

1 Co-expression of calcium channels and delayed rectifier potassium channels  
2 protects the heart from proarrhythmic events

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## 32 **Abstract (140 words)**

33 Cardiac electrical activity is controlled by the carefully orchestrated activity of more than  
34 a dozen different ion conductances. Yet, there is considerable variability in cardiac ion  
35 channel expression levels both within and between subjects. In this study we tested the  
36 hypothesis that variations in ion channel expression between individuals are not random  
37 but rather there are modules of co-expressed genes and that these modules make electrical  
38 signaling in the heart more robust.

39 Meta-analysis of 3653 public RNA-Seq datasets identified a strong correlation between  
40 expression of *CACNA1c* (L-type calcium current,  $I_{CaL}$ ) and *KCNH2* (rapid delayed rectifier  
41  $K^+$  current,  $I_{Kr}$ ), which was verified in mRNA extracted from human induced pluripotent  
42 stem cell-derived cardiomyocytes. *In silico* modeling indicates that the co-expression of  
43 *CACNA1c* and *KCNH2* limits the variability in action potential duration and reduces  
44 susceptibility to early afterdepolarizations, a surrogate marker for pro-arrhythmia.

45

## 46 **Keywords:**

47 Ion channels; co-expression; gene modules; meta-analysis; cardiac action potential, early  
48 afterdepolarization, arrhythmia, drug-induced long QT syndrome

49

## 50 **Introduction**

51 Robust electrical signaling in the heart is critical for co-ordinating the efficient pumping of  
52 blood around the body. Failure of cardiac electrical signaling, even for just a few minutes,  
53 can have fatal consequences, with sudden cardiac death accounting for up to 10% of deaths  
54 in our community (1). Despite decades of research, predicting in advance who is more or  
55 less susceptible to sudden cardiac death remains challenging (2).

56 The action potential (AP) of excitable cells, such as cardiac myocytes and neurons, reflects  
57 the orchestrated activity of at least a dozen distinct ion channels and electrogenic  
58 transporters (3) (4). In such complex systems, both theoretical and experimental studies  
59 have shown that there is considerable inter-individual variability in the combinations of  
60 molecular input parameters that can produce very similar integrated outputs (5) (6). This  
61 has led to a paradigm shift in computational modeling that relies not on generating  
62 idealized outputs based on mean data but rather development of populations of models  
63 that account for the observed variability in molecular inputs (7) (8). Such models are  
64 already proving useful for interrogating inter-individual variability in response to  
65 pathological stimuli (9) (10) (11). Our challenge now is to discern the underlying essence  
66 of these complex systems (12,13) so that we may then make rational interventions to treat  
67 pathology that takes into account inter-individual variation. Specifically, are there  
68 underlying principles regulating cardiac electrical activity that can provide insights into  
69 why some people are more susceptible to sudden cardiac death in response to pathological

70 stimuli, such as drug block of the rapid delayed rectifier potassium channel ( $I_{Kr}$ ) which is  
71 the underlying basis of drug-induced long QT syndrome (di-LQTS) (14).

72 A common approach to discern patterns in multi-dimensional biological problems has  
73 been to look for co-expression networks (13) (15). Co-expression networks are known to  
74 encode functional information (16), with co-expression reflecting co-regulation and co-  
75 functionality (17) (18). To help identify robust co-expression modules, it is helpful to use  
76 meta-analytical approaches, as the aggregation of large numbers of individual networks  
77 across multiple independent experiments averages away noise and reinforces those  
78 correlations that reflect real signals (19) (20) (21).

79 Here, we have used meta-analytic co-expression analysis in large scale human gene  
80 expression data sets to identify modules of co-expressed ion channel genes which were  
81 then used to constrain population models of cardiac electrical activity. These models were  
82 then used to test the hypothesis that co-expression of repolarization and depolarization  
83 currents helps prevent irregular action potentials from emerging when human cardiac  
84 myocytes are exposed to pro-arrhythmic stimuli. We show that tight coupling of current  
85 densities for the L-type calcium current ( $I_{CaL}$ ) and the rapid component of the delayed  
86 rectifier potassium current ( $I_{Kr}$ ) reduced the emergence of pro-arrhythmic early  
87 afterdepolarizations (EADs) and this protection persisted in the face of highly variable  
88 expression of other ion channels, as well as in the presence of pharmacological block of  $I_{Kr}$ ,  
89 a potent pro-arrhythmic stimulus (22). A very important prediction to arise out of our  
90 modelling studies is that in the context of drug block of  $I_{Kr}$  those patients with high  
91 expression of  $I_{CaL}$  and  $I_{Kr}$  experience more EADs and are therefore more likely to be  
92 susceptible to ventricular arrhythmias.

93

## 94 **Results**

95 The shape and duration of action potentials in cardiac myocytes are determined by the  
96 orchestrated activity of voltage-gated sodium, calcium and potassium channels, as well as  
97 a series of electrogenic transporters that regulate intracellular ion concentrations (See  
98 Supplementary data **Figure S1**). These channels, transporters and related intracellular  
99 calcium handling proteins are encoded by a few dozen genes, sometimes referred to as the  
100 *rhythmonome* (23) (see Supplementary data, **Table 1**).

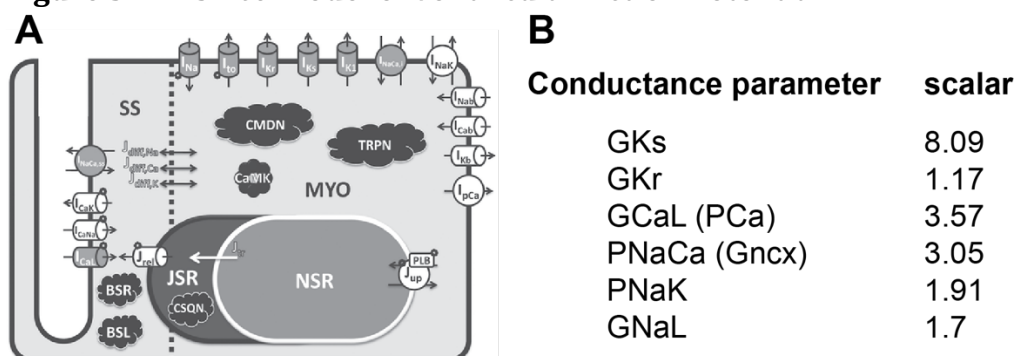
101 To determine whether there were any co-expression patterns among the *rhythmonome*  
102 genes we first undertook an untargeted screen for possible expression correlation patterns  
103 in publicly available RNA-seq data sets (see list of RNA-seq experiments in supplementary  
104 data, **Table 2**). Ranked correlation coefficients from an aggregate co-expression network  
105 that contain data from 3653 samples are illustrated in the heatmap in **Figure 1A**. High  
106 ranked correlations indicate similarity of transcriptional profiles between the genes. A  
107 clustering analysis, as shown by the dendrogram in **Figure 1A**, groups genes according to  
108 their correlation similarities, as defined by the Spearman's correlation coefficients (see

109 color code in **Figure 1A**). There is a large cluster of yellow/green squares in the bottom  
 110 left corner indicating that there are significant levels of correlation amongst many of the  
 111 genes. Furthermore, within this large cluster there are two sub-clusters. The cluster of  
 112 yellow-green squares corresponding to 13 genes in the bottom left corner (red dashed box  
 113 in **Figure 1A**) encode for proteins that regulate calcium fluxes as well as the transient  
 114 outward  $K^+$  current (*KCND3*), which helps to maintain the plateau potential at a level that  
 115 maximizes calcium influx (24). A second sub-cluster, in the upper right quadrant of the  
 116 main cluster, encompasses 10 genes (black dashed box in **Figure 1A**), including *KCNH2*,  
 117 *SCN5a*, *KCNJ12* and *KCNIP2*, that encode for ion channel proteins important for regulating  
 118 action potential duration (APD).

