

# Cross-modal and non-monotonic representations of statistical regularity are encoded in local neural response patterns

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## Abstract

Current neurobiological models assign a central role to predictive processes calibrated to environmental statistics. Neuroimaging studies examining the encoding of stimulus uncertainty have relied almost exclusively on manipulations in which stimuli were presented in a single sensory modality, and further assumed that neural responses vary monotonically with uncertainty. This has left a gap in theoretical development with respect to two core issues: i) are there cross-modal brain systems that encode input uncertainty in way that generalizes across sensory modalities, and ii) are there brain systems that track input uncertainty in a non-monotonic fashion? We used multivariate pattern analysis to address these two issues using auditory, visual and audiovisual inputs. We found signatures of cross-modal encoding in frontoparietal, orbitofrontal, and association cortices using a searchlight cross-classification analysis where classifiers trained to discriminate levels of uncertainty in one modality were tested in another modality. Additionally, we found widespread systems encoding uncertainty non-monotonically using classifiers trained to discriminate intermediate levels of uncertainty from both the highest and lowest uncertainty levels. These findings comprise the first comprehensive report of cross-modal and non-monotonic neural sensitivity

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to statistical regularities in the environment, and suggest that conventional paradigms testing for monotonic responses to uncertainty in a single sensory modality may have limited generalizability.

*Keywords:* Regularity, Prediction, Entropy, Complexity, Multimodal

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## 1. Introduction

Currently, one of the dominant frameworks for understanding brain function couches perception in terms of learning-based predictive processes, which operate by integrating information over multiple temporal scales (e.g., Bornstein & Daw, 2012; Clark, 2013; Friston, 2010). This is a foundational premise in computational and cognitive approaches to economic decision-making, language processing, statistical learning, and low-level sensory processing. These theoretical developments have been accompanied by a rich body of experimental data addressing the neurobiological basis of predictive processing, and in particular, brain systems that encode temporally-unfolding statistical structure in the environment (see Hasson, 2017, for recent review).

There are, however, two substantial limitations to our understanding of the neurobiological systems encoding environmental statistics. First, almost all empirical studies probing the neural systems supporting predictive processing assume that these systems track statistical regularities monotonically; i.e., that the relevant neural systems are ones in which activity increases or decreases monotonically with statistical regularity, predictability, or uncertainty. This assumption is deceptively intuitive and is sufficiently ingrained in neurobiological experiments that it is rarely stated explicitly. Examples include neuroimaging studies that test for linear relations between statistical regularities in stimulus series and response magnitudes (e.g., Bischoff-Grethe, Proper, Mao, Daniels, & Berns, 2000; Harrison, Duggins, & Friston, 2006; Huettel, Mack, & McCarthy, 2002; Strange, Duggins, Penny, Dolan, & Friston, 2005), or studies that contrast structured and random inputs sequences (e.g., Cunillera et al., 2009; McNealy, Mazziotta, & Dapretto, 2006).

That said, there are a few recent exceptions to this assumption. Kidd et al. (2012) found that infants, when presented with sequences of events varying in their predictability (surprisal), were less likely to look away from intermediately surprising events than when events were too predictable or too surprising. This suggests that stimuli of intermediate predictability may receive privileged neural processing with respect to random or highly struc-

32 tured inputs. Along these lines, Nastase et al. (2015) found that whole-brain  
33 connectivity between the anterior cingulate cortex and several brain regions  
34 tracked statistical regularities in auditory stimuli non-monotonically (i.e.,  
35 via a quadratic trend). Non-monotonic responses to regularity are compat-  
36 ible with several types of operations (Hasson et al., 2017; Nastase et al.,  
37 2015). For example, neural systems modeling the environmental generators  
38 of sensory inputs may be maximally engaged by moderately structured in-  
39 puts where model complexity is highest; additionally, systems supporting  
40 exploratory behavior or encoding particular information-theoretic metrics,  
41 such as predictive information rate (Abdallah & Plumbley, 2009), may be  
42 maximally engaged by inputs of intermediate regularity, while not differenti-  
43 ating highly random and highly structured inputs. Identifying brain systems  
44 that respond non-monotonically to uncertainty, particularly ones that do so  
45 in a supra-modal manner, would expose a novel but unappreciated aspect  
46 of neural coding of input statistics, which cannot be explained by low-level  
47 mechanisms such as the construction of prediction, generation of prediction  
48 errors, or any other computational account in which responses scale with  
49 uncertainty.

50 A second, related limitation is that very few studies have directly in-  
51 vestigated whether there exist neural systems that are sensitive to input  
52 statistics in more than one modality. This is one of the core questions in  
53 functional theories of statistical learning (for review, see, e.g., Frost, Arm-  
54 strong, Siegelman, & Christiansen, 2015) but has seldom been addressed from  
55 a neurobiological perspective. Our prior work examining this issue (Nastase  
56 et al., 2014) failed to identify areas sensitive to regularity in both auditory  
57 and visual inputs (and was agnostic to the issue of linear or non-monotonic  
58 trends). Other work in which participants were instructed to predict the  
59 final elements of series varying in predictability reported adjacent (Schubotz  
60 & von Cramon, 2002) or overlapping responses (Schubotz & von Cramon,  
61 2004) in left ventral premotor cortex for different modalities. More recent  
62 work (Meyniel and Dehaene, 2017) has implicated a more widespread net-  
63 work including precentral, intraparietal, and superior temporal cortices in  
64 tracking transition probabilities in auditory and visual series (though no for-  
65 mal conjunction test was performed). Nonetheless, overlapping activations  
66 (i.e., conjunction maps) provide limited evidence for cross-modal representa-  
67 tion of uncertainty, because the finer-grained organization of neural activity  
68 may differ across modalities.

69 The current study was designed to address these limitations by (*a*) sys-

70 tematically probing for both monotonic and non-monotonic neural responses  
71 to statistical regularities in auditory, visual, and audiovisual stimuli, and (b)  
72 determining to what extent these responses are modality-independent. Par-  
73 ticipants were presented with brief  $\sim 10$  s auditory, visual, and audiovisual  
74 series varying across four levels of entropy (i.e., uncertainty, inversely related  
75 to regularity) while performing an orthogonal cover task. The same statisti-  
76 cal constraints were used to generate auditory series consisting of pure tones,  
77 visual series consisting of simple colored shapes, or audiovisual series where  
78 each token was a unique tone/shape combination (thus the uncertainty and  
79 structure of the audiovisual series was identical to that of the auditory-only  
80 and visual-only series). We used multivariate pattern analysis to localize re-  
81 sponse patterns that differentiated series with varying uncertainty in either a  
82 monotonic or quadratic (i.e., non-monotonic) fashion for auditory, visual, and  
83 audiovisual series. We also used multivariate cross-classification to identify  
84 neural systems encoding uncertainty in a modality-general fashion by training  
85 a classifier to discriminate levels of uncertainty in one modality (e.g., visual  
86 series) and then testing it on another modality (e.g., auditory series). This  
87 procedure explicitly tests for systems coding for statistical regularities in the  
88 environment at a level of abstraction that supersedes the sensory features of  
89 the stimuli.

