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Functional Connectome Fingerprinting Using Shallow Feedforward Neural Networks

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Although individual subjects can be identified with high accuracy 2 using correlation matrices computed from resting-state functional magnetic resonance imaging (rsfMRI) data, the performance signifi-3 cantly degrades as the scan duration is decreased. Recurrent neural 4 networks can achieve high accuracy with short duration (72s) data 5 segments but are designed to use temporal features not present in 6 the correlation matrices. Here we show that shallow feedforward neural networks that rely solely on the information in rsfMRI corre-8 lation matrices can achieve state-of-the-art identification accuracies 9 ($\geq 99.5\%$) with data segments as short as 20s and across a range of 10 input data-size combinations when the total number of data points (# 11

regions \times # time points) is on the order of 10,000.

fMRI | Connectome | Neural Network | Fingerprinting

Functional connectome fingerprinting based on the similar-1 ity of correlation coefficient matrices computed from rsfMRI 2 data can identify individuals with high accuracy (> 98%) 3 using long duration (> 12 minute) scans but considerably 4 lower accuracy ($\approx 68\%$) is obtained when the data duration is 5 decreased to 72s (1). Recurrent neural networks (RNN) can 6 achieve high accuracy (98.5%) with short duration (72s) data, 7 presumably reflecting their ability to capture both spatial 8 and temporal features (2, 3). However, it has been shown q that high RNN performance can be achieved even when the 10 temporal order of the fMRI data is permuted (4), suggesting 11 12 that the temporal features are not critical for identification. Here we introduce two shallow feedforward neural networks 13 that can achieve high identification accuracy without the need 14 for recurrent connections. Furthermore, we use these networks 15 to estimate the minimum size of the data needed to robustly 16 identify subjects with high mean accuracy ($\geq 99.5\%$) from 17 short segments of rsfMRI data. 18

19 The two networks considered are shown in Figure 1A and 20 1B. The input to the correlation neural network (corrNN) consists of the upper triangular elements of the correlation 21 coefficient matrix C estimated from a data matrix X consisting 22 of z-normalized time series (of length N) from M regions of 23 interest (ROI). For identification of L subjects, the network 24 structure consists of a fully connected classification layer with 25 L units, a batch normalization layer, and a softmax layer. The 26 27 norm-based neural network (normNN) uses the z-normalized data X as the input. The first stage is a fully connected 28 layer that projects the data onto K hidden units using the 29 $M \times K$ weight matrix W to form the $N \times K$ intermediate 30 matrix Y = XW. In the second stage, the L_2 norm across the 31 time-dimension (i.e. across each column of Y) is computed 32 for each hidden unit to form a summary measure of similarity 33 over the collection of N time points. The resulting vector 34 $F = \sqrt{diag(Y^TY)} = \sqrt{diag(W^TCW)}$ is comprised of K 35

features extracted from the correlation matrix C. The kth feature is proportional to the variance in the direction of the kth column vector of W. If these vectors are randomly oriented and constrained to be unit norm, then the features represent a random sampling of the "peanut" shaped surface of directional variances (5). The subsequent stages in the network are: a batch normalization layer, a fully connected classification layer with L hidden units, a second batch normalization layer, and a softmax layer.

Results

We assessed the performance of the two networks using data from the Human Connectome Project (HCP) (6). Two rsfMRI scans acquired on Day 1 were used for training, while the two scans from Day 2 were used for validation and testing.

For M = 379 ROIs, N = 100 time points (72s duration) per 50 segment, and K = 256 hidden units, the mean classification 51 accuracies of the corrNN and normNN models were 99.9%52 and 99.2%, respectively, for an initial set of 100 subjects, and 53 99.8% and 99.5% for a second independent set of 100 subjects. 54 These accuracies are higher than those reported (94.3%) to 55 98.5%) for RNN models (2, 3). For comparison, the mean 56 classification accuracy using the similarity of the correlation 57 coefficients was 79.4% for 100 time points per segment, which 58 is higher than the 68% mean accuracy reported in (1) using 59 data from a different dataset. 60

We used a greedy search algorithm to assess the relative 61 importance of the ROIs with respect to model accuracy. Im-62 portance maps are shown in the top rows of Figures 1C and 1D, 63 respectively, with the subsequent rows thresholded to highlight 64 the top 15 to 60 ROIs. When considering the top 60 ROIs, 65 the highest number of ROIs for both models are found in 66 the dorsolateral prefrontal cortex followed by inferior parietal 67 cortex, lateral temporal cortex, superior parietal cortex (for 68 CorrNN), inferior frontal Cortex, and dorsal stream visual 69 cortex, where brain regions are as defined in (7). 70

We used the top ROIs to evaluate CorrNN and NormNN 71 performance with 15 to 60 ROIs and 5 to 1000 time points, as 72 shown in Figures 1E and 1F, respectively. As the number of 73 ROIs decreases, the number of time points needed to achieve 74 higher accuracy increases. Defining 99.5% as the threshold for 75 high mean accuracy, we observed that this threshold is sur-76 passed with as few as M = 60 ROIs and N = 100 time points 77 for CorrNN and 40 ROIs and 200 time points for NormNN, 78