119 Overall, the connectivity within the set of rhythmome genes is fairly high in comparison  
 120 to their connectivity to all other genes in the co-expression network (node degree analysis,  
 121  $p \sim 5.7e-14$ ), with a central gene being *CACNA1C*, the gene encoding the alpha subunit of the  
 122 L-type calcium channel (see Supplementary data, **Figure S2**). Although *CACNA1c* clusters  
 123 in the group of calcium handling genes in the bottom left quadrant of the main cluster in  
 124 **Figure 1A**, it also shows high levels of correlation with the cluster of ion channel genes in  
 125 the top right quadrant of **Figure 1A**. In a similar fashion, the *KCNH2* gene, which encodes  
 126 for  $I_{Kr}$ , is included in the ion channel cluster but also shows moderate-high correlations  
 127 with a portion of the calcium handling genes in the bottom left quadrant. The highest  
 128 ranked co-expression partners for *CACNA1C* and *KCNH2* are highlighted in **Figure 1B**.

129 The vast majority of the public RNA-Seq datasets included in our analyses were not heart  
 130 specific. It is, however, noteworthy that there are no strong correlations between the  
 131 expression of any of the individual ion channel or calcium handling genes and the cardiac-  
 132 specific markers included in our analyses: *GATA-4*, *NKX2-5*, *MYL2* and *MYL7*. For example,  
 133 the cardiac marker genes are towards the bottom of the lists in **Figure 1B**. This suggests  
 134 that the correlations within the set of rhythmome genes are not simply a reflection of  
 135 cardiac specific expression but rather represent intrinsic correlations.

136 **Figure S1: In silico model of ventricular Action Potential**

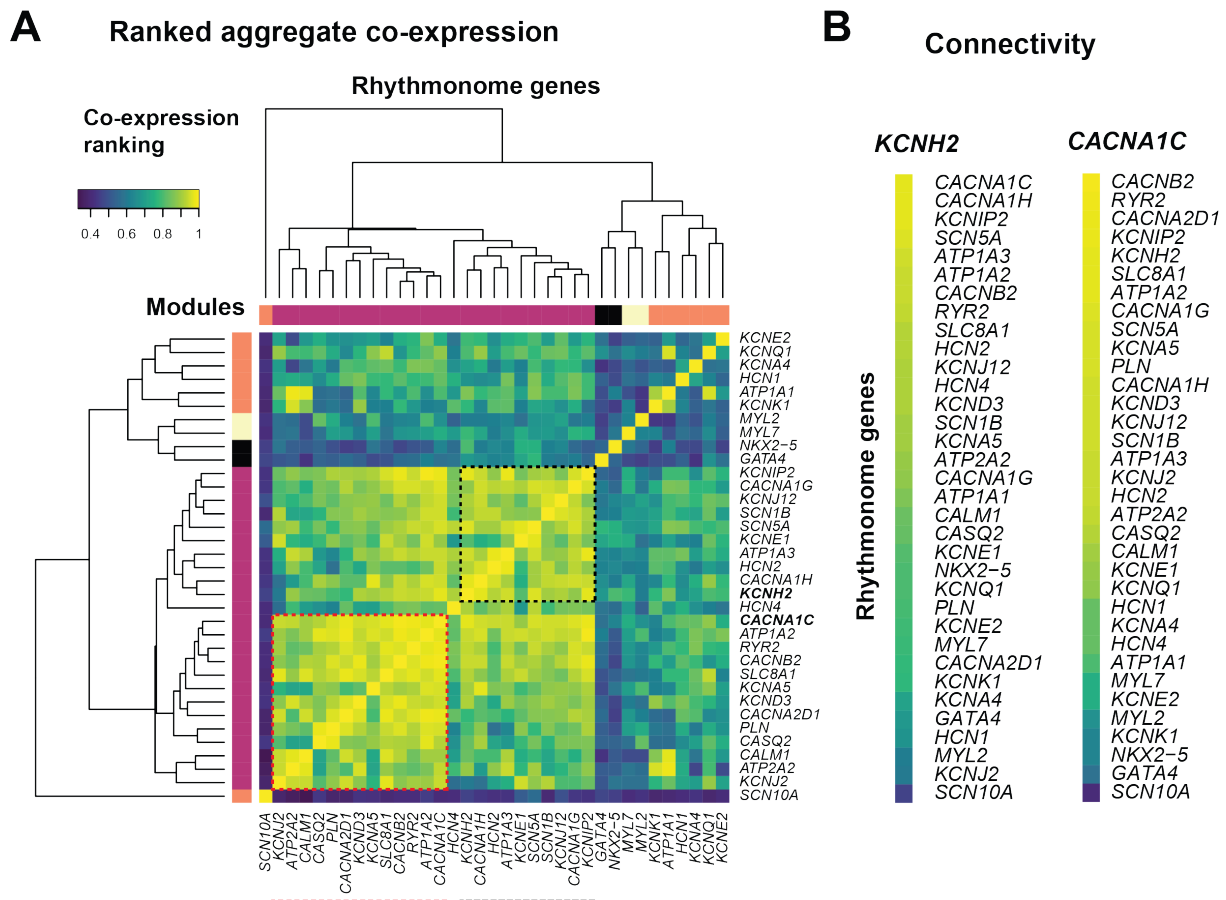


137 **A.** Schematic diagram of the ventricular myocyte model used in this study (reproduced  
 138 from (25) under the CC-BY licence.

139 **B.** Scaling factors applied to the original model were taken from (26)

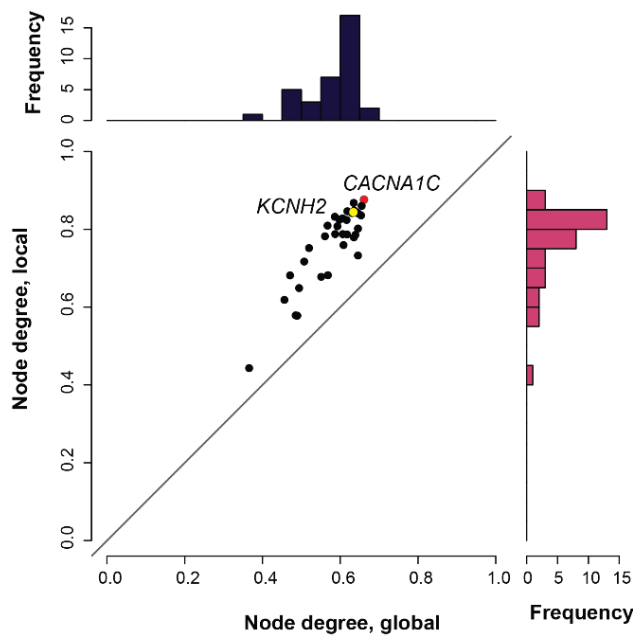
141

142 **Figure 1: Cardiac ion channel and calcium handling protein co-expression**  
 143 **connectivity analysis from published RNA-seq datasets**



144  
 145 **A.** Sub-network of co-expression ranking across 35 genes encoding for cardiac ion channels  
 146 or calcium homeostasis proteins (see Supplementary Table 1). Blue: low ranked  
 147 correlations, yellow: high ranked correlations. The dendrogram illustrates the modules of  
 148 genes with high levels of similarity in their transcriptional profiles. Red and black dashed  
 149 boxes highlight subnetworks of correlated genes **B.** Connectivity of genes to *KCNH2*  
 150 (encodes for  $I_{Kr}$ ) and *CACNA1C* (encodes for  $I_{CaL}$ ).  
 151

152 **Figure S2: Network connectivity for each rhythmome gene**



153  
154 The degree of network connectivity for each rhythmome gene within the local  
155 rhythmome network (y-axis) versus its connectivity within the whole genome (x-axis).  
156 All the rhythmome genes are more highly connected within the local network (i.e., all  
157 the points lie above the line of identity,  $p \sim 5.7e^{-14}$ ). *CACNA1C* is highlighted in red and  
158 *KCNH2* in yellow.

