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3 **Chronic Stability of Single-Channel Neurophysiological Correlates of Gross and Fine**

4 **Reaching Movements in the Rat**

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17 **Abstract**

18 Following injury to motor cortex, reorganization occurs throughout spared brain regions and is
19 thought to underlie motor recovery. Unfortunately, the standard neurophysiological and
20 neuroanatomical measures of post-lesion plasticity are only indirectly related to observed
21 changes in motor execution. While substantial task-related neural activity has been observed
22 during motor tasks in rodent primary motor cortex and premotor cortex, the long-term stability of
23 these responses in healthy rats is uncertain, limiting the interpretability of longitudinal changes in
24 the specific patterns of neural activity during motor recovery following injury. This study
25 examined the stability of task-related neural activity associated with execution of reaching
26 movements in healthy rodents. Rats were trained to perform a novel reaching task combining a
27 ‘gross’ lever press and a ‘fine’ pellet retrieval. In each animal, two chronic microelectrode arrays
28 were implanted in motor cortex spanning the caudal forelimb area (rodent primary motor cortex)
29 and the rostral forelimb area (rodent premotor cortex). We recorded multiunit spiking and local
30 field potential activity from 10 days to 7-10 weeks post-implantation to characterize the patterns
31 of neural activity observed during each task component and analyzed the consistency of channel-
32 specific task-related neural activity. Task-related changes in neural activity were observed on the
33 majority of channels. While the task-related changes in multi-unit spiking and local field
34 potential spectral power were consistent over several weeks, spectral power changes were more
35 stable, despite the trade-off of decreased spatial and temporal resolution. These results show that
36 rodent primary and premotor cortex are both involved in reaching movements with stable
37 patterns of task-related activity across time, establishing the relevance of the rodent for future
38 studies designed to examine changes in task-related neural activity during recovery from focal
39 cortical lesions.

40 **1. Introduction**

41 An important challenge in neuroscience is determining how the brain controls skilled
42 forelimb movements, a topic that has important implications for motor recovery following brain
43 injuries as well as the development of neuroprosthetic systems. Along with non-human primates,
44 rodents are valuable models for examining the neurophysiological basis of motor control. In
45 particular, rodents can learn to perform a wide variety of motor tasks, including: lever press/pull
46 movements with complex timing [1], 2D center-out joystick movements [2], single-pellet reach-
47 to-grasp food retrievals [3, 4], and even control of brain-computer interface systems with neural
48 activity recorded from their motor cortex [5, 6]. Because of their ability to learn complex and
49 flexible motor behaviors, rodent species have become valuable models for studies of motor
50 control, neural plasticity during motor learning, and neural plasticity during recovery from a
51 focal cortical injury [1, 7-11].

52 In humans and non-human primates, complex volitional movement is a result of the
53 output and coordination of activity in several motor areas within the cortex. While not as
54 extensive as the primate motor system, the wide range of motor behaviors examined in rodents is
55 likely facilitated by the presence of multiple differentiated motor areas within the rodent motor
56 cortex. The rodent motor cortex includes two distinct and interconnected areas in which forelimb
57 movements can be elicited with intracortical microstimulation (ICMS) and which both have
58 direct projections to the spinal cord: the caudal forelimb area (CFA) and the rostral forelimb area
59 (RFA) [12, 13]. Based upon the sensory response properties and overall distribution of afferent
60 and efferent fiber connections, it is thought that CFA is homologous to the primate primary
61 motor cortex while RFA shows similarities to the premotor cortices and supplementary motor
62 areas (SMA) [13, 14]. While CFA and RFA are functionally distinct, both demonstrate

63 substantial task-related neural activity during the performance of a reaching task [7]. In part, this
64 may be due to the dense reciprocal connectivity between the two regions [13], which depending
65 on the relative timing of excitation in each area, allows RFA and CFA to modify the output from
66 the other area [15].

67 In addition to contributing to the ability of rodents to perform complex motor behaviors, the
68 presence of multiple distinct forelimb motor areas has important implications for studies
69 examining neural plasticity in secondary motor regions during recovery from a cortical injury,
70 such as stroke or traumatic brain injury. Following a lesion to CFA, rehabilitative training
71 expands motor maps in RFA, suggesting that RFA plays some role in motor recovery [10].
72 However, the specific changes in the roles of CFA and RFA in controlling motor movements
73 after a cortical injury, and the relevance of these changes to motor recovery, remain unclear.
74 While examining task-related neural activity at different stages of motor recovery may help
75 explain the observed anatomical and motor map changes during behavioral recovery, there are
76 several considerations that need to be addressed prior to examining the specific correlates
77 between changes in task-related patterns of neural activity and motor recovery. First, while
78 single-pellet retrieval tasks involving reach-to-grasp movements are sensitive in measuring
79 motor recovery [9, 10, 16, 17], more substantial lesion models can induce significant and
80 persistent deficits limiting successful task performance for extended periods of time [9].
81 Therefore, a behavioral task with graded levels of difficulty will be required to assess the neural
82 correlates of motor recovery across the full time course of motor recovery. Secondly, while
83 previous studies have shown that chronic neurophysiological recordings can be acquired and
84 used for decoding motor parameters and controlling brain-computer interface systems [5, 6, 11],

85 the stability of the relationship between neural activity and motor movements at the level of
86 individual channels is uncertain in rodent models.

87 This study addresses these limitations through a novel automated complex reaching task
88 combining a ‘gross’ lever press with a ‘fine’ single pellet retrieval within a single trial. By
89 combining these two components into a single task, it is possible to examine motor activity in a
90 single animal while modulating the task requirements in terms of the level of fine motor control
91 of the distal forepaw required to successfully complete the task. Additionally, we examined the
92 stability of task-related neural activity over 7-10 weeks. Each task component was associated
93 with robust task-related neural activity showing that both RFA and CFA are involved in
94 controlling reaching movements. Furthermore, both multi-unit activity and local-field potentials
95 were stable over periods of several weeks showing that these features can be used in future
96 studies examining the longitudinal changes in movement-related neural activity during recovery
97 from a cortical injury.

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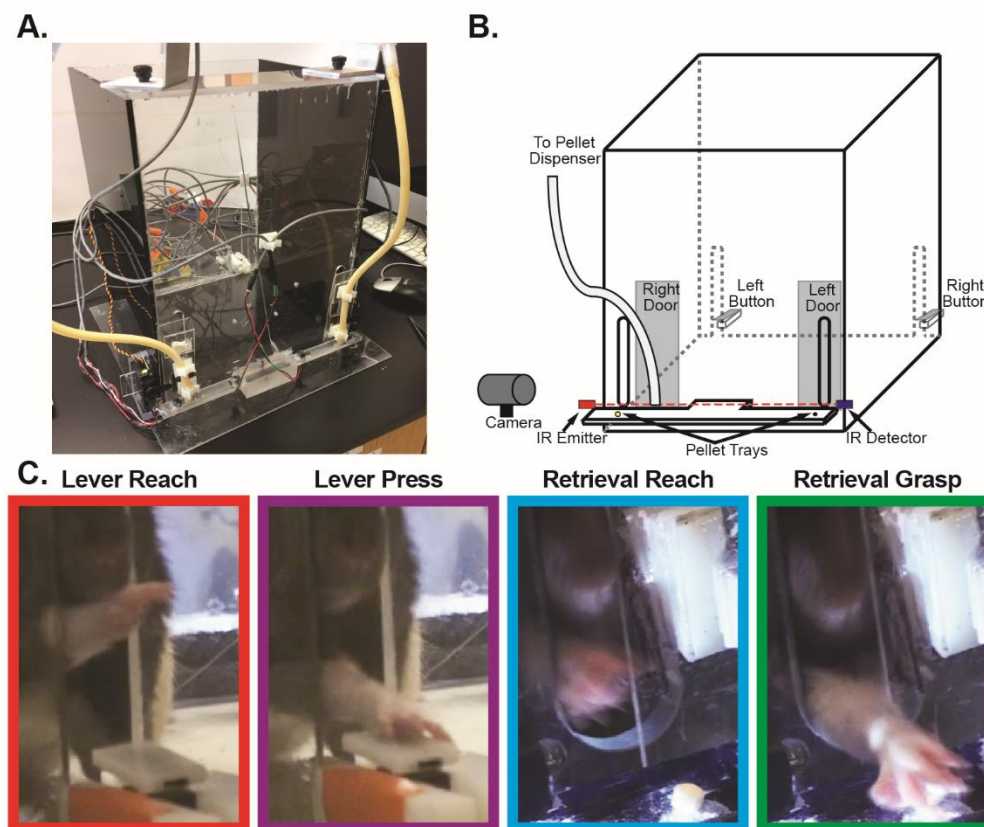
99 **2. Materials and Methods**

100 All procedures were approved by the University of Kansas Medical Center Institutional
101 Animal Care and Use Committee in compliance with *The Guide for the Care and Use of*
102 *Laboratory Animals* (Eighth Edition, The National Academies Press, 2011). To examine the
103 neural correlates of gross and fine reaching movements, five Long-Evans rats (*Rattus*
104 *norvegicus*) were trained to perform a novel complex reaching task utilizing a custom-designed
105 automated behavior box while neural recordings were made from RFA and CFA.

