

1 Cholesterol depletion by M $\beta$ CD enhances membrane tension, its heterogeneity and affects  
2 cellular integrity.

3 Arikta Biswas, Purba Kashyap, Sanchari Datta, Titas Sengupta, Bidisha Sinha\*

4 Dept. of Biological Sciences, Indian Institute of Science Education and Research (IISER)

5 Kolkata, Mohanpur - 741246, West Bengal, India

6 \* Corresponding author (email – [bidisha.sinha@iiserkol.ac.in](mailto:bidisha.sinha@iiserkol.ac.in))

7

### 8 **Abstract:**

9 Cholesterol depletion in cells by M $\beta$ CD remodels the plasma membrane's mechanics and its  
10 interactions with the underlying cytoskeleton. Decoupling the two effects and studying various  
11 alterations to the membrane's mechanical parameters is important for understanding  
12 cholesterol's role in cellular response to stress. By mapping membrane height fluctuations in  
13 single cells, we report that M $\beta$ CD treatment reduces temporal fluctuations and flattens out the  
14 membrane – but does not suppress activity-driven fluctuations. We find that membrane tension  
15 increase contributes most to the altered fluctuations, among the multiple mechanical  
16 parameters computed. Maps also reveal an enhanced long-range heterogeneity within single  
17 cells, both in amplitude of fluctuations and membrane tension on cholesterol depletion. To  
18 check if this alters the tenacity of membrane to mechanical stress we use hypo-osmotic shock.  
19 We find that on M $\beta$ CD treatment, cells are more prone to rupture than control cells, and this is  
20 not hindered by actomyosin perturbations. We report increased rupture sizes on cholesterol  
21 depletion and argue that, together, this indicates decreased lysis and line tension. Therefore,  
22 we show that cholesterol depletion directly affects cell membranes not only by enhancing  
23 membrane-cytoskeleton interactions, but also by increasing membrane tension while reducing  
24 lysis tension – hence making cells prone to rupture.

## 1 INTRODUCTION

2 Cholesterol is one of the key components of cell membranes in mammalian cells <sup>1,2</sup> and  
3 implicated in several cellular functions <sup>3-8</sup> including the formation of membrane structures  
4 essential for cellular integrity <sup>9-12</sup> during stress. Although for some cell types, cholesterol-  
5 sensitive structures like caveolae are important <sup>9,13,14</sup> for tension regulation during stress, red  
6 blood cells (RBCs) -devoid of caveolae- are known to rupture solely by cholesterol depletion  
7 <sup>15</sup>. Cholesterol is thus a critical factor in cell membrane tension regulation <sup>16</sup> since it can impact  
8 the different physical mechanisms used for membrane homeostasis <sup>17</sup>. In model membranes,  
9 cholesterol content not only alters the basic mechanical parameters like bending rigidity <sup>18</sup> and  
10 elastic modulus <sup>19</sup> but also the resistance to rupturing on stress (increasing the line tension <sup>20</sup>).  
11 We therefore ask how cholesterol depletion in cells affects the membrane topology and  
12 dynamics; membrane tension and interaction with cytoskeleton; and cellular integrity on stress.  
13 Cholesterol is depleted by methyl-beta-cyclodextrin (M $\beta$ CD) which encapsulates hydrophobic  
14 entities of the plasma membrane in its inner hydrophobic cavity <sup>21</sup> and extracts cholesterol from  
15 the outer leaflet continuously <sup>22</sup>. Besides its use in cell biology research for cholesterol  
16 extraction <sup>22</sup>, it is also proposed as a drug carrier in anticancer therapies <sup>23</sup>. While its general  
17 effect on tension regulation is not well understood, its impact on membrane mechanics has  
18 been extensively studied by micropipette-aspiration and tether force measurements.  
19 Micropipette aspiration studies report increased membrane stiffening on cholesterol depletion  
20 but show that the integrity of F-actin is essential for this stiffening <sup>3</sup>. While tether force  
21 measurements show that removal or addition of cholesterol to plasma membranes of cells alters  
22 the apparent membrane tension, bending modulus and effective viscosity, increase in  
23 membrane-cytoskeleton adhesion is implicated in increasing the tether force <sup>7,24</sup>. Others  
24 techniques have demonstrated that although cholesterol enrichment reduces the membrane-  
25 cytoskeleton adhesion, it does not change the global cell stiffness <sup>7</sup>, probably due to the

1 alteration in the “deep” cytoskeleton rheology<sup>25</sup>. While in model membranes tether force  
2 measurements can lead to a clear understanding of the effect of cholesterol on membrane  
3 mechanics, there is no such clarity for plasma membranes in live cells – especially due to the  
4 contribution of membrane-cytoskeleton adhesion on the measured apparent membrane tension.  
5 To circumvent this, we use interference reflection microscopy (IRM) to map spatio-temporal  
6 membrane fluctuations in live cells and study the effect of M $\beta$ CD. IRM provides direct  
7 information about the membrane topology<sup>26</sup>, its spatial parameters (correlation lengths) as well  
8 as about the dynamics (correlation timescales, power spectral density, standard deviation (SD)  
9 of fluctuations and spatial heterogeneity of fluctuations)<sup>27</sup>. Further comparison with theoretical  
10 models help extract the viscoelastic parameters like effective viscosity, membrane tension and  
11 confinement parameter. Thus, a detailed picture of the membrane can be accessed by IRM  
12 allowing separate evaluations of changes in membrane tension and that in the membrane-  
13 cytoskeletal adhesions.

14 Besides altering the membrane tension, cholesterol content can change the lysis tension in  
15 model membranes. Does this also happen in cells? The ability to resist lysis is an important  
16 property of lipid membranes in cells<sup>28</sup>. However, stresses generated or received by organs  
17 (flow of fluid on endothelial cells, flow of RBCs, continuous stretching and relaxation of  
18 muscles, etc.) can generate physiological ruptures<sup>29</sup>. Cells rupture when a critical tension (lysis  
19 tension) is overcome and the area strain on lipids crosses a threshold. Theoretical studies  
20 indicate that while pores of sizes below a critical radius rapidly reseal by line tension, larger  
21 pores make the membrane unstable<sup>20,28</sup>. Thus, pores which are responsible for rupturing reach  
22 a critical radius when the critical tension is attained. Membrane rupture has been studied either  
23 by electroporation<sup>20,28</sup> or photoinduced membrane ablation<sup>30</sup>. Unlike these techniques that  
24 apply local stresses at specific locations on membranes, physiological stresses are global  
25 stresses. To understand how cholesterol depletion alters cell membrane integrity, we

1 administer a global mechanical stress (hypo-osmotic shock) on cells and measure the  
2 percentage of cells that rupture (propensity) and the kinetics of the decay of trapped  
3 fluorophores from the ruptured cells. The latter helps us estimate the rupture pore diameter.  
4 Comparing with known models of the lysis tension, line tension and rupture/pore diameter  
5 <sup>20,28,31</sup>, we draw inferences about the effect of cholesterol depletion on line and lysis tension.

## 6 **METHODS**

7 **Cell culture and fixation.** HeLa (human, female), CHO-K1 (hamster, female) and C2C12  
8 (mouse) cells are grown in Dulbecco's Modified Essential Medium (DMEM, Gibco, Life  
9 Technologies, USA) supplemented with 10% foetal bovine serum (FBS, Gibco) and 1% Anti-  
10 Anti (Gibco) and maintained at 37°C in a humidified atmosphere with 5% CO<sub>2</sub>.

11 **Preparation of red blood cells (RBCs).** Human RBCs are prepared freshly before each  
12 experiment by pricking the finger of a healthy human donor. The blood (collected in 1.5 mL  
13 tubes) is centrifuged at 1000g at 4°C for 10 mins <sup>32</sup>. The supernatant (consisting of plasma,  
14 white blood cells and platelets) is carefully removed. The pellet containing the RBCs is  
15 resuspended in 1X Hank's Balance Salt Solution (HBSS (+ Calcium Chloride, + Magnesium  
16 Chloride), Gibco). 150 µl of this resuspended solution is plated on fibronectin (25 µg/ml)  
17 coated coverslips and incubated at 37°C for 3 hrs.

18 **Staining for cholesterol.** HeLa cells, seeded at a concentration of about 20,000 cells/ml  
19 (between passages 3 and 17) are deposited on customized glass bottomed dishes and all  
20 experiments are performed after 16 hrs of seeding. For staining cholesterol, cells are fixed with  
21 4% paraformaldehyde (Sigma, USA) for 15 mins, washed thoroughly with 1X phosphate buffer  
22 saline (PBS, Sigma) and then incubated in 0.1 M glycine (Sigma) for 5 mins. They are washed  
23 well and then incubated with 0.05 mg/ml Filipin III (Santa Cruz Biotechnology, USA) in the  
24 dark for 2 hrs <sup>33</sup>. Cells are always washed before imaging.

1 **Pharmacological treatments.** Cells are incubated with 5  $\mu$ M Cytochalasin D (Cyto D, Sigma)  
2 for 60 mins to inhibit the polymerization of actin filaments<sup>34</sup>. To deplete the cells of cellular  
3 activity, 10 mM sodium azide (Sigma) and 10 mM 2-deoxy D-glucose (Sigma) are added to  
4 cells in M1 Imaging medium (150 mM NaCl (Sigma), 1 mM MgCl<sub>2</sub> (Merck, USA) and 20 mM  
5 HEPES (Sigma)) and incubated for 60 mins<sup>35</sup>. For cholesterol depletion, cells are incubated  
6 with 10 mM methyl-beta-cyclodextrin (M $\beta$ CD, Sigma) in FBS free DMEM for 50 mins<sup>10</sup>. For  
7 dual drug treatments, cells in serum-free medium are treated first with Cyto D for 60 mins and  
8 then with M $\beta$ CD for 50 mins without replacing the medium (Cyto D + M $\beta$ CD). The reverse  
9 order of treatments is denoted as M $\beta$ CD + Cyto D in the study. All the incubations are done at  
10 37 °C.

