

# Event-related causality in Stereo-EEG discriminates syntactic processing of noun phrases and verb phrases

Andrea Cometa<sup>1</sup>, Piergiorgio D'Orio<sup>2,3</sup>, Martina Revay<sup>2,4</sup>, Franco Bottoni<sup>5</sup>, Claudia Repetto<sup>6</sup>, Giorgio Lo Russo<sup>2</sup>, Stefano F. Cappa<sup>7,8</sup>, Andrea Moro<sup>7</sup>, Silvestro Micera<sup>1,9,+</sup>, Fiorenzo Artoni<sup>1,9,10,+</sup>

1. The BioRobotics Institute and Department of Excellence in Robotics and AI, Scuola Superiore Sant'Anna, Viale Rinaldo Piaggio 34, Pontedera, 56025, Italy
2. 'Claudio Munari' Center for Epilepsy Surgery, ASST GOM Niguarda Hospital, Piazza dell'Ospedale Maggiore 3, Milan, 20162, Italy
3. Institute of Neuroscience, CNR, via Volturno 39E, Parma, 43125, Italy
4. Department of Biomedical and Clinical Sciences "L. Sacco", Università degli Studi di Milano, Via Giovanni Battista Grassi 74, Milan, 20157, Italy
5. Istituto Clinico Humanitas, IRCCS, Via Alessandro Manzoni 56, Rozzano, 20089, Italy
6. Department of Psychology, Università Cattolica del Sacro Cuore, Largo A. Gemelli 1, Milan, 20123, Italy
7. Neurocognition Epistemology and theoretical Syntax Research Center (NEtS), Scuola Universitaria Superiore IUSS, Piazza della Vittoria 15, 27100 Pavia, Italy
8. IRCCS Mondino Foundation National Institute of Neurology, Via Mondino 2, Pavia, 27100, Italy
9. Ecole Polytechnique Federale de Lausanne, Bertarelli Foundation Chair in Translational NeuroEngineering, Center for Neuroprosthetics and School of Engineering, Chemin des Mines 9, Geneva, GE CH 1202, Switzerland
10. Functional Brain Mapping Laboratory, Department of Basic Neurosciences, University of Geneva, Chemin des Mines 9, Geneva, GE CH 1202, Switzerland

+ These authors contributed equally to the work

\* E-mails: [fiorenzo.artoni@unige.ch](mailto:fiorenzo.artoni@unige.ch), [silvestro.micera@epfl.ch](mailto:silvestro.micera@epfl.ch)

## Abstract

Syntax involves complex neurobiological mechanisms, which are difficult to disentangle for multiple reasons. Using a protocol able to separate syntactic information from sound information we investigated the neural causal connections evoked by the processing of homophonous phrases, either verb phrases (VP) or noun phrases (NP). We used event-related causality (ERC) from stereo-electroencephalographic (SEEG) recordings in 10 epileptic patients in multiple cortical areas, including language areas and their homologous in the non-dominant hemisphere. We identified the different networks involved in the processing of these syntactic operations (faster in the dominant hemisphere) showing that VPs engage a wider cortical network. We also present a proof-of-concept for the decoding of the syntactic category of a perceived phrase based on causality measures. Our findings help unravel the neural correlates of syntactic elaboration and show how a decoding based on multiple cortical areas could contribute to the development of speech prostheses for speech impairment mitigation.

**Key Words:** SEEG, syntax, partial directed coherence, event-related causality, connectivity, speech, decoding

## 44 Introduction

45  
46 Traditionally, language is analyzed in relation to four main components: the acoustic level, that is the  
47 physical medium humans naturally exploit to convey information and its articulatory–phonatory  
48 counterpart; the lexicon, which is the repertoire of words expressing predicative contents and logical  
49 instructions; syntax, the set of principles to assemble larger units (phrases) from lexical items , in a  
50 recursive potentially infinite way; semantics, an interpretative component which captures the truth value  
51 conditions for each syntactic structure. However, since the acoustic and syntactic information are  
52 crucially intertwined (Ding et al., 2015), even during inner speech (Kayne, 2019; Magrassi et al., 2015),  
53 isolating syntax at the electrophysiological level appears to be an insurmountable empirical task. This is  
54 reflected in the difficulty of developing specific syntax-related tasks for experimental studies of language  
55 neurobiology and it is responsible for the relatively limited knowledge of syntax-related processing in the  
56 brain. Understanding the neural correlates of even the most basic syntactic operations, such as merging  
57 an article with a noun (N) yielding a Noun Phrase (NP) or a pronoun with a verb (V) yielding a Verb  
58 Phrase (VP) remains a crucial challenge for brain and language research (Grodzinsky & Friederici, 2006).

59  
60 In a recent study (Artoni et al., 2020), we designed and used a novel protocol aimed at isolating syntactic  
61 information from the acoustic associated information by exploiting pairs of sentences containing  
62 homophonous strings (same acoustic information but completely different syntactic content).  
63 Specifically, each pair of stimuli contained the same acoustic copy of two homophonous words, which  
64 could be interpreted either as a Noun Phrase (NP) or a Verb Phrase (VP) (**Figure 1A**). This approach  
65 was used to factor out any phonological and prosodical clue in a complete way, even at the subliminal  
66 level. We used this protocol while recording the related cortical activation using stereo-electroencephalo-  
67 graphy (SEEG), an invasive recording technique with unparalleled signal-to-noise ratio and recording  
68 band-width (He et al., 2019; Lachaux et al., 2003).

69  
70 Here, we exploited the same dataset to investigate the amplitude, the direction, and the specific  
71 frequencies of the interactions taking place between brain structures, that is the collection of causal links  
72 elicited by different functional situations known as effective connectivity (Penny et al., 2004). Given the  
73 utmost importance of timing, here we analyze the directed connectivity patterns elicited by a stimulus,  
74 i.e., the event-related causality (ERC). We investigated the dynamical evolution of the causal integration  
75 in response to a specific part of the time-varying stimuli (sentences) - the response window (RW) - either  
76 the NP or the VP. To reach this aim and to characterize and define the different networks involved in  
77 the processing of the syntactic operations yielding a Noun Phrase or a Verb Phrase we used a recently  
78 validated pipeline of ours for the evaluation of ERC in a set RW (Cometa et al., 2021).

79 We also present a proof-of-concept for the decoding of the syntactic category of a perceived sentence  
80 based on causality measures which could contribute to the future development of speech prostheses for  
81 speech impairment mitigation.

83  
84

## 85 Results

### 86 NPs and VPs elicit two unique networks

87 The neural networks elicited by the processing of NPs and VPs were investigated with SEEG. The data  
88 were recorded from 10 Italian-native speaker patients with no language disorders who underwent surgical  
89 operation for drug-resistant epilepsy. NPs and VPs were encoded in the same acoustic stimulus and could  
90 be differentiated only by their syntactic context (some Italian homophonous phrases, such as *la porta* /la  
91 'porta/ – that can be interpreted either as a noun phrase - “the door” - or a verb phrase - “[s/he] brings  
92 her”). After pre-processing, close recording contacts were arranged in groups called mini-regions of  
93 interest (mini-ROIs), each represented by a prototypical contact. The grouping resulted in a total of 396  
94 mini-ROIs in the left – or dominant – hemisphere (DH) and 577 mini-ROIs in the right – or non-  
95 dominant – hemisphere (NDH) (**Figure 1B**). To identify the networks involved in both NPs and VPs  
96 processing (i.e., the group of mini-ROIs bounded together by causal relations), we used Partial Directed  
97 Coherence (PDC) (Baccalá & Sameshima, 2001) and a recently developed pipeline to determine the  
98 significance of ERC elicited by an RW (Cometa et al., 2021).

99

100 We restricted the analysis to connections identified within the ultra-high gamma frequency band (150 to  
101 300 Hz) (Artoni et al., 2020). The pipeline discovered 13 significant connections for the NP case (2 in  
102 the DH and 11 in the NDH) and 20 connections for the VP condition (6 in the DH, 13 in the NDH,  
103 and 1 from the right temporal lobe to the left temporal lobe). We observed 4 connections active for both  
104 phrases in the NDH. Of these shared connections 3 were intra-temporal (**Figure 2A**). All the significant  
105 connections are shown in **Table S1**.

106

107 We compared the estimated connections with the recorded cortico-cortical evoked potentials (CCEPs)  
108 (Matsumoto & Kunieda, 2019), which are an indicator of the presence of a direct cortico-cortical or  
109 cortico-subcortico-cortical anatomical pathway (Matsumoto et al., 2004). Out of all the pairs of channels  
110 with a significant connection, only 11 exhibited a CCEP. The contacts involved in a significant  
111 connection and with a relevant CCEP were placed closer together than those not showing CCEPs (Mann-  
112 Whitney  $U_{22,11} = 53$ ,  $p < 0.005$ ) (**Figure 2B**).