106 **2.1 Custom Behavior Box**

107 A custom automated behavior box was developed that combined a lever press and skilled
108 pellet retrieval into a single trial (Figure 1). The behavior box was constructed from acrylic
109 sheets (12" x 12" x 18" tall, 1/4" thickness). Each box had 15 mm wide vertical slits cut at 30 mm
110 from the edge of the sides of both the front and back panels. A lever with an operating force of
111 20 g was placed directly behind each slit in the back panel with the paddle of the lever centered
112 in the middle of the slit at a height of 28 mm, 23 mm behind the inside edge of the box. The
113 position of the lever could be adjusted, allowing the lever to pass through the slit for temporary
114 placement inside of the box to aid in the initial shaping of behavior. A shelf was placed spanning
115 the entire width of the front of the box at a height of 30 mm. In front of the vertical slit, this shelf
116 began 16 mm outside of the inner edge of the box and extended to 48 mm in front of the inner
117 edge of the box, leaving a gap between the outer edge of the box and the front edge of the shelf.
118 A depression (4 mm diameter, 1 mm depth) was made on the shelf 24 mm outside of the inside
119 edge of the box and aligned to the inside edge of the vertical slit to ensure the consistent position
120 of the food pellet in each trial. An acrylic door was placed in front of each slit in the front panel
121 and was controlled by a linear actuator (Actuonix, Victoria, BC), controlling access to the shelf
122 at the front of the box. Two infrared beam break sensors provided feedback regarding the
123 position of the forepaw to aid in segmenting rodent behavior and switching between task periods.
124 One infrared beam was placed across the front of the box and a second infrared beam was
125 aligned vertically through the pellet location. Levers at the back corners of the box were coupled
126 with the door at the diagonally opposite corner, forcing rats to use the same forepaw for each
127 task component. By aligning the height and distance of the lever at the back of the box with the
128 pellet tray at the front of the box, both the lever press and pellet retrieval required similar
129 ballistic reaching movements with differing requirements for fine movements of the distal

130 forepaw and sensorimotor integration. Task transitions were controlled by an Arduino
131 microcontroller (Arduino Uno, Arduino, Ivrea, Italy) run by a custom-made MATLAB (Version
132 R2017a, MathWorks, Natick, MA) executable function. A webcam was attached to the side wall,
133 perpendicular to the front of the box, and aligned to image across the length of the shelf. Video
134 from the webcam was acquired by the MATLAB executable code at 25 fps to capture reaches to
135 the pellet tray and to control pellet dispensing. The webcam could be positioned at either side of
136 the box to enable testing rats with either a right or left forepaw preference. Two pellet dispensers
137 (Med Associates, Inc., Fairfax, VT) were used to dispense pellets to either side of the pellet
138 shelf. Finally, an LED light was used to allow us to synchronize neural activity, behavioral
139 performance, and videos recorded from additional external video camera.



140

141 **Figure 1. Complex Reaching Task.** To evaluate the neurophysiological correlates of both gross and fine
142 reaching movements within individual animals, we designed a novel, automated behavior box (**A**). **B**. At
143 the beginning of each trial rats were required to use their preferred forearm to depress a lever placed

144 outside an opening at the back corner of the box, causing a door at the front of the box in the corner
145 diagonally opposite from the lever to open, providing access to a food pellet placed on a ledge outside the
146 box. After transitioning to the door, rats reached through an opening to grasp and retrieve the food pellet
147 reward. After detecting an attempt to retrieve the pellet via an infrared beam across the front of the box,
148 the door was automatically closed, preventing repeated retrieval attempts. **C.** To examine the
149 neurophysiological correlates of task performance, video recordings were used to identify the time points
150 for the reach-to-button onset, button press, reach-to-pellet onset, and pellet grasp onset within each trial.
151

152 ***2.2 Task Structure***

153 Prior to the beginning of each trial, both doors were closed, and a pellet was dispensed to
154 the side of the pellet shelf corresponding to the rat's preferred forelimb for pellet retrieval.
155 Initially, rats were required to reach through the back of the box and depress the lever on the side
156 of the box corresponding to their preferred forelimb. Upon depressing the lever, the door at the
157 slit diagonally opposite the lever was opened, providing access to the previously dispensed food
158 pellet on the shelf. After detecting a completed reach through the front of the box, as indicated
159 by the infrared beam break being broken and then subsequently unbroken, the door was closed to
160 limit secondary reaching attempts. If an attempt to retrieve the pellet was not made within 20
161 seconds, the trial was aborted.

162 ***2.3 Behavioral Training***

163 Each rat went through a procedure to gradually shape their behavior to complete the full
164 task. Initially, rats were placed in a non-automated box with a single slit cut in the center of the
165 front panel. Rats were allowed free access to food pellets through this opening to learn to retrieve
166 food pellets and determine forepaw preference. Pellets were placed in the center of the opening
167 on a shelf placed across the front of the box at a height of 30 mm. Once rats began consistently
168 retrieving pellets, their preferred forelimb was determined as the paw that was used on the
169 majority of retrievals. Next, rats were introduced to the automated behavior box and allowed to
170 retrieve pellets through the opening in the front of the box corresponding to their preferred

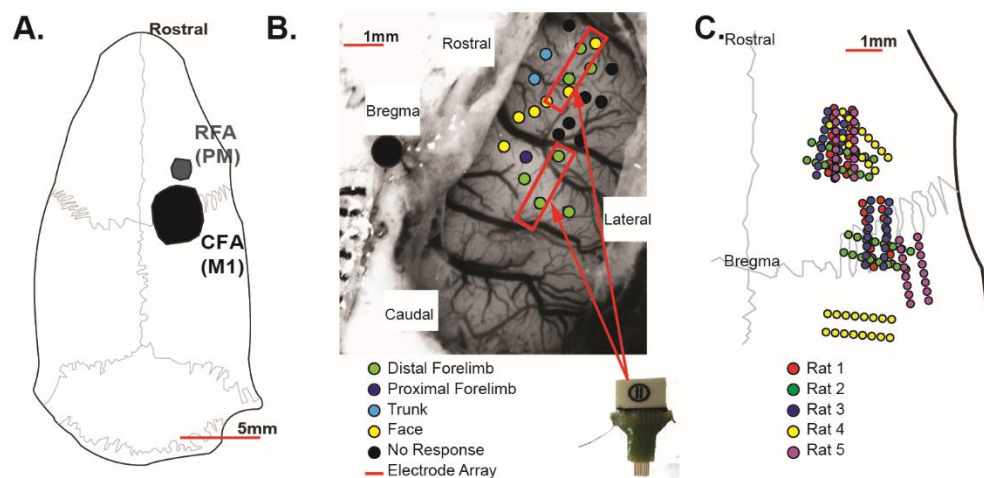
171 forepaw. The door was closed after each retrieval attempt to familiarize rats with the door
172 mechanism. The shelf in the automated behavior box had a gap between the edge of the shelf and
173 the outer edge of the box which reinforced the requirement that the rats fully grasp each pellet,
174 and not retrieve pellets by simply dragging them into the box. After successfully retrieving at
175 least 50% of pellets, the lever press was incorporated into the training. Initially the front edge of
176 the lever paddle was positioned inside the box and rats were cued to interact with the lever via
177 auditory cues and food placed near the lever. A food pellet was dropped into the box by the
178 secondary pellet dispenser each time the lever was depressed. This immediate reward served to
179 reinforce the lever press. After beginning to depress the lever, the lever was gradually moved to
180 its position for the full task, 23 mm outside the inside wall of the box. Next, we paired the lever
181 press to the pellet retrieval. After each lever press, rats were cued to cross to the opposite corner
182 of the box using auditory cues (tapping at the front corner of the box). After beginning to
183 combine the lever press and pellet retrieval, the secondary reward received for the initial lever
184 press was gradually extinguished to avoid any chewing artifact during the trial period. Finally,
185 rats were trained until they successfully retrieved at least 50% of pellets in three consecutive
186 training sessions with 25 trials per session. While total training time was variable, most rats
187 completed each training step in 1-2 weeks and therefore could learn to adequately perform the
188 entire task in 5-10 weeks with 30-minute long training sessions 3-5 days per week (mean \pm SE =
189 33.6 ± 2.75 sessions). Following training, task performance was maintained with 2-3 training
190 sessions per week until surgical procedures could be completed.

191 ***2.4 Surgical Procedures***

192 Once rats achieved a threshold criterion of 50% successful retrievals on the full task in
193 three consecutive sessions, we implanted chronic microwire electrode arrays into RFA and CFA.