11 **Fluctuations based experiments.** Cells are imaged in an onstage 37 °C incubator (Tokai Hit,  
12 Japan) atop a Nikon Eclipse Ti-E motorized inverted microscope (Nikon, Japan) equipped with  
13 adjustable field and aperture diaphragms, 60X Plan Apo (NA 1.22, water immersion), a 1.5X  
14 external magnification and an EMCCD (Evolve 512 Delta, Photometrics, USA). For IRM, an  
15 additional 100 W mercury arc lamp, an interference filter (546  $\pm$  12 nm) and a 50-50 beam  
16 splitter is used as described in<sup>27</sup> and time-lapse images are recorded at EM gain 30 and  
17 exposure time 50 msec for 102 secs at 19.91 frames/sec (2048 frames).

18 **Hypo-osmotic shock induced rupture experiments.** Cells (HeLa and RBCs) are incubated  
19 with 2.5  $\mu$ M Calcein AM (Invitrogen) at 37 °C for 30 mins. They are washed well before fresh  
20 medium (with/without drugs) is added for further experiments. Epifluorescent images are  
21 acquired on the same microscope and camera (used above) with a 10X Plan Apo (NA 0.45,  
22 dry) and a 1.5X external. To calculate rupture diameter, image stacks of Calcein AM loaded  
23 cells are captured (using the FITC filter set) at 100 ms and 0.5 frames/sec for 5 mins. A mixture  
24 of DMEM and deionized water (in the ratio 1:19, 95% hypo-osmotic shock) is then added to

1 the cells and image stacks with the same acquisition settings are captured. For RBCs, the hypo-  
2 osmotic shock is 67% and acquisition rate is 2 frames/sec. To calculate rupture propensity,  
3 dishes of Calcein AM loaded cells are scanned and multiple fields of these cells are captured  
4 in the differential interference contrast (DIC) and epifluorescence modes 15-30 mins after the  
5 hypo-osmotic shock administration.

6 **Calculation of spatio-temporal fluctuations parameters.** MATLAB is used to calculate the  
7 relative height of basal plasma membrane of the cell from the intensities in each pixel of an  
8 IRM image by comparing with images of beads (60  $\mu\text{m}$  diameter polystyrene beads, Bangs  
9 Labs.) imaged on the same day as explained in <sup>27</sup>. Parameters of temporal fluctuations and  
10 spatial undulations in the first branch regions (FBRs, these are regions lying in the first branch  
11 of the interference pattern and limited to 12 x 12 pixels for consistency of analysis) are then  
12 calculated as in <sup>27</sup>. The parameters of spatial undulations include  $SD_{(\text{space})}$  (calculated from  
13 standard deviation (SD) of relative heights across 144 pixels in an FBR, averaged over 20  
14 frames) and correlation length,  $\lambda$  (calculated from spatial autocorrelation functions (ACFs)  
15 across 350 pixels, averaged over 200 frames). The parameters of temporal fluctuations  
16 comprise of mean relative height,  $SD_{(\text{time})}$  (mean and SD of relative heights calculated  
17 respectively in each pixel over 2048 frames and averaged across 144 pixels),  
18  $\overline{\sigma(0.01 \text{ Hz}, 0.1 \text{ Hz})}$ ,  $\overline{\sigma(0.1 \text{ Hz}, 1 \text{ Hz})}$  (calculated as root of the total area under the power  
19 spectral density (PSD) curve between the mentioned frequencies), exponent (calculated as the  
20 linear slope between 0.04-0.4 Hz of the PSD in the log-scale),  $f$  (calculated as the ratio between  
21 background subtracted PSD of treated to control) and correlation time,  $\tau$  (calculated from  
22 temporal ACFs over 2048 frames, averaged over 4 pixels). The Gaussian-ness of temporal  
23 fluctuations is evaluated at each pixel by the Kolmogorov-Smirnov hypothesis testing.  
24 Mechanical parameters  $A$ ,  $\eta_{\text{eff}}$ ,  $\gamma$ ,  $\kappa$ ,  $\mu$  and  $\sigma$  are computed from fitting the PSDs of FBRs to

1  $PSD(f) = \frac{4\eta_{eff}Ak_B T}{\pi} \int_{q_{min}}^{q_{max}} \frac{dq}{(4\eta_{eff}(2\pi f))^2 + [\kappa q^3 + \frac{9k_B T}{16\pi\kappa}\mu q + \sigma q + \frac{\gamma}{q}]^2}$ . Short-range heterogeneity in

2 cells is measured by  $SD(SD_{(time)})$  (calculated from SD of  $SD_{(time)}$  of pixels over 2048 frames  
3 and across 144 pixels) and long-range heterogeneity is calculated by percentage of dissimilar  
4 FBR pairs (calculated as ratio of number of dissimilar FBR pairs (p-values < 0.001) to total  
5 number of FBR pairs; the  $SD_{(time)}$  of all 144 pixels in an FBR is statistically compared to those  
6 in every possible FBRs in pairs, and p-value from a one-way Analysis of Variance (ANOVA)  
7 is calculated). Dissimilar FBR pairs in terms of mean relative height are evaluated from the  
8 ratio of the number of FBR pairs with dissimilar mean relative heights (p < 0.001, one-way  
9 ANOVA) to the total number of FBR pairs. The  $\log(SD \text{ ratio})$  or  $\log(\sigma \text{ ratio})$  is computed as  
10 the ratio of  $SD_{(time)}$  or  $\sigma$  between FBR pairs (bigger value to smaller value) in both dissimilar  
11 and similar sets.

12 **Calculation of rupture propensity.** 15-30 mins after the application of a hypo-osmotic shock,  
13 the total number of cells ( $N_t$ ) present in each field is counted from the DIC images. The total  
14 number of Calcein AM loaded fluorescent cells ( $N_{nr}$ ) in the same field is counted from the  
15 epifluorescent images and the rupture propensity ( $R_p$ ) in that field is calculated as:

16  $Rupture \ propensity = \frac{(N_t - N_{nr})}{N_t}$

17 **Calculation of rupture diameter.** The lipophilic and non-fluorescent Calcein AM can  
18 permeate inside live cells. In the presence of esterases in such cells, the acetoxymethyl group  
19 are cleaved trapping the Calcein (not lipophilic and fluorescent in green) molecules<sup>30,36</sup>. The  
20 trapped Calcein moves out of the cell when it ruptures and hence a rupture corresponds to a  
21 sudden drop in the Calcein intensity in the cell.

22 A model based on simple diffusion (Calcein moves out of the cell by diffusion through the  
23 rupture site) is used to calculate the rupture diameter<sup>30</sup>. This model assumes a cell with  
24 membrane thickness ( $l$ ) and a volume ( $V$ ) to undergo a single point rupture and the rupture

1 pore is assumed to be a cylinder, of length  $l$ , radius  $r$  and cross-section area  $A = \pi r^2$ . To  
2 determine the expected temporal evolution of Calcein concentration ( $c(t)$ ) in the cell, the  
3 expected flux ( $j$ ) is compared with Fick's law. Flux, the number of Calcein particles crossing  
4 the membrane per unit area per unit time is expressed as  $j = -\frac{dN}{Adt} = -\frac{Vdc}{Adt}$ . By Fick's law,  
5 we know,  $j = -D\frac{dc}{dx}$ , where  $D$  is the diffusion constant of Calcein and  $\frac{dc}{dx}$  the concentration  
6 gradient across the pore. Or,  $j = -D\frac{\Delta c}{l}$  where  $\Delta c = c_{out} - c_{in} = -c$  assuming Calcein  
7 concentration outside to be 0. Therefore,  $-\frac{Vdc}{Adt} = D\frac{c}{l}$  or,  $\frac{dc}{c} = -\frac{D.A dt}{V.l}$ . Integration yields,  $c(t)$   
8  $= c(0) \cdot e^{-\frac{t}{\tau_r}}$  where,  $\tau_r = \frac{Vl}{AD}$ . Therefore, the concentration evolution of the flow of Calcein  
9 from inside to outside follows an exponential.

10 A region inside the ruptured cell is selected and its normalized mean intensity (mean intensity  
11 of region in each frame is divided by the mean intensity in the first frame) is plotted with time  
12 using a program written in MATLAB. Two points are chosen such that one marks the start of  
13 this drop and the other marks the trailing end. All data points within this region are fitted to a  
14 double exponential,  $f(t) = Ae^{-bt} + Ce^{-dt}$ . The damping constant  $b$  is used to calculate  $\tau_r$   
15 ( $\tau_r = \frac{1}{b}$ ) while the other represents the photobleaching in the system, if any. Assuming the  
16 radius ( $R$ ) of a typical HeLa cell is  $20 \mu\text{m}$  (and  $V = \frac{4\pi R^3}{3}$  and  $V = 100 \mu\text{m}^3$  for RBCs),  $l$  is  $7$   
17  $\text{nm}$  and  $D$  is  $330 \mu\text{m}^2/\text{s}$ , the rupture diameter,  $r_D(2\tau)$  is calculated from:  $r_D = 2\sqrt{\frac{Vl}{\pi\tau_r D}}$ .