90 In general, we expected different brain systems to track uncertainty within  
91 auditory and visual streams, consistent with emerging views that different  
92 neural systems encode sequential structure or environmental regularities in  
93 different modalities (for recent reviews; see Armstrong, Siegelman, & Chris-  
94 tiansen, 2015; Dehaene, Meyniel, Wacongne, Wang, & Pallier, 2015; Frost et  
95 al., 2015; Hasson, 2017; Milne, Wilson, & Christiansen, 2018). We further  
96 expected that the systems implicated in tracking the level of uncertainty in  
97 audiovisual stimuli would diverge from those tracking uncertainty for unisen-  
98 sory stimuli, as our recent work (Andric, Davis, & Hasson, 2017) indicates  
99 that audiovisual inputs trigger unique computations related to uncertainty.

## 100 **2. Methods**

### 101 *2.1. Participants*

102 Twenty-five right-handed adults (Mean Age =  $26.1 \pm 4.74$  SD; 11 female)  
103 participated in the study, which was conducted at the University of Trento,  
104 Italy. They were recruited from the local student population, provided in-  
105 formed consent, and were reimbursed at a rate of 10 Euro per hour. Partic-

106 ipants reported no history of psychiatric illness, history of substance abuse,  
107 or hearing impairments, and underwent an interview with a board-certified  
108 medical doctor prior to scanning to evaluate other exclusion criteria. Data  
109 from one participant who had completed the study were not included due  
110 to excessive movement during the scanning session. The human research  
111 ethics committee of the University of Trento approved the study. The data  
112 collected here have not been reported in any other study

## 113 *2.2. Design, materials, and procedure*

114 Stimulus events consisted of brief auditory (A), visual (V), or audiovisual  
115 (AV) series. Each series consisted of 32 items presented within 9.6 s at a rate  
116 of 3.3 Hz. These 32 items consisted of a repeated sampling of four tokens  
117 whose presentation order was determined by a first-order Markov process.  
118 For all modalities, each token was presented for 250 ms, followed by a 50 ms  
119 pause. For the auditory series, these tokens were four pure tones (262, 294,  
120 330, 349 Hz; corresponding to middle C, D, E, and F in the Western major  
121 scale). Volume was manually adjusted for each participant until auditory  
122 stimuli were comfortably heard over scanner noise. For the visual series, the  
123 four tokens were four visual stimuli each identified by a unique combination  
124 of shape (circle, square, star, triangle), color (blue, green, red, yellow), and  
125 location (left, right, above, or below the fixation cross; e.g., ‘1’ = blue triangle  
126 presented above the fixation cross). Visual stimuli were presented at 2° visual  
127 angle from the fixation cross so that they could be observed without eye  
128 movement. The AV series consisted of yoked auditory and visual stimuli  
129 (fixed pairs) that were completely mutually informative such that within  
130 each AV series, any given tone was presented with only one visual stimulus.  
131 For each of the AV series, this produced an “alphabet” of only 4 possible  
132 states, analogous to the formal information content within the unisensory  
133 (A or V) series. The complete mutual information between auditory and  
134 visual streams in the AV condition reflected a single generating process, and  
135 consequently, tracking one stream provided complete information about the  
136 other. The specific instantiation of the one-to-one matching between a tone  
137 and a visual stimulus changed across the different AV series.

138 Series in the four conditions were generated using a first-order Markov  
139 process applied to four transition matrices with different levels of Markov  
140 entropy (Markov entropy = 0.81, 1.35, 1.56, 2.0; see Figure 1). We manip-  
141 ulated only these transition probabilities between tokens, while fixing the  
142 marginal frequencies across conditions at 25% per token; i.e., only Markov

143 entropy was manipulated whereas Shannon entropy was fixed at 2 bits (a  
144 uniform distribution where each token is equally likely). We created the ex-  
145 perimental series by repeatedly generating series from the Markov processes,  
146 evaluating those for transition constraints and marginal frequencies, and se-  
147 lecting only those series that exactly fit the generating process in terms of  
148 transition and marginal frequencies. Levels of the Markov entropy factor are  
149 referred to as levels 1, 2, 3, and 4 and indicate an increase in randomness;  
150 note that a positive linear relationship with entropy or uncertainty can also  
151 be described as a negative linear relationship with regularity, structure, or  
152 predictability.

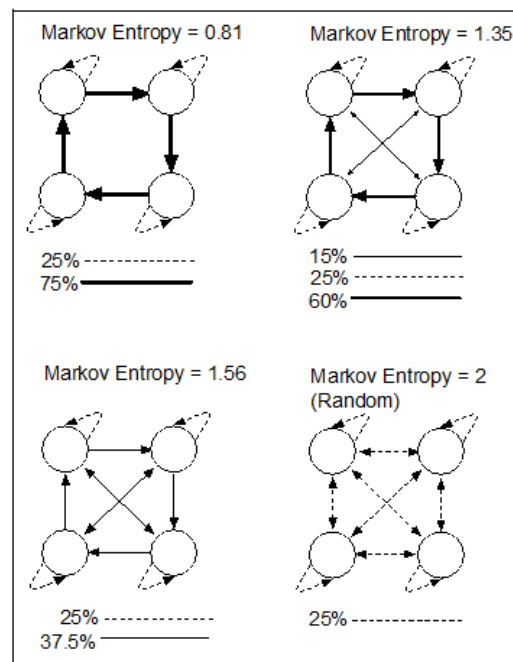


Figure 1: **Transition graphs determining the uncertainty of stimulus series.** In the auditory condition, each token corresponded to a tone. In the visual condition, each token corresponded to a shape of a particular color at one of four locations surrounding the central fixation cross. In the audiovisual condition, each token corresponded to a fixed tone–shape pair that remained unchanged within a series, but differed across series. The transition graphs correspond to entropy labels 1 (top left), 2 (top right), 3 (bottom left), and 4 (bottom right) in the text and figures.