194 At the time of surgery, rats were 23-35 weeks old. Rats were initially anesthetized with
195 isoflurane followed by injections of ketamine (80-100mg/kg) intraperitoneally and xylazine (5-
196 10 mg/kg) intramuscularly. Rats were also given a preoperative dose of penicillin (45,000 IU
197 subcutaneously) to limit the risk of infection. For the duration of the procedure, anesthetic state
198 was confirmed by checking for the presence of a pinch reflex and corneal reflex, and a surgical
199 level of anesthesia was maintained with supplemental injections of ketamine intramuscularly as
200 necessary (10-20 mg/hr). Rats were placed in a stereotaxic frame and an incision was made along
201 the midline of the scalp and the temporalis muscle was resected. A laminectomy was performed
202 to reduce cortical swelling during the procedure. A craniectomy was then made over the
203 sensorimotor cortex of the hemisphere contralateral to the preferred forelimb and the dura was
204 retracted. Two 16-channel tungsten alloy micro-wire arrays with electrode diameters of 50 μm
205 (Tucker-Davis Technologies, Alachua, FL) were implanted in each rat. Arrays were organized in
206 a 2x8 grid with 250 μm spacing between electrodes and 500 μm spacing between rows. A silver
207 wire from the probe was attached to a 00-80 stainless steel skull screw to act as a ground. The
208 first electrode array was implanted into RFA with the second electrode array targeted to CFA as
209 allowed by the size and orientation of the craniectomy and the rodent-specific pattern of
210 vasculature within the craniectomy window. In three rats, the location of CFA and RFA were
211 confirmed using ICMS mapping procedures as described previously [9]. In the remaining two
212 rats, stereotaxic coordinates were used for RFA (3.5 mm anterior to bregma, 2.5 mm lateral to
213 bregma) and CFA (0.5 mm anterior to bregma, 3.5 mm lateral to bregma) [9, 10, 18]. Each
214 electrode array was implanted to a depth of approximately 1500 μm using a motorized
215 micropositioner (Narishige International USA, Inc., Amityville, NY). An example ICMS map
216 used to localize the implant locations is shown in Figure 2B. Electrode locations for all rats

217 relative to skull landmarks are plotted in Figure 2C. The electrode locations in RFA overlap
218 considerably across rats with some variability in the location of the CFA electrode arrays due to
219 the limitations placed by the size of the craniectomy and vasculature pattern. After inserting the
220 electrodes, the cortex was covered with a silicone elastomer (Kwik-Cast, World Precision
221 Instruments, Sarasota, FL), a head cap was constructed from dental acrylic *in situ*, and the scalp
222 was sutured around the head cap. Following the surgery, rats were given penicillin (45,000 IU
223 subcutaneously) to limit the risk of infection. Four doses of buprenorphine (0.05-0.1 mg/kg
224 subcutaneously) and acetaminophen (80-100 mg/kg orally) were given over the next 48 hours as
225 analgesics. All rats were allowed to recover for 10-20 days prior to beginning neurophysiological
226 recordings.



227

228 **Figure 2. Chronic Microelectrode Implants.** **A.** The rodent motor system consists of the caudal
229 forelimb area (CFA), a homologue of M1, as well as a secondary rostral forelimb area (RFA), a
230 homologue of premotor cortex. **B.** Sixteen-channel chronic microwire electrode arrays were implanted
231 into each rat with one array placed in RFA and a second array implanted into CFA. Intracortical
232 microstimulation mapping was used to confirm the locations of RFA and CFA in three rodents with
233 stereotaxic coordinates used to determine implant locations in the remaining rats. **C.** Approximate implant
234 locations relative to skull landmarks were determined from intraoperative photographs. With respect to
235 stereotaxic coordinates, the location of the electrode arrays implanted into RFA was very consistent
236 across rats with more variability in the locations of the CFA arrays due to the variable locations and
237 orientations of blood vessels relative to the craniectomy opening.

238

239 **2.5 Neurophysiological Recordings**

240 Following the microelectrode implantation surgery, rats were given 10-20 days to recover
241 from surgery. After the recovery period, we collected neurophysiological recordings while rats
242 performed the reaching task in the automated behavior box. Rats performed the task 2-3 times
243 per week for up to 10 weeks post-implant (mean \pm SE = 14.6 ± 0.68 sessions). On recording
244 days, rats were briefly anesthetized with isoflurane to ease connection of a recording headstage
245 to each microelectrode array. The headstages, which performed amplification and digitization via
246 an on-board amplifier chip (RHD 2132, Intan Technologies, Los Angeles, CA), were connected
247 through a slip ring commutator (MC573, MOFLON TECHNOLOGY, Shenzhen, China) to an
248 interface board (RHD2000, Intan Technologies, Los Angeles, CA) connected via USB to a PC
249 computer. Neural activity was recorded at 20 kHz while rodents were in the automated behavior
250 box performing the reaching tasks. For each session, signals were recorded while rats performed
251 45 trials or until 45 minutes had elapsed. Occasionally, recording sessions were truncated due to
252 the headstages becoming unplugged prior to session completion.

253 ***2.6 Behavioral Scoring***

254 During training sessions, time stamps of each lever press and infrared beam break were
255 recorded by the recording amplifier as digital inputs. Videos of the reach-to-pellet were captured
256 by a webcam at 25 fps and were synchronized to the neural recordings by the MATLAB
257 interface. Additional video recordings were also made using an external digital video camera
258 (Sony HDR-SR11, Sony Corporation, Tokyo, Japan) at 30 fps. The external camera was either
259 positioned in front of the box to capture a higher resolution view of the reach to the food pellet,
260 behind the lever to capture the lever press, or above the box to capture the rat's movement
261 throughout the box. This orientation alternated on each recording day. External videos were
262 synchronized by capturing an LED light in the field of view that was controlled by the MATLAB

263 interface and simultaneously recorded by the recording amplifier. Behavioral time points were
264 co-registered by visually scoring the video recordings. As shown in Figure 1C, times for the
265 reach to the lever, the lever press, the reach to the food pellet, and the grasp of the food pellet
266 were identified. The times for the reach to the lever and reach to the food pellet were both
267 defined as the frame in which the first forward movement of the paw to begin a reach was
268 observed; the lever press was identified as the time that the lever circuit was electrically closed;
269 and the grasp was defined as the first video frame where flexion of the digits at the end of the
270 reach was observed. Successful trials were defined as trials in which the rat successfully
271 retrieved the pellet on the first reach attempt to avoid potential confounding of neural activity
272 related to an unsuccessful initial retrieval attempt followed by a successful second attempt. The
273 reach to the food pellet and grasp were scored in each session using the webcam videos and
274 confirmed using the external camera videos when available. While lever press time stamps could
275 be identified in each recording, the reach to the lever was only identifiable in the subset of
276 sessions with the external camera placed at the back of the box.

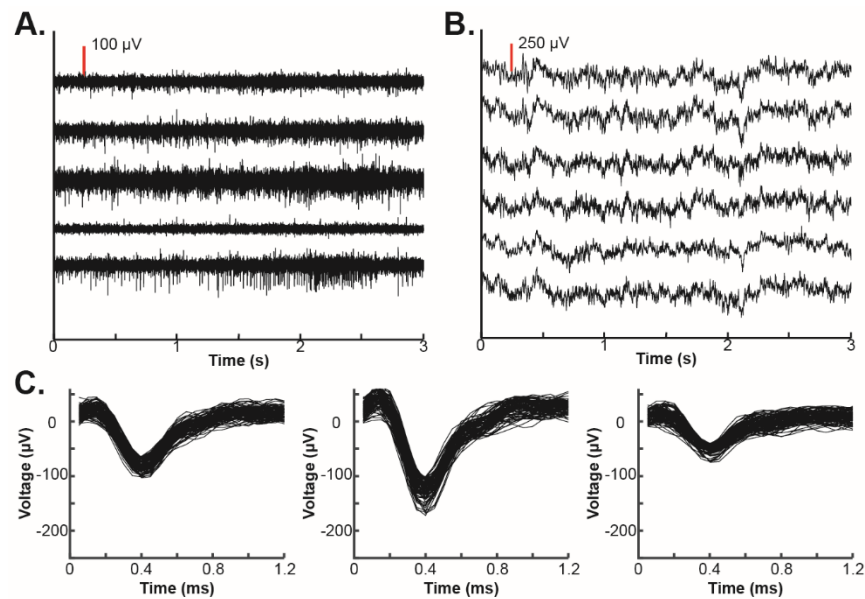
277 *2.7 Data Analysis*

278 Initially, raw local field potentials from all recordings were bandpass filtered from 2Hz-
279 200Hz and visually screened to identify noisy or broken channels to exclude from all further
280 analyses. Data was then processed to examine both multi-unit firing activity and local field
281 potential (LFP) spectral power changes as described below.

282 *2.7.1 Multi-Unit Firing*

283 To determine multi-unit spiking activity, signals were re-referenced to the common
284 average of the non-noisy channels separately for each microelectrode array. Next, signals were
285 band pass filtered from 300-3000Hz using an 8th order elliptic filter. Potential spikes were

286 identified based upon the more stringent criteria of either a fixed threshold of -50 uV or a
287 variable monopolar threshold based upon the background amplitude of the signal for each
288 channel [19]. Detected spikes were automatically clustered using an automated
289 superparamagnetic clustering algorithm [19]. Manual spike sorting was then performed to
290 eliminate non-physiological clusters. Figure 3A shows an example of bandpass filtered data from
291 an exemplar recording session with a number of spike profiles. Figure 3C shows several spike
292 profiles from an exemplar channel using the same recording as the traces shown in Figure 3A.
293 Because we expected that it would be difficult to track single unit profiles across days, spike
294 times from each cluster on a given channel were combined to yield the multi-unit activity for a
295 given channel. Multi-unit firing rates were estimated by convolving a Gaussian waveform of one
296 second duration and a standard deviation of 100 ms with the multi-unit spike times. To examine
297 changes relative to baseline, 1000 random one-second long time windows, excluding all trial
298 windows, were identified. The firing rate during these random time periods was estimated by
299 convolving the multi-unit spike times with a Gaussian waveform as described above and the
300 mean random firing rate was calculated by taking the mean across all time points from each
301 random window. Finally, the firing rate during the recording was normalized by dividing the
302 estimated firing rate by the mean random firing rate and log-transforming. The log-transform
303 was used to normalize the firing rate with increases relative to baseline indicated by positive
304 values and decreases relative to baseline indicated by negative values.



