

Qubad et al. – Visual-field localizer & CBA

1 **Improved correspondence of fMRI visual field localizer data after**  
2 **macroanatomical alignment**

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4 Running Title: Visual field localizer & CBA

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50 **ABSTRACT**

51 The study of the visual system and its role for human cognition in health and disease  
52 with fMRI often requires the use of localizer paradigms to define anatomical regions  
53 of interest (ROIs). However, the considerable degree of interindividual variability of  
54 the cerebral cortex represents an important confound, especially when analyzing  
55 visual localizer data on the group level. Cortex-based alignment (CBA) techniques  
56 lead to a reliable reduction of interindividual anatomical variability. Yet, the potential  
57 benefits of CBA has not been investigated for visual field localizer paradigms used to  
58 map specific parts of the visual field within retinotopically organized early visual  
59 areas. We evaluated CBA for an attention-enhanced visual field localizer mapping a  
60 homologous part of each visual quadrant in a cohort of 50 participants. After CBA,  
61 group ROIs showed markedly increased spatial consistency. CBA also led to an  
62 increase in the probability of activation overlap of up to forty percent. Furthermore,  
63 the size of group ROIs for the lower visual hemifield was larger than for the upper  
64 visual hemifield after CBA. This asymmetry, which mirrors previous findings from  
65 electrophysiological and fMRI studies, was not detectable before CBA. Our results  
66 confirm and extend the utility of CBA for the study of the visual system particularly in  
67 the context of group analyses. This method should be particularly important for the  
68 study of neuropsychiatric disorders with abnormally increased interindividual  
69 anatomical variability.

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72 **KEYWORDS**

73 Human visual cortex, fMRI, visual-field localizer, cortex-based alignment

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## 77 **INTRODUCTION**

78 The visual system includes a multitude of topographical representations of varying resolution  
79 across increasingly specialized visual areas (Wandell, Dumoulin, & Brewer, 2007).

80 Functional magnetic resonance imaging (fMRI) offers a variety of methods either to map  
81 these topographical representations in full, or to localize specific visual areas or retinotopic  
82 positions within their topography. These approaches are essential not only for the fine-  
83 grained study of fundamental properties of the visual system (Wandell et al., 2007), but also  
84 for investigating the role of these areas for higher-order cognitive processes such as visual  
85 attention and working memory (Bergmann, Genç, Kohler, Singer, & Pearson, 2014; Corbetta  
86 & Shulman, 2002; Das, Bennett, & Dutton, 2007; de Haan, Bither, Brauer, & Karnath, 2015;  
87 Goodale & Milner, 2006; Ungerleider, 1982). This also extends to translational studies of  
88 visual dysfunction and its cognitive consequences in neuropsychiatric disorders (Lee et al.,  
89 2019; Silverstein et al., 2009).

90 Methods for fMRI-based visual mapping, i.e. techniques to define regions of interest (ROIs)  
91 in the visual system based on specific functional properties, fall in in three broad categories:  
92 retinotopic mapping, visual field localizer and functional localizer paradigms. Retinotopic  
93 mapping and the more advanced population receptive field mapping allow the complete  
94 delineation of early visual areas (Dumoulin & Wandell, 2008; Sereno et al., 1995; Wandell et  
95 al., 2007). Conversely, visual field localizer paradigms can map a circumscribed region within  
96 a retinotopically organized visual area (Harrison & Tong, 2009; Peters, Kaiser, Rahm, &  
97 Bledowski, 2015). Finally, functional localizers can detect higher-order visual areas such as  
98 the fusiform face area (Yenari, Xu, Tang, Qiao, & Giffard), parahippocampal place area  
99 (Sereno et al.), extrastriate body area (EBA), lateral occipital complex (LOC) etc., which are  
100 clustered and show specialization for the processing of specific categories of complex visual  
101 information (Downing, Chan, Peelen, Dodds, & Kanwisher, 2006; Kanwisher, McDermott, &  
102 Chun, 1997; Wandell et al., 2007). In most fMRI studies, high interindividual anatomical  
103 variability of cortical areas in terms of both size and location constitutes an important  
104 challenge (Brett, Johnsrude, & Owen, 2002; Desai, Liebenthal, Possing, Waldron, & Binder,

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105 2005; Dougherty et al., 2003; Fischl, Sereno, & Dale, 1999; Frost & Goebel, 2012, 2013;  
106 Steinmetz, Fürst, & Freund, 1990; Van Essen et al., 2001; Zilles et al., 1997). For instance, it  
107 has been shown, that primary visual cortex (V1) can differ in size by about 2-fold between  
108 individuals (Dougherty et al., 2003). Furthermore, anatomical variability in terms of location  
109 has been shown to be particularly pronounced in extrastriate visual areas (Bridge, 2011).  
110 This crucial confound reduces the power to reliably map visual areas at the group level.  
111 One way to mitigate this problem for the visual system is to pool single-subject ROIs, while  
112 simultaneously using the overall group-based probability for that ROI at each point in a  
113 Cartesian coordinate system as a constraint (Fedorenko, Hsieh, Nieto-Castañón, Whitfield-  
114 Gabrieli, & Kanwisher, 2010; Julian, Fedorenko, Webster, & Kanwisher, 2012; Nieto-  
115 Castañón & Fedorenko, 2012). While such a single-subject-based analysis improves  
116 sensitivity and functional resolution compared to a standard group-based approach, it does  
117 not actually reduce macroanatomical variability. Additionally, studying the interplay between  
118 visual areas and other cortical areas more directly involved in higher-order cognitive  
119 processes might preclude a single-subject based strategy. This applies in particular to  
120 functional connectomic approaches such as small-world networks, which compute  
121 interactions between brain regions at the whole-brain level (Tost, Bilek, & Meyer-Lindenberg,  
122 2012).

123 Cortex-based alignment (CBA) methods have been proposed as an alternative approach  
124 (Julian et al., 2012). CBA uses a geodesic coordinate system, which allows for a two-  
125 dimensional representation of the cerebral cortex, which respects the cortical topography to  
126 much larger degree than a traditional Cartesian coordinate system (Anticevic et al., 2008;  
127 Frost & Goebel, 2012; Julian et al., 2012). This representation allows the use of individual  
128 cortical folding patterns for a fully data-driven macroanatomical alignment. Compared to  
129 traditional nonlinear volume-based alignment (NVA) procedures (Evans et al., 1993;  
130 Talairach, 1988), CBA considerably improves anatomical correspondence of cortical  
131 structures (Anticevic et al., 2008; Fischl, Sereno, & Dale, 1999; Fischl, Sereno, Tootell, &  
132 Dale, 1999; Pantazis et al., 2010; Van Essen & Drury, 1997).

133 Several studies have compared the impact of NVA and CBA methods on specific visual  
134 mapping techniques. For retinotopic mapping an improvement of functional overlap in both  
135 V1 and V2 after CBA has been demonstrated (Fischl, Sereno, Tootell, et al., 1999; Hinds et  
136 al., 2008). Furthermore, for functional localizer data CBA substantially increases the overlap  
137 of object processing areas LOC, FFA and PPA across subjects (Frost & Goebel, 2012;  
138 Huang, Chen, Jiang, Zhen, & Liu, 2019; Rosenke, van Hoof, van den Hurk, Grill-Spector, &  
139 Goebel, 2020; Weiner et al., 2018). Conversely, the effects of CBA on visual field localizer  
140 paradigms mapping specific retinotopic positions have not been studied. Thus, the utility of  
141 CBA has been demonstrated for two of the three main categories of visual mapping  
142 methods, i.e. those methods, which map whole areas, either defined by cytoarchitectonic  
143 (e.g. V1) or functional (e.g. FFA) properties. Conversely, it remains unclear, to which degree  
144 CBA can improve the alignment of ROIs mapped by visual field localizer paradigms.  
145 Such paradigms are required for the detailed study of the local processing of simple visual  
146 stimuli in early visual areas (Di Russo, Martínez, & Hillyard, 2003; Di Russo, Martínez,  
147 Sereno, Pitzalis, & Hillyard, 2002; Harrison & Tong, 2009; Peters et al., 2015; Shigihara,  
148 Hoshi, & Zeki, 2016). Flashing chequerboards covering the exact area of interest within the  
149 visual field are primarily used for this purpose. Chequerboards lead to a particularly strong  
150 BOLD-signal increase in early visual areas (V1-V3) (Kraft et al., 2005). To maximize the  
151 fidelity of the resulting localizer maps, visual field localizer paradigms typically utilize the fact  
152 that attentional modulation induced by task demands significantly enhances response  
153 reliability across visual areas. This can be accomplished by adding a simple target detection  
154 task (Bressler & Silver, 2010).

