

The role of the fornix in human navigational learning

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1 **Abstract**

2 Studies in rodents have demonstrated that transecting the white matter pathway
3 linking the hippocampus and anterior thalamic nuclei - the fornix - impairs flexible
4 navigational learning in the Morris Water Maze (MWM), as well as similar spatial
5 learning tasks. While diffusion MRI studies in humans have linked fornix
6 microstructure to scene discrimination and memory, its role in human navigation is
7 currently unknown. We used high-angular resolution diffusion MRI to ask whether
8 inter-individual differences in fornix microstructure would be associated with spatial
9 learning in a virtual MWM task. To increase sensitivity to individual learning across
10 trials, we adopted a novel curve fitting approach to estimate a single index of
11 learning rate. We found a significant correlation between learning rate and the
12 microstructure (mean diffusivity) of the fornix, but not that of a control tract linking
13 occipital and anterior temporal cortices (the inferior longitudinal fasciculus, ILF).
14 Further, this correlation remained significant when controlling for hippocampal
15 volume. These findings extend previous animal studies by demonstrating the
16 functional relevance of the fornix for human navigational learning, and highlight the
17 importance of a distributed neuroanatomical network, underpinned by key white
18 matter pathways, such as the fornix, in complex spatial behaviour.

19

20 **Key words:** hippocampus; navigation; spatial learning; cognitive map; diffusion MRI;
21 connectivity

22

23

24

25 **Introduction**

26 The ability to navigate, and learn the location of rewards and goals in the
27 environment, is a fundamental and highly adaptive cognitive function across species
28 (Landau and Lakusta, 2009; Wolbers and Hegarty, 2010; Murray et al., 2016).

29 Lesion studies in animals suggest that this ability depends, in part, on several key
30 brain regions, including the hippocampus, mammillary bodies, and the anterior
31 thalamic nuclei (Sutherland and Rodriguez, 1989; Warburton and Aggleton, 1998;
32 Jankowski et al., 2013), which in turn connect with a broader network including
33 entorhinal, parahippocampal, retrosplenial, and posterior parietal cortex, all thought
34 to be important for navigation (Ekstrom et al., 2017). In particular, the hippocampus,
35 mammillary bodies, and anterior thalamic nuclei are connected anatomically by an
36 arch-shaped white matter pathway called the fornix (Saunders and Aggleton, 2007).
37 Given the role of these interconnected structures in spatial learning and navigation
38 (Jankowski et al., 2013), the ability for these distributed regions to communicate via
39 the fornix may also be critical for successful spatial learning and navigation.

40

41 Indeed, transecting the fornix in rodents and monkeys impairs learning for objects-in-
42 place, but not the objects themselves (Gaffan, 1992, 1994; Simpson et al., 1998).

43 These findings also extend to performance on spatial navigation tasks, most notably
44 the Morris Water Maze (MWM). The MWM is one of the most widely used laboratory
45 tasks in studies of navigational behaviour across non-human species and has been
46 recognized as an excellent candidate for a universal test of spatial navigation ability
47 (Morris, 1984; Possin et al., 2016). In this task, animals are placed in a circular pool
48 and required to swim to a hidden platform beneath the surface using allocentric cues

49 outside the pool. Several studies have shown that fornix-transected rodents are
50 impaired on the MWM, particularly when required to navigate flexibly from multiple
51 positions within the maze (Eichenbaum et al., 1990; Packard and McGaugh, 1992;
52 Warburton et al., 1998; Warburton and Aggleton, 1998; De Bruin et al., 2001; Cain et
53 al., 2006). Fornix transection also impairs allocentric place learning in other maze
54 tasks (O'Keefe et al., 1975; Olton et al., 1978; Packard et al., 1989; Dumont et al.,
55 2015).

56

57 Critically, while these animal studies highlight a key role for the fornix in spatial
58 learning - across both visuo-spatial discrimination and navigation tasks - the role of
59 this white matter pathway in human wayfinding is currently unknown. Studies using
60 diffusion magnetic resonance imaging (dMRI), which allows white matter
61 microstructure to be quantified *in vivo*, have reported associations in healthy human
62 subjects between fornix microstructure and inter-individual differences in scene and
63 spatial context processing across both memory (Rudebeck et al., 2009; Hodgetts et
64 al., 2017) and perceptual tasks (Postans et al., 2014; Hodgetts et al., 2015). Given
65 differences in the visuospatial representations underpinning navigation across
66 rodents and humans (Ekstrom, 2015), it begs the question whether this same
67 extended functional system, structurally linked by the fornix, is similarly important for
68 navigational learning in humans.

