± 5.4
APOE genotype	E3/E3 (%)	25% (3/12)	7.7% (1/13)
	E3/E4 (%)	58.3% (7/12)	69.2% (9/13)
	E4/E4 (%)	16.7% (2/12)	23.1% (3/13)

112 SD = standard deviation

113 APOE = apolipoprotein E

114 **Isolation of peripheral blood mononuclear cells (PBMCs)**

115 Peripheral venous blood samples were collected in ethylenediaminetetraacetic acid (EDTA) tubes
116 (Becton-Dickson, NJ, USA). PBMCs separation was performed within 2 h of blood withdrawal using
117 SepMate™ tubes (StemCell Technologies, BC, Canada) as per manufacturer's instructions. PBMCs
118 were washed twice with PBS containing 1mM EDTA and subsequently frozen in 10% dimethyl
119 sulphoxide (DMSO) (Merck KGaA, Hesse, Germany) and 90% foetal bovine serum (ThermoFisher
120 Scientific, CA, USA) (v/v).

121 **Establishment of 2D and 3D MDMi cultures**

122 MDMi in 2D were generated as described previously (30). Briefly, cryopreserved PBMCs were
123 thawed and seeded onto plates coated with Matrigel (Corning, NY, USA). After 24 h incubation at
124 standard humidified culture conditions (37°C, 5% CO₂), non-adherent cells were removed and a cell
125 population enriched in monocytes remained adhered to the culture vessel. To induce MDMi
126 differentiation, monocytes were then cultured in serum-free RPMI-1640 GlutaMAX medium (Life
127 Technologies, Grand Island, NY, USA) supplemented with 0.1 µg/ml of interleukin (IL)-34 (IL-34)
128 (Lonza, Basel-Stadt, Switzerland), 0.01 µg/ml of granulocyte-macrophage colony-stimulating factor
129 (GM-CSF) (Lonza, Basel-Stadt, Switzerland) and 1% (v/v) penicillin/streptomycin (Life Technologies,
130 Grand Island, NY, USA) for 14 days.

131 To induce MDMi differentiation in 3D, monocytes were resuspended in Matrigel diluted with ice-cold
132 culture medium at a 1:3 ratio. Matrigel-cell mixtures were seeded in 96-well plates with medium
133 containing 0.1 µg/ml IL-34 and 0.01 µg/ml GM-CSF. 3D MDMi were collected or used for
134 downstream assays after an average of 35 days in culture.

135 **Establishment of 2D and 3D human neural progenitor cell (NPCs) cultures**

136 The human ReNcell VM immortalised neural progenitor cell line (EMD Millipore, Billerica, MA,
137 USA) was cultured as per manufacturer's instructions, with some modifications. Briefly, cells were
138 plated onto Matrigel-coated plates for 2D cultures or mixed with a 1:3 Matrigel dilution to initiate the
139 3D cultures. Cells were maintained in DMEM/F12 GlutaMAX medium (Life Technologies, Grand
140 Island, NY, USA) containing 2% (v/v) B27 supplement, 20 µg/ml epithelial growth factor (EGF)
141 (Sigma-Aldrich, MO, USA), 20 µg/ml fibroblast growth factor 2 (FGF-2) (Lonza, Basel-Stadt,
142 Switzerland) and 1% (v/v) penicillin/streptomycin. Both 2D and 3D cultures were spontaneously
143 differentiated for 1, 14 or 30 days by withdrawing growth factors from the maintenance medium (ReN
144 base medium). All cells used were in passages 7-10 to ensure consistent spontaneous neuro-glial
145 differentiation across independent experiments.

146 **Establishment of 3D co-cultures (MDMi and ReNcell VM)**

147 ReNcell VM were plated in 3D as described above and cultured for 1 day in ReN base medium to
148 induce spontaneous differentiation. Monocytes were embedded in a 1:3 Matrigel dilution and seeded
149 with 3D ReNcell VM cultures at 1:2.5 to 1:5 monocyte to ReNcell VM ratios. 3D co-cultures were
150 maintained in 50% (v/v) ReN base medium and MDMi culture medium for an average of 35 days.

151 **Immunocytochemistry**

152 Immunofluorescence staining of 2D cultures was performed as described previously (30). MDMi and
153 ReNcell VM were cultured on 8-well chamber slides (Ibidi, DKSH, Germany) and 13-mm plastic
154 coverslips (Sarstedt, Nümbrecht, Germany), respectively. Cells were fixed in 4% paraformaldehyde

155 (PFA) or ice-cold methanol for 15 min and then washed with PBS. Blocking was performed at RT
156 with 5% bovine serum albumin (BSA) (Sigma-Aldrich, MO, USA) in PBS. Primary antibodies for
157 TREM 2 (1:500; Abcam, # ab201621), P2RY12 (1:200; Alomone Labs, #APR-20), TMEM119 (1:400;
158 Abcam, # ab185333), IBA1 (1:500; Wako, #019-19741), Nestin (1:200; Abcam, #ab22035), GFAP
159 (1:2000; Abcam, #ab4674), GalC (1:50; Santa Cruz, #sc-518055), Doublecortin (DCX) (1:200;
160 Abcam, ab36447) and β III-tubulin (TUBB3) (1:500; BioLegend, #801202) were diluted in blocking
161 solution and incubated overnight at 4°C. Cells were then washed three times with 0.1% Triton-X 100
162 in PBS and incubated with 1:250 Alexa Fluor 488 (#A-11034) / 594 (#A-21203) / 647 (#A-21244)
163 secondary antibodies (ThermoFisher Scientific, CA, USA) for 2 h at RT in the dark and counterstained
164 with a nuclear dye (Hoechst 33342, 1 μ g/ml). Immunofluorescence staining of 3D cultures was
165 performed according to (38) with some modifications. 3D cultures, established on black optical 96-
166 well plates (ThermoFisher Scientific, CA, USA), were fixed with 4% PFA overnight at RT and washed
167 twice with PBS. Cultures were then permeabilised for 30 min with 0.3% Triton-X 100 in PBS, rinsed
168 with PBS and blocked overnight at 4°C with 2% BSA (Sigma-Aldrich, MO, USA) in PBS. Primary
169 antibody solutions were added as described above and incubated for 24 h at 4°C. Secondary antibody
170 solutions were incubated for 5 h at RT in the dark. Following primary and secondary antibody
171 incubations, cultures were washed five times (10 min each) with 0.1% Triton-X 100 in PBS and
172 counterstained with Hoechst 33342. Images were captured using a confocal laser scanning microscope
173 (LSM-780, Carl Zeiss) at 20X and 40X magnification and processed using the Zeiss ZEN software.

174 **RNA extraction and quantitative real-time PCR (qRT-PCR)**

175 RNA and cDNA were prepared as previously described (39). Total RNA was extracted using a Direct-
176 zol RNA Miniprep kit (Integrated Sciences, Australia) as per manufacturer's protocol. Conversion to
177 cDNA was carried out using a SensiFAST™ cDNA synthesis kit (Bioline, London, UK). For qRT-
178 PCR, cDNA was diluted 1:10 to generate working solutions and combined with SensiFAST™ SYBR®
179 Lo-ROX master mix and gene-specific primers (see primer sequences in **Table S1**). The qRT-PCR
180 runs were performed as triplicate on Applied Biosystems ViiA 7 (ThermoFisher Scientific, CA, USA).
181 Endogenous control *18S* was used as a housekeeping gene for normalisation. Relative gene expression
182 levels were calculated using the $\Delta\Delta$ Ct method.

183 **Multiplex bead-based immunoassay**

184 The LEGENDplex™ Human Inflammation (#740809) and Growth Factor (#740180) kits (BioLegend,
185 CA, USA) were used to detect cytokines and growth factors in conditioned media from 3D MDMi and
186 ReNcell VM mono- and co-cultures. The assay was performed as per manufacturer's instructions.
187 Briefly, conditioned media were incubated with a cocktail of antibody-conjugated capture beads. Then

188 biotinylated detection antibodies were added followed by streptavidin-phycoerythrin (SA-PE). The
189 amount of analytes of interest in the samples was calculated as a proportion of the fluorescent signal
190 intensity provided by capture bead-analyte-detection antibody-SA-PE sandwiches. Signals were
191 acquired on a BD LSRFortessa 5 (BD Biosciences, CA, USA) using FACSDiva software, and analysed
192 using Qognit, a cloud-based LEGENDplex™ software (BioLegend, CA, USA). Concentrations (pg/ml)
193 were normalised to total amount of protein in the cultures.

194 **Morphology analysis**

195 Quantification of morphological parameters of MDMi in 2D and 3D mono-cultures was performed by
196 adapting a previous method (40). In brief, phase contrast images acquired with a 20X objective were
197 processed in FIJI software (National Institutes of Health, Maryland, USA) using a macro script that
198 applied a threshold, followed by processing functions “despeckle”, “close” and “remove outliers” that
199 generated a binary image. Binary images were then run on the *AnalyseSkeleton(2D/3D)* plugin, which
200 resulted in skeletonised images. The “results and branch information” outputs from the plugin
201 contained data on branch length, endpoint number and triple and quadruple junctions number. Binary
202 images were also analysed using the *Analyze particles* function in FIJI. This calculated the “solidity”
203 or “ramification index” value, which results from dividing the area of MDMi by its convex area (*i.e.*,
204 area of the smallest polygon drawn around the cell). More ramified cells have a bigger convex area
205 and thus a smaller ramification index (<1). Mean single cell values for each parameter were calculated.
206 The total number of MDMi analysed per donor was 100 in 2D and 20 in 3D.

207 **Cell contacts analysis in 3D co-cultures**

208 Confocal Z-stack images of 3D co-cultures acquired with a 20X objective were rendered in 3D using
209 the Imaris software (Bitplane, Belfast, UK). During image acquisition, the Z-interval was set at
210 “Optimal” so that the number of acquired slices was suitable for the given stack size, objective lens,
211 and pinhole diameter. Following surface modelling using the Surface function in Imaris, the *Surface-*
212 *Surface contact area* extension module was applied to measure the areas in contact between ReNcell
213 VM and MDMi as well as the number of contacts established. Both parameters were then normalised
214 to the total number of MDMi in the image. A total of 200 MDMi in co-culture were analysed for each
215 donor in the HC and AD cohorts.

216 **Preparation of amyloid- β (A β) fibrils**

217 Fluorescein isothiocyanate (FITC)-conjugated amyloid- β peptides 1-42 (FITC-A β ₁₋₄₂) (Bachem,
218 M2585, CH) were dissolved in DMSO to a concentration of 500 μ M and stored at -80°C. FITC-A β ₁₋₄₂
219 were incubated for 24 h at 37°C in the 3D cultures prior to imaging to allow for the fibrillisation of the
220 peptides and formation of A β fibrillary aggregates.

221 **A β aggregates exposure and surveillance analysis**

222 FITC-A β ₁₋₄₂ were added at 5 μ M to MDMi 3D mono- and co-cultures at day 35 of differentiation. After
223 24 h, cultures were imaged on an EVOS FL Auto 2 (ThermoFisher Scientific, CA, USA). Scans were
224 set to image multiple z-stack planes every 12 h for 7 days using a 10X objective. At least 3 fields of
225 view were scanned per well. MDMi located within an area of 90,000 μ m² containing one or more A β
226 fibrillary aggregate were tracked using the *Manual tracking* plugin in FIJI. Migrated distance and
227 velocity of tracked cells were calculated and normalised to the number of MDMi in the analysed areas.
228 Between 100-200 MDMi per individual was tracked in both HC and AD cohorts.

229 **Statistical analysis**

230 All statistical analyses were performed using GraphPad Prism software version 8 (Graphpad Software,
231 CA, USA). Comparisons between two groups were analysed with two-tailed Student's *t*-test or Mann-
232 Whitney *U*, when normality assumptions were not met. Comparisons between three or more groups
233 were analysed by one- or two-way analysis of variance (ANOVA) followed by post-hoc tests. Data
234 are presented as mean \pm SEM or mean \pm SD and $P \leq 0.05$ was considered significant. Statistical
235 significance was determined as * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, **** $P < 0.0001$, as detailed in
236 figure legends.

237 **Results**

238 **MDMi in 3D show increased survival and more mature microglial features compared to 2D**

239 We have previously differentiated monocytes into MDMi in a 2D platform using Matrigel-coated
240 plates (30). To develop a more physiologically relevant MDMi model with a better representation of
241 the 3D structure of the brain, we differentiated monocytes into MDMi in a 3D platform. We embedded
242 the monocytes in Matrigel (**Fig. 1A; Fig. S1A**), resulting in cultures with 6.2-fold higher cell thickness
243 (*i.e.*, size of the Z-stack that captured the whole cell) compared to 2D (**Fig. 1B; Fig. S1B; Movie S1,**
244 **2**). Remarkably, MDMi survival in 3D was significantly increased by 2.5 fold compared to 2D (**Fig.**
245 **1C**). Hence, MDMi were cultured for an average of 14 days in 2D and 35 days in 3D, after which
246 features of cellular ageing, including enlarged cell sizes and increased vacuolisation, were observed.

247 We next examined if the 3D culture conditions affected microglial features in MDMi, including
248 morphology and expression of microglia-enriched markers, compared to 2D. Overall, we observed
249 that 3D MDMi showed a highly ramified branched structure and increased branch complexity
250 compared to 2D (**Fig. 1D**). Branched structure parameters, such as branch length and number of
251 branches (endpoints), and branch complexity parameters, such as number of triple and quadruple
252 junctions (points at which branches divide into three or four sub-branches, respectively), were
253 significantly increased in 3D compared to 2D MDMi (**Fig. 1E-G**). Ramified microglia have a highly
254 branched morphology with a larger convex area than amoeboid cells, thus correlating with a low
255 ramification index (41). We observed that the ramification index of 3D MDMi was lower than 2D
256 MDMi (**Fig. 1H**), confirming an enhanced ramified morphology of MDMi in the 3D platform. Such
257 enhancement in MDMi ramified morphology could be likely due to the larger surface area for growth
258 and differentiation provided by the 3D Matrigel scaffold.