155 We used such an attention-enhanced visual field localizer paradigm to map a circumscribed  
156 location in each visual quadrant across early visual areas in order to define ROIs to be used  
157 for the study of higher cognitive processes. We chose a CBA method using a dynamic group  
158 average as the target brain (Frost & Goebel, 2012). Thus, we eliminated the possible  
159 confound of a static CBA target based on an individual brain, whose cortical folding pattern  
160 might by chance deviate considerably from the group average.

161 Our primary goal was to examine the effects of CBA for a visual field localizer paradigm.  
162 More specifically, we aimed to determine, whether CBA can improve the reliability of  
163 mapping subregions within retinotopically organized visual areas delineated by such a  
164 paradigm at the group level. Based on previous findings for other localizer paradigm classes  
165 and the relatively good structural-functional correspondence in posterior occipital cortex, we  
166 expected to observe a benefit of CBA when aligning subregions within early visual cortex.  
167 Additionally, we compared the two main methods for the definition of single subject ROIs: the  
168 use of peak vertices, i.e. single vertices showing the strongest level of activation in a certain  
169 brain region, and the delineation of a larger ROI, which includes all vertices above a  
170 prespecified threshold, which is kept constant across brain regions (Tong et al., 2016). Our  
171 goal was to compare these two approaches and to assess changes in spatial  
172 correspondence after CBA at the single subject level. Mirroring our hypotheses for the group  
173 analyses, we expected to observe an improved correspondence of single-subject peak-  
174 vertex ROIs after CBA.  
175 Interestingly, several studies have shown differential response properties such as receptive  
176 field size for homologous early visual areas by visual quadrant or hemifield. For instance,  
177 improved behavioral performance and higher BOLD-signal amplitudes were observed in the  
178 lower visual hemifield (Anderson, Cameron, & Levine, 2014; Liu, Heeger, & Carrasco, 2006;  
179 O'Connell et al., 2016; Rubin, Nakayama, & Shapley, 1996). We were therefore also  
180 interested, whether we could observe differences between upper and lower visual hemifields  
181 in our group analysis after CBA. Overall, the aim of the study was to close an important gap  
182 in the evaluation of CBA for the study of the visual system. Since visual field localizers are  
183 crucial for investigating the contribution of the visual system to higher-order cognitive  
184 processes, our results should have implications for the study of visual cognition in both for  
185 basic and translational research.  
186  
187



## 188 **METHODS AND MATERIALS**

### 189 Participants:

190 All participants gave their written consent to participate in the study. The ethical review board  
191 of the Faculty of Medicine at Goethe University granted ethic approval. We recruited 51  
192 healthy volunteers (male: female = 23: 28) with age ranging between 18-43 years (mean =  
193 24). All participants were non-smokers, had no history of neurological or psychiatric illness  
194 and reported normal or corrected-to-normal visual acuity. One participant was left-handed as  
195 assessed by the German version of the Edinburgh Handedness Inventory (Oldfield, 1971).

196

### 197 Stimuli and task:

198 Subjects performed a visual field localizer paradigm (Figure 1) implemented using  
199 Presentation® (Neurobehavioral Systems, Version 18.0) as part of a larger study  
200 investigating the role of visual areas for higher cognitive functions. The task consisted of a  
201 series of flickering black-and-white-colored round shaped chequerboard stimuli (flicker  
202 frequency = 7.5 Hz). Chequerboard stimuli appeared for 2000 ms randomly at one of four  
203 different locations (non-target trial). Each location mapped a homologous position in one of  
204 the four visual quadrants. Our paradigm featured a simple target-detection task. During thirty-  
205 six trials, the two centrally located squares of the chequerboard changed their color to yellow  
206 for 133 ms (target trial). Participants were instructed to press a response box button with  
207 their left thumb as quickly as possible if they detected a target. The task consisted of a total  
208 of 144 trials (36 target trials, 108 standard trials). Thus, target probability was 25 %. The  
209 regular inter-stimulus interval was 0 ms. However, once every 10 to 14 trials the inter-  
210 stimulus interval increased to 2000 ms. Throughout the task a black, x-shaped fixation cross  
211 was displayed at the center of the screen. Participants were instructed to continuously fixate  
212 on the fixation cross. Before the first trial, only the fixation cross was displayed for 10  
213 seconds. After the last trial, only the fixation cross was displayed for 20 seconds. The total  
214 duration of the paradigm was 340 seconds. For the purpose of our analyses we defined a

215 total of four conditions, one for each of the four stimulus locations. Each participant practiced  
216 the task prior to the measurement.

217

218 Acquisition of fMRI data:

219 We acquired functional MRI data on a Siemens 3T MAGNETOM Trio scanner at the Goethe  
220 University Brain Imaging Centre using a gradient-echo EPI sequence (32 axial slices, TR =  
221 2000 ms, TE = 30 ms, FA = 90°, FoV = 192 x 192 mm<sup>2</sup>, voxel size = 3 x 3 x 3 mm<sup>3</sup>, gap = 1  
222 mm). Slices were positioned parallel to the anterior- and posterior commissure. Functional  
223 images were acquired in a single run comprising the acquisition of 170 volumes. Stimulus  
224 presentation was constantly synchronized with the fMRI sequence. Head motion was  
225 minimized with pillows. The task was projected by a beamer onto a mirror attached on the  
226 head coil. Anatomical MRI data for cortex reconstruction and co-registration with functional  
227 MRI data was acquired with a high-resolution T1-weighted 3D volume using a Magnetization-  
228 Prepared Rapid Gradient-Echo (MP-RAGE) sequence.

229

230 Functional image pre-processing:

231 MRI data were pre-processed and analyzed using Brain Voyager 20.6 (Goebel, Esposito, &  
232 Formisano, 2006), the NeuroElf toolbox ([www.neuroelf.net](http://www.neuroelf.net)) and custom software written in  
233 Matlab. Structural data pre-processing included brain extraction, inhomogeneity correction  
234 and transformation into Talairach coordinate space. Initial volume-based pre-processing of  
235 functional MRI data included slice scan time correction and motion correction.

236 At this stage, one subject had to be excluded due to excessive intra-scan motion.

237 After co-registration to the anatomical scans with a boundary-based registration algorithm  
238 (Greve & Fischl, 2009), the functional data were transformed into Talairach coordinate  
239 space.

240 Based on the segmentation of the structural scans along the white–grey matter boundary  
241 (Kriegeskorte & Goebel, 2001), cortical hemispheres were first reconstructed into folded,  
242 topologically correct mesh representations, which were tessellated to produce surface

243 reconstructions. These were subsequently morphed into spherical representations. We then  
244 applied a high-resolution, multiscale cortex-based alignment procedure, which reliably aligns  
245 corresponding gyri and sulci across subjects (Bittner et al., 2017; Goebel et al., 2006). This  
246 CBA approach consists of an initial rigid and a subsequent non-rigid alignment step (Frost &  
247 Goebel, 2012). During the initial step, we aligned the cortical folding pattern of each sphere  
248 rigidly to the cortical folding pattern of a target sphere by global rotation. We used the  
249 resulting rotation parameters with the highest overlap between the curvature of a subject's  
250 sphere and the target sphere as a starting point for the subsequent non-rigid CBA. In this  
251 step, we aligned each cortical folding pattern to a dynamically updated group average  
252 through iterative morphing following a coarse-to-fine matching strategy. During the initial rigid  
253 alignment step, we aimed to avoid the possible confounding effects of a suboptimal selection  
254 of an individual target brain, whose folding pattern might deviate considerably from the cohort  
255 average. To this end, we conducted a preliminary non-rigid CBA procedure, which included  
256 the brains of all 50 participants. The results of this preliminary non-rigid CBA procedure were  
257 only used to generate unbiased average brains to be used as targets for the initial rigid  
258 alignment step.

259 The volumetric functional data were then sampled on the cortical surface incorporating data  
260 from  $-1$  to  $+3$  mm along vertex normals. Based on the vertex-to-vertex referencing from the  
261 folded, topologically correct meshes to the aligned spherical representations, we mapped the  
262 functional data into a common spherical coordinate system. Finally, surface-based pre-  
263 processing of functional MRI data included spatial smoothing using a nearest neighbor  
264 interpolation (1 iteration, approximating a 2D Gaussian smoothing kernel with a FWHM of 1  
265 mm), temporal high-pass filtering (high-pass 0.00903 Hz) and linear trend removal. Spatial  
266 smoothing in surface space is clearly superior to spatial smoothing in volume space  
267 (Brodoehl, Gaser, Dahnke, Witte, & Klingner, 2020). However, we still opted for minimal  
268 spatial smoothing to minimize the loss of accuracy for our visual field localizer.

