Frontal and parietal alpha oscillations reflect 1 attentional modulation of cross-modal matching 2 3

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Abstract

14 Multisensory perception is characterised by attentional selection of relevant sensory inputs and 15 exploitation of cross-modal similarities that promote cross-modal binding. Underlying mechanisms of both top-down and bottom-up modulations have been linked to changes in 16 17 alpha/gamma dynamics in primary sensory cortices. Accordingly, it has been proposed that alpha oscillations provide pulsed inhibition for gamma activity and thereby dynamically route 18 cortical information flow. In this study, we employed a recently introduced multisensory 19 paradigm incorporating both bottom-up and top-down aspects of cross-modal attention in an 20 21 EEG study. The same trimodal stimuli were presented in two distinct attentional conditions, 22 focused on visual-tactile or audio-visual components, for which cross-modal congruence of amplitude changes had to be evaluated. Neither top-down nor bottom-up cross-modal attention 23 24 modulated alpha or gamma power in primary sensory cortices. Instead, we found alpha band 25 effects in bilateral frontal and right parietal cortex. We propose that frontal alpha oscillations 26 reflect the origin of top-down control regulating perceptual gains and that parietal alpha relates 27 to sensory re-orienting. Taken together, we suggest that the idea of selective cortical routing 28 via alpha oscillations can be extended from sensory cortices to the fronto-parietal attention 29 network. 30

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Author contributions

J.M., U.F. and A.K.E. designed the experiment. J.M. recorded the data. J.M. analysed the data. 40

41 J.M. wrote the main manuscript text. J.M., U.F. and A.K.E. reviewed the manuscript. 42

Competing Interests

The authors declare that they have no competing interests. 44

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Data Availability

Behavioural and electrophysiological data will be made available upon request to the 47 48 corresponding author.

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Introduction

50 Human perception is governed by constant influx of information through multiple 51 sensory channels. The act of perceiving routes information flow by active engagement with the 52 multisensory environment, causing sensory inputs to be constantly shaped by modulatory signals reflecting behavioural goals, contextual demands and structural properties of the 53 54 environment. Spotting a singing bird in a tree, for instance, does not depend on tactile processing but on evaluating visual and auditory signals for temporo-spatial congruence. 55 56 Lacing shoes, on the other hand, makes little use of audition but integrates vision and tactile 57 perception in a goal-directed manner. These examples illustrate that multisensory perception is shaped by top-down and bottom-up modulation of sensory inputs. Attempts to understand 58 59 multisensory perception accordingly need to address neural mechanisms underlying both 60 selection of relevant sensory input and exploitation of cross-modal similarities that promote 61 cross-modal binding.

62 A well-described mechanism of stimulus selection via attentional modulation is gain regulation of population responses in sensory regions^{1,2}. In MEG and EEG studies, these gain 63 regulations are likely reflected in alpha band dynamics³. Jensen and Mazaheri⁴ propose that 64 65 alpha band activity plays a general role in the up- and down-regulation of cortical processing 66 capabilities ("gating by inhibition"). By pulsed inhibition, alpha oscillations could effectively gate gamma band activity related to active processing⁵. This has been shown repeatedly in the 67 context of spatial attention^{6,7,8} while evidence supporting its applicability to cross-modal 68 attention is sparse^{9,10}. Additionally, it is unclear whether pulsed inhibition regulates cortical 69 70 processing beyond sensory cortices, for instance in cortical regions exerting top-down control.

71 Mechanisms underlying stimulus-driven cross-modal binding are less well understood. 72 In fact, it remains a matter of debate at what stage of cortical processing such interactions take place^{11,12,13}. While some evidence suggests that input to distinct modalities is processed in 73 parallel and only converges later in regions of the temporal and parietal lobe^{14,15,16}, other 74 75 evidence points out that interactions can already take place at the level of primary sensory regions^{17,18,19}. The disparity of findings is not surprising given that factors driving cross-modal 76 77 integration span from psychophysical (spatial/temporal congruence) to memory-dependent 78 (semantic congruence and cross-modal correspondences). Yet, a linking observation is that lowand high-level integration have been associated with changes in gamma band activity^{13,20,21}. 79

In the EEG study reported here, we employed a recently introduced multisensory
 paradigm incorporating both bottom-up and top-down aspects of cross-modal attention²². This
 paradigm involved a trimodal stimulus consisting of a visual, an auditory and a tactile

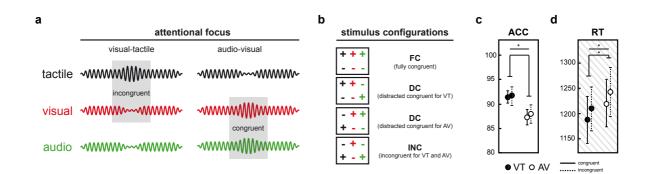


Figure 1: Schematic of matching task and behavioural results. a) Illustration of example trials in the two attentional conditions. Under visual-tactile focus (left), the changes in the target stimuli are incongruent, as the tactile stimulus (black) increases in intensity while the visual stimulus (red) decreases. Under audio-visual focus (right), target change is congruent, since visual and auditory (green) stimuli both increase in intensity. b) In each block, all possible stimulus configurations occurred with equal probability. Intensity changes are depicted by coloured plus/minus signs (colour coding as introduced in a)). c) Accuracy (ACC) in percentage correct. Error bars represent standard deviations. There was no effects of experimental conditions. d) Reactions times in milliseconds (RTs). Error bars represent standard deviations. *ATTENTION* as well as *CONGRUENCE* significantly affected the timing of responses, but not the accuracy of responding (Note: RTs were collected in a previous behavioural study²¹ from the same sample of participants).