113 Significant connections may be biased by clusters of closely placed contacts. Thus, to factor out a possible  
114 effect of this spatial sampling bias, we compared the distribution of the distances between pairs of  
115 contacts showing significant causal connections with the distribution of the distances between all  
116 channels (**Figure 2C**). We did not detect any difference between the two distributions (Mann-Whitney  
117  $U_{29,47987} = 590819$ ,  $p = 0.16$ ).

118 Finally, more significant connections in both NPs and VPs were found in subjects with electrodes placed  
119 in the NDH, in contrast to those with the DH explored (Mann-Whitney  $U_{4,5} = 18.5$ ,  $p < 0.05$ , **Figure**  
120 **2D**). This difference was still present even when normalizing the number of significant directed  
121 connections by the total amount of the possible connections for each subject (Mann-Whitney  $U_{4,5} = 18$ ,  
122  $p < 0.05$ ). Only one subject had both hemispheres explored and showed an inter-hemispheric connection  
123 (VP, from the right temporal lobe to the left one).

### 124 VPs engage a wider network than NPs

125 The recording contacts participating in the NP-related network or the VP-related network were not  
126 spread across the entire cortical surface but rather clustered in specific brain zones – i.e. the anatomical  
127 parcellation of cortical gyri and sulci according to the Destrieux atlas (Destrieux et al., 2010). In total, 64  
128 brain zones were probed in the DH and 88 in the NDH. Out of 152 cortical areas, 11 were involved in  
129 the processing of both homophonous phrases (2 in the DH and 9 in the NDH), 12 participated in the  
130 processing of the VPs alone (6 in the DH and 6 in the NDH) and 6 responded exclusively to NPs (1 in  
131 the DH and 5 in the NDH) (**Figure 2E**).

132 The connectivity estimated by the PDC is a directed causal information flow from one recording contact  
133 called source to another denoted sink. For NPs, all the sources were located bilaterally in the temporal  
134 lobes (2 in the DH and 11 in the NDH). For VPs, the temporal lobes contained 17 sources (5 in the DH  
135 and 12 in the NDH). The other 3 VPs sources were situated in the right occipital lobe, right frontal lobe,  
136 and left insula (**Figure 2F, left**). Most sinks, for both NPs and VPs, were in the two temporal lobes (DH:  
137 2 for NPs and 4 for VPs; NDH: 6 for NPs and 8 for VPs). Other sinks were in the right insula (1 for  
138 NPs, 2 for VPs), in the right frontal lobe (2 for NPs, 1 for VPs), right central lobe (1 for NPs), right  
139 cingulum (1 for NPs, 2 for VPs), left frontal lobe (2 for VPs), and left cingulum (1 for VPs) (**Figure 2F,**  
140 **right**). The lists of the cortical areas containing sources and sinks for a given connection are shown in  
141 **Table S2** and **Table S3**.

142 Overall, VPs elicited more sources or sinks than NPs, engaged a higher number of different cortical areas  
143 in both hemispheres, with almost no brain-zone being more active for NPs.

144 The results show that VPs extended the processing network beyond the temporal lobes.

145 Recording contacts that participated in VPs processing seemed to be located further than those involved  
146 in NPs processing (Mann-Whitney  $U_{13,20} = 93$ ,  $p = 0.08$ , **Figure 2G**), even if not reaching the statistical  
147 significance level  $\alpha = 0.05$ .

## 148 **Syntax processing is faster in the DH**

149 We then looked at the speed of response, or processing time, in the DH and NDH. The latencies of the  
150 peaks in the temporal evolutions of the time-varying significant causalities were thus compared among  
151 hemispheres. We considered only the highest peak, for each time series, occurring during the  
152 homophonous part of the stimuli (**Figure 3A**). These peaks arose earlier in the DH (Mann-Whitney  $U_{8,24}$   
153  $= 54.5$ ,  $p < 0.05$ ), for both NPs and VPs (**Figure 3B**).

154 The peak latencies in the directed connections evoked by the homophonous syntagms did not correlate  
155 linearly with the distances between the recording contacts involved in those connections (Pearson's  $\rho =$   
156  $0.07$ ,  $p = 0.71$ , **Figure 3C**). Moreover, distances between recording contacts implanted in the DH and  
157 NDH and participating in an active connection were not statistically different (Mann-Whitney  $U_{8,24} = 83$ ,  
158  $p = 0.29$ ). Therefore, the difference in peak latencies was likely not due to the channel distribution in the  
159 two hemispheres, but rather solely to the syntactic processing time.

## 160 **Connectivity decodes homophonous phrases**

161 The general neural connectivity estimated by the time-varying PDC was able to determine if the subject  
162 was waiting for the sentence (baseline), listening to the initial part of the sentence, to the homophonous  
163 phrase (RW), or its ending. We used a Long Short-Term Memory Network (LSTM) (Hochreiter &  
164 Schmidhuber, 1997) to classify the stimulus segments with single-trial accuracy equal to 83.75 % (**Figure**  
165 **4A**).

166 We finally extracted time-dependent features only on the identified significant connections. We used a  
167 Support Vector Machine (SVM) (Cortes & Vapnik, 1995) to predict the syntactic content of the  
168 homophonous phrase in the sentence. The accuracy was significantly above chance during the RW phase  
169 (**Figure 4B**).

170 Both models were evaluated using a Leave-One-Subject-Out (LOSO) cross-validation.

171

## Discussion

172

173

174

175

176

177

178

179

180

181

182

183

184

185

186

187

188

189

190

191

192

193

194

195

196

197

198

199

200

201

202

203

204

205

206

207

208

209

210

211

212

213

214

215

216

217

218

219

220

221

222

Language comprehension and production, in particularly syntax processing, are complex and highly integrated tasks continuously carried out by our brain, seemingly without effort. Analysing their neural correlates thus requires sophisticated tools. One of the most promising techniques to identify the different neural processes underlying the syntactic operations leading to the processing of, for example, Noun Phrases or Verb Phrases is offered by directed connectivity evaluation related to the complexity of the large-scale networks. To our knowledge, this is the first time a difference in the connectivity elicited by NPs or VPs processing was identified.

Traditionally, the problem of understanding the neural correlates of syntax is approached by studying the effects of brain lesions or with syntax-related experimental tasks administered during neurophysiological and neuroimaging acquisitions contaminated by confounding factors such as phonology or semantics (Friederici et al., 2017; Vigliocco et al., 2011). Our approach is to leverage NP/VP homophonous phrases. The advantage of our solution is that we can factor out confounding factors by analyzing these homophonous phrases.

The shift from the analysis of isolated lexical elements such as bare Vs and Ns vs. syntactic units, namely VPs and NPs, is obviously a necessary step toward the goal of capturing syntactic information. Lexical elements in isolation contain linguistic information but these pieces of information are artificially expressed in single words whereas natural linguistic expressions always involve syntactic computation. In fact, the stimuli involved syntax in two directions: first, each homophonous phrase was syntactically connected with other words expressing a full-fledged sentence; second, each homophonous phrase contained very different syntactic structures. More specifically: in NPs the surfacing order of the two words composing them, namely an article and a noun, was the same as the underlying structure composing it; in VPs, the situation is completely different and definitely more complex. In all VPs considered here a transformation called *cliticization* takes place. The order of the elements constituting it (a pronoun, playing the role of the object, and a verb) is reversed with respect to the canonical order in an SVO language like Italian; the canonical position of the object is to the right of the verb (Moro, 2016). All in all, the shift from V/N to VP/NP constitutes a necessary and relevant step towards the final goal of cracking the underlying code of human syntax.

The information carried by all the directed connections was able to discriminate between parts of the sentence. The syntactic category of the stimulus was discriminable only by looking at the significant connections, showing the importance of restricting the topology analysis on the few significant connections.

In recent years, there have been important technological and methodological advancements in perceived and imagined speech decoding (Martin et al., 2018; Panachakel & Ramakrishnan, 2021). Recent works focus on the classification of vowels (M. S. Mahmud et al., 2020; N. T. Duc & B. Lee, 2020), syllables (Archila-Meléndez et al., 2018; Brandmeyer et al., 2013; Correia et al., 2015), words (Ossmy et al., 2015; Proix et al., 2022; Vorontsova et al., 2021) and complete sentences (Chakrabarti et al., 2015; Zhang et al., 2012), distinguishing stimuli mainly at the semantic level. The most advanced online decoding techniques rely heavily on the articulatory representation of syllables and words in the motor and supplementary motor cortices (Anumanchipalli et al., 2019). However, this approach can only be applied to patients with intact motor commands, which represent a minority of the patients with speech impairment (Guenther et al., 2009; Wilson et al., 2020). Thus, other decoding strategies that rely on the brain regions that encode speech are needed (Proix et al., 2022).