269

270

271 Cortex-based group fMRI analysis:

272 We performed multi-subject statistical analyses using multiple linear regression of the BOLD  
273 signal. The presentation of each chequerboard stimulus sequence at a single location, was  
274 modelled by an ideal box-car function, which covered the volume of each trial, convolved  
275 with a synthetic two-gamma function. These predictors were used to build the design matrix  
276 of the experiment. Individual statistical maps were generated by associating each voxel with  
277 the F-value corresponding to the specific set of predictors and calculated on the basis of the  
278 least mean squares solution of the general linear model. We created anatomical masks that  
279 only included cortical vertices in our analysis. These masks excluded those subcortical  
280 structures, i.e. parts of thalamus and the basal ganglia, which mapped onto the midline of our  
281 surface reconstructions.

282

283 Group analysis of visual quadrants before and after CBA:

284 We performed analyses focusing on the mapping of the four visual quadrants at the group  
285 level and compared these with results at single subject level. To define the group level ROI  
286 for each visual quadrant, we computed separate weighted contrasts for each quadrant  
287 against the other three quadrants. We assigned a weight of three to the position of interest,  
288 e.g.  $(\beta^{\text{Quad1}} \times 3) / (\beta^{\text{Quad2}} + \beta^{\text{Quad3}} + \beta^{\text{Quad4}})$  ( $p < 0.5$ , Bonferroni corrected). For each resulting  
289 group level ROI, we extracted average time courses (incl. standard errors of the mean =  
290 SEM) for all four conditions. We conducted this analysis both before and after CBA.

291

292 Probability maps before and after CBA:

293 To quantify and visualize variability of functional activation and possible changes due to  
294 macroanatomical alignment, the use of probability maps has been proposed. Probability  
295 maps are specifically useful to quantify inconsistency i.e. the disparity between individuals  
296 regarding the location of a particular (visual) area. To quantify the spatial consistency of  
297 activation patterns before and after CBA, we generated probability maps for each visual  
298 quadrant (Wang, Mruczek, Arcaro, & Kastner, 2015; Yamamoto et al., 2012). These maps

299 represent the relative number of subjects showing significant task activity in our single-  
300 subject analysis. Probability maps for early visual areas before and after CBA were created  
301 based on the previously generated single subject t-maps, with a threshold of a minimum of  
302 ten percent probability. To quantify the change in spatial consistency of activation patterns as  
303 a result of CBA, we created probability difference maps for each position (post-CBA minus  
304 pre-CBA). This allowed us to determine both increases and decreases of spatial consistency  
305 due to CBA.

306

307 Single-subject ROIs of visual quadrants before and after CBA including peak vertex

308 mapping:

309 For analyses at single-subject level, we first defined ROIs for each subject independently  
310 using the same weighted contrasts employed in the group analysis. We applied a more  
311 lenient statistical threshold ( $p < 0.05$  uncorrected). For each resulting single-subject ROI we  
312 extracted average time courses for all four conditions. We then averaged these time courses  
313 across all subjects. Thus, we generated group level average time courses reflecting each  
314 subject's region of maximum activation. We conducted this analysis both before and after  
315 CBA. Additionally, we determined the peak vertex for each subject's four visual quadrant  
316 ROIs, i.e. the vertex with the highest t-value. We then defined extended single-subject peak  
317 vertex ROIs, which also included the six vertices adjacent to the peak vertex (Tong et al.,  
318 2016). For each resulting single-subject peak vertex ROI we extracted average time courses  
319 (incl. SEM) for all four conditions. We then averaged these timecourses across all subjects.  
320 We conducted this analysis both before and after CBA.

321

322 Peak vertex distribution maps:

323 We mapped all peak vertices per visual quadrant before and after CBA and computed the  
324 vertex-wise number of peak vertices to estimate the degree of overlap between subjects.

325

326 **RESULTS**

327 Impact of CBA on spatial consistency of ROIs (group level)

328 Group-level mapping of the four visual quadrants revealed considerable differences before  
329 and after CBA. For the right lower visual quadrant, our analysis before CBA yielded a large  
330 cluster in the left upper occipital cortex, also encompassing posterior parts of temporal  
331 cortex, which decreased considerably in size after CBA and was much more circumscribed.  
332 Conversely, for the other three visual quadrants, our analysis before CBA yielded clusters in  
333 the corresponding parts of the occipital pole, which increased in size after CBA without a  
334 notable change of their center of gravity (Figure 2, Table 1). Overall, after CBA group ROIs  
335 showed markedly greater spatial consistency and vertical symmetry. Additionally, after CBA,  
336 ROIs for the lower visual hemifield were considerably larger in size than ROIs for the upper  
337 visual hemifield. Before and after CBA, average time courses showed clear position  
338 selectivity which increased after CBA (Figure 2).

339

340 Probability maps (group level)

341 Before CBA, probability maps showed a relatively wide spread of functional activation around  
342 the core region of interest defined in our previous group analysis (Figure 3). The maximum  
343 probability of overlap of around 50 % was consistently located at the center of each ROI.  
344 After CBA, probability maps showed a noticeable decrease in the spread of functional  
345 activation around the core region of interest with a corresponding increase in the maximum  
346 probability of overlap. Consequently, probability difference maps (Figure 4) showed an  
347 increase in the probability of overlap of up to 40 % around the core region of interest and a  
348 corresponding peripheral decrease in the probability of overlap of up to 40 %.

349

350 Comparison of full ROIs and extended peak-vertex ROIs (single-subject level)

351 The comparison of time courses averaged over all full single subject ROIs with time courses  
352 averaged over all single subject extended peak-vertex ROIs showed consistently larger  
353 BOLD signal amplitudes for extended peak-vertex ROIs (Figure 5). There was no difference

354 in BOLD signal amplitude before and after CBA for both types of ROI. Before and after CBA,  
355 all ROIs showed comparable clear position selectivity.

356 The rate of success for finding a ROI for each subject was as follows: upper right visual  
357 quadrant 46 out of 50 subjects, upper left visual quadrant 50 out of 50 subjects, lower left  
358 visual quadrant 48 out of 50 subjects, lower right visual quadrant 50 out of 50 subjects.

359

#### 360 Impact of CBA on spatial variability of peak vertex distribution (single-subject level)

361 As with the probability maps at the group level, peak vertex distribution maps at the single-  
362 subject level (Figure 6) showed less spatial variability after CBA with an increased probability  
363 of overlap. Both before and after CBA, the spread of peak vertices was larger for the lower  
364 visual quadrants.

365

## 366 **DISCUSSION**

367 The aim of our study was to evaluate the utility of CBA for a visual field localizer paradigm  
368 used to map a circumscribed region within retinotopically organized visual areas. Our  
369 paradigm mapped homologous regions in each visual quadrant reliably across early visual  
370 areas. As expected, CBA led to a marked reduction in macroanatomical variability. On the  
371 functional level, CBA had a number of beneficial effects.

372 CBA improved the results of the group ROI analysis for all visual quadrants (Figure 2). This  
373 was reflected in both the spatial consistency of the resulting group ROIs and in the signal-to-  
374 noise ratio exemplified by the difference between the BOLD signal amplitude for the  
375 stimulated location compared to the other locations. Probability difference maps showed an  
376 increase in the probability of overlap of up to forty percent in the central region of interest,  
377 which resulted in considerably more focused activation patterns. However, the opposite  
378 effect was observed in more peripheral vertices (Figure 4). The latter effect is most likely not  
379 attributable to a decrease of spatial overlap in the periphery of early visual areas. Rather it  
380 demonstrates that CBA consistently reduces spurious spread-out activation resulting from



381 poor macroanatomical correspondence after NVA. This observation suggests that NVA-  
382 based group analyses generally overestimate the extent of visual areas.

383 Together these findings indicate that CBA substantially increases statistical power when  
384 studying early visual areas at the group level. Naturally, this effect of CBA also extends to  
385 studies with a more global focus, such as connectivity analyses (Brodoehl et al., 2020;  
386 Bullmore & Sporns, 2009).

387 Regarding the comparison between full single-subject ROIs and extended peak-vertex  
388 single-subject ROIs, we made the following observations. As expected, BOLD signal  
389 amplitudes for single subject ROIs were not affected by CBA (Figure 5). Conversely, the  
390 variability of these ROIs as signified by the peak vertex location decreased after CBA (Figure  
391 6). This underscores that the reduction of functional inter-subject variability due to CBA is the  
392 main reason for our improved results at the group level. Furthermore, BOLD signal  
393 amplitudes for the full single-subject ROIs were consistently lower compared to our extended  
394 single-subject peak vertex ROIs (Figure 5). This is well in line with previous findings of larger  
395 effect sizes in volume space for strategies using peak-voxels with or without including directly  
396 neighboring voxels to define ROIs (Tong et al., 2016).