83 component that each underwent a brief increase or decrease in intensity. Participants had to attend two of the stimuli and had to decide whether the attended pair changed congruently or 84 incongruently. In a similar study investigating audio-visual matching with MEG, changes in 85 primary sensory alpha and gamma activity were more profound when participants attended 86 presentations compared to when they were ignored¹⁰. In order to further investigate whether 87 this modulation of alpha/gamma band dynamics holds in situations where attention is not 88 89 holistic but rather modality-based, we presented the same trimodal stimuli in two distinct attentional conditions (top-down), focused on either visual-tactile (VT) or audio-visual (AV) 90 components, for which cross-modal congruence (bottom-up) of amplitude changes had to be 91 92 evaluated (Fig. 1 a). We expected top-down cross-modal attention to selectively enhance primary sensory alpha activity for irrelevant modalities and decrease alpha activity for attended 93 modalities. This increase/decrease in alpha power might be accompanied by a decrease/increase 94 95 in gamma band activity. As a bottom- up effect of cross-modal binding, gamma band activity in sensory cortices or temporal/parietal cortex is expected to be modulated by cross-modal 96 97 congruence.

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Results

99 **Psychophysics and behaviour**

The trimodal stimulus material was designed such that the target amplitude changes in
 each modality were equally salient. This was achieved by estimating detection thresholds for
 each modality and change direction separately using a psychophysical staircase procedure²³.
 Yet, a questionnaire that was completed during debriefing of a preceding behavioural study²²

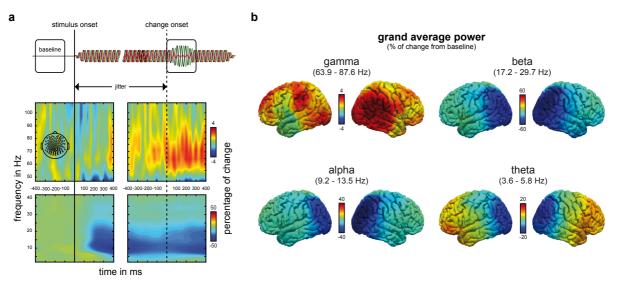


Figure 2: Average time-frequency dynamics in sensor and source space. a) Time-frequency dynamics in sensor space at occipito-parietal channels (topography shown in upper left panel), time locked to stimulus onset (left panels, black solid vertical line) and change onset (right panels, black dashed vertical line. *Top:* Schematic of temporal trial structure displaying the two relevant time-windows used for analysis: a baseline (-400:-100 ms) separated by a jitter (stimulus to change onset between 700 and 1000 ms) from the change interval (0:300 ms). *Bottom:* Time-frequency plots from posterior sensors. Values represent percentage of change from baseline. b) Distribution of band-limited power on the cortical surface in the change interval relative to baseline.

104 indicated that subjective salience of the sensory components was in fact not equal but strongest

- 105 for the visual component. In particular, participants reported that the visual component was
- 106 hardest to ignore when it was task irrelevant (pairwise Wilcoxon rank sum test, Bonferroni

107 corrected, V-T: p = .002, V-A: p = .24, T-A: p = .26). This should be kept in mind for the

108 discussion of the effects of cross-modal attention.

109 The timing and accuracy of responding was analysed with a repeated measure analysis 110 of variance (ANOVA) with factors *ATTENTION* (VT vs. AV) and *CONGRUENCE* (congruent 111 vs. incongruent). Responses were faster but not more accurate when subjects attended cross-112 modally congruent pairs (Fig. 1 d; p < .001, $\eta_p^2 = 0.471$). When participants attended VT, timing 113 as well as accuracy of responding was significantly better compared with the AV conditions 114 (RT: p = .036, $\eta_p^2 = 0.201$; ACC: p = .005, $\eta_p^2 = 0.327$). No interaction effects between 115 *ATTENTION* and *CONGRUENCE* were observed.