305

306 **Figure 3. Electrophysiological Analyses.** Multi-unit firing and local-field potential (LFP) activity were
307 examined in each recording session. **A.** To examine multi-unit firing, signals were re-referenced to the
308 common average and band-pass filtered between 300Hz and 3000Hz. Each trace shows data filtered for
309 multi-unit activity and aligned to the same time point from randomly selected channels in a single rat. A
310 scale of 100 µV is indicated by the vertical red line. **B.** LFP activity was visualized by filtering between
311 5Hz and 300Hz after re-referencing to the common average. Each trace shows data filtered for LFP
312 activity and aligned to the same time point from randomly selected channels in a single rat. A scale of 250
313 µV is indicated by the vertical red line. **C.** To examine multi-unit firing, action potentials were detected
314 using a superparamagnetic clustering algorithm followed by manual sorting to eliminate noisy clusters.
315 Plots show 100 example spikes detected from 3 profiles isolated on a single channel. Following spike
316 sorting, multi-unit activity was generated by combining all single-unit clusters from each individual
317 channel.

318 2.7.2 LFP Spectral Power Estimation

319 Task-related changes in the LFP spectral power were also examined. Raw signals were
320 low-pass filtered at 400 Hz and decimated to a sampling rate of 1000Hz. All harmonics of the
321 60Hz power line noise below the Nyquist frequency were removed using an 8th-order Chebyshev
322 notch filter. Signals were then re-referenced to the common average of all channels with
323 neurophysiological signals separately for each microelectrode array. Examples of the raw LFP
324 signals are shown in Figure 3B. The maximum entropy method, an autoregressive method of
325 spectral estimation, was used to estimate spectral power [20]. A model order of 50 was selected

326 and spectral power was estimated in 2 Hz frequency bins with bin centers ranging from 2 Hz to
327 200 Hz. Spectral power was calculated in 250 ms windows with shifts of 50 ms between
328 windows to examine temporal changes. As with the multi-unit firing rate, 1000 random one-
329 second long time windows, excluding all trial periods, were identified, and the spectral power
330 was estimated in each window. Spectral power estimates were normalized by log-transformation
331 and were then z-scored by subtracting the mean and dividing by the standard deviation of the
332 frequency-specific spectral power estimated from the random time windows. Positive values
333 indicated increases in spectral power at a given frequency relative to its baseline, and negative
334 values indicated decreases in spectral power relative to baseline. Because the high-gamma band
335 (70-105Hz) of the LFP signal has been found to represent localized activity that is strongly
336 correlated with asynchronous spiking [21], the average high-gamma band power was found by
337 averaging the z-scored spectral power for all frequency bins with centers between 70Hz and
338 105Hz.

339 ***2.8 Single-Day Characterization of Task-Related Neural Activity***

340 Initially, the patterns of task-related neural activity during the two components of the task
341 (lever press and pellet retrieval) were characterized using a single exemplar session. For the
342 initial characterization of task-related neural activity, recordings were excluded for each rat until
343 at least one session in which the rat performed 36 trials (80% of the daily goal) was acquired. To
344 allow for examination of both components of the task, the next recording session with the
345 external camera at the back of the box in which each rat performed at least 36 trials (80% of the
346 daily goal) was used for the single-day characterization of task-related neural activity.

347 For each trial within the exemplar session, several behavioral time points were identified
348 for further analysis. Sessions with the external camera behind the box allowed us to use the

349 external camera recordings to identify the onset of reaching movements towards the lever and the
350 lever timing to identify the downward movement used to press the lever, while the webcam at
351 the front of the box was used to identify the onset of reaching movements to the food pellet and
352 the onset of grasping movements. After identifying these time points for each trial, the task-
353 related multi-unit firing rates and spectral power were examined as described below.

354 For each task event considered, a period from 1 s before to 1 s after the event was
355 examined, matching the time of peak activations observed in previous studies of rodent reaching
356 tasks [7]. For the lever press, task-related neural activity recorded from each channel was aligned
357 either to the reach onset or lever press based upon whether the greatest absolute average depth-
358 of-modulation was found by aligning neural activity to the onset of the reach towards the lever or
359 to the lever press itself. Because the neural activity was normalized and log-transformed, signals
360 were normally distributed with increases in neural activity relative to baseline indicated by
361 positive values and decreases in neural activity indicated by negative values. Therefore, the
362 depth-of-modulation was defined as the absolute value of the task-aligned neural activity.
363 Similarly, for the pellet retrieval, each channel was aligned to the onset of the reach or onset of
364 the grasp based upon whether the greatest absolute depth-of modulation was found by aligning
365 neural activity to either the onset of the reach towards the pellet or the onset of the grasping
366 movement. For the lever press, each channel was then classified as statistically significantly
367 modulated and reach-related, statistically significantly modulated and press-related, or not
368 significantly modulated. Similarly, for the pellet retrieval, each channel was also classified as
369 significantly modulated and reach-related, significantly modulated and grasp-related, or not
370 modulated. The statistical significance of each channel and task component's classification was
371 calculated to determine if the peak task-related neural activity was significantly different from

372 chance using an independent samples t-test comparing the distribution of task-related neural
373 activity at the time of the peak absolute depth-of-modulation to a randomly selected distribution
374 of neural activity. The random distribution was derived by collecting the neural activity from
375 1000 random time points collected from outside of any trial period. A significance level of
376 $p < 0.05$ was used to define significance with Bonferroni correction for the total number of
377 comparisons tested across channels and task periods. Each channel with spike profiles identified
378 was classified as described above. Each channel was separately classified based upon whether
379 there were statistically significant increases or decreases of the high-gamma band spectral power
380 during either the lever press or the pellet retrieval. As with the multi-unit firing, the high-gamma
381 band was also used to give each channel two classifications: first, each channel was classified as
382 statistically significantly modulated and reach-related, statistically significantly modulated and
383 press-related, or not significantly modulated for the lever press, and second, each channel was
384 classified as statistically significantly modulated and reach-related, statistically significantly
385 modulated and grasp-related, or not significantly modulated for the pellet retrieval.

386 ***2.9 Chronic Stability of Task-Related Neural Activity***

387 Finally, we sought to examine the chronic stability of task-related neural activity in RFA
388 and CFA. Because videos capturing the lever press were not captured for every recording day
389 due to rotating the position of the external video camera, the analysis of the stability of task-
390 related neural activity was limited to the pellet retrieval component of the task. For each channel
391 with a statistically significant reach or grasp-related change in multi-unit firing rate in the
392 exemplar recording session described above, trials from each recording day were aligned to the
393 reach onset or grasp onset based upon the initial classification from the exemplar recording day.
394 Next, the daily average multi-unit firing rate was calculated for each channel. A global average

395 time course of task-aligned multi-unit firing rate was calculated by averaging the firing rate from
396 all trials across all recording days. Finally, for each channel and recording day, the correlation
397 coefficient (Pearson's r) was calculated between the global and daily averaged firing rate. The
398 consistency of task-related high-gamma band power changes was assessed using the same
399 procedure for all channels with statistically significant reach or grasp-related changes in high-
400 gamma band spectral power in the exemplar session. We then compared the inter-day
401 consistency of single-channel task-related multi-unit firing rate changes with the inter-day
402 consistency of task-related high gamma band power changes using a Wilcoxon rank sum test
403 comparing the distribution of correlation values for the two signal types across all rats, channels,
404 and days.

405 **3. Results**

406 *3.1 Rat Characteristics and Behavioral Performance*

407 All rats learned to perform the task with successful retrievals on 60-80% of trials. Table 1
408 summarizes the overall behavioral performance of each rat. Each rat continued to perform the
409 task with accuracies above 50% success rates, indicating that the microelectrode implantation did
410 not impair the ability to perform the task (Exemplar Sessions: mean \pm SE = 67.4% \pm 4.0%;
411 Overall: mean \pm SE = 63.5% \pm 1.4%). While these performance scores are lower than reported in
412 previous studies of pellet retrieval in rats [9, 10, 17], the gap between the shelf and box required
413 rats to fully lift each pellet and the door restricted repeated reaching attempts, increasing the
414 difficulty of the task. Additionally, to better isolate task-related neural activity, successful trials
415 were defined as trials in which the rat successfully retrieved the pellet on the first attempt. The
416 accuracies observed were similar to other studies with similar placements of pellets on a
417 pedestal, increasing the chances of the rat dislodging the pellet off of the shelf, or in which

418 reaching success was scored using the first attempt [3, 22, 23]. Microelectrode implant locations
419 relative to skull landmarks are shown in Figure 2C. While microelectrodes were implanted
420 contralateral to the preferred forepaw, microelectrode locations in the left hemisphere were
421 reflected across the midline so all microelectrode locations could be visualized on the right
422 hemisphere to allow for comparison across animals. Because we prioritized placing the first
423 array into RFA given its smaller size, the locations of the RFA arrays were highly consistent
424 across rats. The increased variability in the location of CFA arrays is due to the geometric
425 limitations imposed by the craniectomy orientation, patterns of vasculature, and size of the
426 microelectrode arrays as opposed to variability in the location of CFA across rats. While the
427 position of the CFA microelectrode arrays varied, the majority of the individual electrode wires
428 were still within the CFA motor representation.