397 Before CBA we observed the strongest group effects, i.e. the largest group ROIs, for the left  
398 lower and right upper visual quadrant, an effect that clearly did not persist after CBA (Figure  
399 2). Notably, several studies using volume-based fMRI and magnetoencephalographic (Hahn  
400 et al.) analyses reported lateralized effects on neurophysiological parameters in early visual  
401 areas (H. Chen, Yao, & Liu, 2004; Loughnane, Shanley, Lalor, & O'Connell, 2015). Our  
402 observation raises the question, whether these findings could at least partly be explained by  
403 lateralized differences in macro-anatomical variability rather than true functional differences.

404 Conversely, our CBA-aided group analysis allowed us to compare the response properties of  
405 each visual quadrant in a more unbiased way. We observed larger group ROIs for the lower  
406 visual hemifield. In a CBA-based probabilistic atlas of the visual system, which included all  
407 regions that could be defined in more than 50% of subjects, probabilistic ROIs for dorsal V1  
408 and V2 were also noticeably larger than probability maps for ventral V1 and V2, whereas this



409 effect was less clear for V3 (Rosenke et al., 2020). These results are in line with our own  
410 findings and could be attributable to higher residual anatomical variability after CBA in ventral  
411 occipital cortex representing the upper visual hemifield. Alternatively, they could be due to  
412 true differences in response properties such as receptive field size or overall area size. The  
413 latter interpretation is supported by studies showing functional differences between upper  
414 and lower visual hemifields already at the retinal level in the form of differences in receptor  
415 densities. Cone density was higher in the superior parts of the retina which processes  
416 information from lower visual fields. Conversely, higher rod density was observed in the  
417 inferior parts (Curcio & Allen, 1990; Eickhoff, Rottschy, Kujovic, Palomero-Gallagher, &  
418 Zilles, 2008). Moreover, Eickhoff et al. observed dorso-ventral asymmetries in receptor  
419 densities in V2 and V3 (Eickhoff et al., 2008). They found a higher density of GABA-A,  
420 benzodiazepine- as well as muscarinic M3-receptors in ventral parts of V2 and V3.  
421 Furthermore, there is evidence for fundamental differences in receptive field shape from a  
422 pRF mapping study. Estimating both the aspect ratios and the size of the mapped areas, a  
423 more elliptical receptive field shape was observed for the upper visual hemifield represented  
424 by ventral parts of the visual cortex being compared to the lower visual hemifield represented  
425 by dorsal parts of the visual cortex (Silson, Reynolds, Kravitz, & Baker, 2018).  
426 Additionally, there is evidence for a behavioral advantage in the lower visual hemifield for  
427 shape discrimination as well as higher BOLD-signal changes and peak amplitudes of  
428 MEG/EEG responses (Anderson et al., 2014; Hagler, 2014; O'Connell et al., 2016; Rubin et  
429 al., 1996; Schmidtman, Logan, Kennedy, Gordon, & Loffler, 2015). Together, these findings  
430 demonstrate clear differences in the functional architecture of early visual areas representing  
431 the upper and lower visual hemifield. This has been attributed to the fact that the lower visual  
432 hemifield represented by dorsal parts of the occipital lobe is more closely linked to the dorsal  
433 visual pathway, while the upper visual hemifield represented by ventral parts of the occipital  
434 lobe is more closely linked to the ventral visual pathway (Thomas & Elias, 2011; Zito,  
435 Cazzoli, Müri, Mosimann, & Nef, 2016). Furthermore, there is evidence for fundamental  
436 differences in receptive field shape from a pRF mapping study. For the upper visual hemifield

437 represented by ventral parts of the visual cortex an increased size and more elliptical shape  
438 of receptive fields was observed compared to the lower visual hemifield represented by  
439 dorsal parts of the visual cortex (Silson, Reynolds, Kravitz, & Baker, 2018). This implies, that  
440 the lower visual field is more specialized for the precise localization and representation of  
441 space. Our observation of larger ROIs in the lower visual hemifield is in line with these  
442 findings. Thus, our results imply that CBA is a useful tool to extend the study of functional  
443 and behavioral asymmetries in early visual areas to the group level.

444 One important limitation of the current study is the lack of a complementary retinotopic  
445 mapping data set due to time constraints. This data would have allowed us to delineate the  
446 boundaries of early visual areas and pinpoint the exact visual area containing each individual  
447 single-subject ROI. Retinotopic mapping studies indicate that peak activation of single  
448 subjects assessed by visual localizers are not consistently located in the same visual area.  
449 Most localizer tasks show peak activation not in V1 but rather in V2 or V3 (Peters et al.,  
450 2015). It is therefore very likely that our single-subject peak activation did not consistently  
451 belong to the same visual cortical area. With the current data set we cannot determine how  
452 precisely individual visual areas were aligned with CBA, and whether individual levels of the  
453 visual cortical hierarchy were differentially affected.

454 However, the position of our group regions of interest, which bordered the calcarine sulcus  
455 and spanned the occipital pole, indicate that they mainly comprised V2 and V3. Similarly,  
456 after CBA a comparable increase in the probability of overlap was observed in the same part  
457 of occipital cortex. While this is at least suggestive of a relatively consistent benefit of CBA  
458 across visual areas, more fine-grained studies including retinotopic mapping are required to  
459 definitively address this question.

460 Furthermore, we did not use eye tracking to insure sufficient fixation. We also did not include  
461 an additional central attentional control task on the fixation cross, which would have further  
462 encouraged continuous fixation. This was done deliberately in order to keep the difficulty  
463 level adequate for psychiatric patient populations, but it might explain our failure to find  
464 reliable activation in early visual areas in a fraction of our subjects.

465 Our study also has implications beyond mapping the visual system in healthy populations.  
466 First, cortical processing in visual areas can to some degree be characterized more  
467 adequately by its task-specificity, rather than sensory-specificity (Amedi et al., 2007; Bedny,  
468 Pascual-Leone, Dodell-Feder, Fedorenko, & Saxe, 2011; Ptito, Matteau, Gjedde, & Kupers,  
469 2009; Reich, Szwed, Cohen, & Amedi, 2011; Renier et al., 2005; Striem-Amit, Cohen,  
470 Dehaene, & Amedi, 2012). For instance, in blind people primary visual cortex can be adapted  
471 to map spatial locations of sound. It would be interesting to see, whether studying the  
472 retinotopic representation of spatial sound at the group level might also benefit from CBA  
473 (Norman & Thaler, 2019). Second, visual processing deficits are a prominent feature of  
474 neurodevelopmental psychiatric disorders such as ADHD, schizophrenia and autism  
475 spectrum disorders (Bakroon & Lakshminarayanan, 2016; Butler et al., 2001; Butler,  
476 Silverstein, & Dakin, 2008; C. Y. Chen et al., 2002; Hale et al., 2014; Lee et al., 2019; Sanz-  
477 Cervera, Pastor-Cerezuela, González-Sala, Tárraga-Mínguez, & Fernández-Andrés, 2017;  
478 Seymour, Rippon, Gooding-Williams, Schoffelen, & Kessler, 2019; Shimizu, Bueno, &  
479 Miranda, 2014; Silverstein et al., 2009). These deficits can also perturb crucial higher order  
480 cognitive processes including working memory, which underscores the relevance of visual  
481 dysfunction for pro-cognitive interventions (Bittner et al., 2015; Butler, Thompson, Seitz,  
482 Deveau, & Silverstein, 2017; Haenschel et al., 2007). Furthermore, perceptual processes are  
483 an explicit part of the Research Domain Criteria project, which aims to identify constructs of  
484 transdiagnostic relevance in order to establish a psychiatric nosology based on cognitive  
485 dimensions and the underlying brain networks (Cuthbert, 2014; Insel, 2014). Thus, the  
486 current localizer paradigm will be useful to investigate local impairments of visual information  
487 processing as well as disturbances in the interplay between early visual areas and brain  
488 networks supporting higher-order cognitive processes. In this context, an efficient mapping of  
489 the visual system capturing other aspects of the functional organization of the visual system  
490 such as retinotopy will be essential. This approach would benefit from a comprehensive  
491 visual mapping battery combining different localizer techniques. Here, CBA will be  
492 particularly relevant to reduce the confounding effects of increased macroanatomical