116 **ROI analysis**

In Figure 2, we present an overview of time-frequency dynamics during the task as well as distributions of band-limited power for theta, alpha, beta and gamma bands in source space. In order to investigate power changes in oscillatory activity in primary sensory areas occurring after the stimulus increases or decreases, we conducted a regions of interest (ROI) analysis on source projected EEG data in primary visual, auditory and somatosensory cortex. Statistical evaluation was carried out with a repeated measures ANOVA with factors *ROI*, *ATTENTION*

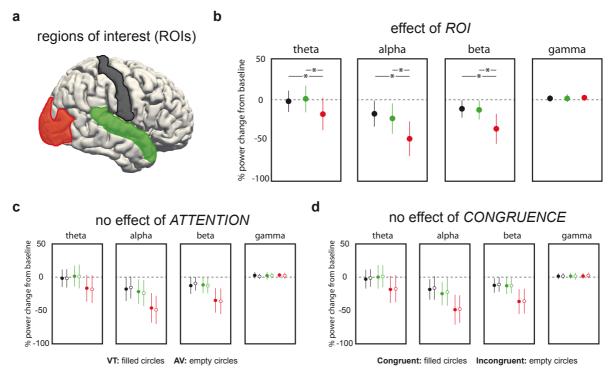


Figure 3: Regions of interest (ROI) analysis of band-limited power during change epoch in primary sensory areas. a) Primary sensory areas used for ROI ANOVA with factors *ATTENTION* (VT vs. AV), *CONGRUENCE* (congruent vs. incongruent) and *ROI* (visual vs. auditory vs. somatosensory); visual = red, auditory = green, somatosensory = black. **b)** Effect of *ROI* is significant for theta, alpha and beta bands, but not gamma band. Asterisk signifies significant comparisons (p < .001). **c)** No significant effect of *ATTENTION*. **d)** No significant effect of *CONGRUENCE*.

123 and CONGRUENCE separately for each frequency band (Fig. 3, see Methods for details). Significant effects of *ROI* were observed for theta, alpha and beta bands (for all, p < .001 and 124 $\eta_n^2 > 0.5$; see Fig. 3 b). In the gamma band, *ROI* did not explain a significant amount of variance 125 (p = .689). Simple effects analysis for the lower frequency bands showed that decreases in 126 power were significantly stronger in visual compared with both auditory and somatosensory 127 128 ROIs (for all comparisons, p < .001; Fig. 3 b). Power changes in auditory and somatosensory ROIs did not differ (for all, p > .05). The main effects and interactions of ATTENTION and 129 *CONGRUENCE* were not significant (for all, p > .05; Fig. 3 c + d). 130

131 Cluster statistics

To complement the ROI analysis, we conducted a whole-brain analysis of task-related power changes in the interval after stimulus increases and decreases evaluated by means of nonparametric cluster-based permutation statistics (see *Methods* for details). For the *ATTENTION* contrast (VT *minus* AV), significant differences were found in the alpha band. In two roughly symmetric clusters, VT attention was associated with stronger power decrease of alpha oscillations when compared with AV attention (Fig. 4 a). In the left hemisphere, the cluster was situated in the border region of pre-central gyrus, middle frontal gyrus (MFG) and bioRxiv preprint doi: https://doi.org/10.1101/477034; this version posted November 27, 2018. The copyright holder for this preprint (which was not certified by peer review) is the author/funder. All rights reserved. No reuse allowed without permission.

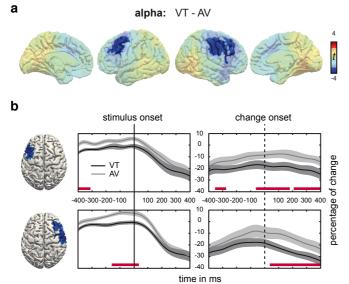


Figure 4: Effect of *ATTENTION* (VT - AV). a) Cluster-based permutation statistic of the contrast VT *minus* AV in the alpha band during change interval. Tvalues of the respective contrasts are depicted. Shaded voxels are non-significant. b) Time-course of alpha activity within significant clusters. Shading corresponds to the standard error of the mean. Red bars indicate temporal regions of significance as determined by permutation testing (see *Methods* for details).

superior frontal gyrus encompassing the frontal eye fields (FEF; p = .031). In the right 139 hemisphere, the cluster was situated similarly but expanded further into pre- and post-central 140 gyrus (p = .005). In a next step, we analysed time courses of alpha power modulations within 141 142 these two clusters (Fig. 4 b, see *Methods*). Throughout the entire time course, alpha power was 143 lower for VT than for AV attention. This difference was significant before stimulus onset in both hemispheres (left: [-400; -312] ms, right: [-165; 43] ms), in a short epoch prior to change 144 145 onset in the left hemisphere ([-348; -286] ms) and throughout the whole change epoch in both 146 hemispheres (left: [-69; 177] ms and [211; 400] ms, right: [43; 400] ms).

When evaluating the effect of CONGRUENCE (attended congruent minus attended 147 148 incongruent), significant differences were found in alpha and theta bands (Fig. 5). Theta power 149 was higher for congruent trials compared to incongruent trials in large parts of the medial wall of both hemispheres (Fig. 5 a). This effect was significant in a left hemispheric cluster stretching 150 151 from posterior to anterior cingulate cortex. In a next step, we analysed the contributions of fully 152 congruent (FC) and distracted congruent (DC) trials to the overall effect of congruence (see Fig. 1 b and Methods for details). It was driven by FC trials for which theta power was increased 153 154 in cingulate cortex of both hemispheres, and in small clusters in left and right intraparietal sulcus (IPS) as well as left inferior frontal gyrus (IFG) and right MFG (Fig. 5 c). No significant 155 156 theta power differences were seen when comparing distracted congruent with incongruent trials 157 (Fig. 5 e).

