1	Longitudinal brain structure changes in Parkinson's disease: a replication study
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16 Abstract

17

18	Context. An existing major challenge in Parkinson's disease (PD) research is the identification of
19	biomarkers of disease progression. While Magnetic Resonance Imaging (MRI) is a potential source of PD
20	biomarkers, none of the MRI measures of PD are robust enough to warrant their adoption in clinical
21	research. This study is part of a project that aims to replicate 11 PD studies reviewed in a recent survey
22	(JAMA neurology, 78(10) 2021) to investigate the robustness of PD neuroimaging findings to data and
23	analytical variations. Objective. This study attempts to replicate the results in Hanganu et al. (Brain,
24	137(4) 2014) using data from the Parkinson's Progression Markers Initiative (PPMI). Methods. Using 25
25	PD subjects and 18 healthy controls, we analyzed the rate of change of cortical thickness and of the
26	volume of subcortical structures, and we measured the relationship between MRI structural changes and
27	cognitive decline. We compared our findings to the results in the original study. Results. (1) Similarly to
28	the original study, PD patients with mild cognitive impairment (MCI) exhibited increased cortical
29	thinning over time compared to patients without MCI in the right middle temporal gyrus, insula, and
30	precuneus. (2) The rate of cortical thinning in the left inferior temporal and precentral gyri in PD patients
31	correlated with the change in cognitive performance. (3) There were no group differences in the change of
32	subcortical volumes. (4) We did not find a relationship between the change in subcortical volumes and the
33	change in cognitive performance. Conclusion. Despite important differences in the dataset used in this
34	replication study, and despite differences in sample size, we were able to partially replicate the original
35	results. We produced a publicly available reproducible notebook allowing researchers to further
36	investigate the reproducibility of the results in Hanganu et al. (2014) when more data becomes available
37	in PPMI.
38	
39	Introduction

40

41	Parkinson's disease (PD), one of the most common neurodegenerative diseases, is often characterized by
42	akinesia, bradykinesia, tremor, and is commonly associated with mild cognitive impairment which
43	significantly decrease overall quality of life [1]. These symptoms are accompanied by atrophy of the
44	cortical and subcortical brain structures as well as cortical thinning [2]. As a result, there has been interest
45	in determining whether MRI measures of atrophy can be used as a biomarker of cognitive decline.
46	Overall, gray matter atrophy and cortical thinning are present in early PD, while frontal atrophy and
47	temporoparietal thinning are associated with cognitive impairment in PD [3].
48	
49	MRI-derived measures of the structural brain changes occuring in PD have emerged as potential
50	diagnostic and prognostic tools to understand the trajectory of PD. Structural imaging, especially regional
51	cortical thickness and loss of gray matter volume, has been considered helpful in determining a PD
52	diagnosis, progression prognosis, and distinguishing PD from other dementias [2]. However, the need to
53	further investigate the sensitivity, reliability, effect of confounding factors, and overall generalizability of
54	these progression measures has been highlighted (e.g., [3]) and such rigorous validation is likely a factor
55	preventing the adoption of MRI measures as outcome measures in PD clinical research.
56	
57	The replication of neuroimaging findings has been challenged in multiple ways in recent years. For
58	example, in the study of Botvinik-Nezer et al. [4], 70 independent teams were asked to analyze the same
59	dataset using the methods of their choice. Results obtained across research teams did not concur on five
60	out of the nine ex-ante hypotheses, reaching agreement levels ranging from 21% to 37%. Furthermore, the
61	identification of regional brain atrophy in PD has been of interest as a possible marker of certain
62	symptoms of PD and of the progression of PD [2]. However, studies conducted in non-PD populations
63	have shown that estimates of regional volume [5,6] and of cortical thickness vary depending on the
64	software toolbox [7,8]. Overall, a range of factors matter in the replicability of neuroimaging findings,
65	including computational environments [9,10], analysis tools and versions [11,12], statistical models [13],
66	and study populations [14].

