

1 A Domain-general Cognitive Core defined in 2 Multimodally Parcellated Human Cortex

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11 **Abstract**

12 Countless brain imaging studies document “multiple-demand” (MD) regions co-activated
13 by a broad domain of tasks, but with little consensus over exact anatomy and functional
14 properties. To overcome these limitations, we use data from 449 subjects from the
15 Human Connectome Project, with cortex of each individual parcellated using
16 neurobiologically grounded multi-modal MRI features. In contrast to unfocused swathes
17 of activation, the conjunction of three cognitive contrasts reveals a core of 10 widely
18 distributed MD regions per hemisphere that are most strongly activated and functionally
19 interconnected, surrounded by a penumbra of 17 further regions. Subcortically, MD
20 activity is seen especially in the caudate and cerebellum. Comparison with canonical
21 resting state networks shows MD regions concentrated in the fronto-parietal network but
22 extending into three other networks. MD activations show modest relative task
23 preferences accompanying strong co-recruitment. With precise anatomical delineation,
24 we offer a basis for cumulative study of MD functions and their role in the assembly of
25 flexible cognitive structures.

26 **Keywords**

27 Multiple-demand; multi-modal; cortical parcellation; executive functions; cognitive
28 control; working memory; reasoning; math; fronto-parietal; resting state; domain-
29 general.

30 Introduction

31 Thought and behavior can be conceptualized as complex cognitive structures within
32 which simpler steps are combined to achieve an overall goal (Luria, 1966; Miller et al.,
33 1968; Newell, 1990). Each step or cognitive episode involves a rich combination of
34 relevant external and internal inputs, computations, and outputs, assembled into the
35 appropriate relations as dictated by current needs. A system capable of such behavior
36 must be equipped with a flexible control structure that can appropriately select, modify
37 and assemble each cognitive step on demand.

38 In line with a system's role in organizing complex cognition, selective damage to specific
39 regions in the frontal and parietal cortex is associated with disorganized behavior (Luria,
40 1966; Milner, 1963; Norman and Shallice, 1986), including significant losses in fluid
41 intelligence (Duncan et al., 1995; Glascher et al., 2010; Roca et al., 2010; Warren et al.,
42 2014; Woolgar et al., 2018, 2010). Numerous functional neuroimaging studies converge
43 on a similar set of frontal and parietal regions that are co-activated when performing a
44 diverse range of cognitively demanding tasks, including selective attention, working
45 memory, problem solving, response inhibition and much more (Cole and Schneider,
46 2007; Duncan and Owen, 2000; Fedorenko et al., 2013; Hugdahl et al., 2015). We refer
47 to this network of regions as the multiple-demand (MD) system, reflecting their co-
48 recruitment by multiple task demands (Duncan, 2013, 2010). MD activity is commonly
49 seen in lateral and dorsomedial prefrontal cortex, in the anterior insula, and within and
50 surrounding the intraparietal sulcus, with an accompanying activation often reported
51 near the occipito-temporal border. Many resting-state fMRI (rfMRI) studies report a
52 similar (but not identical as we will demonstrate) "fronto-parietal" network whose
53 components show strongly correlated time series (Ji et al., 2019; Laumann et al., 2015;
54 Power et al., 2011; Yeo et al., 2011), parts of which are proposed to act as
55 communication hubs owing to their connectivity patterns with other cortical networks
56 (Gordon et al., 2018; Power et al., 2013). Cortical MD regions are also associated with
57 subcortical regions that are co-activated across multiple tasks and are strongly
58 functionally connected with the MD cortex. Though much less studied, these are
59 putatively distributed in restricted sub regions of the basal ganglia, thalamus and
60 cerebellum (Buckner et al., 2011; Choi et al., 2016; Halassa and Kastner, 2017).

61 In non-human primates, fMRI studies have identified a putative cortical MD network
62 organized in anatomically similar and likely evolutionarily homologous regions (Ford et
63 al., 2009; Mitchell et al., 2016; Premereur et al., 2018). Single-neuron studies in these
64 regions reveal highly dynamic and adaptive neural activity patterns that encode many
65 kinds of task-relevant information such as stimulus features, goals, actions, rules and
66 rewards (Duncan, 2001; Miller and Cohen, 2001; Stokes et al., 2013). Further, these
67 neurons are characterized by their mixed selectivity, i.e., activity driven by complex
68 conjunctions of relevant stimuli, processes and task events (Fusi et al., 2016; Naya et
69 al., 2017; Rigotti et al., 2013; Sigala et al., 2008). With access to many kinds of
70 information, adaptive neural activity, and conjunctive coding of task-relevant

71 information, the MD system is well positioned to assemble the rich, integrated control
72 structures of complex behavior (Duncan, 2013). Like a skeleton, the MD system is
73 hypothesized to support the assembly of each task episode by integrating processing in
74 multiple brain regions to access and bind the required information and cognitive
75 operations (Dehaene et al., 1998; Desimone and Duncan, 1995; Miller and Cohen,
76 2001; Norman and Shallice, 1986).

77 While MD activity has been reported since the early days of human brain imaging
78 (Duncan and Owen, 2000), there remains little consensus over core questions including
79 the precise anatomy of MD regions, their differentiation from nearby regions with quite
80 different functional properties, their functional specializations and their connectivity. In
81 large part, we suggest, the lack of cumulative progress reflects the absence of a clear
82 and detailed anatomy of MD activity, with results usually described in terms of large,
83 loosely-defined regions such as “dorsolateral prefrontal cortex”. This lack in precise
84 anatomy is the product of traditional fMRI analysis methods, based on volume-based
85 registration methods in part driven by cortical folds, and the employment of substantial
86 data smoothing that blurs the data. Coupled with the fact that cortical folds vary
87 substantially across individuals, even in twins (Glasser et al., 2016b; Van Essen et al.,
88 2012), and functional areas often do not respect cortical folds (Amunts et al., 2000;
89 Coalson et al., 2018), this has led to significant limitations in relating function to
90 structure in the brain using traditional approaches. Region of interest (ROI) methods
91 can be valuable in identifying individual differences in functional localization, but their
92 definitions are typically based on statistical thresholds that do not necessarily conform
93 to neurobiological criteria. Furthermore, for many questions there are no consensus
94 ROIs, thus limiting comparison and integration of results across studies.

95 To address these issues, we localized MD activity in relation to the recent state-of-the-
96 art multi-modal Human Connectome Project (HCP) parcellation of human cortex
97 (Glasser et al., 2016a). The HCP cortical parcellation relies on high quality multimodal
98 MRI features (cortical thickness, myelin content, rfMRI connectivity, task fMRI activity),
99 along with surface-based analysis methods (Coalson et al., 2018; Glasser et al., 2016b,
100 2013) and new areal-feature-based registration algorithms (Robinson et al., 2018,
101 2014), to parcellate human cortex into 360 regions (180 per hemisphere). Areal
102 delineations were derived from overlapping multi-modal criteria, and areas were named
103 using correspondence with the neuroanatomical literature where possible, bringing a
104 consistent basis in neurobiology and potentially improved comparison with homologous
105 regions in other species.

106 We analyzed data from 449 HCP subjects, each having a defined individual-specific
107 cortical parcellation. Combining data from 3 task contrasts that tap into working
108 memory, relational reasoning, and arithmetic, we determined which areas show MD
109 properties and examined their functional profiles, patterns of resting state connectivity,
110 and relations to subcortical structures. Our results reveal an extended, largely
111 symmetrical MD network of 27 cortical areas, distributed across frontal, parietal and

112 temporal lobes. We divide this extended MD system into a core of 10 regions most
113 strongly activated and strongly interconnected, plus a surrounding penumbra, and we
114 relate this functional division to canonical resting state networks also derived from HCP
115 data (Ji et al., 2019). Across the extended MD system, activation profiles for our 3 task
116 contrasts suggest a picture of substantial commonality, modulated by modest but highly
117 significant functional differentiations. MD activation, and strong connectivity with the
118 cortical MD core, are also identified in several subcortical regions. Our results define a
119 highly specific, widely distributed and functionally interconnected MD system, which we
120 suggest forms an integrating core for complex thought and behavior.

121 **Results**

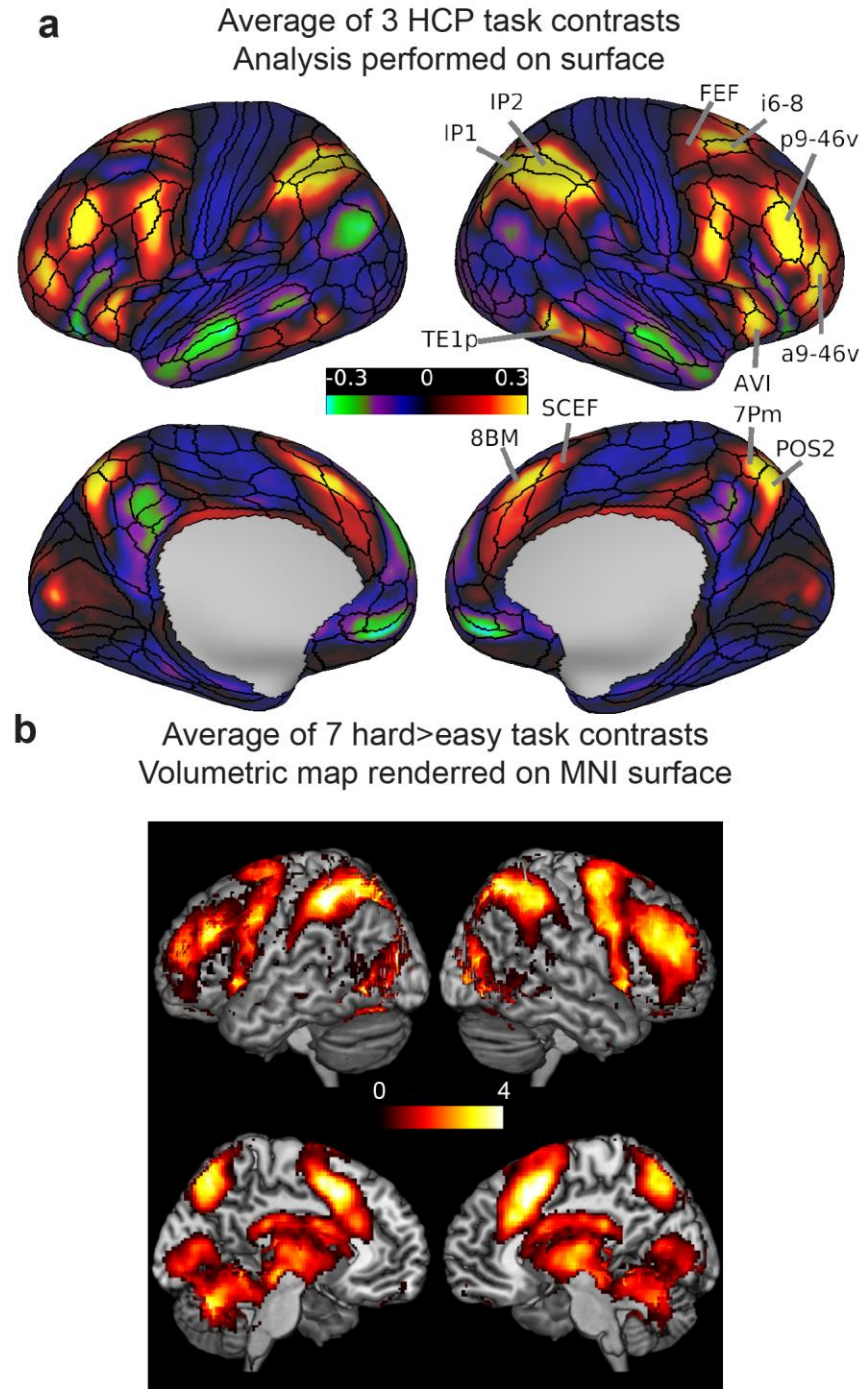
122 We analyzed a cohort of 449 HCP subjects (**for details on data acquisition and**
123 **preprocessing see Methods sections 1-4**). For our major analysis, each subject's
124 cerebral cortex was parcellated into 360 regions (180 per hemisphere) corresponding to
125 the HCP Multi-Modal Parcellation (MMP) 1.0. Parcellation used an automated classifier
126 to define the borders of each area based on learned features from multiple MRI
127 modalities, including cortical thickness, myelin content, rfMRI connectivity and task fMRI
128 activations (**see Methods section 5**). Subject-specific parcellation ensured that task
129 and rest fMRI signals extracted from the defined areas would respect individual
130 differences in their sizes, shapes and locations even in the case of subjects with
131 atypical topologic arrangements.