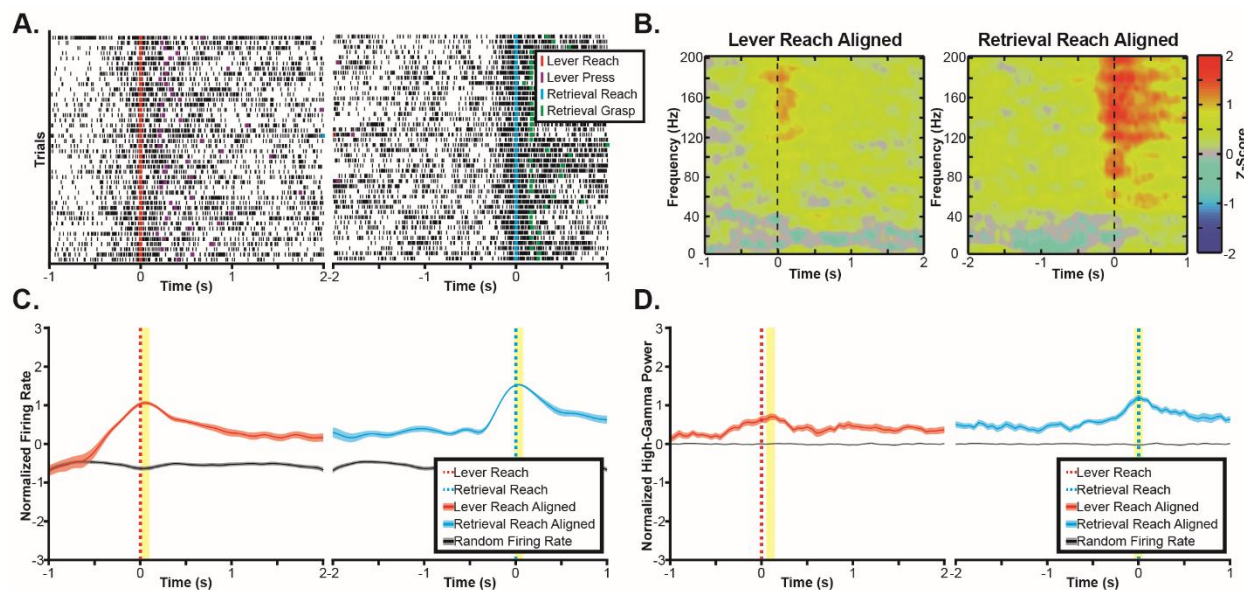
429 **Table 1. Summary of Task Performance**

Rat	Preferred Forepaw	Total Sessions	Total Trials	Successful Trials	Percent Accuracy	Exemplar Session Date (Days Post-Implant)	Number of Exemplar Trials	Successful Exemplar Trials	Exemplar Percent Accuracy
1	Right	13	371	215	58.0%	25	36	23	63.9%
2	Right	13	506	332	65.6%	24	44	28	63.6%
3	Left	16	671	440	65.6%	13	44	32	72.7%
4	Left	16	648	411	63.4%	20	45	36	80.0%
5	Left	15	493	320	64.9%	24	44	25	56.8%

431 **3.2 Task-Related Neural Activity During ‘Gross’ and ‘Fine’ Reaching Movements**

432 Initially, we sought to characterize the patterns of task-related neural activity observed in
433 an exemplar recording session. The task-related multi-unit firing activity from several exemplar
434 channels is shown in Figures 4-6. In the first channel (Figure 4A and C), a statistically significant
435 increase in firing rate is observed during reaching in both task contexts. Specifically, the peak
436 multi-unit firing was significantly different from chance when aligned either to the reach to the
437 lever or the reach towards the pellet, with a stronger modulation observed during the pellet
438 retrieval. Additionally, when compared to the pre-movement period, there was a weaker but

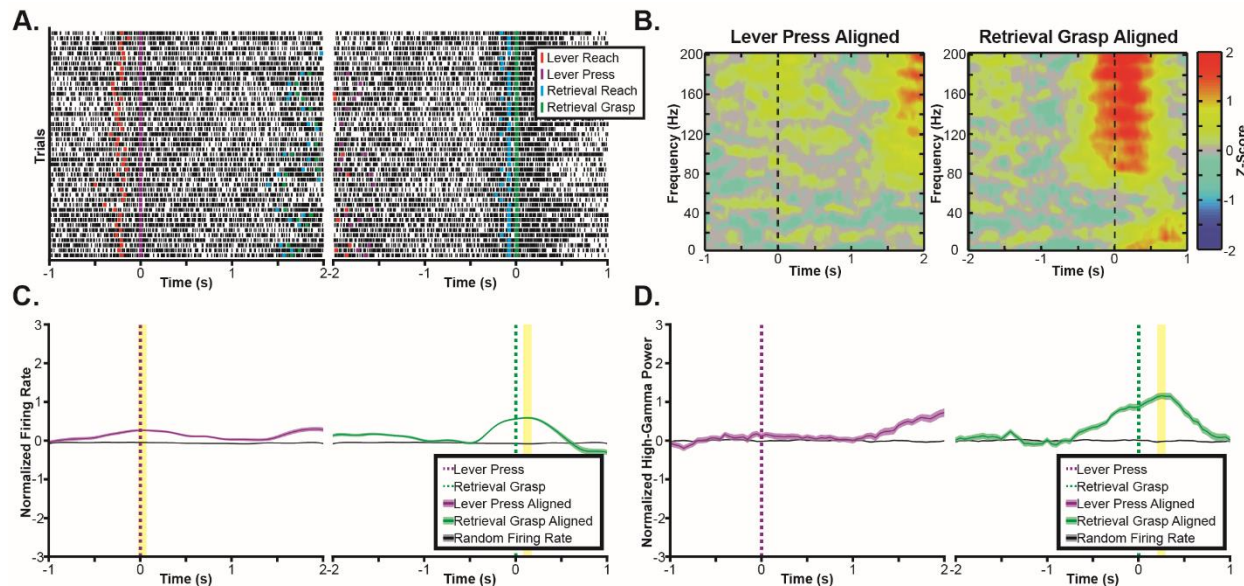
439 consistent increase in firing rate maintained during the period between the lever press and the
440 pellet retrieval. While this period was variable in length, the maintained increase in neural
441 activity is apparent either when aligned to the reach towards the lever or the reach towards the
442 pellet. In a second exemplar channel (Figure 5A and C) a grasp-related increase in firing rate is
443 illustrated. In this channel, there was a small but statistically significant increase in firing rate
444 around the lever press and a larger statistically significant increase in firing rate observed when
445 aligned to the grasp. While this increase began before the reach towards the pellet, there was a
446 stronger depth-of-modulation observed when aligning trials to the grasp than when aligning trials
447 to the reach onset. Finally, other channels showed a more complex response. For example, the
448 channel shown in Figure 6 displayed a statistically significant decrease in firing rate with a peak
449 just after the lever press and a statistically significant increase in firing rate immediately before
450 the reach towards the food pellet.



451

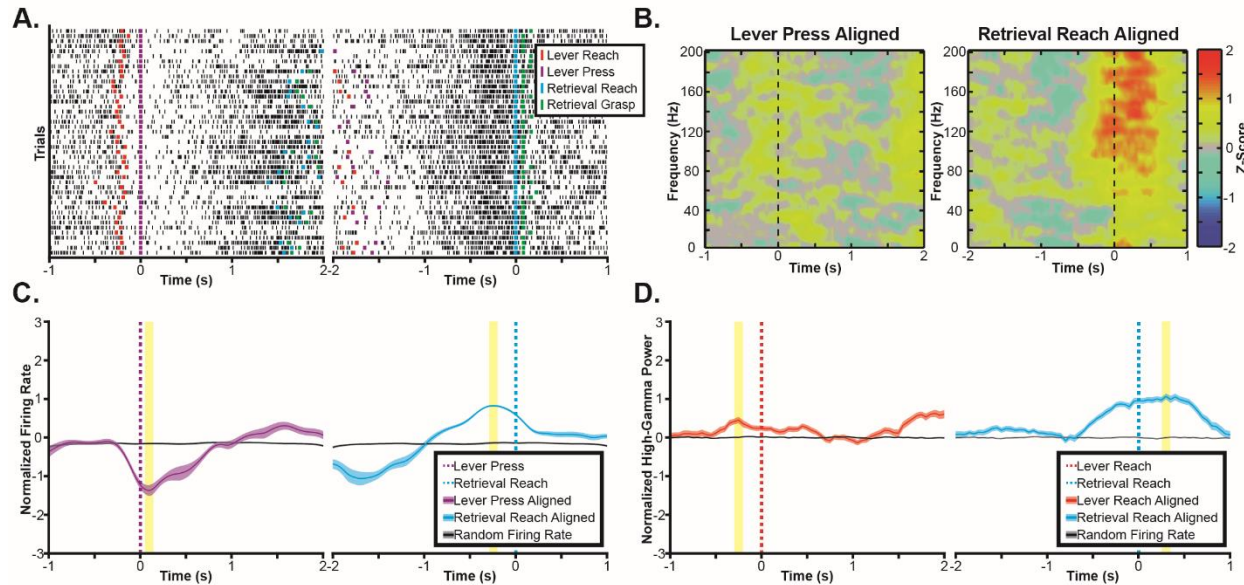
452 **Figure 4. Exemplar Reach-Related Channel.** **A.** Raster plots show multi-unit spike times (black ticks)
453 aligned to the onset of the reaching movement towards the lever (left) and food pellet (right), showing an
454 increase in firing rate correlated to the reach onset. **B.** Spectral power changes are plotted aligned to the
455 onset of reaching movements to the lever (left) and pellet (right). Spectral power changes were log
456 transformed and z-scored relative to randomly selected time windows between trials, therefore, positive