259 We have previously reported that MDMi cultured in 2D showed a microglial phenotype compared to
260 monocytes demonstrated by the upregulated expression of microglia-enriched markers, including
261 *PROS1*, *GPR34*, *GAS6* and *TREM2*, and the downregulated expression of the leukocyte marker *CD45*
262 (30). Expectedly, all seminal microglial markers (*IBAI*, *PROS1*, *GPR34*, *TMEM119*, *GAS6* and
263 *TREM2*) were upregulated and *CD45* was downregulated in 3D MDMi compared to monocytes (**Fig.**
264 **1I**). Interestingly, in comparison to 2D, we observed a significantly increased expression of *PROS1*,
265 *GPR34* and *TMEM119* in 3D MDMi, while similar expression levels were observed for *IBAI*, *GAS6*
266 and *TREM2* between 3D MDMi and 2D MDMi (**Fig. 1I**). These results suggest that the 3D culture
267 was able to promote selective microglia-enriched markers in MDMi. Importantly, as immature
268 microglia have been reported to lack *TMEM119* expression (42), the upregulation of *TMEM119* in 3D
269 MDMi compared to 2D MDMi further indicates an enhanced microglial maturity in the 3D platform.

270 Finally, positive immunostaining of Trem2 and P2ry12 proteins in 3D MDMi confirmed the retention
271 of microglial proteins in MDMi for up to 35 days (**Fig. S1C**).

272 Overall, these results demonstrate that MDMi cultured in 3D survive longer in culture and better
273 recapitulate microglial features, including a more ramified morphology and enhanced expression of
274 microglial core genes, compared to 2D.

275 **Human neural progenitor cells differentiated in 3D generate more mature neuro-glial** 276 **populations compared to 2D**

277 To mimic the neuro-glial cues present in the brain microenvironment, we used the immortalised human
278 neural progenitor cell (NPC) line ReNcell VM to establish a co-culture platform with MDMi. ReNcell
279 VM are derived from the ventral mesencephalon region of a foetal brain (43) and give rise to mixed
280 populations of astrocytes, oligodendrocytes and neurons upon differentiation (43, 44). Using
281 immunofluorescence, we confirmed the presence of cells expressing nestin (NPC marker), GFAP
282 (immature and mature astrocyte marker), GalC (oligodendrocyte progenitor cells (OPCs) and mature
283 oligodendrocyte marker) and doublecortin (DCX, immature neuron marker) after 1 and 30 days of
284 ReNcell VM differentiation in 2D (**Fig. 2A**). As ReNcell VM differentiate, they lose their stemness
285 and proliferative capacity. This was confirmed by a significant decrease in *Ki67* expression, a
286 proliferation marker, by day 14 of differentiation that was further decreased by day 30 of
287 differentiation (**Fig. 2B**). Consistently, the reduction of stemness was reflected by the decreased
288 expression of well-known markers of radial glial progenitor cells (*SOX2*, *NESTIN*, *GLAST* and *BLBP*)
289 by day 30. In contrast, immature astrocyte, OPCs and neuron markers (*GFAP*, *PLP-1* and *TBR2*,
290 respectively) showed increased expression trends after day 1 of differentiation. Markers indicating
291 enhanced astrocytic (*GLT-1*), oligodendrocytic (*GalC*) and neuronal (*MAPT*, *synaptophysin (SYP)*)
292 maturity showed a similar upregulation by day 30 but reached lower expression levels than those from
293 radial glia and immature glial markers (**Fig. 2C**). Overall, these results demonstrate that differentiation
294 of ReNcell VM generates mixed neuro-glial cell populations with predominance of glial cell types
295 including radial glial progenitor cells, astrocytes and OPCs.

296 We next examined whether differentiation under 3D Matrigel culture conditions would enhance the
297 maturity of ReNcell VM-derived neuro-glial cell populations compared to 2D. Hence, we
298 differentiated ReNcell VM in 2D and 3D for 1 day (**Fig. 2D**). We observed that 3D ReNcell VM
299 showed a significant reduction of *Ki67* expression and a significant increase of mature astrocyte and
300 neuron marker (*GLT-1* and *SYP*, respectively) expression compared to 2D (**Fig. 2E-F**). These results
301 indicate that the 3D platform enhances the maturation of the astrocytic and neuronal populations in
302 ReNcell VM within 1 day of differentiation compared to 2D.

303 Together, ReNcell VM-derived neuro-glial populations provide a multicellular brain-like environment
304 that allows for the generation of co-cultures with MDMi, which represent more complex and
305 physiologically relevant MDMi models.

306 **MDMi co-cultured in 3D with human neural progenitor cells elicit an inflammatory response to** 307 **aggregated amyloid- β (A β)**

308 We next generated co-cultures of MDMi and ReNcell VM. Monocytes, pre-mixed with Matrigel, were
309 added to 3D ReNcell VM differentiated for 1 day. Both cell types were then left to differentiate
310 together for 35 days, resulting in a mixed 3D co-culture containing MDMi and ReNcell VM-derived
311 radial glial progenitor cells, neurons, astrocytes and OPCs (**Fig. 2G**). Interestingly, we observed that
312 in 3D co-culture, monocytes readily differentiated into MDMi with a microglia-like morphology (**Fig.**
313 **2H**). This is in contrast to 2D co-culture, where monocytes retained their round morphology (**Fig. S2**).
314 This indicates that the 3D platform is able to provide culture conditions suitable for co-culturing MDMi
315 and ReNcell VM, likely due to the support of the 3D Matrigel scaffold.

316 A β aggregation is a major histopathological hallmark of AD brains. Hence, we incorporated FITC-A β
317 peptides into the 3D co-cultures. Remarkably, we observed that FITC-A β peptides readily formed
318 substantial aggregates within 24 h of incubation in 3D (**Fig. 2I; Fig. S3**) as opposed to 2D, where
319 FITC-A β remained in peptides (**Fig. S3**). This suggests that 3D culture conditions may increase A β
320 aggregation (**Fig. S3**), which is consistent with previous reports showing an accelerated A β
321 accumulation in 3D hydrogel-based cultures due to limited diffusion of the A β peptides (34, 38, 45).
322 High A β plaque load has been shown to induce pro-inflammatory responses in microglia from
323 transgenic AD mouse models (46, 47). Hence, we next investigated whether MDMi are functional in
324 3D co-culture and respond to FITC-A β aggregates. We used a multiplex immunoassay to measure
325 cytokines released in the conditioned medium of FITC-A β -treated 3D co-cultures, and 3D mono-
326 cultures of ReNcell VM and MDMi. We observed a significantly upregulated secretion of classical
327 pro-inflammatory cytokines IL-1 β (2.8 fold) and IL-18 (2.3 fold), and similar trends for IL-6, in 3D
328 co-cultures treated with FITC-A β compared to untreated conditions (**Fig. 2J**). Secretion of other pro-
329 inflammatory cytokines, including IL-8, IFN- α 2, MCP-1, IFN- γ and IL-10 was also stimulated by
330 FITC-A β (**Fig. S4**). These inflammatory responses to A β were largely mediated by MDMi in the 3D
331 co-cultures, as observed by significant changes in cytokine secretion following treatment in 3D MDMi
332 mono-cultures, while 3D ReNcell VM mono-cultures remained unchanged (**Fig. 2J, S4**).

333 Overall, these results indicate that MDMi elicit a broad inflammatory response in the 3D platforms
334 and demonstrate the functional capability of the 3D MDMi culture systems to model
335 neuroinflammation in AD.

336 **Disease-specific differences in 2D and 3D mono-cultures of AD patient-derived MDMi**

337 We next generated 2D and 3D MDMi mono-cultures from healthy control (HC) individuals and AD
338 patients selected based on matched sex, age and APOE genotype (**Table 1**). Monocytes from HC and
339 AD individuals were successfully differentiated into MDMi using 2D and 3D platforms (**Fig. 3A**).
340 Survival of both HC and AD MDMi was significantly increased in 3D compared to 2D by 2.6 and 2.4
341 fold, respectively, while no differences in survival between HC and AD MDMi were observed in
342 neither of the platforms (**Fig. 3B**).

343 To determine if 2D and 3D AD MDMi mono-cultures recapitulate disease-specific differences, we
344 examined phenotypic features (morphology and expression of AD risk genes) associated with AD
345 brain microglia in human and mouse models and compared them 1) between HC and AD cohorts and
346 2) between culture platforms. Quantification of morphological parameters (**Fig. S5**) revealed that when
347 MDMi are cultured in 2D or 3D, HC and AD MDMi have similar branch length, number of branches
348 (endpoints), number of triple and quadruple junctions, and ramification index (**Fig. 3C-G**). This
349 suggests that HC and AD MDMi exhibit a similar branch structure and complexity in both 2D and 3D
350 platforms.

351 We then assessed if those morphology parameters vary between culture platforms within the HC and
352 AD cohorts. Comparison of branched structure parameters (branch length and number) between 2D
353 and 3D MDMi showed similar trends in HC and AD, including similar branch length and increased
354 number of branches in 3D compared to 2D (**Fig. 3C, D**). Interestingly, this contrasted with branch
355 length in a young HC cohort (20-40 years of age) of MDMi (**Fig. 1E**), where MDMi exhibited longer
356 branches in 3D compared to 2D. This may be explained by an age-related effect, where MDMi from
357 elderly donors (60-80 years of age) have impaired response to branching signals and long-term culture
358 in a 3D Matrigel scaffold. Further studies should confirm this observation.

359 Comparison of branch complexity parameters (triple and quadruple junctions) between 2D and 3D
360 MDMi showed a similar trend in number of triple junctions but differed in number of quadruple
361 junctions between the HC and AD cohorts. While the number of triple junctions increased in 3D
362 compared to 2D MDMi in both HC and AD (**Fig. 3E**), the number of quadruple junctions increased in
363 3D compared to 2D MDMi in HC but remained unchanged in AD (**Fig. 3F**). Comparison of
364 ramification index showed a significant decrease in 3D compared to 2D MDMi in both HC and AD
365 cohorts, confirming a more ramified morphology in 3D MDMi (**Fig. 3G**). Overall, our results show
366 that the 3D platform is able to enhance branch number, ramified morphology and complexity
367 parameters in MDMi from HC individuals compared to 2D. However, the 3D platform induced an
368 increase in branch number and ramified morphology but was not able to enhance all complexity
369 parameters in MDMi from AD patients compared to 2D.

370 A recent study done in mouse models has suggested that AD risk genes present in microglia
371 functionally influence microglial behaviour (15). In keeping with this, we examined 1) if risk genes
372 are present/enriched in AD compared to HC MDMi, and 2) if these risk genes are differentially
373 expressed in AD MDMi when cultured in 3D compared to 2D mono-cultures. A panel of AD risk
374 genes including *CLU*, *TREM2*, *PLCG2* and *PILRB* was examined by qRT-PCR. Fold change of
375 expression in 3D compared to 2D revealed heterogeneous distributions within the HC and AD cohorts,
376 with 3D MDMi showing increased trends of enhanced expression within AD patients than HC
377 individuals for most risk genes (*CLU*, *PLCG2* and *PILRB*) (**Fig. 3H, I**). Interestingly, *PILRB*
378 expression was significantly upregulated in 3D AD MDMi compared to 3D HC MDMi (**Fig. 3J**), while
379 no significant differences were observed for the other genes (**Fig. S6**). These results demonstrate that
380 the 3D platform is able to enhance the expression of microglia-specific AD risk genes in AD MDMi
381 compared to 2D and reflects the heterogeneity of disease phenotypes within AD patients.

382 **Disease-specific differences in 3D co-cultures of AD patient-derived MDMi**

383 We next characterised MDMi from HC individuals and AD patients in the 3D co-culture platform (**Fig.**
384 **4A**). As observed in 3D MDMi mono-cultures, survival of MDMi in 3D co-culture was extended by
385 2.5 fold compared to 2D MDMi mono-cultures and was similar to 3D MDMi mono-cultures in both
386 HC and AD cohorts (**Fig. 4B**). The increased survival of MDMi in 3D co-culture indicates that ReNcell
387 VM do not affect MDMi viability. Consistently, similar expression of the apoptosis marker *BAX*
388 between HC and AD 3D co-cultures (**Fig. 4C**) suggests that the cell ratio of MDMi and ReNcell VM
389 and the duration of the co-culture were favourable.

390 To investigate whether AD MDMi reflect disease-specific differences compared to HC MDMi in 3D
391 co-culture, we analysed microglial behaviours known to be altered in AD brains, including 1) cell-to-
392 cell interaction with neuro-glial cells, 2) secretion of growth factors and cytokines, and 3) migratory
393 and inflammatory responses to A β aggregates. The marked synapse loss in AD is predominantly
394 mediated by microglia through aberrant synapse engulfment (6). Hence, we first examined if the cell-
395 to-cell interactions between AD MDMi and ReNcell VM show differences compared to HC MDMi in
396 the 3D co-cultures. We performed a 3D rendering and subsequent surface reconstruction of
397 immunofluorescent 3D co-culture images using the Imaris software (**Fig. 4D**). The ‘*surface-surface*
398 *contact area*’ extension was used to quantify the area of contact between MDMi (labelled with Iba1)
399 and ReNcell VM (labelled with the astrocyte- and neuron-specific markers GFAP and β III-tubulin
400 (TUBB3), respectively) and the number of contact points established between both cell types.
401 Interestingly, we observed a significantly smaller area of contact and a reduced number of contact
402 points between MDMi and ReNcell VM in AD compared to HC 3D co-cultures (**Fig. 4E, F**). This

403 suggests an impairment in the cell-to-cell interactions between MDMi and ReNcell VM in AD 3D co-
404 cultures that might have implications in disease.

