

1 **Gaze and Movement Assessment (GaMA): Inter-site validation of a**
2 **visuomotor upper limb functional protocol**

3
4 Heather E. Williams¹, Craig S. Chapman², Patrick M. Pilarski³, Albert H. Vette^{1,4,5}, Jacqueline S.
5 Hebert^{3,4,5*}

6
7

8 ¹Department of Mechanical Engineering, Faculty of Engineering, University of Alberta,
9 Edmonton, Alberta, Canada

10
11 ²Faculty of Kinesiology, Sport, and Recreation, University of Alberta, Edmonton, Alberta,
12 Canada

13
14 ³Department of Medicine, Faculty of Medicine and Dentistry, University of Alberta, Edmonton,
15 Alberta, Canada

16
17 ⁴Department of Biomedical Engineering, Faculty of Medicine and Dentistry, University of
18 Alberta, Edmonton, Alberta, Canada

19
20 ⁵Glenrose Rehabilitation Hospital, Alberta Health Services, Edmonton, Alberta, Canada

21
22
23
24
25
26
27

28 * Corresponding author

29 E-mail: jhebert@ualberta.ca

30
31

32 **Abstract**

33 **Background:** Successful hand-object interactions require precise hand-eye coordination with
34 continual movement adjustments. Quantitative measurement of this visuomotor behaviour could
35 provide valuable insight into upper limb impairments. The Gaze and Movement Assessment
36 (GaMA) was developed to provide protocols for simultaneous motion capture and eye tracking
37 during the administration of two functional tasks, along with data analysis methods to generate
38 standard measures of visuomotor behaviour. The objective of this study was to investigate the
39 reproducibility of the GaMA protocol across two independent groups of non-disabled participants,
40 with different raters using different motion capture and eye tracking technology.

41 **Methods:** Twenty non-disabled adults performed the Pasta Box Task and the Cup Transfer Task.
42 Upper body and eye movements were recorded using motion capture and eye tracking,
43 respectively. Measures of hand movement, angular joint kinematics, and eye gaze were compared
44 to those from a different sample of twenty non-disabled adults who had previously performed the
45 same protocol with different technology, rater and site.

46 **Results:** Participants took longer to perform the tasks versus those from the earlier study, although
47 the relative time of each movement phase was similar. Measures that were dissimilar between the
48 groups included hand distances travelled, hand trajectories, number of movement units, eye
49 latencies, and peak angular velocities. Similarities included all hand velocity and grip aperture
50 measures, eye fixations, and most peak joint angle and range of motion measures.

51 **Discussion:** The reproducibility of GaMA was confirmed by this study, despite a few differences
52 introduced by learning effects, task demonstration variation, and limitations of the kinematic
53 model. The findings from this study provide confidence in the reliability of normative results
54 obtained by GaMA, indicating it accurately quantifies the typical behaviours of a non-disabled

55 population. This work advances the consideration for use of GaMA in populations with upper limb
56 sensorimotor impairment.
57

58 **Introduction**

59 Various sensorimotor impairments including stroke [1], amputation [2], and spinal cord
60 injury [3] lead to deficits in upper limb performance that can hamper activities of daily living
61 requiring precise hand-object interactions [4]. Various functional assessments are used to gauge
62 the functional impact of upper limb impairment and to monitor rehabilitative progress thereafter
63 [5], [6]. However, such assessments often do not precisely quantify hand and joint movements,
64 grip adjustments [7], [8], or hand-eye interaction, which is recognized as an important behaviour
65 during grasp control [9], [10]. Quantitative measurement of visuomotor behaviour collected during
66 the execution of functional tasks can enhance the understanding of these movement features.
67 Measurement technologies commonly used for this purpose include eye tracking and motion
68 capture. Assessments reliant on such specialized equipment, however, suffer from a lack of
69 standardized protocols and can be criticized as not being generalizable to activities of daily
70 function. Furthermore, technology-based assessments risk becoming obsolete as newer
71 technologies emerge, hindering the opportunity for robust comparisons over time.

72 The Gaze and Movement Assessment (GaMA) protocol was designed to overcome these
73 limitations. GaMA includes two standardized functional upper limb tasks that incorporate common
74 dextrous hand demands of daily living [7]. GaMA also includes an analysis software, which
75 requires a standardized data set of synchronized motion and eye data coordinates as input (obtained
76 using motion capture and eye tracking during functional task execution), and outputs metrics of
77 hand movement, angular joint kinematics, and eye gaze behavior [7]–[9]. GaMA’s input data set
78 can be obtained by various data collection hardware and software solutions, rendering the
79 assessment protocol amenable to technological evolution (for example, markerless motion capture
80 and mobile eye trackers). Additionally, GaMA measures remain relevant and equipment-

81 independent for future comparative purposes, potentially both within and across research sites.
82 The ability to compare results across sites would be extremely valuable as it could facilitate larger
83 subgroup comparisons when smaller populations of individuals with upper limb impairments are
84 studied, such as upper limb prosthesis users.

85 In order to validate a new protocol such as GaMA, it is essential to determine
86 reproducibility. Reproducibility of a test or method is defined as the closeness of the agreement
87 between independent results obtained by following the same procedures, but under different
88 experimental conditions [11]. Due to the inherent variability found in clinical populations,
89 reproducibility of a test to assess movement behaviour is typically first studied in a non-disabled
90 population. While intra-rater test-retest reliability of GaMA has been demonstrated for hand
91 movement and angular joint kinematic measures for non-disabled individuals [7], [8], it has yet to
92 be determined whether these and other measures obtainable by GaMA are reproducible across
93 raters and sites. Furthermore, it is often assumed that the non-disabled population will behave
94 similarly (or identically) across test sites; yet, it is known that deviations from protocols can result
95 in data set disparity amongst the population [12]. If a standardized protocol can be shown to yield
96 measures that are similar across sites, the data sets could be combined for a richer understanding
97 (or more saturated data set) of non-disabled movement behaviour.

98 The objective of this study, therefore, was to conduct an inter-site validation of GaMA by
99 assessing the reproducibility of the visuomotor measures in non-disabled individuals presented by
100 Valevicius et al. and Lavoie et al. [7]–[9]. More specifically, this study sought to determine
101 whether the same hand movement, angular joint kinematic, and eye gaze measures could be
102 obtained by testing a second independent group of non-disabled participants, at a different site
103 equipped with different motion capture and eye tracking technology, and administered by a
104 different rater. Establishing the reproducibility of GaMA in the non-disabled population advances

105 its consideration as an outcome assessment protocol for populations with sensorimotor
106 impairments of the upper limb.

107 **Methods**

108 For comparative purposes, the research conducted by Valevicius et al. [7], [8] and Lavoie
109 et al. [9] is referred to in this paper as ‘the original study’, and the data set analyzed by these studies
110 is referred to as ‘the original data set’. The new research presented in this article is referred to as
111 ‘the repeated study’ and its data as ‘the repeated data set’. Unless otherwise specified, the same
112 procedures were followed in both studies. Ethical approval for these procedures was obtained by
113 the University of Alberta Health Research Ethics Board (Pro00054011), the Department of the
114 Navy Human Research Protection Program, and the SSC-Pacific Human Research Protection
115 Office.

116

117 **Participants**

118 A total of 22 non-disabled adults were recruited to participate in the repeated study. Data
119 from two participants were removed due to problems arising from software issues. The
120 characteristics of the 20 participants from the original study [7]–[9] and the 20 participants in the
121 repeated study are detailed in **Error! Reference source not found.** In both studies, two
122 participants performed the tasks without corrected vision, since they had to remove their glasses
123 to don the eye tracker. These participants, however, reported that their vision was sufficient to
124 allow them to confidently perform the task.

125

126 **Table 1: Original and repeated study participant characteristics.**

Research Participant Characteristics	Original Study	Repeated Study
Male participants	11	13
Female participants	9	7
Self-reported right-handed participants	18	19
Participants with normal or corrected to normal vision	18	18
Participant age (years – mean \pm standard deviation)	25.8 \pm 7.2	24.4 \pm 7.3
Participant height (cm – mean \pm standard deviation)	173.8 \pm 8.3	171.0 \pm 7.7

127

128 Equipment

129 Motion capture and eye tracking hardware and software specifications for the original
130 study and the repeated study are indicated in **Error! Reference source not found.** The equipment
131 was set up in the repeated study as specified in the original study [7]–[9]. Rigid plates and a
132 headband (each holding four retroreflective markers) were attached to the participant in
133 accordance with Boser et al.’s *Clusters Only* kinematic model [13]. To improve rigid body motion
134 tracking in the repeated study, the hand plates were redesigned as shown in Fig 1. For both studies,
135 markers were attached to the index finger (middle phalange) and thumb (distal phalange) [7]; a
136 head-mounted eye tracker was placed on the participant and positioned in accordance with the
137 manufacturer’s instructions; and a motion capture calibration pose was collected for each
138 participant, as outlined by Boser et al. [13].

139

140 **Table 2: Specifications of the motion capture and eye tracking systems used in the original**
141 **and repeated studies.**

Specifications	Original Study	Repeated Study
Motion capture camera	Vicon Bonita 10 (Vicon Motion Systems Ltd, Oxford, UK)	OptiTrack Flex 13 (Natural Point, OR, USA)
Number of cameras	12	8

Camera sampling frequency	120 Hz	120 Hz
Head-mounted binocular eye tracker	Dikablis Professional 2 (Ergoneers GmbH, Manching, Germany)	Pupil (Pupil Labs GmbH, Berlin, Germany)
Eye camera sampling frequency	60 Hz	120 Hz

142
143

144 **Fig 1. Retroreflective marker placement.** Marker placement for participants in the original study
145 (A) and repeated study (B), showing differences in the hand marker plate designs.