69

70 To test this, we acquired dMRI data in healthy human subjects who performed a
71 human analogue of the MWM (Figure 1). In this task, individuals were required to
72 learn, over trials, the location of a hidden sensor within a virtual art gallery. Similar to

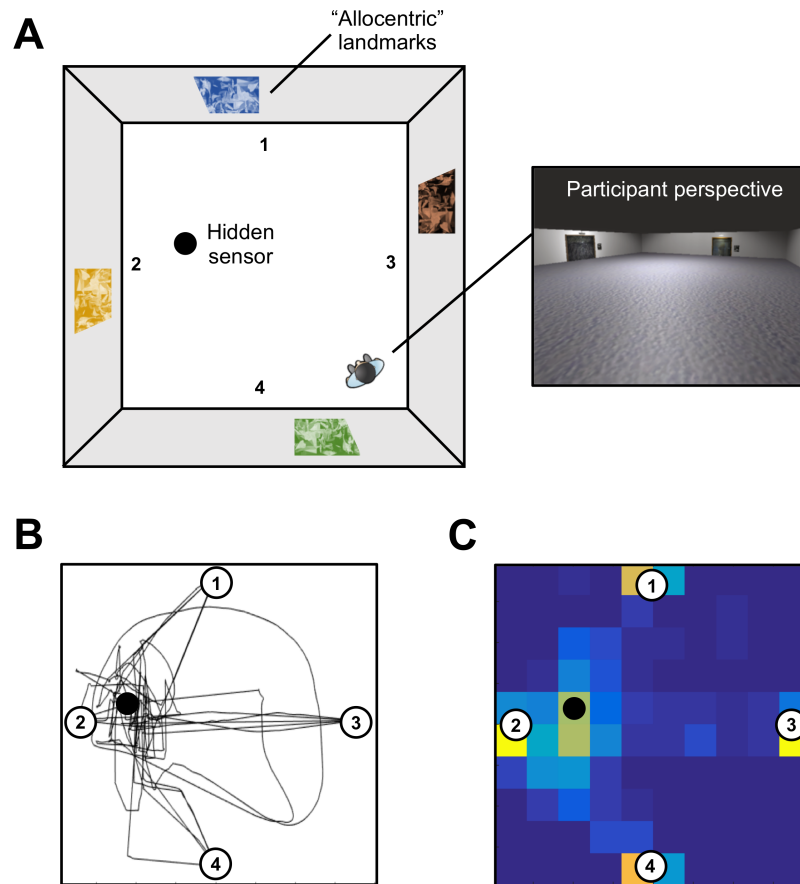
73 the rodent paradigm, subjects were required to navigate from multiple starting
74 positions, thus placing greater demand on flexible allocentric processing (Figure 1).
75 To create a single index of navigational learning rate, we used a curve fitting
76 approach to model the time taken to reach the sensor across trials (for similar
77 approaches, see Stepanov and Abramson, 2008; Pereira and Burwell, 2015; Kahn et
78 al., 2017). We predicted, based on previous work (Packard and McGaugh, 1992;
79 Warburton and Aggleton, 1998; Cain et al., 2006; Hodgetts et al., 2015), that
80 microstructure of the fornix, but not a control tract connecting occipital and anterior
81 temporal cortices (the “inferior longitudinal fasciculus”, ILF) (Latini, 2015), would be
82 significantly related to spatial learning rate in a virtual MWM task.

83

84 **Methods**

85 ***Participants***

86 Thirty-three healthy volunteers (15 males, 18 females; mean age = 24 years; SD =
87 3.5 years) were scanned at the Cardiff University Brain Research Imaging Centre
88 (CUBRIC). These same participants completed a virtual Morris Water Maze task in a
89 separate behavioural session. All subjects were fluent English speakers with normal
90 or corrected-to-normal vision. Participation in both sessions was undertaken with the
91 understanding and written consent of each subject. The research was completed in
92 accordance with, and approved by, the Cardiff University School of Psychology
93 Research Ethics Committee.



94

95 **Figure 1. The virtual reality Morris Water Maze.** (A) Birds-eye schematic of the
96 virtual art gallery that the participants explore during the task. The artwork on the
97 outer walls of the gallery are the “landmarks” in the virtual arena. An example first
98 person perspective from within the maze is shown. (B) Movement trajectories and
99 (C) location heatmap across all 20 trials for an example participant.

100

101 **Virtual Morris Water Maze Task**

102 We used the virtual MWM task developed by Kolarik et al. (2016). This task was
103 created using Unity 3D (Unity Technologies, San Francisco) and required
104 participants to explore, from a first-person perspective, a virtual art gallery using the
105 arrow keys on the computer keyboard (Figure 1A). The room was 8 x 8 virtual m² in

106 size, and contained four distinct paintings, one on each wall of the environment. On
107 a given trial, the participants' task was to locate a hidden sensor on the floor as
108 quickly as possible. This sensor occupied 0.25% of the total floor space (i.e., an 0.8
109 x 0.8 m² square). When the participant walked over the hidden platform it became
110 visible and the caption 'You found the hidden sensor' was displayed in the centre of
111 the screen. At this point, the exploration time was recorded automatically and a 10
112 second countdown appeared in the centre of the display during which the
113 participants could freely navigate the room. After this countdown, an inter-trial
114 window appeared and the participants could click on a button to start the next
115 learning trial. The maximum duration of each learning trial was 60 seconds. If the
116 participant did not find the target location within this period, the sensor became
117 visible. The task involved 20 learning trials, which comprised five blocks of four trials.
118 Within each block, participants started from each of the four starting positions
119 (arbitrary North, South, East, West). The movement trajectories and location
120 heatmap for an example participant is shown in Figure 1B-C.