In the alpha band, cross-modal congruence modulated power in large parts of medial and lateral cortex. In incongruent trials, stronger decrements of alpha power occurred in bilateral medial superior frontal cortex and left MFG (Fig. 5 b). Congruent trials were associated with stronger decrements in alpha power in bilateral medial occipito-parietal cortex and right

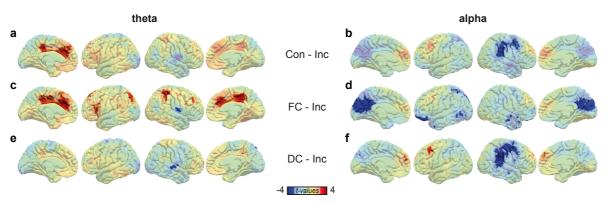


Figure 5. Effect of *CONGRUENCE* (Congruent - Incongruent). **a+b**) Cluster-based permutation statistic of the contrast *Congruent* - *Incongruent* in the alpha (a) and theta (b) band during change interval. All subplots depict t-values. Shaded voxels are non-significant. **c**) Contrast between theta power in *fully congruent* (FC) and *incongruent* trials. **d**) Contrast between alpha power in *fully congruent* (FC) and *incongruent* (FC) and *incongruent* (DC) and *incongruent* trials. **f**) Contrast between alpha power in *distracted congruent* (DC) and *incongruent* trials.

inferior parietal and middle frontal cortex. The latter difference was significant in a cluster
covering the right temporoparietal junction (TPJ), but stretching rostrally towards right MFG.
Next, we disentangled contributions from FC and DC trials as before for theta power. While
FC trials significantly drove the effect in medial occipito-parietal cortex (Fig. 5 d), DC trials
contributed significantly to the effect in medial and left middle frontal cortex (Fig. 5 e). The
effect in right TPJ and MFG was dominated by DC trials (Fig. 5 d).

168

Discussion

We investigated bottom-up and top-down modulation of sensory processing in a cross-169 modal matching task involving visual, auditory and tactile perception. Contrary to our 170 expectations, we did not find alpha/gamma oscillations in primary sensory areas to be 171 modulated by bottom-up or top-down cross-modal attention. This finding is surprising given 172 173 that both processes have often been noted to be accompanied by alpha/gamma modulations in sensory cortices^{3,6,7,10,18,19}. Our explanation for the lack of primary sensory modulation is the 174 nature of the task: many, if not most, multisensory studies employ detection tasks with near-175 176 threshold sensory stimulation. In these situations of low sensory drive, both bottom-up and topdown modulation of sensory input can be expected to have higher impact compared with 177 situations of strong sensory drive. Stimulus-driven cross-modal enhancement by spatio-178 179 temporal congruence, for instance, is assumed to obey the law of inverse effectiveness, meaning 180 that there is an inverse relationship between possible cross-modal enhancement and stimulus intensity²⁴. Here, however, all stimulus intensities were clearly supra-threshold with 181 182 superimposed amplitude changes. Top-down as well as bottom-up modulation of sensory processing might thus be subtle and hence not detectable by EEG. Instead, we found theta 183 184 oscillations in cingulate cortex and most notably alpha oscillations in frontal and parietal cortex 185 to be modulated. In the following, we propose that frontal alpha oscillations reflect the origin

of top-down control regulating perceptual gains and that parietal alpha oscillations relate to
sensory (re-)orienting. Theta activity in cingulate cortex is finally discussed in the context of
adaptive task-switching behaviour circumventing cross-modal matching.

Reduction of alpha power in bilateral FEF and MFG as well as right pre-/post-central 189 190 gyrus was stronger for VT cross-modal attention compared to AV attention. This difference was significant even before stimulus onset. Besides their role in oculomotor control, the FEF 191 192 have been described as important structures in top-down attention²⁵. In a study using TMS, 193 Grosbas and Paus showed that disruption of activity in FEF shortly before the onset of the target in a visuospatial covert attention task facilitated responses²⁶. Conversely, 10 Hz TMS over the 194 right FEF was shown to impair visual search of unpredictable items with low salience²⁷. Moore 195 196 and Armstrong reconciled this conflicting evidence by suggesting that the FEF has a general role in regulating visual gain²⁸. In their study, electric stimulation of FEF in the monkey either 197 enhanced or inhibited responses to visual stimuli in V4 depending on whether retinopically 198 199 corresponding sites were stimulated. Studies in humans supported this idea by showing that TMS over FEF could increase phosphene or contrast sensitivity of extrastriate cortex 29,30 . This 200 top-down modulation of visual cortex was demonstrated even in the absence of sensory input³¹. 201 Likewise, anticipatory alpha and stimulus related gamma activity in occipito-parietal cortex 202 could be modulated by TMS over FEF³². The strength of modulation was shown to correlate 203 with the strength of structural connectivity between frontal and parietal cortex via the superior 204 205 longitudinal fasciculus³³. Thus, animal and human studies jointly conclude that the FEF can 206 dynamically modulate the gain of down-stream visual cortex independent of sensory input. In 207 our study, FEF/MFG likely facilitated cross-modal matching by modulating visual gain to 208 counter visual dominance. Although stimulus intensity was titrated to be balanced across 209 modalities (see *Methods*), we have reason to assume that perceived salience was highest for the 210 visual component. In a questionnaire that was completed during debriefing of the preceding 211 behavioural study, we asked participants to rank the difficulty to ignore a given modality. Most 212 participants reported that visual components were hardest and tactile components easiest to ignore. This finding is in line with a pattern of sensory dominance found for combinations of 213 visual, auditory and somatosensory stimuli in a discrimination task³⁴. Sensory dominance can 214 be problematic under the assumption that cross-modal matching is not independent of 215 216 perceptual gain. This is most likely the case for stimulus-driven aspects of multisensory 217 integration - the idea of inverse effectiveness, after all, assumes multimodal stimuli of low but comparable intensity²⁴. Consequentially, decreased power of alpha oscillations in FEF/MFG is 218 taken as evidence for an increased down-regulation of visual gain in VT conditions to account 219 for unequal subjective salience of the stimuli to be matched. 220