146

147 Data Collection

148 In both studies, the two functional tasks introduced by Valevicius et al. (the Pasta Box Task
149 and Cup Transfer Task) [7] were administered. Each participant completed 20 error-free trials of
150 the two tasks, while simultaneous motion and eye tracking data were collected. Prior to this, each
151 participant was given verbal instructions, a demonstration, and at least one familiarization trial of
152 each functional task. Task order was randomized for each participant. At least two gaze
153 calibrations (outlined by Lavoie et al. [9]) were collected before participants executed their initial
154 trial of each task, and one after they completed their final trial of the last task; given that there
155 were two functional tasks, a minimum of 5 calibrations were performed per participant.

156 The original data collection protocol differed from the repeated study in one notable way.
157 In the original study, every participant performed a total of 60 trials of each task, 20 of which were
158 under each of the following conditions: (1) only motion capture data were collected, (2) only eye
159 tracking data were collected, and (3) both motion capture and eye tracking data were collected. As
160 the repeated study consisted solely of collecting data during simultaneous motion capture and eye
161 tracking, it was only compared to that of the original data set captured under condition (3) ‘both’.

162 In the original study, the order of conditions for each participant was block randomized to one of
163 4 block orders, with motion (1) and both (3) conditions always sequential. As a consequence of
164 the partial randomization order, three quarters of the original study participants were afforded at
165 least 20 extra trials executing each functional task prior to testing under the ‘both’ condition.

166

167 Experimental Data Analysis

168 Data analysis in the repeated study was undertaken as outlined by Valevicius et al. and
169 Lavoie et al. [7]–[9]: motion capture marker trajectory data and pupil position data were filtered
170 and synchronized; hand movement and angular kinematic measures were calculated; the virtual
171 location of the participant’s gaze (represented by a gaze vector) was determined using gaze
172 calibration data; and gaze fixations to areas of interest were calculated. Due to insufficient pupil
173 data, the data from one participant were removed from the repeated data set for the Cup Transfer
174 Task, and data from four participants were removed for the Pasta Box Task.

175 For each functional task, the repeated data set were divided into distinct *movements* based
176 on hand velocity, the velocity of the task object(s), and grip aperture values, as per Valevicius et
177 al. [7]. The data from each movement were further segmented into the *phases* of ‘Reach’, ‘Grasp’,
178 ‘Transport’, ‘Release’, and ‘Home’; the Home phase was not used for data analysis. Due to the
179 short duration of the Grasp and Release phases, combined *movement segments* of ‘Reach-Grasp’
180 and ‘Transport-Release’ were used in hand movement analysis [7]. Eye latency measures were
181 calculated at instances of *phase transition*, both at the end of a Grasp phase and at the beginning
182 of a Release phase (referred to as ‘Pick-up’ and ‘Drop-off’ by Lavoie et al. [9]). An illustration of
183 how one distinct movement was separated into the abovementioned subsets (phases, movement
184 segments, and phase transitions) can be found in Fig 2.

185

186 **Fig 2. Phase transitions, phases, and movement segments within one movement.** Typical hand
 187 and object velocity profiles are displayed in grey and orange lines, respectively. Reach, Grasp,
 188 Transport and Release phases are presented along the bar as red, orange, blue and green,
 189 respectively. Home (grey bar) refers to the standardized location to which the hand returns at the
 190 completion of the movement.

191

192 GaMA Measures

193 Duration (phase and trial), hand movement, angular joint kinematic, and eye gaze measures
 194 were calculated for the original and repeated studies, as outlined by Valevicius et al. [7], [8] and
 195 Lavoie et al. [9], and are listed in **Error! Reference source not found.** Lavoie et al.’s ‘fixations
 196 to future’ measure was not considered in this study as these fixations were shown to be unlikely to
 197 occur in non-disabled participants for both tasks [9]. In addition to the measures listed in **Error!**
 198 **Reference source not found.**, the relative duration of each phase was calculated as the percent of
 199 time spent in that phase, relative to the given Reach-Grasp-Transport-Release sequence.

200

201 **Table 3: Comparative measures, including duration, hand movement, angular joint**
 202 **kinematic, and eye gaze measures, and the subsets of each movement for which they were**
 203 **calculated.**

Type of Measure	Measures	Movement Subsets
Duration (from Lavoie et al. [9])	Phase duration	Reach, Grasp, Transport, Release
Hand movement (from Valevicius et al. [7])	Hand distance travelled Hand trajectory variability Peak hand velocity Percent-to-peak hand velocity Number of movement units	Reach-Grasp, Transport-Release
	Peak grip aperture Percent-to-peak grip aperture Percent-to-peak hand deceleration	Reach-Grasp
	Percent fixation to Hand in Flight Number of fixations to Hand in Flight	Reach, Transport

	Eye Arrival Latency Eye Leaving Latency	End of Grasp, Beginning of Release
Angular joint kinematics (from Valevicius et al. [8])	Peak angle, range of motion, and peak angular velocity for the following degrees of freedom: <ul style="list-style-type: none"> • Trunk flexion/extension • Trunk lateral bending • Trunk axial rotation • Shoulder flexion/extension • Shoulder abduction/adduction • Shoulder internal/external rotation • Elbow flexion/extension • Forearm pronation/supination • Wrist flexion/extension • Wrist ulnar/radial deviation 	Movement only
Eye gaze (from Lavoie et al. [9])	Percent fixation to Current Number of fixations to Current	Reach, Grasp, Transport, Release

204
205
206

In the repeated study, the calculation of hand movement measures was altered due to the creation of a virtual rectangular prism, which approximated the participant’s hand position at each point in time. Using the centre of this prism, hand position and velocity were subsequently calculated. For comparative purposes, the original study’s hand movement results were recalculated via this methodology rather than the original calculation of Valevicius et al. using the average position of the three hand plate markers [7]).

212

213 Statistical Analysis

214 The aim of the statistical analysis was to detect significant differences between the original
215 and repeated data sets, and to determine whether such differences were more pronounced for
216 particular movements and/or movement subsets (phase, movement segment, or phase transition).
217 To investigate differences between the two groups of participants, a series of repeated-measures
218 analyses of variance (RMANOVAs) and pairwise comparisons were conducted for each measure
219 and task. RMANOVA group effects or interactions involving group were followed up with either

220 an additional RMANOVA or pairwise comparisons between groups if the Greenhouse-Geisser
221 corrected p value was less than 0.05. Pairwise comparisons were considered to be significant if the
222 Bonferroni corrected p value was less than 0.05. Detailed statistical analysis methods can be found
223 in supplementary materials (S1 Text).

224 **Results**

225 **Duration**

226 For both the Pasta Box Task (or ‘Pasta’) and the Cup Transfer Task (or ‘Cups’), the
227 repeated study participants took significantly more time to complete the tasks than the original
228 study participants (Pasta: 11.8 ± 3.4 seconds versus 8.8 ± 1.2 seconds, $p < 0.01$; Cups: 13.9 ± 2.5
229 seconds versus 10.5 ± 1.3 seconds, $p < 0.0001$). The repeated study participants had longer phase
230 durations than the original study participants, with all Grasp and Transport phases and the
231 Movement 2 Release phase significantly prolonged in Pasta, and all phases significantly prolonged
232 in Cups (S2 Table). The two participant groups, however, displayed similar relative phase
233 durations throughout both tasks, with no significant differences.

234

235 **Hand Movement**

236 The repeated study participants had greater hand distances travelled than the original study
237 participants, with significant increases in Movement 1 & 3 segments of Pasta (S3 Table) and in all
238 Cups movement segments, except for Movement 1 & 4 Transport-Releases (S4 Table). However,
239 Fig 3 (Pasta) and Fig 4 (Cups) show that the average hand trajectories chosen by both participant
240 groups were similar. The repeated study participants also had larger hand trajectory variability
241 than the original study participants, with significant increases in all Pasta movement segments

242 except for Movement 3 Transport-Release (S4 Table) and all Cups movement segments (S5
243 Table). The repeated study participants had a greater number of movement units than the original
244 study participants, with significant increases in all movement segments of Pasta and for Movement
245 1 & 4 Reach-Grasp and Movement 1 to 3 Transport-Release segments of Cups.

246

247 **Fig 3. Pasta Box Task hand trajectories.** Trajectories are displayed for participants in the original
248 (pink) and repeated (blue) studies for Movements 1, 2, and 3. The solid lines represent participant
249 group averages, and the three-dimensional shading represents the standard deviation of participant
250 group means.

251

252 **Fig 4. Cup Transfer Task hand trajectories.** Trajectories are displayed for participants in the
253 original (pink) and repeated (blue) studies for Movements 1, 2, 3, and 4. The solid lines represent
254 participant group averages, and the three-dimensional shading represents the standard deviation of
255 participant group means.

256

257 Participants in the original and repeated studies had similar hand velocity profiles for both
258 tasks, as shown in Fig 5A and 5B. Although the peaks in the repeated study appeared smaller,
259 these differences were non-significant throughout both tasks (S4 Table and S5 Table). Significant
260 percent-to-peak hand velocity differences were identified for the Movement 1 Reach-Grasp
261 segment of Pasta and the Movement 2 & 3 Reach-Grasp segments of Cups, but the differences
262 between the mean values of the two participant groups were less than one standard deviation of
263 the original study results. Participants in the original and repeated studies showed similar percent-
264 to-peak hand deceleration values, with no significant differences in Pasta and a significantly

265 difference only for the Movement 4 Reach-Grasp segment of Cups. However, the difference
266 between the mean values of the two participant groups in this movement segment was less than
267 one original study standard deviation.