18 **Statistical Analysis.** For fluctuations-based experiments, calibration with beads and control  
19 experiment with cells without any treatment are performed with each set of experiment. At  
20 least 10 cells are imaged for each condition and  $\sim 20$ - $40$  FBRs analysed for each cell. In most  
21 cases, analysis is collated over at least three sets of experiments performed on different days.  
22 For comparisons between populations of cells, a one-way ANOVA combined with a Tukey  
23 post-hoc test is performed to determine the statistical significance (\* denotes  $p < 0.05$ , \*\*



1 denoted  $p < 0.001$ ) whenever the parameters have similar variances and have Gaussian  
2 distributions. A Mann-Whitney U test is done whenever the parameters are not Gaussian  
3 (checked if the mean and median values are not similar). The experiments with hypo-osmotic  
4 shock are done on at least three days. Rupture diameter is calculated from multiple cells in a  
5 single field in each day and rupture propensity is calculated from multiple fields imaged in a  
6 day. Values of rupture propensity higher than mean + 2SD are considered as outliers are  
7 removed for the box plots. A Mann-Whitney U test is done to determine the statistical  
8 significance (\* denotes  $p < 0.05$ , \*\* denoted  $p < 0.001$ ). No specific tests are done to check the  
9 normality of the data.

## 10 **DATA AVAILABILITY**

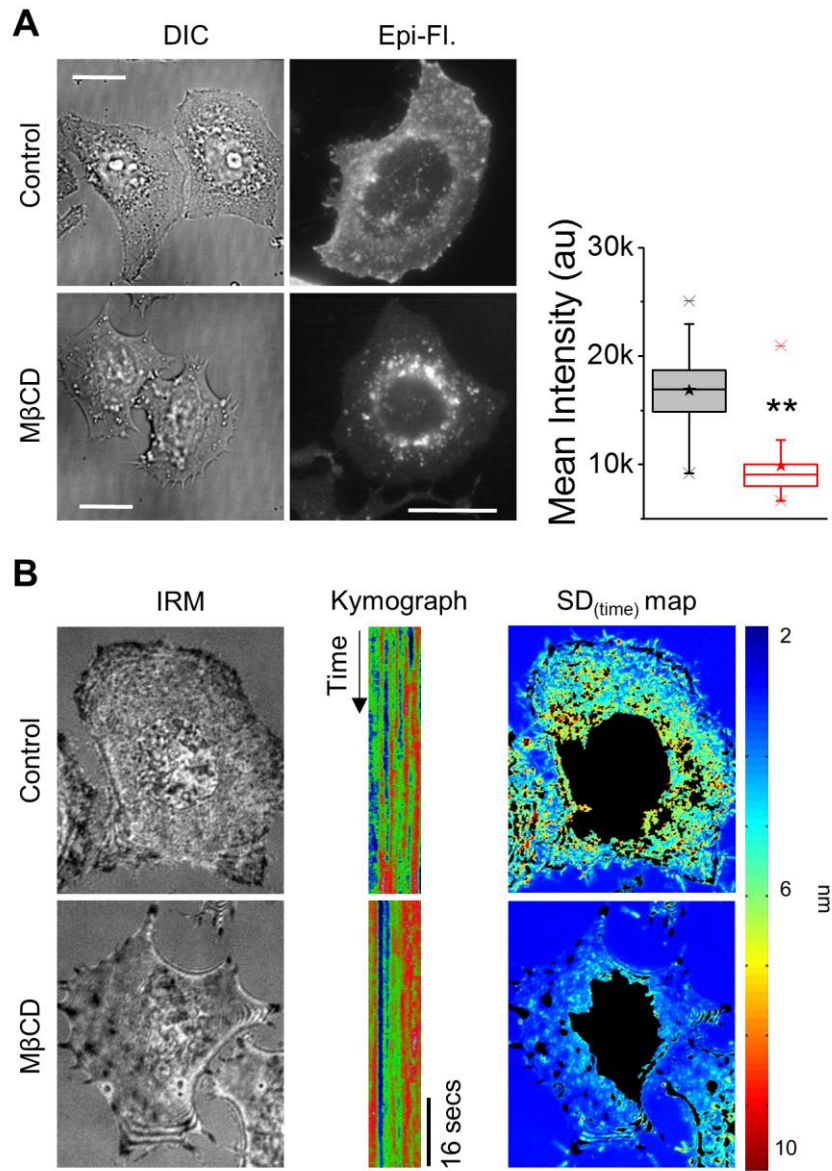
11 The datasets generated and analysed during the current study are available from the  
12 corresponding author on reasonable request.

## 13 **RESULTS**

### 14 M $\beta$ CD treatment decreases temporal fluctuations and flattens out spatial undulations

15 HeLa cells are depleted of cholesterol by M $\beta$ CD and stained with Filipin III to check for  
16 cholesterol depletion (Fig. 1 A, *left*). As seen in earlier reports<sup>37</sup>, images show filipin staining  
17 at the plasma membrane in control cells which is lost on M $\beta$ CD treatment, thereby, increasing  
18 the contrast of the intracellular vesicles. A quantification of mean Filipin III fluorescence at  
19 the membrane shows a ~40% (N = 30 cells) decrease on cholesterol depletion (Fig. 1 A, *right*).  
20 Imaging cells in the IRM mode (Fig. 1 B, *left* and Movie S1) reveals that the topology and  
21 dynamics of the basal plasma membrane is significantly altered on M $\beta$ CD treatment. The  
22 changes in the dynamics can be visualized by the color-coded kymographs (Fig. 1 B, *middle*)  
23 which show reduced variations after cholesterol depletion. Next, we convert intensity in the  
24 images to relative heights<sup>27</sup> and quantify various spatio-temporal parameters of the height-

1 fluctuations. The amplitude of the temporal fluctuations ( $SD_{(time)}$ ) reduces on M $\beta$ CD treatment.  
2 This is evident from  $SD_{(time)}$  maps (Figs. 1 B, *right* and S1 A-B) as well as from statistics  
3 obtained from ~1500 first branch regions (FBRs) across ~70 cells per condition. There is a  
4 slight but significant decrease in the amplitude obtained from spatial maps ( $SD_{(space)}$ ) for the  
5 same sets of cells (Fig. S1 C). Together, these data imply that spatio-temporal fluctuations are  
6 damped on cholesterol depletion. Though the reduction in power-spectral density (Fig. 2 A) is  
7 observed to be more prominent at lower frequencies (~ 0.01- 0.1 Hz) (Fig. 2 A, *inset*), the  
8 calculated amplitudes ( $\bar{\sigma}$ ) at both frequency bands – 0.01-0.1 Hz and 0.1-1 Hz – show a  
9 significant reduction on cholesterol depletion (Fig. 2 B). The PSD's power-law dependence on  
10 frequency, captured by the exponent, increases (from -4/3 to -1) on M $\beta$ CD treatment (Fig. S1  
11 D), implying increased damping<sup>38,39</sup>.



1

2 **Figure 1: Effect of MβCD mediated cholesterol depletion on membrane topology.**

3 A) Representative DIC and epifluorescent images of Filipin III stained control and MβCD  
4 treated HeLa cells. Right: Box plot of mean intensity of Filipin III in cells in mentioned  
5 conditions (N = 30 cells each). Centre lines of boxes show the medians; stars show the  
6 means; boxes limits indicate the 25th and 75th percentiles; and whiskers extend 1.5  
7 times the interquartile range from the 25th and 75th percentiles. \*\* p value < 0.001,  
8 Mann-Whitney U test.

9 B) Representative IRM (left) images, kymographs of 1 μm regions (middle, scale bar: 16  
10 secs) and SD<sub>(time)</sub> maps of control vs. MβCD treated cells (non FBRs blacked out).