159 To investigate whether the meta-analytic co-expression patterns observed in **Figure 1**  
160 were also seen in human heart cells, we extracted mRNA from human induced pluripotent  
161 stem cell-derived cardiomyocytes (hiPSC-CMs) (27) obtained from 10 patients with no  
162 known heart disease. All samples contained high levels of cardiac marker genes (*MYL7*,  
163 *GATA4* and *NKX2.5*) (**Figure 2A**). Furthermore, the levels of expression of the housekeeper  
164 genes, *GPADH* and *HRPT1* were similar across samples (see data at right side of **Figure 2A**).  
165 The levels of expression of most rhythmome genes showed variations between the  
166 samples that spanned approximately an order of magnitude. However, similar to the  
167 generic tissue RNA-Seq datasets, there were modules of co-expressed genes (e.g., see  
168 dashed box in bottom left quadrant of **Figure 2B**). Most of the 13 genes in the cluster in  
169 **Figure 2B** are present in the modules highlighted by the black and red dashed boxes in  
170 **Figure 1A**. Conversely, many of the ion channel genes contained in the modules  
171 highlighted in **Figure 1** are not present in the module in **Figure 2** (e.g. *KCNJ2/KCNJ12*,  
172 which encodes for  $I_{K1}$ ; *KCND3*, which encodes for  $I_{T0}$ ; and *SCN5a*, which encodes for  $I_{Na}$ ).  
173 These genes are all known to be expressed at lower levels in embryonic hearts and so  
174 unsurprisingly they are not well expressed in the hiPSC-CM lines (28).

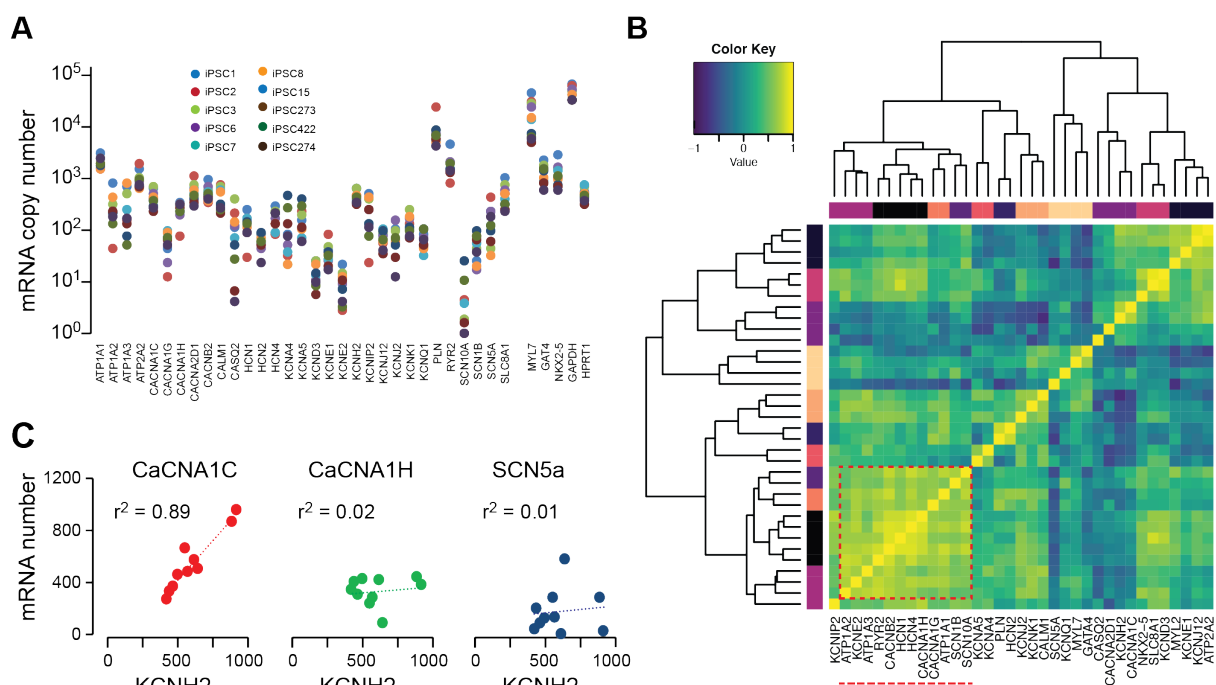
175 We next looked to see if there were any specific relationships between genes encoding  
176 depolarization and repolarization currents, within the hiPSC-CM expression profiles. In  
177 **Figure 2C**, we have plotted the expression of *KCNH2* versus the genes that encode for the  
178 depolarization currents that showed the highest levels of correlation with expression of  
179 *KCNH2* in the generic tissue datasets (see **Figure 1B**, i.e., *CACNA1c*, *CACNA1H* and *SCN5a*).

180 The most notable correlation that was observed in the hiPSC-CMs was that between *KCNH2*  
 181 and *CACNA1c*;  $r^2 = 0.89$  (**Figure 2C**).

182 As the only robust relationship that we observed in both the generic tissue sets and the  
 183 hiPSC-CM lines was the co-expression of *KCNH2* and *CACNA1c*, we focused on this pair for  
 184 our subsequent studies. To investigate whether co-expression modules of ion channel  
 185 genes might influence integrated cardiac electrical function, we used an *in silico* approach.  
 186 First, we simulated a population of 1000 human cardiac action potentials where random  
 187 scalar values, chosen from a log normal distribution with mean 1 and standard deviation  
 188 of 0.5 (**Figure 3A**, lower panel), was applied to every conductance in each iteration of the  
 189 action potential model (see **Figure 3A** and Supplementary Data, **Movie S1**).

190  
 191 **Figure 2: HiPSC-CM mRNA correlation analysis**

192



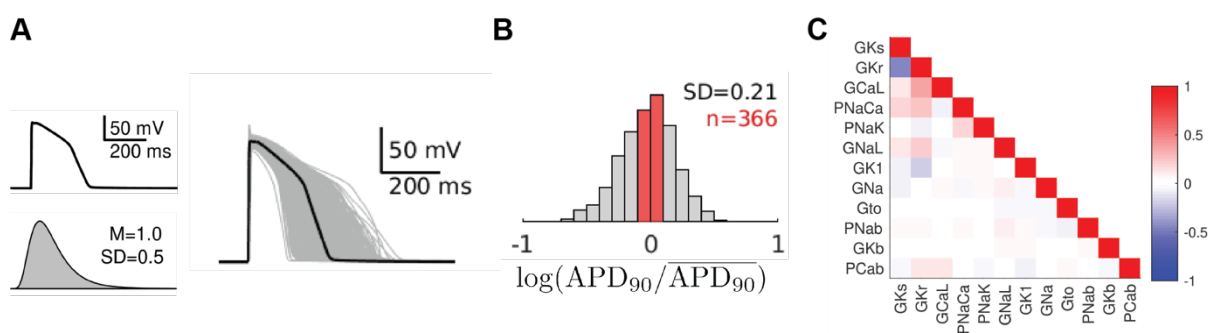
193  
 194 **A.** plot of all mRNAs (log axis) for 10 hiPSC-CM lines. Note that there are high levels of  
 195 expression of cardiac markers (*MYL7* as well as *NKX2-5* and *GATA4*) in all cell lines. Also  
 196 there is less variability in the levels for the housekeeping genes (*GAPDH* and *HPRT1*)  
 197 compared to that seen for the ion channels and calcium handling proteins. **B.** Correlation  
 198 matrix for hiPSC-CM mRNA. The red dashed box highlights the module with the highest  
 199 correlations. **C.** Correlation plots for *KCNH2* versus genes that encode the major  
 200 depolarizing currents (*CACNA1c*, *CACNA1H* and *SCN5a*).