121

122 ***MRI acquisition***

123 Whole brain dMRI data were acquired at the Cardiff University Brain Research
124 Imaging Centre (CUBRIC) using a 3T GE HDx Signa scanner with an eight-channel
125 head coil. Single-shell high-angular resolution dMRI (HARDI) (Tuch et al., 2002) data
126 were collected with a single-shot spin-echo echo-planar imaging pulse sequence
127 with the following parameters: 30 directions; TE= 87 ms; 60 continuous slices
128 acquired along an oblique-axial plane with 2.4 mm thickness and no gap. The scans
129 were cardiac-gated using a peripheral pulse oximeter placed on the participants'
130 fingertips. A T1-weighted 3D FSPGR sequence was also acquired with the following

131 parameters: TR= 7.8 ms; TE= 3 ms, TI= 450 ms, flip angle= 20°; FOV= 256 mm*192
132 mm*172 mm; 1 mm isotropic resolution.

133

134 ***Diffusion MRI preprocessing***

135 Diffusion MRI data were corrected for subject head motion and eddy currents using
136 ExploreDTI (Version 4.8.3; Leemans and Jones, 2009). The bi-tensor 'Free Water
137 Elimination' (FWE) procedure was applied *post hoc* to correct for voxel-wise partial
138 volume artifacts arising from free water contamination (Pasternak et al., 2009). Free
139 water contamination (from cerebrospinal fluid) is a particular issue for white matter
140 pathways located near the ventricles (such as the fornix), and has been shown to
141 significantly affect tract delineation (Concha et al., 2005). Following FWE, corrected
142 diffusion-tensor indices FA and MD were computed. FA reflects the extent to which
143 diffusion within biological tissue is anisotropic, or constrained along a single axis,
144 and can range from 0 (fully isotropic) to 1 (fully anisotropic). MD ($10^{-3}\text{mm}^2\text{s}^{-1}$) reflects
145 a combined average of axial diffusion (diffusion along the principal axis) and radial
146 diffusion (diffusion along the orthogonal direction).

147

148 ***Tractography***

149 Deterministic whole brain white matter tractography was performed using the
150 ExploreDTI graphical toolbox. Tractography was based on constrained spherical
151 deconvolution (CSD) (Jeurissen et al., 2011), which can extract multiple peaks in the
152 fiber orientation density function (fODF) at each voxel. This approach permits the
153 representation of crossing/kissing fibers in individual voxels. Each streamline was
154 reconstructed using an fODF amplitude threshold of 0.1 and a step size of 1mm, and
155 followed the peak in the fODF that subtended the smallest step-wise change in

156 orientation. An angle threshold of 30° was used and any streamlines exceeding this
157 threshold were terminated.

158

159 Three-dimensional reconstructions of each tract were obtained from individual
160 subjects by using a waypoint region of interest (ROI) approach, based on an
161 anatomical prescription. Here, “AND” and “NOT” gates were applied, and combined,
162 to extract tracts from each subject’s whole brain tractography data. These ROIs were
163 drawn manually on the direction-encoded FA maps in native space by one
164 experimenter (MS) and quality assessed by other experimenters (CJH, ANW).

165

166 *Fornix*

167 A multiple region-of-interest (ROI) approach was adopted to reconstruct the fornix
168 (Metzler-Baddeley et al., 2011). This approach involved placing a seed point ROI on
169 the coronal plane at the point where the anterior pillars enter the fornix body. Using a
170 mid-sagittal plane as a guide, a single AND ROI was positioned on the axial plane,
171 encompassing both crus fornici at the lower part of the splenium of the corpus
172 callosum. Three NOT ROIs were then placed: (1) anterior to the fornix pillars; (2)
173 posterior to the crus fornici; and (3) on the axial plane, intersecting the corpus
174 callosum. Once these ROIs were placed, and the tracts reconstructed, anatomically
175 implausible fibers were removed using additional NOT ROIs (see Hodgetts et al.,
176 2017).

177

178 *Inferior longitudinal fasciculus (ILF)*

179 Fiber-tracking of the ILF (control tract) was performed using a two-ROI approach in
180 each hemisphere (Wakana et al., 2007). First, the posterior edge of the cingulum

181 bundle was identified on the sagittal plane. Reverting to a coronal plane at this
182 position, a SEED ROI was placed that encompassed the whole hemisphere. To
183 isolate streamlines extending towards the anterior temporal lobe (ATL), a second
184 ROI was drawn at the most posterior coronal slice in which the temporal lobe was
185 not connected to the frontal lobe. Here, an additional AND ROI was drawn around
186 the entire temporal lobe. Similar to the fornix protocol above, any anatomically
187 implausible streamlines were removed using additional NOT ROIs. This approach
188 was carried out in both hemispheres; diffusion properties of the left and right ILF (for
189 both FA and MD) were averaged across hemispheres to provide a bilateral measure
190 of ILF FA and MD in each participant.

191

192 ***Grey matter volumetry***

193 Bilateral hippocampal volume was derived using FMRIB's Integrated Registration &
194 Segmentation Tool (FIRST; Patenaude et al., 2012). As temporal lobe substructures
195 have been shown to correlate with intracranial volume (Moran et al., 2001),
196 individual-level hippocampal volumes were divided by total intracranial volume
197 (eTIV) to create proportional scores (Westman et al., 2013).