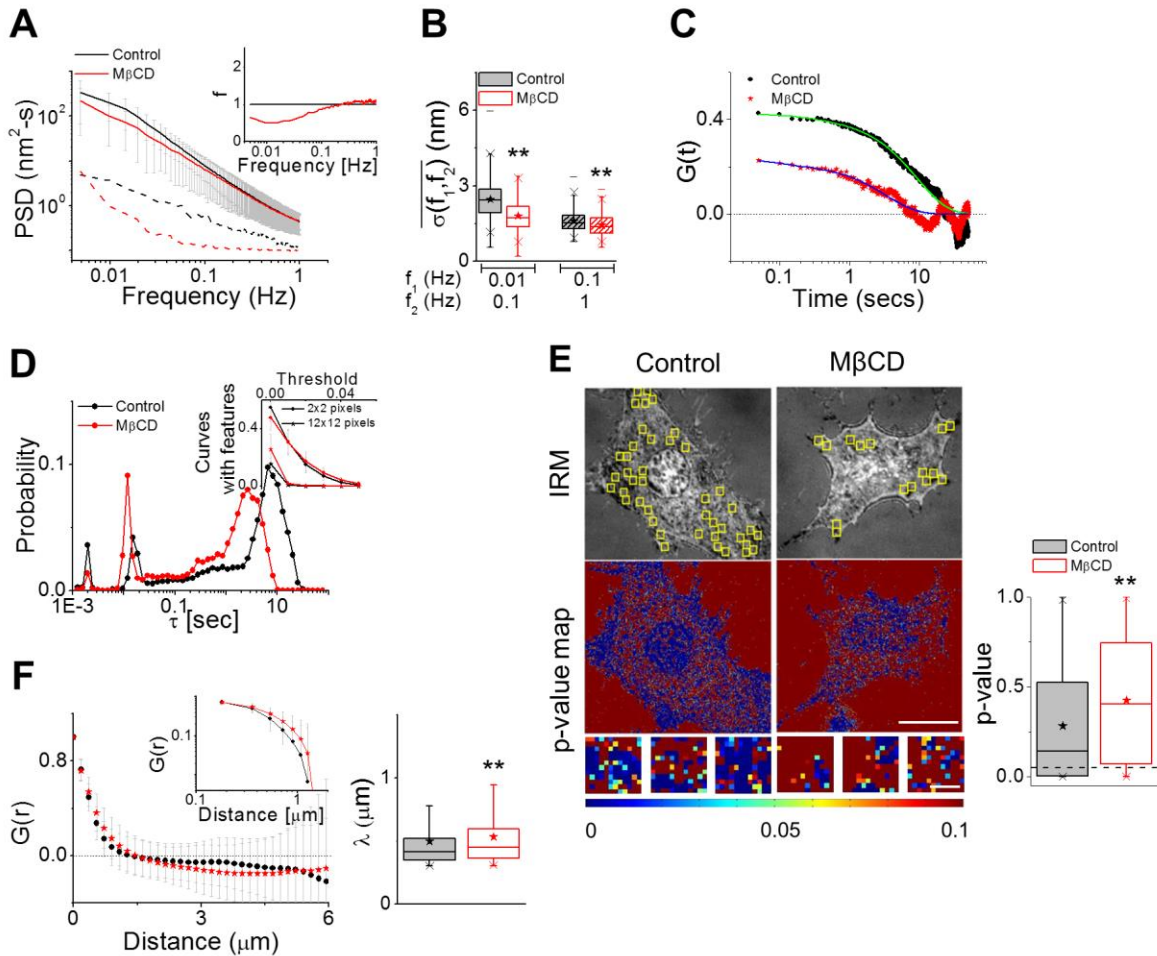
11 Scale bar: 10 μm. See Table S1 for statistics.

12

13 We next analyse the temporal data to understand how cholesterol depletion affects the

14 contribution of activity-driven processes to the observed fluctuations. We, first, compute the

1 temporal ACFs and find reduced correlation strengths on M $\beta$ CD treatment (Fig. 2 C). While  
2 this is expected, since reduced fluctuations decrease the signal to noise ratio, we also check for  
3 signatures of active fluctuations by extracting the correlation timescales ( $\tau$ ). Surprisingly, the  
4 distribution of correlation timescales still retains peaks in the 0.2-2 sec range (Fig. 2 D). This  
5 range is usually under-represented when ATP-dependent metabolic activity is hampered by  
6 ATP depletion<sup>27</sup> The other signature of active fluctuations is the presence of “bumps” in ACFs  
7 which are known to be affected by ATP depletion<sup>27,40</sup> On cholesterol depletion, in this study,  
8 we find that similar proportions of ACFs have “bumps” (Fig. 2 D, *inset*). Increasing the region  
9 of averaging from 2x2 pixels (0.36  $\mu$ m x 0.36  $\mu$ m) to 12x12 pixels (2.14  $\mu$ m x 2.14  $\mu$ m), we  
10 find the proportion of ACFs with bumps to decrease – suggesting that localized ATP-dependent  
11 processes still affect membrane fluctuations even after cholesterol is depleted. Is the level of  
12 “Gaussian-ness” of fluctuations in these cells also retained? We map the p-values of  
13 Kolmogorov-Smirnov hypothesis testing to quantify similarity of the temporal fluctuations at  
14 each pixel with Gaussian distributions – where higher p-values indicate greater similarity to  
15 Gaussian fluctuations (Fig. 2 E). We find that the p-values increase significantly on M $\beta$ CD  
16 treatment. Such increase may result either from the loss of ATP-dependent fluctuations<sup>27,41</sup> or  
17 may be a result of a reduction in the strength of fluctuations. On analysing data for mitotic  
18 cells, where, fluctuation-strength reduces with respect to interphase cells, we find an increase  
19 in Gaussian-ness. These cells are expected to retain ATP-dependent activities as also  
20 corroborated by existence of correlation timescales at 0.2-2 secs. The level of Gaussian-ness  
21 is, thus, determined more by the strength of the fluctuations than by the presence/absence of  
22 ATP-dependent fluctuations. Together, this indicates that cholesterol depletion reduces  
23 fluctuations without removing activity-driven fluctuations.



1

2 **Figure 2: Cholesterol depletion by MβCD reduces temporal fluctuations without**  
 3 **abrogating the signatures of activity.**

4 A) Averaged PSDs of FBRs in MβCD treated cells and their controls (solid lines) with  
 5 their backgrounds (dashed lines); inset shows  $f$  (ratio of background subtracted PSDs).

6 B) Box plots of  $\sigma(f_1, f_2)$  in two different frequency regimes. (A-B)  $N = 70$  cells each,  
 7  $n_{\text{control}} = 1688$  FBRs,  $n_{\text{M}\beta\text{CD}} = 1474$  FBRs. \*\* p value < 0.001, one-way ANOVA.

8 C) Typical temporal ACFs of single 2x2 pixels FBRs in the two conditions.

9 D) Weighted distribution of correlation timescales obtained from temporal ACFs. Inset  
 10 shows a plot of fraction of curves with features vs. threshold used to detect the features  
 11 ( $n_{\text{control}} = 2890$  fits,  $n_{\text{M}\beta\text{CD}} = 3071$  fits,  $N = 21$  cell each).

12 E) FBRs overlaid in yellow on IRM images and their corresponding whole cell and FBR  
 13 (Scale bar: 1  $\mu\text{m}$ ) p-value maps (Kolmogorov-Smirnov hypothesis testing). Right: p-  
 14 value for FBRs in control vs. cholesterol depleted cells.  $n_{\text{control}} = 53568$  pixels,  $n_{\text{M}\beta\text{CD}} =$   
 15 42480 pixels.

16 F) Averaged spatial ACFs (and their log-log plots, top inset) for control and cholesterol  
 17 depleted cells ( $N = 70$  cells,  $n_{\text{control}} = 624$  FBRs,  $n_{\text{M}\beta\text{CD}} = 541$  FBRs). Right: Correlation  
 18 lengths.

19 \* p value < 0.05, \*\* p value < 0.001, Mann-Whitney U test.

20

1 To understand the alterations to the spatial membrane topology, we first quantify the changes  
2 in relative height. On cholesterol depletion, the average membrane-substrate distance (and its  
3 variability) increases significantly (Fig. S1 E). Autocorrelation function of the spatial height  
4 profiles (Fig. 2 F) show that the correlation length increases significantly (from  $0.49 \pm 0.27 \mu\text{m}$   
5 to  $0.53 \pm 0.28 \mu\text{m}$ ) on M $\beta$ CD treatment. Together with decreased  $SD_{(\text{space})}$ , this implies that  
6 cholesterol depletion spatially flattens the membrane. The trends of altered spatio-temporal  
7 parameters are checked in M $\beta$ CD treated- CHO and C2C12 cells (Fig. S1 F-I). As seen in  
8 HeLa, the other cell lines show reduced amplitudes of temporal fluctuations. Exponent, mean  
9 relative height and correlation length also increase on M $\beta$ CD treatment in these cell lines (like  
10 HeLa).