Here, we decoded the acoustic stimuli exploiting 29 different speech-encoding cortical areas spanning the entire brain. Only recently such strategy has been used in the decoding of groups of syllables and words (Proix et al., 2022).

However, our approach relies on the time evolution of the connectivity values between recording contacts. This solution has the advantage of assuring high inter-subject generalizability as shown by the

223 LOSO validation results: the connectivity features are independent of the location of the implanted leads,  
224 which may differ from subject to subject. Also, our method is well suited to be implemented in an online  
225 decoder. Moreover, the signals that drive the decoding are directly entangled to the syntactic  
226 representation of the stimuli rather than their phonological - and articular - components.  
227 We believe that a decoding strategy that relies on multiple language-encoding cortical areas will drastically  
228 improve the performance of speech prostheses and may be the key missing piece for the development  
229 of this technology.

230  
231 We showed that VPs processing, compared to NPs processing, elicited a significantly higher number of  
232 directed connections, linked together more brain structures both in the DH and in the NDH, and  
233 involved the activation of a wider cortical network. VPs processing was distributed beyond temporal  
234 lobes, pushing the information from sources located in the right frontal lobe and left insula, to sinks in  
235 both frontal lobes, anterior cingulate regions, and right insula. This suggests a greater network small-  
236 worldness for NPs, with a preference for short-range connections over long range ones.  
237 Most of the literature converges on a more extended cerebral involvement in verb processing than for  
238 nouns (Lukic et al., 2021; Vigliocco et al., 2011). However, again, most evidence came from tasks  
239 requiring the processing of N/V as words in isolation: this is the first time an approach based on  
240 homophonous phrases, hence syntax, is used.

241  
242 Temporal lobes (both in the DH and in the NDH) seem to be the main hub in which the syntactic  
243 operations leading to NPs or VPs are analyzed and processed. For NPs all the information flow started  
244 from these areas, while for VPs 3 out of 20 sources were placed outside the temporal lobes (with the one  
245 in the right occipital cortex very close to temporal areas). Also, sinks were mostly located in the temporal  
246 lobes. The important role of the temporal lobes, in particular of left posterior regions, in syntactic  
247 processing is supported by lesion and imaging evidence (Friederici et al., 2017; Matchin & Hickok, 2020).  
248 The comparison of the estimated directed connections with the CCEPs arising between recording  
249 contacts showed a partial discrepancy. While the structural connectivity underlying CCEPs is well known  
250 (e.g., the Human Connectome Project) (Van Essen et al., 2012), the functional and effective connectivity  
251 are patterns of highly heterogeneous causal relationships that may reflect processes occurring during  
252 many different temporal time scales (Honey et al., 2009; Keller et al., 2014; Matsui et al., 2011; Shmuel &  
253 Leopold, 2008; Vincent et al., 2007). The event-related causality identified here, is thus the expression of  
254 more complex neural processes, for which there are no unique a priori hypotheses.

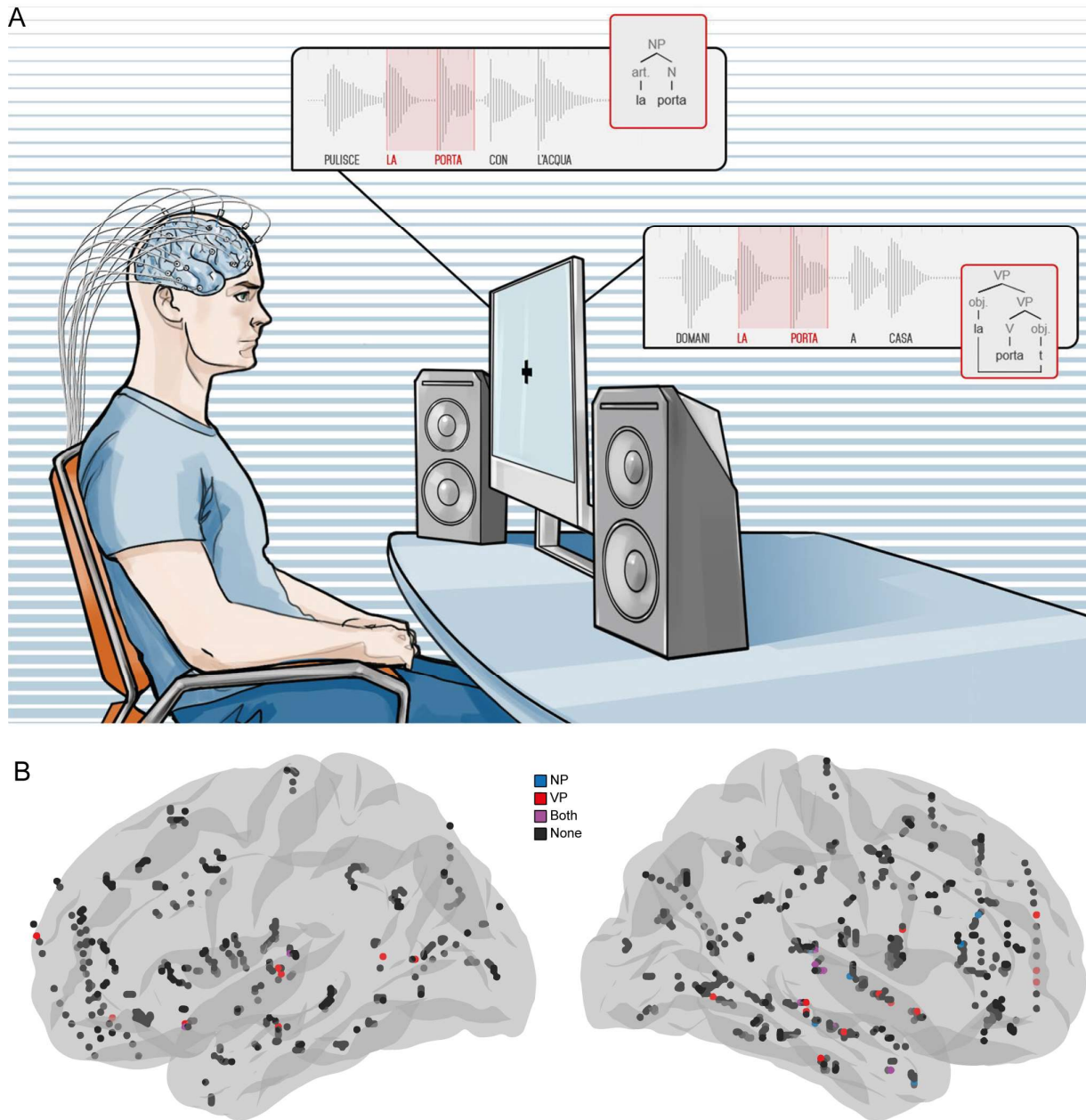
255 Interestingly, recording contacts involved in a significant connection and showing at the same time  
256 CCEPs were implanted closed together than the pairs of channels without relevant CCEPs. Indeed,  
257 CCEPs may terminate their propagation early (Keller et al., 2014; Logothetis et al., 2010), which is in  
258 agreement with the description of CCEPs as supported by short-range local relations arising from direct  
259 hardwired connections via cortico-cortical or cortico-subcortico-cortical pathways (Matsumoto et al.,  
260 2004). This suggests that syntax-related processing relies mostly on long-range connections between  
261 cortical areas, expressing network-level neural synchronization supported by long-range, indirect  
262 structural pathways, typical of high-level cognitive processing (Salmelin & Kujala, 2006).

263  
264 Earlier peaks in the connectivity time-series in the DH revealed that the syntax processing elicited by our  
265 stimuli started first in the temporal lobes of the left hemispheres and then spread to the right cortices.  
266 The directed links from DH to NDH that are necessary to transfer the information from one hemisphere  
267 to the other were not deemed significant because they were probably active during all sentence  
268 processing, and so they were masked during the search for the causal connections with the highest  
269 amplitude increase during the homophonous part of the stimulus. Also, only 1 subject out of 10 was  
270 explored in both hemispheres.