198

199 ***Statistical analysis of maze learning***

200 To increase sensitivity to individual-level performance across learning trials, and to
201 derive a single index of learning rate, we analysed the relationship between spatial
202 learning and fornix tissue microstructure using a curve fitting approach (see e.g.,
203 Pereira and Burwell, 2015; Kahn et al., 2017). Performance on each learning trial
204 was defined by the time (in seconds) to reach the hidden sensor. As can be seen in
205 Figure 2A, there was high inter-individual variability in spatial learning, with subjects

206 varying in both learning speed and the shape of their learning pattern. Here,
207 individual learning data was fit using a power function: Time to sensor = $a * x^b$,
208 where b specifies the slope of the fitted power model.

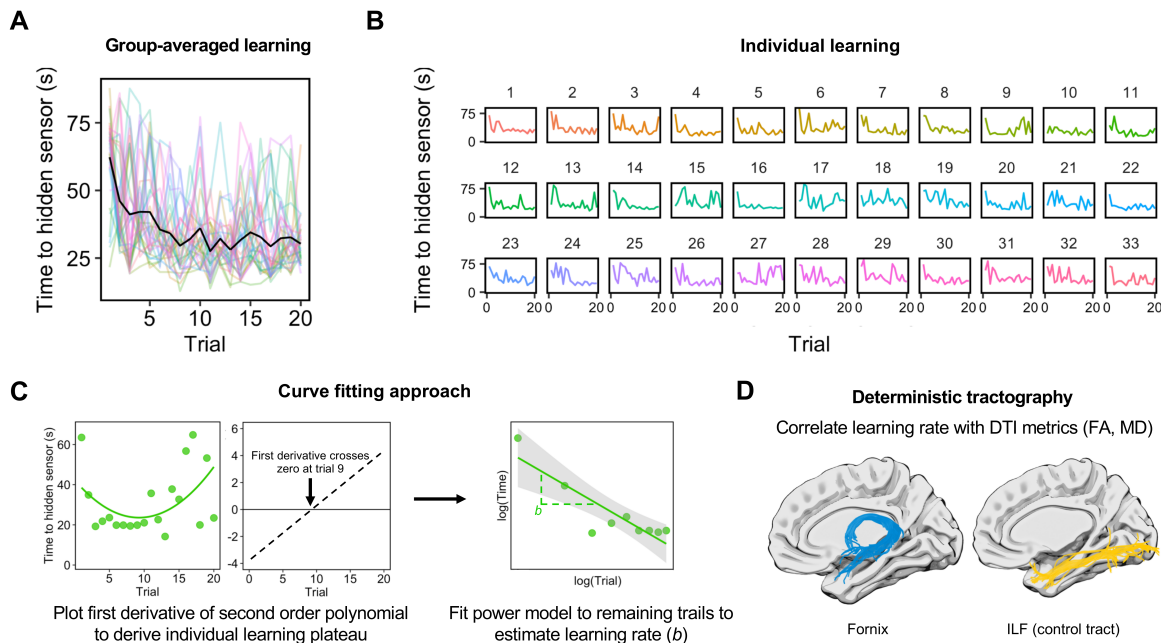
209

210 One aspect of this data is that some subjects learned quickly (and plateaued) before
211 displaying variable, or slow, performance in the later trials (e.g., subjects 9, 13, and
212 20; Figure 2B). This presents a challenge for a curve fitting approach across all trials
213 (and potentially produces counterintuitive results), as some of the fastest learners
214 will show the poorest model fits. For instance, both subjects 9 and 16 display an
215 initial steep learning curve and an early plateau (Figure 2B), but a power model fit to
216 *all trials* provides a poor fit of the subject who does not sustain performance until the
217 end of the task. In order to account for this complexity in learning patterns, we
218 adopted a data-driven approach to determine a cut-off in individual subjects.

219 Specifically, a second-order polynomial model was fit to all trials in each subject
220 using the curve fitting toolbox in Matlab (Mathworks, Inc.). The cut-off was defined as
221 the trough of this curve, which is where the first derivative of the second-degree
222 polynomial crosses zero (Figure 2C). Trials up to and including this cut-off were then
223 modelled using a power function (mean trials included = 14.3; range = 7 – 20).

224

225



226

227 **Figure 2. Modelling navigational learning in individual participants. MWM task**

228 learning at the (A) group-level and (B) individual-level. Y-axes represent the time to

229 reach the hidden sensor in seconds. The number of trials (total = 20) is shown on the

230 x-axis. (C) Method for determining the number of learning trials to-be-modelled.

231 Some participants appeared to learn rapidly and plateau before displaying variable

232 performance in later trials. For instance, a power model fits the example participant's

233 latency data poorly when all trials are considered. In order to capture initial learning,

234 therefore, we fitted the latency data (across all trials) with a second-order polynomial

235 in each subject. The point at which the first derivative of this polynomial crossed zero

236 was used to define the number of trials to-be-modelled. The trials up to this point

237 were then fit with a power function and the b parameter derived to index learning

238 rate. Power fits are shown by linearly fitting the log-transformed data. (D) Learning

239 rate measures were correlated with diffusion metrics (FA, MD) from the fornix (blue)

240 and the ILF (yellow). Tract reconstructions are shown against an inflated brain for

241 visualisation purposes.