132 The analysis was based on three suitable fMRI contrasts available in the HCP data:
133 working memory 2-back versus 0-back (WM 2bk>0bk), hard versus easy relational
134 processing (Relational H>E), and math versus story (Math>Story). The first two are
135 standard hard>easy contrasts as commonly used to define MD activity (Duncan and
136 Owen, 2000; Fedorenko et al., 2013). Math>story was added because previous results
137 show a strong MD-like activation pattern associated with arithmetic processing (Amalric
138 and Dehaene, 2017, 2016). For working memory and relational processing, stimuli were
139 visual, whereas for math>story, stimuli were auditory.

140 **Cortical organization of the MD system at the group level**

141 Before considering subject-specific areal analyses, we generated an overview of
142 potential MD areas by calculating a group average MD map. For this, we simply
143 averaged the group average beta maps of the 3 task contrasts and overlaid the
144 resulting combined map on the HCP MMP 1.0 parcellation (**Figure 1a; see also Figure**
145 **S1 for each contrast separately**). Group average maps were generated by aligning
146 each subject's multi-modal maps using areal-feature-based surface registration
147 (MSMAll, Robinson et al 2014; 2018; **see Methods section 4**). MSMAll registration is
148 not substantially driven by cortical folding patterns but instead utilizes myelin and
149 connectivity features to significantly improve the alignment of areas across subjects,
150 with peak probability overlaps reaching >90% for most areas (Coalson et al., 2018),
151 thus allowing us to identify putative areas with MD properties.

152 **Figure 1a** shows the resulting overview. To allow a visual comparison, **Figure 1b**
153 shows a previous MD group-average volumetric map, created by the conjunction of 7
154 hard>easy task contrasts (Fedorenko et al., 2013). Though the two maps are similar,
155 these data emphasize the improved definition obtained with the HCP data and surface-
156 based and areal-feature-based registration methods. On the lateral frontal surface are
157 several clearly distinct activations that show strong bilateral symmetry, with surrounding
158 inactive regions. Tight bands of MD activity are also identifiable in dorsomedial frontal
159 cortex, along the depths of the intraparietal sulcus spreading up to the gyral surface,
160 with an additional restricted region of MD activity in the dorsomedial parietal lobe. The
161 MD region often reported at the occipito-temporal border is also clearly defined in
162 posterior temporal cortex. Even based on these average data, the improved co-
163 registration of the HCP data allows clearer delineation of functional regions, as
164 predicted by Coalson et al., 2018. Rather than broad, fuzzy swaths of MD activity, these
165 data suggest a highly specific but anatomically distributed network of MD regions.



166

167 **Figure 1. (a)** Average of the 3 HCP group average task contrasts (WM 2bk>0bk,
168 Relational H>E, Math>Story). Values are beta estimates. Black contours correspond to
169 the HCP multi-modal parcellation MMP_1.0 (210V) areal borders. **(b)** MD map from
170 Fedorenko et al. (2013) computed by averaging 7 hard>easy task contrasts (2mm
171 smoothed). Values are t-statistics. Data available at <http://balsa.wustl.edu/XXXX>.

172 **Definition of extended and core MD regions using subject-specific cortical**
173 **parcellation**

174 We next analyzed mean activation values extracted from each subject-specific area. We
175 averaged beta values across vertices within each area, yielding one value per area per
176 subject. For each of our 3 behavioral contrasts, we identified areas with a significant
177 positive difference across the group of 449 subjects ($p < 0.05$, Bonferroni corrected for
178 180 areas). To improve signal-to-noise ratio (SNR), we leveraged the symmetry
179 between hemispheres (see **Figure S2**) and averaged areal activations across
180 hemispheres.

181 The conjunction of significant areas across the 3 contrasts revealed a set of twenty-
182 seven areas, which we will refer to as the extended MD system (**Figure 2a**; note that
183 average activations from the two hemispheres are projected onto the left). The
184 distribution of the areas closely matches the activations observed in **Figure 1a** and has
185 broad similarity to previous characterizations of MD activity but with substantially
186 improved anatomical precision and several novel findings.

187 On the dorsal lateral frontal surface, we identify area i6-8 which is immediately anterior
188 to area FEF (a common label given to activations in this region). i6-8 is a newly defined
189 area in the HCP MMP1.0, in the transitional region between classical BA6 and BA8.
190 Localization of MD activity in i6-8, rather than FEF, suggests distinctness from
191 activations driven simply by eye movements in complex tasks. In the HCP MMP1.0,
192 FEF is clearly defined as a distinct area from i6-8 based on several criteria including its
193 anatomical location just anterior to the eye-related portion of the motor cortex and its
194 strong functional connectivity with the LIP/VIP visual complex and the premotor eye field
195 area (PEF) (Glasser et al., 2016).

196 Near the frontal pole, we identify area a9-46v as a strongly active MD region, separated
197 from the posterior region p9-46v. This separation confirms prior indications of a distinct
198 anterior MD frontal region (**see Figure 1b**). Both a9-46v and p9-46v areas overlap with
199 area 9-46v as delineated cyto-architectonically by Petrides and Pandya (1999) but here
200 are separated into anterior and posterior portions by intervening areas that differ in their
201 myelin and functional connectivity profiles (Glasser et al., 2016). Posterior to p9-46v is a
202 further focus of activity in IFJp, with weaker activity in the surrounding regions 8C and
203 6r.

204 In the anterior insula, we identify AVI and an adjacent region of the frontal operculum,
205 FOP5. AVI overlaps with superior portions of the architectonic area lai of Öngür et al.,
206 2003 (see Glasser et al., 2016). Previous work has attempted to distinguish activity in
207 the anterior insula from the adjacent frontal operculum, with the peak often near the
208 junction of the two (Amiez et al., 2016). In our data, AVI is the more strongly activated.

209 While previous characterizations of parietal MD activity have focused on the
210 intraparietal sulcus, our results reveal a much more detailed picture, with strongest MD
211 activation in regions of the intraparietal sulcus (IP1, IP2 and PFM), surrounded by the

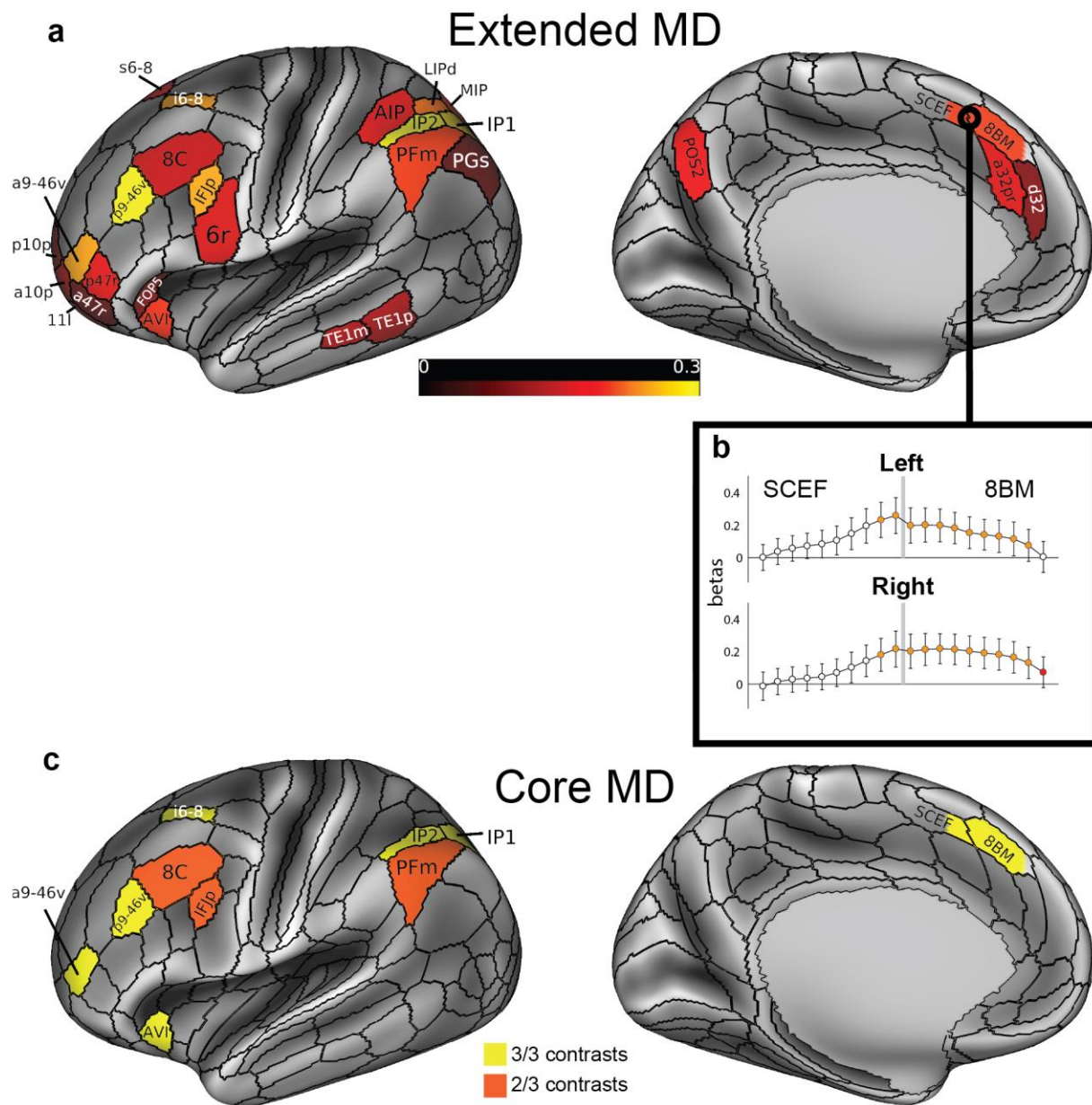
212 relatively weaker MD areas dorsally (AIP, LIPd, MIP) and ventrally (PGs). On the dorso-
213 medial parietal surface, data have sometimes hinted at an additional MD region on the
214 dorsomedial surface (see **Figure 1b**). Here we robustly identify the area POS2, a newly
215 defined area in the MMP1.0 that differs from its neighbours in all major multi-modal
216 criteria.

217 On the lateral surface of the temporal lobe we identify two further areas, TE1m and
218 TE1p. In many previous studies, fronto-parietal MD activity has been accompanied by a
219 similar region of activity in temporo-occipital cortex (e.g. Fedorenko et al., 2013). In
220 many cases, a reasonable interpretation would be higher visual activity, reflecting the
221 visual materials of most imaging studies. In the current study, however, the arithmetic
222 task was auditorily presented, while the other two contrasts were visual, suggesting a
223 genuine MD region.

224 In **Figure 1a**, the dorso-medial frontal activation spans the border between 8BM/SCEF.
225 In the individual-subject analysis, however, SCEF was not significantly activated across
226 all 3 contrasts. We thus investigated whether the activation indeed spans the border
227 between the two areas. For each subject, we divided each of the two areas into 10
228 equal segments along their anterior to posterior extent. **Figure 2b** shows that activation
229 in this region starts to build up midway along SCEF, peaks at the border and is
230 sustained throughout 8BM. We then tested whether each segment would survive as an
231 extended MD region on its own. Indeed, all 8BM segments (except for the one most
232 anterior segment on the left hemisphere) survived, whereas only the anterior 2
233 segments of SCEF were statistically significant (**Figure 2b**; see **Figure S3** for further
234 independent evidence of heterogeneity around the 8BM/SCEF border). Based on these
235 results, for subsequent analyses we combined the statistically significant segments of
236 8BM and SCEF into a single 'area' labelled 8BM/SCEF.