201 The baseline action potential produced by this model (black trace in right hand panel of  
 202 **Figure 3A**) has a duration at the point of 90% repolarization ( $APD_{90}$ ) of 264 ms. The  
 203 population of 1000 cardiac cells generated by randomly scaling the conductances exhibited  
 204  $APD_{90}$  values that ranged from ~120 ms to ~500 ms (**Figure 3A**, right panel, and **Figure**  
 205 **3B**). We next selected those cells with  $APD_{90}$  values that fell within 20% of the mean value

206 (red bars, **Figure 3B**) to determine if there were any patterns of ion channel co-expression  
 207 that could contribute to keeping the  $APD_{90}$  within this narrow selected range. The  
 208 correlation matrix of the conductance scaling factors for the selected cells (**Figure 3C**)  
 209 reveals a positive correlation between  $G_{Kr}$  and  $G_{CaL}$  ( $R=0.36$ ) as well as an inverse  
 210 correlation for  $G_{Kr}$  and  $G_{Ks}$  ( $R=-0.46$ ). The positive correlation between the conductance  
 211 scalars  $G_{Kr}$  and  $G_{CaL}$  in the *in silico* modelling dataset (**Figure 3**) suggests that the  
 212 correlation seen between *CACNA1c* and *KCNH2* mRNA expression in both the public RNA-  
 213 Seq datasets (**Figure 1**) and the hiPSC-CM dataset (**Figure 2**) would contribute to reducing  
 214 the population variability in  $APD_{90}$  values.

215 We next repeated our previous simulation of 1000 action potentials but forced the  
 216 conductance scaling factors for  $I_{Kr}$  and  $I_{CaL}$  to be identical in each cell (denoted co-  
 217 expression in **Figure 4**, also see Data supplement, **Movie S2**). The scaling factors for all  
 218 other conductances remained independent. The distribution of  $APD_{90}$  values for both  
 219 independent and co-expression cell populations becomes broader as the level of variability  
 220 is increased (**Figure 4A-C**). However, the spread of  $APD_{90}$  values in the cells with identical  
 221  $G_{CaL}$ - $G_{Kr}$  scalars is always narrower than in the cell populations with independent  $G_{CaL}$ - $G_{Kr}$   
 222 scalar values. For example, in the case of **Figure 4B**, the variance of the  $APD_{90}$  values was  
 223 0.026 for the co-expression dataset but 0.046 for the independent dataset (see  
 224 supplementary data **Figure S3-C**). Another notable feature of the data in **Figure 4C** is that  
 225 early afterdepolarisations (EADs) begin to appear in the cell population with independent  
 226 scalars when the scalar variability,  $\sigma^2$ , exceeds 0.20 (also see supplementary data **Figure**  
 227 **S4**). The number of cells with an EAD are indicated in parentheses above each distribution  
 228 in **Figure 4C**.

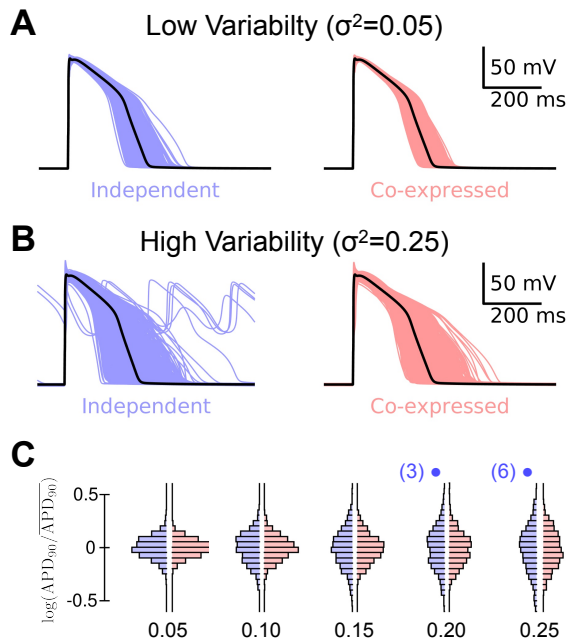
229  
 230 **Figure 3: *In silico* predictions of conductance scalars that give  $APD_{90}$  values in the**  
 231 **normal range**



232  
 233 **A.** Baseline AP model and frequency histogram of scalars (log normal distribution with a  
 234 mean of 1 and SD of 0.5) used to generate the population of 1000 APs with the baseline AP  
 235 (all scalars set to 1.0) shown in black. **B.** Frequency histogram of  $APD_{90}$  values for the 1000  
 236 simulations with those falling within  $\pm 20\%$  of the mean value shown in red. **C.** correlation  
 237 matrix for sets of conductance scalars that gave  $APD_{90}$  values within  $\pm 20\%$  of the mean  
 238 value



239 **Figure 4: Impact of  $I_{Kr}$ - $I_{CaL}$  co-expression and conductance scalar variability on**  
240 **APD90 variability**  
241



242 Raw APs for independent (blue) and co-expression of  $G_{Kr}$ - $G_{CaL}$  (red) for **A.** low scalar  
243 variability ( $\sigma^2=0.05$ ) and **B.** high scalar variability ( $\sigma^2=0.25$ ). Note the presence of EADs in 6  
244 of the APs in the independent group with  $\sigma^2 = 0.25$ . **C.** Histograms of  $\log(\text{APD}_{90}/\text{mean APD}_{90})$   
245 distributions for co-expressed (red) or independent (blue)  $G_{Kr}$ - $G_{CaL}$  simulations with  $\sigma^2 = 0.05$ ,  
246 0.1, 0.15, 0.2, 0.25. The numbers in parentheses above the 0.2 and 0.25 groups indicate the  
247 number of EADs in each independent scalars group.  
248  
249

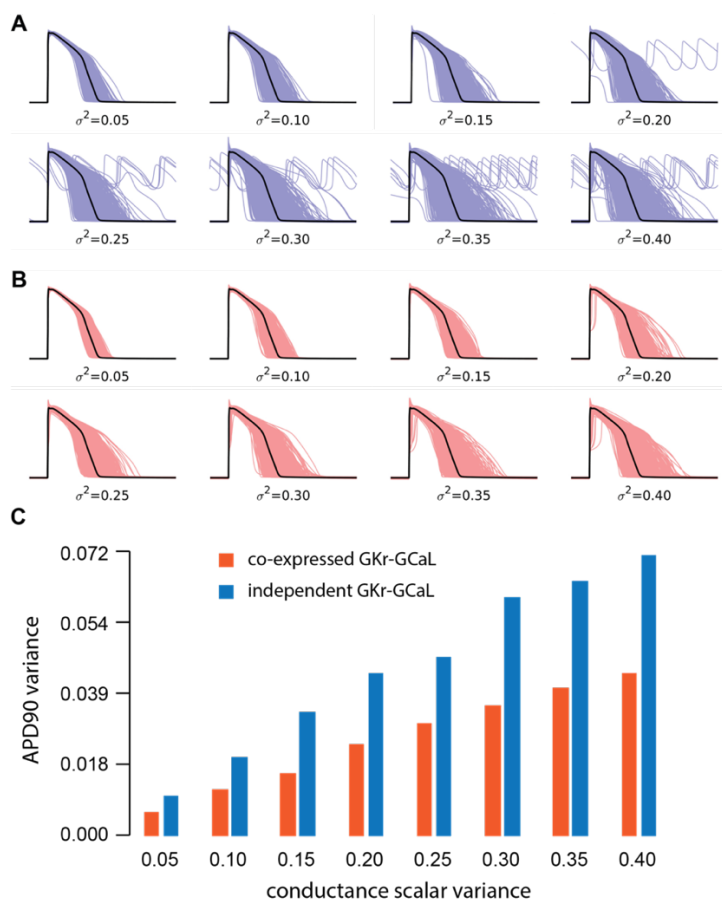
250 **Movie S1**

251

252 **Movie S2**

253

254 **Figure S3: Population models of ventricular APs with different levels of scalar**  
 255 **variance**