67

68	This study is a part of a reproducibility evaluation project that aims to replicate 11 structural MRI
69	measures of PD reviewed in Mitchel et al. [2]. The goal of the present study is to replicate the work by
70	Hanganu et al. [15] to test whether prior findings regarding structural MRI-derived PD biomarkers
71	replicate in a different dataset using similar analytical methods. Hanganu et al. [15] compared the change
72	of gray matter volume and cortical thinning over time between PD patients with mild cognitive
73	impairment (PD-MCI), PD patients without mild cognitive impairment (PD-non-MCI), and healthy older
74	controls (HC); and also tested the relationship between longitudinal structural changes and cognitive
75	decline in the PD patients. They reported four main findings: (Finding 1) an increased rate of cortical
76	thinning in PD patients with mild cognitive impairment compared to PD patients without MCI (mainly
77	affecting the right temporal regions, insula, and inferior frontal gyrus), and compared to healthy controls
78	(mainly in the right temporal regions and supplementary motor area); (Finding 2) a correlation between
79	the change in Montreal Cognitive Assessment (MoCA) scores and cortical thinning in the bilateral
80	temporal lobe, right occipital medial lobe, and the left postcentral gyrus in PD patients; (Finding 3) an
81	increased loss of the amygdala and nucleus accumbens volumes as well as overall cortical thickness for
82	the PD-MCI group compared to HC; (Finding 4) a correlation between the change of the right amygdala
83	and thalamus volumes and the change in MoCA scores in PD patients.
0.4	

84

85 The results of Hanganu et al. [15] are of clinical interest because they provide insight into the relationship 86 between structural brain changes and cognitive impairment, thus highlighting possible neural substrates of 87 PD-related cognitive impairment [16]. Our study addresses the issue of MRI measure replicability, 88 investigates crucial elements of reporting the study to make it replicable, and discusses the impact of 89 study design decisions on the replicability. The goal of our study was to attempt to replicate the original 90 findings using a different cohort. We used open data from the Parkinson's Progression Markers Initiative 91 (PPMI; www.ppmi-info.org) in order to construct a similar patient cohort as that used in the original 92 study and we followed the data processing methods and statistical analyses from the original study.

- 93
- 94 Methods
- 95
- 96 Participants
- 97

98 The original study included 15 PD-non-MCI, 17 PD-MCI and 18 HC. In order to reconstruct this cohort, 99 PD patients and HC were selected from PPMI to attempt to match the sample size and demographics of the 100 groups in the original study. The following criteria were used to define the PD cohorts: clinical diagnosis 101 of PD, available T1-weighted images at two research visits, Hoehn and Yahr stage I and II (the stage was 102 stable across the two visits for each patient), testing performed at PD OFF state, available MoCA scores, 103 and the absence of any other neurological condition. Data was collected after approval of the local ethics 104 committees of the PPMI's participating sites. All participants provided written informed consent. This study 105 was conducted in accordance with the Declaration of Helsinki and was exempt from the Concordia 106 University's Research Ethics Unit.

107

Patients were divided into PD-MCI and PD-non-MCI groups. In the original study, MCI was diagnosed on the basis of the presence of subjective complaints of cognitive impairment, objective impairment on two or more neuropsychological tests in one domain of cognitive function and the absence of dementia. In the PPMI dataset, patients are already classified as having MCI or not using a very similar criteria for classification, and thus the existing classification was used. Diagnosis of MCI in the PPMI is determined based on the following criteria: impairment in at least one cognitive domain, decline from pre-morbid function, and lack of significant impact of cognitive impairment on daily function.

115

116 Ten PD-MCI (M age = 67.6; SD = 5.8), 15 PD-non-MCI (M age = 63.4; SD = 9.4), and 18 HC participants 117 were selected (M age = 66.9; SD = 6.1). PD-non-MCI and HC group sample sizes match those of the original 118 study but an insufficient number of PD-MCI patients were identified in the PPMI dataset that met all the

- original inclusion criteria, thus our sample is smaller than the original sample (n=10 vs n=17). Descriptive
- 120 statistics are reported in Table 1.
- 121