271  
272 Focal lesion, behavioral, fMRI and electrophysiological studies provide converging evidence for a  
273 dominant role of one hemisphere (the left in right-handers and in the majority of left-handers) for most  
274 aspects of language processing (Tzourio-Mazoyer et al., 2017). Here we detected more significant

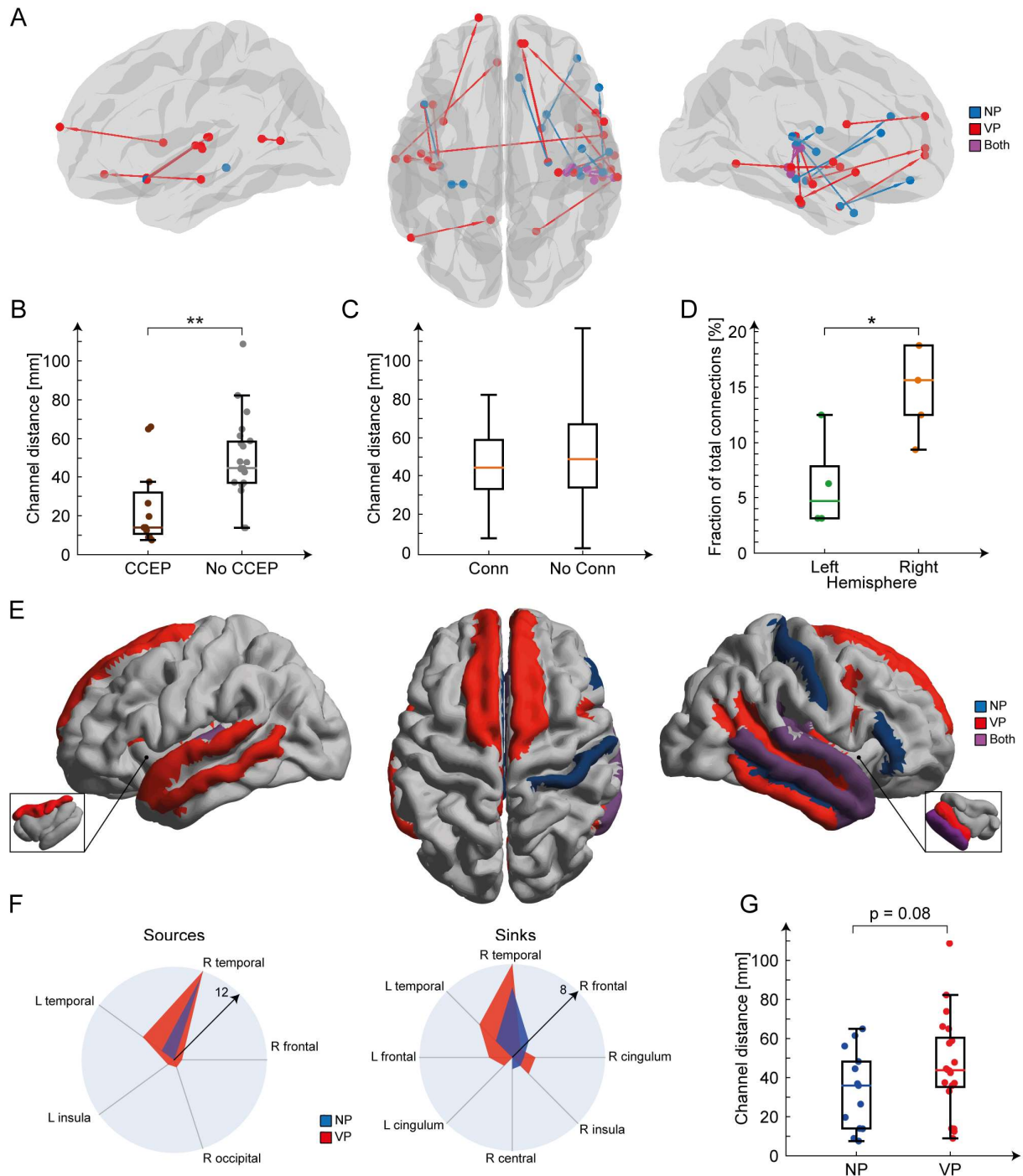
275 connections arising in the NDH than in the DH. Previous studies claim that speech perception is the  
276 only aspect of bi-hemispheric language processing, even if the successive linguistic elaboration is carried  
277 mainly by the DH (Hickok & Poeppel, 2000; Poeppel et al., 2008). We hypothesize that the lesser number  
278 of significant connections in the DH may be due to the spread of the syntactic-related information to the  
279 NDH after it is first processed in the DH. However, future work is needed to better characterize the role  
280 of the NDH in syntax processing.

281  
282 In conclusion, these results represent an important step forward in human language comprehension,  
283 contributing to the full characterization of syntactic processing. We showed a specific brain activity  
284 encoding a syntactic distinction, which is faster in the DH. Since, even from a purely formal point of  
285 view, syntactic processing cannot be compared with other computational systems, language-related or  
286 not (Chomsky, 2014; Moro, 2014b, 2014a), it is reasonable to conclude that the network highlighted here  
287 is not only specific but arguably it is uniquely dedicated to syntax. We prove that it is possible to decode  
288 the syntactic structure of a phrase by looking at the connections elicited by speech processing between  
289 multiple cortical areas. This could contribute to the future development of speech prostheses for speech  
290 impairment mitigation (Anumanchipalli et al., 2019).



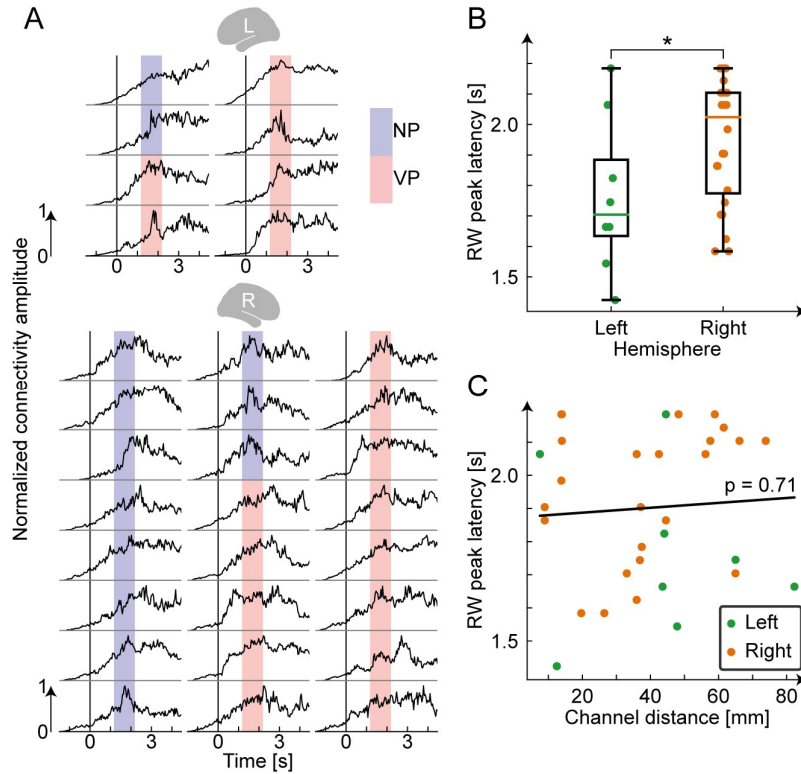
**Figure 1. Experimental set-up. (A)** Example of a set of homophonous sequences (i.e., strings of words with the same sound but different syntactic structure) used in the experiment. For example, in PULISCE LA PORTA CON L'ACQUA (s/he cleans the door with water), the phonemic sequence [la 'pɔrta] (written here as: la porta) is a Noun Phrase (NP), while in DOMANI LA PORTA A CASA (tomorrow s/he brings her home), the same sequence is a Verb Phrase (VP). From (Artoni et al., 2020). **(B)** Mini-region-of-interests (merged across all subjects) in the dominant (left) and non-dominant (right) hemispheres. Contacts involved in the NP-related network are highlighted in blue, those involved in the VP processing network are highlighted in red, and those participating in both networks are coloured in purple.