405 In the context of AD, microglia secrete factors that alter neuron and astrocyte homeostasis, thereby
406 contributing to disease pathogenesis (48). Hence, we next compared the secretory profiles of HC and
407 AD MDMi in 3D co-cultures using a multiplex immunoassay in conditioned medium collected after
408 35 days of co-culture. Overall, we observed that AD MDMi in 3D co-culture secreted higher levels of
409 platelet-derived growth factor AA (PDGF-AA) and erythropoietin (EPO) and lower levels of
410 interferon- γ (IFN- γ) compared to HC MDMi in 3D co-culture (**Fig. 4G-I**). This indicates that AD
411 MDMi exhibit an altered secretory activity in the 3D co-culture. Additionally, when comparing the
412 secretion to 3D MDMi mono-cultures, we observed a significant upregulation of PDGF-AA, EPO (**Fig.**
413 **4G, H**) and other neurotrophic factors such as Angiopoietin 2 and the granulocyte-macrophage colony
414 stimulating factor (GM-CSF) (**Fig. 4J, K**) in 3D co-cultures from both HC and AD cohorts. Secretion
415 of these factors by 3D ReNcell VM mono-cultures was higher for PDGF-AA and EPO and lower for
416 IFN- γ , Angiopoietin 2 and GM-CSF when compared to 3D MDMi mono-cultures (dotted lines in **Fig.**
417 **4G-K**). This suggests that the interaction between MDMi and ReNcell VM in the 3D co-cultures has
418 a functional impact on either cell type. Overall, these results suggest that the 3D co-culture platform
419 provides a suitable environment for AD MDMi to display functional impairments.

420 Microglia in the vicinity of A β plaques have been shown to exhibit altered proliferation, migration,
421 clustering around A β aggregates and A β uptake in a mouse model of AD (49). Hence, in order to study
422 MDMi behaviours in the presence of A β depositions, we added FITC-A β into 3D co-cultures from HC
423 individuals and AD patients and live imaged for 7 days (**Fig. 4L; Movie S3**). We observed that AD
424 MDMi surveyed longer distances and at a higher velocity around A β aggregates compared to HC
425 MDMi, with no significant changes in the proportion of MDMi that clustered around the A β aggregates
426 (**Fig. 4M-O**). Interestingly, measurement of inflammatory cytokine secretion using multiplex
427 immunoassay revealed disease-specific differences between HC and AD MDMi in 3D co-cultures
428 treated with FITC-A β . When A β was present in the cultures, IL-6 secretion was significantly decreased
429 in AD compared to HC 3D co-cultures, while increasing trends were observed for IL-1 β , IL-18 (**Fig.**
430 **4P**) and other pro-inflammatory cytokines such as TNF- α and IL-10 (**Fig. S7**). Such differences were
431 not observed under untreated conditions. Together, these results indicate that AD MDMi respond
432 differently to AD-related stressors compared to HC MDMi when modelled in the 3D co-culture
433 platform.

434 **Drug treatment induces differential cytokine gene expression in MDMi cultured in 2D and 3D**

435 Cytokines are key secreted molecules used by microglia to execute inflammatory and neuromodulatory
436 functions. Moreover, altered cytokine levels have been reported in AD brains and may have important
437 roles in disease pathogenesis (50). To investigate cytokine expression profiles in MDMi we analysed
438 a panel of inflammatory cytokines (*IL-6*, *TNF- α* , *IL-8*, *TGF- β* , *IL-10*, *IL-1 β* and *IL-18*) by qRT-PCR.
439 We then examined for potential differences 1) between culture platforms and 2) between HC and AD
440 cohorts. When comparing cytokine expression levels between platforms in the HC cohort, no
441 significant differences were observed for any of the cytokines (**Fig. 5A**). However, in the AD cohort,
442 *IL-8* was significantly downregulated in 3D co-culture compared to 3D MDMi mono-culture, and
443 *TGF- β* and *IL-18* were significantly downregulated in 3D co-culture compared to 2D MDMi (**Fig. 5B**).
444 When comparing between HC and AD MDMi in either platform, we observed a significantly
445 decreased expression of *TNF- α* in AD MDMi compared to HC only in the 3D MDMi platform (**Fig.**
446 **S8A**). No disease-specific differences were observed for the rest of cytokines (**Fig. S8B-G**). Together,
447 these results demonstrate cytokine changes dependent on platform, which were more evident in MDMi
448 from AD patients than HC individuals.

449 Based on the differences in baseline cytokine expression between platforms, we next investigated
450 whether drug treatment alters such platform-dependent responses in the HC and AD cohorts. For this,
451 we trialled two FDA-approved compounds, dasatinib and spiperone, which have anti-cancer and anti-
452 psychotic properties, respectively. Additionally, these drugs have been shown to mitigate
453 inflammation in *in vitro* models of microglia (51, 52) and murine models of AD (53) and have
454 potential as re-purposed drugs for treating neuroinflammation. Dasatinib-treated MDMi from HC
455 individuals showed a significantly reduced expression of *IL-6* in 3D compared to 2D MDMi, while
456 expression levels for the rest of cytokines remained unchanged between platforms (**Fig. 5C**).
457 Dasatinib-treated MDMi from AD patients showed a significantly increased expression of *IL-8*, *TGF- β*
458 and *IL-1 β* in 3D compared to 2D MDMi. Similarly, *IL-8* was upregulated in 3D co-cultures compared
459 to 2D MDMi (**Fig. 5D**). Spiperone-treated MDMi showed similar cytokine expression levels in all
460 platforms in the HC cohort (**Fig. S9A**) and a significant downregulation of *TNF- α* in 3D AD co-
461 cultures compared to 3D AD MDMi mono-cultures (**Fig. S9B**). When compared to untreated
462 conditions, dasatinib induced significant changes (*i.e.*, downregulation of *TGF- β* and *IL-1 β* in HC and
463 AD MDMi, respectively) only in the 2D platform (**Fig. 5C, D**), while spiperone did not significantly
464 alter cytokine expression in any platform (**Fig. S9A, B**).

465 Interindividual variability in drug responses was displayed using heatmaps, which show cytokine
466 expression levels in 2D and 3D MDMi from each individual in the HC and AD cohorts (**Fig. 5E, F**;
467 **Fig. S9C, D**). When comparing within HC individuals or AD patients, cytokine expression in MDMi
468 showed high heterogeneity in both 2D and 3D platforms. For example, in the dasatinib-treated HC

469 MDMi cohort, *IL-10* was highly expressed in 2D MDMi from individuals 1 and 3 compared to
470 individuals 4 and 5 (**Fig. 5E**). In the dasatinib-treated AD MDMi cohort, *IL-10* was highly expressed
471 in 2D MDMi from patients 2, 3, 6 and 7 compared to patients 4 and 8 (**Fig. 5F**). When considering
472 dasatinib-treated 3D MDMi, *IL-8* showed highly variable expression in HC and AD, with individual
473 4 and patient 3 showing a notably upregulated gene expression compared to the rest of patients (**Fig.**
474 **5E, F**). Importantly, differences between dasatinib-treated 2D and 3D MDMi in each particular HC or
475 AD individual were also demonstrated in the heatmaps. Some examples include divergent expression
476 levels of *IL-8* in HC individual 4, *IL-10* in HC individual 1 (**Fig. 5E**), *IL-8* in AD patient 3 and *IL-10*
477 in AD patients 2 and 3 (**Fig. 5F**). Similar trends in the heterogeneity of drug responses within and
478 between 2D and 3D MDMi were observed for spiperone-treated MDMi (**Fig. S9C, D**).
479 Overall, these results suggest that drug treatment induces differential cytokine expression in MDMi
480 from both HC individuals and AD patients in a culture platform-dependent manner.

481 **Discussion**

482 Research involving human microglia is hampered by the lack of model systems that faithfully
483 recapitulate their dynamic characteristics *in vivo*, particularly those associated with disease.
484 Generating more representative microglia model systems will address this shortcoming and help
485 elucidate microglia-mediated disease mechanisms, expediting pre-clinical investigations of microglia-
486 targeted therapeutics and better clinical outcomes (54).

487 Recreating physiologically relevant culture conditions to mimic the interaction of microglia with other
488 brain cell types and the extracellular matrix is crucial for accurately modelling the role of microglia in
489 disease. To date, no study has attempted to culture human microglia that have not been genetically
490 modified in a 3D system resembling human brain tissue. In an effort to develop more representative
491 *in vitro* models of human microglia, we used MDMi, a model system of microglia-like cells that has
492 emerged as a promising, patient-specific drug screening platform for neurological diseases (55, 56).
493 Previous reports have shown that MDMi morphologically and functionally resemble brain-resident
494 human microglia and express bonafide microglial markers (28-31). In this study, we developed novel
495 MDMi platforms that incorporate relevant *in vivo* cues resembling the microenvironment of the brain.
496 This was achieved by utilising a hydrogel-based 3D model to culture MDMi in microenvironments of
497 increasing complexity and physiological relevance, firstly as 3D MDMi mono-cultures and secondly
498 as 3D co-cultures of MDMi with neural progenitor cells.

499 Our study showed that a 3D hydrogel-based culture enhances MDMi survival, the extent and
500 complexity of ramification (branching) and the expression of mature microglial markers (*i.e.*,
501 *TMEM119*) compared to standard 2D culture conditions. In addition, we have demonstrated the
502 feasibility of culturing MDMi together with neuro-glial cells derived from human immortalised neural
503 progenitor cells (*i.e.*, ReNcell VM) in a 3D co-culture setting. Our findings also confirmed that MDMi
504 are capable of producing broad inflammatory responses upon exposure to inflammatory stimuli, which
505 is preserved in both 3D mono- and co-culture models.

506 We observed an enhanced maturation of microglial and neuro-glial cells in both our MDMi and
507 ReNcell VM 3D mono-cultures compared to 2D, in keeping with previous studies that used similar
508 3D cell models of primary rodent microglia and astrocytes (57, 58) and human induced neural stem
509 cell lines (59, 60). The enhanced maturation of microglia-like features in 3D MDMi could be attributed
510 to their increased survival in culture. Our model therefore shows two major advantages. Firstly, it
511 better mimics *in vivo* growth conditions. Secondly, it provides a longer time frame for differentiation
512 of monocytes into more mature MDMi that more closely represent brain microglia. Future studies

513 should examine whether MDMi in 3D co-culture develop an enhanced maturation of microglia-like
514 features compared to MDMi in 2D and 3D mono-cultures.

515 Microglia are involved in the pathogenesis of AD and contribute to the clinical heterogeneity observed
516 among patients. Hence, 3D MDMi models offer a great opportunity to study AD microglia in a patient-
517 specific manner. To investigate the capability of MDMi to model phenotypical features of AD
518 microglia in the 2D and 3D mono-culture and co-culture platforms, we generated MDMi cultures using
519 monocytes from living AD patients, a major advantage of our 3D AD MDMi platform. Unlike murine
520 or human immortalised microglia cell lines used in previous studies (45, 61), MDMi are patient-
521 derived and have not been genetically modified, being therefore more physiologically relevant and
522 clinically applicable. In addition, the use of cell samples obtained from living patients allows for
523 longitudinal modelling of disease progression in AD, a prerequisite for targeted treatment at various
524 stages of the disease.

525 We first compared cellular aspects in our 2D and 3D MDMi mono-culture models that have been
526 reported to be altered in microglia isolated from post-mortem AD patient brains. Analysis of the MDMi
527 branched morphology revealed similarities between HC and AD MDMi in both the 2D and the 3D
528 mono-culture models. These similarities most likely reflect age-related phenotypes described in human
529 AD microglia rather than activated phenotypes observed in microglia from AD mouse models. Indeed,
530 this age-related phenotype, termed HAM (human Alzheimer's microglia) was originally described in
531 myeloid cell populations isolated from human AD post-mortem brain samples at later stages of disease
532 (11). The HAM profile showed substantial overlap of age-associated gene expression patterns between
533 AD and control samples. Therefore, HC and AD MDMi are likely to have similar morphologies
534 irrespective of the culture platform. Our 3D platform revealed a failure of AD MDMi to fully increase
535 morphological complexity, particularly in relation to the number of quadruple junctions (points
536 connecting four sub-branches), compared to 2D. However, all complexity parameters, including
537 number of triple (points connecting three sub-branches) and quadruple junctions, were enhanced in 3D
538 HC MDMi compared to 2D. This potentially suggests that AD MDMi have an altered branching
539 complexity, only evident when culturing in a 3D platform. Microglial branches are highly dynamic
540 and constantly survey the brain microenvironment, phagocytosing dysfunctional synapses and
541 releasing trophic factors that support neural connectivity (62). Prior studies have identified a reduced
542 number of junctions in human AD microglial branches (63) and less AD microglial arborisation area
543 compared to age-matched HC (64). Our findings highlight that despite longer differentiation time in a
544 brain-like 3D structural environment, AD MDMi in 3D are not able to fully increase the outgrowth of
545 sub-branches in the same way as HC MDMi.