268

269 **Fig 5. Hand velocity profiles for the Pasta Box Task (A) and the Cup Transfer Task (B); and**
270 **grip aperture profiles for the Pasta Box Task (C) and the Cup Transfer Task (D).** Original
271 study data are presented in pink, and repeated study data in blue. The solid lines represent
272 participant group averages, and the shading represents one standard deviation of the participant
273 group means. This task is segmented into Reach (red), Grasp (orange), Transport (blue), Release
274 (green), and Home (grey) phases for each movement.

275

276 Participants in the original and repeated studies had similar grip aperture profiles for both
277 tasks, as shown in Fig 5C and 5D, with no significant differences in peak grip aperture identified
278 for either task. Also, no significant differences in percent-to-peak grip aperture were identified in
279 Pasta, and a significant difference was only identified in the Movement 4 Reach-Grasp segment
280 of Cups.

281

282 Angular Joint Kinematics

283 Angular kinematic trajectories illustrating the average joint trajectories of participants are
284 shown in Fig 6 (Pasta) and Fig 7 (Cups). Similar angular kinematic profiles existed between the
285 original and repeated study participants, with only a few differences; participants in the repeated
286 study had an increased standard deviation for trunk flexion/extension (both tasks), and an offset
287 was present between the wrist flexion/extension angles (both tasks) and between the wrist

288 ulnar/radial deviations angles (Pasta only) of the two participant groups. Angular kinematic
289 measures are presented in **Error! Reference source not found.** (Pasta) and **Error! Reference**
290 **source not found.** (Cups). The original and repeated study participants generally had similar peak
291 joint angles in both tasks. Significant peak angle differences were found in wrist flexion/extension
292 for Movements 1 and 2 of Pasta and all movements of Cups, and in wrist radial/ulnar deviation for
293 all movements of Pasta.

294

295 **Fig 6. Pasta Box Task angular joint trajectories.** Original (pink) and repeated (blue) studies
296 angular joint trajectories for trunk flexion/extension, lateral bending, and axial rotation; shoulder
297 flexion/extension, abduction/ adduction, and internal/external rotation; elbow flexion/extension
298 and forearm pronation/supination; and wrist flexion/extension and ulnar/radial deviation. The solid
299 lines represent participant group averages, and the shading represents one standard deviation of
300 the participant group means. The task is segmented into Reach (red), Grasp (orange), Transport
301 (blue), Release (green), and Home (grey) phases for each movement.

302

303 **Fig 7. Cup Transfer Task angular joint trajectories.** Original (pink) and repeated (blue) studies
304 angular joint trajectories for trunk flexion/extension, lateral bending, and axial rotation; shoulder
305 flexion/extension, abduction/ adduction, and internal/external rotation; elbow flexion/extension
306 and forearm pronation/supination; and wrist flexion/extension and ulnar/radial deviation. The solid
307 lines represent participant group averages, and the shading represents one standard deviation of
308 the participant group means. The task is segmented into Reach (red), Grasp (orange), Transport
309 (blue), Release (green), and Home (grey) phases for each movement.

310

311 **Table 4: Pasta Box Task angular joint kinematic values, with significant results of the**
 312 **RMANOVAs and pairwise comparisons.**

		Peak Angle (degrees)			Range of Motion (degrees)			Peak Angular Velocity (degrees/s)		
	M	<i>p</i>	Original	Repeated	<i>p</i>	Original	Repeated	<i>p</i>	Original	Repeated
Trunk FE	1	ns	-2.1 ± 2.4	-0.9 ± 4.7	ns	4.9 ± 1.6	6.0 ± 2.2	ns	18.8 ± 5.4	23.7 ± 7.8
	2	ns	-2.7 ± 2.6	0.2 ± 5.0	*	3.6 ± 1.0	5.8 ± 2.5	*	14.9 ± 5.4	22.9 ± 8.4
	3	ns	-2.1 ± 2.5	0.2 ± 5.0	ns	4.9 ± 1.4	7.3 ± 4.2	*	18.2 ± 5.0	28.4 ± 13.6
Trunk LB	1	ns	6.5 ± 3.5	8.6 ± 5.4	ns	8.7 ± 2.8	10.2 ± 4.2	ns	21.7 ± 5.5	19.9 ± 8.0
	2	ns	0.2 ± 2.5	1.7 ± 2.4	*	5.6 ± 2.0	8.2 ± 2.6	ns	12.8 ± 3.6	15.0 ± 3.7
	3	ns	7.2 ± 3.5	11.6 ± 6.0	*	11.8 ± 2.8	17.3 ± 6.6	ns	21.3 ± 3.9	24.2 ± 6.6
Trunk AR	1	ns	6.0 ± 3.9	5.0 ± 4.6	ns	17.8 ± 2.4	14.9 ± 4.9	ns	42.6 ± 6.6	37.0 ± 11.1
	2	ns	13.7 ± 3.9	12.4 ± 5.5	ns	15.1 ± 3.0	13.8 ± 4.6	ns	33.4 ± 8.3	36.8 ± 13.6
	3	ns	13.3 ± 3.8	12.9 ± 5.8	ns	25.5 ± 3.0	24.1 ± 8.2	ns	58.6 ± 10.8	52.3 ± 17.1
Sho FE	1	ns	51.3 ± 10.6	49.3 ± 6.5	ns	69.3 ± 7.6	61.4 ± 8.5	*	192.3 ± 39.4	143.8 ± 44.1
	2	ns	64.9 ± 11.4	64.7 ± 8.7	ns	72.1 ± 9.7	67.1 ± 9.9	*	200.8 ± 40.9	154.1 ± 45.0
	3	ns	66.8 ± 11.2	67.0 ± 8.8	ns	86.0 ± 9.9	81.7 ± 10.1	ns	233.0 ± 40.4	192.8 ± 54.2
Sho AA	1	ns	-5.8 ± 5.1	-6.1 ± 6.8	ns	19.3 ± 6.5	20.1 ± 5.2	ns	76.6 ± 23.6	65.6 ± 27.0
	2	ns	1.4 ± 7.2	3.1 ± 9.4	ns	25.6 ± 8.8	25.6 ± 8.0	ns	81.5 ± 30.7	69.7 ± 21.3
	3	ns	3.5 ± 6.9	4.0 ± 8.6	ns	28.9 ± 9.1	32.0 ± 10.5	ns	101.7 ± 27.6	90.0 ± 24.3
Sho IER	1	ns	22.8 ± 10.0	16.4 ± 8.4	ns	44.0 ± 7.9	41.5 ± 9.2	*	151.1 ± 32.3	112.5 ± 40.8
	2	ns	32.6 ± 10.4	27.3 ± 9.6	ns	32.6 ± 6.7	27.8 ± 6.9	*	123.3 ± 23.1	89.4 ± 34.4
	3	ns	34.9 ± 9.6	29.7 ± 9.7	ns	54.2 ± 6.8	55.7 ± 10.2	ns	180.4 ± 33.8	148.9 ± 44.4
Elbow FE	1	ns	92.1 ± 11.9	85.4 ± 11.5	ns	76.4 ± 10.6	73.1 ± 10.2	*	274.2 ± 53.8	218.5 ± 62.1
	2	ns	103.6 ± 12.8	98.6 ± 12.7	ns	81.2 ± 9.6	78.8 ± 9.6	ns	268.1 ± 47.5	226.1 ± 51.4
	3	ns	103.8 ± 13.2	102.3 ± 12.2	ns	88.4 ± 11.6	87.4 ± 11.3	ns	270.3 ± 48.6	226.8 ± 55.2
Frm PS	1	ns	40.1 ± 22.5	33.8 ± 20.2	ns	77.0 ± 15.9	78.9 ± 19.0	*	308.6 ± 70.4	244.7 ± 72.5
	2	ns	51.3 ± 22.3	44.7 ± 20.2	ns	51.4 ± 18.2	47.1 ± 12.4	ns	176.4 ± 57.6	149.2 ± 51.7
	3	ns	51.4 ± 21.7	42.7 ± 19.9	ns	90.9 ± 17.3	85.3 ± 16.4	ns	181.8 ± 47.9	169.5 ± 62.2
Wrist FE	1	*	-18.6 ± 12.4	-29.1 ± 8.7	ns	28.6 ± 6.1	31.0 ± 8.4	*	136.8 ± 30.4	109.3 ± 27.2
	2	*	-11.8 ± 13.8	-23.5 ± 12.2	ns	25.5 ± 8.9	32.0 ± 10.3	ns	122.3 ± 36.4	119.6 ± 37.0
	3	ns	-12.6 ± 11.4	-22.5 ± 15.3	ns	32.3 ± 8.0	36.4 ± 14.7	ns	123.9 ± 38.6	123.0 ± 42.6
Wrist URD	1	*	14.6 ± 7.8	*23.1 ± 7.1	ns	30.9 ± 5.6	25.7 ± 7.4	*	108.9 ± 39.3	77.7 ± 30.1
	2	*	18.8 ± 7.8	*26.4 ± 6.8	ns	24.7 ± 7.3	22.4 ± 7.6	*	95.6 ± 23.0	69.1 ± 24.1
	3	*	16.3 ± 7.3	*24.6 ± 7.0	ns	29.7 ± 4.7	26.4 ± 5.8	*	117.5 ± 28.0	88.8 ± 30.8

313 Angular kinematic values include peak angle (degrees), range of motion (degrees), and peak
 314 angular velocity (degrees/s) of each movement (M) for trunk flexion/extension (FE), lateral
 315 bending (LB), and axial rotation (AR); shoulder (Sho) flexion/extension, abduction/adduction
 316 (AA), and internal/external rotation (IER); elbow flexion/extension and forearm
 317 pronation/supination (Frm PS); and wrist flexion/extension and radial/ulnar deviation (RUD). For
 318 the results of the pairwise comparisons (in column *p*), * indicates a *p* value less than 0.05, **
 319 indicates a *p* value less than 0.005, and ns indicates a *p* value that is not significant. Highlighted
 320 table cells also indicate significant differences (red = higher and blue = lower repeated study
 321 value).