153 There were 12 conditions in the factorial design corresponding to the fully  
154 crossed 4 entropy levels and 3 sensory modalities (A, V, AV). We used 12

155 different series for each of these 12 conditions (i.e., 144 experimental series in  
156 total). These stimuli were presented over four experimental runs, with each  
157 run containing three series from each of the 12 conditions. Participants per-  
158 formed an orthogonal cover task in which they were instructed to monitor the  
159 fixation cross at the center of the display, and press a response key whenever  
160 the fixation cross began to rotate and alternate in color. These events served  
161 as catch trials, occurring six times during each run, and were unrelated to the  
162 entropy and modality manipulations. During each of the four experimental  
163 runs, performance was monitored online and not analyzed further; responses  
164 to catch trials were tracked by the experimenter and participants were pro-  
165 vided feedback at the end of each run if a response was missed to encourage  
166 improved performance. In contrast to studies that encourage or require ex-  
167 plicit prediction (e.g., Schubotz & von Cramon, 2002, 2004), we used a cover  
168 task to measure passive sensitivity to sensory regularities. Existing work  
169 suggests that explicit and implicit statistical learning tasks engage distinct,  
170 but partially overlapping neural systems (e.g., Aizenstein et al., 2004). The  
171 trial timing for each run was based on a rapid event-related fMRI protocol  
172 with jittered inter-stimulus intervals and an implicit baseline consisting of  
173 observation of the fixation cross. The presentation sequence was determined  
174 by the optseq utility (Dale, 1999), which generates a trial set optimized for  
175 this type of experimental design. Each run began with an 18.7 s rest interval  
176 to allow for signal stabilization.

### 177 *2.3. fMRI acquisition*

178 Images were acquired with a 4T MRI scanner (Bruker Medical, Ettlin-  
179 gen, Germany) using a birdcage-transmit, 8-channel receiver head coil (USA  
180 Instruments, Inc., OH, USA). Two T1-weighted 3D MPRAGE structural im-  
181 ages were acquired (1 mm<sup>3</sup> isotropic voxels, GRAPPA iPAT = 2, 5:36 min  
182 each). One was optimized for optimal contrast (MPRAGE\_CNR) between  
183 gray and white matter tissue (TE/TR/TI/flip angle = 4.18 ms/2700 ms/1020  
184 ms/7°) and the other was optimized for signal to noise ratio (MPRAGE\_SNR)  
185 in gray and white matter tissue (TE/TR/TI/flip angle = 3.37 ms/2500  
186 ms/1200 ms/12°; Papinutto & Jovicich, 2008). For functional MRI, single-  
187 shot EPI BOLD functional images were acquired using the point-spread-  
188 function distortion correction method (Zaitsev, Hennig, & Speck, 2004). Two  
189 hundred and eighty-five EPI volumes lasting 627 s in total were acquired dur-  
190 ing each of the four functional runs for 1,140 total volumes and 2,508 s total  
191 acquisition time (TR/TE = 2.2 s/33 ms, matrix 64 x 64, with 37 interleaved



192 slices parallel to AC/PC, 3 mm<sup>3</sup> isotropic voxels, slice skip factor = 15%,  
193 flip angle = 75.0°). Cardiac and respiratory measurements were not collected  
194 during fMRI acquisition.

#### 195 *2.4. Preprocessing*

196 Preprocessing of fMRI data was carried out using FEAT (fMRI Expert  
197 Analysis Tool) Version 6.00, part of FSL (FMRIB's Software Library; Jenk-  
198 inson, Beckmann, Behrens, Woolrich, & Smith, 2012). The first six volumes  
199 of every fMRI run were discarded prior to analysis. The following preprocess-  
200 ing steps were then applied: motion correction using MCFLIRT (Jenkinson,  
201 Bannister, Brady, & Smith, 2002); slice-timing correction using Fourier-space  
202 time-series phase-shifting; non-brain removal using BET (Smith, 2002); spa-  
203 tial smoothing using a 5 mm FWHM Gaussian kernel; grand-mean intensity  
204 normalization of the entire 4D dataset by a single multiplicative factor; and  
205 high-pass temporal filtering (Gaussian-weighted least-squares straight line  
206 fitting, with  $\sigma = 50.0$  s).

207 In order to control for motion, confound matrixes were created using the  
208 dvars metric (Power, Barnes, Snyder, Schlaggar, & Petersen, 2012) using  
209 the `fsl_motion_outliers` tool. The dvars metric quantifies intensity differences  
210 between adjacent volumes after realignment (motion correction). Volumes  
211 that exceeded a boxplot cutoff threshold of 1.5 times the interquartile range  
212 were included in a confound matrix to be excluded in the first-level regression  
213 model by treating them as a regressor of no interest. This method is similar  
214 to excluding outlier time points from the regression model, but does not  
215 adversely affect temporal filtering or the autocorrelation structure.

#### 216 *2.5. Regression model*

217 Single-participant analyses were conducted using FSLs FEAT (Jenkinson  
218 et al., 2012). A general linear model was constructed using FILM with local  
219 autocorrelation correction (Woolrich, Ripley, Brady, & Smith, 2001). The  
220 regression model included 12 regressors of interest: 4 (entropy levels)  $\times$  3  
221 (sensory modality), where each 9.6 s event was modeled as a boxcar function  
222 convolved with a single-gamma hemodynamic response function. Note that  
223 we did not model or analyze the individual tokens (occurring at 3.3 Hz) com-  
224 prising each event. Regressors of no interest included the catch trials eliciting  
225 button presses as well as a set of standard and extended motion parameters:  
226 6 standard motion regressors, as well as their squares, temporal derivatives,  
227 squared derivatives, and the motion confound matrix determined using the



228 dvars metric. We did not include a global signal covariate as stimulus series  
229 were brief (corresponding to approximately four functional volumes) and pre-  
230 sented in pseudorandom order with jittered onsets, and because global signal  
231 regression may alter the inter-voxel correlation structure to which multivari-  
232 ate analysis are sensitive (Caballero-Gaudes & Reynolds, 2016).

## 233 *2.6. Normalization*

234 The structural images optimized for contrast-to-noise ratio (CNR) were  
235 preprocessed using the `fsl_anat` tool according to the following steps: reorien-  
236 tation to MNI conventions (`flsreorient2std`); automatic cropping (`robustfov`);  
237 bias field correction (`FAST`); nonlinear normalization to a whole-brain MNI  
238 template (`FNIRT`); brain extraction based on the alignment to the MNI tem-  
239 plate, and segmentation according to tissue type and subcortical structures.

240 After estimating the first-level regression model, we aligned the statistical  
241 maps to MNI space in a single step by concatenating three transformation  
242 matrices resulting from the following three alignment stages. In a first step,  
243 each structural image was aligned to the first EPI volume in each run (i.e.,  
244 the first of the six discarded volumes; the image with the strongest anatom-  
245 ical contrast) using a 3 degrees-of-freedom (translation-only) linear FLIRT  
246 alignment. In a second step, boundary-based registration (Greve & Fischl,  
247 2009) was used to co-register the first EPI volume to the bias corrected,  
248 skull-stripped, and segmented structural image. In a third step the struc-  
249 tural image was nonlinearly aligned to the MNI template using an initial 12  
250 degrees-of-freedom linear registration step followed by nonlinear registration  
251 with a warp resolution of 10 mm.