As discussed above, balancing perceptual gains across modalities by top-down 221 222 modulation likely enables optimal use of stimulus-driven aspects of cross-modal matching. 223 These bottom-up factors were ubiquitous in this task; on each trial, participants were 224 simultaneously confronted with three salient events, that is, intensity changes in each modality. 225 Although each change of intensity by itself possessed some degree of bottom-up salience, we 226 suggest that cross-modal congruence amplified salience through cross-modal binding¹³. When 227 cross-modal binding was enhanced between attended modalities, responses were facilitated. 228 This was especially pronounced for fully congruent trials where conflict, and thus the need for 229 actual matching, was absent. All other trials were either distracted congruent (attended 230 modalities change congruently, but the distractor diverged) or attended incongruent (one of the 231 attended modalities is congruent to the distractor). In these cases, cross-modal binding was 232 always stronger between two given modalities compared to the respective third. When contrasting the EEG of these trials, we find alpha band effects in the right temporoparietal 233 234 junction (rTPJ) and right MFG. Specifically, distracted congruent conditions were associated 235 with decreased power of alpha oscillations in these regions compared with attended incongruent 236 trials. In accordance with the "gating by inhibition" theory, we conclude that the rTPJ/rMFG 237 were more strongly disinhibited when attended modalities had a stronger bottom-up drive for 238 cross-modal binding. The TPJ receives inputs from visual, auditory and somatosensory cortex 239 and is richly connected to temporal and frontal sites, making it an important hub for the 240 interaction of multisensory integration and attention³⁵. Accordingly, lesions to the right TPJ typically result in neglect^{36,37}. A dominant interpretation of rTPJ's functional role is its 241 involvement in (spatial) re-orienting based on stimulus salience³⁸. In a model integrating goal-242 243 directed and stimulus-driven attention, it is suggested that a dorsal network comprising FEF 244 and IPS instantiates attentional sets. As a counterpart, a ventral network comprising rTPJ and 245 right ventral frontal gyrus mediates bottom-up signals acting as a circuit-breaker for the dorsal system. Studies employing multisensory paradigms have noted rTPJ's involvement in 246 247 processing cross-modal congruence. In a study investigating visual-tactile pattern matching, pre-stimulus alpha and beta power in right supramarginal gyrus differentiated between 248 detection and congruence-evaluation tasks³⁹. Another study showed that alpha power in right 249 250 posterior regions was more strongly supressed during congruent compared with incongruent audio-visual speech presentations⁴⁰. Taken together with our results, we suggest that the rTPJ 251 252 detects the increased salience of congruent cross-modal events. While each trial might, in principle, result in attentional capture by any of the three modalities, cross-modal binding by 253 congruence might serve as a reliable "cue" for re-orienting towards the relevant modalities. 254 255 Thereby, cross-modal binding between attended modalities might support modality-based re-256 orienting.

257 As pointed out above, fully congruent trials were characterised by the absence of cross-258 modal conflict. In the EEG, these highly salient trials were associated with stronger alpha power reductions in medial occipito-parietal cortex. In an event-related potentials study featuring 259 260 visual, auditory and somatosensory stimuli, RT facilitation was correlated with the latency of 261 the P300, which was localised in precuneus⁴⁰. Other research suggests that alpha power 262 reductions in occipito-parietal cortex and P300 dynamics are functionally coupled⁴¹. Here, enhanced involvement of medial occipito-parietal cortex is proposed to reflect increased 263 264 bottom-up salience due to multisensory enhancement, i.e., increased perceptual gains of concurrent congruent sensory input to more than one modality⁴². In addition to mere bottom-265 266 up sensory salience, fully congruent stimuli occurred in only 25 % of all trials and were thereby 267 salient. Actual cross-modal matching was required only in the remaining 75 % of trials where 268 two modalities changed congruently while the third modality diverged. An efficient strategy would accordingly be to "switch" between these two tasks, i.e., between detecting highly salient 269 270 events and cross-modal matching of conflicting input. In addition to the alpha band effect in 271 precuneus, fully congruent trials were also associated with a relative increase in theta power in 272 bilateral cingulate cortex. Theta band activity in cingulate cortex has previously been related to the adjustment of stimulus response mappings⁴³. Together with insular cortex, cingulate cortex 273 274 is part of a salience network which has importance for both bottom-up detection of salient events and switching between large-scale networks to adaptively control behaviour⁴⁴. Here, it 275 276 is suggested that reduced alpha power in medial occipito-parietal cortex related to multisensory 277 enhancement acts as a salience signal detected by cingulate cortex which in turn initiates 278 adaptive task-switching behaviour.