493 variability in disorders such as schizophrenia in order to detect true group differences and  
494 true functional variability (Anticevic et al., 2008; Manoach, 2003). On the other hand, CBA  
495 should also be crucial for investigating the neurodevelopmental underpinnings of increased  
496 macroanatomical variability itself. To this end the inclusion of probabilistic atlases containing  
497 information about gene expression profiles (French & Paus, 2015) as well as cyto- and  
498 receptor archectonics (Gulban et al., 2020; Hawrylycz et al., 2012) will be valuable.  
499 Our CBA approach relied solely on cortical curvature information to reduce macroanatomical  
500 variability. The advantage of this method is its feasibility for the vast majority of fMRI data  
501 sets, since it only requires a structural brain scan of sufficient quality. Among comparable  
502 methods it is the most data driven and objective approach. However, the achievable degree  
503 of reduction of macroanatomical variability is limited by the variable and imperfect correlation  
504 between brain structure and brain function (Fischl, Sereno, Tootell, et al., 1999; Van Essen &  
505 Drury, 1997). Therefore, more advanced methods additionally utilize orthogonal functional  
506 data to further reduce anatomical variability. This includes the use of activation patterns or  
507 functional connectivity patterns to improve macroanatomical alignment across the whole  
508 brain (Conroy, Singer, Guntupalli, Ramadge, & Haxby, 2013; Frost & Goebel, 2013; Sabuncu  
509 et al., 2009). Furthermore, a more complex approach has been proposed, which aligns  
510 cortical data using ‘areal features’ more closely tied to cortical areas than cortical folding  
511 patterns, including maps of relative myelin content and functional resting state networks  
512 (Glasser et al., 2016). These methods have shown to provide a relevant additional reduction  
513 of macroanatomical variability for a variety of paradigms including visual functional localizers.  
514 Future studies should also evaluate these methods for retinotopic mapping and visual field  
515 localizers. Moreover, it has been demonstrated for early auditory areas, that the additional  
516 use of a probabilistic atlas of cytoarchitectonically defined areas further improves standard  
517 CBA results (Tomasello, Wennekers, Garagnani, & Pulvermüller, 2019). Such an approach  
518 would easily be feasible for the visual system.  
519 To summarize, we demonstrated the clear superiority of CBA compared to NVA for the  
520 analysis of visual field localizer data on the group level indicated by a forty percent increase

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521 of overlap of ROIs. Our findings extend previous studies examining other major categories of  
522 visual mapping techniques. They underscore the comparable loss of information and  
523 statistical power incurred by the use of NVA methods in the majority of fMRI studies.  
524 Therefore, CBA and other comparable methods should be seriously considered as a  
525 standard procedure for the detailed study of visual information processing and its disturbance  
526 in mental disorders.  
527

528 **Figure Legends**

529 **Figure 1 – Visual field Localizer Paradigm**

530 The task consisted of flickering, black-and-white colored checkerboards that appeared  
531 randomly at homologous positions of the participant's visual quadrant. Only in 25 % of the  
532 trials the two centrally located squares changed their color into yellow for 133 ms.  
533 Participants were required to press a response box button when noticing that. During the  
534 whole task participants were instructed to fixate a black, x-shaped fixation cross presented in  
535 the center of the screen. Checkerboards appeared for 2000 ms. The regular inter-stimulus  
536 interval (Shaffer et al.) was 0 ms. Every 10 to 14 trial the ITI extended to 2000 ms.

537

538 **Figure 2 – Group analysis of visual quadrants**

539 Surface-based group results (a) before and (b) after CBA and averaged time courses. After  
540 CBA, group ROIs showed greater spatial consistency and ROIs for the lower visual hemifield  
541 were larger in size than ROIs for the upper visual hemifield. Average timecourses (incl. SEM)  
542 showed clear position selectivity which was higher after CBA.

543 ROI/graph colors: red = upper left (UL) visual quadrant, orange = lower left (LL) visual  
544 quadrant, light-blue = lower right (LR) visual quadrant, dark-blue = upper right (UR) visual  
545 quadrant.

546

547 **Figure 3 – Probability Maps**

548 Probability Maps (a) before and (b) after CBA for each visual quadrant. The color code grey-  
549 to-white indicates an increase in the probability of overlap. Probability maps (a) before CBA  
550 showed a maximum probability of overlap of up to 50 %. Probability maps (b) after CBA  
551 showed a maximum probability of overlap of up to 90 %.

552

553

554 **Figure 4 – Probability Difference Maps**

555 Probability difference maps (post-CBA minus pre-CBA). The color code dark-red-to-white  
556 indicates an increase of activation overlap. The color code blue-to-green indicate a decrease  
557 of activation overlap. Overall, at the center of each ROI the probability of overlap increased  
558 by up to forty percent after CBA.

559

560 **Figure 5 – Average timecourses of visual quadrants**

561 Average timecourses (incl. SEM) of visual quadrants for full single-subject and single-subject  
562 extended peak vertex ROIs before and after CBA. Extended peak-vertex ROIs showed  
563 consistently larger BOLD-signal amplitudes. Average timecourses showed clear position  
564 selectivity which was unaffected by CBA.

565 ROI/graph colors: red = upper left (UL) visual quadrant, orange = lower left (LL) visual  
566 quadrant, light-blue = lower right (LR) visual quadrant, dark-blue = upper right (UR) visual  
567 quadrant. Dashed lines = single subject extended peak-vertex ROIs, solid lines = full single-  
568 subject ROIs.

569

570 **Figure 6 – Peak vertex distribution maps**

571 For each visual quadrant single-subject peak vertices were mapped (a) before and (b) after  
572 CBA and a vertex-wise number of peak vertices were computed to estimate the degree of  
573 overlap. The color code turquoise-to-red indicates an increase in the degree of overlap. After  
574 CBA, we observed reduced spatial variability of peak vertex location.

575

576 **Table 1 – Talairach coordinates**

577 Table 1 depicts the Talairach coordinates of the group ROIs of the corresponding visual  
578 quadrants before and after CBA.

579

580

581

582 **Author contributions**

583 All authors made substantial contributions to the conception or design of the work, or the  
584 acquisition, analysis, or interpretation of data. AR and RAB acquired funding. RAB, BP, MS  
585 and LR designed the experiment. MQ, CVB-S, LR and RAB acquired the data. ER and RG  
586 provided analytical tools. MQ and RAB analysed the data. MQ and RAB undertook the  
587 literature searches and wrote the first draft of the manuscript. All authors contributed to and  
588 revised the manuscript. All authors read and approved the final manuscript.

589

590 **DISCLOSURES**

591 The authors have declared that there are no conflicts of interest in relation to the subject of  
592 this study.

593

594 **DATA AVAILABILITY STATEMENT**

595 The data that support the findings of this study are available from the corresponding author  
596 upon reasonable request.