122 Table 1. Descriptive statistics

	Mean ± SD			<i>p</i> value		
	PD-MCI	PD-non-	HC	PD-MCI	PD-	PD-non-
	(n = 10)	MCI (n =	(n = 18)	vs PD-	MCI	MCI vs
		15)		non-MCI	vs HC	HC
sex (M/F)	10/0	10/5	15/3	1	1	1
age (y)	67.6 ± 5.8	63.4 ± 9.4	66.9 ± 6.1	0.21	0.76	0.2
education (y)	14.6 ± 2.4	14.5 ± 1.9	16.1 ± 2.9	0.92	0.17	0.66
Duration Time 2 - 1 (m)	23.9 ± 9.0	19.1 ± 5.4	14.5 ± 2.9	0.11	< .001	0.003
disease duration	4.9 ± 3.3	5.1 ± 3.1	-	0.9	-	-
UPDRS III ON (Time 1)	20.2 ± 14.3	17.7 ± 9.6	-	0.72	-	-
UPDRS III OFF (Time 1)	25.2 ± 13.0	22.3 ± 10.8	-	0.55	-	-
UPDRS III OFF (Time 2)	29.3 ± 13.6	25.7 ± 11.3	-	0.47	-	-
MoCA (Time 1)	24.3 ± 1.9	25.9 ± 1.8	-	0.05	-	-
MoCA (Time 2)	24.5 ± 2.4	27.0 ± 1.7	-	0.006	-	-

123 Group differences computed with Student's t-test for continuous variables and with χ^2 test for the

- 125 MCI, Mild Cognitive Impairment; MoCA, Montreal Cognitive Assessment; UPDRS, Unified Parkinson's
- 126 Disease Rating Scale.

127

- 128 Image acquisition and preprocessing
- 129

MRI images were taken from the PPMI which uses a standardized study protocol and the following parameters: repetition time = 2.3 s, echo time = 2.98 s, inversion time = 0.9 s, slice thickness = 1 mm, number of slices = 192, field of view = 256 mm, and matrix size = 256×256 . However, since PPMI is a multisite project there may be slight differences in the sites' setup. Scans were acquired using different 3T scanners (Philips Achieva n=2; Siemens Prisma fit n=8; Siemens Prisma n=4; Siemens Skyra n=2; Siemens TrioTim n=64; Siemens Verio n=6). There were scans with echo time (TE) that diverged from the

¹²⁴ categorical variable.

136	standardized protocol: one image with $TE = 2.52$ s, one image with $TE = 1.91$ s, three images with $TE =$
137	2.91 s, one image with $TE = 2.93$ s, four images with $TE = 2.95$ s, four images with $TE = 2.96$ s, two images
138	with TE = 3.06s. Additionally, two images had TE = 2.94 s, TR = 6.49 s, and TE = 2.91 s, TR 6.26 s.
139	
140	T1-weighted brain images were processed using FreeSurfer 7.1.1 [17]. The longitudinal preprocessing
141	stream was used to calculate the change in cortical thinning and subcortical volumes [18]. FreeSurfer's
142	recon-all function was used for cortical reconstruction. First, all timepoints were processed cross-
143	sectionally with the default workflow, then an unbiased template from the two timepoints was created for
144	each subject, finally data was processed longitudinally. Specifically an unbiased within-subject template
145	space and image [19] is created using robust, inverse consistent registration [20]. Several processing steps,
146	such as skull stripping, Talairach transforms, atlas registration as well as spherical surface maps and
147	parcellations are then initialized with common information from the within-subject template, significantly
148	increasing reliability and statistical power [18]. The rate of change of cortical thickness between the two
149	timepoints was calculated for each subject. Cortical thickness was smoothed with a 10 mm FWHM kernel.
150	The original study also reported manual correction of misclassified tissue types, which was not performed
151	in our study since the protocol for it was insufficient to replicate.

152

153 Statistical analyses

154

Structural brain images and Montreal Cognitive Assessment (MoCA) scores from the initial and the followup visits were analyzed consistently with the 4 main findings reported in the original study. (Finding 1) We tested vertex-wise differences in the change of cortical thickness between HC, PD-MCI, and PD-non-MCI groups with an ANCOVA model. (Finding 2) We tested the correlation between the change of cortical thickness and the change of MoCA scores in PD-MCI, PD-non-MCI, and PD-all (all PD patients) groups. The time between the two visits was added as a covariate in the general linear models. Cluster-wise p-value threshold was used at the p < .05 level. The rate of change of the cortical thickness was calculated with the