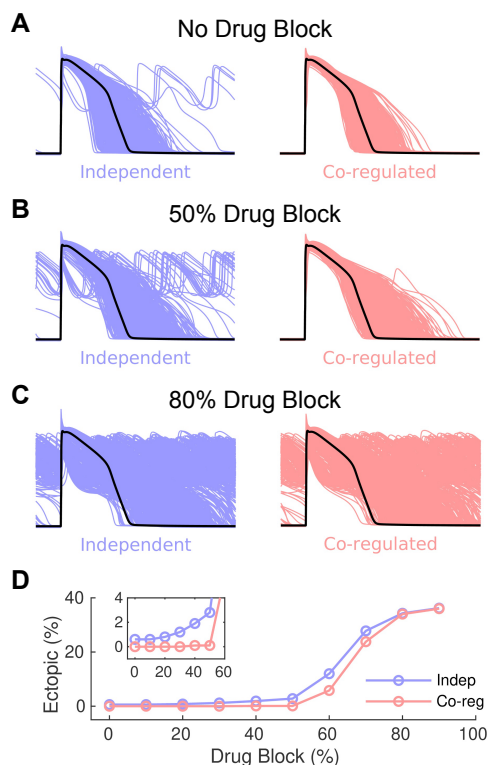
256 **A-B.** Population of models with variance systematically increased from  $\sigma^2 = 0.05$  to 0.40  
 257 for independent conductance scalars for  $G_{Kr}$  and  $G_{CaL}$  **(A)**, or co-expression conductance  
 258 scalars for  $G_{Kr}$  and  $G_{CaL}$  **(B)**. As the variance increases, the number of cells that develop  
 259 EADs increases in the independent series. Conversely, for the co-expression models, there  
 260 are no EADs even at variances up to 0.4. **C.** Variance of the APD<sub>90</sub> distributions for each set  
 261 of conductance scalar inputs for independent (blue) and co-expression (red) of  $I_{Kr}$  and  $I_{CaL}$ .  
 262 Note that the variance of the APD<sub>90</sub> distribution was always greater for the independent  
 263 simulations (p<0.008 between groups, paired t-test)  
 264

265 We next investigated whether coupling of the conductance scalars for  $G_{Kr}$  and  $G_{CaL}$   
 266 influenced the generation of EADs in response to a pathological stimulus. Specifically, how  
 267 cells respond to drug block of  $I_{Kr}$ , the underlying cause of di-LQTS (22). Example  
 268 populations of action potentials obtained for independent and co-expression populations  
 269 with  $I_{Kr}$  block of 0%, 50% and 80% are illustrated in **Figure 5**. As the extent of  $I_{Kr}$  block is  
 270 increased (from A to C), the proportion of simulated action potentials producing EADs  
 271 increases. It is also clear that at lower levels of  $I_{Kr}$  block, EADs were more frequent when  
 272  $G_{CaL}$  and  $G_{Kr}$  scalars were modulated independently (see **Figure 5B** and inset to **Figure 5D**).  
 273 However, the proportion of simulations developing EADs in both the independent and co-  
 274 expression populations becomes similar when the extent of  $I_{Kr}$  block exceeds 80% (**Figure**  
 275 **5D**).

276 It is well established that only a subset of patients exposed to drugs that block  $I_{Kr}$  (29), or  
277 with a mutation causing 50% loss of  $I_{Kr}$  function (30), will develop life threatening  
278 arrhythmias. This is consistent with the prediction made by our simulated drug block  
279 experiments shown in **Figure 5**. We therefore asked whether the data from the co-  
280 expression datasets could tell us anything about what factors might predispose to the  
281 development of EADs in the presence of a drug that blocks  $I_{Kr}$ . Analysis of the subset of  
282 scalars within the co-expression dataset that produced the 50 longest APs without EADs,  
283 compared to the subset of scalars that resulted in APs with EADs, is illustrated in **Figure**  
284 **6A and 6B** respectively. Notably, the longest APs without EADs had low  $G_{CaL}$  scalars (and  
285 hence low  $G_{Kr}$  scalars) before addition of drug block. Conversely, the APs that developed  
286 EADs had higher  $G_{CaL}$  and  $G_{Kr}$  scalars. In **Figure 6C**, we have plotted the APD<sub>90</sub> values for  
287 cells in the highest (red) and lowest (blue) quartiles of  $G_{CaL} - G_{Kr}$  scalars. As expected, the  
288 low  $G_{CaL}$  group showed longer APD<sub>90</sub> values on average compared to the high  $G_{CaL}$  group  
289 (see the continuous lines in **Figure 6C**). Furthermore, for the 70%  $I_{Kr}$  block scenario, 44%  
290 of the high  $G_{CaL}$  group have developed EADs whereas only 7% of the low  $G_{CaL}$  group have  
291 developed EADs (compare red and blue bars at 70% drug block in **Figure 6C**). Thus, higher  
292  $G_{CaL}$  is associated with a greater risk of developing EADs in response to moderate levels of  
293  $I_{Kr}$  block. A similar pattern of results was observed when  $G_{CaL}$  and  $G_{Kr}$  were allowed to vary  
294 independently, except that in this scenario the difference between the high  $G_{CaL}$  and low  
295  $G_{CaL}$  groups was even more dramatic at lower levels of  $I_{Kr}$  block (see supplementary data  
296 **Figure S4**).

297  
298

**Figure 5: Impact of  $G_{Kr}$ - $G_{CaL}$  co-expression on response to drug block of  $I_{Kr}$**

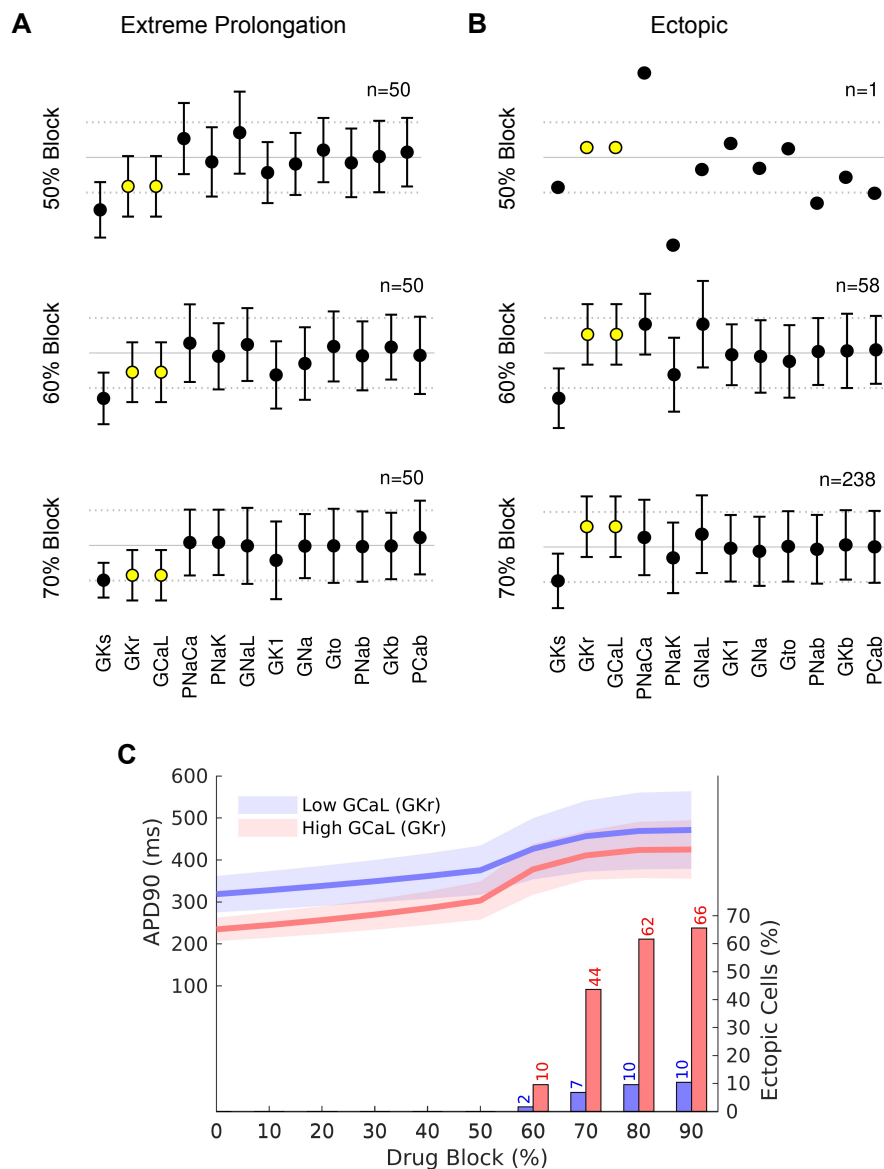


299

300 Raw APs for co-expressed  $G_{Kr}$ - $G_{CaL}$  (red) and independent (blue)  $G_{Kr}$ - $G_{CaL}$  populations,  
 301 with scalar variance  $\sigma^2 = 0.25$ , for **A.** control, **B.** 50%  $I_{Kr}$  block and **C.** 80%  $I_{Kr}$  block. **D.** plot  
 302 of % of AP simulations with EADs versus %  $I_{Kr}$  block (co-expression, red and  
 303 independent, blue). The inset in panel D shows an expanded view of the % EADs at small  
 304 levels of  $I_{Kr}$  block.