242 Using this approach, we derived a single measure of learning rate, denoted by the b
243 parameter (or slope) of the fitted power model (b ; mean = -0.32, SD = 0.08, range = -
244 0.49 to -0.19). The b parameter reflects slope curvilinearity in each subject, where
245 lower, negative values reflect more convex downward curves and thus faster
246 learning rates. As such, we predict a positive association between fornix MD and
247 learning rate, and negative associations between fornix FA and learning rate.

248

249 Directional Pearson correlations were conducted between the learning rate and free
250 water corrected MD and FA values for the fornix and ILF (Figure 2D). The resulting
251 coefficients were compared statistically using directional Steiger Z-tests (Steiger,
252 1980) within the 'cocor' package in R (Diedenhofen and Musch, 2015).

253 Pearson correlations were Bonferroni-corrected by dividing $\alpha = 0.05$ by the number
254 of statistical comparisons for each DTI metric (i.e., $0.05/2 = 0.025$) (Lakens, 2016).

255 Prior to correlational analyses, outliers for each tract and metric were identified and
256 removed using the Tukey method in R. This excluded an extreme value for fornix
257 MD, fornix FA, and ILF FA. To exclude poor performers who were not engaging with
258 the task, we used a resampling approach where individual-level data was shuffled
259 over 500 permutations and confidence intervals (CIs) derived. Participants with a
260 model R^2 that fell outside the CI of their individually-defined random distribution were
261 excluded (Subjects 10, 15, 17, 18 and 21).

262

263 We also conducted Bayesian correlation analyses using JASP ([https://jasp-](https://jasp-stats.org)
264 [stats.org](https://jasp-stats.org)). From this, we report default Bayes factors and 95% Bayesian credibility
265 intervals (BCI). The Bayes factor, expressed as BF_{10} grades the intensity of the
266 evidence that the data provide for the alternative hypothesis (H_1) versus the null

267 (H₀) on a continuous scale. A BF₁₀ of 1 indicates that the observed finding is equally
268 likely under the null and the alternative hypothesis. A BF₁₀ much greater than 1
269 allows us to conclude that there is substantial evidence for the alternative over the
270 null. Conversely BF₁₀ values substantially less than 1 provide strong evidence in
271 favour of the null over the alternative hypothesis (Wetzels and Wagenmakers, 2012).

272

273 Complementary Spearman's rho tests were also conducted for our key correlations.
274 The strength of Spearman's correlations were compared directly using a robust
275 bootstrapping approach (Wilcox, 2016), as implemented using 'comp2dcorr' in
276 Matlab (<https://github.com/GRousselet/blog/tree/master/comp2dcorr>).

277

278 **Results**

279 ***Correlating navigational learning with tract microstructure***

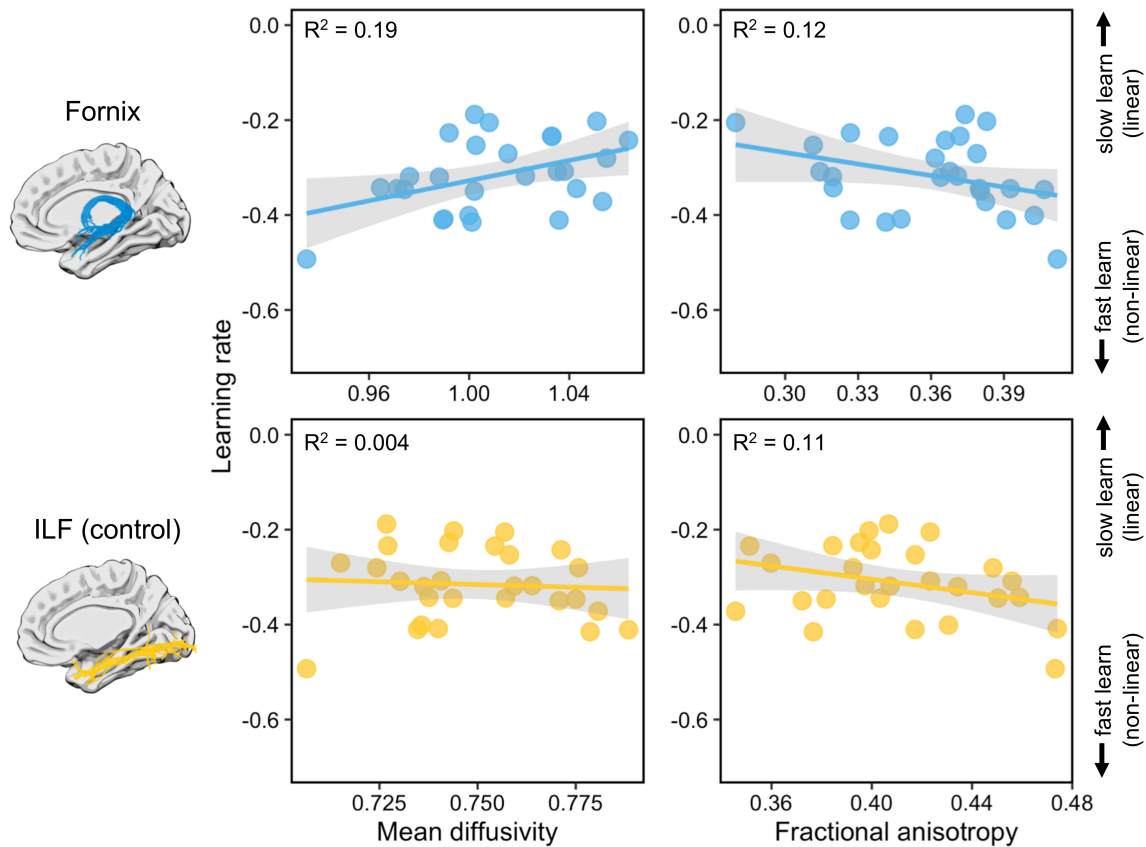
280 There was a significant positive correlation between the derived learning rate and
281 fornix MD, as shown in Figure 3. This suggests that those subjects with lower fornix
282 MD had faster learning rates ($r = 0.44$, $p = 0.01$, 95% BCI [0.09, 0.68], $B_{+0} = 5.5$;
283 Figure 3). There was no significant relationship between individual learning rate and
284 MD in a control tract - the inferior longitudinal fasciculus (ILF; $r = -0.06$; $p = 0.62$,
285 95% BCI [0.37, 0.01], $B_{0+} = 5.38$). A directional Steiger Z-test (Steiger, 1980)
286 revealed that the correlation between derived learning rate and fornix MD was
287 significantly greater than with ILF MD ($z = 2.26$, $p = 0.01$).