546 Gene expression of microglial AD risk genes, including *CLU*, *TREM2*, *PLCG2* and *PILRB*, in AD
547 MDMi, revealed an overall increased expression of AD risk genes in 3D compared to 2D mono-
548 cultures. However, there was prominent person-to-person variation in the expression level of the above
549 genes within both HC and AD cohorts, which reflects clinical heterogeneity observed in patients.
550 Importantly, *PILRB* (an activating immune receptor) was significantly upregulated in AD MDMi 3D
551 mono-cultures compared to HC, which suggests that the 3D MDMi model provides a suitable
552 screening platform with improved clinical translation to identify other AD risk genes and microglia-
553 targeted therapeutics.

554 To assess the fidelity of AD MDMi in recapitulating disease-specific alterations in 3D co-cultures, we
555 evaluated aspects such as the interaction of MDMi with neuro-glial cells, their secretory profiles and
556 migration around A β aggregates. As previously described, microglia establish physical contacts with
557 neurons through identified molecular mechanisms (65). Our results showed reduced physical contacts
558 between AD MDMi and ReNcell VM-derived neuro-glial cells compared to HC. Alterations in such
559 microglia-neuron interactions could impact the microglial capacity to respond to neuronal damage,
560 providing a potential mechanism underlying neuron degeneration in AD.

561 Microglia in AD and ageing have dysfunctional secretomes (66). We observed altered secretion
562 patterns of PDGF-AA, EPO and IFN- γ in AD 3D co-cultures when compared to HC, in agreement
563 with previous observations in AD patients. An unbalanced distribution of PDGF-AA immunopositive
564 cells has been linked to gliosis in AD post-mortem brains (67). Moreover, protein expression levels of
565 EPO receptors in astrocytes have been found to be altered in post-mortem hippocampal brain sections
566 from AD patients (68). Likewise, plasma levels of IFN- γ have been shown to fluctuate according to
567 disease severity in AD patients (69) and studies in mice have demonstrated that IFN- γ impacts
568 neurogenesis and synaptic plasticity (70). Taken together, our findings suggest that MDMi in 3D co-
569 culture recapitulate alterations reported in AD patients and are therefore an exciting new platform for
570 disease modelling.

571 Microglia have a canonical role in the removal of A β aggregates (71). In order to validate the functional
572 response of MDMi to A β aggregates, we investigated the behaviour of these cells in 3D co-culture in
573 the presence of A β aggregates. Our results showed that AD MDMi migrate longer distances at a faster
574 speed compared to HC. Similarly, elevated migration rates were observed in human immortalised
575 microglia cultured in a 3D tri-culture model with ReNcell VM overexpressing pathogenic A β species
576 (45). However, an AD mouse model with aberrant A β production showed decreased microglial
577 migration towards A β plaques (72), highlighting important differences between human and murine
578 microglia responses to A β . Our findings warrant further investigation of microglial motility as a

579 potentially dysregulated cellular feature in AD brains. Whether an increase in surveillance and speed
580 of AD MDMi correlates with an impaired branched complexity in these cells remains to be elucidated
581 in future studies.

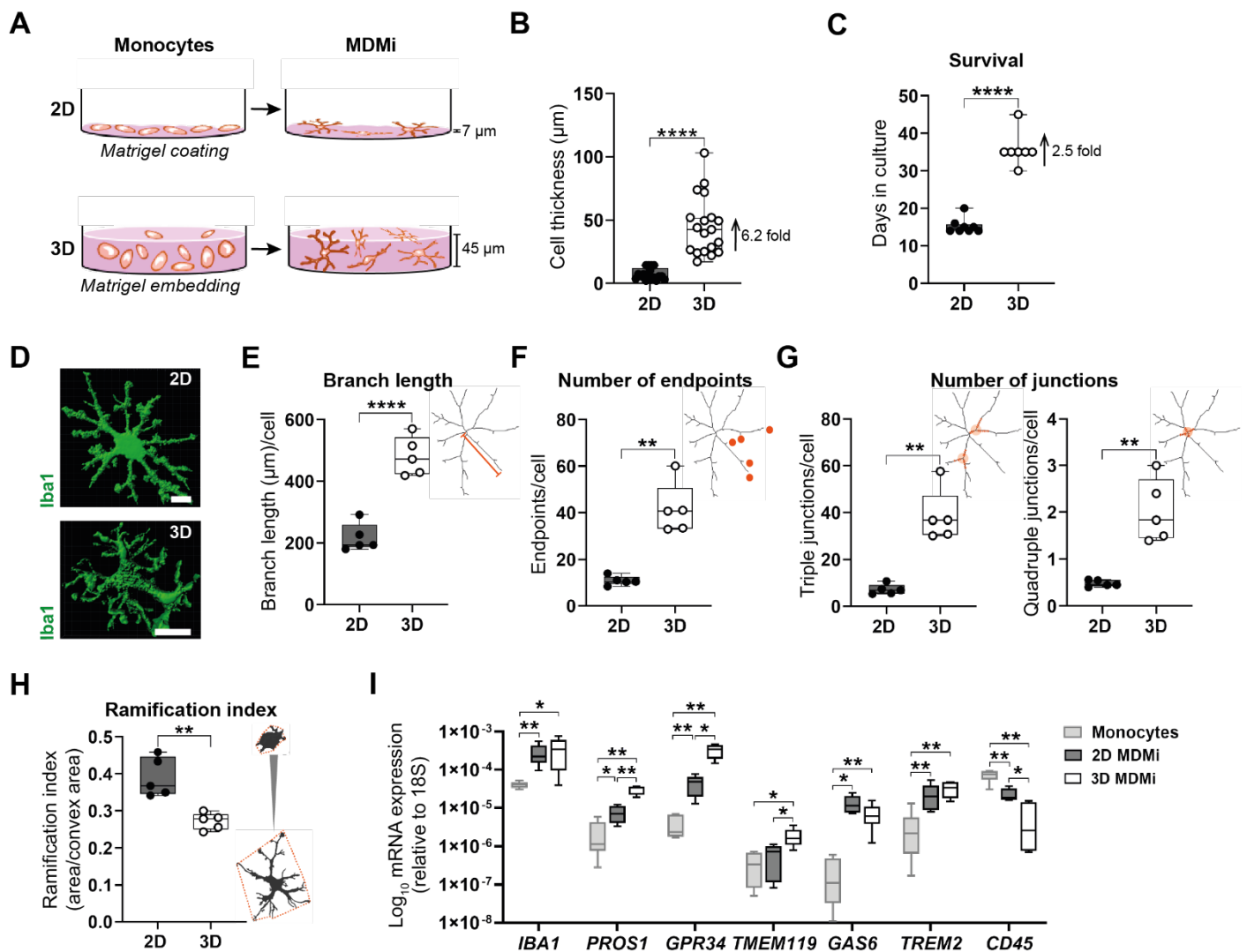
582 Interestingly, we did not observe differences in the number of MDMi that clustered around A β
583 aggregates. However, we observed changes in pro-inflammatory cytokine secretion in MDMi from
584 AD compared to HC. Altogether, this suggests that AD MDMi may have unique disease-specific
585 chemotactic and secretory responses against A β . Future studies should investigate how such changes
586 in MDMi impact the phagocytic clearance of A β aggregates in the 3D co-cultures. Overall, disease-
587 specific differences exhibited by AD MDMi in the 3D co-culture platform confirm the possibility to
588 model disease in AD patient-specific MDMi using culture platforms that better recapitulate the brain
589 microenvironment.

590 Preliminary drug testing demonstrated the utility of the 3D MDMi models as personalised drug
591 screening tools. The main reasons are as follows. First, differences in MDMi drug responses between
592 2D and 3D culture conditions reflect the functional impact of MDMi cultured in a more biologically
593 relevant 3D environment. This is in agreement with a previous study carried out on tumour cell lines,
594 which described varied treatment outcomes relating to cell proliferation depending on the culture
595 system (73). Moreover, another study reported more similarities in drug-induced cellular responses
596 between 3D cultures and *in vivo* conditions than compared to 2D cultures (74). Future investigations
597 should determine whether drug responses from our 3D MDMi models correlate better with responses
598 identified in animal models and clinical data from patients. Second, patient heterogeneity in MDMi
599 drug responses was evident, supporting the translatability of our 3D platforms to measure individual
600 patient responses in the clinic and further validating our *in vitro* systems as promising alternative
601 platforms for personalised drug screening.

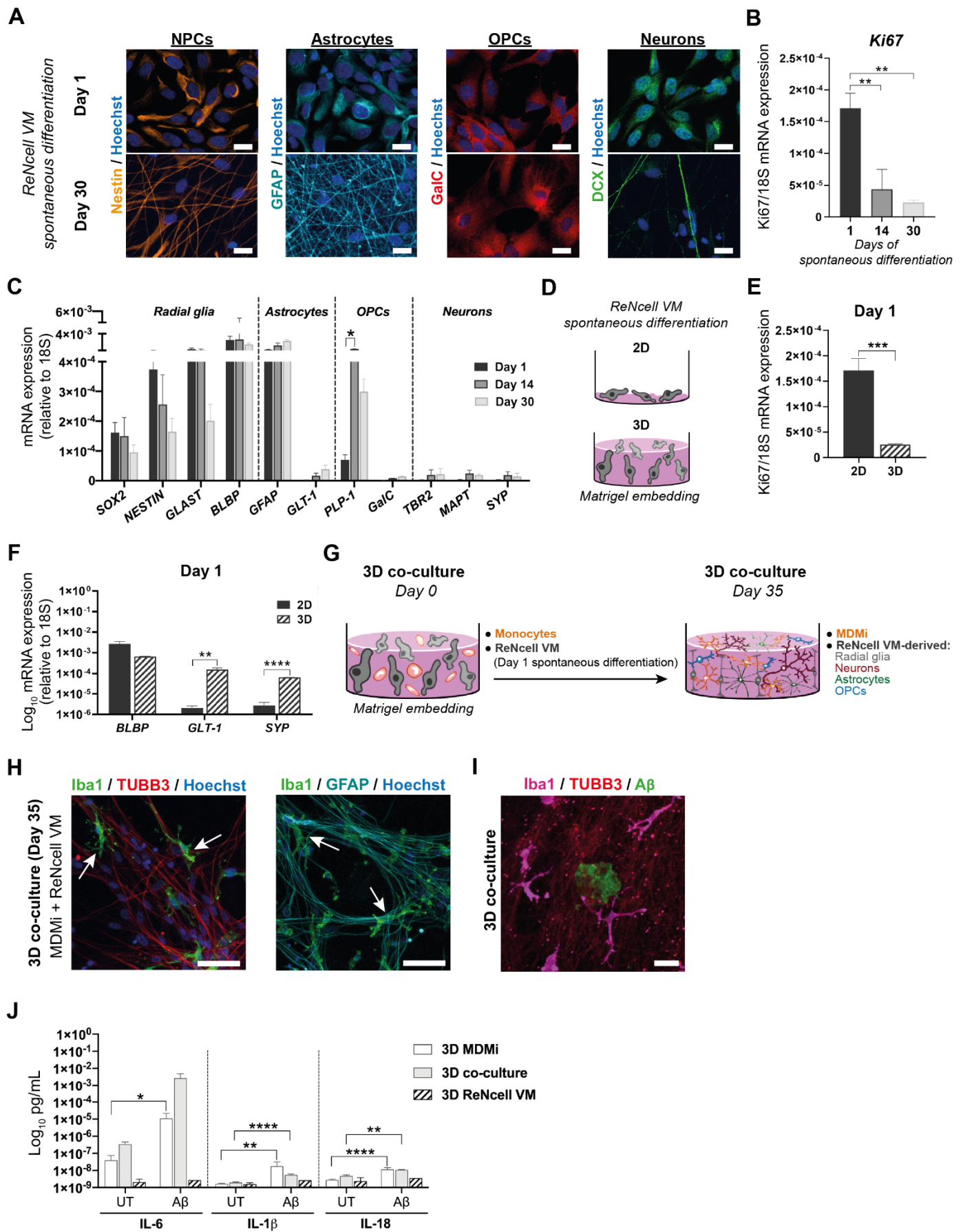
602 To further enhance our 3D MDMi model systems, microfluidic technology that accounts for the
603 dynamic interstitial fluid flow within the brain could be used (75). Moreover, the addition of patient
604 hiPSC-derived neural progenitor cells into the 3D MDMi co-cultures would make this platform more
605 personalised and likely a more accurate representation of the human brain. Finally, more-defined
606 synthetic hydrogels may enable us to more carefully dissect the functionality of MDMi in 3D cultures
607 given their consistent and tuneable properties.