162	formula: (Thickness at Time 1 – Thickness at Time 2) / (Time 2 – Time 1). Subcortical volumes were
163	adjusted for the estimated total intracranial volume as well as the averages of the two time points using
164	regression-based correction, in line with the original study. (Finding 3) We tested the differences in regional
165	volume changes between the three groups using t-tests and (Finding 4) measured the correlations between
166	the change in MoCA scores and change of the subcortical volumes and cortical thickness in each group
167	using Pearson correlation.
168	
169	Code availability
170	
171	We used publicly available software to facilitate reproducing our study. Pandas v. 1.5.2 was used to
172	define the cohort from PPMI data files. FreeSurfer 7.1.1 was used for image preprocessing and vertex-
173	wise analyses. We used a containerized version of FreeSurfer managed by Boutiques 0.5.25
174	(doi:10.5281/zenodo.3839009). The containerized FreeSurfer analyses were executed through the Slurm
175	batch manager on the Narval cluster (https://docs.alliancecan.ca/wiki/Narval/en) hosted at Calcul Québec
176	and part of Digital Research Alliance of Canada.
177	
178	The code and results are publicly available at https://github.com/LivingPark-MRI/hanganu-etal-2014.
179	Data used in the notebook were downloaded directly from the PPMI and cannot be shared publicly due to
180	its Data Usage Agreements preventing republishing data. We developed a Python package (LivingPark
181	utils, available at https://github.com/LivingPark-MRI/livingpark-utils) to download and manipulate PPMI
182	data directly from the original PPMI database. As a result, our notebook can be re-executed by anyone
183	with a PPMI account.
184	
185	Results

187 Vertex-wise results

188

We found numerous group differences in the rate of change of cortical thickness. The results are reportedin Table 2 and Fig. 1.

191

- 192 PD-MCI vs. PD-non-MCI. The two patient groups differed in the rate of cortical thinning. The PD-MCI
- 193 group, compared to PD-non-MCI patients, had an increased rate of cortical thinning in the right middle
- 194 temporal and precentral gyri as well as right insula. PD-non-MCI group exhibited an increased thinning in
- 195 the left precuneus compared to the PD-MCI group.

196

- 197 *PD-MCI vs. HC.* The HC group had increased cortical thinning in the right precentral and supramarginal
- 198 gyri, left superior frontal gyrus, and bilateral superior parietal lobule, compared to the PD-MCI group.

- 200 PD-non-MCI vs. HC. The HC group had increased cortical thinning in the right precuneus as well as
- 201 precentral and supramarginal gyri compared to the PD-non-MCI group.
- 202

203 Table 2. Vertex-wise group differences in the rate of change of cortical thickness

	Size					clusterwise
Group and region	(mm²)	MNI X	MNI Y	MNI Z	Max	<i>p</i> -value
PD-MCI vs PD-non-MCI						
L precuneus	901.62	-15.4	-45.2	65.8	2.8711	.0004
R precentral	808.31	45	-4.9	49.8	-4.3574	.0026
R insula	689.83	36.1	-16.4	-3.4	-4.285	.0066
R MTG	636.56	42.1	7.1	-37.1	-4.7243	.0108
PD-MCI vs HC						
L SPL	1596.42	-12.2	-55.4	59.9	3.4112	.0002
L SFG	816.25	-8.3	35.1	34	4.2357	.0006
R precentral	619.04	15	-12.2	61.8	2.4693	.0144
R supramarginal	578.61	37.3	-29.7	39.5	3.0369	.0221
R SPL	563.81	29.5	-48.4	42.7	3.9183	.0256

PD-non-MCI vs HC						
R SMG	1010.34	35.7	-30.6	39.6	4.4171	.0002
R precentral	580.49	43.5	-9.4	46.2	3.8495	.0211
R precuneus	537.11	8.6	-71.2	40	3.6102	.0384

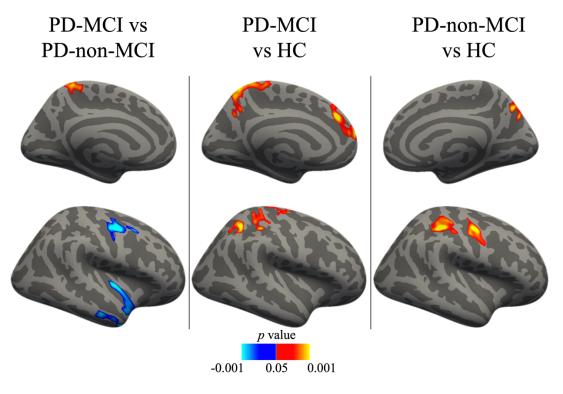
HC, healthy controls; Max, maximum -log10(p value) in the cluster; MTG, middle temporal gyrus; PD-