## 252 *2.7. Multivariate pattern analysis*

### 253 *2.7.1. General approach and preparation for MVPA*

254 We used multivariate pattern analysis to classify entropy conditions from  
255 distributed neural response patterns, with a focus on the issue of cross-modal  
256 classification (Kaplan, Man, & Greening, 2015; Kriegeskorte, 2011; Nastase,  
257 Halchenko, Davis, & Hasson, 2016). To localize brain areas that contained  
258 information about entropy, classification was performed using spherical volu-  
259 metric searchlights (e.g., Kriegeskorte, Goebel, & Bandettini, 2006; Pereira,  
260 Mitchell, & Botvinick, 2009). Each searchlight had a 3-voxel radius (6 mm),  
261 and on average included 107 voxels (SD = 21 voxels).

262 We performed two types of classification where the classification targets  
263 were assigned so as to capture the two types of dissociations that were of

264 theoretical interest: (i) classification of high versus low entropy conditions  
265 (approximating a “linear profile”); and (ii) classification of the two extreme  
266 (high, low) versus the two intermediate levels of entropy (“quadratic pro-  
267 file”). In this latter classification analysis, we assigned the label “extreme”  
268 to entropy levels 1 and 4, and the label “intermediate” to the entropy levels  
269 2 and 3, and then proceeded with standard two-class classification. For the  
270 classifier to perform at 100% accuracy, it must, in left-out test data, classify  
271 both levels 1 and 4 as “extreme”, and levels 2 and 3 as “intermediate”.

272 First, we applied standard within-modality pattern classification to iden-  
273 tify brain regions that discriminated levels of uncertainty in a linear or  
274 quadratic fashion. In this procedure, classifiers were trained and tested on  
275 response patterns *within* the same sensory modality (A, V, AV).

276 Second, to evaluate cross-modal sensitivity to entropy (i.e., information  
277 about entropy condition that generalizes across sensory modality), classifiers  
278 were trained on stimuli in the auditory modality and tested on stimuli in  
279 the visual modality (and vice versa) and the results averaged (as in, e.g.,  
280 Man, Kaplan, Damasio, & Meyer, 2012; Oosterhof, Tipper, & Downing,  
281 2012). Note that the audiovisual condition was not examined in the cross-  
282 classification scheme.

### 283 2.7.2. Implementation of MVPA

284 We extracted regression coefficients from the first-level univariate general  
285 linear model, for each of the 12 conditions, and propagated those to a gray  
286 matter mask comprising the union of individual gray masks across partici-  
287 pants (50% gray matter probability from FSL’s FAST) in MNI space. This  
288 gray matter mask contained 196,634 2 mm<sup>3</sup> voxels after removing any voxels  
289 invariant across all samples and participants. Regression coefficients were  
290 averaged across the four runs within each participant prior to classification  
291 analysis to create a single map per condition, and then normalized (Z-scored)  
292 across features (voxels) within each searchlight (Misaki, Kim, Bandettini, &  
293 Kriegeskorte, 2010; Nastase et al., 2016). This normalization scheme ensures  
294 that the classifier cannot capitalize on regional-average differences in response  
295 magnitude (i.e., within a searchlight) between the different conditions.

296 Classification was performed using linear support vector machines (SVMs;  
297 Boser, Guyon, & Vapnik, 1992) with the soft-margin parameter  $C$  automat-  
298 ically scaled to the norm of the data. All classification analyses were per-  
299 formed using leave-one-*participant*-out cross-validation (e.g., Clithero, Smith,  
300 Carter, & Huettel, 2011; Mourao-Miranda, Bokde, Born, Hampel, & Stet-

301 ter, 2005). That is, for each cross-validation fold, the decision boundary was  
302 constructed based on samples from 24 of the 25 participants, and tested on  
303 the left-out participant. This procedure was repeated until each participant  
304 served as the test participant, and the classification accuracies were aver-  
305 aged across cross-validation folds. It has been shown (e.g., Allefeld, Gorgen,  
306 & Haynes, 2016) that a leave-one-participant-out procedure more rigorously  
307 ensures that classification generalizes across participants than applying stan-  
308 dard second-level statistical tests to classification accuracies that are based  
309 on leave-one-run-out cross-validation within participants.

310 In the cross-modal classification analysis, for each cross-validation fold  
311 the decision boundary was constructed based on samples from one sensory  
312 modality (e.g., auditory) in 24 participants, then tested on samples from the  
313 other sensory modality (e.g., visual) in the left-out participant. All multivari-  
314 ate analyses were performed using the PyMVPA software package (Hanke et  
315 al., 2009).

316 To determine the statistical significance of searchlight classification ac-  
317 curacies we used nonparametric randomization tests shuffling the entropy  
318 condition assignments (e.g., Etzel, 2015, 2017; Nastase et al., 2016). That is,  
319 for each permutation, the condition labels were randomly reassigned for all  
320 participants and the entire searchlight classification analysis (cross-validated  
321 across participants) was recomputed. For each searchlight analysis, 1,000  
322 permutations were computed per searchlight, resulting in a distribution of  
323 searchlight maps under the null hypothesis of no systematic relationships  
324 among the condition labels. The actual searchlight classification accuracy  
325 was then compared against this null distribution to determine a p-value per  
326 searchlight. The permutation test respected the stratification of the data  
327 such that entropy labels were permuted within each participant, and for  
328 cross-classification permuted within each modality (nested within partici-  
329 pants). When classifying highly-regular and random series (entropy levels 1  
330 and 4), only labels 1 and 4 were permuted. When classifying extreme ver-  
331 sus intermediate levels of entropy (quadratic profile), labels were permuted  
332 to ensure that the two extreme entropy levels were assigned the same label  
333 (“extreme” or “intermediate”) and that the intermediate levels were both  
334 assigned the other label.