#### 11 Cholesterol depletion by M $\beta$ CD increases membrane tension and its heterogeneity

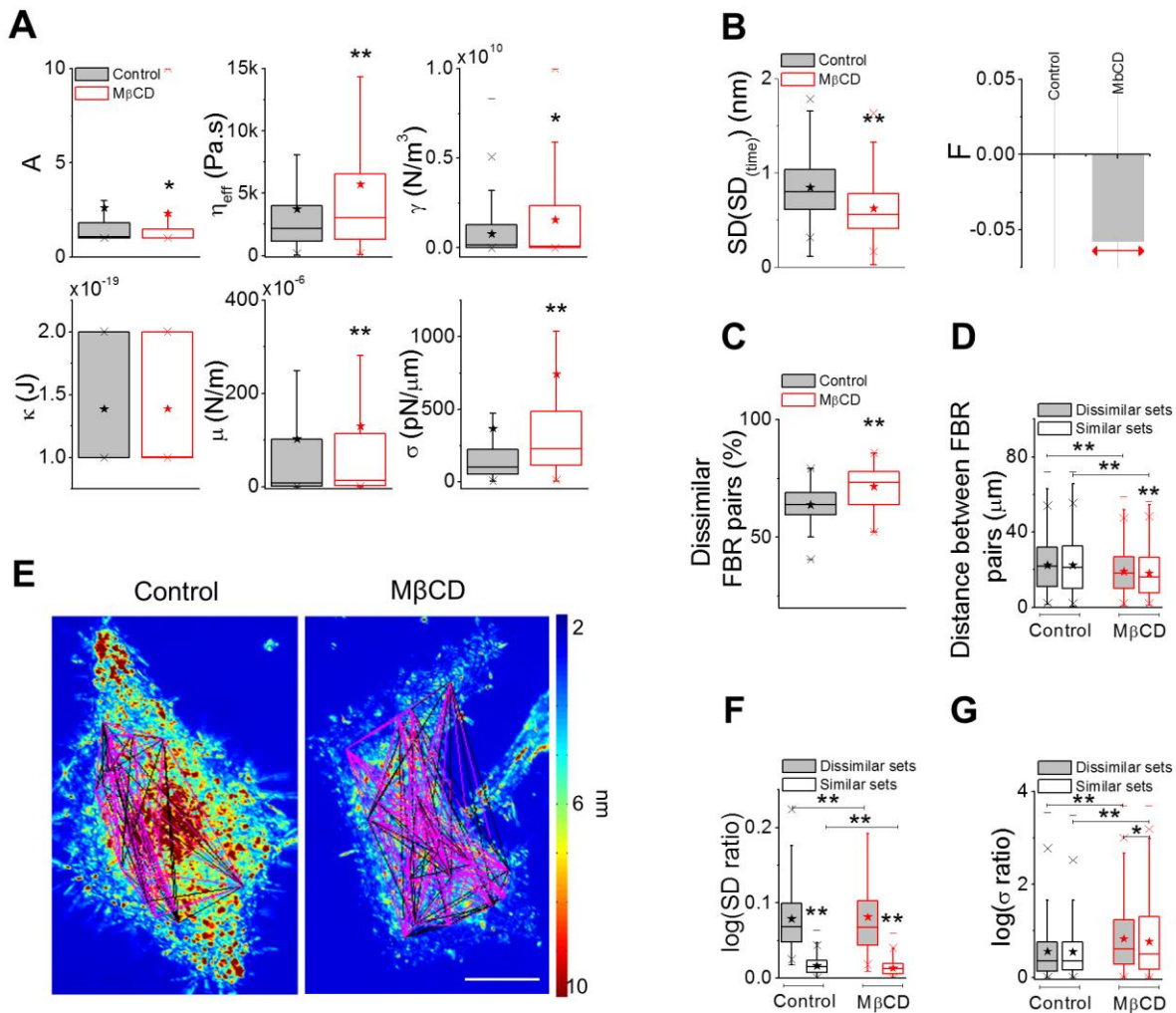
12 We next compute membrane mechanical properties by fitting the PSDs with a theoretical model  
13 <sup>27</sup> to further characterize the effect of cholesterol depletion. The model predicts the PSD for a  
14 confined (confinement,  $\gamma$ ) membrane of defined tension ( $\sigma$ ), bending rigidity ( $\kappa$ ) and shear  
15 modulus ( $\mu$ ) in a viscous surrounding (of effective viscosity,  $\eta_{\text{eff}}$ ) and acted on by active forces  
16 to increase the temperature “A” times <sup>38,40,42,43</sup>. On fitting, we find that while A decreases,  $\eta_{\text{eff}}$ ,  
17  $\gamma$ ,  $\mu$ , and  $\sigma$  increases significantly on M $\beta$ CD treatment (Fig. 3 A). Since multiple parameters  
18 are affected, we next sought to understand which one is the most important in altering the  
19 fluctuation amplitude. For this, we compared the SD of the control set with the SD calculated  
20 from simulated PSDs. The simulated PSDs are generated from different sets of observed fitting  
21 parameters. We chose a whole set of fitting parameters corresponding to a control set and then  
22 changed only one parameter at a time to that of a M $\beta$ CD treated set. This is done for each of  
23 the parameters – A to  $\sigma$ . The ratio of the SD of the original control set and the SD calculated  
24 from the simulated PSD is calculated and the log of these values are plotted to understand the  
25 different contributions. We find that with all other parameters being same to the control,

1 changing  $\sigma$  has the most significant effect in the reduction of SD. Hence, we believe that  
2 although multiple parameters are altered on M $\beta$ CD treatment, alterations in membrane tension  
3 govern the change in fluctuations (Fig. S2 A).

4 We next seek to understand the effect of cholesterol depletion on the spatial heterogeneity and  
5 characterize both short (inside an FBR,  $<2.14 \mu\text{m}$ ) and long-range heterogeneity (distances  
6 ranging from  $2.14 \mu\text{m} - 54 \mu\text{m}$ ). To compute short-range heterogeneity, we calculate the  
7  $\text{SD}(\text{SD}_{(\text{time})})$  and find a reduction in this quantity after M $\beta$ CD treatment (Fig. 3 B, *left*). To  
8 normalize out the effect of the reduced mean, we calculate the Fano factor of the fluctuations  
9 and find a reduction on cholesterol depletion (Fig. 3 B, *right*). Long-range heterogeneity is  
10 calculated by comparing all possible pairs of FBRs in cells and obtaining the p-values (of  
11  $\text{SD}_{(\text{time})\text{S}}$ ) to segregate similar ( $p > 0.001$ ) and dissimilar ( $p < 0.001$ ) FBR pairs. The percentage  
12 of dissimilar FBR pairs increases on cholesterol depletion (Fig. 3 C). To understand what  
13 factors, lead to this increased dissimilarity, we calculate the distance between FBR pairs for all  
14 similar and all dissimilar sets – and compare the mean values of each set. In control cells, there  
15 is no significant difference in the distance between FBR pairs in similar and dissimilar sets.  
16 However, the dissimilar set shows significantly higher mean distance than the similar set in the  
17 cholesterol depleted cells (Fig. 3 D). We visualize the sets (similar: magenta lines, dissimilar:  
18 black lines) in both conditions to understand if there is a correlation between dissimilarity and  
19 their location in cells. We find that neither sets are located at a specific region in the cells – e.g.  
20 cell periphery, perinuclear regions, etc. (Figs. 3 E and S2 B) in any of the two conditions. We  
21 next check if membrane-substrate distances are responsible for the observed increase in long-  
22 range heterogeneity. For this, we compute p-values for all FBR pairs based on their mean  
23 relative heights and find that although dissimilar pairs exist ( $\sim 62\%$ ) – this does not change on  
24 cholesterol depletion (Fig. S2 C, *left*). For these sets of similar and dissimilar FBR pairs, the  
25 distance between pairs do not vary significantly in either of the conditions (Fig. S2 C, *right*).

1 Again, visualizing the connections show that there is no striking correlation to their underlying  
2 mean height profile (Fig. S2 D). Therefore, the increased spatial heterogeneity is neither driven  
3 by altered adhesion state nor by specific intracellular localization. It is important to note that  
4 such long-range spatial heterogeneity is not increased by ATP depletion or cytoskeletal  
5 perturbations, as observed earlier by our group<sup>27</sup>. To check if the dissimilar and similar sets  
6 have different values of SD and  $\sigma$ , we find the  $SD_{(time)}$  ratio (calculated between the bigger and  
7 smaller value for each pair) in every pair of the two sets in each condition. We find that in  
8 control and M $\beta$ CD treated cells, the SD ratio is smaller for similar pairs than the dissimilar  
9 ones (Fig. 3 F). On computing the  $\sigma$  ratio, in the same way, we find that the dissimilar sets in  
10 cholesterol depleted cells have a higher tension than the similar sets (Fig. 3 G). This analysis,  
11 along with the variability in tension on M $\beta$ CD treatment (Fig. 3 A) confirms that the increased  
12 spatial heterogeneity in fluctuations maps on to the increased heterogeneity in tension.  
13 However, the increase in  $\sigma$  ratio on cholesterol depletion observed in both similar and  
14 dissimilar sets points out that the tension heterogeneity is amplified independent of the  
15 corresponding SD ratios.





1

2 **Figure 3: Membrane mechanical parameters and tension heterogeneity in single cells.**

3 A) Membrane mechanical parameters  $A$ ,  $\eta_{\text{eff}}$ ,  $\kappa$ ,  $\mu$ ,  $\sigma$  and  $\gamma$  obtained from fitting PSDs to  
 4 theoretical model ( $n_{\text{control}} = 1031$  FBRs,  $n_{\text{M}\beta\text{CD}} = 977$  FBRs,  $N = 70$  cells each)

5 B)  $\text{SD}(\text{SD}_{(\text{time})})$  for the two conditions (left) and the Fano factor (right).  $n_{\text{control}} = 1688$  FBRs,  
 6  $n_{\text{M}\beta\text{CD}} = 1474$  FBRs, statistical testing by one-way ANOVA.

7 C) Box plot of the number of dissimilar FBR pairs evaluated by comparing  $\text{SD}_{(\text{time})}$ .  
 8 Statistical testing by one-way ANOVA.

9 D) Distance between FBR pairs that have dissimilar (grey filled) and similar (no filled) SD  
 10 values in the two conditions.  $n_{\text{control}} = 15158$  dissimilar sets, 8148 similar sets;  $n_{\text{M}\beta\text{CD}} =$   
 11 12451 dissimilar sets, 4986 similar sets.

12 E) Lines in magenta and black connect FBRs that are dissimilar and similar in SD values  
 13 respectively. The lines are overlaid on the  $\text{SD}_{(\text{time})}$  maps and each node represents the  
 14 centre of an FBR.