288

289 A moderate trend was observed between fornix FA and learning rate but this did not
290 reach our experiment-wise significance level ($r = -0.34$, $p = 0.04$, 95% BCI [-0.62, -
291 0.04], $B_{-0} = 1.99$; Figure 3). There was no significant correlation between ILF FA and

292 learning rate ($r = -0.17$; $p = 0.2$, 95% BCI $[-0.51, -0.01]$, $B_0 = 1.68$). These two
 293 correlations did not differ significantly ($z = 0.22$, $p = 0.21$).

294



295

296 **Figure 3.** The correlation between tract microstructure and learning rate (*b*
 297 parameter) for the fornix (top row) and the inferior longitudinal fasciculus (ILF).

298

299 **Controlling for hippocampal volume**

300 To examine whether hippocampal volume contributes to the microstructural-
 301 behavioural correlations reported above, partial correlations (both frequentist and
 302 Bayesian) were conducted. The significant positive correlation between the learning
 303 rate parameter and fornix MD remained when controlling for bilateral hippocampal
 304 volume ($r = 0.4$, $p = 0.02$, $BF_{+0} = 3.59$), as seen in prior studies (Hodgetts et al.,

305 2017). For fornix FA, a slightly stronger negative trend was observed ($r = -0.35$, $p =$
306 0.04 , $BF_0 = 0.09$) when hippocampal volume was controlled for, though this did not
307 reach our experiment-wise significance level (i.e., $p = 0.025$). When examining
308 hippocampal volume, independent of fornix microstructural measures, there was no
309 significant association found between hippocampal volume and learning rate ($r =$
310 0.03 , $p = 0.94$, 95% BCI $[-0.25, -0.002]$, $B_0 = 10.2$).

311

312 ***Non-parametric correlations between tract microstructure and learning***

313 Finally, we also conducted complementary directional Spearman's rho tests for our
314 key correlations, with such tests robust to univariate outliers (Croux and Dehon,
315 2010). As above, Spearman's correlations were Bonferroni-corrected by dividing $\alpha =$
316 0.05 by the number of statistical comparisons for each DTI metric (i.e., $0.05/2 =$
317 0.025). A significant positive association was observed between learning rate and
318 fornix MD ($\rho = 0.4$, $p = 0.02$). No significant association was found with ILF MD ($\rho = -$
319 0.18 , $p = 0.82$). A strong trend was found between the b parameter and fornix FA (ρ
320 $= -0.32$, $p = 0.05$) but not ILF FA ($\rho = -0.21$, $p = 0.14$).

321

322 A direct comparison between these correlations revealed a significant difference
323 between fornix MD and ILD MD and their association with navigation learning rate,
324 as indicated by the bootstrap distribution not overlapping with zero (95% CI = $0.2 -$
325 0.88 , $p = 0$). There was no significant difference between the FA correlations (95%
326 CI = $-0.7191 - 0.2962$, $p = 0.4$).

327

328

329

330 **General discussion**

331 Using a virtual-reality analogue of a classic navigational paradigm, the Morris Water
332 Maze (Morris, 1984), we asked whether inter-individual variation in the
333 microstructure of the fornix (linking hippocampus with medial diencephalon and
334 prefrontal cortex) is related to individual differences in navigational learning. To
335 increase sensitivity to individual learning across trials we adopted a curve fitting
336 approach (Kahn et al., 2017), which generated a single index of learning rate ('b') in
337 each individual. We found that fornix microstructure (particularly MD) was
338 significantly associated with navigational learning rate in a virtual MWM task, as
339 defined by the slope of the fitted power model, and this association remained when
340 controlling for bilateral hippocampal volume. Furthermore, this effect was
341 significantly stronger than that seen for the ILF, a control tract linking occipital and
342 anterior temporal cortices, which has previously been implicated in semantic learning
343 (Qi et al., 2015; Ripollés et al., 2017).