335 We performed nonparametric cluster-level inference using a Monte Carlo  
336 procedure simulating clusters of random Gaussian noise (Forman et al.,  
337 1995). To constrain the spatial smoothness of the noise simulation, we com-  
338 puted residual searchlight accuracy maps by subtracting the average accu-

339 racy (across participants) from each participant’s accuracy (as in Linden,  
340 Oosterhof, Klein, & Downing, 2012, p. 630). The mean smoothness along  
341 the  $x$ -,  $y$ -, and  $z$ -axes of these residual accuracy maps was calculated us-  
342 ing AFNI’s 3dFWHMx and supplied to AFNI’s 3dClustSim to estimate the  
343 extent of significant searchlight clusters occurring by chance. For the *cross*-  
344 modal searchlight classification procedure, we report clusters that survived a  
345 voxel-level cluster-forming threshold of  $p < .05$  (assessed using permutation  
346 tests) and a cluster-level threshold of  $p < .05$ , controlling for the family-  
347 wise error rate. For the *within*-modality searchlight classification, we use a  
348 slightly more conservative single-voxel cluster-forming threshold ( $p < .01$ ;  
349 cluster-level correction,  $p < .05$ ).

350 To relate the current study to prior reports of hippocampal sensitivity to  
351 statistical regularities (e.g., Bornstein & Daw, 2012; Covington et al., 2018;  
352 Schapiro et al., 2014; Turk-Browne et al., 2009), and because the search-  
353 light approach is not particularly well-suited to subcortical structures, we  
354 additionally performed classification analyses within an anatomically defined  
355 hippocampal region of interest (ROI). For each participant, left and right hip-  
356 pocampal volumes were automatically segmented using FSL’s FIRST (Pate-  
357 naude, Smith, Kennedy, & Jenkinson, 2011) and then normalized to MNI  
358 space following the same procedure described above for the whole brain.  
359 Voxels in MNI space assigned to hippocampus in 50% or more participants  
360 were included in the final hippocampal ROI. We then performed the clas-  
361 sification analyses described above (i.e., cross-modal and within-modality,  
362 as well as linear and quadratic classification) within the hippocampus ROIs  
363 using leave-one-participant-out cross-validation. We analyzed the right and  
364 left hippocampal volumes separately. Significant classification within the  
365 hippocampus was assessed using the randomization test described above.

### 366 **3. Results**

#### 367 *3.1. Sensitivity to uncertainty in auditory, visual and audiovisual series*

368 Using a multivariate searchlight analysis, we first evaluated two questions:  
369 *i*) whether local neural response patterns discriminate between high- and  
370 low-uncertainty conditions (approximating a linear trend), and *ii*) whether  
371 response patterns discriminate the two intermediate levels of regularity from  
372 both the most- and least-regular conditions (approximating a quadratic trend).  
373 Responses discriminating high and low entropy are consistent with predictive  
374 processing, while responses discriminating intermediate and extreme levels

375 of entropy may reflect processes modeling the complexity of the system gen-  
376 erating the stimuli.

377 For the *auditory modality*, we identified two regions discriminating high  
378 and low entropy: left precentral gyrus (PCG) and right insula, with peak  
379 searchlight classification accuracies of 77–79%, cross-validated across partic-  
380 ipants (theoretical chance = 50% here and for all subsequent classification  
381 results). We found a much more extensive set of regions that discriminated  
382 the intermediate levels of auditory regularity from both high and low levels  
383 (a quadratic discrimination with respect to entropy levels; Figure 2). These  
384 included bilateral superior and middle temporal gyri (STG, MTG), right  
385 transverse temporal gyrus (TTG), occipital regions bilaterally, and the cere-  
386 bellum, with peak two-way classification accuracies of 67–70% (see Table 1  
387 for all significant cluster locations).

388 [Table 1 around here]

389 For the *visual modality* we identified four clusters discriminating high and  
390 low entropy series: left post-central gyrus (PoCG), right STG, right cuneus,  
391 and left rectal gyrus, with peak classification accuracies of 75–79%. We also  
392 identified several clusters discriminating intermediate levels of regularity from  
393 both the highest and lowest levels. The largest of the clusters was located  
394 in the right caudate, with additional clusters in the left fusiform gyrus, right  
395 inferior temporal gyrus, and right superior medial frontal gyrus. Peak clas-  
396 sification accuracies in these significant clusters of searchlights ranged from  
397 67% to 70%.

398 For the audiovisual stimuli, we identified three clusters that discriminated  
399 high and low entropy conditions: right PoCG, left superior occipital gyrus,  
400 and the left middle cingulate gyrus, with peak classification accuracies of  
401 71–77%. Additionally, in several regions the classifier discriminated the in-  
402 termediate and extreme entropy levels, including the left STG, right TTG,  
403 left PoCG, left cerebellum, and right supplementary motor area (SMA), with  
404 peak classification accuracies of 64–70%.

### 405 3.2. *Cross-modal sensitivity to uncertainty*

406 We used cross-modal searchlight classification to identify brain areas  
407 where response patterns discriminating levels of uncertainty generalized (i.e.,  
408 were similar) across the auditory and visual modalities. Classifiers were  
409 trained to discriminate between levels of regularity in one sensory modality

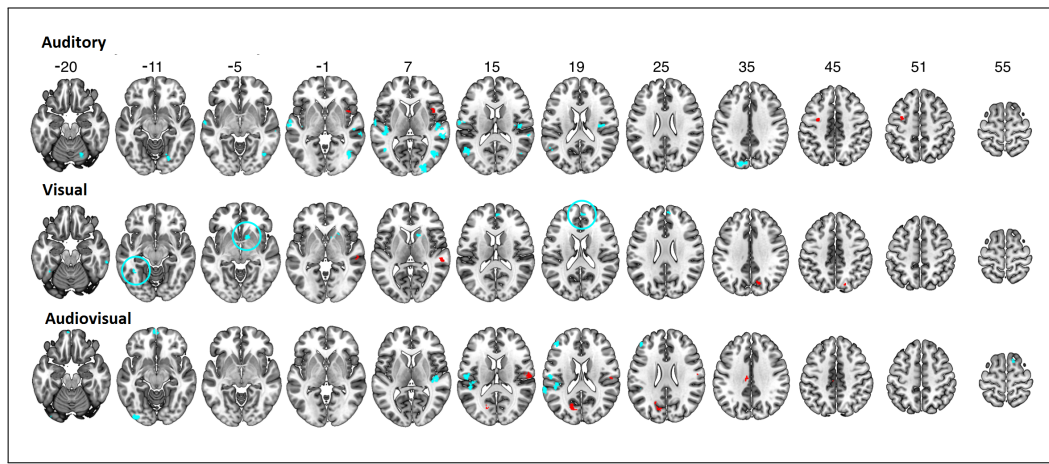


Figure 2: **Neural sensitivity to uncertainty in the auditory, visual, and audiovisual series.** Significant clusters of searchlights where response patterns reliably discriminated highly regular and random series are indicated in red. Significant clusters where response patterns discriminated the two intermediate levels of regularity from the two extreme levels (a quadratic discrimination) are plotted in cyan (cluster-level  $p < .05$ , corrected for multiple comparisons). Classifiers were tested using leave-one-participant-out cross-validation and statistically evaluated using permutation tests.