Taken together, we provide evidence that cross-modal matching in complex 279 280 multisensory environments heavily relies on mechanisms of attention. Our results contrast with 281 the majority of studies on multisensory integration concerned with stimulus detection where 282 attentional load is typically low. Here, participants were confronted with a highly challenging 283 multisensory setting. In order to counter the bias imposed by visual dominance, top-down regulation of perceptual gains likely supported an optimal exploitation of cross-modal 284 285 similarities that promote perceptual binding. This was associated with decreased alpha band 286 power in frontal cortices proposed to reflect the origin of top-down modulation. Likewise, 287 bottom-up drive for cross-modal binding was related to changes in alpha power in right parietal 288 cortex proposed to represent the bottom-up modulatory signal underlying sensory re-orienting. Both findings provide evidence for an extension of the idea that alpha/gamma dynamics 289 290 indicate selective cortical routing beyond sensory cortex to the fronto-parietal attention 291 network.

292

Methods

293 **Participants**

Twenty-one participants entered the study and received monetary compensation for their participation. They were on average 23.8 ± 2.5 years old and 11 of them were female (10 male). Vision, audition and tactile perception were normal and none of them had a history of neurological or psychiatric disorders. After an explanation of the experimental procedure, participants gave written consent. The ethics committee of the University Medical Center Hamburg-Eppendorf approved the study which was carried out in accordance with the declaration of Helsinki.

301 Experimental design

302 On each trial, we presented a trimodal stimulus consisting of a visual, an auditory and a tactile component that each underwent a brief increase or decrease in intensity (see Stimulus 303 Material for details). Block-wise, participants attended either visual-tactile (VT) or audio-304 305 visual (AV) bimodal pairs and ignored the respective third component. The task was to decide whether the attended bimodal pairs changed congruently (i.e., in the same direction) or 306 307 incongruently (i.e., in different directions; see Fig. 1 a). Verbal responses had to be withheld 308 until stimulus offset to minimise myogenic artifacts. Therefore, reaction times (RTs) could not 309 be evaluated. Instead, we present RT data of the same sample of participants from the behavioural study preceding the EEG study²². In each block, all possible eight stimulus 310 configurations of increases and decreases across modalities were presented with equal 311 312 probability (Fig. 1 b). VT and AV blocks containing 64 trials presented in randomised order 313 were alternating. Data were collected on two separate days with identical experimental 314 procedure so that EEG data of 1280 trials was collected from each participant. Prior to statistical 315 analysis, trials were pooled without taking change direction into account. For instance, fully 316 congruent trials were both trials where all modalities underwent decrements and trials where 317 all modalities underwent increments (Fig. 1 b, pooling is indicated by boxes).

318 **Stimulus material**

Visual contrast, auditory loudness and vibration strength were experimentally increased or decreased. The magnitudes of change per modality and direction were individually estimated prior to the experimental sessions using the same psychometric step function as described in Misselhorn et al. $(QUEST)^{22,23}$. Intensity changes had a duration of 300 ms and onsets were jittered across trials between 700 and 1000 ms after stimulus onset (Fig. 2 a). In total, sensory stimulation had a fixed duration of 2 s. As visual stimulation, an expanding circular grating was centrally presented against a grey background on a CRT screen with a visual angle of 5°. The auditory component consisted of a complex sinusoidal tone (13 sine waves: 64 Hz and its first
6 harmonics as well as 91 Hz and its first 5 harmonics, low-frequency modulator: 0.8 Hz) played
back with audiometric insert earphones binaurally at 70 dB (E-A-RTONE 3A, 3M, USA). As
tactile stimulation, high-frequency vibrations (250 Hz on C2 tactors, Engineering Acoustics
Inc., USA) were delivered to the tips of both index fingers.

331 EEG

332 EEG was recorded from 128 active electrodes (Easy Cap, Germany) including four ocular electrodes referenced to the nose. Data was sampled at 1000 Hz with an amplitude 333 334 resolution of 0.1 uV using BRAINAMP MR amplifier (Brain Products, Germany) and digitised 335 after analog filtering (low cutoff: 10 s, high cutoff: 1000 Hz). Offline, data was down-sampled 336 to 500 Hz and digitally filtered (high-pass: 1 Hz, low-pass: 120 Hz, notch: 49-51 Hz, 99-101 Hz). Epochs of 2.5 s were cut from -500 ms relative to stimulus onset until stimulus offset and 337 338 normalised to the pre-stimulus baseline. Next, data was re-referenced to the common average 339 and linear trends were removed from all epochs. From the four ocular channels, two bipolar 340 channels for horizontal and vertical eve movements were derived.