344

345 These results build upon previous animal studies that highlight a potential key role
346 for the fornix in mediating place learning and navigational behaviour. Critically, we
347 provide novel evidence, using a MWM task analogous to that used in animals
348 (Kolarik et al., 2016; Possin et al., 2016), that the fornix supports navigational
349 learning in humans. In rodents, fornix transection has been shown to impair MWM
350 learning, as characterised by more gradual learning slopes and slower latencies in
351 finding the hidden platform (Eichenbaum et al., 1990; Packard and McGaugh, 1992;
352 Warburton and Aggleton, 1998; Cain et al., 2006). By applying a curve fitting
353 approach, we were able to characterise the steepness of learning slopes at the

354 individual participant level, and relate this directly with fornix microstructure.
355 Strikingly consistent with the animal studies described above, reduced structural
356 connectivity in the fornix (indexed by higher MD) was related to more gradual
357 learning rates. Further, by identifying individual learning plateaus in a data-driven
358 way, this approach also accounts for potential fatigue, mind-wandering or other
359 factors that may affect performance later in the learning session.

360

361 Similar to lesioning hippocampus and anterior thalamic nuclei, learning deficits
362 following fornix transection in rodents are also more severe when the animal is
363 required to navigate from multiple start positions (Eichenbaum et al., 1990). Such
364 findings suggest, therefore, that this broader neuroanatomical system, structurally
365 underpinned by the fornix (Aggleton et al., 2010), supports spatial learning in a
366 flexible manner (i.e., from novel start positions, or from different perspectives), rather
367 than response-based learning, that appears to recruit regions outside this extended
368 hippocampal system, specifically the caudate nucleus (Packard and McGaugh,
369 1992; Devan et al., 1996; Chersi and Burgess, 2015). Consistent with this, we
370 observed an association between navigational learning and fornix properties in a
371 task which required participants to navigate to the goal from multiple starting
372 positions.

373

374 Overall, this study provides support for the idea that an individual's spatial navigation
375 ability (Wolbers and Hegarty, 2010) is underpinned, at least in part, by the integrated
376 functioning of a distributed neuroanatomical network, comprising not only individual
377 regions (such as the hippocampus and anterior thalamic nuclei), but also the white

378 matter connections linking these brain areas (Jankowski et al., 2013; Murray et al.,
379 2016). While MWM performance is considered to depend, at least partly, on the
380 ability to form and utilise detailed allocentric mental representations, or “cognitive
381 maps” (Tolman, 1948; O’Keefe and Nadel, 1976), human and animal studies
382 suggest that the role of the fornix in spatial processing may be linked to mechanisms
383 beyond spatial mapping *per se*.

384

385 For instance, while fornix transection impairs, or at least slows, navigational learning
386 in the MWM (Warburton and Aggleton, 1998), as discussed above, these
387 impairments are not as severe as that seen following lesions to the anterior thalamic
388 nuclei or the hippocampus proper (Eichenbaum et al., 1990; Warburton and
389 Aggleton, 1998; Cain et al., 2006). This is not to suggest that fornix connectivity is
390 not important for place representations (Miller and Best, 1980; Shapiro et al., 1989),
391 but rather that the fornix may support processes which help build and support
392 detailed cognitive maps (e.g., scene-based processing, path integration) in
393 conjunction with other brain areas involved in a broader navigation network
394 (Whishaw and Maaswinkel, 1998; Gaffan et al., 2001). For instance, evidence from
395 non-human primates suggests a potential key role in forming conjunctive scene
396 representations (Gaffan, 1991; Hodgetts et al., 2015; Murray et al., 2017). The ability
397 to learn and remember object-in-scene associations, as well as naturalistic scenes,
398 is impaired significantly following fornixectomy (Gaffan, 1992; Gaffan et al., 2001;
399 Buckley et al., 2008).

400

401 Convergent with scene learning deficits reported in monkeys, diffusion MRI studies
402 in humans have reported associations between fornix microstructure and scene
403 recollection (Rudebeck et al., 2009), complex scene discrimination (Postans et al.,
404 2014; Hodgetts et al., 2015) and the ability to retrieve spatiotemporal detail in real-
405 world memories (Hodgetts et al., 2017). Rather than suggesting a selective role in
406 allocentric spatial navigation *per se*, these studies support the view that the
407 connections established by the fornix may be critical for integrating scenes into
408 coherent spatial representations, which then may contribute to the generation of
409 detailed map-like representations useful for navigation (Ryan et al., 2010; Fidalgo
410 and Martin, 2016). An alternative account (Relational Memory Theory), by contrast,
411 posits that while the extended hippocampal system is essential to spatial navigation
412 via a cognitive map, its role derives from the relational organization and flexibility of
413 cognitive maps and not from a selective role in the spatial domain (Eichenbaum,
414 2017; see also Ekstrom and Ranganath, 2017). The initial formation of such flexible
415 spatial relations has been argued to critically rely on cholinergic system modulation
416 of the hippocampus (Ikonen et al., 2002), which is dependent on the fornix (Alonso et
417 al., 1996), consistent with our findings.