457 values indicate increases in spectral power, and negative values indicate decreases in spectral power. A
458 broadband increase in spectral power in frequencies above 60Hz was observed for both the reach to the
459 button and the reach to the pellet. **C.** Multi-unit firing rates were estimated by convolving a Gaussian
460 waveform with spike times and then averaging firing rates across trials, showing a statistically significant
461 ($p < 0.05$) increase in firing rate aligned to the onset of the reach in both task components. The statistically
462 significant peak firing rates are indicated by the yellow highlighting. **D.** High-gamma band (70Hz-110Hz)
463 power also significantly increased around both the reach to the lever (left) and the reach to the food pellet
464 (right). The statistically significant peak modulations of high-gamma band spectral power are indicated by
465 the yellow highlighting.



466

467 **Figure 5. Exemplar Grasp-Related Channel.** **A.** Raster plots show multi-unit spike times (black ticks)
468 aligned to the lever press (left) and onset of the pellet grasp (right), showing an increase in firing rate
469 correlated to the grasp onset. **B.** Spectral power changes are plotted aligned to the lever press (left) and
470 pellet grasp (right). Spectral power changes were log transformed and z-scored relative to randomly
471 selected time windows between trials, therefore, positive values indicated increases in spectral power, and
472 negative values indicate decreases in spectral power. A broadband increase in spectral power in
473 frequencies above 60Hz was observed for the pellet grasp. **C.** Multi-unit firing rates were estimated by
474 convolving a Gaussian waveform with spike times and then averaging across trials. Mean firing rates
475 synchronized to the grasp were significantly ($p < 0.05$) higher than expected by chance. The statistically
476 significant peak firing rates are indicated by the yellow highlighting. **D.** High-gamma band (70Hz-110Hz)
477 power also significantly increased around the pellet grasp (right). The statistically significant peak
478 modulation of high-gamma band spectral power during the grasp is indicated by the yellow highlighting.



479

480 **Figure 6. Exemplar Pellet-Related Channel.** **A.** Raster plots show multi-unit spike times (black ticks)
481 aligned to the lever press (left) and onset of the reach to the pellet (right), showing a decrease in firing
482 rate correlated to the lever press followed by an increase in firing rate prior to the reach to the pellet. **B.**
483 Spectral power changes are plotted aligned to the reach to the lever (left) and reach to the pellet (right).
484 Spectral power changes were log transformed and z-scored relative to randomly selected time windows
485 between trials, therefore, positive values indicated increases in spectral power, and negative values
486 indicate decreases in spectral power. A broadband increase in spectral power in frequencies above 60Hz
487 was observed for the reach to the food pellet (right) with a smaller increase in broadband spectral power
488 observed before the reach to the lever. **C.** Multi-unit firing rates were estimated by convolving a Gaussian
489 waveform with spike times and then averaging across trials. Mean firing rates show a complex task
490 response with firing rates significantly ($p < 0.05$) decreased around the lever press and then significantly
491 ($p < 0.05$) increased immediately prior to the reach to the food pellet. The statistically significant peak
492 firing rates are indicated by the yellow highlighting. **D.** High-gamma band (70Hz-110Hz) power did not
493 show a decrease around the lever press but instead showed a small, but statistically significant ($p < 0.05$),
494 increase in high gamma band power prior to the reach to the lever. The high-gamma band power
495 maintained the significant increase in activity around the reach to the food pellet observed in the multi-
496 unit firing rate with an increased duration of activity. The statistically significant peak modulations of
497 high-gamma band spectral power are indicated by the yellow highlighting.

498

499 Along with modulations of multi-unit firing rate, widespread modulations of the high-
500 gamma band spectral power were also observed. Figures 4-6 also contain time-frequency plots
501 showing task-related changes in spectral power throughout the frequency spectrum as well as the
502 specific change in high-gamma band (70-105Hz) power for the same exemplar channels as the

503 multi-unit firing rate. Across each exemplar, increases in high-gamma band power were
504 observed in the same channels and task periods where increases in multi-unit firing rate were
505 observed. Specifically, increases in broadband spectral power were observed when aligned to
506 both the reach to the lever and reach to the pellet in the channel shown in Figure 4, for the grasp
507 but not the lever press in the exemplar channel shown in Figure 5, and for the reach to the pellet
508 in Figure 6. While increases in multi-unit firing rate and high gamma band power were often
509 observed in the same channel, the high gamma band did not exhibit task-related decreases. In the
510 exemplar channel shown in Figure 6, firing rate decreased around the lever press, while a small
511 but statistically significant increase in high-gamma band spectral power was observed. The time
512 scales of changes in high-gamma band spectral power were also often extended relative to multi-
513 unit firing rate. This longer modulation of activity is particularly apparent for the pellet retrieval
514 in Figure 5 (grasp) and Figure 6 (reach to the pellet).

515 The range of task-related activations observed was characterized across all channels and
516 all animals. The topography of microelectrodes classified as related to each task component is
517 shown in Figure 7. The proportion of channels classified as related to each task component are
518 summarized for multi-unit firing rate changes in Table 2. Of the 118 channels with at least one
519 spike profile found, 98 channels had statistically significant task-related changes in multi-unit
520 firing rate. While more channels had firing-rate changes during the pellet retrieval than the lever
521 press, more channels were classified as reach-related than were classified as lever press-related
522 or grasp-related. For the pellet retrieval this difference in the number of reach-related and grasp-
523 related channels appears to stem from RFA, where almost three times more channels were
524 classified as reach-related than were classified as grasp-related. The proportion of channels
525 classified as related to each task component using high-gamma band power changes are shown in

526 Table 3. Because LFP power changes can be detected in the absence of spike profiles, more
 527 channels had statistically significant changes in high gamma band power than had changes in
 528 multi-unit firing rate. For lever press high-gamma band power changes, the vast majority of
 529 channels were classified as reach-related, with a smaller number classified as lever press-related.
 530 Classification using high-gamma band spectral power was similar to the classification using
 531 multi-unit firing activity for the lever press. However, this classification differed for pellet
 532 retrieval. When classified based upon the changes in high-gamma band spectral power, the
 533 proportion of reach and grasp-related channels were similar, with a slightly higher number of
 534 reach-related than grasp-related channels in RFA.

535 **Table 2. Summary of significant task-related changes in multi-unit firing rate**

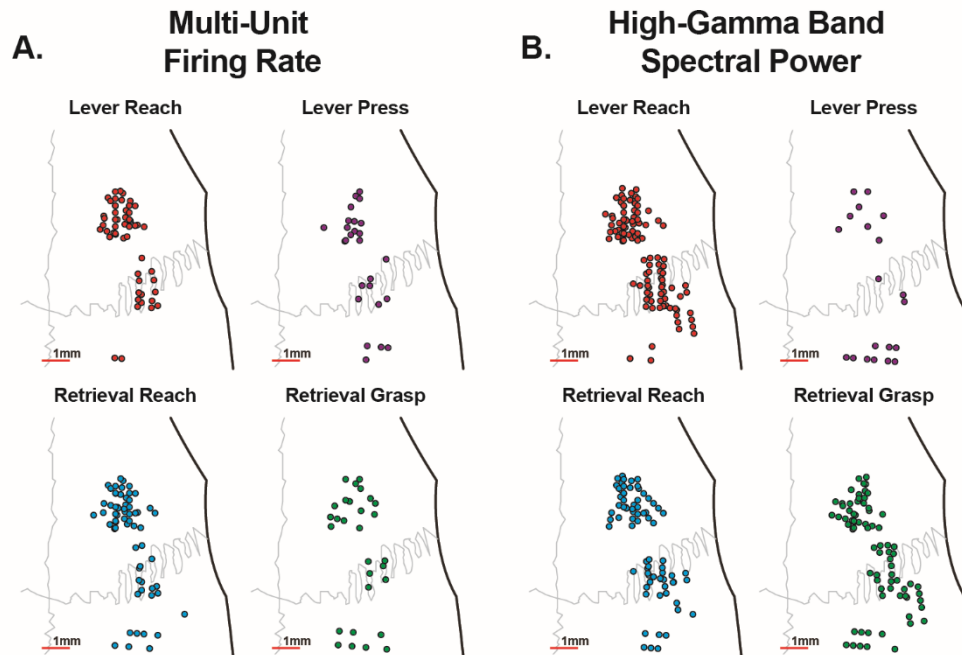
Area	Total Channels	Channels with Spikes	Button Press					Retrieval					Any Activation
			Reach		Press		Total	Reach		Grasp		Total	
			Increases	Decreases	Increases	Decreases		Increases	Decreases	Increases	Decreases		
RFA	76	60 (79.0%)	32 (42.1%)	2 (2.6%)	5 (6.6%)	10 (13.2%)	49 (64.5%)	37 (48.9%)	4 (5.3%)	12 (15.8%)	4 (5.3%)	57 (75.0%)	59 (77.6%)
CFA	79	58 (73.4%)	15 (19.0%)	1 (1.3%)	7 (8.9%)	4 (5.1%)	27 (34.2%)	20 (25.3%)	1 (1.3%)	12 (15.2%)	1 (1.3%)	34 (43.0%)	39 (49.4%)
Total	155	118 (76.1%)	47 (30.3%)	3 (1.9%)	12 (7.7%)	14 (9.0%)	76 (49.0%)	57 (36.8%)	5 (3.2%)	24 (15.5%)	5 (3.2%)	91 (58.7%)	98 (63.2%)