237 To further identify the most active areas within the extended MD system, for each
238 contrast we identified areas with activation stronger than the mean across the full set of
239 27 regions (one sample t-test, $p < 0.05$, Bonferroni correction for the 27 extended MD
240 areas). Seven areas were significant in all three contrasts: i6-8, p9-46v, a9-46v,
241 combined 8BM/SCEF area (see below), AVI, IP2 and IP1. Three more areas were
242 significant in two of the three contrasts (**Figure 2c**): IFJp (relational processing and
243 math), 8C and PFm (working memory and relational processing). We refer to this group
244 of areas as the core MD system, with remaining areas of the extended MD system
245 termed the MD penumbra.

246 Overall, these results identify an extended set of domain-general MD regions. The
247 precise subject-specific areal definitions allowed the identification of several novel areas
248 and improved localization of previously known ones. In the following sections, we further
249 explore the functional properties of core and penumbra regions.



250

251 **Figure 2. (a)** The extended MD system: conjunction of significant areas across 3
 252 functional contrasts. Areal colors reflect average betas across the 3 contrasts. Data are
 253 averaged across hemispheres, and for illustration projected here onto the left. **(b)**
 254 Pattern of activity in regions SCEF (posterior) and 8BM (anterior), divided into posterior
 255 to anterior segments. Grey bar indicates 8BM/SCEF border. Orange indicates segments
 256 that are part of the extended MD system when activity from both hemispheres is
 257 combined (i.e. segments with activity significantly above zero in all 3 behavioral
 258 contrasts). Red indicates one additional segment that survives as part of the extended

259 MD system when activity from each hemisphere is tested separately. **(c)** The core MD
260 system: areas with activity estimates that were significantly higher than the mean
261 activity of all extended MD areas in all 3 contrasts (yellow) and 2 out of 3 contrasts
262 (orange). Data available at <http://balsa.wustl.edu/XXXX>.

263 **Functional connectivity of the multiple-demand cortex and its relation to resting-**
264 **state networks**

265 Next we investigated functional connectivity patterns within the MD network and in
266 relation to the rest of the brain using resting state fMRI data (1 hour per subject). A
267 functional connectivity (FC) matrix for each subject was calculated (180x180 areas per
268 hemisphere; full correlation of spatial ICA+FIX and temporal ICA-cleaned time series;
269 **see Methods section 7**). In this analysis, for ease of calculation we retained the
270 original 8BM and SCEF areas, considering only 8BM as core and SCEF as penumbra.

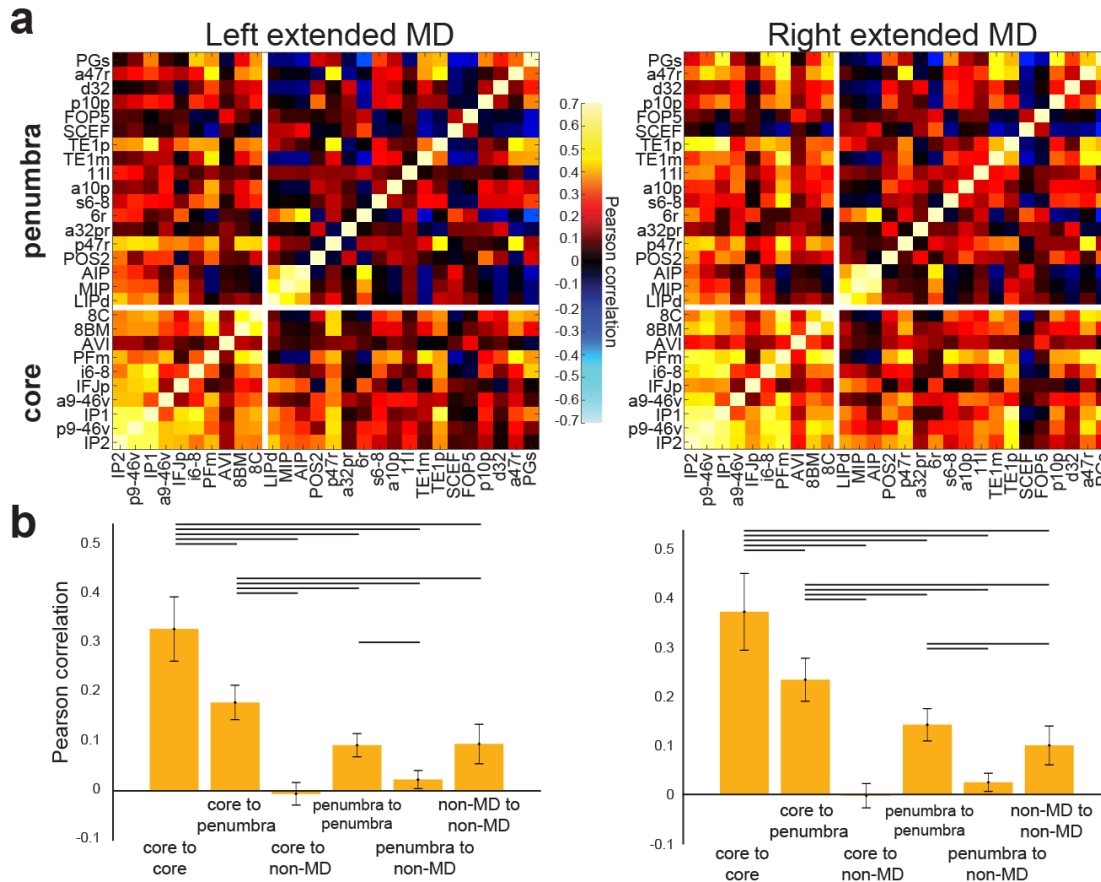
271 **Figure 3a** shows the group average connectivity matrix for the extended MD system,
272 separated into core and penumbra. Despite their wide spatial separation, core MD
273 areas show stronger functional connectivity with each other than with the penumbra. To
274 test the robustness of these patterns, for each subject we calculated mean values for 6
275 different types of cortical connections and compared them using multiple paired sample
276 t-tests (**Figure 3b; see Methods section 7**). In both hemispheres, functional
277 connectivity between core MD regions was significantly stronger than both their
278 connectivity with the penumbra (left $t(448)= 93.1$, right $t(448)= 79.4$), and the internal
279 penumbra connectivity (left $t(448)= 79.4$, right $t(448)= 66.3$). Mean connectivity of both
280 core and penumbra MD areas with the remainder of the brain were near zero.

281 We next investigated the spatial similarity between the MD network defined from our
282 conjunction of 3 task contrasts and canonical fMRI resting state networks. For this
283 purpose, we utilized the recent Cole-Anticevic Brain Network Parcellation (CAB-NP)
284 which analyzed resting state data from 337 HCP subjects and identified network
285 communities across HCP MMP1.0 areas (Ji et al., 2019). A comparison of the extended
286 MD and the CAB-NP network parcellation (**Figure 4a**) suggests points of both
287 convergence and divergence. Strikingly, all core MD areas lie within the fronto-parietal
288 network (FPN) of CAB-NP (**Figure 4a, top left**). In contrast, penumbra MD areas
289 occupy portions of four networks: FPN, cingulo-opercular network (CON), dorsal
290 attention network (DAN) and the default mode network (DMN) (**Figure 4a, top right**).
291 Importantly, examination of the whole CAB-NP FPN network shows most but not all
292 areas within the MD core or penumbra (left FPN: 10 core, 10 penumbra, 8 non-MD;
293 right FPN: 10 core, 8 penumbra, 4 non-MD) (**Figure 4a, bottom**).

294 To emphasize the central role of core MD, we again compared different connectivity
295 subgroups (**Figure 4b**; paired sample t-tests, $p < 0.05$, Bonferroni corrected). Within the
296 FPN, we found that connections between core MD regions stand out strikingly in their
297 strength relative to their connectivity with other FPN regions (core-core with core-
298 penumbra: left $t(448)= 60.8$, right $t(448)= 41.6$; and core-core with core-non-MD FPN
299 regions: left $t(448)= 87.7$, right $t(448)= 80.1$). Further within the FPN, core-penumbra
300 connections are stronger than core-non-MD connections (left $t(448)= 57.7$, right $t(448)=$
301 72.4). Second, we examined connectivity of core MD regions, all lying within FPN, to
302 penumbra and non-MD regions within each of DAN, CON and DMN. The results again
303 highlight a consistent pattern of stronger connectivity between core and penumbra MD

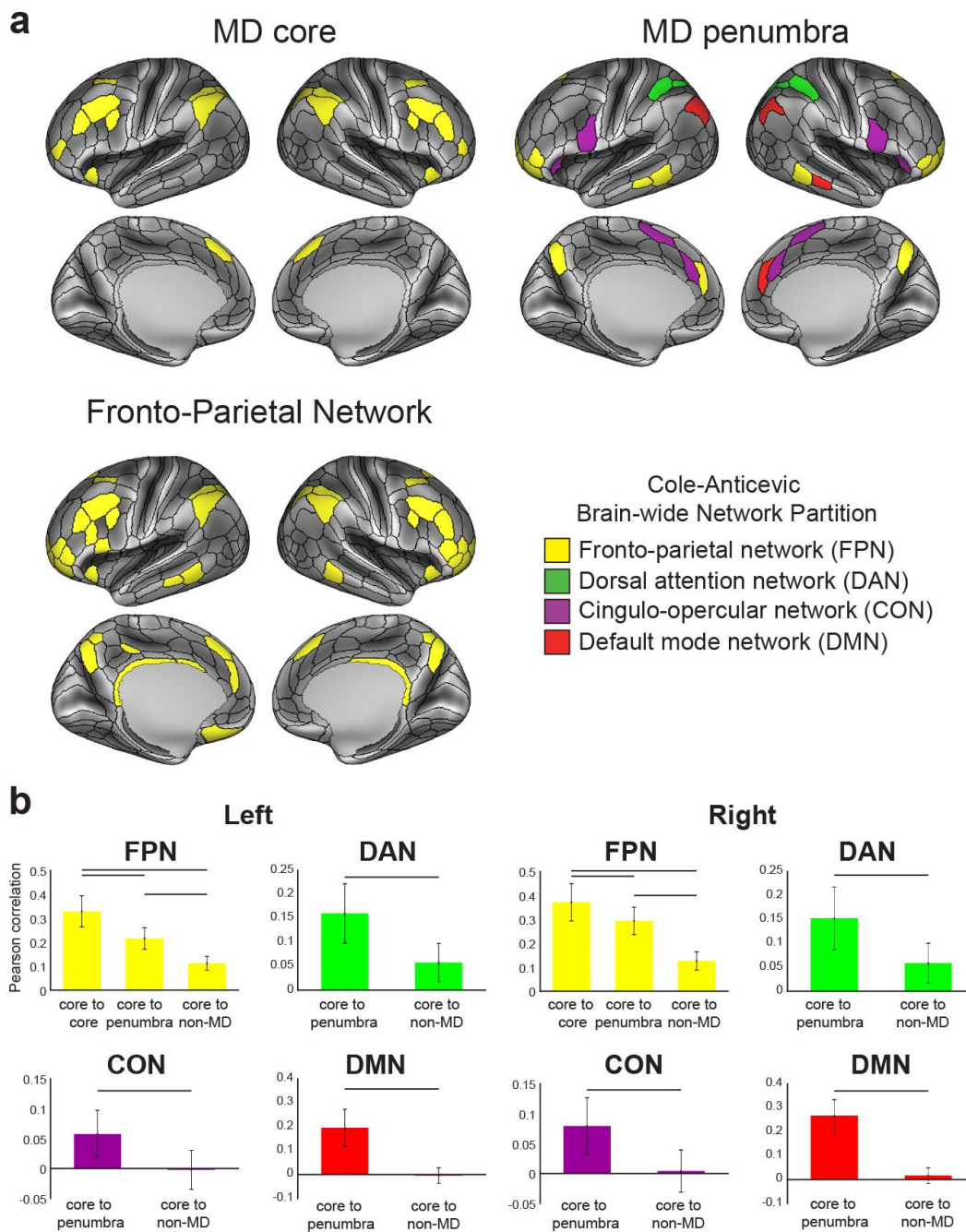
304 regions vs core and non-MD regions within each of the three networks (DAN (left
305 $t(448)= 46.5$, right $t(448)= 41.1$), CON (left $t(448)= 36.3$, right $t(448)= 42.3$) and DMN
306 (left $t(448)= 67.9$, right $t(448)= 86.1$) (**Figure 4b**).