305  
 306  
 307

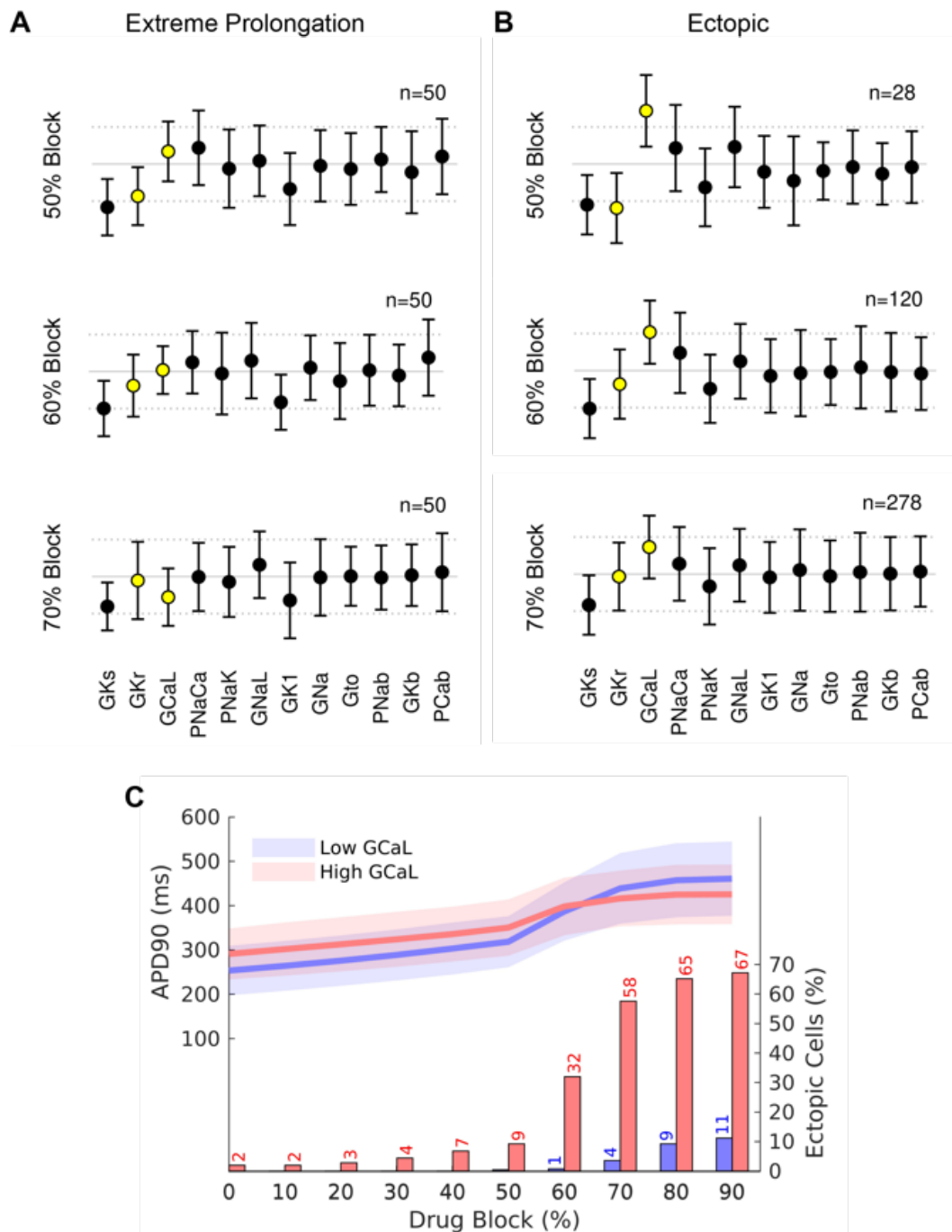
**Figure 6: High  $G_{CaL}$  increases risk of EAD formation at moderate  $I_{Kr}$  block**



308  
 309 Scalars (box and whisker plots) for the population of cells with  $G_{Kr}$ - $G_{CaL}$  co-expression. **A.** 50  
 310 cells with the longest APD<sub>90</sub> values and no EAD with increasing %  $I_{Kr}$  block. **B.** scalars (box  
 311 and whisker plots) for cells with EADs with increasing %  $I_{Kr}$  block. The  $G_{CaL}$  and  $G_{Kr}$  scalars  
 312 are highlighted in yellow. **C.** APD<sub>90</sub> values (left axis) for the highest (red) and lowest (blue)  
 313 quartile of cells according to baseline  $G_{CaL}$  scalar. The continuous lines show the mean value  
 314 and shaded area shows  $\pm 1$  SD). The percentage of EADs in each quartile is shown as columns  
 315 (see axis on right side of graph). The corresponding plots for the population of cells with  
 316 independent  $G_{Kr}$ - $G_{CaL}$  scalars are show in the Supplementary data (**Figure S4**)

317 **Figure S4: High  $G_{CaL}$  increases risk of EAD formation at moderate  $I_{Kr}$  block even**  
 318 **when  $G_{CaL}$  and  $G_{Kr}$  are varied independently**

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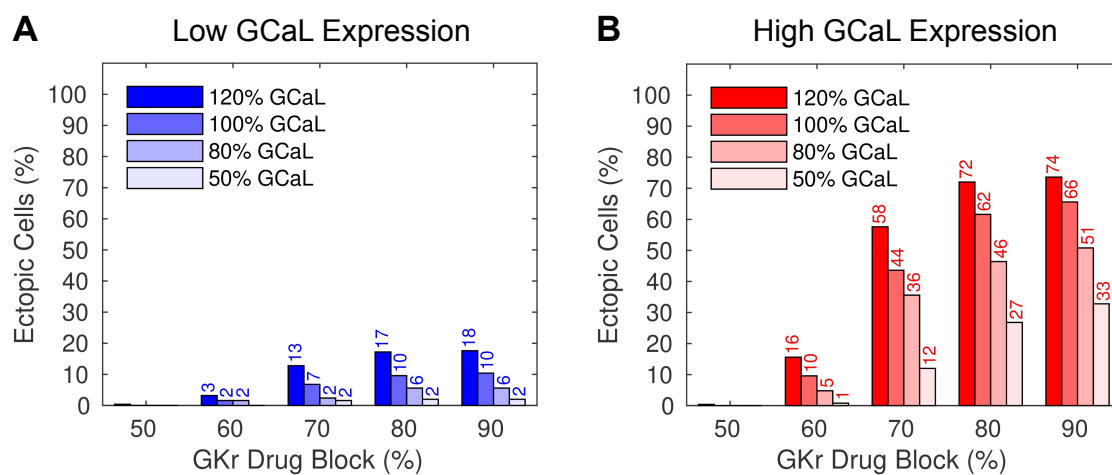


321  
 322 Conductance scalars (box and whisker plots) that give **A**. The 50 most extreme APD values  
 323 or **B**. EADs for the population of cells with independent regulation of  $G_{Kr}$  and  $G_{CaL}$ .  
 324 **C**. Plot of APD<sub>90</sub> values for the highest quartile of  $G_{CaL}$  (red) and lowest quartile of  $G_{CaL}$  (blue)  
 325 versus % drug block of  $I_{Kr}$ . The continuous line shows mean and shaded regions show  $\pm 1$   
 326 standard deviation. The column graph shows the % of cells that develop EADs at each level  
 327 of drug block.