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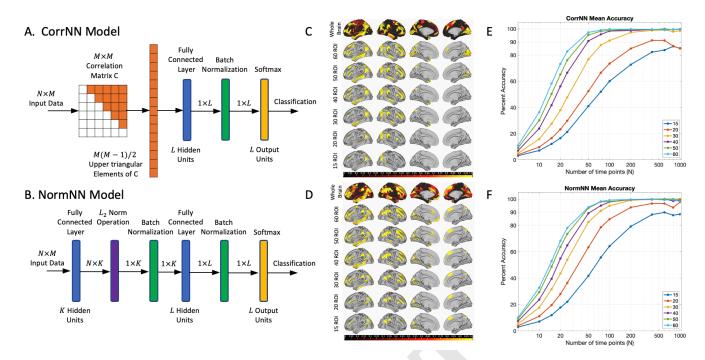


Fig. 1. (A,B) CorrNN and NormNN model structures. (C,D) Top rows: Maps showing the relative importance of the ROIs for identification accuracy with maximum importance of 1.0 indicated in yellow. The remaining rows are thresholded to show the locations of the top 15 to 60 ROIs. (E,F) Mean identification accuracies as a function of the number of time points and ROIs.

⁷⁹ corresponding to $M \times N = 6000$ or 8000 total data points, ⁸⁰ respectively.

To further explore the dependence on number of ROIs and 81 time points, we considered combinations (M, N) where the 82 total number of data points was constrained to be equal to 83 or close to either 6000 or 10,000 (see Figure 2 caption). For 84 CorrNN, high mean accuracies are obtained for two of the 85 combinations (dark red squares) with 6000 data points and 86 all five of the combinations (dark red diamonds) with 10,000 87 points, respectively. 88

For NormNN, the number of parameters exhibits a linear 89 dependence on the number of ROIs (M) as compared to the 90 quadratic dependence for CorrNN (see Figure 2 caption). To 91 better compare the models, we increased K by powers of 2 up 92 to the value $K_{eq} = 0.5L \left(M^2 - M\right) / (M + L + 3)$ for which the 93 numbers of NormNN and CorrNN parameters were equivalent, 94 while also including K_{eq} as one of the possible options. In figure 95 2b, we show NormNN accuracies obtained for either (1) the 96 97 minimum value of $K \geq 256$ that surpassed the 99.5% threshold or (2) the value $K \leq K_{eq}$ that achieved the highest accuracy 98 when the threshold was not met. High mean accuracies were 99 obtained for three and four of the combinations with 6000 and 100 10,000 data points, respectively. As shown by the histograms, 101 the high mean CorrNN and NormNN accuracies correspond 102 to robust identification performance with the majority of the 103 trials demonstrating 100 percent prediction accuracy. 104

Using the ROIs determined from the first 100 subjects we evaluated performance on the 2nd set of 100 subjects for the combinations denoted in Figure 2. High mean CorrNN accuracies ($\geq 99.5\%$) were maintained for both of the previously identified high performance combinations with 6000 points and three of the combinations with 10,000 points, with the remaining two combinations (with $M \geq 300$) exhibiting slightly lower accuracies ($\geq 99.33\%$) for the 2nd dataset. Thus, the same set of ROIs can offer comparable and high levels of performance across independent datasets.

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For NormNN we find that the first layer trained weights are 115 randomly distributed so that the features after the L_2 norm 116 operation represent an approximately uniform sampling of the 117 directional variance surface of C. Indeed, high performance 118 can also be achieved by replacing the first layer with a set of 119 random Gaussian weights. The generalizability of the features 120 across datasets exhibits a dependence on the number of units 121 K. For example, when using first layer weights trained using 122 the first set of subjects, performance for the combination 123 (50, 200) with K = 256 drops from 99.66% for the first 100 124 subjects to 97.98% for the second 100 subjects. Increasing 125 to 512 units with weights trained using the first set yields 126 accuracies of 99.64% and 99.52% for the first and second sets, 127 respectively. Essentially the same accuracy levels (99.59% and 128 99.56%) are obtained when using random weights for the first 129 layer. Thus, generalizability of the NormNN features increases 130 when there is a higher number of features to characterize the 131 directional variance. 132

Discussion

We have shown that shallow feedforward models can identify 134 subjects based solely on information in rsfMRI correlation ma-135 trices, with CorrNN directly using the correlation coefficients 136 as features while NormNN uses features related to the direc-137 tional variance surface. The performance levels achieved are 138 state-of-the-art, with high (> 99.5%) mean identification accu-139 racies robustly obtained with 6000 to 10,000 data points. For 140 comparison, the convolutional RNN presented in (3) achieved 141 98.5% accuracy with 23,600 data points. 142