307 While these results show substantial overlap between MD and FPN – especially for MD
308 core – they also indicate additional structure revealed by the FC data. Connectivity is
309 especially strong between regions within the extended MD system, and strongest
310 between core regions within the canonical FPN. Strong functional connectivity,
311 especially for the core, suggests a suitable architecture for widespread integration of
312 distributed brain states.



313

314 **Figure 3.** Functional connectivity (FC) of the MD system. **(a)** FC (Pearson correlation)
 315 across the MD system. Regions of the extended MD system are separated into core
 316 and penumbra, with regions within each set ordered by mean activation (beta) across
 317 our 3 functional contrasts. Note the strength of core MD connectivity (lower left box) vs
 318 penumbra connectivity (upper right box). **(b)** Statistical comparison (paired sample t-
 319 test) between different groups of connections. Lines highlight a statistically significant
 320 difference ($p < 0.05$, Bonferroni corrected for 30 comparisons). Data available at
 321 <http://balsa.wustl.edu/XXXX>



322

323 **Figure 4. MD system and resting state networks (a)** Resting state network assignments
 324 from the Cole-Anticevic Brain-wide Network Parcellation (CAB-NP; Ji et al., 2018) for
 325 the core (left) and penumbra (middle) MD areas, compared to the whole CAB-NP
 326 fronto-parietal network (FPN). **(b)** Statistical comparison (paired sample t-test) of
 327 connection types for each CAB-NP network. Data available at
 328 <http://balsa.wustl.edu/XXXX>

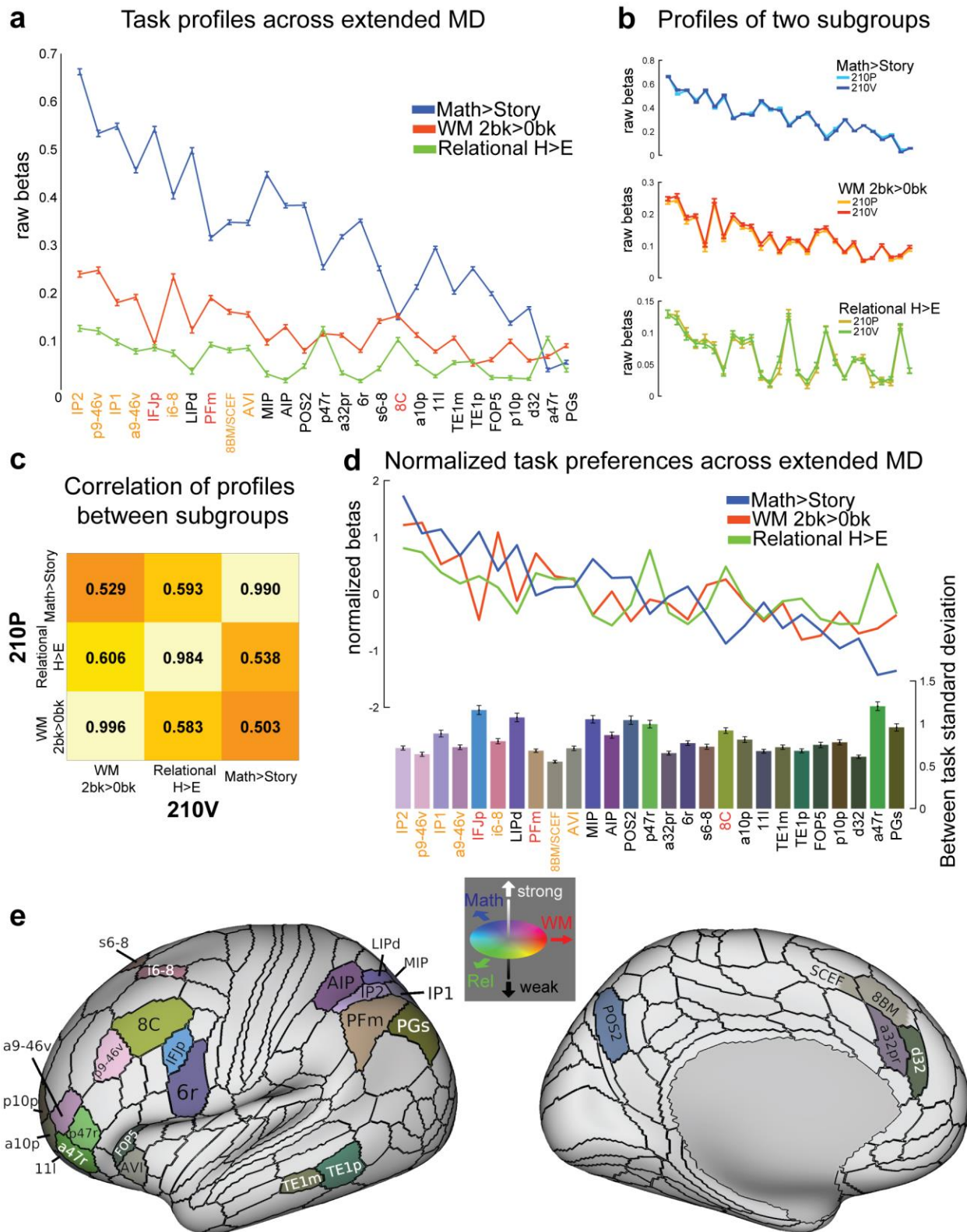
329 **Task profiles across the multiple-demand cortex**

330 By definition, every MD area showed a significant positive result in each of our 3
331 behavioral contrasts. Across areas, nevertheless, we explored relative preferences for
332 one contrast over another. To evaluate this quantitatively, **Figure 5a** shows the mean
333 response of each area (averaged across hemispheres) for each contrast.
334 Predominantly, the picture is one of consistency. For nearly all areas, activation was
335 strongest for the math>story contrast, and weakest for hard>easy relational processing.
336 Against this general background, however, there was also differentiation between
337 profiles, with varying patterns of peaks and troughs.

338 To test the robustness of these patterns, we compared activation profiles in two
339 independent groups of subjects (210P and 210V, the parcellation and validation groups,
340 respectively, used to create the HCP MMP1.0 in Glasser et al., 2016), constructed to
341 avoid shared family membership. As shown in **Figure 5b**, the activation profile for each
342 contrast is almost identical for the two groups. **Figure 5c** quantifies this by correlating
343 activity profiles (**in Figure 5b**) for the two subject groups. Very high correlations on the
344 diagonal ($r > 0.98$) highlight how the precise pattern of activation for a given contrast is
345 very stable when averaged over many individuals. Off-diagonal correlations are much
346 lower ($r \sim 0.5-0.6$). Although all tasks engage all MD areas, there remains considerable
347 and highly consistent inter-areal diversity in precise activation patterns.

348 To illustrate this inter-areal diversity between the three contrasts, we plotted the
349 normalized profile for each contrast (**line plots in Figure 5d**). For each contrast and
350 each subject, we z-scored activations across MD regions, then averaged the z-scores
351 across subjects. For each region, bar heights (**Figure 5d, bottom**) show the standard
352 deviation of these normalized z-scores across tasks, separately calculated for each
353 subject and then averaged over subjects. Bars were also colored to highlight the relative
354 task preferences (see **Figure 5e**, where the same colors are projected onto the cortical
355 surface).

356 The results reveal a diversity of relative task preferences across the extended MD
357 network. Relative preference for relational reasoning (green) occurs in a cluster of
358 anterior frontal areas inferior to the core region a9-46v, as well as in 8C. Dorsal frontal
359 regions (e.g. i6-8 and s6-8) show relative preference for working memory, whereas
360 dorsal parietal regions (AIP/LIPd/MIP, and POS2) show relative preference for math.
361 Other relative preferences occur across most regions. Despite relative consistency
362 across the entire extended MD network – with the strongest activation for Math>Story,
363 and weakest for relational processing – there is also clear evidence of relative functional
364 specialization, with each area showing modest but consistent relative preference for one
365 contrast over another.



367 **Figure 5.** Task profiles across the MD system. **(a)** Raw activation estimates (betas) for
368 each contrast. Areas are sorted from left to right according to the strength of their MD
369 response (average across the 3 contrasts). Error bars represent SEM. Core MD areal
370 labels are colored in orange (survived in all 3 contrasts) and red (survived in 2 out of 3
371 contrasts). **(b)** Task profiles for two independent groups of subjects (210P and 210V).
372 **(c)** Correlation of task profiles between groups. **(d)** Normalized task profiles across the
373 MD system as line plots. Bar heights represent between-task standard deviation,
374 separately calculated for each subject and averaged over subjects. Bar colors indicate
375 relative preferences between tasks. Color wheel indicates red for working memory
376 (WM), green for relational processing (Rel), and blue for math. Intermediate colors show
377 mixed preferences. Brighter and darker colors reflect stronger and weaker MD
378 activation, respectively. **(e)** Cortical projection of the RGB color weighted normalized
379 task profiles. Data available at <http://balsa.wustl.edu/XXXX>

380 **Subcortical components of the multiple-demand system**

381 To identify the subcortical components of the MD system we used the same 3
382 behavioral contrasts used for cortical areas. Each subcortical structure was segmented
383 separately for every subject (**see Methods section 4**), thus avoiding mixing signals
384 from nearby structures or white matter. For each structure, we first identified the
385 significantly activated voxels for each contrast separately (one sample t-test, FDR
386 corrected for each structure separately, $p < 0.05$) and then identified the conjunction of
387 significant voxels across the three contrasts. This revealed activation regions bilaterally
388 mainly in the caudate nucleus and cerebellum. Caudate activation peaked in the head
389 and spread into the body (**Figure 6a, left panel**). Cerebellar activation included
390 separate medial and lateral portions of crus I and II (on dorsal and ventral lateral
391 surface) (**Figure 6a, right panel**). Activations appear to be largely symmetrical across
392 hemispheres.

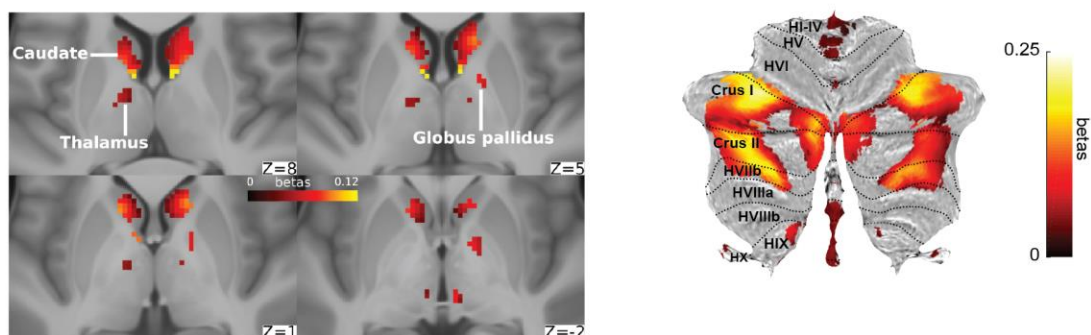
393 We identified two additional small regions in the thalamus bilaterally (antero-medial
394 portion) and the anterior portion of the right globus pallidus (**Figure 6a**). Interestingly,
395 larger bilateral portions of the thalamus (anterior dorso-medial), putamen (dorso-
396 anterior/mid portion) and globus pallidus (dorso-anterior portion) were significantly
397 activated in only two contrasts (working memory and math) and were deactivated in the
398 relational processing contrast.