608 In conclusion, we describe reproducible and easy-to-generate 3D *in vitro* models of MDMi that are
609 able to recapitulate potentially important AD-specific differences associated with diseased microglia,
610 not identified in 2D models. This study opens new doors to generate patient-specific drug testing

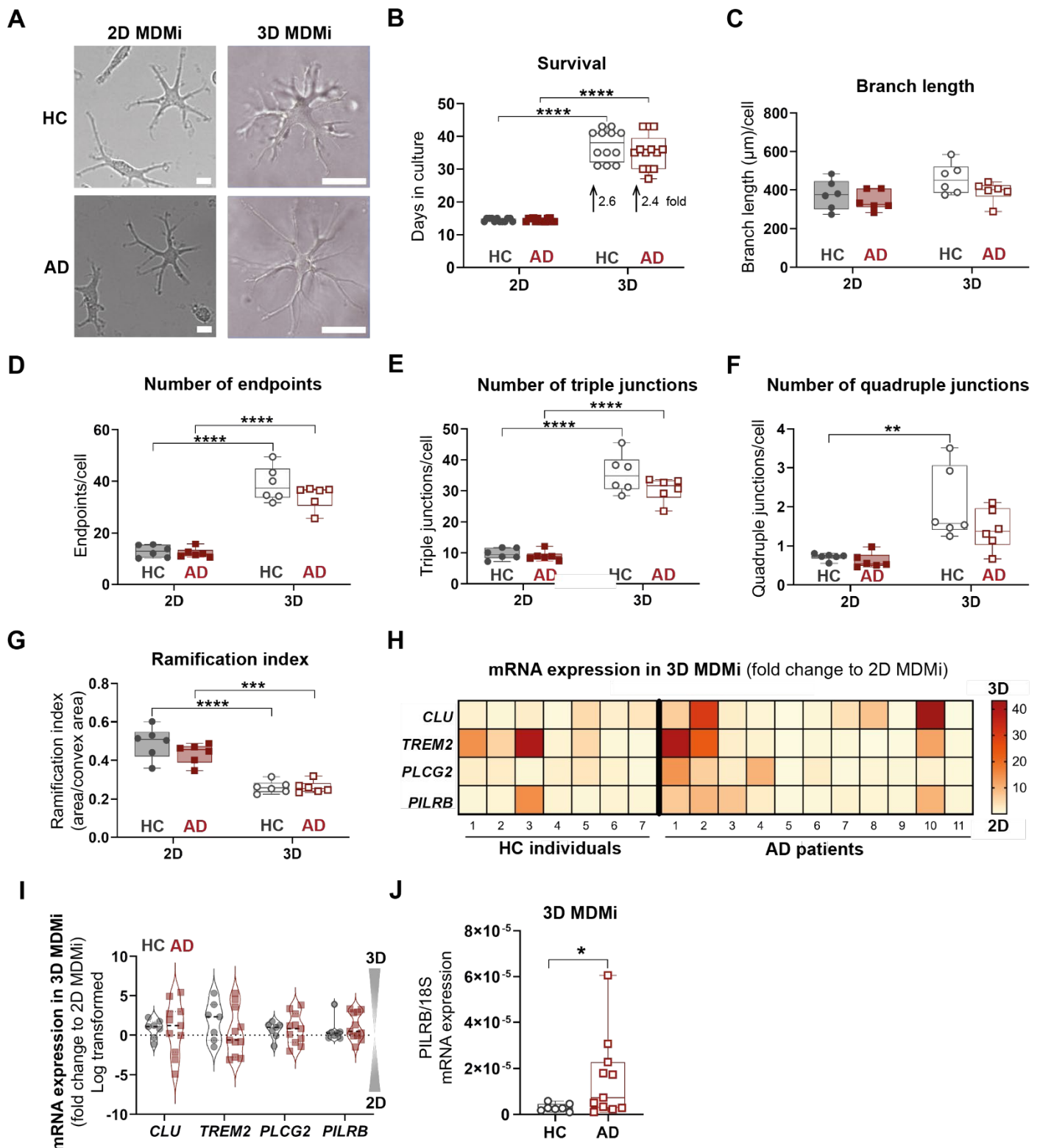
611 platforms that support the development of microglia-targeted therapeutic interventions tailored for AD
612 patients and potentially other neurological disorders.



613 **Fig. 1. Generation and characterisation of distinctive microglia features in 2D and 3D MDMi.**
 614 (A) Schematic illustration of monocyte differentiation into MDMi in 2D, achieved by seeding the monocytes on a Matrigel-coated surface, or in 3D, achieved by embedding the monocytes in a thick
 615 Matrigel layer. (B) Cell thickness of MDMi in 2D ($n = 17$ independent cultures) and 3D ($n = 19$
 616 independent cultures) cultures. (C) Survival of 2D ($n = 8$) and 3D MDMi ($n = 7$). (D) 3D surface
 617 rendered images of 2D and 3D MDMi stained for Iba1 (green). Scale bars, 25 μm . Quantification of
 618 morphological parameters in 2D ($n = 5$) and 3D MDMi ($n = 5$), including (E) branch length, (F)
 619 number of endpoints, (G) number of junctions, including triple junctions (left) and quadruple junctions
 620 (right) and (H) ramification index (area/convex area). Representative skeleton and binary images are
 621 included on the right of each graph to illustrate the morphological measurements. (I) mRNA
 622 expression of microglia- (*IBA1*, *PROS1*, *GPR34*, *TMEM119*, *GAS6*, *TREM2*) and leukocyte-enriched
 623 (*CD45*) markers in the starting monocyte population ($n = 6$) and the resulting 2D ($n = 7$) and 3D ($n =$
 624 6) MDMi cultures. Data are presented as mean \pm SD. Each single data point represents one biological
 625 replicate. Unpaired Student's t test with or without Welch's correction, two-tailed; one-way ANOVA
 626 with Tukey's multiple comparison test in I; * $P < 0.05$, ** $P < 0.01$, **** $P < 0.0001$.

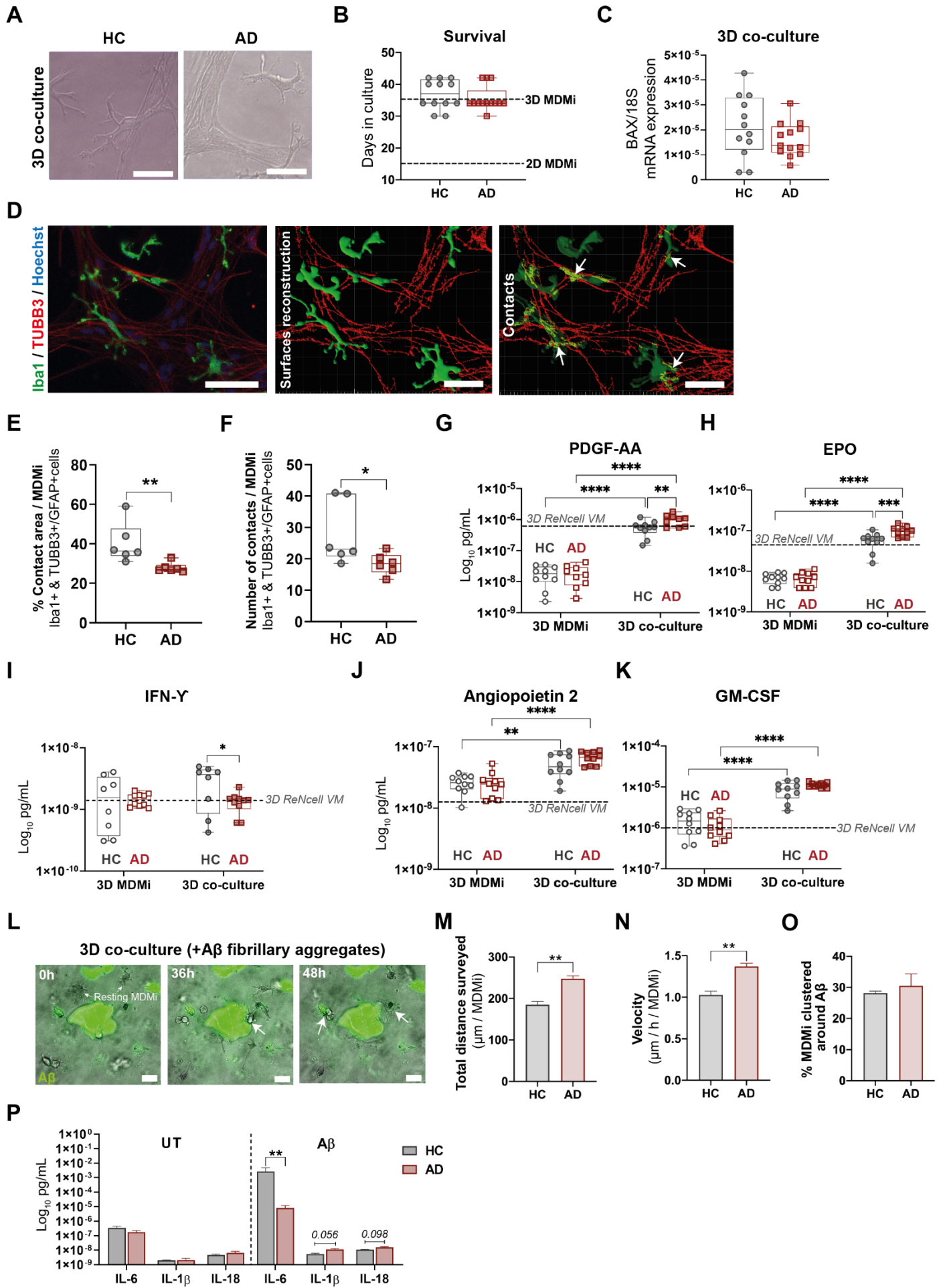


628 **Fig. 2. MDMi in 3D co-culture with ReNcell VM-derived neuro-glial cells exhibit inflammatory**
629 **responses towards A β aggregates. (A)** Immunostaining of 2D ReNcell VM cultures differentiated
630 for 1 and 30 days shows expression of characteristic markers of neural progenitor cells (NPCs; Nestin),
631 astrocytes (GFAP), oligodendrocyte progenitor cells (OPCs; GalC) and neurons (Doublecortin, DCX).
632 Scale bars, 100 μ m. **(B)** *Ki67* mRNA expression in 2D ReNcell VM cultures differentiated for 1, 14
633 or 30 days ($n = 3$ independent experiments). **(C)** mRNA expression of a panel of radial glia (NPCs),
634 astrocytes, OPCs and neuron markers in 2D ReNcell VM at days 1, 14 and 30 of spontaneous
635 differentiation ($n = 3$ independent experiments). **(D)** Schematic of ReNcell VM cultures undergoing
636 spontaneous differentiation for 1 day in 2D, or in 3D upon embedment in Matrigel. mRNA expression
637 of **(E)** the proliferation marker *Ki67* alongside the **(F)** the radial glia marker *BLBP*, the mature astrocyte
638 marker *GLT-1* and the mature neuron marker *Synaptophysin (SYP)* in 2D ($n = 3$ independent
639 experiments) and 3D ($n = 3$ independent experiments) ReNcell VM cultures spontaneously
640 differentiated for 1 day. **(G)** Schematic depicting how the 3D co-culture is generated: monocytes pre-
641 mixed with Matrigel are added to a 3D culture of ReNcell VM differentiated for 1 day (left). The co-
642 culture is left to differentiate for 35 days, giving rise to a mixed population of MDMi with ReNcell
643 VM-derived neuro-glial cells (right). **(H)** Immunofluorescence analysis of MDMi and ReNcell VM
644 3D co-culture at day 35 of differentiation. MDMi were stained for Iba1 (arrows) and ReNcell VM
645 were stained for β 3-tubulin (TUBB3) and GFAP. Scale bars, 100 μ m. **(I)** Immunofluorescence image
646 of 3D co-cultures containing FITC-A β aggregates. Scale bar, 100 μ m. **(J)** Concentration of secreted
647 pro-inflammatory cytokines IL-6, IL-1 β and IL-18 by 3D MDMi ($n = 2$) and ReNcell VM ($n = 1$)
648 mono-cultures and 3D co-cultures ($n = 3$) upon exposure to FITC-A β aggregates. Data are presented
649 as mean \pm SEM. One-way ANOVA with Tukey's multiple comparison test in **B, C**; unpaired Student's
650 *t* test with or without Welch's correction, two-tailed in **E, F, J**; * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$,
651 **** $P < 0.0001$.