205 non-MCI, Parkinson's disease without mild cognitive impairment; PD-MCI, Parkinson's disease with

206 mild cognitive impairment; SFG, superior frontal gyrus; SMG, supramarginal gyrus; SPL, superior

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207 parietal lobule.
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208



210 Fig. 1. Vertex-wise group differences in the rate of change of cortical thickness. Cold colors

211 represent increased cortical thinning in the first group compared to the second group, warm colors

- 212 represent increased cortical thinning in the second group compared to the first group. Results
- 213 corrected with the cluster-wise threshold (p < .05).

214 HC, healthy controls; PD-MCI, Parkinson's disease with mild cognitive impairment; PD-non-MCI,

215 Parkinson's disease without mild cognitive impairment.

216

217	There was a significant negative correlation between the change in MoCA scores and the rate of change
218	of the right middle frontal gyrus thickness in the PD-MCI group ($p < .05$). There was a positive
219	correlation between the MoCA and the rate of change of the left inferior temporal and precentral gyri
220	across all PD patients ($p < .05$). The correlations were not significant in the PD-non-MCI group. The
221	results are reported in Table 3 and Fig. 2.
222	

Table 3. Vertex-wise correlation between the rate of change of cortical thickness and the change in



Group and region	Size (mm²)	MNI X	MNI Y	MNI Z	Max	clusterwise <i>p</i> -value
PD-all						
L ITG	592.67	-53.3	-20.1	-33.1	3.4012	.0177
L precentral	523.77	-24.4	-16.8	64.5	2.5887	.0406
PD-MCI						
R rostral MTG	749.67	30.1	43.1	16.9	-4.0378	.0004

225 ITG, inferior temporal gyrus; L, left; Max, maximum -log10(p value) in the cluster; MCI, mild cognitive

226 impairment; MTG, middle temporal gyrus; R, right.

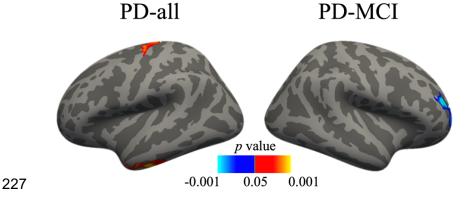


Fig. 2. Vertex-wise correlation between the rate of change of cortical thickness and the change in

229 Montreal Cognitive Assessment scores in the PD-all and PD-MCI groups.

230

231 Volumetric results

- 233 Group comparisons of the volumetric change of subcortical regions revealed increased decrease of the
- thalamus volume in the PD-MCI group compared to PD-non-MCI (p = .01). There was a difference in the
- change of the putamen volume between the PD-non-MCI and HC groups (p = .02), with HC exhibiting
- increased thinning. The results are reported in Table 4.
- 237

Table 4. Group differences in the volumetric change of the subcortical regions and the overall cortical

239 thickness

	PD-MCI		PD-non-MCI		Н	C	<i>p</i> values		
							PD-MCI vs	PD-	
	mean	%	mean	%	mean	%	PD-non-	MCI vs	PD-non-
							MCI	HC	MCI vs HC
CoTh	0.006	-0.57	0	-0.11	0.006	-0.21	.44	1	.5
Thal	-223.24	-2.56	210.34	1.25	-51.26	-0.68	.01	.28	.09
Caud	36.33	0.51	-12.99	-0.25	-9.36	-0.2	.63	.56	.95
Put	-16.38	-0.66	115.21	1.03	-86.9	-0.92	.21	.26	.02
Hipp	-50.43	-1.76	4.56	-1.14	24.22	-0.49	.43	.22	.74
Amyg	-39.03	-4.97	-5.15	-2.24	25.98	-0.65	.57	.2	.5
Nacc	-9.89	-1.23	-3.06	-0.82	8.04	0.23	.81	.52	.58

240 Subcortical volumes are presented in mm³, cortical thickness in mm. Amyg, amygdala; Caud, caudate;

241 CoTh, cortical thickness; Hipp, hippocampus; Nacc, nucleus accumbens; Put, putamen; Thal, thalamus.

- 242
- 243 Correlation analysis did not show any significant correlation between the change of MoCA scores and the
- change in volume of subcortical structures. Results are reported in Table 5.
- 245