322
323
324

Table 5: Cup Transfer Task angular joint kinematic values, with significant results of the RMANOVAs and pairwise comparisons.

	M	p	Peak Angle (degrees)		p	Range of Motion (degrees)		p	Peak Angular Velocity (degrees/s)	
			Original	Repeated		Original	Repeated		Original	Repeated
Trunk FE	1	ns	-4.4 ± 2.5	-1.2 ± 6.2	*	3.0 ± 1.5	4.7 ± 1.9	**	10.7 ± 3.4	16.0 ± 4.7
	2	ns	-6.3 ± 2.5	-2.9 ± 5.7	ns	9.1 ± 3.3	10.2 ± 2.5	ns	23.1 ± 6.8	25.2 ± 6.4
	3	ns	-5.6 ± 2.8	-2.1 ± 6.1	ns	9.6 ± 3.1	11.2 ± 3.2	ns	27.2 ± 7.8	31.8 ± 12.2
	4	ns	-5.7 ± 2.7	-3.0 ± 6.5	ns	4.7 ± 2.5	6.0 ± 1.5	ns	13.0 ± 4.1	16.6 ± 5.3
Trunk LB	1	ns	-0.4 ± 1.8	1.9 ± 3.9	**	4.8 ± 1.9	7.7 ± 2.3	ns	9.9 ± 3.6	12.0 ± 3.4
	2	ns	0.3 ± 4.1	1.9 ± 4.6	ns	7.2 ± 2.4	9.5 ± 3.6	ns	16.5 ± 6.0	19.0 ± 8.1
	3	ns	-0.6 ± 3.2	2.2 ± 4.1	**	6.2 ± 1.9	9.4 ± 3.3	ns	15.1 ± 3.7	20.9 ± 10.3
	4	ns	-1.1 ± 3.0	0.8 ± 4.4	*	4.0 ± 1.4	5.7 ± 2.0	ns	10.8 ± 3.4	12.9 ± 5.3
Trunk AR	1	ns	8.9 ± 3.7	7.7 ± 5.1	ns	9.3 ± 2.5	9.2 ± 2.7	ns	20.6 ± 4.0	21.5 ± 5.2
	2	ns	17.1 ± 5.0	15.7 ± 4.7	ns	10.7 ± 2.8	11.3 ± 3.4	ns	28.1 ± 7.4	30.1 ± 9.3
	3	ns	17.2 ± 5.0	16.4 ± 5.0	ns	16.7 ± 4.2	16.9 ± 4.7	ns	39.1 ± 9.8	44.2 ± 15.9
	4	ns	10.3 ± 3.9	8.6 ± 4.8	ns	7.9 ± 2.4	7.2 ± 2.3	ns	22.6 ± 7.3	22.2 ± 6.7
Sho FE	1	ns	49.2 ± 14.6	43.9 ± 9.1	*	62.7 ± 13.5	50.8 ± 11.4	*	142.1 ± 42.8	104.5 ± 31.7
	2	ns	56.8 ± 10.4	55.7 ± 7.3	ns	30.9 ± 6.2	29.6 ± 4.9	ns	103.9 ± 29.7	77.9 ± 31.7
	3	ns	57.5 ± 11.0	56.4 ± 7.5	ns	73.6 ± 10.4	66.6 ± 8.9	*	228.2 ± 58.8	174.3 ± 61.6
	4	ns	49.5 ± 14.8	43.7 ± 10.7	ns	29.6 ± 9.0	26.4 ± 8.6	ns	104.7 ± 25.0	95.2 ± 34.5
Sho AA	1	ns	-8.1 ± 4.7	-6.3 ± 6.2	ns	27.5 ± 7.1	23.7 ± 5.4	ns	80.4 ± 23.4	65.8 ± 19.7
	2	ns	-1.4 ± 5.9	-3.4 ± 8.2	ns	18.7 ± 5.6	16.2 ± 4.2	*	63.7 ± 17.1	49.3 ± 14.3
	3	ns	0.1 ± 5.5	-1.1 ± 7.7	ns	28.7 ± 8.6	23.9 ± 6.3	ns	98.1 ± 34.9	79.3 ± 33.0
	4	ns	-13.9 ± 6.9	-14.4 ± 7.1	ns	26.1 ± 6.0	21.7 ± 5.8	*	74.9 ± 19.4	59.3 ± 16.5
Sho IER	1	ns	44.9 ± 14.9	35.5 ± 10.9	ns	51.5 ± 13.9	41.2 ± 10.6	*	116.0 ± 57.8	74.1 ± 23.8
	2	ns	43.6 ± 13.8	34.8 ± 10.2	ns	33.1 ± 7.5	28.2 ± 6.5	**	180.2 ± 36.3	120.5 ± 43.1
	3	ns	41.8 ± 13.8	32.4 ± 10.1	*	49.9 ± 12.2	38.8 ± 10.4	*	188.8 ± 56.6	131.8 ± 49.3
	4	ns	46.6 ± 14.7	37.9 ± 11.8	ns	39.5 ± 9.6	36.6 ± 8.5	*	160.1 ± 39.0	120.4 ± 41.4
Elbow FE	1	ns	84.7 ± 12.3	78.5 ± 11.7	ns	44.6 ± 9.4	48.8 ± 10.7	ns	173.4 ± 44.5	150.6 ± 39.0
	2	ns	70.6 ± 11.6	66.6 ± 11.7	ns	60.4 ± 8.1	58.8 ± 8.2	ns	196.8 ± 30.6	174.5 ± 39.5
	3	ns	93.3 ± 12.9	84.0 ± 11.2	ns	84.6 ± 9.3	78.7 ± 11.8	*	281.1 ± 59.3	226.6 ± 63.3
	4	ns	84.7 ± 13.4	84.3 ± 11.6	ns	48.3 ± 6.0	53.5 ± 6.9	ns	227.7 ± 43.2	213.9 ± 43.6
Frm PS	1	ns	50.7 ± 21.5	50.2 ± 17.7	ns	31.0 ± 11.5	36.3 ± 11.2	ns	113.9 ± 24.3	125.4 ± 37.1
	2	ns	36.7 ± 19.5	43.2 ± 18.6	**	46.9 ± 12.6	62.9 ± 15.0	ns	182.4 ± 44.5	190.5 ± 69.2
	3	ns	49.7 ± 22.2	38.8 ± 19.9	ns	64.2 ± 11.5	62.5 ± 17.9	ns	196.2 ± 49.1	154.7 ± 52.7
	4	ns	43.3 ± 21.0	45.1 ± 19.8	ns	46.6 ± 9.7	56.6 ± 15.0	ns	188.6 ± 67.7	184.0 ± 50.4
Wrist FE	1	**	35.6 ± 11.4	22.8 ± 10.5	ns	74.2 ± 14.4	81.0 ± 16.4	ns	283.1 ± 74.0	259.6 ± 68.2
	2	*	28.4 ± 13.6	14.8 ± 10.2	ns	57.2 ± 7.4	55.2 ± 11.5	ns	276.5 ± 78.2	219.9 ± 87.4
	3	*	0.9 ± 14.9	-12.7 ± 10.5	ns	34.6 ± 10.9	41.9 ± 11.1	ns	162.9 ± 65.2	138.2 ± 37.0
	4	**	44.5 ± 13.6	28.6 ± 10.9	ns	61.7 ± 10.1	58.6 ± 13.1	*	299.9 ± 63.0	237.5 ± 65.5
Wrist URD	1	ns	24.6 ± 11.4	24.3 ± 7.5	**	37.7 ± 8.5	26.4 ± 8.2	**	134.9 ± 34.7	81.9 ± 26.4
	2	ns	23.6 ± 9.6	24.2 ± 7.6	ns	27.7 ± 6.1	23.1 ± 7.7	**	122.5 ± 35.3	84.1 ± 26.9
	3	ns	15.8 ± 7.4	18.1 ± 8.2	ns	25.1 ± 6.2	20.6 ± 6.3	**	115.0 ± 35.4	73.7 ± 22.1
	4	ns	26.9 ± 11.7	26.5 ± 7.8	ns	23.5 ± 6.0	20.5 ± 8.8	*	126.4 ± 33.9	91.8 ± 34.6

325 Angular kinematic values include peak angle (degrees), range of motion (degrees), and peak
326 angular velocity (degrees/s) of each movement (M) for trunk flexion/extension (FE), lateral
327 bending (LB), and axial rotation (AR); shoulder (Sho) flexion/extension, abduction/adduction
328 (AA), and internal/external rotation (IER); elbow flexion/extension and forearm
329 pronation/supination (Frm PS); and wrist flexion/extension and radial/ulnar deviation (RUD). For
330 the results of the pairwise comparisons (in column p), * indicates a p value less than 0.05, **

331 indicates a *p* value less than 0.005, and ns indicates a *p* value that is not significant. Highlighted
332 table cells also indicate significant differences (red = higher and blue = lower repeated study
333 value).
334

335 The original and repeated study participants also had similar ROM values in Pasta,
336 although significant differences were found for the Movement 2 trunk flexion/extension ROM and
337 the Movement 2 & 3 trunk lateral bending ROM. However, these differences were quite small
338 (with the largest being 5.3°). In Cups, differences in ROMs were significant in more movements
339 and degrees of freedom (DOFs), as indicated by the shading in **Error! Reference source not**
340 **found.** However, the significant trunk ROM differences were quite small (both less than 2°), and
341 the significant shoulder ROM differences were less than the respective original study standard
342 deviations for those DOFs.