Consistent with prior observations (1), high performance 143

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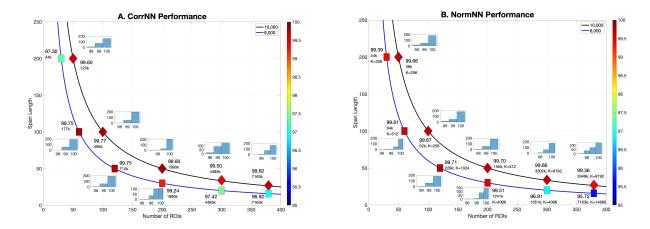


Fig. 2. (A,B) CorrNN and NormNN identification accuracies for combinations (M, N) of numbers of ROIs (M) and span lengths (N) that are constrained to have either 6000 or 10,000 data points, with the exception of the combinations (379, 16), (300, 34), and (379, 27), which have 6064, 10,200, and 10,233 data points, respectively. Mean accuracies are indicated by labels and color scale. The numbers of model parameters (in thousands) for CorrNN $\left(0.5L\left(M^2 - M + 6\right)\right)$ and NormNN (K (M + L + 3) + 3L) are also listed (with L = 100), as are the numbers of hidden units (K) for NormNN combinations. For combinations where CorrNN mean accuracy is greater than 99%, auto-scaled histograms show the distribution of identification accuracies obtained over 250 test trials per combination.

can be achieved when using a subset of the ROIs, including
those located in frontoparietal and lateral temporal regions.
The same set of ROIs can be used to achieve high performance
across independent datasets, suggesting that the predictive
value of inter-subject variability in the functional boundaries
and connectivity of these regions generalizes across datasets.

While combinations with span lengths as short as 27 points 150 (19.5s; CorrNN (379, 27)) can offer high performance, they 151 require a large number of model parameters. In contrast, 152 combinations with fewer ROIs but increased span lengths (e.g. 153 (100, 100)) achieve high performance with one to two orders 154 of magnitude fewer parameters. For NormNN the number of 155 trainable parameters can be further decreased through the use 156 of random weights in the first layer. 157

The effectiveness of the feedforward networks for distinguishing individuals with relatively little data suggests that similar future approaches may have the potential to more fully utilize the information contained in rsfMRI data to better identify disease-related differences.

163 Materials and Methods

164 165 Data and Preprocessing. We used pre-processed rsfMRI data from the 100 Unrelated Subjects subset of the HCP1200 Data Release 166 and an additional 100 subjects from the S900 subset. HCP pre-167 processing included detrending, denoising, and registration to a 168 169 common cortical surface. We divided the data into 379 regions of interest (ROI) consisting of 360 ROIs in the cortex as defined in (7)170 and 19 subcortical ROIs as defined in the group average parcellation 171 provided by the HCP (6). The time series were averaged within 172 each ROI and global signal regression was applied to the ROI time 173 174 series.

Training, Validation, and Testing. We used the ROI-averaged data 175 from day one as the training set (2 scans; 1200 pts per scan) 176 and data from day two as validation and test sets (1 scan each). 177 The performance was initially assessed using K = 379 ROIs and 178 N = 100 time points. Overlapping data segments were used with 179 shifts of 1 point between segments for training and 25 points for both 180 181 validation and testing. The full connected layers were initialized with the Glorot uniform initializer We used the Adam optimizer with 182 learning rate, β_1 , and β_1 values of 0.001, 0.9, and 0.999, respectively. 183 We used a batch size of 64 and monitored the validation loss every 184

600 steps with patience set to 30 monitoring steps, with learning rate annealed by halving it every 100 monitoring points.

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Using the trained model weights, we assessed the relative impor-187 tance of the ROIs by first looping over all 379 ROIs, independently 188 zeroing out the data from each ROI, and finding the ROI for which 189 the model retained its maximum accuracy. The identified ROI data 190 was eliminated (i.e. set to zero) for the remainder of the process 191 and the search was repeated over the remaining 378 ROIs to select 192 the next ROI for elimination. This process was continued until only 193 one ROI remained. The importance score of each ROI was $1 - M_c$ 194 where M_c denotes the model accuracy just prior to ROI elimination. 195

We then examined performance across a range of ROI numbers 196 (K = 15 to 60; with the top K ROIs selected based on importance197 scores) and durations (N = 5 to 1000 time points), retraining the 198 models for each combination (K, N) with 1 point shifts for both 199 training and validation. Testing was performed with 250 randomly 200 chosen initial starting points with the exception of 200 sequential 201 points for N = 1000. Performance using additional parameter 202 combinations was also evaluated. 203

We used the approach of (1) to identify subjects based on similarity of the correlation coefficient matrices. Target matrices were calculated using all the data from day one, whereas test matrices were calculated using data segments from day two. Identification was performed by computing the spatial correlation between the test and target matrices and then matching (with replacement) each test matrix to the most highly correlated target matrix. 200

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