Table 5. Correlation between the rate of change of the subcortical volumes and the change in Montreal

247 Cognitive Assessment scores

	PD	PD-all		PD-MCI		PD-non-MCI	
Structure	r	р	r	р	r	р	
R Thalamus	-0.03	.89	0.09	.81	0.07	.80	
R Caudate	0.09	.68	-0.18	.61	0.28	.31	
R Putamen	0.02	.92	0.14	.7	0.1	.73	

R Pallidum	0	1	-0.07	.84	0.33	.22
R Hippocampus	-0.1	.64	-0.04	.92	-0.05	.85
R Amygdala	-0.24	.26	-0.25	.48	-0.27	.33
R Nucleus accumbens	0.04	.87	0.38	.27	-0.12	.66
L Thalamus	0.19	.37	0.14	.71	0.48	.07
L Caudate	0	1	-0.29	.42	0.42	.12
L Putamen	-0.03	.9	-0.17	.63	0.19	.50
L Pallidum	0.05	.81	0.02	.97	0.15	.61
L Hippocampus	-0.01	.96	-0.08	.82	0.07	.81
L Amygdala	0.24	.26	0.32	.36	0.34	.22
L Nucleus accumbens	0.02	.92	-0.07	.85	0.12	.67

²⁴⁸ L, left; MCI, mild cognitive impairment; PD-non-MCI, Parkinson's disease without mild cognitive

249 impairment; PD-MCI, Parkinson's disease with mild cognitive impairment; R, right.

250

251 Discussion

252

253 This study attempted to replicate the results of Hanganu et al. [15], which focused on the longitudinal

254 changes in the cortical thickness and subcortical gray matter volume in PD patients. Group differences

between PD patients with and without MCI were investigated along with the relationship between the

structural changes and cognition. We used the analytic methods described in the paper and applied them

to a different dataset of PD patients with and without MCI, and HC.

258

259 We have replicated the differences in the rate of cortical thinning between the PD-MCI and PD-non-MCI

groups (Finding 1 in [15]), which supports the notion that these two patient groups differ in the rate of

261 neurodegeneration. Patients with MCI had increased cortical thinning of the right MTG and insula, which

262 overlaps with the regions reported in the original study. However, we did not replicate the group

263 differences involving the HC group.

264

We found a relationship between the decrease in cognitive performance and cortical thinning of the left precentral gyrus and ITG in PD patients. The ITG cluster partially overlaps with the area reported in the

267	original study. Although the structural changes were not found in the exact same brain voxels, the data
268	supports the role of the thinning of the temporal regions in PD patients' cognition (Finding 2 in [15]).
269	Additionally, we found a relationship between the increase of the cognitive performance and cortical
270	thinning of the right MFG in the PD-MCI group. This result was not reported in the original study and
271	provides additional insight into potential structural changes in PD populations. Overall, we have
272	replicated the original vertex-wise results (Findings 1 and 2 in [15]) to a certain extent.
273	
274	Volumetric results (Findings 3 and 4 in [15]) were not replicated. The original study reported group
275	differences in the change of overall cortical thickness as well as volumes of amygdala and nucleus
276	accumbens. Instead, we found higher atrophy of thalamus in the PD-MCI compared to PD-non-MCI
277	group, and higher putamen atrophy in the PD-MCI group compared to HC. Hanganu et al. [15] reported a
278	correlation between the change in cognitive performance and the change in gray matter volume in the
279	right thalamus and amygdala in PD patients. We found no significant correlations across all subcortical
280	regions.
281	
282	There are several factors that may explain the differences between the original results and the results of
283	our replication. Most importantly, the two studies differ in the sample sizes for the PD-MCI group. We
284	were unable to select enough PD patients with MCI that met all the inclusion criteria which reduced the
285	chance to replicate the results. This was troublesome despite the fact that we used PPMI, one of the
286	largest publicly available PD dataset. PPMI is a relatively new initiative and is lacking much longitudinal
287	data. Our Jupyter notebook remains accessible and can be re-run as new data becomes available in PPMI.
288	Importantly, current neuroscience recommends using larger sample sizes to avoid inflation of effect sizes.
289	Sample sizes used in research are increasing and recent data suggest that brain-wide association studies
290	may require as many as thousands of participants to define reliable brain-behavior relationships [21].