343 The repeated study participants exhibited differences in peak angular velocities in most
344 DOFs in both tasks. The peak angular velocities in the trunk DOFs of repeated study participants
345 were usually greater than those of original study participants, with significant trunk
346 flexion/extension differences in Movement 1 and 2 of Pasta and Movement 1 of Cups. The peak
347 angular velocities in the remaining DOFs of the repeated study participants were usually smaller
348 than for the original study participants, with most significantly lower.

349

350 Eye Gaze

351 The repeated and original study participants exhibited similar eye fixations, with no significant
352 differences identified in either task, as shown in S5 Table (Pasta) and S6 Table (Cups). Significant
353 eye arrival latency differences were identified in all Grasp phase transitions and the Movement 3
354 Release phase transition of Pasta, as well as the Movement 3 phase transitions of Cups. No

355 significant eye leaving latency differences were identified in Pasta, but significant differences were
356 identified in the Movement 3 Release transition in Cups.

357 **Discussion**

358 Measures that were consistent between the original and repeated studies included all hand
359 velocity, grip aperture, and eye fixation results, along with most peak joint angle and ROM results.
360 Although participants in the repeated study took more time to complete each functional task
361 (greater overall duration), similar relative phase durations between the participant groups indicated
362 that the repeated study participants did not spend a disproportionate amount of time in any one
363 phase.

364 Participants in the original study may have displayed faster performance due to the prior
365 functional task trials that they completed (that is, during task trials where only motion capture or
366 eye tracking data were captured in the original study). This presumption is likely, given that
367 practice has been shown to decrease functional test completion time [14]. The longer phase
368 durations exhibited by the repeated study participants led to both increased eye arrival latencies
369 and decreased eye leaving latencies. Furthermore, their longer movement times resulted in
370 decreased joint angular velocities in shoulder, elbow, forearm, and wrist DOFs.

371 Learning effects may have also contributed to discrepancies in hand movement measures
372 between the original and repeated study participants. The repeated study participants exhibited an
373 increased number of movement units and increased hand trajectory variability, both of which were
374 likely due to the influence of fewer practice opportunities [15], [16]. Furthermore, increased hand
375 trajectory variability presumably contributed to the repeated study participants' increased average
376 hand distance travelled. Hand trajectory variances would be expected to be away from, or in
377 avoidance of, obstacles present in all task movements (box walls and the partition in the Cup

378 Transfer Task, and the shelf frames in the Pasta Box Task). Future studies that employ GaMA
379 should standardize the amount of functional task practice opportunities that participants receive.

380 Task demonstration variations by raters may also have contributed to task duration
381 differences between the two participant groups. Although the same script was used to explain the
382 tasks to participants in each study, small variances in task demonstration speed may have been
383 introduced by the raters. Since the timing of demonstrations is known to influence the resulting
384 pace of participants' movements [17], a slower demonstration may have contributed to the
385 repeated study's increase in task duration time. It is recommended that a standard task
386 demonstration video be created and shown to all participants to reduce the possible effects of rater
387 demonstration variation.

388 The angular kinematic measures revealed offsets in the wrist flexion/extension and
389 ulnar/radial deviation measures of the repeated study participants, likely due to differences in the
390 kinematic calibration pose across the two studies. Such calibration errors are known to be the main
391 limitation of the *Clusters Only* model [13]. In addition, a large standard deviation in trunk
392 flexion/extension was observed for repeated study participants, also likely attributable to errors in
393 the kinematic calibration. That is, the calibration of this DOF depends on how each participant
394 chooses to 'stand upright'. To limit such deviations in joint angles, the rater must ensure that the
395 participant does not have a bent wrist and is standing as upright as possible, when a kinematic
396 calibration pose is captured.

397 Further angular kinematics variations were observed between the two participant groups,
398 in both the forearm pronation/supination and wrist radial/ulnar deviation ROMs. Such deviations
399 were introduced by the *Clusters Only* model, which calculates wrist and forearm angles in a
400 manner that is different from other DOFs. This alternative calculation method was chosen because,
401 during the required calibration pose, participants struggled to align their wrist axes of rotation with

402 the global coordinate system, either due to their elbow carrying angle or their inability to supinate
403 their forearm the required amount. As such, the model uses the local coordinate system of the
404 forearm plate to calculate wrist and forearm joint angles. Small misplacements of the forearm
405 marker plate, however, can introduce wrist and forearm joint angle calculation errors. To combat
406 this limitation of the *Clusters Only* model, the rater must take care to align the forearm marker
407 plate with the long axis of the forearm when it is affixed to the participant.

408 Although little has been done to validate eye tracking and/or motion capture methods in
409 upper limb movement research, many studies have validated motion capture methods for gait
410 measurements [18]. Gait studies commonly revealed that inconsistencies in motion capture marker
411 placement were a large source of anatomical model errors [18]. The *Clusters Only* model used by
412 GaMA attempts to address this issue as it does not require precise individual marker placement,
413 and has been shown to be more reliable than anatomical models [13]; it does, however, introduce
414 its own variability caused by calibration pose inconsistencies. Gait reliability research has also
415 identified intrinsic participant-to-participant variation within a given population and trial-to-trial
416 variation for a given participant [18], [19]. Such variation could, at least partially, also explain
417 movement behaviour differences between the original and repeated data sets of this study.

418 Limitations

419 Given that this study manipulated numerous experimental factors when comparing the
420 visual and movement measures of two groups of non-disabled participants, it had limitations. It
421 was infeasible for this research to determine the degree to which these factors (different
422 participants, sites, equipment, raters, and task experience opportunities) affected movement
423 measure variation. Additional research on the effects of training could shed more light onto
424 whether or not the amount of practice fully explains the difference in results between the two

425 studies. Although assessment of inter-site/inter-rater reliability of GaMA using the same
426 participant group would also provide valuable information by reducing the effects of inter-
427 participant variability, for this study, a new participant group presented an opportunity to analyze
428 a wider range of normative behaviour; an important consideration when designing an assessment
429 tool to be used to characterize functional impairments.

430 **Conclusions**

431 Overall, the results of the repeated study were similar to those obtained by Valevicius et
432 al. and Lavoie et al. [7]–[9]. Most hand movement, angular joint kinematic, and eye gaze results
433 exhibited by participants in the repeated study were consistent with those observed in the original
434 study. Most significant differences between the results could be explained by the amount of
435 practice that participants in the two studies received, demonstration variations introduced by the
436 rater, and the limitations of the *Clusters Only* kinematics model. Due to its demonstrated
437 reproducibility, it is expected that, in the future, GaMA can serve as a reliable and informative
438 functional assessment tool across different sites and for individuals with sensorimotor impairments
439 in the upper limb.

440

441 **Acknowledgements**

442

443 We thank Quinn Boser, Aida Valevicius and Thomas R. Dawson for assistance with the
444 original data set analysis.

445

446

447 **References**

- 448 [1] C. E. Lang *et al.*, “Deficits in grasp versus reach during acute hemiparesis,” *Exp. Brain Res.*,
449 vol. 166, no. 1, pp. 126–36, 2005.
- 450 [2] A. J. Metzger, A. W. Dromerick, R. J. Holley, and P. S. Lum, “Characterization of
451 compensatory trunk movements during prosthetic upper limb reaching tasks,” *Arch. Phys.*
452 *Med. Rehabil.*, vol. 93, no. 11, pp. 2029–34, 2012.
- 453 [3] S. Mateo, A. Roby-Brami, K. T. Reilly, Y. Rossetti, C. Collet, and G. Rode, “Upper limb
454 kinematics after cervical spinal cord injury: A review,” *J. Neuroeng. Rehabil.*, vol. 12, no.
455 1, p. 9, 2015.
- 456 [4] A. Shumway-Cook and M. H. Woollacott, *Motor control: Translating research into clinical*
457 *practice: Fourth edition*. 2014.
- 458 [5] E. K. Stokes, *Rehabilitation Outcome Measures*. 2011.
- 459 [6] I. M. Velstra, C. S. Ballert, and A. Cieza, “A Systematic Literature Review of Outcome
460 Measures for Upper Extremity Function Using the International Classification of
461 Functioning, Disability, and Health as Reference,” *PM R*, vol. 3, no. 9, pp. 846–60, 2011.
- 462 [7] A. M. Valevicius *et al.*, “Characterization of normative hand movements during two
463 functional upper limb tasks,” *PLoS One*, vol. 13, no. 6, 2018.
- 464 [8] A. M. Valevicius *et al.*, “Characterization of normative angular joint kinematics during two
465 functional upper limb tasks,” *Gait Posture*, vol. 69, pp. 176–186, 2019.
- 466 [9] E. B. Lavoie *et al.*, “Using synchronized eye and motion tracking to determine high-
467 precision eye-movement patterns during object- interaction tasks,” *J. Vis.*, vol. 18, no. 6, p.
468 18, 2018.
- 469 [10] M. Cognolato, M. Atzori, and H. Müller, “Head-mounted eye gaze tracking devices: An
470 overview of modern devices and recent advances,” *J. Rehabil. Assist. Technol. Eng.*, vol. 5,
471 pp. 1–13, 2018.
- 472 [11] P. Slezák and I. Waczulíková, “Reproducibility and repeatability,” *Physiol. Res.*, vol. 60,
473 no. 1, pp. 203–4, 2011.
- 474 [12] O. Pinzone, M. H. Schwartz, P. Thomason, and R. Baker, “The comparison of normative
475 reference data from different gait analysis services,” *Gait Posture*, vol. 40, no. 2, pp. 286–
476 90, 2014.
- 477 [13] Q. A. Boser *et al.*, “Cluster-based upper body marker models for three-dimensional