410 and then tested on input from the other modality using leave-one-participant-  
411 out cross-validation. Cross-modal classification of high and low entropy se-  
412 ries revealed significant clusters of searchlights in left orbitofrontal cortex  
413 (OFC), left MTG, and right cerebellum (see Figure 3, red clusters; cluster-  
414 level  $p < .05$ , corrected for multiple comparisons). These significant clusters  
415 had peak classification accuracies of 66–70% cross-validated across partici-  
416 pants (theoretical chance = 50%). Interestingly, cross-modal classification  
417 discriminating intermediate and extreme levels of entropy (analogous to a  
418 U-shaped discrimination) was extensive (Figure 3, cyan clusters), implicat-  
419 ing the right inferior frontal gyrus, SMA and SMG bilaterally, left PCG and  
420 MFG, left cerebellum, left superior parietal lobule, left inferior occipital and  
421 fusiform gyri, and the right insula (cluster-level  $p < .05$ , corrected for mul-  
422 tiple comparisons; see Table 2 for all significant clusters and Supplementary  
423 Movie for 3D rendering). These areas exhibited peak two-way classification  
424 accuracies of 61–64%.

425

[Table 2 around here]



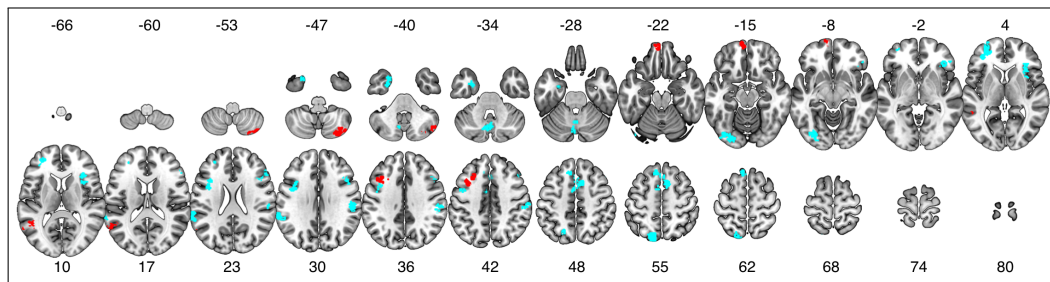


Figure 3: **Cross-modal searchlight classification of input uncertainty.** The searchlight analysis identified brain regions where classifiers trained to discriminate levels of regularity in one modality (e.g., auditory inputs) could successfully classify levels of regularity in the other modality (e.g., visual inputs, and vice versa). Significant clusters of searchlights where response patterns for highly regular and random series could be reliably classified across the auditory and visual modalities are indicated in red. Significant clusters of searchlights with reliable cross-modal classification of intermediate and extreme levels of regularity are plotted in cyan. Classifiers were tested on the left-out modality using leave-one-participant-out cross-validation, and statistically evaluated using permutation tests. Searchlight results are statistically significant at cluster-level  $p < .05$ , corrected for multiple comparisons.

### 426 3.3. Hippocampal analysis

427 Given prior studies implicating the hippocampus in associative learning,  
428 statistical learning, and sensitivity to uncertainty more generally (Strange  
429 et al., 2005; Harrison et al., 2006; Turk-Browne et al., 2009; Reddy et al.,  
430 2015), we conducted multivariate analyses analogous to those reported for  
431 searchlights above within anatomically-defined left and right hippocampus  
432 ROIs. Given their potentially differential roles in contextual integration (see  
433 Hartzell, Tobia, Davis, Cashdollar, & Hasson, 2015), we separately analyzed  
434 response patterns in the left and right hippocampus. As in the previous anal-  
435 yses, we tested for responses discriminating both high and low entropy levels,  
436 and intermediate and extreme entropy levels for auditory, visual, and audio-  
437 visual stimuli (thus six tests per left and right hippocampus, 12 total). In  
438 addition, we evaluated cross-modal linear and quadratic classification anal-  
439 yses (two tests per left and right hippocampus, four total). Due to the  
440 exploratory nature of the analysis we did not control for family-wise error  
441 over the 16 tests.

442 The analysis yielded two suggestive findings. For the right hippocampus,  
443 response patterns discriminated highly regular and random audiovisual series  
444 with 71% accuracy (theoretical chance = 50%,  $p = .003$ , permutation test,



445 uncorrected). In the left hippocampus, cross-modal classification of highly  
446 regular and random series reached 62% accuracy ( $p = .004$ , permutation  
447 test, uncorrected). Apart from these two instances, all other tests yielded  
448 accuracies very close to or below chance level.

#### 449 **4. Discussion**

450 Our main aims were to determine whether it is possible to identify mono-  
451 tonic and non-monotonic neural sensitivity to uncertainty, and whether these  
452 neural signatures generalize across sensory modalities. Our main findings are  
453 as follows. First, multivariate pattern classification analysis proved highly  
454 sensitive, suggesting that neural response patterns contain information dif-  
455 ferentiating levels of uncertainty in short input series. Response patterns not  
456 only discriminated between highly regular and random series, which is to be  
457 expected from the existing literature (e.g., Cunillera et al., 2009; McNealy et  
458 al., 2006), but in some areas also discriminated the two intermediate levels of  
459 uncertainty from the two extremes. This latter finding is consistent with the  
460 view (e.g., Nastase et al., 2014; Kidd et al., 2012; Hasson, 2017) that sensitiv-  
461 ity to input statistics may comprise computations for which neural activity  
462 does not scale monotonically with uncertainty. The resulting network of brain  
463 regions includes perisylvian areas implicated in prior work (e.g., Tobia et al.,  
464 2012) and overlaps with areas characterized by intermediate-scale temporal  
465 receptive windows (Hasson et al., 2008; Lerner, Honey, Silbert, & Hasson,  
466 2011). Uncertainty in audiovisual stimuli engaged some systems recruited  
467 in the auditory condition (e.g., superior temporal cortex), but also recruited  
468 prefrontal systems.

469 Equally important, when probing for supra-modal sensitivity to uncer-  
470 tainty, we identified a number of regions where it was possible to decode the  
471 level of uncertainty in one modality using a classifier trained discriminate lev-  
472 els of uncertainty in the other modality. Interestingly, cross-modal responses  
473 differentiating intermediate from extreme levels of entropy comprised a fairly  
474 widespread network, whereas relatively few areas differentiated high and low  
475 levels of uncertainty in a cross-modal fashion.