536
537

538 **Table 3. Summary of significant task-related changes in high-gamma band (70-110Hz) power**

Area	Total Channels	Button Press			Retrieval			Any Task Modulation
		Reach	Press	Total	Reach	Grasp	Total	
RFA	78	53 (68.0%)	8 (10.3%)	61 (78.2%)	41 (52.6%)	37 (47.4%)	78 (100%)	78 (100%)
CFA	79	50 (63.3%)	12 (15.2%)	62 (78.5%)	33 (41.8%)	39 (49.4%)	72 (91.1%)	73 (92.4%)
Total	157	103 (65.6%)	20 (12.7%)	123 (78.3%)	74 (47.1%)	76 (48.4%)	150 (95.5%)	151 (96.2%)

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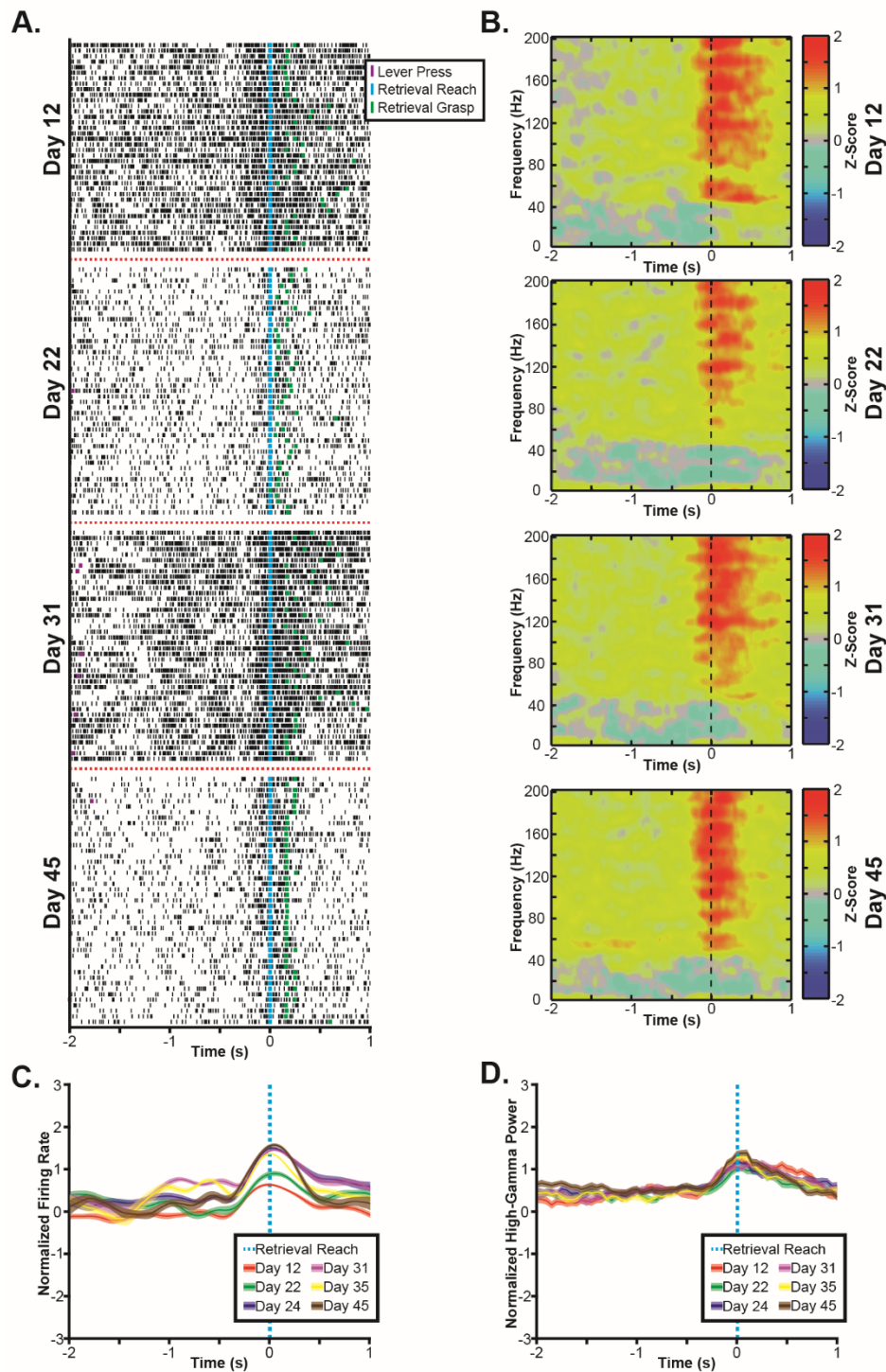
540

541 **Figure 7. Microelectrode Classification.** Each microelectrode was classified based upon whether it was
542 significantly modulated by the reach to the lever, the lever press, or not modulated during the lever press.
543 Similarly, each electrode was also classified as modulated when aligned to the reach to the food pellet,
544 when aligned to the grasp of the pellet, or not modulated during the retrieval. Each classification was
545 made using both the multi-unit firing rate (A) and high-gamma band (70-110Hz) spectral power (B).
546 When examining changes in multi-unit firing rate, more channels were modulated by the reaching
547 movements than either the lever press or grasping movements. Additionally, more of the channels
548 modulated by reaching movements were located in RFA than in CFA. When examining changes in high-
549 gamma band power, while more channels were modulated by the reach than the button press, because of
550 the decrease in temporal specificity, a similar number of channels were modulated by both the reach and
551 the grasp. In contrast to the multi-unit firing rate, similar numbers of electrodes with significant task-
552 related activations aligned to the reach were found in both CFA and RFA.

553 **3.3 Consistency of Rodent Task-Related Neural Activity**

554 In addition to characterizing the task-related activations observed in RFA and CFA, we
555 investigated whether task-related activations in RFA and CFA were stable over several weeks.
556 The task-related multi-unit firing and spectral power changes for an exemplar channel are shown
557 for several recording sessions in Figure 8. On each recording day, an increase in multi-unit firing
558 rate was observed around the reach towards the pellet. Because the background firing rate
559 differed across days, the depth-of-modulation was variable across days. In contrast, a similar

560 broadband increase in high-gamma band power was observed for each session with a similar
561 depth-of-modulation observed in each day shown.

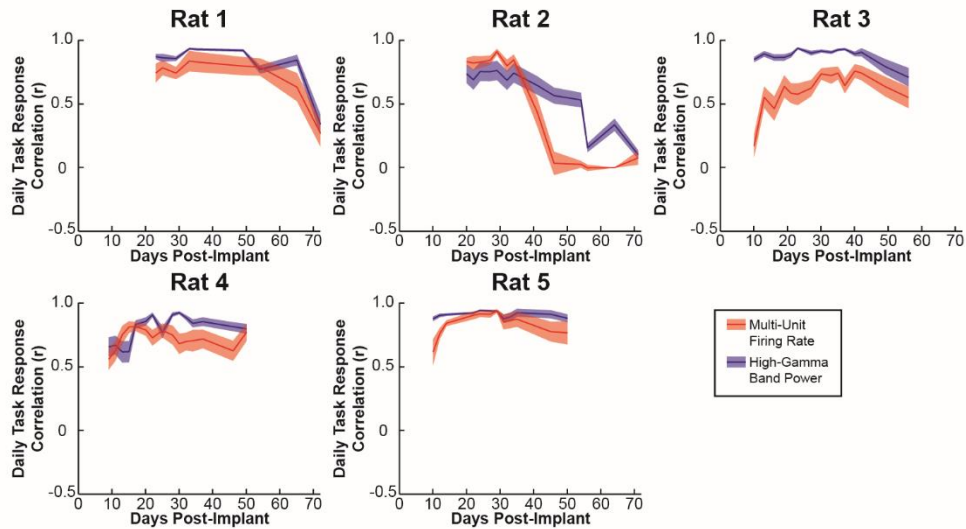


562

563 **Figure 8. Exemplar task-related activity across recording days. A.** Raster plots show multi-unit spike
564 times (black ticks) aligned to the onset of the reaching movement towards the food pellet on several

565 recording days, showing an increase in firing rate correlated to the reach onset that is conserved across
566 days. **B.** Spectral power changes are plotted aligned to the onset of reaching movements to the pellet on
567 the same days. Spectral power changes were log transformed and z-scored relative to randomly selected
568 time windows between trials, therefore, positive values indicate increases in spectral power, and negative
569 values indicate decreases in spectral power. A broadband increase in spectral power in frequencies above
570 60Hz is observed aligned to the reach in each day. **C.** Multi-unit firing rates were estimated by
571 convolving a Gaussian waveform with spike times and then averaging firing rates across trials, showing a
572 statistically significant ($p < 0.05$) increase in firing rate aligned to the onset of the reach. While the timing
573 of this increase in firing rate is conserved across days, there is some variance in the depth-of-modulation
574 observed. **D.** High-gamma band (70Hz-110Hz) power also significantly increased around the reach to the
575 food pellet with similar depth-of-modulations observed on each recording day. All plots were generated
576 from the same exemplar channel within RFA of a single animal.