597



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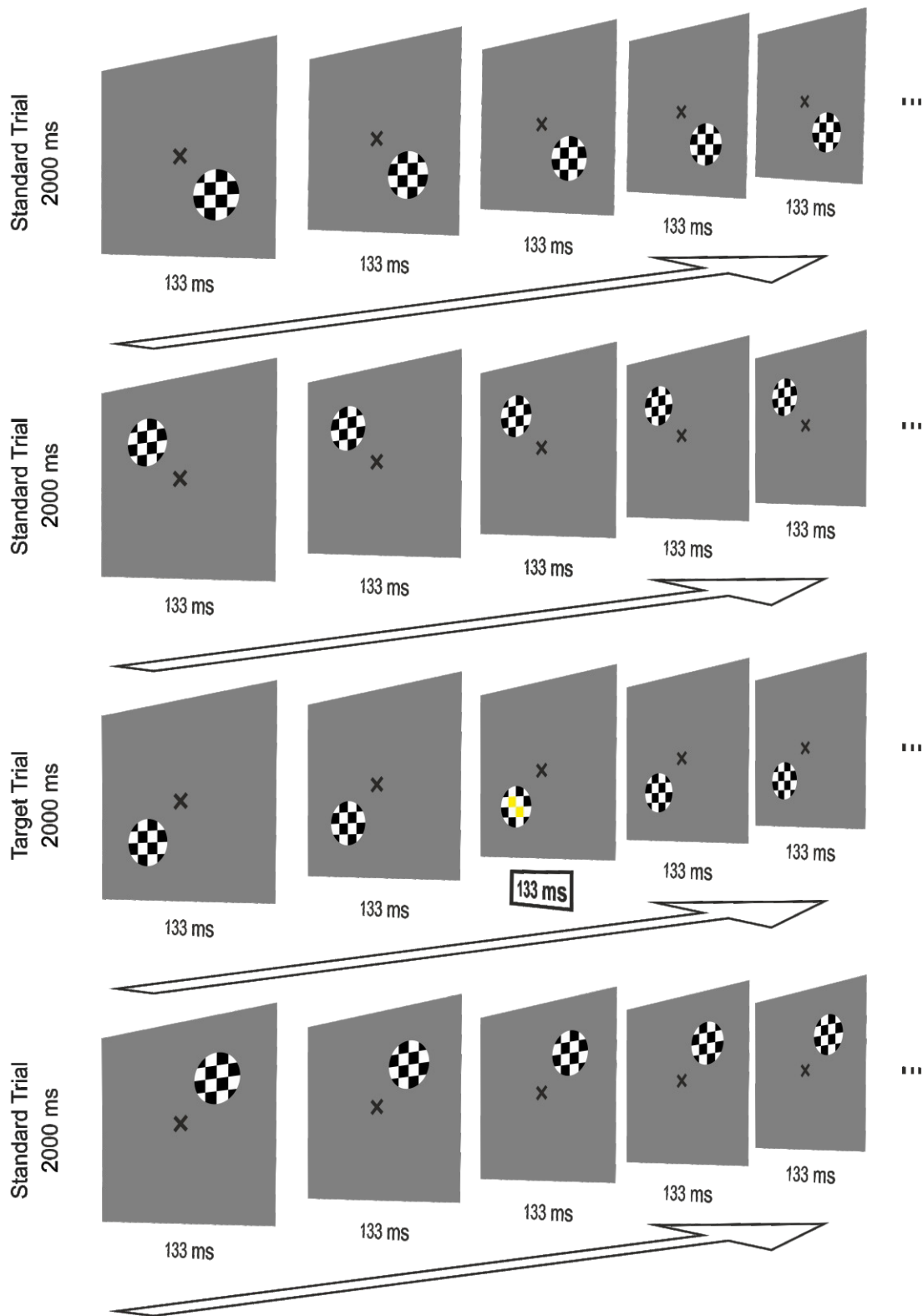
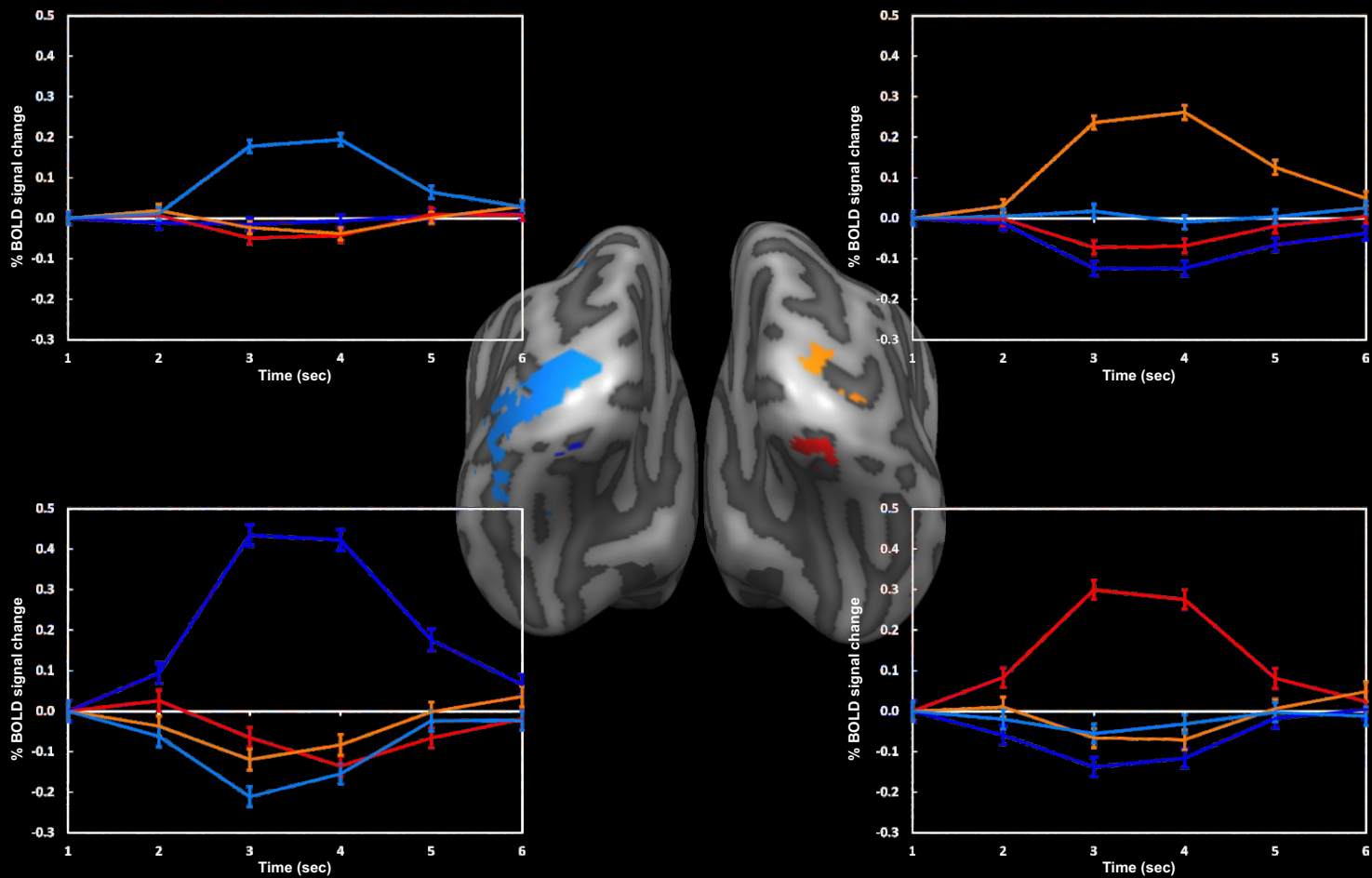
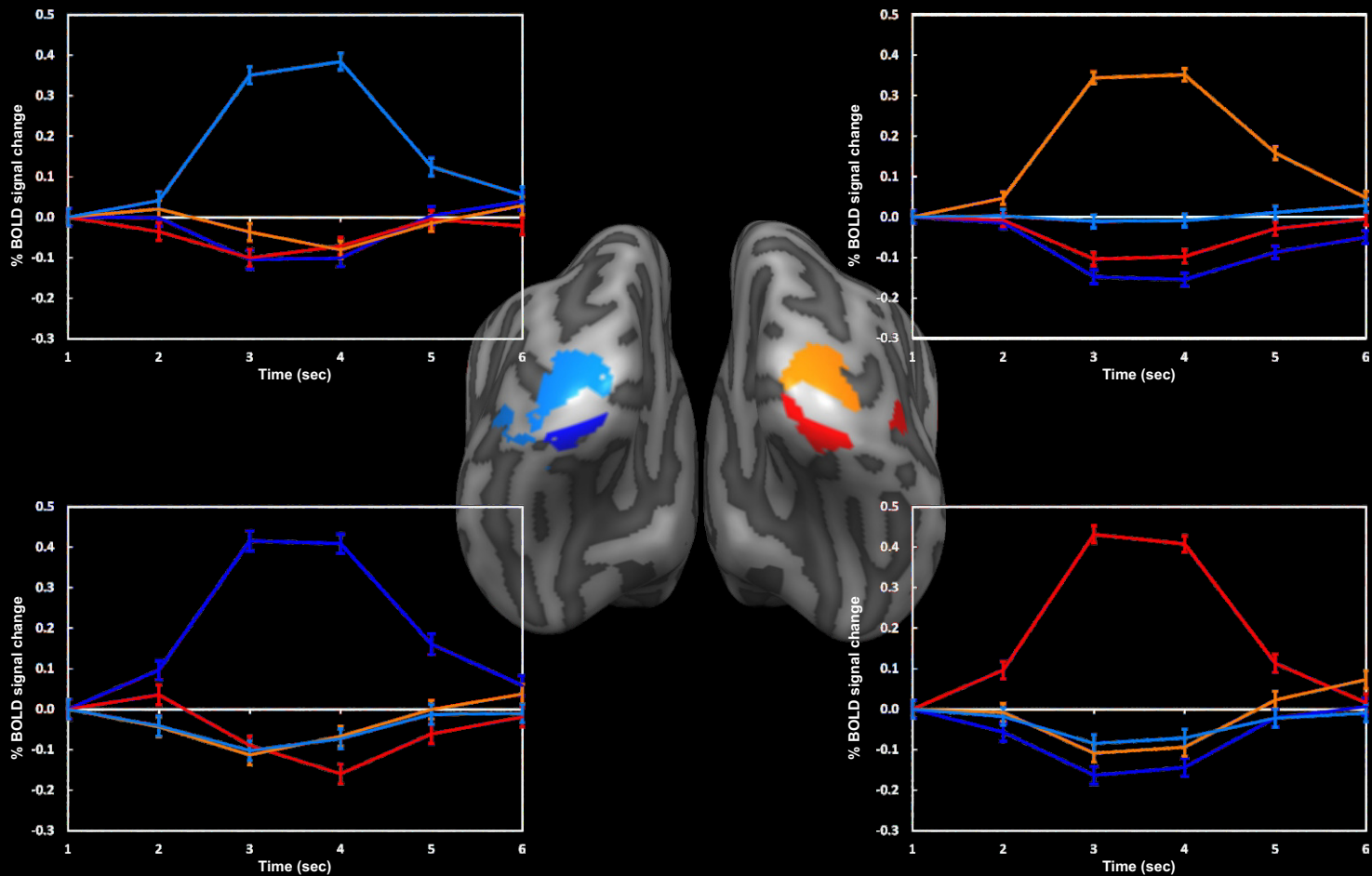