399 In a parallel analysis using resting state data, we aimed to identify the subcortical voxels
400 showing significant functional connectivity with the cortical core MD areas. For this
401 analysis we used the group average dense FC matrix for half of the subjects (210V
402 group) (**see Methods section 7**). **Figure 6b** shows the statistically significant
403 subcortical voxels (FDR corrected, $p < 0.05$). The patterns follow closely the task-
404 identified regions in the caudate nucleus and cerebellum bilaterally. In addition, FC
405 analysis identified significant voxels in bilateral portions of the thalamus (anterior dorso-
406 medial), putamen (dorso-anterior/mid portion) and globus pallidus (dorso-anterior
407 portion), similar to the regions activated in the working memory and math contrasts.

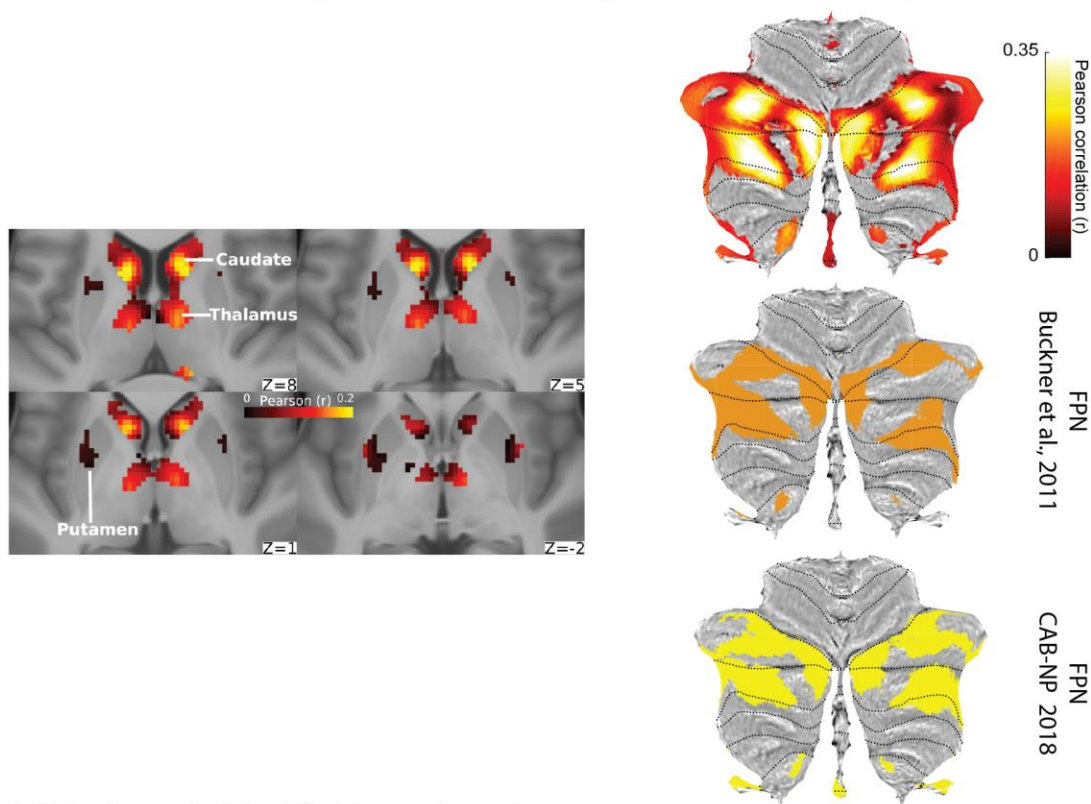
408 We were able to further compare the MD cerebellar regions with the fronto-parietal
409 network (FPN) identified by resting state data from two studies: Bucker et al 2011 (7
410 networks parcellation results from 1000 subjects) and CAB-NP (Ji et al., 2018; results
411 from 339 HCP subjects). **Figure 6b (right panel)** illustrates the strong similarity
412 between the FPNs from both studies and the cerebellar MD hotspots in crus I and II.

413 Due to the lack of individually defined nuclei within each subcortical structure, we
414 measured the degree of overlap between the task vs rest identified MD regions, within
415 each structure, at the group average level. Almost all task-identified MD voxels in
416 caudate, cerebellum and thalamus (except right thalamus) were also detected in the
417 resting state data. Thus, together, task and rest fMRI data converge on identifying a
418 strongly connected subcortical domain related to the cortical MD core.

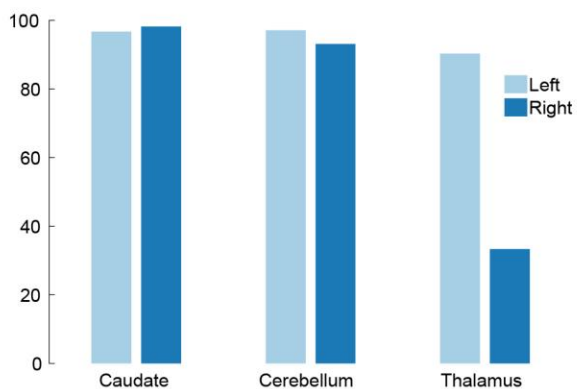
a Task-identified MD voxels (conjunction of the 3 contrasts)



b Rest-identified MD voxels (functional connectivity with cortical MD core)



c % MD task voxels identified by rest voxels



420 **Figure 6.** Subcortical MD components. **(a)** Left: Conjunction of significant voxels across
421 the three tasks. Right: Cerebellar activity is projected on a flat cerebellum with lines
422 representing anatomical borders (Diedrichsen and Zotow, 2015). **(b)** Left: Subcortical
423 voxels with significant connections to the cortical core MD areas. Right: *(top)* Cerebellar
424 MD connectivity projected on a flat map. *(middle)* FPN from Buckner et al. (2011).
425 *(bottom)* FPN from Ji et al. (2018). **(c)** Percentage of task MD voxels also identified by
426 resting connectivity with MD core. Data available at <http://balsa.wustl.edu/XXXX>

427 **Discussion**

428 In this study, we used the HCP MMP1.0 cortical parcellation, based on neurobiologically
429 grounded multi-modal MRI features, to demonstrate that diverse cognitive tasks from
430 different sensory modalities engage a widely distributed multiple-demand (MD) network
431 of relatively few areas, in the frontal, parietal and temporal cortices. We identified a set
432 of core regions, characterized by their strong activation and interconnectivity,
433 surrounded by a penumbra, with relatively weaker activations and interconnectivity. We
434 also isolated a set of localized subcortical MD regions, especially in the caudate nucleus
435 and cerebellum, which share strong connectivity with the cortical core MD.

436 Our use of subject-specific cortical parcellation provides compelling evidence for the
437 existence of highly specific MD regions in the human brain. The improved anatomical
438 precision offered by the HCP methods disclosed novel findings regarding the
439 anatomical and functional organization of the MD network, as well as the functional
440 connectivity of its components.

441 Why should the brain contain this precise network of MD regions, co-activated during
442 many cognitive activities? On the one hand, MD regions are strongly interconnected,
443 with a widespread and broadly consistent activity profile across tasks. On the other,
444 they are differentiated, with quantitative differences between tasks in precise activity
445 profile. We suggest that this picture is consistent with a system engaged in large-scale
446 integration of brain activity. Within the extended MD system, we propose that the core
447 regions, most strongly active and interconnected, lie at the heart of information
448 integration and exchange. Surrounding penumbra regions, with their connectivity into
449 multiple cortical networks, feed diverse information into the core. Across the entire MD
450 system, co-activation reflects information integration and exchange, while modest
451 functional preferences reflect differential connectivity and information access. Together,
452 these properties allow MD regions, with associated subcortical regions, to build
453 cognitive structures suited to any current task. These proposals are developed and
454 extended in the following sections.

455 **Broad anatomical distribution and relative functional preferences**

456 Our data delineate a highly specific MD network, with core and penumbra components
457 widely distributed across the cortex. Compared to previous data, our results clarify
458 several aspects of this distributed MD pattern.

459 One such clarification concerns activations in the posterior dorsal prefrontal cortex,
460 often seen in prior work (**see Figure 1b**) in a region close to the FEF. With the
461 increased spatial specificity of the current data, we show that MD activation is localized
462 anterior and dorsal to the FEF, including regions i6-8 (core) and s6-8. These results
463 strongly suggest that MD activation is distinct from activations driven simply by eye
464 movements in complex tasks. Both i6-8 and s6-8 show strongest preference for the WM
465 contrast.

466 Near the frontal pole, we localized MD activation in one core region (a9-46v) and 5
467 surrounding penumbra regions. There has been much debate concerning an anterior-
468 posterior gradient of activation on the lateral frontal surface. On the one hand, many
469 tasks produce activation near to the frontal pole, suggesting an MD-like pattern
470 (Ramnani and Owen, 2004). On the other, many studies suggest selective activity in
471 this region, for example associated with abstract reasoning (Bunge et al., 2005;
472 Christoff et al., 2009) or hierarchically-organized cognitive control (Badre, 2008; Badre
473 and Nee, 2018). Our results show that a9-46v is almost as strongly co-activated as
474 more posterior core regions, arguing against a simple gradient of activation. Its adjacent
475 penumbra regions (a47r, p47r) also show clear MD activation but with relative functional
476 preference for the abstract relational reasoning task, matching previous reports of
477 reasoning activation in this region.

478 The combined 8BM/SCEF MD area on the medial frontal surface showed the least
479 functional preference (**Figure 5d**). Our findings show MD activation rising to and
480 peaking at the border between 8BM and SCEF, with similar patterns also visible in other
481 task contrasts and fine-grained analysis of functional connectivity (**Figure S3**). In our
482 group-average map, hints of task activation near areal borders can also be seen at the
483 borders of 8C/IFJp and POS2/7Pm (**Figure 1a**). Though detailed analysis of these
484 functional transitions is beyond our scope here, it is possible that here too MD activation
485 peaks near areal borders. Borders between these areas were defined using robust
486 multiple overlapping functional, architectural and/or topological criteria (Glasser et al.,
487 2016a). Thus, we speculate that our data may reflect close interaction between areas
488 sharing the border, reflecting the general principle of spatial proximity between brain
489 regions that are in close communication.

490 Previously, many studies have revealed a band of occipito-temporal activation
491 accompanying activation of fronto-parietal MD regions (**see Figure 1b**). As most tasks
492 used in these studies have been visual, a plausible interpretation might be top-down
493 input into higher visual areas. In our data we identified two penumbra regions, TE1m
494 and TE1p, in posterior temporal cortex. Since these regions were activated by the
495 auditory as well as the visual contrasts, the interpretation of top-down input into higher
496 visual areas is less plausible. The location of these regions midway between higher
497 visual areas, auditory areas and language and semantic areas (Fedorenko et al., 2011;
498 Pobric et al., 2007; Visser et al., 2010) suggests a genuine MD region, situated to
499 integrate higher visual, auditory and semantic/language processing. Similar to previous
500 findings in Broca's area (see Fedorenko et al., 2012), these data highlight an MD area
501 with close proximity to language regions.

502 Previous studies employing math tasks identify an MD-like pattern that is commonly
503 interpreted as a domain-specific "math network" (Amalric and Dehaene, 2017). Our
504 results show that the math contrast engages all extended MD regions, but with relative
505 preferences among dorsal parietal areas (AIP, LIPd, MIP; and POS2 on the medial

506 surface) and dorsal frontal region IFJp. We note that in our data, math preferences are
507 potentially confounded with auditory preferences (Michalka et al., 2015).