15 F) Box plot of  $\log$  SD ratio of dissimilar and similar sets in control vs. cholesterol treated  
 16 cells.

17 G) Box plot of  $\log$   $\sigma$  ratio of dissimilar and similar sets in the above-mentioned conditions.  
 18  $n_{\text{control}} = 15135$  dissimilar pairs, 8171 similar pairs;  $n_{\text{M}\beta\text{CD}} = 12713$  dissimilar pairs, 4724  
 19 similar pairs.  
 20

1 N = 70 cells each. \* p value < 0.05, \*\* p value < 0.001, Mann-Whitney U test. Scale  
2 bar: 10  $\mu$ m. See Table S1 for statistics.  
3

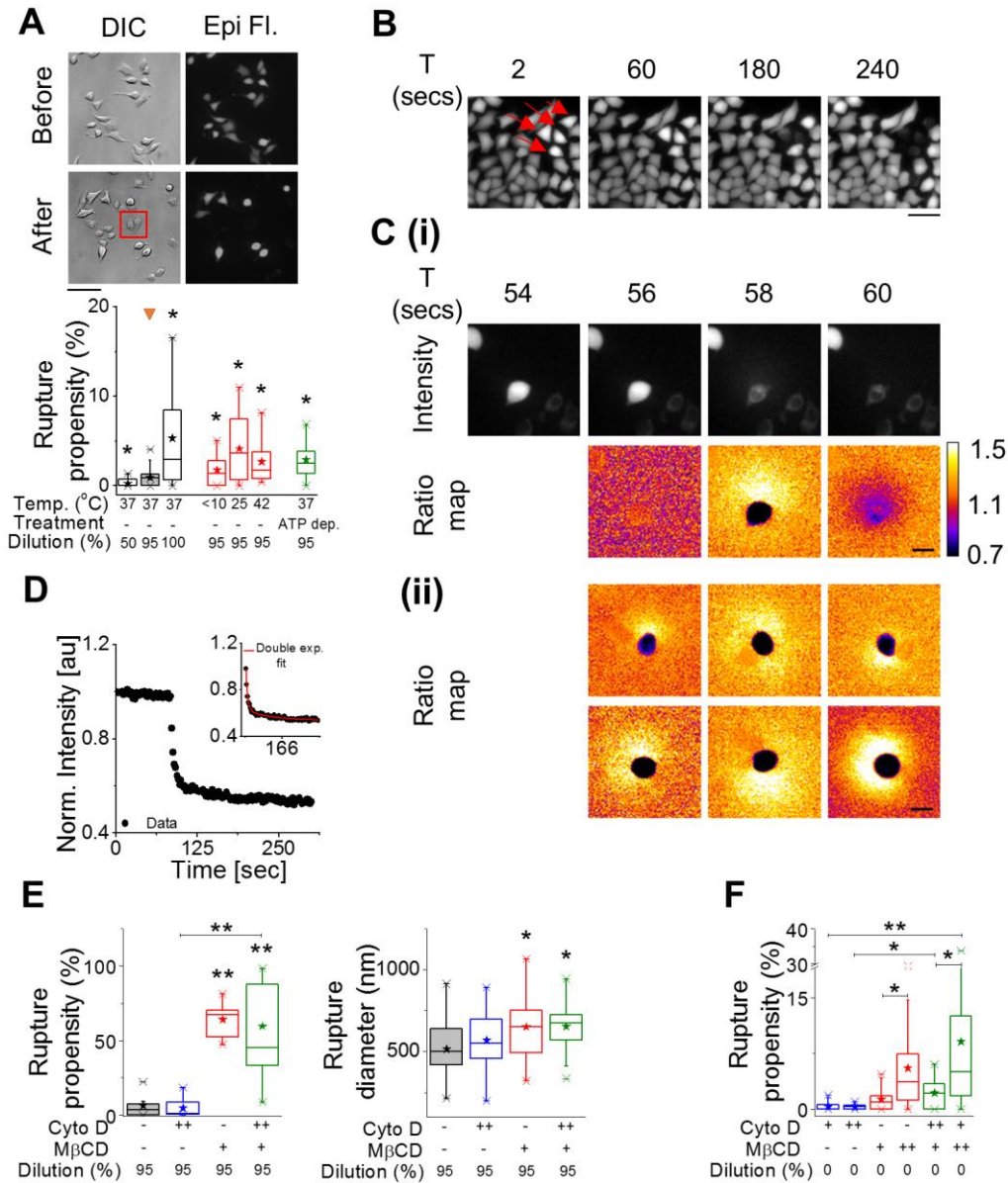
4 There is a decrease in  $SD(SD_{(time)})$  in CHO cells depleted of cholesterol (as in HeLa cells) but  
5 there is no significant change in the short-range heterogeneity in cholesterol depleted C2C12  
6 cells (Fig. S2 E, *left*). The long-range heterogeneity does not show any significant change on  
7 cholesterol depletion in CHO or C2C12 cells (Fig. S2 E, *right*). But, it is noteworthy that, in  
8 both cell lines, M $\beta$ CD treatment leads to an increase in  $\sigma$  and its variability (Fig. S2 F).

9 We compare  $\gamma$  values between control and M $\beta$ CD treated cells to check if our results show  
10 increased membrane-cytoskeleton adhesion as reported earlier<sup>44</sup>. We find that, for HeLa cells,  
11 there is a significant increase in  $\gamma$  on M $\beta$ CD treatment.  $\gamma$  defines the overall confinement - due  
12 to membrane-cytoskeleton as well as membrane-substrate interactions. Since cholesterol  
13 depletion increases the membrane-substrate distances (Fig. S1 E), we believe that the  
14 amplification in  $\gamma$  is due to increased membrane-cytoskeletal adhesion. The increase in  
15 damping (higher exponent) and effective viscosity, also, support this inference. In CHO and  
16 C2C12 cells,  $\gamma$  is not significantly altered by M $\beta$ CD treatment. The increase in mean relative  
17 height is also larger in these cell lines, which we believe, may cancel out the effect of  
18 membrane-cytoskeleton attachment. Though the overall increase in membrane-cytoskeleton  
19 adhesion is clear in HeLa cells, the effect is not robust across different days of experiments or  
20 across cell lines. While IRM helps us to estimate membrane tension, we acknowledge that we  
21 cannot separate out the contribution of confinement by the cytoskeleton from that of damping  
22 by the substrate.

23 Therefore, the most robust effect of M $\beta$ CD on membrane mechanics in single cells is to  
24 increase the membrane tension and its spatial heterogeneity. In the next section, we address  
25 how M $\beta$ CD treatment alters the rupture propensity and affects the lysis tension in cells.

1 Hypo-osmotic shock induced membrane rupturing propensity and rupture diameter increases  
2 on M $\beta$ CD mediated cholesterol depletion

3 We use hypo-osmotic shock to impart global mechanical stress (Movies S2 and S3) on cell  
4 membranes and assess its propensity to rupture. We load HeLa cells with Calcein AM and  
5 analyse the cells before and at least 15 mins after hypo-osmotic shock. Cells with ruptured  
6 membrane lose the internal Calcein AM and are hence identified by comparing their absence  
7 in fluorescence images to their presence in DIC images (Fig. 4 A). Rupture propensity is  
8 defined as the percentage of cells that undergo rupturing and it increases on increasing the  
9 strength of the hypo-osmotic shock. Rupture propensity also increases when the temperature is  
10 decreased from 37 °C to <10 °C or 25 °C or increased to 42 °C (Fig. 4 A, *right*). ATP depletion,  
11 too, increases rupture propensity, but only to 5-10% (Fig. 4 A, *right*). We find that RBCs (Fig.  
12 S3 A), in general, have a much higher rupture propensity than HeLa cells. In addition to  
13 calculating rupture propensity, we also follow the Calcein-AM loaded cells (HeLa and RBCs)  
14 after hypo-osmotic shock and find that rupturing events lead to a sudden loss in internal mean  
15 intensity (Figs. 4 B and S3 B). Ratio maps (Fig. 4 C) between consecutive images show that  
16 the rupturing is marked by fluorescence loss from the whole cell and by a simultaneous and  
17 sudden increase of fluorescence in the surrounding medium that is often asymmetric (Figs. 4C  
18 and S3 C). This indicates to a loss of intensity is due to a single-point rupture and is also seen  
19 in RBCs (Fig. S3 C, *left*). Fitting the temporal intensity profile (Figs. 4 D and S3 C, *right*) with  
20 exponential decay functions yields a time-constant which is used to estimate the rupture  
21 diameter based on a simple model that assumes fluorescence loss from the lesion by pure  
22 diffusion.



1

2 **Figure 4: Membrane rupture induced by hypo-osmotic/iso-osmotic medium in the**  
 3 **presence of MβCD.**

4 A) Top: DIC and epifluorescent images of Calcein AM labelled HeLa cells before and  
 5 after the administration of a 95% hypo-osmotic shock (scale bar, 100 μm). Among  
 6 others, the cells in the box are representatives of membrane rupture. Bottom: Box plot  
 7 of rupture propensity of cells due to change in hypoosmotic stress, change in  
 8 temperature and ATP depletion (N = 3 experiments each).

9 B) Top: Time lapse images of Calcein AM loaded HeLa cells undergoing rupture  
 10 (arrowheads in red) (scale bar, 50 μm).

11 C) (i) Intensity and ratio ( $\frac{\text{Intensity of frame}}{\text{Intensity of previous frame}}$ ) map of a rupturing cell followed in  
 12 time to show single point rupture. (ii) Representative ratio maps of six different cells  
 13 showing asymmetric spread of fluorescence after rupture (Scale bar, 30 μm).

14 D) A time profile of normalized mean intensity of a cell; inset shows the double  
 15 exponential fit to the profile.

- 1 E) Box plots of rupture propensity (left) and rupture diameter (right) of 95% hypo-osmotic  
2 shock administered HeLa cells under control, Cyto D (2 hr post treatment), M $\beta$ CD (50  
3 mins post treatment) and Cyto D + M $\beta$ CD conditions (N = 3 experiments each).  
4 F) Box plots of rupture propensity of cells under Cyto D, M $\beta$ CD and dual drug treatments  
5 (N = at least 3 experiments each).  
6 '+' denotes 60 mins treatment (for Cyto D), 50 mins (for M $\beta$ CD), '++' denotes 120 mins  
7 treatment. \* p value < 0.05, \*\* p value < 0.001, Mann-Whitney U test. See Table S1 for  
8 statistics.