- 478 kinematic analysis: Comparison with an anatomical model and reliability analysis,” *J.*
479 *Biomech.*, vol. 72, pp. 228–234, 2018.
- 480 [14] S. Y. Schaefer, A. Saba, J. F. Baird, M. B. Kolar, K. Duff, and J. C. Stewart, “Within-
481 session practice effects in the jebsen hand function test (JHFT),” *Am. J. Occup. Ther.*, vol.
482 72, no. 6, pp. 7206345010p1-7206345010p5, 2018.
- 483 [15] W. G. Darling and J. D. Cooke, “Changes in the variability of movement trajectories with
484 practice,” *J. Mot. Behav.*, vol. 19, no. 3, pp. 291–309, 1987.
- 485 [16] L. Shmuelof, J. W. Krakauer, and P. Mazzoni, “How is a motor skill learned? Change and
486 invariance at the levels of task success and trajectory control,” *J. Neurophysiol.*, vol. 108,
487 no. 2, pp. 578–94, 2012.
- 488 [17] J. G. Williams, “Visual Demonstration and Movement Production: Effects of Timing
489 Variations in a Model’s Action,” *Percept. Mot. Skills*, vol. 68, no. 3 Pt 1, pp. 891–6, 2011.
- 490 [18] J. L. McGinley, R. Baker, R. Wolfe, and M. E. Morris, “The reliability of three-dimensional
491 kinematic gait measurements: A systematic review,” *Gait Posture*, vol. 29, no. 3, pp. 360–
492 369, 2009.
- 493 [19] M. H. Schwartz, J. P. Trost, and R. A. Wervey, “Measurement and management of errors
494 in quantitative gait data,” *Gait Posture*, vol. 20, no. 2, pp. 196–203, 2004.
- 495

496 **Supporting Information**

497 **S1 Text.** Detailed statistical analysis.

498

499 **S2 Table.** Phase duration values for the Pasta Box Task and Cup Transfer Task, with significant
500 results of the pairwise comparisons. For the results of the pairwise comparisons (in column p), *
501 indicates a significant p value less than 0.05, ** indicates a p value less than 0.005, and “ns”
502 indicates a p value that is not significant.

503

504 **S3 Table.** Pasta Box Task hand movement values for each movement segment, with significant
505 results of the pairwise comparisons. For the results of the pairwise comparisons (in column p), *
506 indicates a significant p value less than 0.05, ** indicates a p value less than 0.005, and “ns”
507 indicates a p value that is not significant.

508

509 **S4 Table.** Cup Transfer Task hand movement values for each movement segment, with
510 significant results of the pairwise comparisons. For the results of the pairwise comparisons (in
511 column p), * indicates a significant p value less than 0.05, ** indicates a p value less than 0.005,
512 and “ns” indicates a p value that is not significant.

513

514 **S5 Table.** Pasta Box Task eye movement values, with significant results of the pairwise
515 comparisons. For the results of the pairwise comparisons (in column p), * indicates a significant p
516 value less than 0.05 and “ns” indicates a p value that is not significant.

517

518 **S6 Table.** Cup Transfer Task eye movement values, with significant results of the pairwise
519 comparisons. For the results of the pairwise comparisons (in column p), * indicates a significant
520 p value less than 0.05 and “ns” indicates a p value that is not significant.

521

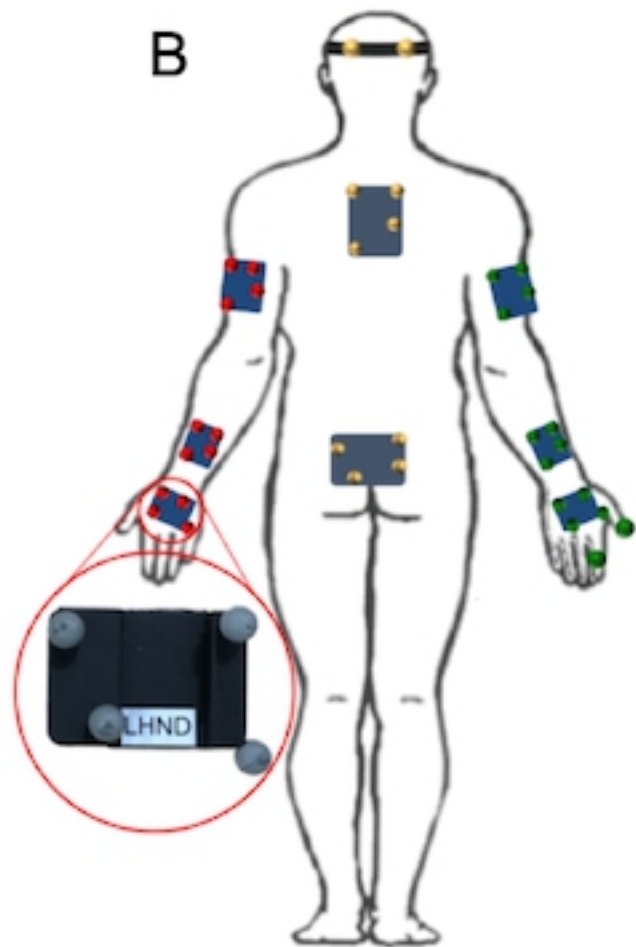
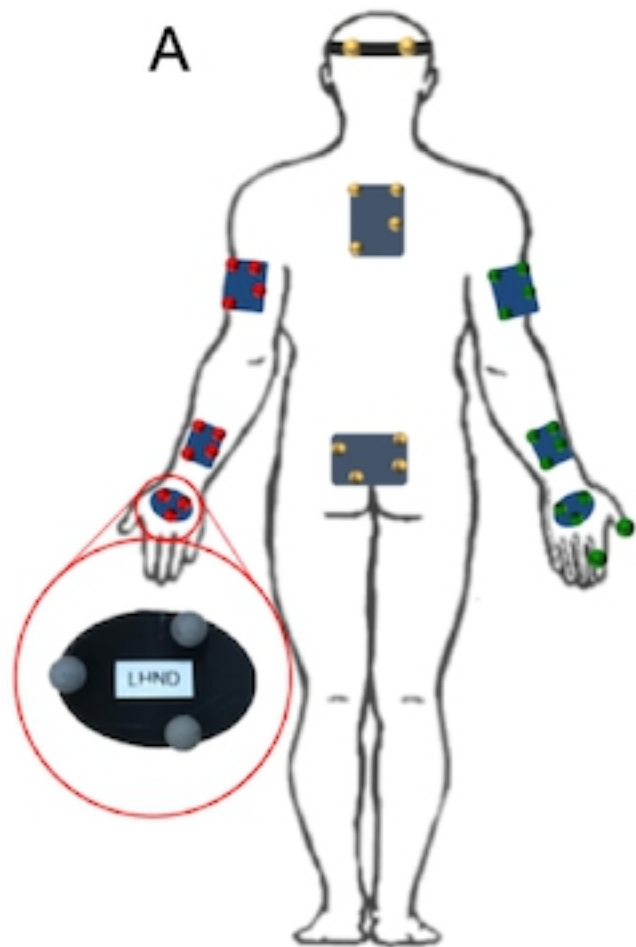