508 Very likely, relative functional specializations reflect differential anatomical connections.
509 While putative homologous MD regions in macaques (Mitchell et al., 2016) share many
510 anatomical connections, each also has its own unique fingerprint of connections to and
511 from other brain regions (Markov et al., 2014; Petrides and Pandya, 1999).
512 Acknowledging the current inadequacy of accurate cross-species mapping, these
513 studies portray a picture of a strongly physically interconnected MD system, with its sub
514 regions differentially connected to other brain areas.

515 On this view, different MD regions are well placed to access different kinds of
516 information. Different tasks, emphasizing different kinds of information lead to partial
517 functional specializations. However, as an integrated cognitive episode is formed, its
518 different contents must be integrated and bound to their functional roles. The rich
519 interconnections between MD regions offer a clear substrate for information exchange
520 and integration.

521 **MD cortex and resting state networks**

522 In this study we identified the extended MD system using a conjunction of three task
523 contrasts. Using MD regions identified from task data, we proceeded to demonstrate
524 strong within-network functional connectivity at rest. As expected, our analysis of resting
525 state data shows much convergence with canonical functional networks derived from
526 the same data (Ji et al., 2019). Within these canonical networks, however, we find
527 additional fine-grained structure. MD core regions constitute a subset of areas within the
528 canonical FPN that are distinguished by especially strong mutual connectivity. This
529 strong connectivity occurs despite wide anatomical separation. In contrast to this core,
530 penumbra regions are distributed across several canonical networks. Again, compared
531 to other regions within those networks, they are distinguished by especially strong
532 connectivity with the MD core. These results support the picture of MD regions as a
533 strong communication skeleton, with penumbra regions in particular drawing together
534 information from several distinct large-scale networks.

535 This conclusion is reminiscent of extensive recent work using network science
536 approaches (e.g., graph theory) to identify putative cortical communication hubs
537 (Bassett and Sporns, 2017; Bertolero et al., 2018; Petersen and Sporns, 2015; Sporns,
538 2014). In this graph theoretic approach, hubs are defined by broad connectivity and/or
539 spatial proximity to multiple cortical networks. Typically they include a set of regions
540 resembling the current MD system, but also others including the temporo-parietal
541 junction, extensive regions of the mid- and posterior cingulate and more (Gordon et al.,
542 2018; Power et al., 2013). These connective findings are broadly consistent with our
543 proposal that MD regions act as an integrative skeleton for cognitive activity, but leave
544 open the question of precise relations between the MD pattern, defined with converging
545 task contrasts, and the definition of hubs based solely on functional connectivity.
546 Because hubs are defined by connectivity with multiple cortical networks, their
547 identification depends on the granularity with which these networks are separated. Such

548 limitations do not apply to definition of MD regions based on converging task contrasts.
549 Further work may help to contrast the functional role of MD regions relative to hubs
550 defined by connectivity but not showing robust activation across multiple diverse tasks.

551 Unique connectivity between MD regions can also be revealed by recent work using
552 temporal ICA (tICA), which generates components that are temporally independent
553 (Glasser et al., 2018a; see also Van Essen and Glasser, 2018). We were able to identify
554 at least one rest and one task tICA component with strong spatial similarity (whole brain
555 absolute Pearson correlation $r = 0.74$ and 0.76 respectively) to the group average MD
556 map from figure 1a (Figure S4). These results demonstrate that the use of automated
557 methods such as tICA has the potential to identify a richer set of brain states, both in
558 rest and task, by imposing temporal but not spatial constraints on the derived
559 components.

560 **Subcortical MD regions**

561 Our data reveal several subcortical MD regions with strong functional connectivity with
562 the cortical MD core. First is the head of the caudate nucleus, also associated with a
563 smaller region in the anterior globus pallidus. In nonhuman primates, the anterior
564 portion of the caudate receives projections from all prefrontal regions (Averbeck et al.,
565 2014). Tracer studies have established that the dorso-lateral prefrontal, dorso-medial
566 prefrontal and parietal cortices, in addition to strong cortico-cortical interconnections,
567 also share converging projections to the caudate, mainly targeting its head, as well as to
568 the globus pallidus (Alexander et al., 1986; Choi et al., 2016; Haber, 2003; Hampson et
569 al., 2006; Kemp and Powell, 1970; Middleton and Strick, 2000; Yeterian and Pandya,
570 1991). Within the striatum, overlap in the projection zones of nearby cortical areas may
571 in part be mediated by interdigitating dendrites and axons that cross functional
572 boundaries (Averbeck et al., 2014; Haber, 2003). These anatomical findings are
573 consistent with the identified MD activations in the head of the caudate and strongly
574 support its putative role in information integration.

575 We also identified distributed MD regions in the cerebellum. Tracer studies identify
576 polysynaptic connections between the prefrontal cortex and the lateral portions of crus I
577 and II as well as vermal lobules VII and IX (see Buckner, 2013 and Ramnani, 2006),
578 largely overlapping with our MD cerebellar regions. In addition, previous studies have
579 implicated similar cerebellar regions in several aspects of complex cognitive activity
580 (King et al., 2018) as well as encoding task-relevant information (Balsters et al., 2013).
581 Importantly, MD cerebellar regions do not overlap with motor-related regions
582 (Diedrichsen and Zotow, 2015). Not surprisingly, there is strong overlap between the
583 cerebellar regions identified here, by converging task contrasts and strong connectivity
584 to the MD cortical core, and the FPN-related cerebellar network defined in previous
585 studies (Buckner et al., 2011; Ji et al., 2019). Importantly, the cerebellar MD regions
586 were identified by connections with the more spatially restricted cortical MD core in
587 comparison with the cortical FPN, further suggesting a central role for the cortical MD
588 core.

589 We also identified putative MD regions in the anterior portion of the thalamus. In this
590 case, small regions identified from our conjunction of task contrasts compare with a
591 larger region identified using resting state connectivity. The connectivity identified
592 thalamic regions are in line with the findings of numerous studies reporting strong
593 anatomical and functional connectivity between thalamic nuclei (especially medio-dorsal
594 portions) and fronto-parietal cortices (Haber, 2003; Halassa and Kastner, 2017). The
595 notably small task-identified parietal MD region reflects deactivation of the majority of
596 parietal cortex in relational reasoning.

597 Further work at higher field MRI strength (e.g., 7T) may help clarify the role of these and
598 other subcortical regions associated with the cortical MD system. Meanwhile, in
599 agreement with known anatomy, our data suggest extensive cortical-subcortical
600 interaction in control of complex cognitive activity.

601 **Creating the structure of complex cognition**

602 In behavior and thought, the richness of even a simple cognitive event, and the precise
603 relations that must be established between different components of that event, call for a
604 widely-connected system, able to access any kind of cognitive content. Our data
605 highlight several properties that suit the MD system to construct complex cognitive
606 episodes. The MD system is made up of regions that are widely dispersed anatomically,
607 yet tightly functionally connected and co-recruited by tasks of many different kinds. Our
608 data identify a core, with the strongest pattern of widespread recruitment and
609 connectivity, supported by a surrounding penumbra.

610 Owing to their differential anatomical and functional connections, different MD regions
611 may be preferentially recruited during tasks with different contents. However, their
612 strong interconnectedness likely allow different information to become quickly integrated
613 and exchanged, leading to a dominant pattern of co-activation. Extensive MD
614 connections to other regions also suggest a broad role in coordinating brain activity in
615 service of the task at hand. This proposal conforms with the finding that the MD system,
616 among different brain networks, is the most striking in changing its global brain
617 connectivity during different task states (Cole et al., 2013).

618 The ability of the MD system to dynamically and broadly represent many kinds of
619 information is supported by numerous human fMRI studies employing multi-variate
620 pattern analysis (MVPA), as well as electrophysiological studies in animals (Miller and
621 Cohen, 2001; Stokes et al., 2013; see Woolgar et al., 2016 for a comprehensive review
622 of MVPA studies). In putative monkey MD regions, many studies identify neurons with
623 mixed selectivity, allowing integration of specific stimuli and specific task contexts
624 (Genovesio et al., 2016; Naya et al., 2017; Parthasarathy et al., 2017; Rigotti et al.,
625 2013; Stokes et al., 2013). Conjunctive coding/mixed selectivity is likely critical in
626 assembling the correct structured relations between the component parts of a cognitive
627 episode (Duncan, 2013; Rigotti et al., 2013).

628 For cumulative progress in understanding brain activity, a basic step is definition of an
629 accepted set of component regions. In the case of MD activity, progress has been slow
630 because we lack such a precise definition, leading to many thousands of studies
631 showing similar activity patterns, but little agreement over questions such as functional
632 similarity/differentiation. Based on the HCP multi-modal parcellation, our work defines a
633 precise network of core MD regions and their surrounding penumbra, and establishes a
634 pattern of widespread co-recruitment, relative functional differentiation, and strong
635 connectivity. Precisely specified MD regions provide a basis for detailed functional
636 investigation, cross-reference between studies, and identification of cross-species
637 homologs. With these results, we lay the groundwork for a new phase in understanding
638 one of the brain's most important, best-known but least understood functional networks.
639

640 **Methods**

641 **1. Subjects**

642 The analyzed dataset consisted of 449 healthy volunteers from the Human Connectome
643 Project (HCP) S500 release. Subjects were recruited from Washington University (St.
644 Louis, MO) and the surrounding area (186 males, 263 females, with age ranges (22-25
645 n=69; 26-30 n=208; 31-35 n= 169; 36+ n=3). Informed consent was obtained from each
646 subject as approved by the institutional review board at Washington University at St.
647 Louis.

648 **2. Image Acquisition**

649 MRI acquisition protocols have been previously described (Glasser et al., 2013; Smith
650 et al., 2013; Uğurbil et al., 2013). All 449 subjects underwent the following scans:
651 structural (at least one T1w and one T2w scan), fMRI (4 runs X 15 minutes), and task
652 fMRI (7 tasks, 46.6 minutes total). Images were acquired using a customized 3T
653 Siemens 'Connectom' scanner having a 100mT/m SC72 gradient insert and using a
654 standard Siemens 32-channel RF receive head coil. At least one 3D T1w MPRAGE and
655 one 3D T2w SPACE image were acquired at 0.7 mm isotropic resolution. Whole brain
656 rfMRI and task fMRI data were acquired using identical multi-band EPI sequence
657 parameters of 2 mm isotropic resolution with a TR=720 ms. Spin echo phase reversed
658 images were acquired during the fMRI scanning sessions to enable accurate cross-
659 modal registrations of the T2w and fMRI images to the T1w image in each subject
660 (standard dual gradient echo fieldmaps were acquired to correct T1w and T2w images
661 for readout distortion). Additionally, the spin echo field maps acquired during the fMRI
662 session (with matched geometry and echo spacing to the gradient echo fMRI data) were
663 used to compute a more accurate fMRI bias field correction and to segment regions of
664 gradient echo signal loss.

665 **3. Task Paradigms**

666 Each subject performed 7 tasks in the scanner over two sessions. In the current study
667 we analyzed data from 3 tasks: working memory (performed in session 1),
668 math/language and relational processing (performed in session 2). Subjects performed
669 2 runs of each task. The following task details are adapted from Barch et al. (2013) on
670 HCP fMRI tasks.

671 *Working Memory*: Each run consisted of 8 task blocks (10 trials of 2.5 s each, for 25 s)
672 and 4 fixation blocks (15 s each). Within each run, 4 blocks used a 2-back working
673 memory task (respond 'target' whenever the current stimulus was the same as the one
674 two back) and the other 4 used a 0-back working memory task (a target cue was
675 presented at the start of each block, and a 'target' response was required to any
676 presentation of that stimulus during the block). A 2.5 s cue indicated the task type (and
677 target for 0-back) at the start of the block. On each trial, the stimulus was presented for
678 2 s, followed by a 500 ms ITI. In each block there were 2 targets, and (in the case of the

679 2-back task) 2–3 non-target lures (repeated items in the wrong n-back position, either 1-
680 back or 3-back). Stimuli consisted of pictures of faces, places, tools and body parts;
681 within each run, the 4 different stimulus types were presented in separate blocks.
682 Subjects had to respond to non-targets using a middle finger press and to targets using
683 an index finger press.