9

10 M $\beta$ CD treatment results in an enhanced rupture propensity and an increased rupture diameter  
11 on hypo-osmotic shock (Fig. 4 E). As reported earlier <sup>15</sup>, we too see that RBCs and a small  
12 percentage of HeLa cells rupture in isotonic media when treated with M $\beta$ CD (Figs. 4 F and S3  
13 E). We also find that increasing M $\beta$ CD concentration enhances rupture propensity in RBCs  
14 while rupture diameter matches that with hypo-osmotically shocked control cells (Fig. S3 D,  
15 E).

16 Next, to understand the role of cytoskeleton in the measured effect, we perform experiments in  
17 which cells are first treated with Cyto D before M $\beta$ CD treatment and then a hypo-osmotic  
18 shock is administered. We find that Cyto D, on its own does not alter the rupture propensity or  
19 rupture diameter on hypo-osmotic shock (Fig. 4 E). Similar values of rupture propensity and  
20 rupture diameter in M $\beta$ CD treated cells as well as Cyto D + M $\beta$ CD cells on hypo-osmotic  
21 shock show that the effect of M $\beta$ CD is not abrogated by Cyto D. This indicates that the  
22 cytoskeleton is not essential for the effect of M $\beta$ CD on membrane integrity. This effect is also  
23 seen in M $\beta$ CD pre-treated cells (Fig. 4 F) and is found to be more pronounced in RBCs (Fig.  
24 S3 E and Movie S4).

25 Thus, cholesterol depletion by M $\beta$ CD alters membrane mechanics by increasing the membrane  
26 tension, reducing the line and lysis tension which together enhance the rupturing propensity of  
27 the membrane with or without external stress. These effects are not mediated through the  
28 enhanced membrane-cytoskeleton interactions.

## 29 **DISCUSSION**

1 In this paper, we use interference based membrane fluctuation maps to visualize and quantify  
2 the effect of M $\beta$ CD mediated cholesterol depletion on cell membranes and their integrity. We  
3 report reduced temporal fluctuations and enhanced spatial flattening of the membrane on  
4 cholesterol depletion. Our study further focuses on the mechanics of the membrane – which,  
5 in contrast to earlier reports clearly shows that the membrane tension increases on cholesterol  
6 depletion. We also find that the interaction of the membrane with its underlying actin  
7 cytoskeleton increases, as reported previously<sup>7</sup>.

8 Mapping fluctuations within single cells enables us to correlate the enhanced spatial  
9 heterogeneity in fluctuations with that in membrane tension. While fluctuations, in general,  
10 need not necessarily correlate with membrane tension, we show that the increased tension on  
11 M $\beta$ CD treatment has a major contribution to the observed reduction in fluctuations. Even  
12 though the strength of the fluctuations is reduced, flattening out membrane undulations  
13 (increased correlation lengths) and reducing local non-uniformity (within  $2.16 \times 2.16 \mu\text{m}^2$   
14 regions) do not abrogate signatures of active fluctuations in cholesterol depleted cells. But,  
15 when temporal fluctuation-amplitudes between different pairs of such regions located at  
16 different parts of the cell are compared, M $\beta$ CD treated cells have more ‘dissimilar’ pairs than  
17 control cells. This implies that, in these cells, fluctuations can differ between membrane  
18 patches located at length scales larger than  $2.16 \mu\text{m}$ . We further show that these regions are  
19 also differently tensed – the variability in tension being bigger than between ‘similar’ regions.  
20 Though the amplification of the long-range heterogeneity in fluctuations by M $\beta$ CD treatment  
21 is robust in HeLa, it is not so in other cell lines (CHO or C2C12). However, the reduction in  
22 temporal fluctuations and its short-range variability, the increase in tension and its variability  
23 as well as the flattening of spatial undulations on cholesterol depletion are consistent in all the  
24 cell lines studied. These observations, together, clarify the effect of M $\beta$ CD mediated  
25 cholesterol depletion on membrane mechanics and its spatial variability.

1 The ability to resist membrane rupture on hypo-osmotic shock is expected to be lost on  
2 cholesterol depletion<sup>14</sup> and is also seen in this study. However, our work addresses the role of  
3 membrane mechanics by quantifying the effect of M $\beta$ CD on rupture propensity and diameter  
4 with and without hypo-osmotic shock. In cells with (HeLa) and without caveolae (RBCs), we  
5 find that M $\beta$ CD aids ruptures, even in absence of external perturbation, implying that it  
6 destabilizes the membrane mechanically. The measured rupture diameter ( $r$ ) corresponds to  
7 ratio of the membrane's line to surface tension ( $\gamma/\Sigma$ ) during lysis. Estimations show that the  
8 energy<sup>20,28</sup> required to open the pore ( $\Delta E = \frac{\pi\gamma^2}{\Sigma} = \pi\gamma r \sim 12 \text{ k}_B\text{T}$  (for RBCs), 200 k<sub>B</sub>T (for  
9 HeLa), assuming a lower limit  $\gamma \sim 1 \text{ pN}$  and using observed radii of rupture, 15 nm and 250  
10 nm, for RBC and HeLa cells respectively) is too high and contrasts the observed probability of  
11 rupture (expected ( $\exp(-\Delta E/ \text{k}_B\text{T})$ ):  $6 \times 10^{-6}$ , observed: 0.092, for RBCs without hypo-osmotic  
12 shock and in the presence of M $\beta$ CD). This implies that the ruptures could be induced by local  
13 defects in the membrane where there is a substantial reduction in line and lysis tension. While  
14 the exact values of tension cannot be extracted, we evaluate the relative changes in rupture  
15 diameter and propensity (Supporting Discussion) and argue that line<sup>20,45</sup> and lysis tension are  
16 reduced by M $\beta$ CD in both RBCs and HeLa cells. It is possible that increased long-range spatial  
17 heterogeneity in fluctuations and membrane tension of M $\beta$ CD treated cells reflect the existence  
18 of defects and that the increase in basal membrane tension by cholesterol depletion takes the  
19 system closer to the lowered lysis tension, hence aiding rupturing.

20 In conclusion, this work shows that under cholesterol depletion by M $\beta$ CD, cells not only have  
21 altered fluctuations reflecting a flattening of spatial undulations but also shows a clear increase  
22 in membrane tension along with an increased long-range heterogeneity in fluctuations.  
23 Enhanced rupture rates and rupture diameter due to M $\beta$ CD show that the membrane is also  
24 made vulnerable to rupture by a lowering of lysis and line tension.

## 25 **ACKNOWLEDGEMENTS**

1 This work was supported by the Wellcome Trust/DBT India Alliance Fellowship (grant  
2 number IA/I/13/1/500885) awarded to Bidisha Sinha. We thank Rajesh Kumble Nayak for the  
3 code for calculating the PSD, Jayasri Das Sarma for HeLa cells, Rupak Datta for CHO cells  
4 and Kaushik Sengupta (Saha Institute of Nuclear Physics, Kolkata) for the C2C12 cells.

## 5 **AUTHOR CONTRIBUTIONS**

6 Conceptualization, B.S.; Methodology, B.S., A.B., T.S., S.D., P.K.; Software, B.S., A.B.;  
7 Validation, A.B., B.S.; Investigation, A.B., P.K., S.D., T.S.; Formal Analysis, A.B., P.K.; Data  
8 Curation: A. B.; Writing – Original Draft, B.S., A.B.; Writing – Review & Editing, T.S., P.K.;  
9 Visualization, A.B.; Supervision, B.S.; Funding Acquisition, B.S.

## 10 **DECLARATION**

11 The authors declare no competing financial interest.

## 12 **REFERENCES**

- 13 1. Yeagle, P. L. Cholesterol and the cell membrane. *BBA - Rev. Biomembr.* **822**, 267–287  
14 (1985).
- 15 2. Ikonen, E. Cellular cholesterol trafficking and compartmentalization. *Nat. Rev. Mol.*  
16 *Cell Biol.* **9**, 125–138 (2008).
- 17 3. Byfield, F. J., Aranda-Espinoza, H., Romanenko, V. G., Rothblat, G. H. & Levitan, I.  
18 Cholesterol Depletion Increases Membrane Stiffness of Aortic Endothelial Cells.  
19 *Biophys. J.* **87**, 3336–3343 (2004).
- 20 4. Goodwin, J. S., Drake, K. R., Remmert, C. L. & Kenworthy, A. K. Ras Diffusion Is  
21 Sensitive to Plasma Membrane Viscosity. *Biophys. J.* **89**, 1398–1410 (2005).
- 22 5. Shvartsman, D. E., Gutman, O., Tietz, A. & Henis, Y. I. Cyclodextrins but not  
23 compactin inhibit the lateral diffusion of membrane proteins independent of  
24 cholesterol. *Traffic* **7**, 917–926 (2006).