Fig1

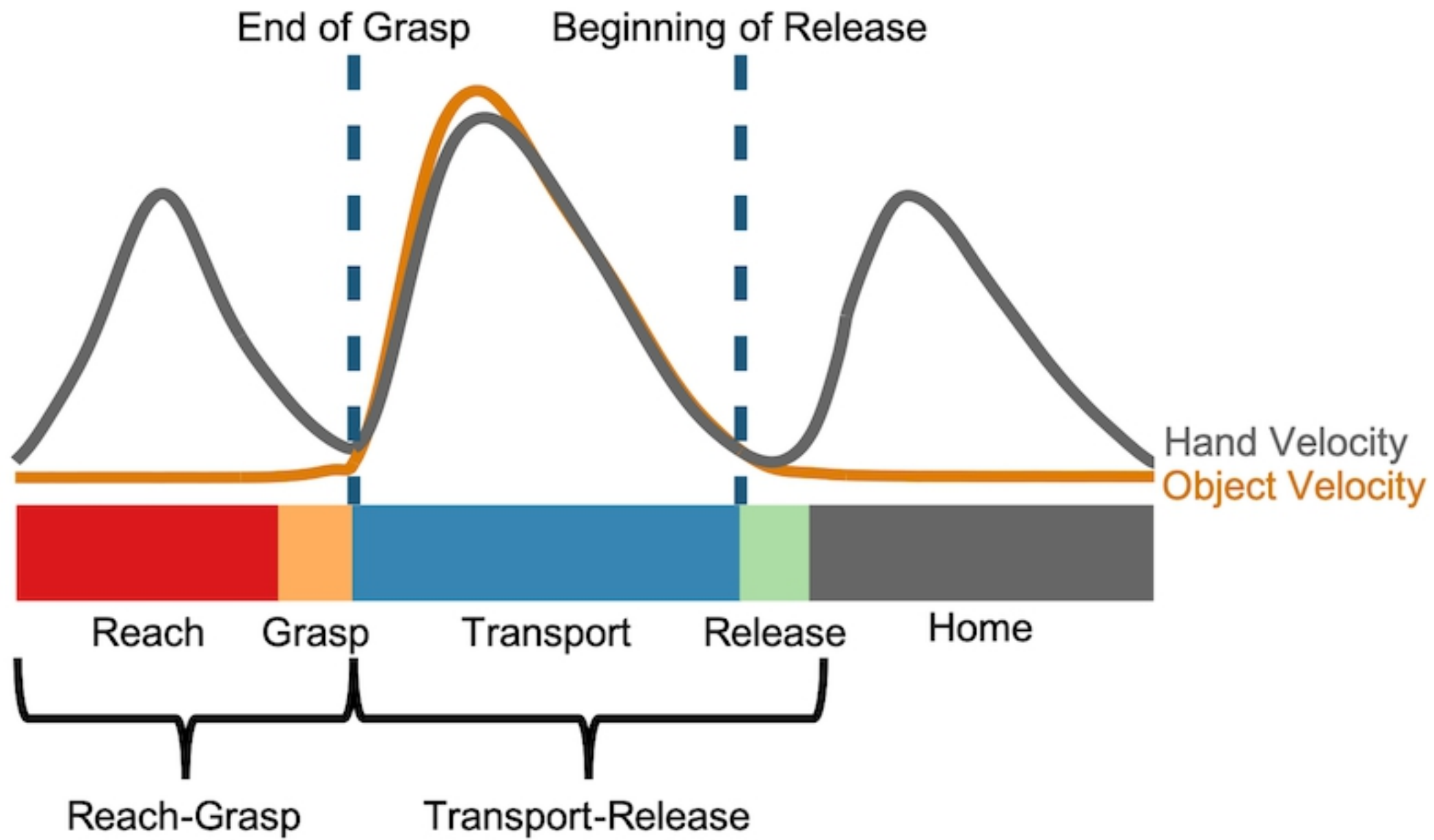


Fig2

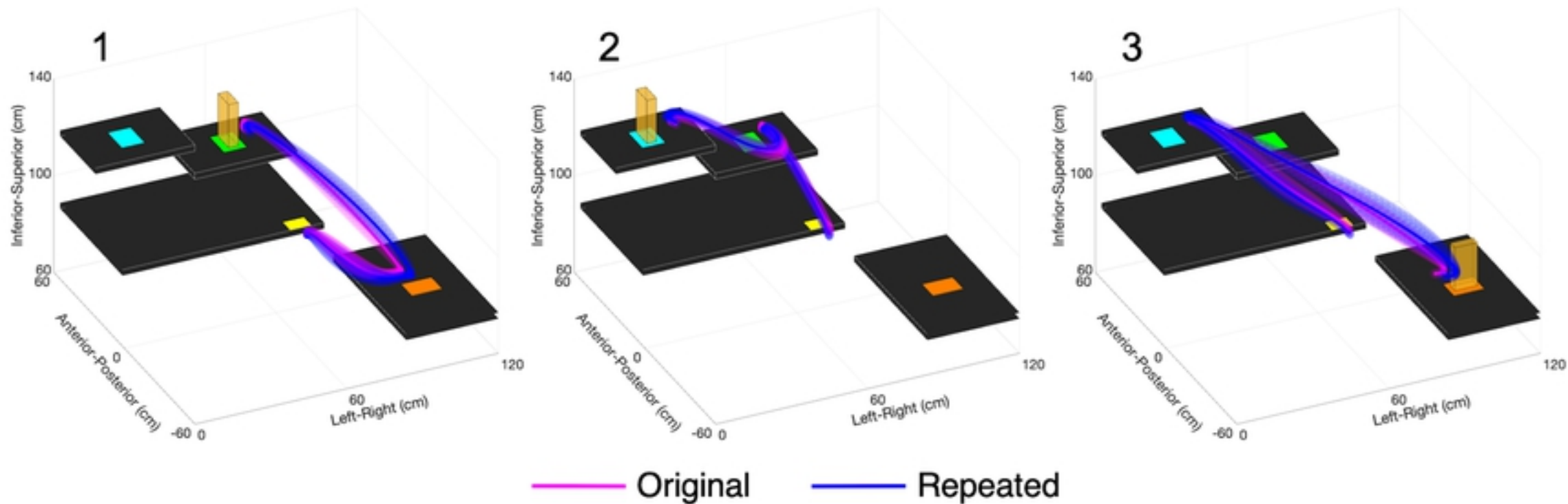


Fig3

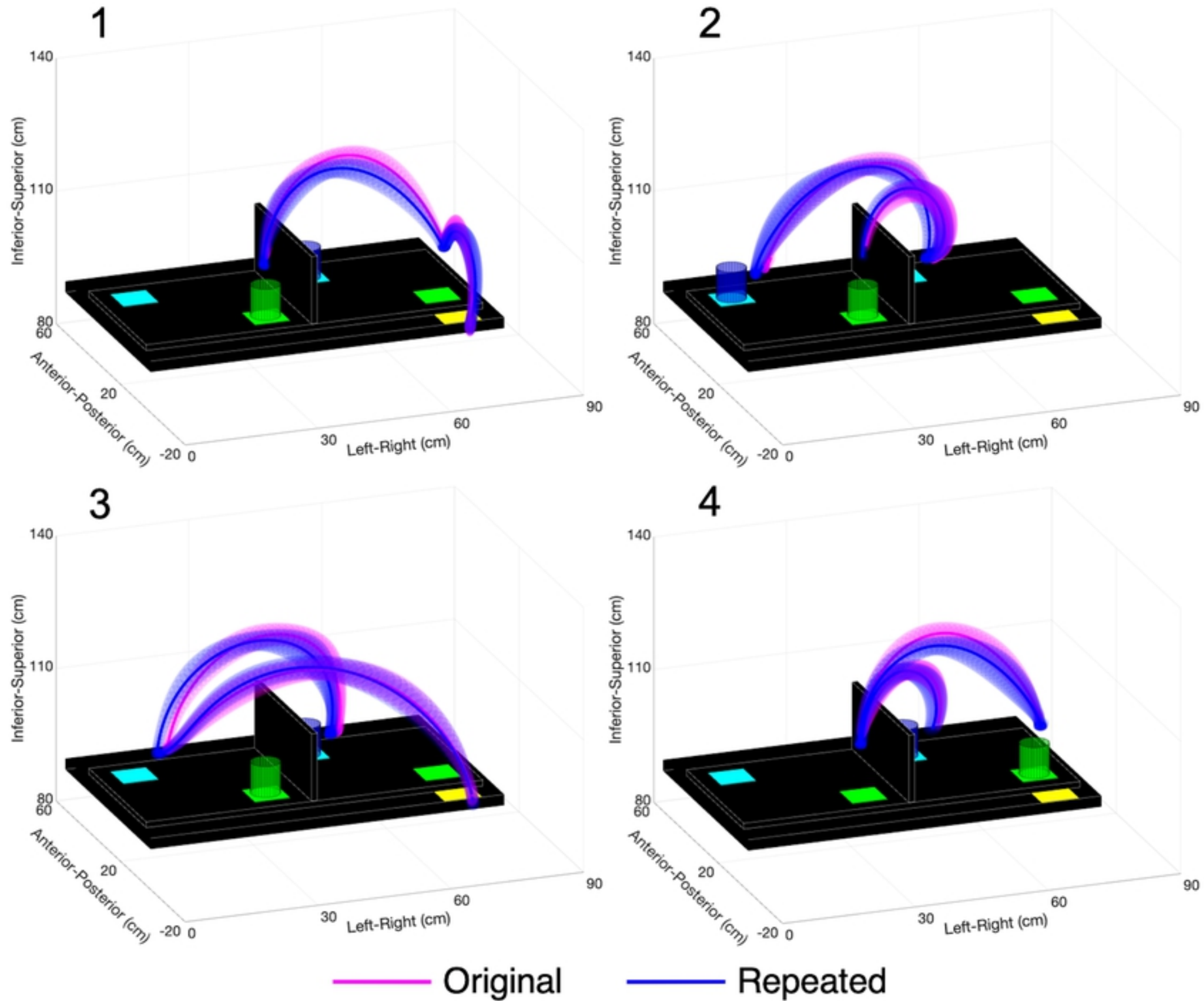