##### 476 *4.1. Cross-modal and non-monotonic sensitivity to uncertainty*

477 Few studies have directly examined whether there are neurobiological  
478 systems that track the level of regularity in sensory inputs in a supra-modal  
479 fashion; that is, independently of sensory modality. Two studies by Schubotz

480 et al. compared processing of regularity in either auditory and visual se-  
481 ries (Schubotz & von Cramon, 2002) or abstract series and motor actions  
482 (Schubotz & von Cramon, 2004), reporting adjacent and overlapping activ-  
483 ity patterns in premotor cortex. However, both studies required participants  
484 to deliberately predict future events, which makes it unclear whether the  
485 results are a result of endogenous processing or explicit executive demands.  
486 In our own prior work (Nastase et al., 2014), we identified areas sensitive to  
487 regularity for either auditory or visual inputs, but found no area that was  
488 generally sensitive in both modalities. As noted in the Introduction, conjunc-  
489 tions of unisensory response maps provide only weak evidence for abstract,  
490 supra-modal computations (e.g., Peelen & Downing, 2006). Rather, in the  
491 current study we used cross-modal classification, which provides a more ro-  
492 bust test of representational content shared across modalities (Man et al.,  
493 2012; Kaplan et al., 2015).

494 The cross-modal searchlight classification analysis identified an extensive  
495 supra-modal network of regions, some discriminating highly regular from ran-  
496 dom inputs (the typical contrast in univariate studies of uncertainty), and  
497 others differentiating the intermediate and extreme conditions in a quadratic  
498 fashion. Cross-modal regions discriminating the most regular from random  
499 inputs were limited to the left posterior middle temporal gyrus, the left pre-  
500 motor cortex/middle frontal gyrus, and left orbitofrontal cortex. The pos-  
501 terior lateral temporal cortex is multisensory, receiving input from both au-  
502 ditory and visual association cortices (Barnes & Pandya, 1992; Beauchamp,  
503 Argall, Bodurka, Duyn, & Martin, 2004). It may be that multi-modal tem-  
504 poral areas sensitive to regularity in the environment are recruited similarly  
505 across modalities, and prior work has shown that this area tracks regular-  
506 ity in visual series (Bischoff-Grethe, Proper, Mao, Daniels, & Berns, 2000).  
507 Cross-modal sensitivity to uncertainty in premotor cortex is consistent with  
508 prior findings (Schubotz & von Cramon, 2002) documenting its sensitivity  
509 to the complexity of auditory and visual series, though in non-overlapping  
510 areas. Meyniel and Dehaene (2017) have also linked this region to tracking  
511 confidence and uncertainty in simple auditory and visual series.

512 Cross-modal sensitivity to uncertainty observed in orbitofrontal cortex is  
513 consistent with recent theories implicating this region, and limbic cortices  
514 more generally, as a source of predictive feedback signals conveyed to lower-  
515 level perceptual areas (Chanes & Barrett, 2016; Trapp & Bar, 2015). As the  
516 highly regular and random series differ in the extent to which they license pre-  
517 dictions, observed differences in the response topographies in these areas may

518 reflect the operation of predictive processes. Finally, in a post-hoc analysis,  
519 we discovered that response patterns in the right hippocampus differentiate  
520 highly structured and random audiovisual series, while the left hippocampus  
521 differentiates structured and random series across modalities. These sug-  
522 gestive results support previous work pointing to associative learning in the  
523 hippocampus in the context of implicit learning (Turk-Browne et al., 2009,  
524 Reddy et al., 2015). In future work, cross-modal classification may prove  
525 useful in testing whether the hippocampus encodes statistical regularities in  
526 a supra-modal fashion.

527 Cross-modal responses discriminating the intermediate and extreme levels  
528 of regularity were surprisingly prevalent (seen in the spatial extent of cyan  
529 clusters in Figure 3). On the left, these were found in the middle frontal  
530 gyrus, temporal pole, lateral occipital cortex, intraparietal sulcus, and au-  
531 ditory association cortex. On the right, significant clusters were identified  
532 in the supramarginal gyrus and inferior frontal gyrus. Immediately rostral  
533 to the premotor cluster that discriminated high and low entropy conditions  
534 cross-modally, we identified another cross-modal cluster that discriminated  
535 intermediate from extreme entropy levels. Schubotz et al. (2002) had sug-  
536 gested that different areas in premotor cortex are involved in prediction of  
537 auditory and visual stimuli, such that prediction of auditory sequences uti-  
538 lizes premotor areas involved in verbal articulation, and prediction of visual  
539 sequences utilizes areas involved in hand movement. Expanding on this idea,  
540 our findings suggest a finer-grained, common substrate for the representa-  
541 tion of uncertainty across modalities in premotor cortex. Quadratic entropy  
542 discrimination was also found in the dorsomedial prefrontal cortex bilater-  
543 ally. We have previously documented an analogous type of non-monotonic,  
544 U-shaped response profile to regularity in auditory series when considering  
545 short (10 s) epochs (Tobia, Iacovella, Davis, & Hasson, 2012), as well as  
546 U-shaped whole-brain connectivity profiles for the anterior cingulate cortex  
547 during long periods of auditory stimulation (Nastase et al., 2015).

548 These quadratic, non-monotonic response profiles are compatible with  
549 several types of computational accounts, as we have previously discussed in  
550 detail (Nastase et al., 2015; Hasson, 2017). In brief, they may be indicative  
551 of systems that do not explicitly code for statistical predictability or regu-  
552 larity per se, but instead are involved in modeling the system generating the  
553 sensory input. This modeling process may be outwardly reflected in an ap-  
554 parent U-shaped response profile because such model descriptions are simpler  
555 to construct for environmental systems that generate highly regular or ran-

556 dom inputs than for systems that generate inputs with intermediate levels of  
557 regularity. Another possibility is that these brain areas subserved prediction of  
558 multiple future transitions (e.g., two stimuli into the future,  $t + 1$ ,  $t + 2$ ), and  
559 are sensitive to *predictive information rate* (PIR): the degree to which the  
560 stimulus at time  $t + 1$  impacts the observers' certainty regarding the stimulus  
561 expected at  $t + 2$ . Computational work has shown that PIR is maximal for  
562 series with intermediate levels of disorder, but lowest for both very regular  
563 and random series (Abdallah & Plumbley, 2009). A third possibility is that  
564 these brain areas are involved in the generation of predictions and sensitive  
565 to prediction error, but only so long as predictions are licensed by the input.  
566 This might be reflected in gradually increasing activity as disorder increases  
567 within a reasonable bound, but with a subsequent decline for the random  
568 condition, where no predictions are licensed. Thus, both the highly ordered  
569 and random condition would be accompanied by low prediction errors. We  
570 note, however, that the latter interpretation may be the least plausible for  
571 the relatively brief 10 s series presented here, because for such short random  
572 series it may be quite difficult to establish evidence that prediction is not  
573 licensed, particularly given the tendency to perceive streaks in completely  
574 random inputs (Huettel et al., 2002).