Figure 1

(a) pre-CBA



(b) post-CBA

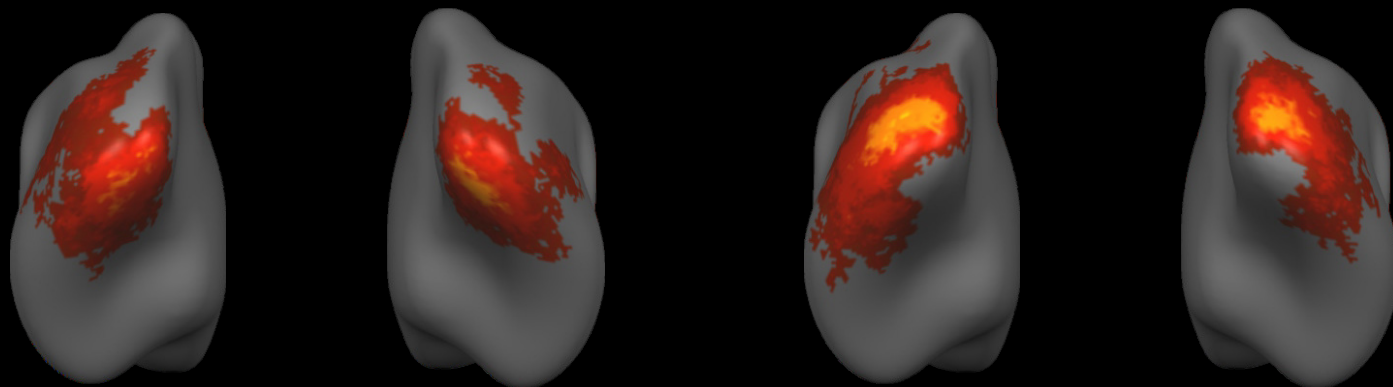


UR Quadrant    UL Quadrant    LL Quadrant    LR Quadrant

Figure 2



**(a) pre-CBA**



UR Quadrant

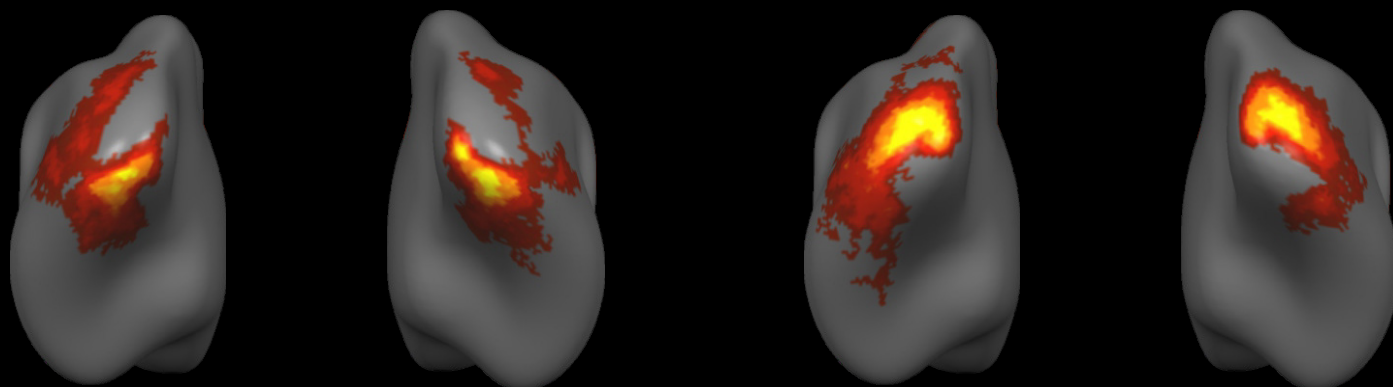
UL Quadrant

LR Quadrant

LL Quadrant



**(b) post-CBA**



UR Quadrant

UL Quadrant

LR Quadrant

LL Quadrant

Figure 3

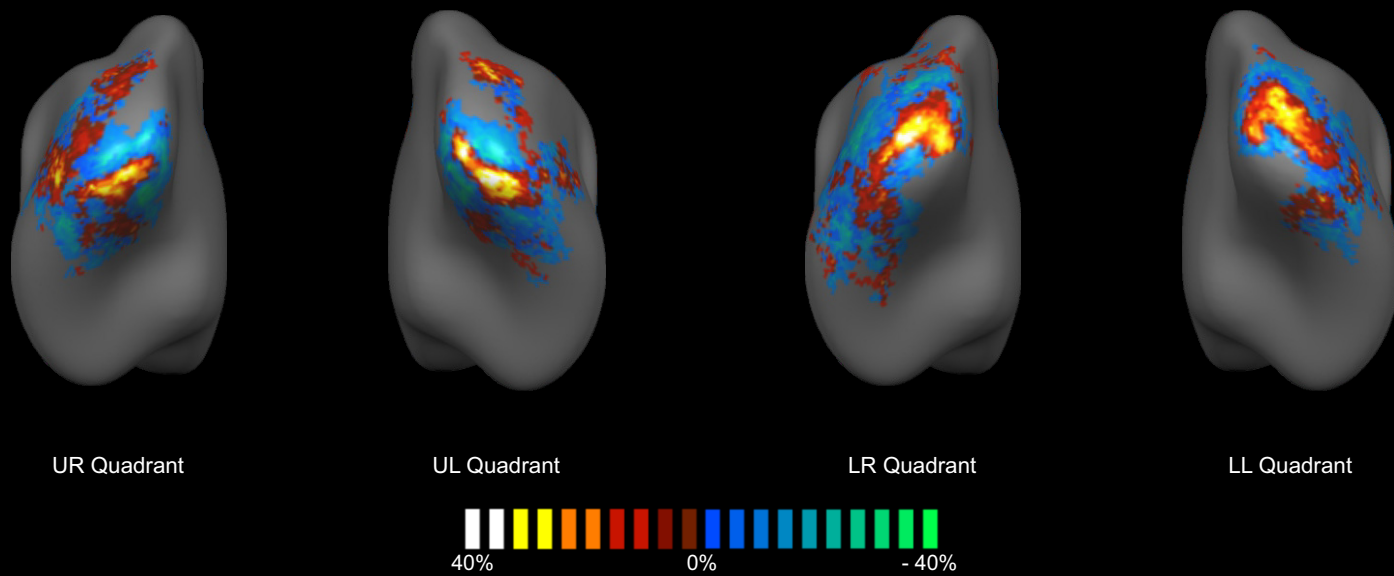


Figure 4

(a) pre-CBA

(b) post-CBA

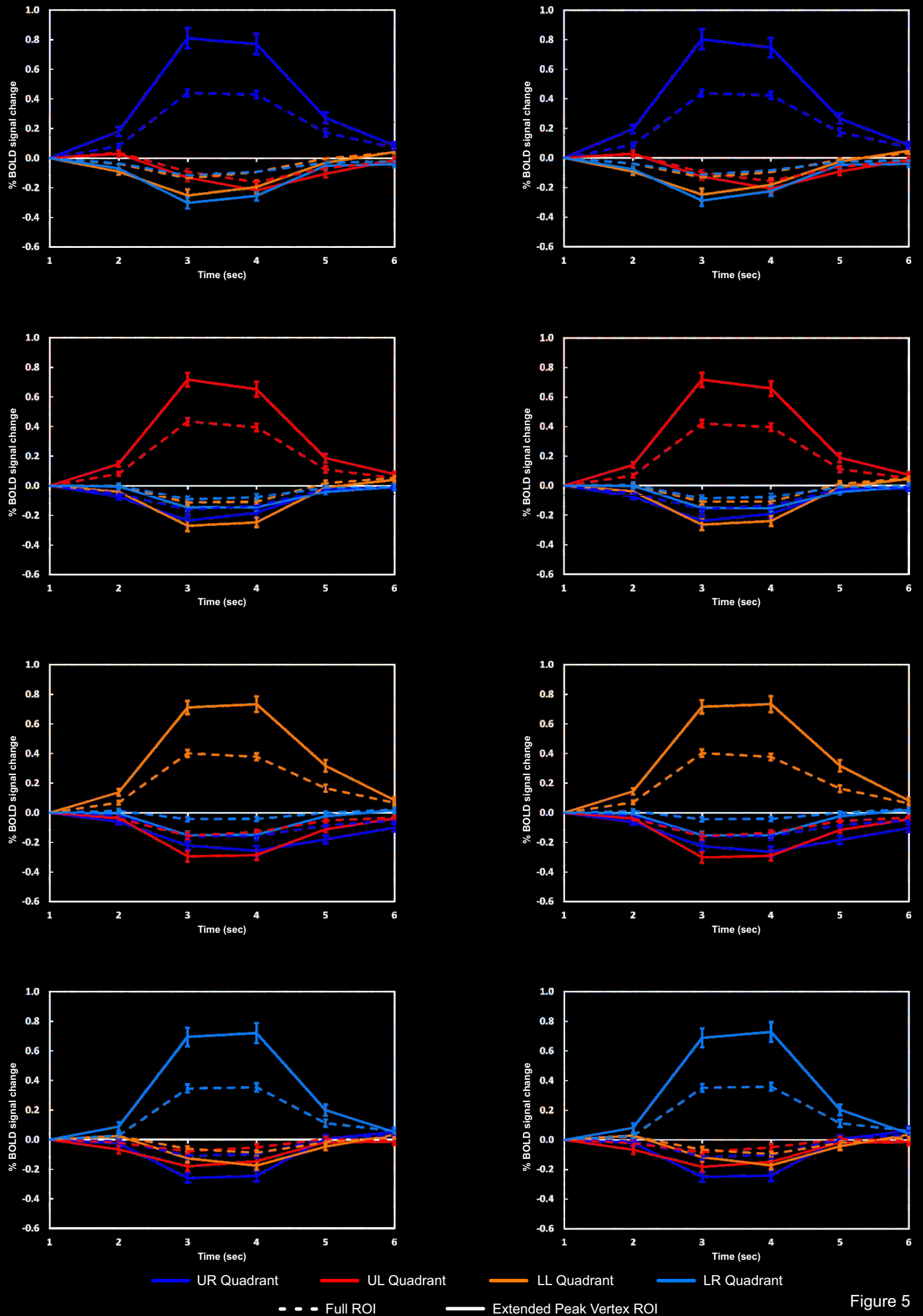
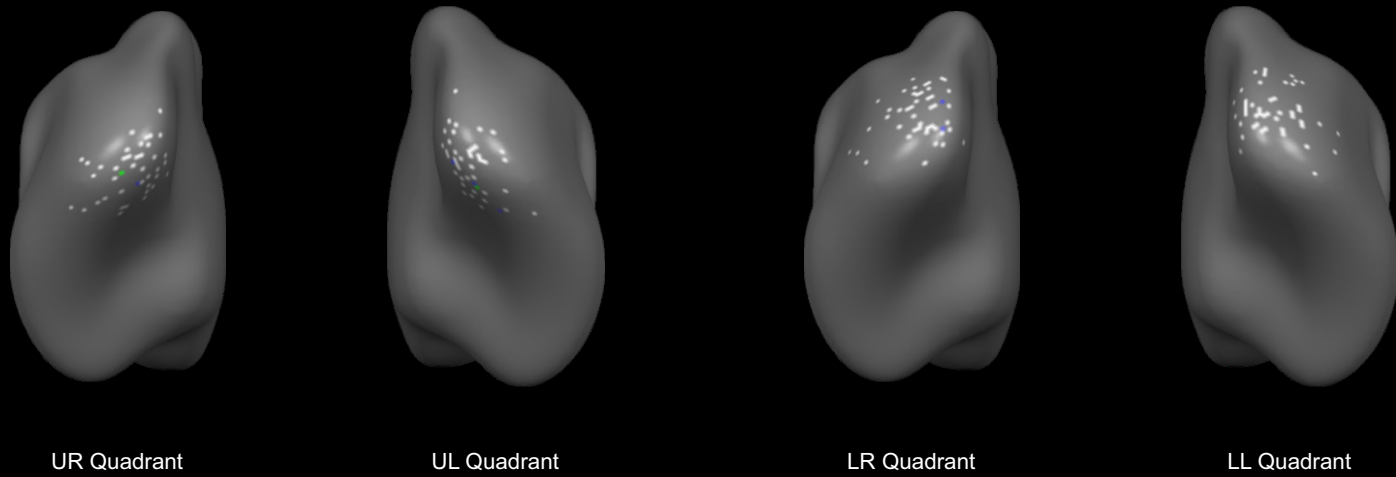