328

329 A corollary of our prediction that patients with high  $G_{CaL}$  are more susceptible to EADs  
 330 when exposed to a drug that blocks  $I_{Kr}$ , is that co-administration of a drug that blocks  $I_{CaL}$   
 331 would reduce the incidence of EADs. Magnesium, which is used in the acute management  
 332 of di-LQTS (14), is a weak calcium channel blocker. Raising plasma  $[Mg^{2+}]$  from 1.5 to 2.5  
 333 mM would be expected to inhibit  $I_{CaL}$  by ~20% (31), conversely reducing  $[Mg^{2+}]$  from 1.5  
 334 to 0.5 mM would be expected to increase  $I_{CaL}$  by ~20%. When we increased  $I_{CaL}$  by 20%,  
 335 the incidence of EADs in the high  $G_{CaL}$  group increased from 10% to 16% for the 60%  $I_{Kr}$   
 336 block simulation and from 44% to 58% for the 70%  $I_{Kr}$  block simulations (see **Figure 7**). A  
 337 drug that inhibited  $I_{CaL}$  by 20% caused a modest decrease in the percentage of cells with  
 338 EADs and reduction of  $I_{CaL}$  by 50% had a correspondingly larger effect, for example,  
 339 reducing EADs from 44% to 12% in the 70%  $I_{Kr}$  block scenario (**Figure 7**).

340  
 341 **Figure 7: Effect of modifying  $I_{CaL}$  on incidence of EADs in response to  $I_{Kr}$  drug block.**



342  
 343  $I_{CaL}$  was increased 20% to mimic hypomagnesaemia, reduced 20% to mimic  
 344 hypermagnesaemia (see text for details), or reduced 50% to mimic administration of a  
 345 calcium channel blocker. In both the quartile of cells with the lowest  $G_{CaL}$  scalars (blue, **A**)  
 346 and the quartile of cells with the highest  $G_{CaL}$  scalars (red, **B**) the incidence of EADs  
 347 increased when  $G_{CaL}$  was enhanced and decreased when  $G_{CaL}$  was decreased. The  
 348 observed differences were most pronounced with moderate (60-70%)  $I_{Kr}$  drug block.

349  
 350 **Discussion**

351 Cardiac electrical activity is regulated by the interdependent activity of a plethora of ion  
 352 channels, transporters and calcium handling proteins (4). Understanding the precise  
 353 details of how these conductances interact to control the rhythm of the heart has been an  
 354 enduring source of fascination. In this study, we have used meta-analytical techniques to  
 355 interrogate the large numbers of RNASeq datasets that have been deposited in public  
 356 access databases, to look for patterns of co-expressed genes that might help decipher the  
 357 control of cardiac electrical activity. The most important pair of co-expressed genes,  
 358 identified both in the public RNA Seq datasets (**Figure 1**) and in heart cells derived from

359 hiPSC lines (**Figure 2**), was that of *CACNA1c* ( $I_{CaL}$ ) and *KCNH2* ( $I_{Kr}$ ). Using an *in silico*  
360 approach we demonstrated that tight co-expression of *CACNA1c* and *KCNH2*, against a  
361 background of variability of all other ion channels, helps to control the duration of  
362 repolarization (**Figure 4**). More importantly, the co-expression of *CACNA1c* and *KCNH2*  
363 helps to protect the heart from early after depolarizations when they are exposed to drugs  
364 that block  $I_{Kr}$  (**Figure 5**). Our simulations also suggest that inter-individual differences in  
365 pro-arrhythmic responses to  $I_{Kr}$  drug block can be explained by inter-individual differences  
366 in levels of *CACNA1c* expression (**Figure 6**).

367 Over the last few years, numerous groups have shown that there is considerable  
368 heterogeneity of ion channel expression amongst excitable cells, including neurons (32)  
369 and cardiac myocytes (7,19). Furthermore, since the pioneering work of Eva Marder and  
370 colleagues, the presence of modules of co-expressed ion channel genes has also been well  
371 appreciated(15). These previous studies, however, relied on patch clamp analysis of  
372 isolated cells (15,33) and qPCR analysis (15) of individual ion channel mRNA, which are  
373 highly laborious and so have been restricted to only a few important ion channel genes.  
374 The advent of high throughput transcriptomic analyses has greatly facilitated the  
375 identification of conserved networks of co-expressed gene modules amongst the entire set  
376 of expressed genes (21). By applying meta-analytic approaches to a large number of  
377 independent datasets one can more readily discern genuine co-expression signals from  
378 noise, as well as explore smaller gene modules (21). In our analysis of a subset of  
379 rhythmome genes (35 members, **Table S1**) within a large library of public RNA Seq  
380 datasets, (see **Table S2**) we identified two clusters of genes: a first subset that  
381 predominantly affects calcium handling and a second subset that predominantly affects  
382 membrane potential (see **Figure 1**). The nodes within each of these clusters that are most  
383 closely connected within the rhythmome relative to all other genes are *KCNH2* and  
384 *CACNA1c* (**Figure S2**). This is analogous to a network of networks (34), where the *KCNH2*-  
385 *CACNA1c* link provides an interconnection of the two networks. Independent evidence to  
386 corroborate an important link between calcium handling and regulation of cardiac action  
387 potential duration comes from the large genome-wide association studies (GWAS) of QT  
388 interval duration which identified SNPs in a number of calcium handling genes as well as  
389 *KCNH2* as being important determinants of QT interval in the population (35).

390 Due to the large number of associations we were testing for in our network analyses, it is  
391 possible that some would occur by chance. That we were able to confirm the presence of  
392 at least some of the co-expression modules in an independent dataset, i.e. the hiPSC-CM  
393 (see **Figure 2**) provides important corroborative evidence that these co-expression  
394 patterns are real and therefore likely to have physiological relevance. It should also be  
395 noted that many ion channels important for function in adult cardiac myocytes are not  
396 expressed at significant levels in immature cardiac myocytes, such as those derived from  
397 hiPSC (e.g. *SCN5a*, *KCNQ1*, *KCNJ12*, *KCND3*, (28)). It is therefore possible that we have

398 underestimated the number of genes within the modules of co-expressed genes in adult  
399 cardiac myocytes.

400 The patterns of co-expressed genes we observed show some important similarities, as well  
401 as differences to previous studies. Banyasz et al. (33) and Rees et al. (18) have both  
402 demonstrated that the expression of  $I_{CaL}$  is correlated with the sum of the major  
403 repolarizing ion currents in guinea-pig and mouse respectively. However, the molecular  
404 players involved in cardiac electrical activity in rodents are quite distinct to humans (36).  
405 In humans, the most important determinant of repolarization duration at baseline is  $I_{Kr}$   
406 (37), whereas in guinea-pig  $I_{Ks}$  and  $I_{Kr}$  play equally important roles (33) and in mice the  
407 fast component of the transient outward current ( $I_{to,f}$ ) and the ultra-rapid delayed rectifier  
408 ( $I_{Kur}$ ) are the major repolarization currents (18). Thus, there is a common factor between  
409 our study showing co-expression of *KCNH2* and *CACNA1c* in human and the previous  
410 rodent studies, i.e., all studies show a correlation between  $I_{CaL}$  and the major repolarizing  
411 currents present in that species. Our study, however, is the first to demonstrate the  
412 important co-expressed genes in human heart tissue.

413 Identifying modules of co-expressed genes are the first step in seeking to understand the  
414 logic of complex systems (6). Understanding how such modules impact function in health  
415 and disease is the next challenge. In neuronal cells, Marder and colleagues have shown that  
416 modules of co-expressed ion channels play an important role in regulating action potential  
417 firing patterns (38). Rees and colleagues, have demonstrated that modules of co-expressed  
418 depolarization and repolarization currents can help to ensure normal amplitude calcium  
419 transients, a critical determinant of overall heart function (18). We have extended these  
420 studies to show that in normal heart cells, co-expression of *KCNH2* (repolarization) and  
421 *CACNA1c* (depolarization) channels help to maintain the plateau duration of the action  
422 potential, which in turn likely contributes to regulating the duration and amplitude of the  
423 calcium transient. More importantly, our studies provide the first insights into how  
424 patterns of co-expressed ion channel genes influence the hearts response to pathological  
425 stimuli.