575 Areas encoding audiovisual entropy were largely non-overlapping with  
576 areas encoding entropy in unisensory visual and auditory series, which is  
577 consistent with prior work (Andric, Davis, & Hasson, 2017). This relatively  
578 modest overlap is also consistent with behavioral work suggesting that mul-  
579 tisensory regularities are learned independently of regularities conveyed via  
580 their unisensory constituents (Seitz, Kim, van Wassenhove, & Shams, 2007).  
581 In the current experiment, the auditory and visual channels in the audio-  
582 visual condition provided redundant statistical information (mutual infor-  
583 mation was maximal). This may have produced a more efficient encoding  
584 of the series tokens themselves, in this way affording greater sensitivity to  
585 audiovisual regularities.

586 Although participants performed an orthogonal cover task, we cannot rule  
587 out the possibility that implicit attentional allocation may have co-varied  
588 with the entropy manipulation. Attention and prediction are related con-  
589 structs and often conflated experimental work (Summerfield & Egner, 2009),  
590 where statistical regularities licensing expectations are often used to guide  
591 attention (Posner, Snyder, & Davidson, 1980; Zhao, Al-Aidroos, & Turk-  
592 Browne, 2013). Recent work on the interaction of these processes has met  
593 with mixed results (Jiang, Summerfield, & Egner, 2013; Kok et al., 2012)

594 and our experiment was not designed to adjudicate between these processes.  
595 Note that our procedure for normalizing response patterns may be robust to  
596 simple attentional effects (by mean-centering each searchlight), but does not  
597 necessarily rule out more complex attentional effects (Jehee, Brady, & Tong,  
598 2011; Nastase et al., 2017).

599 Our findings point to the importance of examining non-monotonic re-  
600 sponses to predictability and uncertainty when studying brain systems sen-  
601 sitive to input statistics, as such responses may be as prevalent as the more-  
602 studied monotonic response profiles. More generally, they demonstrate the  
603 utility and importance of using cross-modal classification for drawing conclu-  
604 sions about supra-modal computations underlying statistical learning. While  
605 work to date, including our own, has largely failed to identify supra-modal  
606 systems sensitive to sequential structure, suggesting that sensory cortices  
607 support these computations (e.g., Dehaene et al., 2015; Nastase et al., 2014;  
608 Schubotz & von Cramon, 2002), this conclusion may rely in part on ana-  
609 lytic limitations. The cross-classification approach used here suggests that  
610 widespread association cortices are sensitive to structure in sequential stimuli  
611 across sensory modalities.

#### 612 *4.2. Methodological considerations*

613 Multivariate approaches provide specific insights into distributed neural  
614 representation, with prior studies suggesting that searchlight pattern analyses  
615 are both more sensitive and more opportunistic in exploiting potential con-  
616 founding variables (Coutanche, 2013; Davis et al., 2014; Jimura & Poldrack,  
617 2012). As such, several considerations should be discussed when interpreting  
618 the current findings. First, the searchlight approach provides coarse localiza-  
619 tion, as each searchlight aggregates information over numerous (i.e., over 100)  
620 voxels and overlaps with numerous neighboring searchlights. Furthermore,  
621 to better approximate other correlation-based classification analyses (e.g.,  
622 Haxby et al., 2001), we normalized (i.e., Z-scored) response patterns across  
623 voxels within each searchlight prior to classification (Misaki et al., 2010;  
624 Nastase et al., 2016). This procedure effectively removes any searchlight-  
625 average differences in response magnitude between experimental conditions.  
626 The classifier therefore operates solely on distributed response topographies  
627 of relative activity, and cannot capitalize on general differences in overall  
628 response magnitudes across conditions within a given searchlight. Aban-  
629 doning this normalization scheme and allowing the classifier to also utilize

630 regional-average response magnitudes would likely more closely approximate  
631 a conventional univariate analysis.

632 Davis et al. (2014) argued that multivariate analyses may appear to of-  
633 fer greater sensitivity than univariate analyses because they exploit idiosyn-  
634 cratic within-participant response variability that is typically discarded at  
635 the group level in univariate analyses. However, this concern holds primarily  
636 for within-participant classification analyses where the result of classifica-  
637 tion (e.g., classification accuracy, cross-validated across runs within a par-  
638 ticipant) is then aggregated in a group level statistical analysis. In contrast,  
639 here we used leave-one-*participant*-out cross-validation, which limits classi-  
640 fiers to voxel-level response variability that is consistent across participants.  
641 Allefeld and colleagues (2016, pp. 382–383) have demonstrated that perform-  
642 ing second-level statistical tests on participant-level classification accuracies  
643 (which are typically distributed asymmetrically above chance) does not prop-  
644 erly perform population-level inference (effectively testing only the global null  
645 hypothesis that there is no effect for any participant). When separate clas-  
646 sifiers are trained per participant, accuracies may result from idiosyncratic  
647 patterns that distinguish conditions in one individual but do not generalize  
648 to other individuals. Allefeld and colleagues suggest that performing cross-  
649 validation across participants, on the other hand, effectively provides rigorous  
650 population inference. However, this approach comes with a potential cost.  
651 Specifically, leave-one-participant-out cross-validation requires that response  
652 patterns are spatially registered across participants (within the radius of a  
653 searchlight). Although all participants' data were spatially normalized to the  
654 MNI template prior to classification, anatomical alignment cannot in prin-  
655 ciple perfectly align fine-grained functional topographies and yields differen-  
656 tially effective alignment across the brain (Guntupalli et al., 2016; Haxby  
657 et al., 2011). While our results add to previous work in demonstrating that  
658 cross-participant classification is feasible (e.g., Mourao-Miranda et al., 2005),  
659 due to the imperfect registration of functional topographies, classification  
660 may rely on relatively coarse-grained response topographies differentiating  
661 levels of uncertainty.

#### 662 4.3. Summary

663 To date, relatively modest progress has been made in developing neurobio-  
664 logical accounts of uncertainty that extend beyond explanations of monotonic  
665 responses in single modalities. The current study informs current neurobi-  
666 ological models of neural sensitivity to statistical regularities in two ways.



667 We identified neural systems that encode information about statistical regu-  
668 larities in a supra-modal manner, as evidenced by cross-modal multivariate  
669 classification. In addition, our findings emphasize that the human brain re-  
670 sponds to uncertainty both monotonically and non-monotonically, suggesting  
671 that some brain regions track uncertainty *per se*, while others code for struc-  
672 tural features of the systems generating the sensory input.

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