577 The stability of task-related neural activity was quantified by calculating the correlation
578 between the daily and overall average modulation for each channel with a significant task-related
579 modulation in the exemplar recording session. These correlations are shown for each rat in
580 Figure 9 and summarized in Table 4. The task-related neural activity was largely stable for each
581 rat, decreasing only when recording quality becomes impaired, such as in Rat 1 starting around
582 day 70 post-implant and in Rat 2 starting around 40 days post-implant. While both multi-unit
583 firing rate changes and high-gamma band power changes were stable over time, daily task-
584 related changes in high-gamma band power were more correlated to the overall average task-
585 related changes in high-gamma band power than multi-unit firing rates were. Specifically, the
586 distribution of correlations between daily and overall task-related modulations was significantly
587 higher for high-gamma band spectral power changes than for multi-unit firing rate changes
588 (Wilcoxon rank sum test, $p = 4.04 \times 10^{-44}$).



589

590 **Figure 9. Cross-Day Stability.** The stability of task-related changes in neural activity was examined by
 591 determining the correlation between the daily mean firing rate and the overall mean firing rate as well as
 592 the correlation between the daily high-gamma band power change and the overall mean high-gamma band
 593 power change for each channel. Plots show the mean daily correlation across channels and the error bars
 594 show the standard error. While a decrease in signal quality was observed at 9 weeks and 5 weeks in rats 1
 595 and 2 respectively, overall, task-related changes in multi-unit activity and high-gamma band power were
 596 stable across days for each rat. While changes in multi-unit firing rate and high-gamma band power were
 597 both stable across recording days, the task-related the high-gamma band power change had higher
 598 correlations between the daily and overall mean than was observed for task-related multi-unit firing rate
 599 changes. Additionally, high-gamma band power changes show a slower decrease in stability from the
 600 degradation in signal quality observed in rats 1 and 2.

601 **Table 4. Summary of the stability of task-related changes in multi-unit firing rate and high-gamma**
 602 **band power.**

Rat	Multi-Unit Firing		High-Gamma Band Spectral Power	
	Channels (n)	Mean Daily Correlation (r)	Channels (n)	Mean Daily Correlation (r)
1	14	0.714	31	0.814
2	15	0.496	26	0.574
3	21	0.610	30	0.878
4	21	0.721	30	0.797
5	16	0.835	31	0.910
Total	87	0.670	148	0.801

603

604 4. Discussion

605 This study used a novel automated behavior box to demonstrate the widespread nature of

606 reach and grasp-related neural activity in the rat primary motor cortex (CFA) and premotor

607 cortex (RFA). Previous studies have demonstrated task-related modulation of activity during
608 reaching tasks including center-out movements of a lever, push/pull movements of a lever, and
609 pellet retrieval tasks [1, 7, 11, 24-26]. Importantly, these previous studies found that neural
610 activity could be used to decode movement parameters, such as kinematics and kinetics [11, 25].
611 Here we examined the neural correlates of reaching movements using a novel automated
612 behavior box that combined a gross reaching task (lever press) and a fine reaching task (skilled
613 pellet retrieval) in close temporal succession. While previous examples of automated rodent
614 behavior boxes have been described, our system adds the ability to examine two similar but
615 distinct and relatively unconstrained reaching tasks in the same animals [22, 23, 27]. As with
616 these previous systems, the use of an automated system reduces the level of supervision
617 necessary to train rodents to perform reaching movements and eliminates many potential biases
618 inherent in manually administered tasks.

619 Interestingly, a greater number of channels were active during the skilled pellet retrieval
620 than during the lever press, potentially indicating greater cortical involvement in planning and
621 executing the pellet retrieval than the lever press. This increased activity during the pellet
622 retrieval is reasonable when considering that this task component is more complex and involves
623 increased use of the distal forelimb muscles. Therefore, the increased task-related neural activity
624 during the pellet retrieval may represent specific or increased activation of neurons during distal
625 movements as has been observed in premotor areas of non-human primates during tasks
626 requiring distal forelimb movements [28, 29]. Additionally, while the lever press is indirectly
627 associated with the food reward, the pellet retrieval is directly associated with the reward. As
628 RFA has been shown to encode an expectation of reward [26], some of the observed increases in
629 activity may be associated with the direct expectation of the food reward.

630 The combination of gross and fine reaching movements into a single behavioral task
631 provides a new tool to examine the neural basis of reaching and grasping in rodents. Previous
632 studies have argued for a specific role for RFA in grasping based upon the patterns of
633 movements elicited by long-train ICMS [30]. However, lesion studies have produced conflicting
634 results with some studies showing deficits in reach-to-grasp tasks after a lesion to CFA [10, 17]
635 while other studies have found grasp-specific deficits isolated to lesions of RFA and not CFA
636 when temporary lesions were induced with cortical cooling [30]. Isolating the specific
637 differences in the roles that RFA and CFA play in controlling reaching and grasping is
638 complicated by the fact that both regions exhibit extensive task-related neural activity during
639 reach-to-grasp tasks [7] that are likely affected in part by the complex interactions between the
640 two regions [15]. Our data have found that task-related activity in RFA was most modulated
641 when aligned to the onset of reaching movements, however this may be due to a role of RFA in
642 planning the combined reach-to-grasp movement as opposed to a specific role of RFA in
643 reaching as opposed to grasping.

644 Because rodents have both primary and secondary forelimb motor regions, a number of
645 studies have utilized rodent models of stroke and traumatic brain injury to examine the role of
646 neuroplasticity in motor recovery [9, 10, 17]. In particular, ICMS mapping studies have found
647 that expansions of RFA are associated with recovery of function following a lesion to CFA [10].
648 While rodents can learn to modulate activity in the perilesional cortex [6], the specific
649 relationship between functional changes in perilesional cortex and secondary motor regions is
650 unknown. The combined behavioral task demonstrated here is particularly relevant for
651 examining the changes in task-related neural activity associated with post-injury neuroplasticity.
652 While the lever press requires only a gross reaching movement, the pellet retrieval has the

653 additional requirements of fine control of the distal forepaw and increased integration of sensory
654 and motor information to successfully grasp and retrieve the pellet. Furthermore, the lever press
655 task is more likely to be successfully completed in the early period of motor recovery which will
656 allow for the assessment of the contribution of neuroplasticity to changes in task-related neural
657 responses during the subacute period when the level of motor recovery is insufficient to allow for
658 successful performance on the single-pellet retrieval task [9, 18].

659 Importantly, the task-related changes in neural activity were stable in individual channels
660 over the 7-10 week period examined. While both task-related multi-unit firing and high-gamma
661 band power changes persist over this period, the LFP high-gamma band showed more
662 consistency across days. This increased stability is likely due to the difficulty in isolating the
663 same individual neurons across days and the increased susceptibility of multi-unit firing rates to
664 noise in the recordings. Previous studies examining chronic recordings in humans and non-
665 human primates have observed that less than 40% of single-units were stable through a period of
666 15 days [31]. Additionally, changes in firing rate and spike amplitude are even seen within single
667 recording days [32]. The finding that reaching related neural activity in RFA and CFA is stable
668 over several weeks has particularly important implications for examining the role of
669 neuroplasticity in recovery from a focal cortical lesion. Specifically, while multi-unit firing may
670 be used to compare the proportion of channels with firing rate changes aligned to specific
671 components of the task with greater temporal precision, LFP signals may be more valuable for
672 examining changes in the relative strength of activations across days in single channels.

673 **5. Conclusions**

674 Collectively, we have demonstrated a novel complex rodent reaching task incorporating a
675 gross lever press with a fine pellet retrieval into a single trial. Importantly, there were widespread

676 task-related changes in neural activity during both task periods from microelectrodes in RFA and
677 CFA, demonstrating a significant cortical involvement in both reaching tasks. Furthermore, this
678 cortical involvement is maintained over months with stable task-related changes in neural
679 activity observed at the level of single channels. These results serve to further characterize the
680 normal role of rodent primary and secondary motor areas in planning and executing forelimb
681 movements and further establish the rat as a model species for future studies examining the
682 changes in the specific relationship between neural activity and forelimb movements associated
683 with neuroplasticity following manipulation to the rodent sensorimotor system.

684

685 **Author Contributions**

686 Conceived and designed the experiments: DTB DJG RJN; Performed the experiments: DTB DJG
687 MDM; Analyzed the data: DTB; Contributed analysis tools: MDM; Wrote the paper: DTB RJN

688

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693 **Competing Interests**

694 The authors have no relevant financial conflicts of interest related to this work.

695 **Data Availability**

696 The data underlying the findings reported in this manuscript have been deposited in an online
697 Open Science Framework repository that will be made public at the time of publication in
698 accordance with the journal Data Availability Policy.

699

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