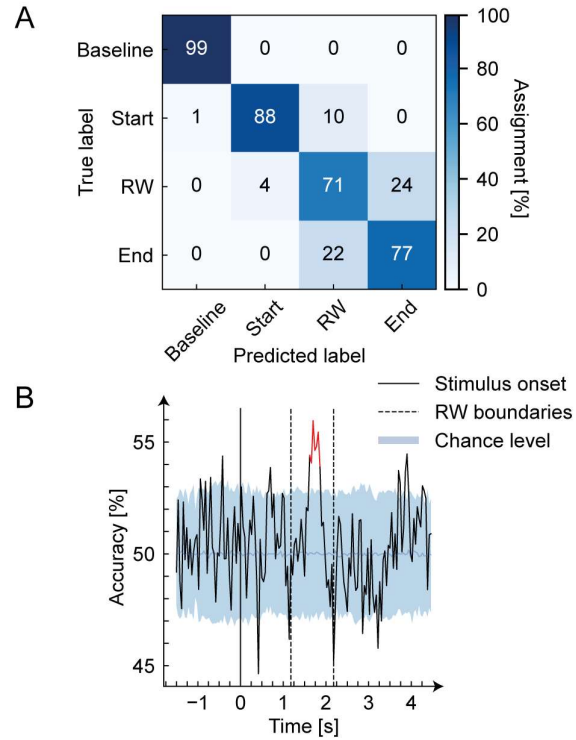


**Figure 2. VPs engage a wider and more complex network.** **(A)** Lateral and dorsal views of the identified directed connections. Nodes and edges are highlighted in blue for the Noun Phrase (NP) processing network, in red for the Verb Phrase related network, or purple if shared by both processing systems. **(B)** Box plots of the distances between the contacts involved in a significant connection and with a relevant cortico-cortical evoked potential (CCEP) and between those not showing CCEPs. **(C)** Box plots of the distances between pairs of explored contacts, whether a significant connection exists between them (Conn) or not (No Conn). **(D)** Box plots of the number of connections in subjects with electrodes in the non-dominant (right) hemisphere and in those in which only the dominant (left) was probed. The vertical axis is normalized by the total number of significant directed connections identified across all subjects. **(E)** Lateral and dorsal views of the active brain zones during NPs (blue) processing, VPs (red) processing, or both (purple). An active brain zone is a cortical area containing one or more recording contacts that act as sources or sinks for a certain directed connection. The zoom-in pictures show the left and right insula. **(F)** Radar plots of the number of sources (left) and sinks (right) in each cerebral lobe, for the two conditions NP (blue) and VP (red). **(G)** Box plots of the distances between contacts involved in a significant connection during NP and VP processing.

2



**Figure 3. Syntax is faster in the dominant hemisphere. (A)** Time series of the identified directed connections, in the dominant (L, top) and non-dominant (R, bottom) hemispheres. Each time series is normalized between 0 and 1. The 0 in the time axis is the start of the sentence, the coloured area represents the homophonous part (or response window - RW). Directed connections that are significant when listening Noun Phrases (NP) have this area coloured in blue, while those significant for Verb Phrases (VP) have this area highlighted in red. **(B)** Box plots of the latencies of the connectivity peaks during the RW in the dominant hemisphere (left) and in the non-dominant one (right). **(C)** Scatter plot of latencies of the peaks during the RW as function of the distances between channel pairs.



**Figure 4. Connectivity decodes sentence structure. (A)** Confusion matrix for the prediction of the stimulus phase. **(B)** Time-varying accuracy of the classification of noun phrases vs verb phrases. The blue line represents the median of the chance level, the boundaries of the light blue band are the 5th and 95th percentiles of the chance level distribution. The red part of the plot is the accuracy significantly above the chance level ( $p < 0.005$ ).

295 **Acknowledgments**

296 This work was financed by the Italian Ministry of Education, University and Research (MIUR) through  
297 PRIN-2017 'INSPECT' (Project 2017JPMW4F) and by the Bertarelli Foundation.  
298

299 **Author contributions**

300 Conceptualization: S.F.C., A.M., and S.M.; Methodology: F.B., C.R., G.L.R., S.F.C., A.M., and S.M.;  
301 Software: A.C. and F.A.; Validation: A.C., F.A., P.d.O., and M.R.; Formal Analysis: A.C.; Investigation:  
302 P.d.O. and M.R.; Resources: G.L.R. and S.M.; Data Curation: A.C., F.A., P.d.O., and M.R.; Writing,  
303 Review and Editing: A.C., F.A., S.F.C., A.M., and S.M.; Visualization: A.C.; Supervision: G.L.R., S.F.C.,  
304 A.M., and S.M.; Project Administration: S.F.C., A.M., and S.M.; Funding Acquisition: S.M.

## 305 STAR Methods

### 306 Resource availability

#### 307 *Lead Contact*

308 Further information and requests for resources should be directed to and will be fulfilled by the lead  
309 contact, Fiorenzo Artoni (fiorenzo.artoni@unige.ch).

310

#### 311 *Materials availability*

312 This study did not generate new unique materials.

313

#### 314 *Data and code availability*

315 All the data used for the study are available from the authors upon reasonable request.

316 This study adapts built-in MATLAB functions, the EEGLAB toolbox, the BrainNet Viewer toolbox,  
317 and several publicly available *Python* packages to handle, analyze and plot data. Custom code is available  
318 from the authors upon request.

319 Any additional information required to re-analyze the data reported in this paper is available from the  
320 lead contact upon request.

### 321 Experimental model and subject detail

#### 322 *Human subjects*

323 In total, 23 patients were recruited. All of them underwent surgical implantations of intracerebral  
324 electrodes for refractory epilepsy (Cossu et al., 2015) in the “Claudio Munari” Epilepsy Surgery Center  
325 of Milan, Italy (Cossu et al., 2005; Munari et al., 1994). The strategy of implantation was defined purely  
326 based on clinical needs, to locate the epileptogenic zone.

327 All patients completed all experimental sessions. During the 24h before the experimental recording, no  
328 seizure occurred, no alterations in the sleep/wake cycle were observed, and no additional  
329 pharmacological treatments were applied. No language or neuropsychological deficits were found in any  
330 patients. Also, no anatomical alterations were made evident by magnetic resonance. High-frequency  
331 stimulation (50 Hz, 3 mA, 5 sec) through SEEG electrodes was used to assess language dominance in all  
332 subjects. Two patients also underwent an fMRI study during a language task before the implantation of  
333 the electrodes.

334 Thirteen patients were excluded from the analysis. Eight of them exhibited pathological SEEG contacts.  
335 The others five patients showed no explored recording contacts with a task-related significant activation  
336 in our previous study (Artoni et al., 2020). Full demographic data are shown in **Table S4**.

337 A total of 2186 recording contacts (median 210, range 168-272) were implanted, divided into 164  
338 electrodes (median 16.5, range 13-19). The number of contacts in the grey matter was 1439 (65.8%); 586  
339 recording contacts in the language dominant hemisphere (DH). The DH was explored in 5 subjects  
340 (median electrodes 16, range 3-18; median contacts 210, range 25-225). The non-dominant hemisphere  
341 (NDH) was explored in 6 subjects (median electrodes 15, range 14-19; median contacts 208, range 182-  
342 272). SEEG exploration involved both hemispheres with a preference for the non-dominant side in 1  
343 patient.

344 Overall, 68 electrodes were implanted in the temporal lobe (26 in DH, 42 in NDH), 43 in the frontal  
345 lobe (22 in DH, 21 in NDH), 22 in the central lobe (9 in DH, 13 in NDH), and 30 in the parieto-occipital  
346 region (9 in DH and 21 in NDH).

347 The present study received the approval of the Ethics Committee of ASST Grande Ospedale  
348 Metropolitanu Niguarda (ID 939-2.12.2013) and informed consent was obtained from all participants.

## 349 **Methods details**

### 350 ***Stimuli***

351 The set of stimuli is based on three characteristics of Italian. First, some definite articles are pronounced  
352 exactly like some object clitic pronouns (such as [la] written as *la*; it can be both “the - fem.sing.” or “her  
353 - fem.sing.”). Second, the syntax of articles and clitic pronouns is very different: articles precede nouns,  
354 complements follow verbs, but object clitics are placed before the verb. Third, the Italian lexicon contains  
355 several homophonous pairs of nouns and verbs, such as [ˈpɔrta] (written *porta*), which can either mean  
356 “door” or “brings”. A set of pairs of words such as [la ˈpɔrta] (written as *la porta*) can thus be interpreted  
357 either as a noun phrase (“the door”) or a verb phrase (“brings her”) depending on the syntactic context  
358 (homophonous phrases). For example, in PULISCE LA PORTA CON L’ACQUA (s/he cleans the door  
359 with water), *la porta* is a Noun Phrase (NP), while in DOMANI LA PORTA A CASA (tomorrow s/he  
360 brings her home), *la porta* is a Verb Phrase (VP).

361 To be sure to eliminate phonological and prosodical factors, the pronunciation of one homophonous  
362 phrase was copied in the syntactic counterpart. No other semantic or lexical distinction differentiated the  
363 two types of phrases.

364 The acoustic stimuli were recorded using a Sennheiser Microphone MH40P48, connected via a Firewire  
365 400 to an Apple OSX 10.5.8 with a Motu Ultralight Mk3 sound card. The stimuli were edited and  
366 mastered using Audiodesk 3.02 and Peak Pro7, respectively. Files were generated in 16 bits, with a  
367 sampling frequency equal to 44.1 kHz; intensity was normalized to 0 Db and rendered in .wav format.  
368 All sentences were read by the same person, an Italian native speaker, male, 53 years old.  
369

### 370 ***Surgical procedure and recording equipment***

371 SEEG electrodes have a diameter of 0.8 mm. They contain 5 to 18 recording contacts, which are 2 mm  
372 long and spaced by 1.5 mm. The strategy of implantation was planned on 3D multimodal imaging and  
373 the electrodes were stereotactically implanted with robotic assistance. The position of every recording  
374 contact was assessed by registering a post-implantation Cone-Beam-CT (O-arm scanner, Medtronic,  
375 Minneapolis, Minnesota) to pre-implantation T1 weighted MR images.