Pre-processing. Trials with incorrect answer and large non-stereotypical artifacts were 341 342 excluded from further processing. Subsequently, independent component analysis (ICA) was performed separately for low and high frequency bands (low band: 1-30 Hz, high band: 30-120 343 344 Hz). Thereby, stereotypical low-frequency artifacts (for instance eve movements and heart beat) 345 and high-frequency artifacts (i.e. myogenic activity) could be separated more reliably from neuronal activity. For both bands, principal components analysis was performed first to reduce 346 347 data such that 99 % of variance is retained. Subsequently, ICA was performed on the rankreduced data using the infomax algorithm⁴⁵. Artifactual ICs were identified and rejected with 348 respect to time course, spectrum and sensor topography⁴⁶. For the high band, saccade-related 349 350 transient potentials were removed additionally⁴⁷. Finally, all epochs were visually inspected 351 and epochs with remaining artifacts were rejected. Furthermore, a subset of 19 electrodes (i.e. 352 most outer facial, temporal and neck electrodes) was excluded from further analysis due to poor signal-to-noise ratio. Lastly, data was stratified such that all conditions in the ensuing analysis 353 354 hold the same amount of data within subjects. On average, 426 ± 89 trials per participant entered 355 the analysis.

Source reconstruction of band-limited signals. Cleaned data in low and high bands were joined and epoched with respect to stimulus onset as well as change onset. Prior to filtering data into narrow bands by means of wavelet analysis, event related potentials were subtracted in order to remove phase-locked responses. A family of 40 complex Morlet wavelets *w* with lengths of 2 s was constructed for logarithmically spaced frequencies between 2 and 120 Hz.

361
$$w(t, f_0) = A * e^{-\frac{t^2}{2\sigma_t^2}} * e^{2\pi f_0 t}$$

The number of cycles per wavelet (m) were logarithmically spaced between 3 and 10 and 362 subsequently rounded off. Wavelets were normalised by factor $A = \sigma_t \sqrt{\pi}^{-\frac{1}{2}}$ with $\sigma_t =$ 363 $m/2\pi f_0$. Single trial data was convolved with the Morlet wavelets by multiplication in the 364 365 frequency domain using fast fourier transformation with boxcar windows. Wavelet filtered 366 single trial data was then reconstructed in source space using exact low-resolution brain electromagnetic tomography (eLORETA; regularisation: 0.05)⁴⁸. Lead fields were computed 367 for a three-shell head model⁴⁹. The customised cortical grid was derived from a cortical surface 368 369 provided by Freesurfer in MNI space by reducing the number of cortical nodes from 270000 to 10000⁵⁰. Dipole directions at each node of the cortical grid were estimated by means of singular 370 371 value decomposition of the trial averaged spectral power individually for all bands and kept constant for all trials of the given participant. Induced power was computed from these source 372 373 reconstructed band-limited time domain signals. Power in the epoch after change onset was 374 baseline corrected using the baseline of the mean over all conditions from -400 to -100 ms 375 relative to stimulus onset (Fig. 2 a). By visual inspection of the resulting time-frequency landscapes, frequency bands in the theta, alpha, beta and gamma range were chosen 376 377 individually for each participant (mean values and range in parentheses; theta: 4.7 [3.6; 5.8] Hz, alpha: 11.5 [9.2; 13.5] Hz, beta: 23.0 [17.2; 29.7] Hz, gamma: 78.9 [63.9; 87.6] Hz). 378 Statistical analysis was carried out for the post-change interval ([0; 300] ms) only. 379

380 Statistical analysis

Behaviour. Accuracy of responding (ACC) within experimental conditions was
analysed using a repeated-measures analysis of variance (ANOVA) with factors *ATTENTION*(VT vs. AV) and *CONGRUENCE* (congruent vs. incongruent). The timing of verbal responses
was not analysed because subjects were instructed to withhold responses until stimulus offset.
Instead, data from the previous behavioural study was re-analysed for the sub-sample of
participants enrolled in this EEG study²¹. The same ANOVA as described above for ACCs was
evaluated.

EEG: Regions of interest (ROIs) analysis. Primary cortical regions for vision, audition
 and tactile perception were chosen from the Freesurfer atlas which is constructed by gyral
 identification and parcellation based on anatomical landmarks⁵⁰. For each frequency band,
 baseline-corrected, time and ROI averaged data in the post-change interval was evaluated by
 means of ANOVA with factors *ROI* (visual vs. auditory vs. somatosensory), *ATTENTION* (VT
 vs. AV) and *CONGRUENCE* (congruent vs. incongruent) and. Simple effects of significant
 ANOVA effects were assessed by paired-sample t-tests applying Bonferroni correction.