- 1 6. Kwik, J. *et al.* Membrane cholesterol, lateral mobility, and the phosphatidylinositol  
2 4,5-bisphosphate- dependent organization of cell actin. *PNAS* **100**, 13964–13969  
3 (2003).
- 4 7. Sun, M. *et al.* The effect of cellular cholesterol on membrane-cytoskeleton adhesion. *J.*  
5 *Cell Sci.* **120**, 2223–2231 (2007).
- 6 8. Norman, L. L. *et al.* Modification of Cellular Cholesterol Content Affects Traction  
7 Force, Adhesion and Cell Spreading. *Cell Mol Bioeng.* **3**, 151–162 (2010).
- 8 9. Dulhunty, A. F. & Franzini-Armstrong, C. The relative contributions of the folds and  
9 caveolae to the surface membrane of frog skeletal muscle fibres at different sarcomere  
10 lengths. *J. Physiol.* **250**, 513–39 (1975).
- 11 10. Parpal, S., Karlsson, M., Thorn, H. & Strålfors, P. Cholesterol Depletion Disrupts  
12 Caveolae and Insulin Receptor Signaling for Metabolic Control via Insulin Receptor  
13 Substrate-1, but Not for Mitogen-activated Protein Kinase Control\*. *J. Biol. Chem.*  
14 **276**, 9670–9678 (2001).
- 15 11. Richter, T. *et al.* High-resolution 3D quantitative analysis of caveolar ultrastructure  
16 and caveola-cytoskeleton interactions. *Traffic* **9**, 893–909 (2008).
- 17 12. Fielding, C. J. & Fielding, P. E. Cholesterol and caveolae: Structural and functional  
18 relationships. *Biochim. Biophys. Acta - Mol. Cell Biol. Lipids* **1529**, 210–222 (2000).
- 19 13. Prescott, L. & Brightman, M. W. The sarcolemma of *Aplysia* smooth muscle in freeze-  
20 fracture preparations. *Tissue Cell* **8**, 241–258 (1976).
- 21 14. Sinha, B. *et al.* Cells Respond to Mechanical Stress by Rapid Disassembly of  
22 Caveolae. *Cell* **144**, 402–413 (2011).
- 23 15. Irie, T. *et al.* Cyclodextrin-induced hemolysis and shape changes of human  
24 erythrocytes in vitro. *J. Pharmacobiodyn.* **5**, 741–4 (1982).
- 25 16. Morris, C. E. & Homann, U. Cell Surface Area Regulation and Membrane Tension.

- 1        *Membr. Biol.* **179**, 79–102 (2001).
- 2    17.    Kosmalska, A. J. *et al.* Physical principles of membrane remodelling during cell  
3        mechanoadaptation. *Nat. Commun.* **6**, 7292 (2015).
- 4    18.    Evans, E. & Needham, D. Physical properties of surfactant bilayer membranes:  
5        thermal transitions, elasticity, rigidity, cohesion and colloidal interactions. *J. Phys.*  
6        *Chem.* **91**, 4219–4228 (1987).
- 7    19.    Needham, D. & Nunn, R. S. Elastic deformation and failure of lipid bilayer  
8        membranes containing cholesterol. *Biophys. J.* **58**, 997–1009 (1990).
- 9    20.    Zhelev, D. V. & Needham, D. Tension-stabilized pores in giant vesicles: determination  
10       of pore size and pore line tension. *BBA - Biomembr.* **1147**, 89–104 (1993).
- 11   21.    Atger, V. M. *et al.* Cyclodextrins as catalysts for the removal of cholesterol from  
12       macrophage foam cells. *J. Clin. Invest.* **99**, 773–780 (1997).
- 13   22.    Zidovetzki, R. & Levitan, I. Use of cyclodextrins to manipulate plasma membrane  
14       cholesterol content: evidence, misconceptions and control strategies. *Biochim Biophys*  
15       *Acta.* **1768**, 1311–1324 (2007).
- 16   23.    Gidwani, B. & Vyas, A. A Comprehensive Review on Cyclodextrin-Based Carriers for  
17       Delivery of Chemotherapeutic Cytotoxic Anticancer Drugs. *Biomed Res. Int.* **2015**,  
18       (2015).
- 19   24.    Khatibzadeh, Nima, Gupta, S. Effects of cholesterol on nano-mechanical properties of  
20       the living cell plasma membrane. *Soft Matter* **8**, 8350–8360 (2012).
- 21   25.    Byfield, F. J., Tikku, S., Rothblat, G. H., Gooch, K. J. & Levitan, I. OxLDL increases  
22       endothelial stiffness, force generation, and network formation. *J. Lipid Res.* **47**, 715–  
23       723 (2006).
- 24   26.    Limozin, L. & Sengupta, K. Quantitative reflection interference contrast microscopy  
25       (RICM) in soft matter and cell adhesion. *ChemPhysChem* **10**, 2752–2768 (2009).

- 1 27. Biswas, A., Alex, A. & Sinha, B. Mapping Cell Membrane Fluctuations Reveals Their  
2 Active Regulation and Transient Heterogeneities. *Biophys. J.* **113**, 1768–1781 (2017).
- 3 28. Moroz, J. D. & Nelson, P. Dynamically Stabilized Pores in Bilayer Membranes.  
4 *Biophys. J.* **72**, 2211–2216 (1997).
- 5 29. McNeil, P. L. & Steinhardt, R. A. Loss, restoration, and maintenance of plasma  
6 membrane integrity. *J. Cell Biol.* **137**, 1–4 (1997).
- 7 30. Thorpe, W. P., Toner, M., Ezzell, R. M., Tompkins, R. G. & Yarmush, M. L.  
8 Dynamics of Photoinduced Cell Plasma Membrane Injury. *Biophys. J.* **68**, 2198–2206  
9 (1995).
- 10 31. Taupin, C., Dvolaitzky, M. & Sauterey, C. Osmotic pressure induced pores in  
11 phospholipid vesicles. *Biochemistry* **14**, 4771–5 (1975).
- 12 32. Klem, S., Klingler, M., Demmelmair, H. & Koletzko, B. Efficient and Specific  
13 Analysis of Red Blood Cell Glycerophospholipid Fatty Acid Composition. *PLoS One*  
14 **7**, e33874 (2012).
- 15 33. Lai, Q. *et al.* E2F1 inhibits circulating cholesterol clearance by regulating Pcsk9  
16 expression in the liver. *JCI Insight* **2**, 1–16 (2017).
- 17 34. Yahara, I., Harada, F., Sekita, S., Yoshihira, K. & Natori, S. Correlation between  
18 Effects of 24 Different Cytochalasins on Cellular Structures and Cellular Events and  
19 Those on Actin In Vitro. *J. Cell Biol.* **92**, 69–78 (1982).
- 20 35. Renard, H.-F. *et al.* Endophilin-A2 functions in membrane scission in clathrin-  
21 independent endocytosis. *Nat. Lett.* **517**, 493–496 (2014).
- 22 36. Tenopoulou, M., Kurz, T., Doulias, P., Galaris, D. & Brunk, U. T. Does the calcein-  
23 AM method assay the total cellular ‘ labile iron pool ’ or only a fraction of it ?  
24 *Biochem. J.* **403**, 261–266 (2007).
- 25 37. Wilhelm, L. P. *et al.* STARD3 mediates endoplasmic reticulum-to-endosome

- 1 cholesterol transport at membrane contact sites. *EMBO J.* **36**, 1412–1433 (2017).
- 2 38. Gov, N., Zilman, A. G. & Safran, S. Cytoskeleton confinement and tension of red  
3 blood cell membranes. *Phys. Rev. Lett.* **90**, 228101 (2003).
- 4 39. Brochard, F. & Lennon, J. F. Frequency spectrum of the flicker phenomenon in  
5 erythrocytes. *J. Phys.* **36**, 1035–1047 (1975).
- 6 40. Rodríguez-García, R. *et al.* Direct Cytoskeleton Forces Cause Membrane Softening in  
7 Red Blood Cells. *Biophys. J.* **108**, 2794–2806 (2015).
- 8 41. Monzel, C. *et al.* Measuring fast stochastic displacements of bio-membranes with  
9 dynamic optical displacement spectroscopy. *Nat. Commun.* **6**, 8162 (2015).
- 10 42. Helfrich, W. Elastic Properties of Lipid Bilayers Elastic Properties of Lipid Bilayers:  
11 Theory and Possible Experiments. *Z. Naturforsch* **28**, 3–7 (1973).
- 12 43. Alert, R., Casademunt, J., Brugués, J. & Sens, P. Model for Probing Membrane-Cortex  
13 Adhesion by Micropipette Aspiration and Fluctuation Spectroscopy. *Biophys. J.* **108**,  
14 1878–1886 (2015).
- 15 44. Levitan, I., Shentu, T. P., Sun, M. & Forgacs, G. in *Mechanobiology of the*  
16 *Endothelium* (2014). at  
17 <[https://books.google.co.in/books?id=foSbBgAAQBAJ&pg=PA146&lpg=PA146&dq=mechanobiology+of+the+endothelium+chapter+7&source=bl&ots=bCafjlwhjJ&sig=dNIaDvqxsPdLN\\_H0McxrP2BhwaI&hl=en&sa=X&ved=0ahUKEwjsrIuR8OXXAhVLvY8KHQ2TBpEQ6AEIPTAF#v=onepage&q=mechanobiology](https://books.google.co.in/books?id=foSbBgAAQBAJ&pg=PA146&lpg=PA146&dq=mechanobiology+of+the+endothelium+chapter+7&source=bl&ots=bCafjlwhjJ&sig=dNIaDvqxsPdLN_H0McxrP2BhwaI&hl=en&sa=X&ved=0ahUKEwjsrIuR8OXXAhVLvY8KHQ2TBpEQ6AEIPTAF#v=onepage&q=mechanobiology)>  
18 =mechanobiology+of+the+endothelium+chapter+7&source=bl&ots=bCafjlwhjJ&sig=  
19 dNIaDvqxsPdLN\_H0McxrP2BhwaI&hl=en&sa=X&ved=0ahUKEwjsrIuR8OXXAhV  
20 LvY8KHQ2TBpEQ6AEIPTAF#v=onepage&q=mechanobiology>
- 21 45. Karatekin, E. *et al.* Cascades of transient pores in giant vesicles: Line tension and  
22 transport. *Biophys. J.* **84**, 1734–1749 (2003).
- 23