376 SEEG sampling rate during the experiment was set to 1 kHz (patients 1-12) or 2 kHz (patients 13-23).  
377 Recordings were carried out using a 192-channels EEG-1200 (Neurofax, Nihon Kohden). All recording  
378 contacts were re-referenced to two leads in the white matter, in which electrical stimulations did not  
379 produce any manifestation.  
380

### 381 ***Recording protocol***

382 Each subject rested in a comfortable armchair. Stimuli were delivered using the software Presentation  
383 (Neurobehavioral Systems). Phrases were delivered via audio amplifiers at the minimum volume for  
384 words to be perceived with ease, according to the subject. During stimuli delivery, subjects gazed at a 27  
385 inches cross on a screen. A synchronization TTL trigger spike was sent to the SEEG trigger port at the  
386 beginning of the sentence. Jitter and delays were lower than 1 ms. The experiment lasted around 30  
387 minutes. At the end of each task, subjects were always able to correctly answer short questions about the  
388 stimuli. A camera was used to control for eye movement, silence, and any unexpected behavior from the  
389 patients.  
390

### 391 ***Data pre-processing***

392 An anti-aliasing band-pass filter (0.015-500 Hz) was applied at the hardware level. Recordings acquired  
393 at 2 kHz were down-sampled to 1 kHz. Artifacts and pathological interictal activity were controlled and  
394 removed by clinicians and scientists by visual inspection. Recordings were annotated with the events  
395 triggered by the beginning of each word in all stimulus sentences. Epochs were extracted from -1.5 s to  
396 4.5 s time-locked to the beginning of each stimulus. The length of the epochs always ensured the inclusion  
397 of the complete stimulus presentation. Epochs with notable artifacts were rejected. Contacts in white  
398 matter were excluded from the subsequent analysis.

399

#### 400 ***Cortico-cortical evoked potentials***

401 During the presurgical evaluation, an effective connectivity of the explored brain areas was assessed for  
402 each subject by evaluating the Cortico-Cortical Evoked Potentials (CCEP) elicited by Single-Pulse  
403 Electrical Stimulation (SPES) (Matsumoto et al., 2017; Russo et al., 2021; Trebault et al., 2018).

404 In the condition of eyes open resting wakefulness, SPES was delivered through each pair of adjacent  
405 contacts, with at 5 mA current intensity, a single pulse of 0.5 ms (biphasic rectangular stimuli of  
406 alternating polarity), at 1 Hz frequency, for 15 s.

407 The presence of CCEPs response following a SPES was visually verified by trained neurophysiologists.

408

#### 409 ***Stimulus-evoked causality estimation***

410 To estimate the stimulus-evoked directed connections, recording contacts were first divided into mini-  
411 regions of interest (mini-ROIs). Then, the Partial Directed Coherence (PDC), a measure deriving from  
412 the Granger causality framework (Baccalá & Sameshima, 2001; Geweke, 1982; Granger, 1969) was  
413 computed. Finally, a non-parametric statistical test was used to evaluate the significant connections  
414 elicited in the response window (RW), i.e., the part of interest of the stimulus (NP or VP). This stimulus-  
415 evoked causality estimation pipeline, designed for SEEG data, is proposed in (Cometa et al., 2021).

416

#### 417 Mini ROI extraction

418 Recording contacts showing high correlation coefficients between their time series were combined into  
419 mini-ROIs. Specifically, mini-ROIs are groups of leads having an averaged across trials coefficient of  
420 determination  $R^2 > 0.8$ . The prototypical channel of a mini-ROI was selected as the one showing the  
421 highest linear correlation with the mini-ROI mean time series. Mini-ROIs grouping was performed  
422 independently for each subject. Most mini-ROIs were populated by just one channel, with the most  
423 numerous ones not being populated by more than 3 recording contacts. All leads contained in a single  
424 mini-ROI were spatially very close and always belonged to the same electrode.

425

#### 426 Causality estimation

427 Within the Granger causality framework, a time series  $x_j(t)$  causes another time series  $x_i(t)$  if knowledge  
428 of past samples of  $x_j(t)$  reduces the prediction error for the current sample of  $x_i(t)$ . The relation  
429 between  $x_j(t)$  and  $x_i(t)$  can be estimated by fitting a time-varying multivariate autoregressive (MVAR)  
430 model on  $\mathbf{X}(t)$ :

$$\mathbf{X}(t) = [x_1(t), x_2(t), \dots, x_D(t)]^T \quad (1)$$

431 where  $D$  is the total number of channels.

432 The MVAR model assumes a linear relationship between the channels in  $\mathbf{X}(t)$  of the form:

$$\mathbf{X}(t) = - \sum_{k=1}^p A_k(t) \mathbf{X}(t-k) + \mathbf{e}(t) \quad (2)$$

433 Where  $A_k(t)$  is the time-varying  $D \times D$  MVAR coefficients matrix,  $\mathbf{e}(t)$  is a white noise process with  
434 covariance matrix  $\mathbf{W}$  and  $p$  is the model order. The  $A_k(t)$  matrices were derived by using a general linear  
435 Kalman Filter (GLKF) (Milde et al., 2010). To estimate the model order  $p$ , the Bayesian information  
436 criterion (BIC) was used (Schwarz, 1978), resulting in  $p = 4$  for all subjects.

437 After estimating, trial by trial, the  $A_k(t)$  matrices, the single-trial time-varying  $PDC(f, t)$  (Astolfi et al.,  
438 2008) was computed.

439 To lower the computational complexity of the pipeline, PDC time samples were down-sampled by a  
440 factor of 40 (from 6000 samples to 150). Frequencies were averaged into overlapping frequency bins  
441 (width = 50 Hz, overlap = 25 Hz, range = 0 – 300 Hz).

442 Subsequent analysis was done only in the ultra-high gamma frequency range (150 – 300 Hz), i.e., on  
443 frequency bins from [125-175 Hz] to [250-300 Hz].

444

#### 445 Significance during the homophonous phrase

446 All the next steps of the algorithm were independently applied for each syntactic structure (NPs or VPs),  
447 each subject, and each frequency band  $f$ . Linear interpolation time-warping was used to align the RW  
448 across all trials (Artoni et al., 2017; Do et al., 2021; Gwin et al., 2011; Nordin et al., 2019). Baseline  
449 correction was then carried out by dividing  $PDC_{ij}(f, t)$ , trial by trial and for each  $i, j$  ( $i \neq j$ ) couple  
450 independently, by its mean baseline value. The  $\overline{PDC}_{ij}(f, t)$  matrices were obtained by averaging  
451  $PDC_{ij}(f, t)$  over trials. The mean values of the  $\overline{PDC}_{ij}(f, t)$  during the RW were calculated for each pair  
452  $i, j$  ( $i \neq j$ ) of channels. These mean values were compared against a null distribution: to generate the  
453 null (permutation) distribution and to control for false discovery rate (Maris & Oostenveld, 2007; Nichols  
454 & Holmes, 2002) the time samples of the  $\overline{PDC}_{ij}(f, t)$  were shuffled 1000 times and the mean values  
455 during the RW were re-computed for each permutation. The maximum mean value across all channel  
456 couples was retained for each permutation.

457 A  $p$ -value for each recording contact pair was calculated by comparing the original mean connectivity  
458 value in the RW with the permutation distribution. The  $p$ -value was the number of instances in the null  
459 distribution that were greater than the mean RW causality. Significance was then assigned to connections  
460 between pairs of leads whose  $p$ -value was below a certain threshold. The threshold was set to 0.33, being  
461 the lowest one that allowed the arising of at least one significant connection for either NPs or VPs in  
462 every subject, in at least one of the considered frequency bins.

463

#### 464 ***Latency analysis***

465 To detect the peaks in connectivity during the RW of the stimuli, the average connectivity time series  
466 were first smoothed. A Savgol filter was used (Guiñón et al., 2007). The polynomial order was set to 2,  
467 with 9-samples long windows. The window size was chosen as the knee of the curve formed by the sum  
468 of absolute differences between the smoothed time series and the raw ones for different window lengths.  
469 The latencies were defined as the time instant at which the maximum of each smoothed time series  
470 occurred, within the homophonous phrase interval.