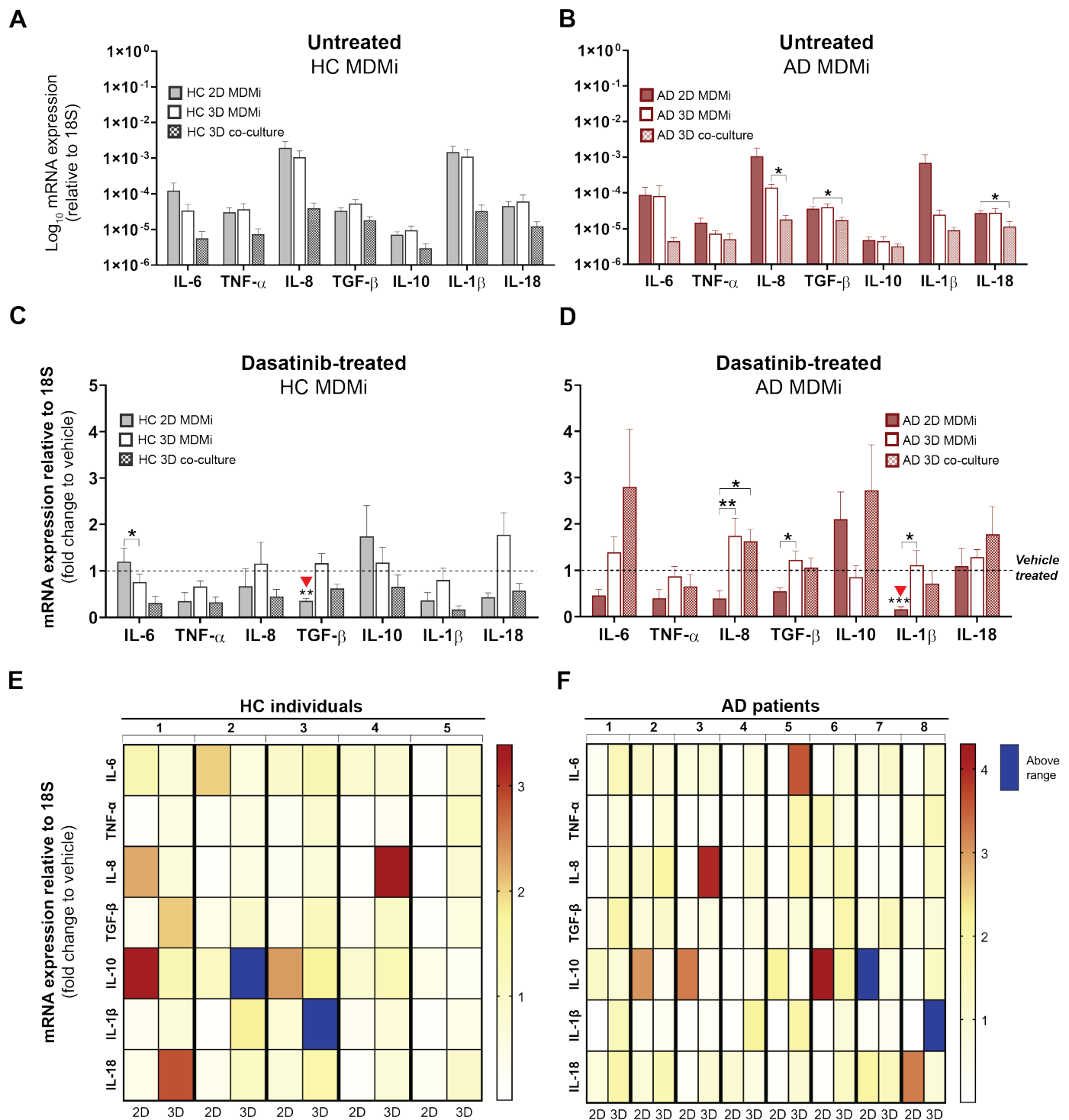


652 **Fig. 3. AD-associated phenotypes in 2D and 3D MDMi mono-cultures related to morphology and**
 653 **expression of AD risk genes. (A)** Representative bright field images of HC and AD MDMi in 2D and
 654 3D mono-cultures. Scale bars, 100 μ m. **(B)** Survival of HC ($n = 12$) and AD ($n = 13$) MDMi in 2D and
 655 3D mono-cultures. Quantification of morphological parameters in 2D and 3D MDMi from both HC
 656 ($n = 6$) and AD ($n = 6$) cohorts, including **(C)** branch length, **(D)** number of endpoints, **(E)** number of
 657 triple junctions, **(F)** number of quadruple junctions and **(G)** ramification index. **(H)** Heatmap
 658 representing HC ($n = 7$) and AD ($n = 11$) individual-specific fold changes in gene expression levels of

659 the AD risk genes *CLU*, *TREM2*, *PLCG2* and *PILRB* in 3D MDMi compared to 2D. Red-yellow colour
660 spectrum shows relative fold change of 3D MDMi as compared to 2D MDMi. **(I)** Violin plot
661 representation of fold change (log transformed) of mRNA expression in 3D to 2D HC ($n = 7$) and AD
662 ($n = 11$) MDMi. **(J)** mRNA expression of the AD risk gene *PILRB* in 3D HC ($n = 7$) and AD ($n = 11$)
663 MDMi. Data are presented as mean \pm SD. Each single data point represents one biological replicate.
664 Two-way ANOVA with Tukey's multiple comparison test; unpaired Student's t test with or without
665 Welch's correction, two-tailed in **I**; * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, **** $P < 0.0001$.



666 **Fig. 4. AD-associated phenotypes in 3D co-cultures related to cell-to-cell interaction with ReNcell**
667 **VM, secretory activity and responses to A β aggregates. (A)** Representative bright field images of
668 HC and AD co-cultures. Scale bars, 100 μ m. **(B)** Survival of HC ($n = 12$) and AD ($n = 13$) MDMi in
669 3D co-cultures. **(C)** Gene expression of the pro-apoptotic marker *BAX* in HC ($n = 12$) and AD ($n = 13$)
670 3D co-cultures. **(D)** Immunostaining against Iba1 (green) and TUBB3 (red) and 3D surface
671 reconstruction of a 3D co-culture. Areas of contact between Iba1+ (MDMi) and TUBB3+ (ReNcell
672 VM) cells are highlighted in yellow (white arrows). Scale bars, 100 μ m. Quantification of **(E)** contact
673 area and **(F)** number of contacts between Iba1+ and TUBB3+/GFAP+ cells in HC ($n = 6$) and AD (n
674 = 6) 3D co-cultures. Concentration of **(G)** platelet-derived growth factors AA (PDGF-AA), **(H)**
675 erythropoietin (EPO), **(I)** interferon- γ (IFN- γ), **(J)** angiopoietin 2 and **(K)** granulocyte-macrophage
676 colony stimulating factor (GM-CSF) secreted by HC ($n = 8-10$) and AD ($n = 9-10$) MDMi in 3D mono-
677 cultures and co-cultures. Baseline secretion by 3D ReNcell VM mono-cultures is represented with a
678 dotted black line. **(L)** Representative images of 3D co-cultures containing FITC-A β aggregates in
679 which MDMi exhibit a resting, ramified morphology at 0h and progressively become polarised
680 acquiring an activated, round morphology with enlarged soma upon reaching and clustering on the A β
681 deposit at 36 h and 48 h (white arrows). Scale bars, 100 μ m. **(M)** Total surveillance distance, **(N)**
682 velocity and **(O)** clustering around A β aggregates of HC ($n = 2$) and AD ($n = 4$) MDMi in 3D co-
683 cultures containing A β aggregates. **(P)** Concentration of pro-inflammatory cytokines IL-6, IL-1 β and
684 IL-18 secreted by untreated (UT) and A β -treated HC ($n = 3$) and AD ($n = 4$) MDMi in 3D co-cultures.
685 Data are presented as mean \pm SD in **B, C, E-K**; mean \pm SEM in **M-P**. Each single data point represents
686 one biological replicate. Unpaired Student's *t* test with or without Welch's correction, two-tailed in **B,**
687 **C, M-P**; Mann-Whitney test, two-tailed in **E, F**; two-way ANOVA with Tukey's multiple comparison
688 test in **G-K**; * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, **** $P < 0.0001$.



689 **Fig. 5. Dasatinib treatment induces cytokine expression responses that differ between culture**
 690 **format and are heterogeneous among HC and AD MDMi.** Log-transformed mRNA expression of
 691 the inflammatory cytokines IL-6, TNF- α , IL-8, TGF- β , IL-10, IL-1 β and IL-18 in untreated (A) HC (n
 692 = 8) MDMi and (B) AD (n = 12) MDMi in all culture formats (2D and 3D mono-cultures and 3D co-
 693 cultures). Fold change in cytokine mRNA expression levels following 24 h exposure to 100nM
 694 dasatinib compared to vehicle (DMSO)-treated cultures in (C) HC (n = 6) and (D) AD (n = 8) 2D and
 695 3D MDMi mono-cultures and 3D co-cultures. Red arrowheads indicate significance compared to
 696 vehicle-treated condition. Dotted black lines represent baseline responses of vehicle-treated cultures.
 697 Heatmaps showing (E) HC (n = 5) and (F) AD (n = 8) donors-specific changes in mRNA expression

698 from MDMi mono-cultures in 2D and 3D. Red-yellow colour spectrum represents relative fold change
699 of mRNA expression after dasatinib treatment compared to vehicle. Expression changes falling outside
700 the displayed range are indicated in dark blue. Data are presented as mean \pm SEM. One-way ANOVA
701 with Dunnett's multiple comparison test; $**P < 0.01$, $**P < 0.01$, $***P < 0.001$.

702 **Acknowledgements:** We would like to thank the volunteers from QIMR Berghofer who have donated
703 blood to this project and the participants recruited through the PISA study. We also thank the
704 Microscopy, Flow cytometry, Sample Processing and Statistical teams at QIMR Berghofer for their
705 assistance. Special thanks to Kurt Giuliani for helpful insights on LEGENDplex™ data analysis. Lastly,
706 we acknowledge the coordinators of the PISA study, Professor Michael Breakspear, Jessica Adsett
707 and Natalie Garden.

708 **Funding:** This study was supported by grants from NHMRC (APP1125796). PISA is funded by a
709 National Health and Medical Research Council (NHMRC) Boosting Dementia Research Initiative
710 Team Grant (APP1095227). C.C-L. is recipient of The University of Queensland PhD scholarship.
711 M.K.L. is supported by an NHMRC Boosting Dementia Leadership Fellowship (APP1140441).
712 A.R.W. is supported by an NHMRC Senior Research Fellowship (APP1118452).

713 **Author contributions:** C.C-L., H.Q., L.E.O. and A.R.W. conceived and designed the study. C.C-L.
714 and H.Q. performed experiments. C.C-L., H.Q. and T.H.N. analysed data. C.C-L., H.Q., R.S. and
715 A.R.W. interpreted data. Y.S., C.C.G. and M.K.L. coordinated blood collection from the PISA study.
716 C.C-L. wrote the manuscript. H.Q., R.S., L.E.O. and A.R.W. provided critical feedback in reviewing
717 and editing. All authors reviewed and commented on the final version of the manuscript.

718 **Competing interests:** A.R.W. and H.Q. are listed as co-inventors of provisional patent
719 AU2020/050513. The authors declare no other competing interests.

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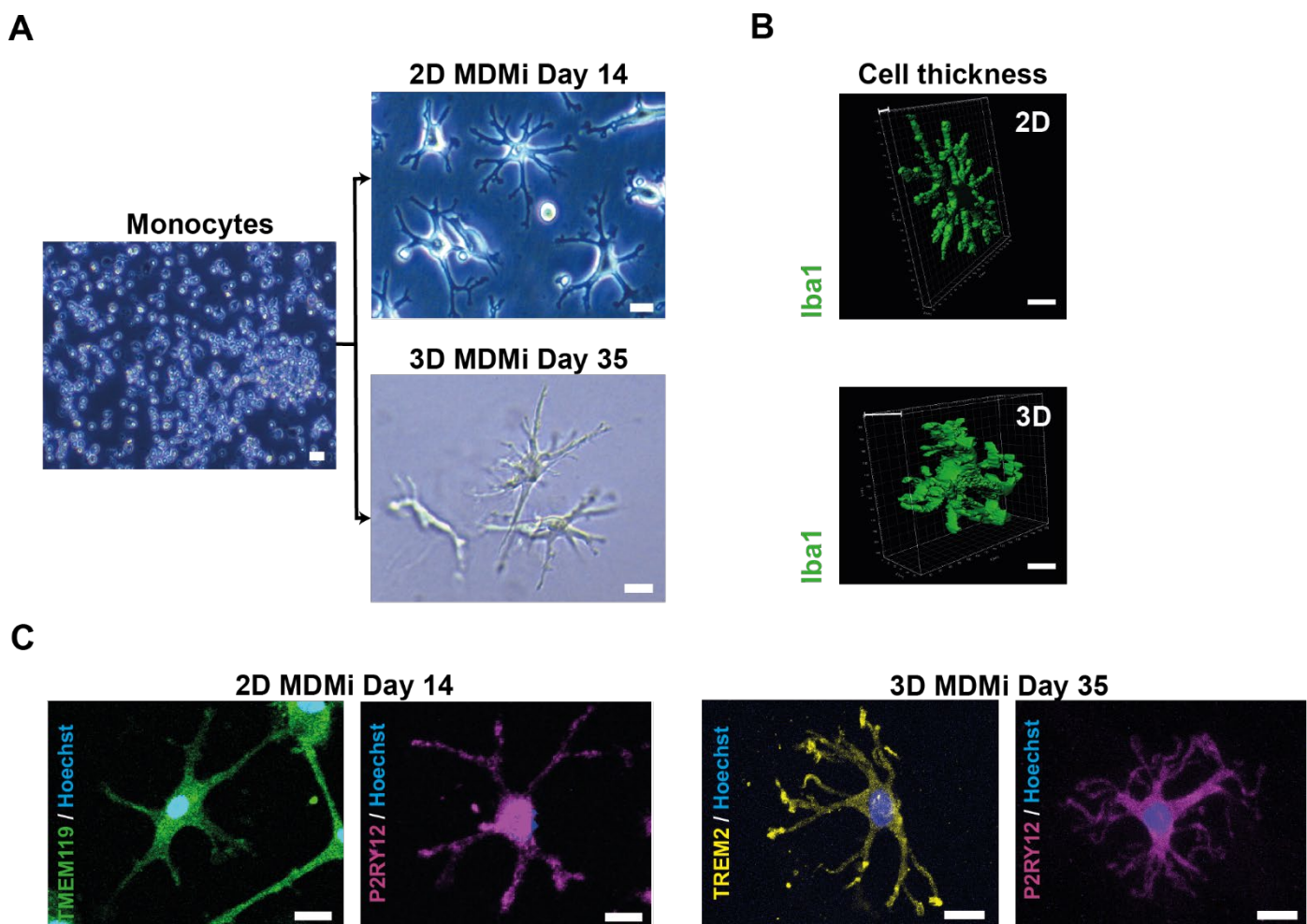
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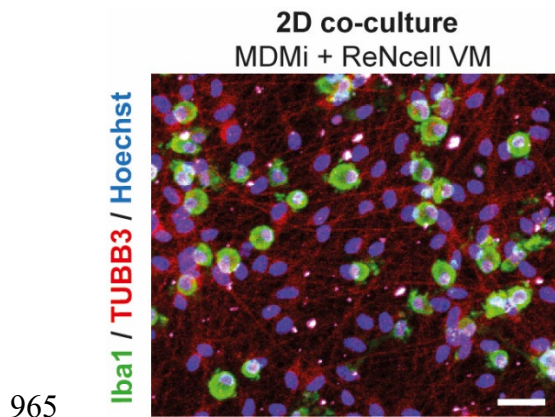
957 **Table S1. qRT-PCR primer sequences.**