Fig4

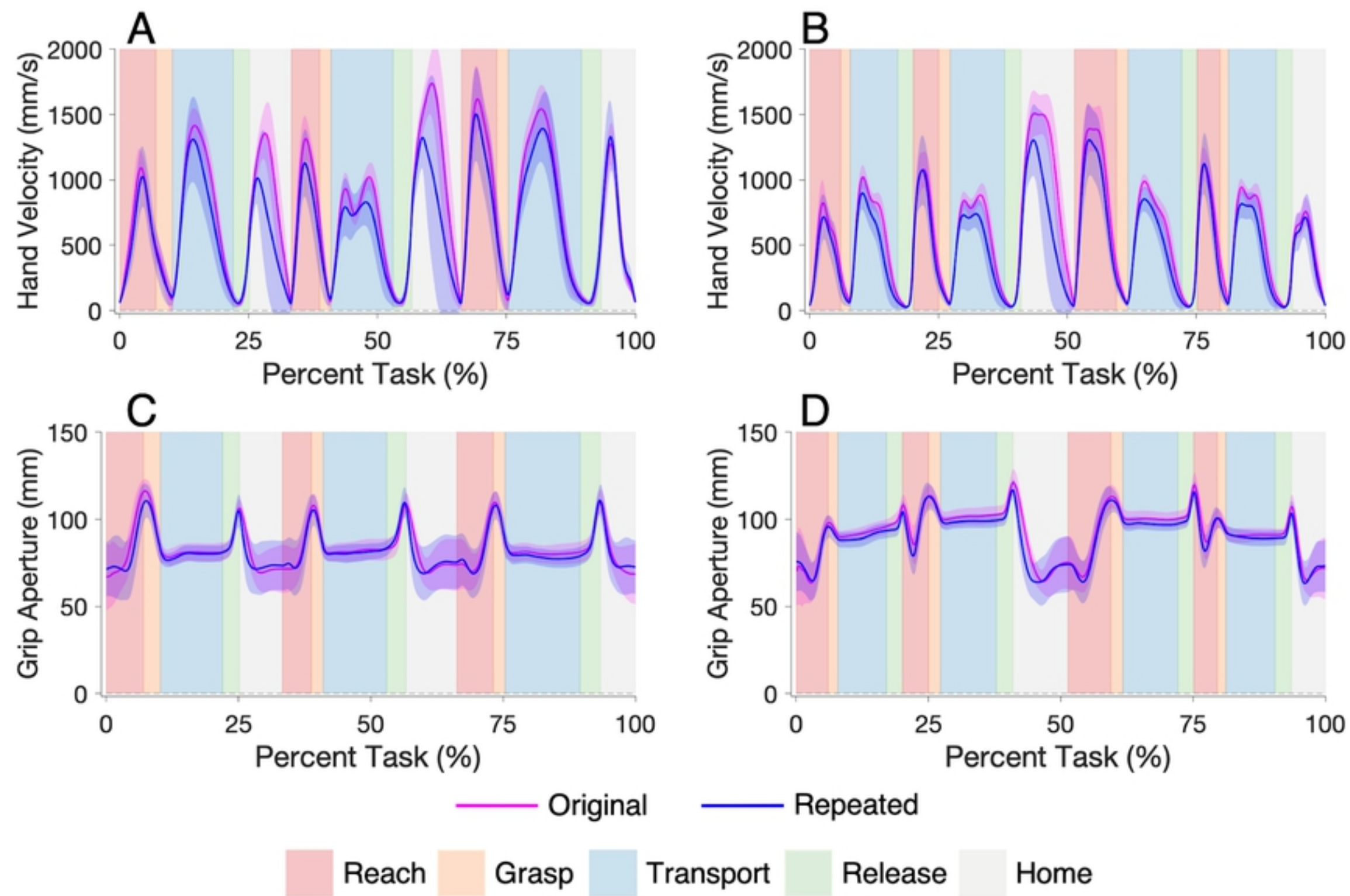


Fig5

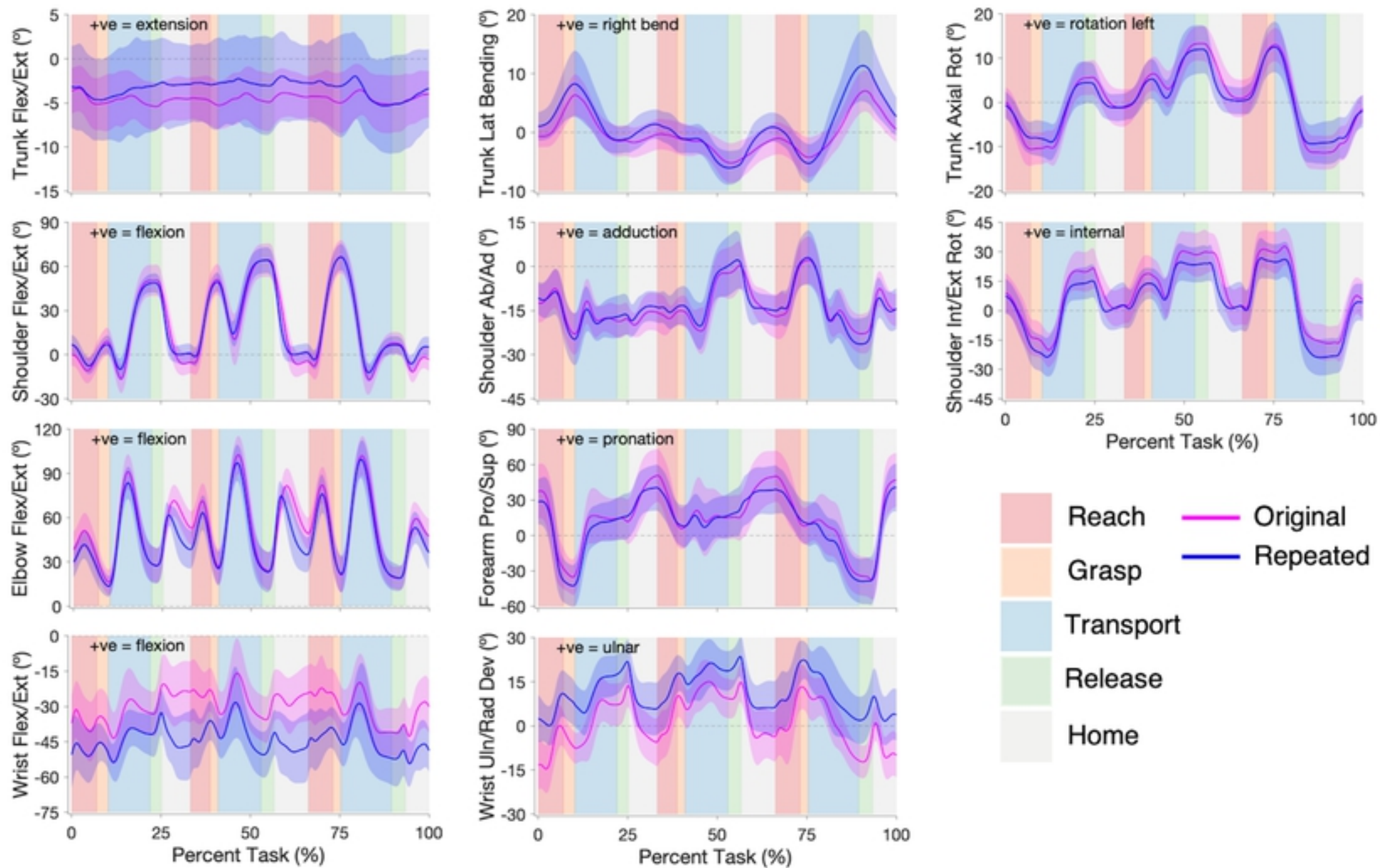


Fig6

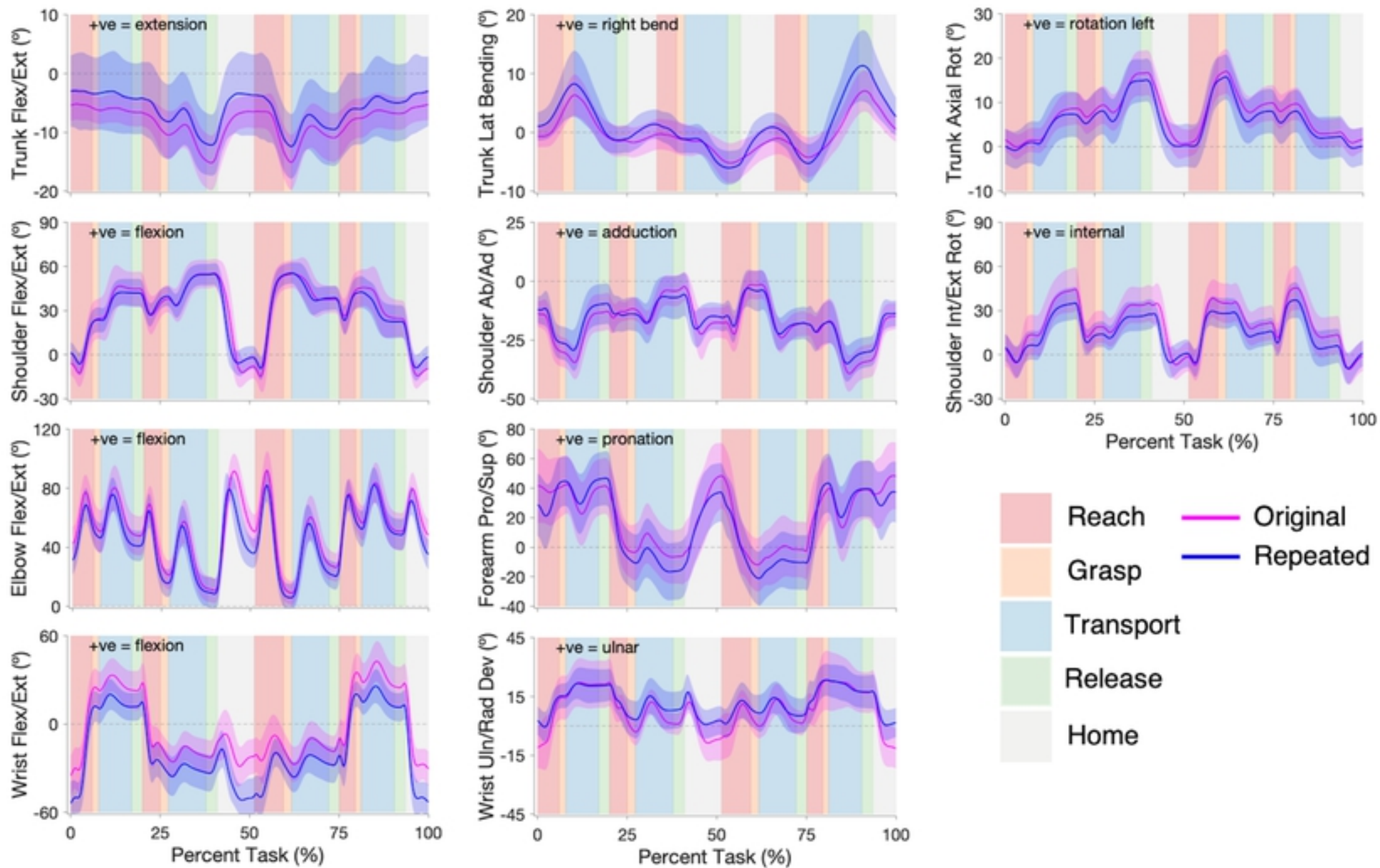


Fig7