684 *Math/language*: Each run consisted of 4 blocks of a math task interleaved with 4 blocks
685 of a story task. The lengths of the blocks varied (average of approximately 30 s), but the
686 task was designed so that the math task blocks matched the length of the story task
687 blocks, with some additional math trials at the end of the task to complete the 3.8 min
688 run as needed. The math task required subjects to complete addition and subtraction
689 problems, auditorily presented. Each trial had a problem of the form “ $X + Y =$ ” or “ $X - Y$
690 $=$ ”, followed by two choices. The subjects pushed a button to select either the first or the
691 second answer. Problems were adapted to maintain a similar level of difficulty across
692 subjects. The story blocks presented subjects with brief auditory stories (5–9 sentences)
693 adapted from Aesop's fables, followed by a 2-alternative forced choice question that
694 asked the subjects about the topic of the story. The example provided in the original
695 Binder paper (p. 1466) is “For example, after a story about an eagle that saves a man
696 who had done him a favor, subjects were asked, ‘That was about revenge or
697 reciprocity?’”. For more details on the task, see Binder et al. (2011).

698 *Relational Processing*: Stimuli were drawn from a set of 6 different shapes filled with 1
699 of 6 different textures. In the hard condition, subjects were presented with 2 pairs of
700 objects, with one pair at the top of the screen and the other pair at the bottom of the
701 screen. They were told that they should first decide what dimension(s) differed across
702 the top pair of objects (shape or texture) and then they should decide whether the
703 bottom pair of objects also differed along the same dimension(s) (e.g., if the top pair
704 differs only in shape, does the bottom pair also differ only in shape?). In the easy
705 condition, subjects were shown two objects at the top of the screen and one object at
706 the bottom of the screen, and a word in the middle of the screen (either “shape” or
707 “texture”). They were told to decide whether the bottom object matched either of the top
708 two objects on that dimension (e.g., if the word is “shape”, is the bottom object the same
709 shape as either of the top two objects?). For the hard condition, stimuli were presented
710 for 3500 ms, with a 500 ms ITI, with four trials per block. In the easy condition, stimuli
711 were presented for 2800 ms, with a 400 ms ITI, with 5 trials per block. Each type of
712 block (hard or easy) lasted a total of 18 s. In each of the two runs of this task, there
713 were 3 hard blocks, 3 easy blocks and 3 16 s fixation blocks.

714 **4. Data preprocessing**

715 Data were preprocessed using the HCP's minimal preprocessing pipelines (Glasser et
716 al., 2013). Briefly, for each subject, structural images (T1w and T2w) were corrected for
717 spatial distortions and used for accurate extraction of cortical surfaces and subcortical
718 structures. To align subcortical structures across subjects, structural images were

719 registered using non-linear volume registration to Montreal Neurological Institute (MNI)
720 space.

721 Functional images (rest and task) were corrected for spatial distortions, motion
722 corrected, and mapped from volume to surface space using ribbon-constrained volume
723 to surface mapping. Subcortical data were also projected to the set of extracted
724 subcortical structure voxels and combined with the surface data to form the standard
725 CIFTI grayordinates space. Data were smoothed by a 2mm FWHM kernel in the
726 grayordinate space that avoids mixing data across gyral banks for surface data and
727 avoids mixing areal borders for subcortical data. Rest and task fMRI data were
728 additionally identically cleaned up for spatially specific noise using spatial ICA+FIX
729 (Salimi-Khorshidi et al., 2014) and global structured noise using temporal ICA (Glasser
730 et al., 2018).

731 For accurate cross-subject registration of cortical surfaces, a multi-modal surface
732 matching (MSM) algorithm (Robinson et al., 2014) was used to optimize the alignment
733 of cortical areas based on features from different modalities. MSMSulc ('sulc': cortical
734 folds average convexity) was used to initialize MSMAll, which then utilized myelin,
735 resting state network (RSN) and rfMRI visuotopic maps. Myelin maps were computed
736 using the ratio of T1w/T2w images (Glasser et al., 2014; Glasser and Van Essen, 2011).
737 Individual subject RSN maps were calculated using a weighted regression method
738 (Glasser et al., 2016a).

739 **5. HCP multi-modal parcellation and areal classifier**

740 The HCP multi-modal parcellation map (MMP) 1.0 (Glasser et al., 2016) was first
741 created using a semi-automated approach utilizing the group average maps of multiple
742 modalities (cortical thickness, myelin, resting state functional connectivity, and task
743 activations). For each modality, the gradient was computed as the 1st spatial derivative
744 along the cortical surface; ridges were local regions with the highest value and thus the
745 most sudden change in a feature. Overlapping gradient ridges across modalities were
746 used to draw putative areal borders with manual initialization and algorithmic
747 refinement. Defined areas were reviewed by neuroanatomists, compared whenever
748 possible to previously identified areas in the literature, and labelled. This resulted in
749 defining 180 areas per hemisphere. A multi-modal areal classifier was then developed
750 for automated definition of areas in each subject using the multi-modal feature maps.
751 The classifier was trained, tested and validated on independent groups of subjects from
752 the same 449 cohort used in this study (Glasser et al., 2016a).

753 **6. Task fMRI analysis**

754 Task fMRI analysis steps are detailed in Barch et al. (2013). Briefly, autocorrelation was
755 estimated using FSL's FILM on the surface. Activity estimates were computed for the
756 preprocessed functional time series from each run using a general linear model (GLM)
757 implemented in FSL's FILM (Woolrich et al., 2001). For the *working memory* task, 8
758 regressors were used - one for each type of stimulus in each of the N-back conditions.

759 Each predictor covered the period from the onset of the cue to the offset of the final trial
760 (27.5 s). For the *math* task, 2 regressors were used. The math regressor covered the
761 duration of a set of math questions designed to roughly match the duration of the story
762 blocks. The story regressor covered the variable duration of a short story, question, and
763 response period (~30 s). For the *relational processing* task, two regressors were used,
764 each covering the duration of 18 s composed of four trials for the hard condition and five
765 trials for the easy condition. In each case, linear contrasts of these predictors were
766 computed to estimate effects of interest: WM 2bk>0bk, Relational H>E, and
767 Math>Story.

768 All regressors were convolved with a canonical hemodynamic response function and its
769 temporal derivative. The time series and the GLM design were temporally filtered with a
770 Gaussian-weighted linear highpass filter with a cutoff of 200 seconds. Finally, the time
771 series was prewhitened within FILM to correct for autocorrelations in the fMRI data.
772 Surface-based autocorrelation estimate smoothing was incorporated into FSL's FILM at
773 a sigma of 5mm. Fixed-effects analyses were conducted using FSL's FEAT to estimate
774 the average effects across runs within each subject.

775 For further analysis of effect sizes, beta 'cope' maps was performed using custom built
776 MATLAB scripts after moving the data from the CIFTI file format to the MATLAB
777 workspace. Activity estimates on the surface vertices were averaged across vertices
778 that shared the same areal label for each subject. Unless mentioned otherwise,
779 parametric statistical tests (one-sample and paired sample t-tests) were used.

780 **7. rfMRI Functional connectivity analysis**

781 For each subject, a 'parcellated' FC map was computed by averaging the time series
782 across cortical vertices that shared the same areal label and correlating the average
783 time series giving a 360x360 FC matrix for each subject.

784 For comparison of connection types (Figure 3b, d), connectivities for each subject were
785 simply averaged across each group of areas following r-to-z transformation.

786 For subcortical analysis, the group average dense FC map for the 210V subjects group
787 was used for the identification of subcortical voxels. For each subcortical voxel, an
788 average connectivity to the cortical MD core was obtained by first calculating
789 connectivity to each core area (after averaging across each area's vertices), and then
790 averaging these connectivities following r-to-z transformation. A permutation testing
791 approach (100,000 permutations) was used to identify the significant voxels by building
792 a null distribution for each voxel based on its FC estimate to sets of 10 random brain
793 areas. A voxel was determined as significantly connected to the MD system when its FC
794 estimate was in the top 97.5th percentile.

795 **Data availability.** [upon acceptance] Data used for generating each of the imaging-
796 based figures [will be] made available by the BALSAs database. Selecting the URL at the
797 end of each figure will link to a BALSAs page that allows downloading of a scene file plus
798 associated data files; opening the scene file in Connectome Workbench will recapitulate
799 the exact configuration of data and annotations as displayed in the figure.

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807 **Author Contributions (CRediT taxonomy)**

808 Conceptualization, J.D., M.A.; Methodology, M.A, J.D., M.F.G, D.C.V.E; Formal
809 Analysis, M.A., M.F.G; Writing – original draft, M.A, J.D.; Writing – Review & Editing
810 M.A, J.D., M.F.G, D.C.V.E