426 Sudden death due to abnormalities of cardiac electrical signaling is a major cause of  
427 mortality (1). Predicting in advance who is more or less susceptible to sudden cardiac  
428 death and therefore warrants prophylactic treatment remains challenging (2). A key to  
429 being able to predict who is at greatest risk is understanding why different people respond  
430 differently to the same pro-arrhythmic stimulus. Based on the results of our *in silico*  
431 studies, we have provided two important insights into the nature of interindividual risk for  
432 developing arrhythmias in response to drugs that block  $I_{Kr}$ , the major cause of drug-  
433 induced cardiac arrhythmias (14). First, cells with low  $G_{CaL}$  (and hence low  $G_{Kr}$  at baseline)  
434 exhibited the greatest prolongation of AP duration when exposed to  $I_{Kr}$  drug block. Second,  
435 cells with high  $G_{CaL}$  (and hence high  $G_{Kr}$  at baseline) showed greater propensity for  
436 development of EADs at moderate levels of  $I_{Kr}$  drug-block (**Figure 6**). An important  
437 implication of the observation that a high  $G_{CaL}$  increases the susceptibility to EADs in



438 response to drug block of  $I_{Kr}$  is that the co-administration of an  $I_{CaL}$  blocker should reduce  
439 the risk of EADs (as shown in **Figure 7**). This is consistent with the observation that the  
440 administration of magnesium, which is a mild calcium channel blocker (31), is helpful in  
441 the acute management of patients with drug-induced *torsades de pointes* (14), and  
442 conversely that hypomagnesaemia, which would stimulate  $I_{CaL}$ , can exacerbate *torsades de*  
443 *pointes* (39). It is also consistent with the observation that drugs that block  $I_{CaL}$  and  $I_{Kr}$  (e.g.,  
444 verapamil) are not associated with drug-induced arrhythmias (40) and that verapamil  
445 prevented the development of *torsades de pointes* in rabbit hearts exposed to an  $I_{Kr}$  blocker  
446 (41). However, given that calcium channel blockers are contra-indicated in some  
447 ventricular arrhythmias (42), and the likelihood that patients who have drug-induced  
448 LQTS may have other underlying cardiac conditions (14), one should be cautious about  
449 prescribing calcium channel blockers. Conversely, it would be reasonable to consider using  
450 calcium channel blockers to treat patients with LQTS type 2 (i.e. patients with an isolated  
451 loss of  $I_{Kr}$  function) who continue to have cardiac events despite treatment with  $\beta$ -blockers  
452 (43).

453 In summary, we have demonstrated that meta-analysis of large-scale gene expression data  
454 sets is a powerful technique for discerning underlying patterns in gene expression, and  
455 that this can provide insights into disease causation at an individual level. Specifically, we  
456 have demonstrated that the co-expression of *KCNH2* ( $I_{Kr}$ ) and *CACNA1c* ( $I_{CaL}$ ) plays an  
457 important role in regulating cardiac repolarization both in health and in disease.

458

## 459 **Methods**

### 460 **Analysis of public RNASeq datasets**

461 An aggregate co-expression gene network was built from public data, similar to that  
462 described previously(44). Briefly, 75 human RNA-seq expression experiments (listed in  
463 Supp **Table S2**) that passed quality control and had a least 10 samples (3653 samples in  
464 total) were downloaded from the Gemma database (45). Approximately thirty thousand  
465 genes were used for the network, limited only to those with Entrez gene identifiers. A co-  
466 expression network was generated for each experiment by calculating Spearman's  
467 correlation coefficients between every gene pair and then ranking these values (44). An  
468 aggregate gene co-expression network was then generated by averaging across all the  
469 individual networks, and re-ranking the final network. This final aggregate network was  
470 then used to determine the co-expression ranking between genes that encode for the set  
471 of ion channels and calcium handling proteins that determine the shape and duration of  
472 the human ventricular AP, the so-called rhythmome gene subset (see Supp **Table S1**).  
473 Network connectivity of the gene set was measured by comparing the weighted local node  
474 degree to the global node degree(46). Node degrees are the sum of the total connections a  
475 node (here gene) has within a network. Local node degree refers to the sum of connections  
476 (here the ranked correlation) within the rhythmome gene set, while global node degree

477 is the sum of connections to that gene across all the genes in the network. Code for the  
478 analysis is available at <https://github.com/sarbal/hERG-cal>

#### 479 **Human induced pluripotent stem cell derived cardiac myocytes.**

480 Human iPSC lines, generated from healthy patients by Stanford Cardiovascular Institute  
481 Biobank, as previously described (47), were a generous donation from Joseph Wu  
482 (Stanford Cardiovascular Institute). HiPSC colonies were maintained on Matrigel®  
483 (Corning) coated plates in chemically defined medium (mTeSR1™, StemCell technologies),  
484 and passaged using Dispase (StemCell technologies). For differentiation, hiPSCs were  
485 dissociated by incubating at 37°C for 7 minutes with TrypLE™ Express (ThermoFisher) and  
486 seeded at 125000 cells/cm<sup>2</sup> on a Matrigel® coated 12 well plate, in mTeSR™1 medium  
487 supplemented with StemMACS™ Y27632 (Miltenyi Biotec). Once the cells reached greater  
488 than 95% confluency, differentiation was initiated using STEMdiff™ Cardiomyocyte (CM)  
489 differentiation and Maintenance Kit (StemCell technologies). At day 15, CMs were  
490 dissociated by incubation in Collagenase Type I (ThermoFisher) for 45 minutes at 37°C to  
491 break up the matrix and then incubated in 0.25% Trypsin with EDTA for 7 minutes at room  
492 temperature followed by filtering through a 40 µm cell strainer (48). The CMs were seeded  
493 on a Fibronectin coated 96-well plate (Greiner Bio-One) and maintained in CM  
494 maintenance medium for 10-15 days before they were harvested for mRNA expression  
495 analysis. Total RNA was obtained from 40,000 hiPSC-CMs lysed using QIAzol Lysis reagent  
496 (Qiagen). The RNA was purified using miRNeasy® Mini Kit (Qiagen), and all samples had  
497 RIN values >7.5, and were analysed using Agilent Bioanalyzer pico-chip. RNA samples were  
498 hybridised with probes designed to detect 35 known rhythmome genes using nCounter  
499 (NanoString Technologies, see Supplementary **Table S1**), which was performed at the  
500 Ramaciotti Centre for Genomics (UNSW).

#### 501 **Computer modelling**

502 Human cardiac APs were simulated using the endocardial configuration of the O'Hara-  
503 Rudy (ORD11) model (25) with key conductances modified as described by Krogh-Madsen  
504 et al. (26) (See Supp **Figure S1**). The original ORD11 code was adapted to run in the Brain  
505 Dynamics Toolbox for Matlab (49). To incorporate population variability in ion channel  
506 expression levels the maximum conductance for each current was multiplied by  
507 conductance scalar ( $G_x$ ), that was drawn from a random log-normal distribution (37), with  
508 unit mean and variance that was systematically manipulated from 0.05 to 0.5. All models  
509 were paced at 1Hz with a stimulus of -40 mV and duration of 1 ms and allowed to  
510 equilibrate for 300 beats. We then analysed the next four beats (to allow for the possibility  
511 of development of alternans) after the equilibration stage. The peaks in those APs were  
512 identified using the Matlab *findpeaks* function. Individual beats were classified as ectopic  
513 if they had secondary peaks that were separated by more than 100 ms. The set of four beats  
514 were further classified as *alternans* if the profile of any of the APs deviated from each other  
515 by more than 1 mV at any time point. In a second set of simulations, we repeated the same  
516 method as above except that the random multipliers applied to both  $I_{CaL}$  and  $I_{Kr}$  were

517 identical. This case we denote co-expression whereas the former case we denote  
518 independent expression.

519

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527

528

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