471

#### 472 ***Cortical surface plotting***

473 Mini-ROIs (**Figure 1B**), active directed connections (**Figure 2A**), and active cortical areas (**Figure 4A**)  
474 were graphically represented using the *BrainNet Viewer* toolbox for Matlab (Xia et al., 2013). Plotting was  
475 done using MNI coordinates on a FreeSurfer *fsaverage* template (Fischl, 2012; Wu et al., 2018).

476

#### 477 ***Decoding***

##### 478 Response window prediction

479 The prediction of the phase of the stimulus was carried out on a trial-by-trial basis. All the connections  
480 were used. The time-varying connectivity amplitudes were divided into overlapping bins of size 20  
481 samples and step 1 sample. These were fed to a Long Short-Term Memory network (LSTM) (Hochreiter  
482 & Schmidhuber, 1997) together with the labels corresponding to the stimulus phase (baseline, sentence  
483 start, RW, sentence ending) of the last sample of the overlapping windows.

484 The training was carried out using a Leave-One-Subject-Out (LOSO) cross-validation procedure. For  
485 each fold of the LOSO cross-validation, 2 trials of the training set were removed and used as the  
486 validation set. The decoder hyperparameters were optimized according to the performance on the  
487 validation set.

488 A weighted version of the categorical cross-entropy (Martín Abadi et al., 2015; Y. Ho & S. Wookey, 2020)  
489 was used as the loss function to minimize during the training of the LSTM, with the weights for each  
490 class inversely proportional to the length of the stimulus phase.

491 The accuracy was obtained by averaging the accuracies across all folds of the LOSO cross-validation.

492 Code implementation was based on the *TensorFlow* package for python (Martín Abadi et al., 2015).



### 493 Syntactic content decoding

494 The prediction of the content of the homophonous phrases (NP vs VP) was carried out on a trial-by-  
495 trial basis. Only the significant connections were selected, regardless of whether the connections were  
496 significant during NPs or VPs processing. For each time point, a number of values equal to the number  
497 of significant connections were thus retained, corresponding to the amplitudes of the significant  
498 connections during that instant. A total of 7 features were then calculated for each time point: the  
499 statistical moments up to order 4, the median, the maximum, and the range (the difference between the  
500 maximum and the minimum).

501 A Support Vector Machine (Cortes & Vapnik, 1995) with a radial basis function kernel was trained for  
502 each time point. The training was carried out using a nested cross-validation procedure: (i) LOSO cross-  
503 validation was used to split the dataset into training and test set, and (ii) for each fold of the LOSO cross-  
504 validation, 10 fold cross-validation was used to furtherly divide the training set into training and validation  
505 set.

506 The inner validation loop was used to optimize the decoder hyperparameters and to perform feature  
507 selection through the minimum redundancy maximum relevance (Radovic et al., 2017) algorithm.

508 The time-varying accuracy was obtained by averaging the accuracies across all folds of the LOSO cross-  
509 validation procedure.

510 For each time point, the predicted labels were compared 1000 times with 1000 shuffled versions of the  
511 test set labels (NP or VP) to calculate the chance level. The procedure was repeated for each fold of the  
512 LOSO cross-validation, resulting in a null distribution of 1000 x (number of fold) accuracy values. An  
513 exact p-value was obtained by comparing the original accuracy with the null distribution.

514 The time-varying p-values were corrected for the multiple comparisons using a cluster-size-based  
515 statistical non-parametric mapping approach (Nichols & Holmes, 2002) and deemed significant if lower  
516 than  $\alpha = 0.05$ .

517 Code implementation was based on the *scikit-learn* package for python (Pedregosa et al., 2011).

518

### 519 **Quantification and statistical analysis**

520 The non-normality of the data undergoing statistical testing was assessed using Shapiro-Wilk tests  
521 (Shapiro & Wilk, 1965). Sizes  $n1$  and  $n2$  of the independent samples undergoing Mann-Whitney tests  
522 (Neuhäuser, 2011) and the associated  $U$  statistics are reported in the Results Section as  $U_{n1,n2} = U$ .  
523 Statistical significance level  $\alpha$  was 0.05. The inter-hemispheric significant connection that arose in one  
524 subject was not considered in the tests comparing connections in the DH versus connections in the  
525 NDH. Tests were computed using the *scipy* package for *Python* (Virtanen et al., 2020).

526

527 **KEY RESOURCES TABLE**

REAGENT or RESOURCE	SOURCE	IDENTIFIER
Software and Algorithms		
MATLAB	MathWorks	<a href="https://www.mathworks.com/">https://www.mathworks.com/</a>
EEGLAB toolbox for MATLAB	Swartz Center for Computational Neuroscience	<a href="http://EEGLAB.ucsd.edu">EEGLAB (ucsd.edu)</a>
Python	Python	<a href="http://Welcome.to.Python.org">Welcome to Python.org</a>
Scipy ecosystem for Python	Scipy	<a href="http://SciPy.org">SciPy.org</a>
scikit-learn	Scikit-Learn	<a href="http://scikit-learn.org">scikit-learn.org</a>
Pytorch	Google AI	<a href="https://doi.org/10.5281/zenodo.4724125">10.5281/zenodo.4724125</a>
BrainNet Viewer toolbox for MATLAB	Xia et al., 2013	<a href="http://NTRC:BrainNet.Viewer:Tool/Resource.Info">NTRC: BrainNet Viewer: Tool/Resource Info</a>
Presentation	Neurobehavioral Systems	<a href="http://Neurobehavioral.Systems(neurobs.com)">Neurobehavioral Systems (neurobs.com)</a>

528  
529  
530

## 531 **References**

532

533 Anumanchipalli, G. K., Chartier, J., & Chang, E. F. (2019). Speech synthesis from neural decoding of  
534 spoken sentences. *Nature*. <https://doi.org/10.1038/s41586-019-1119-1>

535 Archila-Meléndez, M. E., Valente, G., Correia, J. M., Rouhl, R. P. W., van Kranen-Mastenbroek, V. H.,  
536 & Jansma, B. M. (2018). Sensorimotor Representation of Speech Perception. Cross-Decoding

537 of Place of Articulation Features during Selective Attention to Syllables in 7T fMRI. *Eneuro*,  
538 5(2), ENEURO.0252-17.2018. <https://doi.org/10.1523/ENEURO.0252-17.2018>

539 Artoni, F., d’Orio, P., Catricalà, E., Conca, F., Bottoni, F., Pelliccia, V., Sartori, I., Russo, G. L., Cappa,  
540 S. F., Micera, S., & Moro, A. (2020). High gamma response tracks different syntactic structures

541 in homophonous phrases. *Scientific Reports*, 10(1), 7537. [https://doi.org/10.1038/s41598-020-](https://doi.org/10.1038/s41598-020-64375-9)  
542 64375-9

543 Artoni, F., Fanciullacci, C., Bertolucci, F., Panarese, A., Makeig, S., Micera, S., & Chisari, C. (2017).

544 Unidirectional brain to muscle connectivity reveals motor cortex control of leg muscles during  
545 stereotyped walking. *NeuroImage*, 159, 403–416.

546 <https://doi.org/10.1016/j.neuroimage.2017.07.013>

547 Astolfi, L., Cincotti, F., Mattia, D., De Vico Fallani, F., Tocci, A., Colosimo, A., Salinari, S., Marciani,  
548 M. G., Hesse, W., Witte, H., Ursino, M., Zavaglia, M., & Babiloni, F. (2008). Tracking the time-

549 varying cortical connectivity patterns by adaptive multivariate estimators. *IEEE Transactions on*  
550 *Biomedical Engineering*. <https://doi.org/10.1109/TBME.2007.905419>

551 Baccalá, L. A., & Sameshima, K. (2001). Partial directed coherence: A new concept in neural structure  
552 determination. *Biological Cybernetics*. <https://doi.org/10.1007/PL00007990>

553 Brandmeyer, A., Farquhar, J. D. R., McQueen, J. M., & Desain, P. W. M. (2013). Decoding Speech  
554 Perception by Native and Non-Native Speakers Using Single-Trial Electrophysiological Data.