Primer	Forward sequence	Reverse sequence	Size (bp)
<i>18S</i>	TTCGAGGCCCTGTAATT GGA	GCAGCAACTTTAATATA CGCTATTGG	123
<i>IBA1</i>	TGCCATCCTAAAAATG ATCCTGATG	AGATAGCTTTCTTGGCTG GGG	86
<i>CD45</i>	GCAGCTAGCAAGTGGT TTGTTC	AAACAGCATGCGTCCTT TCTC	92
<i>PROS1</i>	TTGCACTTGTAACCAG GTTGG	CAGGAACAGTGGTAACT TCCAG	132
<i>GAS6</i>	CTCTCTCTGTGGCACTG GTA	CCTTGATCTCCATTAGGG CCAA	105
<i>GPR34</i>	CCTGATGTCCAGTAAC ATTCGC	CATGCAGGGAGTATCCT GGT	116
<i>TREM2</i>	TCTTTGTACACAGAGCTG TCC	TCATAGGGGCAAGACAC CTG	88
<i>TMEM119</i>	CTTCCTGGATGGGATA GTGGAC	GCACAGACGATGAACAT CAGC	96
<i>KI67</i>	GAGGTGTGCAGAAAAT CCAAA	CTGTCCCTATGACTTCTG GTTGT	78
<i>SOX2</i>	CCACCTACAGCATGTCC TACTCG	GGGAGGAAGAGGTAACC ACAGG	117
<i>NESTIN</i>	CTCAGCTTTCAGGACCC CAA	GTCTCAAGGGTAGCAGG CAA	183
<i>GLAST</i>	GGTTGCTGCAAGCACT CATCAC	CACGCCATTGTTCTCTTC CAGG	95
<i>BLBP</i>	GGCTTTGCCACTAGGC AGG	TGACCACTTTGTCTCCTT CTTGA	76
<i>GFAP</i>	GAGGTTGAGAGGGACA ATCTGG	GTGGCTTCATCTGCTTCC TGTC	128
<i>GLT-1</i>	TAGCCGCCATCTTTATA GCC	CGGCTGTCAGAATGAGG AGC	150
<i>PLP-1</i>	GGCCACTGGATTGTGTT TCT	AGGTGGTCCAGGTGTTG AAG	386-491
<i>GalC</i>	GCAACCTCCCGACTTCT AGTA	ACCACTCGTATCCTCGG AAATA	199
<i>TBR2 (EOMES)</i>	CGGCCTCTGTGGCTCAA A	AAGGAAACATGCGCCTG C	76
<i>MAPT</i>	CTCGCATGGTCAGTAA AAGCAA	GGGTTTTTGTGCTGGAATCC TGGT	153
<i>Synaptophysin (SYP)</i>	CTGCAATGGGTCTTCGC CA	ACTCTCGGTCTTGTGGC AC	96
<i>PILRB</i>	CCATCAAGGGGACCAA ACTCA	TCTGAGTGCCCTTTGCTT TC	118
<i>BAX</i>	TGGCAGCTGACATGTTT TCTGAC	TCACCAACCACCCTGG TCTT	195
<i>IL-6</i>	TGCAATAACCACCCT GACC	TGCGCAGAATGAGATGA GTTG	104

<i>IL-8</i>	AGACAGCAGAGCACAC AAGC	ATGGTTCCTTCCGGTGGT	62
<i>IL-10</i>	TGCTGGAGGACTTTAA GGGTTA	GATGCCTTTCTCTTGGAG CTTA	254
<i>TNF-α</i>	CAGCCTCTTCTCCTTCC TGAT	GCCAGAGGGCTGATTAG AGA	123
<i>TGF-β</i>	CGCGTGCTAATGGTGG AAA	CTCGGAGCTCTGATGTG TTGAA	97
<i>IL-1β</i>	AATCTGTACCTGTCCTG CGTGTT	TGGGTAATTTTGGGATC TACTCT	78
<i>IL-18</i>	AACAACTATTTGTTCG AGGAAT	TGCCACAAAGTTGATGC AAT	72



958 **Fig. S1. 2D and 3D MDMi show different cell thickness and positive immunostaining for**
 959 **microglia-enriched markers.** (A) Representative bright field images of monocytes and 2D and 3D
 960 MDMi after 14 (top) or 35 (bottom) days of differentiation, respectively. Scale bars, 25 μ m. (B)
 961 3D reconstruction images of Iba1-stained MDMi and thickness of 2D and 3D MDMi. Scale bars, 25
 962 μ m. (C) Immunofluorescence of 2D and 3D MDMi for TMEM119, P2RY12 and TREM2. Scale bars, 25
 963 μ m.
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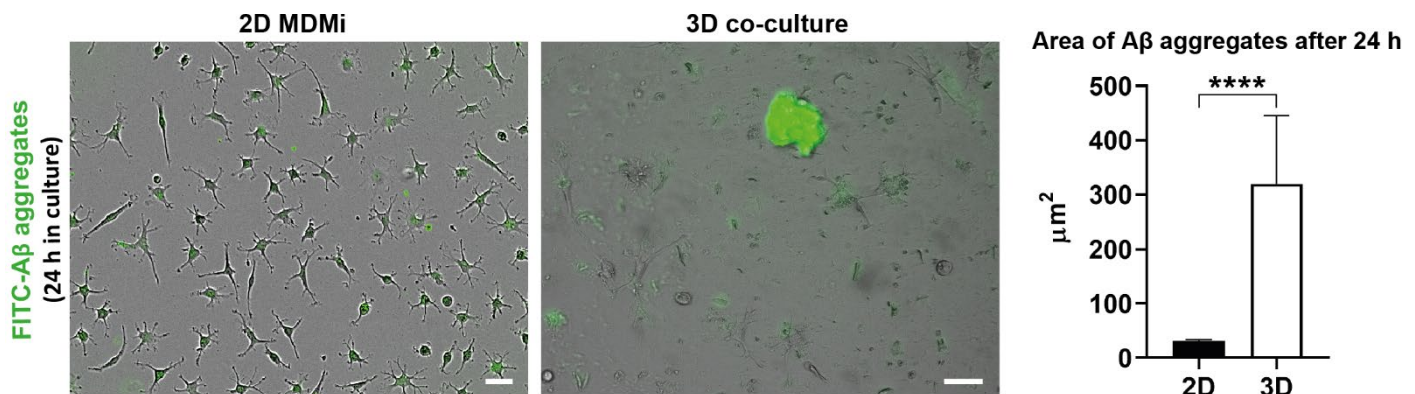
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Fig. S2. Characterisation of 2D MDMi and ReNcell VM co-cultures. MDMi co-culture with ReNcell VM-derived neuro-glial cells in 2D is insufficient for monocyte differentiation into MDMi, as monocytes retain a round morphology after 40 days in 2D co-culture. MDMi were stained for Iba1 and ReNcell VM were stained for β 3-tubulin (TUBB3). Scale bar, 100 μ m.



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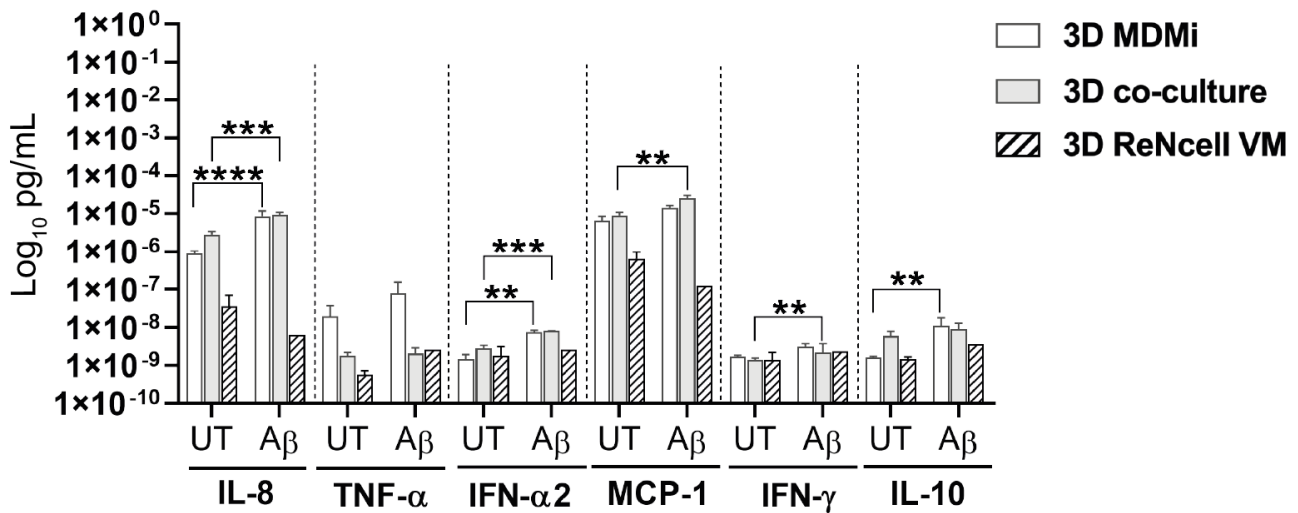
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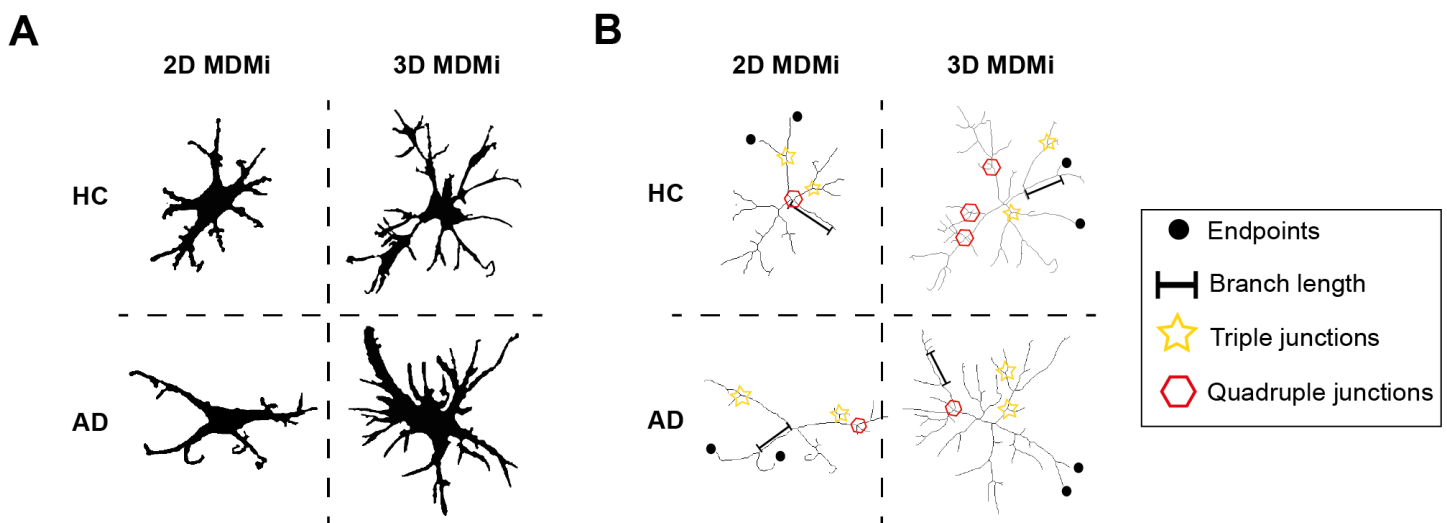
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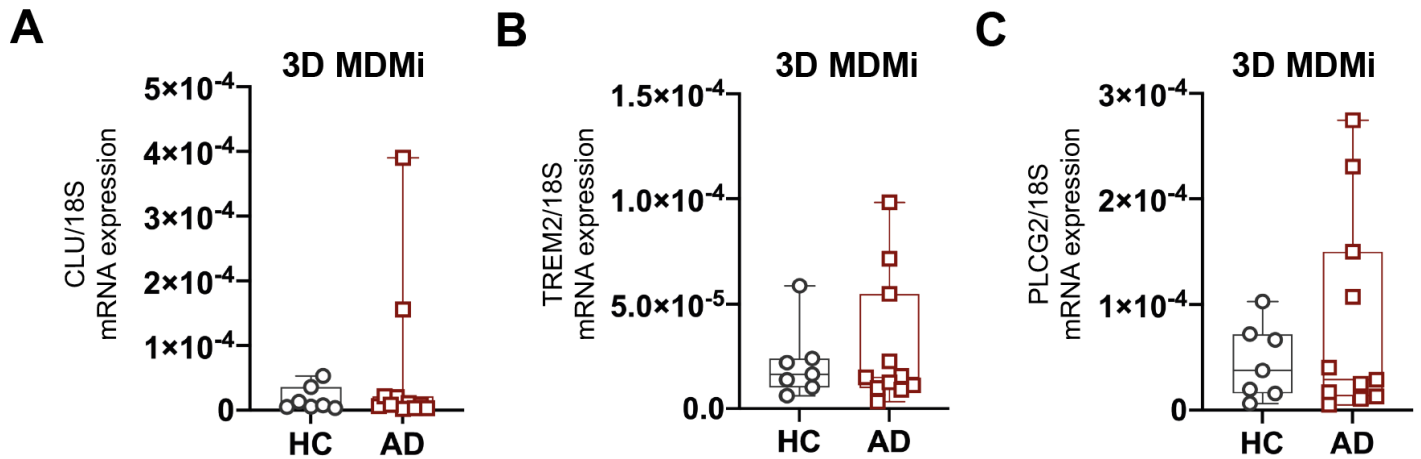
Fig. S3. FITC-A β peptides form larger aggregates in 3D compared to 2D after 24 h in culture. FITC-A β peptides were added to 2D MDMi and 3D co-cultures. Imaging was conducted following incubation for 24 h. Area of A β aggregates (μ m²) was quantified for comparison between the 2D MDMi ($n = 3$) and 3D co-cultures ($n = 3$). Scale bars, 100 μ m. Data are presented as mean \pm SEM. Mann-Whitney test, two-tailed; **** $P < 0.0001$.