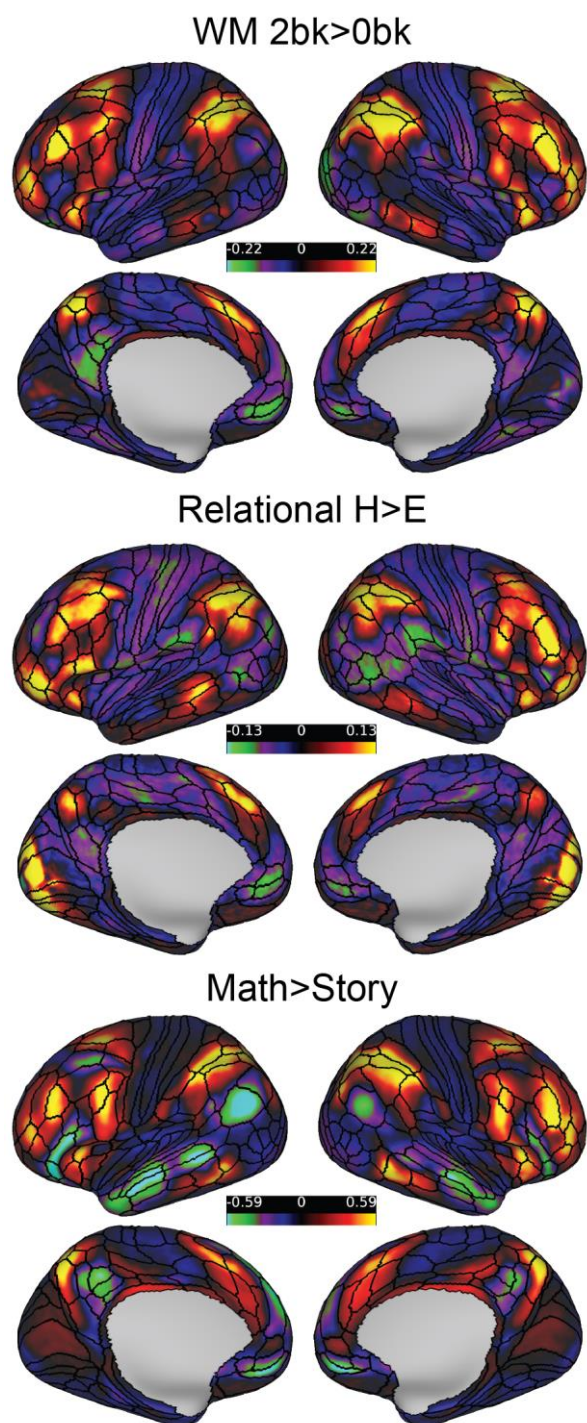
811 **Declaration of interests**

812 The authors declare no competing interests.

813

814 **Supplementary Figures**

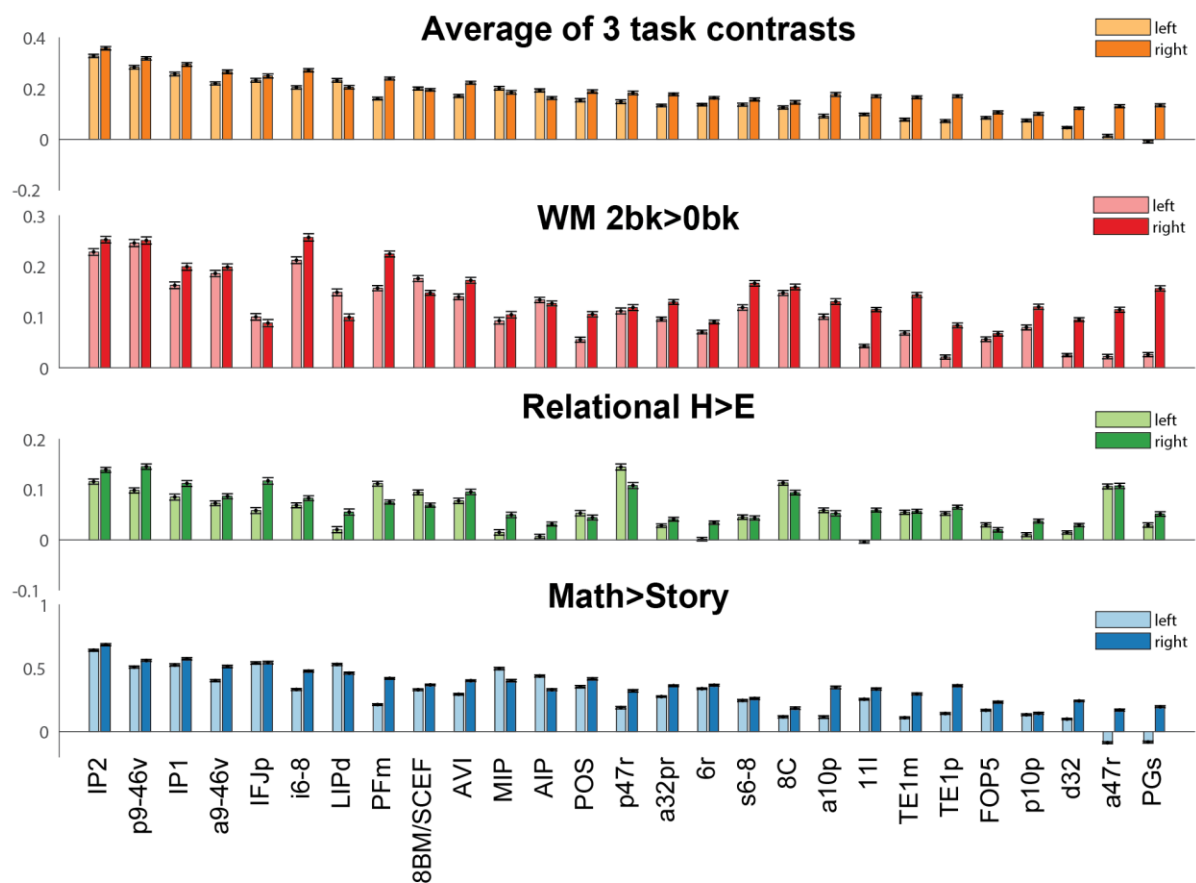
815



816

817 **Figure S1. Contrast maps for each task.**

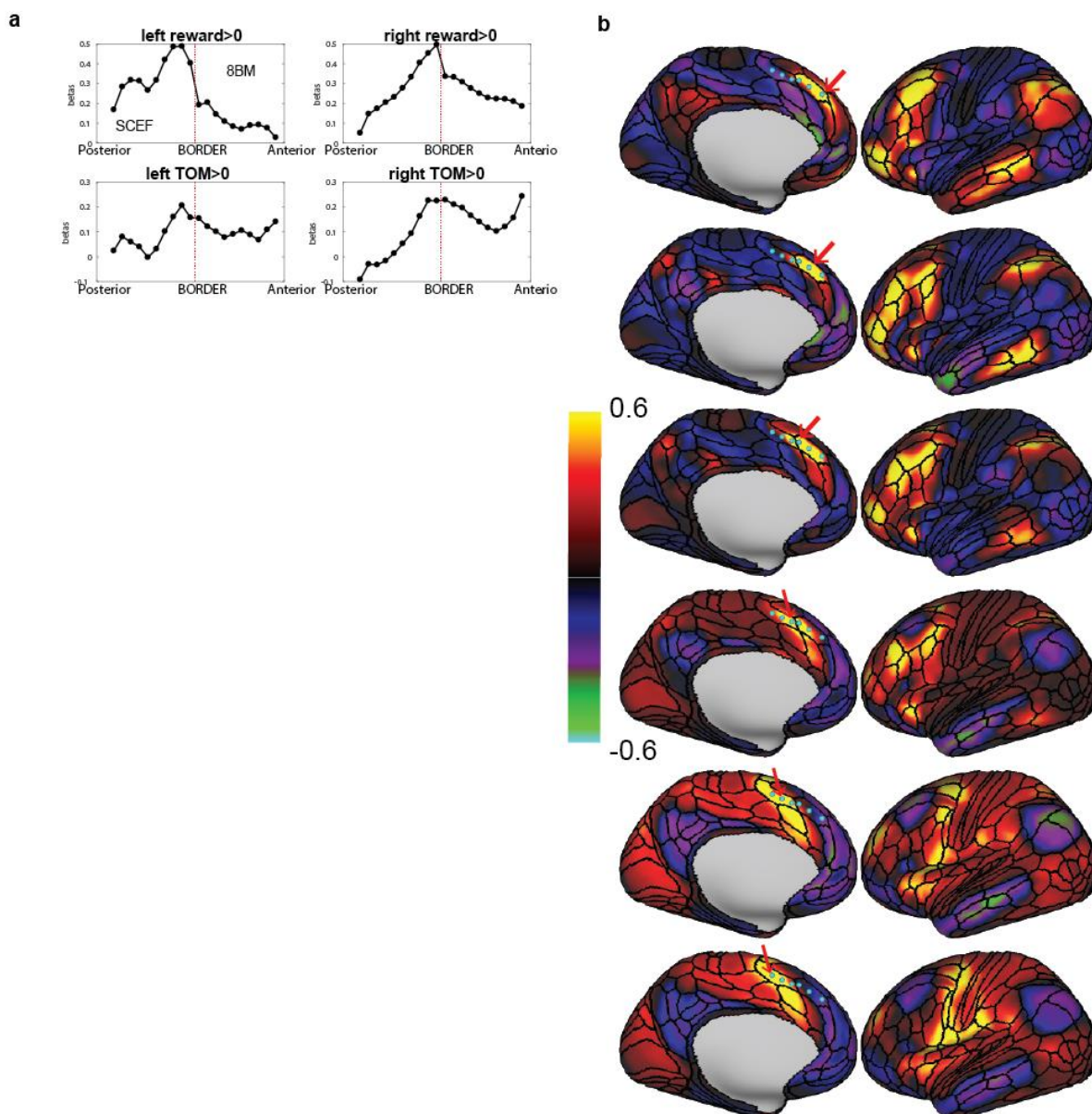
818



819

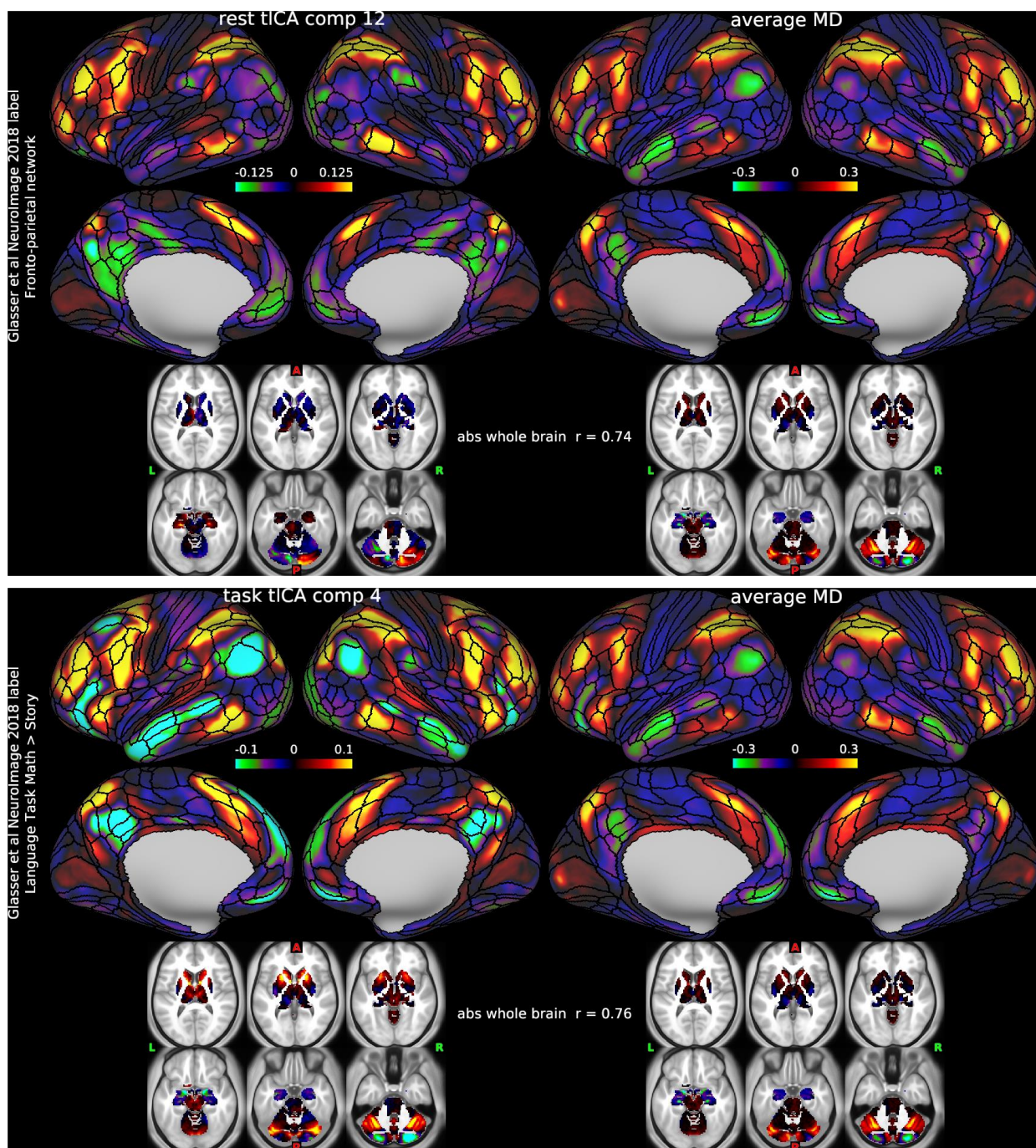
820 **Figure S2. Extended MD for each hemisphere.** Group average responses for the MD
 821 areas of both hemispheres. First row: average of the 3 HCP contrasts. Second row:
 822 Working memory. Third row: Relational reasoning. Fourth row: Math>story. Error bars
 823 are SEMs.

824



825

826 **Figure S3. 8BM/SCEF border.** (a) Group average responses for two HCP contrasts
827 across the 8BM/SCEF border, Reward>Baseline and Theory of Mind (TOM)>Baseline,
828 showing a similar pattern of build up within SCEF reaching a peak near the 8BM/SCEF
829 border. (b) Functional connectivity maps for seeds (210V map, left hemisphere) along
830 an antero-posterior gradient for the left 8BM/SCEF areas. Arrows mark the seed related
831 to each column's maps. Note how the seed in row 4 is in SCEF near the 8BM/SCEF
832 border and still shows an MD like connectivity pattern, especially the strong connectivity
833 to i6-8. More posterior seeds in SCEF show a markedly different pattern with strong
834 connectivity to FEF. Color scale is Pearson correlation (r).



835

836 **Figure S4. MD and temporal ICA.** Most correlated temporal ICA components (from
837 Glasser et al., 2018a) with MD average map. Top: rest tICA component 12. Bottom:
838 task tICA component 4.

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