EEG: Whole-brain permutation statistics. Complementing ROI analysis, a whole brain 395 396 exploratory analysis of differences between experimental conditions was conducted and evaluated by means of nonparametric cluster-based permutation statistics⁵¹. A null distribution 397 398 was computed by randomly drawing trials into two sets per subject (300000 permutations). For 399 each node of the cortical grid, a paired-sample t-test was computed between averaged power of 400 the two sets and statistical maps were thresholded (p < .05). Significant clusters were found and 401 the size of the largest cluster was noted. This procedure was carried out separately for the four 402 frequency bands. Contrasts corresponding to a 2 (ATTENTION) x 2 (CONGRUENCE) design 403 were computed and evaluated against the aforementioned null-hypothesis (cut-off: 99th 404 percentile). Reported *p*-values are Bonferroni-corrected.

405 Cluster statistics were complemented by post-hoc analyses that were designed (1) to 406 detail on the time-course of the *ATTENTION* effect and (2) to disentangle the contributions of 407 sub-conditions to the overall effect of *CONGRUENCE*.

408(1) For clusters showing a significant effect of ATTENTION, we computed the time course of 409 average within cluster spectral power separately for visual-tactile and audio-visual conditions. 410 Significance of the difference between time courses was evaluated using nonparametric cluster-411 based permutation statistics (300000 permutations). For each permutation, time courses were shuffled and paired-sample t-tests between VT and AV were computed for each sample. The 412 413 number of samples included in the longest temporally continuous cluster of significant difference was noted to form the maximum statistic null distribution. In the original data, 414 415 periods of significant difference between attentional conditions were considered significant in the temporal domain when they held more samples than the 99th percentile of the null 416 417 distribution.

418(2) For this analysis we differentiated according to whether attended stimulus components were 419 "fully congruent" or "distracted congruent". Fully congruent (FC) means that all stimulus 420 components, including the distracting modality, change congruently (that is, all components 421 increased or decreased in intensity; Fig. 1 b, top box). Distracted congruent (DC) means that 422 the distractor's change direction deviates from the change direction in the attended modalities 423 (Fig. 1 b, middle boxes). In this case, the participant has to resolve the conflict between attended 424 congruence and unattended incongruence. In order to disentangle these two scenarios, we 425 computed contrasts of FC respectively DC against attended incongruent conditions. 426

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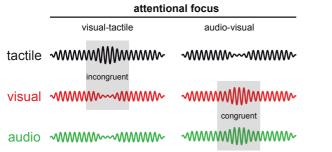
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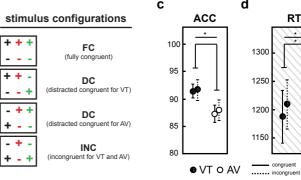
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b

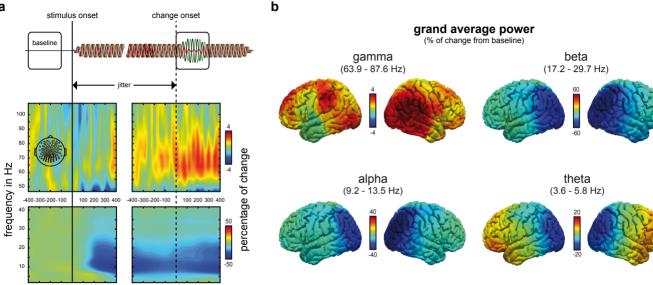




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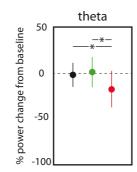


time in ms

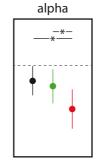
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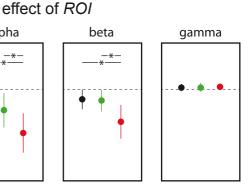
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regions of interest (ROIs)

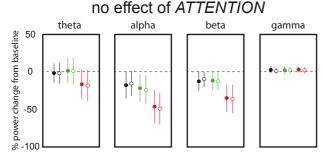


d

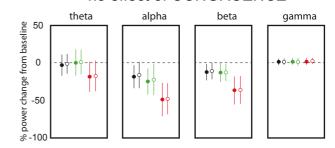




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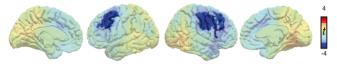


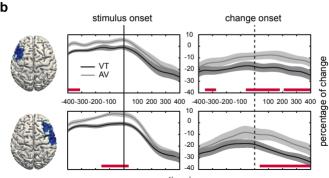
no effect of CONGRUENCE



VT: filled circles AV: empty circles Congruent: filled circles Incongruent: empty circles

alpha: VT - AV

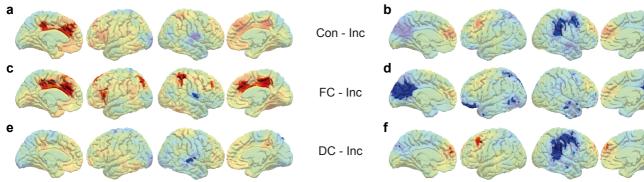




time in ms

theta

alpha



-4 t-values 4