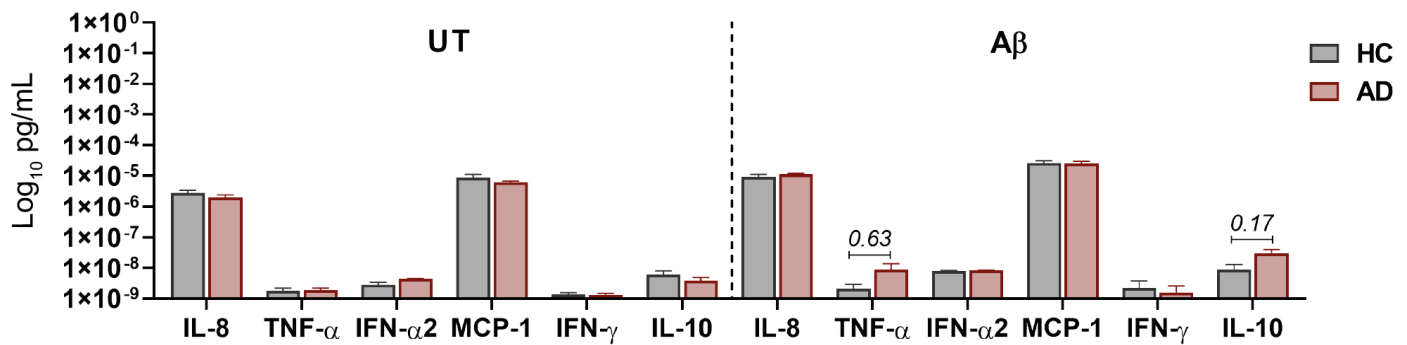
975 **Fig. S4. Pro-inflammatory cytokine secretion profiles of 3D MDMi, 3D co-culture and 3D**
 976 **ReNcell VM.** Concentration of secreted pro-inflammatory cytokines IL-8, TNF-α, IFN-α2, MCP-1,
 977 IFN-γ and IL-10 by 3D MDMi ($n = 2$) and ReNcell VM ($n = 1$) mono-cultures and 3D co-cultures (n
 978 $= 3$) upon exposure to FITC-Aβ aggregates for 7 days. Data are presented as mean ± SEM. Unpaired
 979 Student's t test with or without Welch's correction, two-tailed; ** $P < 0.01$, *** $P < 0.001$, **** $P <$
 980 0.0001 .



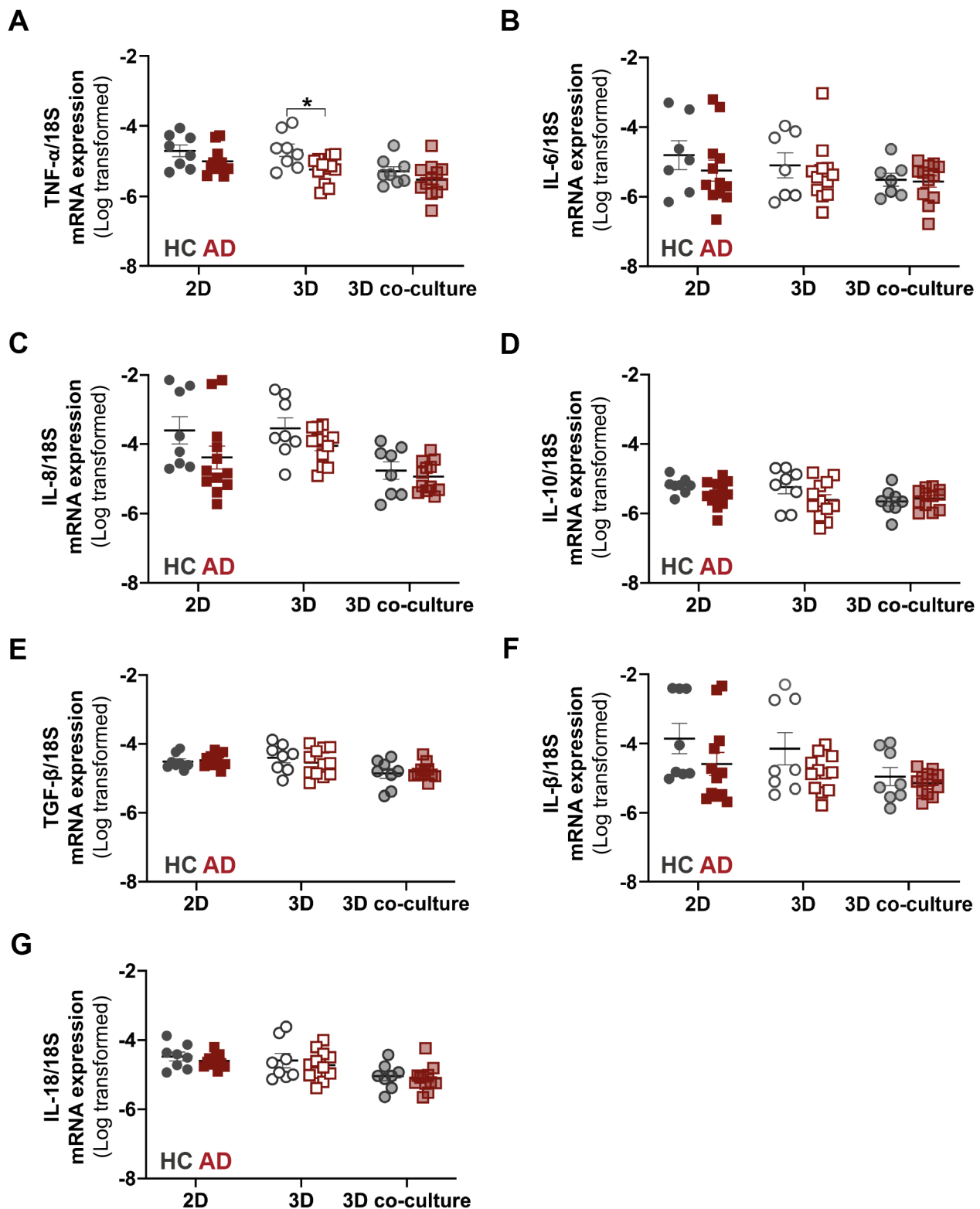
981 **Fig. S5. Depiction of morphological parameter measurements in HC and AD MDMi in 2D and**
 982 **3D mono-cultures.** (A) Binary and (B) skeleton images of HC and AD MDMi in 2D and 3D mono-
 983 cultures showing the morphological parameters (endpoints, branch length, triple and quadruple
 984 junctions) analysed to estimate the branched structure and complexity of MDMi.



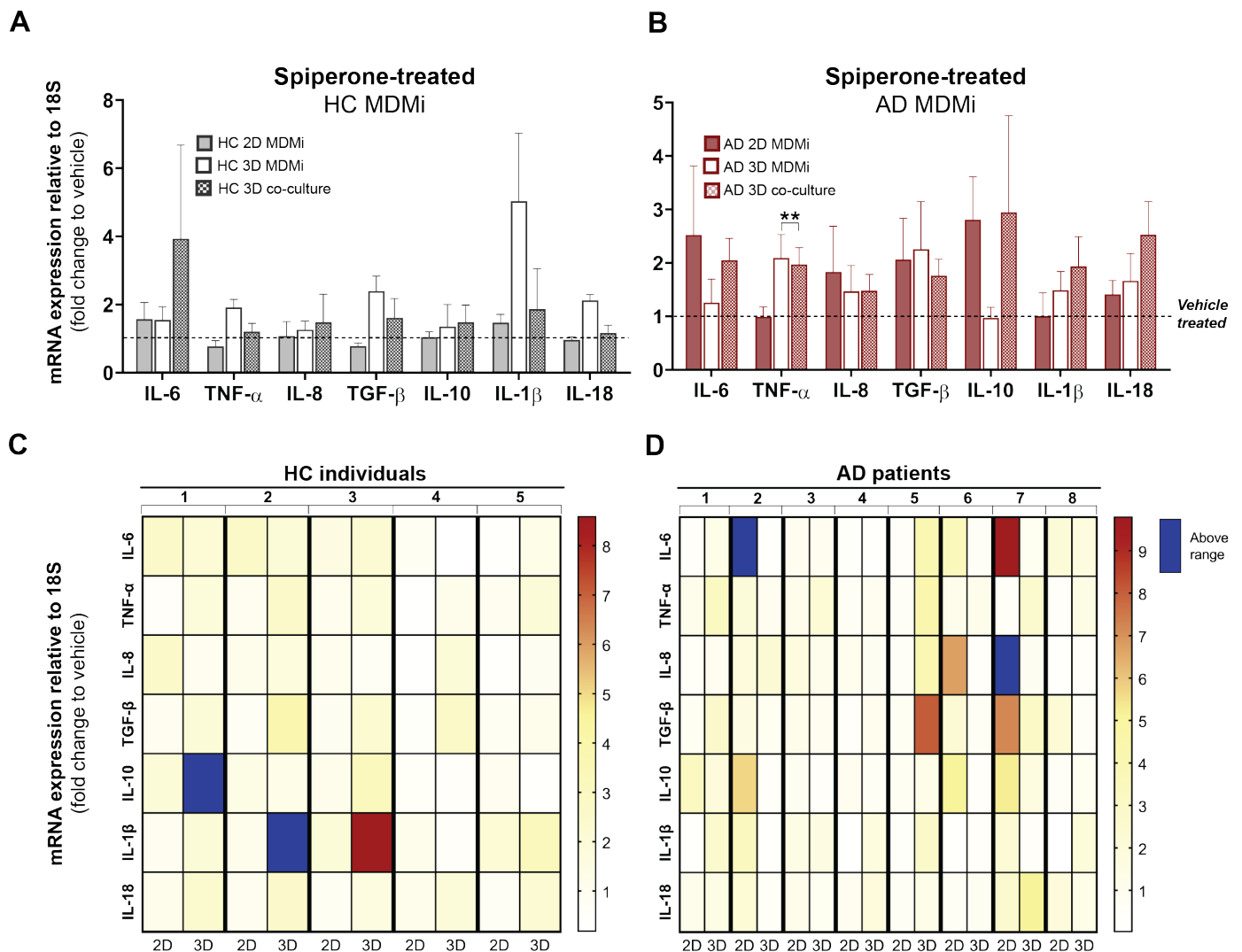
985 **Fig. S6. Gene expression of AD risk genes in HC and AD 3D MDMi.** qRT-PCR quantification of
 986 (A) *CLU*, (B) *TREM2* and (C) *PLCG2* mRNA expression in 3D MDMi mono-cultures from HC ($n =$
 987 7) and AD ($n = 11$) donors. Data are presented as mean \pm SD. Each single data point represents one
 988 biological replicate. Unpaired Student's t test with or without Welch's correction, two-tailed.



989 **Fig. S7. Inflammatory cytokine secretion by HC and AD 3D co-cultures under untreated and**
 990 **$A\beta$ -treated conditions.** Concentration of secreted IL-8, TNF- α , IFN- α 2, MCP-1, IFN- γ and IL-10 are
 991 displayed in HC ($n = 3$) and AD ($n = 4$) MDMi 3D co-cultures. Data are presented as mean \pm SEM.
 992 Unpaired Student's t test with or without Welch's correction, two-tailed.



993 **Fig. S8. Cytokine expression profiles in HC and AD MDMi 2D and 3D mono-cultures and 3D**
994 **co-cultures.** Log-transformed mRNA expression of the inflammatory cytokines (A) TNF- α , (B) IL-6,
995 (C) IL-8, (D) IL-10, (E) TGF- β , (F) IL-1 β and (G) IL-18 in HC ($n = 7-8$) and AD ($n = 12$) MDMi
996 cultures. Data are presented as mean \pm SD. Each single data point represents one biological replicate.
997 Comparisons between HC and AD MDMi in either culture format were performed using unpaired
998 Student's t test with or without Welch's correction, two-tailed; * $P < 0.05$.



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Fig. S9. Spiperone treatment induces cytokine expression responses that differ between culture format and are heterogeneous among HC and AD MDMi. Fold change in cytokine mRNA expression levels following 24 h exposure to 1 μ M spiperone compared to vehicle (DMSO)-treated cultures in **(A)** HC ($n = 5$) and **(B)** AD ($n = 8$) 2D and 3D MDMi mono-cultures and 3D co-cultures. Dotted black lines represent baseline responses of vehicle-treated cultures. Heat maps showing **(C)** HC ($n = 5$) and **(D)** AD ($n = 8$) donors-specific changes in mRNA expression from MDMi mono-cultures in 2D and 3D. Red-yellow colour spectrum represents relative fold change of mRNA expression after spiperone treatment compared to vehicle. Expression changes falling outside the displayed range are indicated in dark blue. Data are presented as mean \pm SEM. One-way ANOVA with Dunnett's multiple comparison test; $**P < 0.01$.