418

419 Note, it is possible that some individual differences in navigational performance may
420 actually reflect differences in types of spatial strategies employed. For instance,
421 while some individuals may use a strategy akin to cognitive mapping, i.e., based on
422 allocentric vectors from the “landmarks” to the hidden sensor, some individuals may
423 use a strategy based on matching and integrating disparate viewpoints from the
424 sensor location; a strategy more akin to building a model of the broader scene and

425 layout (Wolbers and Wiener, 2014). While participants were not asked about their
426 use of spatial strategies in the current study, this would be an interesting avenue for
427 disentangling scene-based and cognitive mapping approaches in future studies.

428

429 While our findings support the notion that an extended hippocampal-based system,
430 mediated by the fornix, may be important for navigational learning in humans, it was
431 notable that the fornix association was present when controlling for HC volume.
432 Further, there was no independent association between place learning and HC
433 volume in this task. Though some studies have found associations between
434 hippocampal grey matter volume and navigational ability in humans (Maguire et al.,
435 1997; Bohbot et al., 1998; Schinazi et al., 2013; Chrastil et al., 2017), others have
436 shown that fornix microstructure (but not hippocampal volume) predicts individual
437 differences in remembering spatiotemporal aspects of autobiographical memories
438 (e.g., Hodgetts et al., 2017). In addition, studies of individuals with profound
439 orientation deficits (termed development topographical disorientation, or DTD)
440 similarly show impairments in connectivity patterns to the hippocampus (in this case,
441 between hippocampus and prefrontal cortex). Interestingly, like in our study,
442 hippocampal grey matter does not appear to explain these differences (Iaria et al.,
443 2009; Iaria and Barton, 2010). This highlights that variation in broader
444 neuroanatomical systems, rather than regional volumetric variation, may be
445 particularly sensitive to individual differences in navigational learning.

446

447 Similar to our previous work, we observed stronger effects for fornix MD versus FA
448 (Postans et al., 2014; Hodgetts et al., 2015). The biological interpretation of this

449 difference is not straightforward, as variation in either measure could arise from
450 multiple aspect(s) of the underlying white matter, including axon density, axon
451 diameter, myelination, and the manner in which fibres are arranged in a voxel
452 (Beaulieu, 2002). A recent study reported strong correspondence between DTI
453 microstructural indices and underlying myelin microstructure, where high FA was
454 linked to high myelin density and a sharply tuned histological orientation profile,
455 whereas high MD was related to diffuse histological orientation and low myelin
456 density (Seehaus et al., 2015). Diffusion MRI studies applying more advanced
457 biophysical models of white matter microstructure may be able to provide additional
458 insight into the specific biological attributes underlying these brain-behaviour
459 associations (Assaf et al., 2017; Huber et al., 2018).

460

461 The causes of inter-individual variation in white matter microstructure are not fully
462 understood, but likely involve a complex interplay between genetic and
463 environmental factors over the lifespan. Evidence from both adults and neonates, for
464 instance, suggests that the microstructure of the fornix is highly heritable (Lee et al.,
465 2015; Budisavljevic et al., 2016). The fornix is also one the earliest white matter
466 tracts to mature, reaching its peak FA and minimum MD before age 20 (Lebel et al.,
467 2012), and potentially nearing maturation during infancy and childhood (Dubois et
468 al., 2008). At the same time, evidence suggests that fornix microstructure displays
469 learning-related plasticity, even over short time periods. For instance, short-term
470 spatial learning, in both rodents and humans, has been shown to induce alterations
471 in diffusion indices of fornix microstructure (Hofstetter et al., 2013). Similarly,
472 navigational ability is influenced by both genetic factors and experience (Lee and
473 Spelke, 2010; Wolbers and Hegarty, 2010). Thus, fornix microstructure is likely to

474 both shape, and be shaped by spatial navigation, in a bidirectional fashion (Bechler
475 et al., 2018).

476

477 To conclude, by modelling learning performance on a virtual-reality water maze, we
478 showed that the microstructure of the main white matter pathway linking the
479 hippocampus and medial diencephalon – the fornix – predicted individual differences
480 in human navigational learning. These results suggest that a full understanding of
481 the biological underpinnings of individual differences in human navigational ability
482 requires not only the analysis of individual processing regions, but of a distributed
483 “navigation system”, underpinned by white matter. Critically, given the vulnerability of
484 this brain system to the deleterious effects of aging (Lester et al., 2017), but also
485 pathology in Alzheimer’s disease (Braak and Braak, 1991; Oishi et al., 2012), it is a
486 key priority to develop behavioural markers of navigational ability that are sensitive to
487 individual variation in this network, as seen here. One study in rodents, for instance,
488 found that poorer learning on the MWM in early life predicted cognitive impairment in
489 later life, but also that extensive training in poorer learners buffered against age-
490 related learning impairments (Hullinger and Burger, 2015). Studies such as this
491 highlight the potential of navigational learning, particularly as assessed using
492 translation paradigms (Possin et al., 2016), for characterising, and potentially
493 ameliorating, the effects of cognitive decline.

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748 **Author contributions**

749 CJH, MS, BK, ADE and KSG contributed to the conception and design of the
750 experiment; MS collected imaging and behavioural data; CJH, MS, ANW, BK and JZ
751 analysed the data; CJH wrote the manuscript with input from all other authors.

752

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