Figure 5

(a) pre-CBA



(b) post-CBA

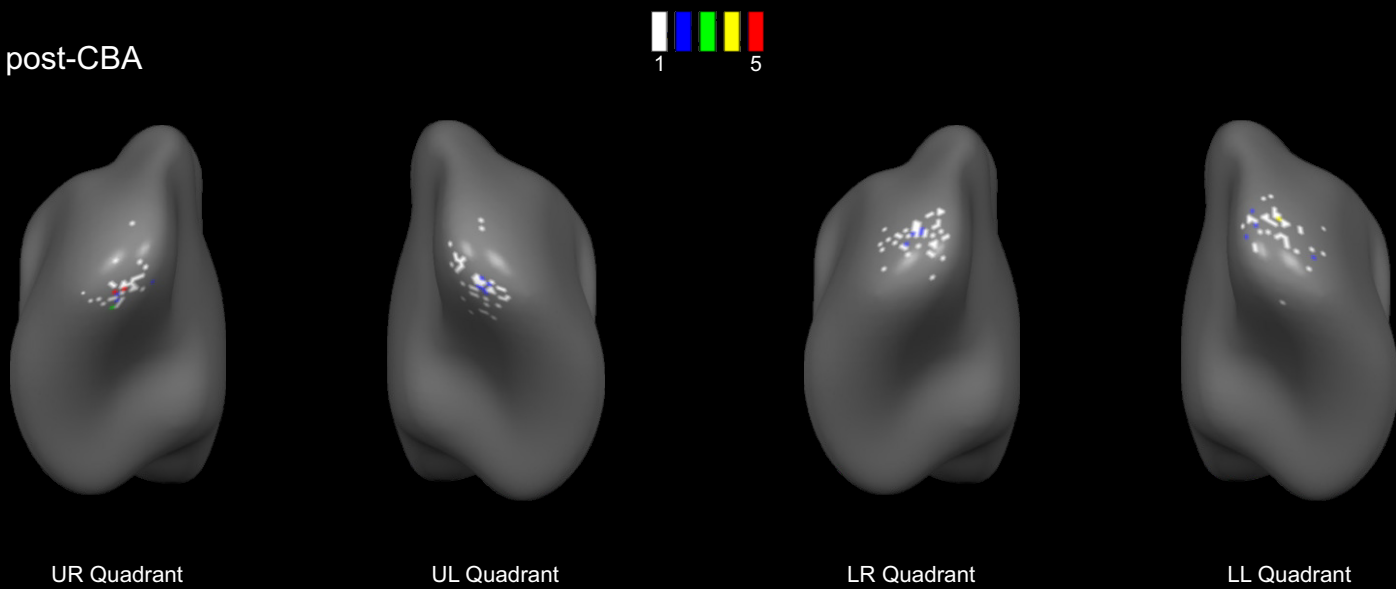


Figure 6

**Table 1**

Region of interest		Number of vertices	Talairach coordinates (in mm)		
			x	y	z
upper right visual quadrant	pre CBA	6	-18	-80	-15
	post CBA	58	-18	-80	-15
upper left visual quadrant	pre CBA	47	24	-75	-14
	post CBA	82	18	-77	-15
lower left visual quadrant	pre CBA	295	-42	-64	5
	post CBA	161	-24	-91	-4
lower right visual quadrant	pre CBA	28	23	-90	3
	post CBA	127	9	-94	-5