292 Differences between the samples may also affect replicability. There are no established clinical measures 293 to infer disease severity in the brain, but disease duration, UPDRS score (a measure of symptom severity), 294 and medication use are sometimes used as proxy measures. Average disease duration was very similar in 295 our sample compared to the original study suggesting the patients were roughly matched. However, some 296 patients had not yet started PD medications in our sample whereas all patients in the original study were 297 already taking dopaminergic medications, and the UPDRS score was also a few points lower in our 298 sample compared to the original study's sample, both of which suggest that the replication sample we 299 constructed from the PPMI cohort had slightly milder disease than the sample included in the original 300 study. Our sample is also slightly older than the original cohort. Furthermore, despite using the same 301 inclusion criteria as the original study, it is possible that other differences in sample characteristics may 302 have contributed to the incomplete replication. Conclusions drawn from our data should not be expanded 303 to different clinical populations (e.g., more severe PD patients).

304

305 Differences in neuroimaging data acquisition protocols and MRI scanners can also influence replicability.
306 Data used in our study was acquired using different MRI scanners. Although PPMI uses a standardized
307 protocol for data acquisition we cannot rule out the possibility that the reported differences may be related
308 to the variability introduced by using various scanners, even though the vast majority of scans were
309 acquired with a Siemens scanner. Ideally all participants should be scanned with the same machine but
310 the benefits of collecting more data in a multisite project outweighs the advantages of a single-stage
311 acquisition.

312

313 Software versions may also have impacted the results. FreeSurfer 5.3. for Centos 4 was used in the 314 original study. This version of FreeSurfer was released 10 years ago and is no longer supported or 315 recommended, hence we used version 7.1.1. for Centos 7 instead. Although the software version 316 shouldn't drastically change the clinical results, it is possible that it introduced variability during 317 preprocessing or during the statistical analysis stage. We used the mri glmfit-sim method to perform the

318 analysis (including cluster correction) while the original study used the QDEC (Query, Design, Estimate, 319 Contrast) method with mri surfcluster. Our method is more stringent but also more reliable. It might have 320 established more reliable borders between the gray and white matters. Filip et al. [22] reported structural 321 group differences in data analyzed with FreeSurfer 5.3. which were not replicated with version 7.1. 322 Previous studies indicated that software version may impact structural brain analyses [7,9]. We will test 323 the impact of software variability in our future work. 324 325 We thoroughly followed the original processing pipeline reported by Hanganu et al. [15]. Nevertheless, it 326 is possible that we have missed some steps which could have influenced the results. We did not perform 327 manual correction of misclassified brain tissue as this procedure cannot be objectively replicated. This 328 may have impacted the analysis regarding smaller subcortical structures. There might be slight differences 329 in the statistical models that we were not aware of. Any of the aforementioned discrepancies from the 330 original study could have impacted the ability to replicate the results. Once the analyses were conducted, 331 we contacted the authors of the original study to obtain their feedback, which importantly contributed to 332 the discussion section. 333 334 Finally, there is a negative bias in replication studies, coming from the fact that researchers conducting 335 replications focus on following original methods rather than getting positive results. Therefore, it is 336 expected that more negative results are reported in replications than in original studies. We encourage 337 scientists to follow all the steps and details from the original studies instead of simply aiming to replicate 338 positive results. 339 340 We encountered multiple challenges while attempting to replicate the study by Hanganu et al. [15]. 341 Analysis details are necessarily limited in the methods section of most papers which left us to infer some 342 analytic steps. We also had difficulty constructing a similar cohort from publicly available PD data, which 343 led to some differences in the patient characteristics between the original and replication samples, and to

344	differences in sample size. We have published a Jupyter notebook that the research community can use to
345	replicate our study. While respecting the PPMI data usage agreement, it clearly defines the criteria to
346	define the study population (using the Pandas library), the preprocessing pipeline and software version
347	(through containerized tools), and the statistical model that was used to obtain the results. Our notebook
348	addresses some of the aforementioned challenges encountered during our study and can be re-run over
349	time to update the study as more data gets added to PPMI.
350	
351	We continue to investigate the replicability of MRI-derived PD biomarkers by replicating other clinical
352	studies. Arafe et al. as well as Wang et al. report the results of their work in this Special Collection.
353	
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355	
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