555 *PLOS ONE*, 8(7), e68261. <https://doi.org/10.1371/journal.pone.0068261>

- 556 Chakrabarti, S., Sandberg, H. M., Brumberg, J. S., & Krusienski, D. J. (2015). Progress in speech  
557 decoding from the electrocorticogram. *Biomedical Engineering Letters*.  
558 <https://doi.org/10.1007/s13534-015-0175-1>
- 559 Chomsky, N. (2014). *Aspects of the Theory of Syntax* (Vol. 11). MIT press.
- 560 Cometa, A., D’Orio, P., Revay, M., Micera, S., & Artoni, F. (2021). Stimulus evoked causality estimation  
561 in stereo-EEG. *Journal of Neural Engineering*, 18(5), 056041. [https://doi.org/10.1088/1741-](https://doi.org/10.1088/1741-2552/ac27fb)  
562 [2552/ac27fb](https://doi.org/10.1088/1741-2552/ac27fb)
- 563 Correia, J. M., Jansma, B. M. B., & Bonte, M. (2015). Decoding Articulatory Features from fMRI  
564 Responses in Dorsal Speech Regions. *The Journal of Neuroscience*, 35(45), 15015.  
565 <https://doi.org/10.1523/JNEUROSCI.0977-15.2015>
- 566 Cortes, C., & Vapnik, V. (1995). Support-vector networks. *Machine Learning*, 20(3), 273–297.  
567 <https://doi.org/10.1007/BF00994018>
- 568 Cossu, M., Cardinale, F., Castana, L., Citterio, A., Francione, S., Tassi, L., Benabid, A. L., & Lo Russo,  
569 G. (2005). Stereoelectroencephalography in the presurgical evaluation of focal epilepsy: A  
570 retrospective analysis of 215 procedures. *Neurosurgery*, 57(4), 706–718; discussion 706-718.
- 571 Cossu, M., Fuschillo, D., Casaceli, G., Pelliccia, V., Castana, L., Mai, R., Francione, S., Sartori, I.,  
572 Gozzo, F., Nobili, L., Tassi, L., Cardinale, F., & Lo Russo, G. (2015).  
573 Stereoelectroencephalography-guided radiofrequency thermocoagulation in the epileptogenic  
574 zone: A retrospective study on 89 cases. *Journal of Neurosurgery*, 123(6), 1358–1367.  
575 <https://doi.org/10.3171/2014.12.JNS141968>
- 576 Destrieux, C., Fischl, B., Dale, A., & Halgren, E. (2010). Automatic parcellation of human cortical gyri  
577 and sulci using standard anatomical nomenclature. *NeuroImage*, 53(1), 1–15.  
578 <https://doi.org/10.1016/j.neuroimage.2010.06.010>
- 579 Ding, N., Melloni, L., Zhang, H., Tian, X., & Poeppel, D. (2015). Cortical tracking of hierarchical  
580 linguistic structures in connected speech. *Nature Neuroscience*. <https://doi.org/10.1038/nn.4186>

- 581 Do, T.-T. N., Lin, C.-T., & Gramann, K. (2021). Human brain dynamics in active spatial navigation.  
582 *Scientific Reports*, 11(1), 13036. <https://doi.org/10.1038/s41598-021-92246-4>
- 583 Fischl, B. (2012). FreeSurfer. *NeuroImage*, 62(2), 774–781.  
584 <https://doi.org/10.1016/j.neuroimage.2012.01.021>
- 585 Friederici, A. D., Chomsky, N., Berwick, R. C., Moro, A., & Bolhuis, J. J. (2017). Language, mind and  
586 brain. *Nature Human Behaviour*, 1(10), 713–722. <https://doi.org/10.1038/s41562-017-0184-4>
- 587 Geweke, J. (1982). Measurement of linear dependence and feedback between multiple time series.  
588 *Journal of the American Statistical Association*. <https://doi.org/10.1080/01621459.1982.10477803>
- 589 Granger, C. W. J. (1969). Investigating Causal Relations by Econometric Models and Cross-spectral  
590 Methods. *Econometrica*. <https://doi.org/10.2307/1912791>
- 591 Grodzinsky, Y., & Friederici, A. D. (2006). Neuroimaging of syntax and syntactic processing. *Current*  
592 *Opinion in Neurobiology*, 16(2), 240–246. <https://doi.org/10.1016/j.conb.2006.03.007>
- 593 Guenther, F. H., Brumberg, J. S., Wright, E. J., Nieto-Castanon, A., Tourville, J. A., Panko, M., Law, R.,  
594 Siebert, S. A., Bartels, J. L., Andreasen, D. S., Ehirim, P., Mao, H., & Kennedy, P. R. (2009). A  
595 Wireless Brain-Machine Interface for Real-Time Speech Synthesis. *PLOS ONE*, 4(12), e8218.  
596 <https://doi.org/10.1371/journal.pone.0008218>
- 597 Guiñón, J., Ortega, E., García-Antón, J., & Pérez-Herranz, V. (2007). *Moving average and Savitzki-Golay*  
598 *smoothing filters using Matlab*.
- 599 Gwin, J. T., Gramann, K., Makeig, S., & Ferris, D. P. (2011). Electro cortical activity is coupled to gait  
600 cycle phase during treadmill walking. *NeuroImage*, 54(2), 1289–1296.  
601 <https://doi.org/10.1016/j.neuroimage.2010.08.066>
- 602 He, B., Astolfi, L., Valdes-Sosa, P. A., Marinazzo, D., Palva, S. O., Benar, C. G., Michel, C. M., &  
603 Koenig, T. (2019). Electrophysiological Brain Connectivity: Theory and Implementation. *IEEE*  
604 *Transactions on Biomedical Engineering*. <https://doi.org/10.1109/TBME.2019.2913928>
- 605 Hickok, G., & Poeppel, D. (2000). Towards a functional neuroanatomy of speech perception. *Trends in*  
606 *Cognitive Sciences*, 4(4), 131–138. [https://doi.org/10.1016/S1364-6613\(00\)01463-7](https://doi.org/10.1016/S1364-6613(00)01463-7)

- 607 Hochreiter, S., & Schmidhuber, J. (1997). Long Short-Term Memory. *Neural Computation*.  
608 <https://doi.org/10.1162/neco.1997.9.8.1735>
- 609 Honey, C. J., Sporns, O., Cammoun, L., Gigandet, X., Thiran, J. P., Meuli, R., & Hagmann, P. (2009).  
610 Predicting human resting-state functional connectivity from structural connectivity. *Proceedings of*  
611 *the National Academy of Sciences of the United States of America*.  
612 <https://doi.org/10.1073/pnas.0811168106>
- 613 Kayne, R. S. (2019). What Is Suppletion? On \*Goed and on Went in Modern English. *Transactions of the*  
614 *Philological Society*. <https://doi.org/10.1111/1467-968X.12173>
- 615 Keller, C. J., Honey, C. J., Mégevand, P., Entz, L., Ulbert, I., & Mehta, A. D. (2014). Mapping human  
616 brain networks with cortico-ortical evoked potentials. *Philosophical Transactions of the Royal Society*  
617 *B: Biological Sciences*. <https://doi.org/10.1098/rstb.2013.0528>
- 618 Lachaux, J. P., Rudrauf, D., & Kahane, P. (2003). Intracranial EEG and human brain mapping. *Journal*  
619 *of Physiology Paris*. <https://doi.org/10.1016/j.jphysparis.2004.01.018>
- 620 Logothetis, N. K., Augath, M., Murayama, Y., Rauch, A., Sultan, F., Goense, J., Oeltermann, A., &  
621 Merkle, H. (2010). The effects of electrical microstimulation on cortical signal propagation.  
622 *Nature Neuroscience*. <https://doi.org/10.1038/nn.2631>
- 623 Lukic, S., Borghesani, V., Weis, E., Welch, A., Bogley, R., Neuhaus, J., Deleon, J., Miller, Z. A., Kramer,  
624 J. H., Miller, B. L., Dronkers, N. F., & Gorno-Tempini, M. L. (2021). Dissociating nouns and  
625 verbs in temporal and perisylvian networks: Evidence from neurodegenerative diseases. *Cortex;*  
626 *a Journal Devoted to the Study of the Nervous System and Behavior*, 142, 47–61.  
627 <https://doi.org/10.1016/j.cortex.2021.05.006>
- 628 M. S. Mahmud, F. Ahmed, M. Yeasin, & G. M. Bidelman. (2020). Decoding Categorical Speech  
629 Perception from Evoked Brain Responses. *2020 IEEE Region 10 Symposium (TENSYP)*, 766–  
630 769. <https://doi.org/10.1109/TENSYP50017.2020.9230856>

- 631 Magrassi, L., Aromataris, G., Cabrini, A., Annovazzi-Lodi, V., & Moro, A. (2015). Sound  
632 representation in higher language areas during language generation. *Proceedings of the National*  
633 *Academy of Sciences*. <https://doi.org/10.1073/pnas.1418162112>
- 634 Maris, E., & Oostenveld, R. (2007). Nonparametric statistical testing of EEG- and MEG-data. *Journal of*  
635 *Neuroscience Methods*. <https://doi.org/10.1016/j.jneumeth.2007.03.024>
- 636 Martín Abadi, Ashish Agarwal, Paul Barham, Eugene Brevdo, Zhifeng Chen, Craig Citro, Greg S.  
637 Corrado, Andy Davis, Jeffrey Dean, Matthieu Devin, Sanjay Ghemawat, Ian Goodfellow,  
638 Andrew Harp, Geoffrey Irving, Michael Isard, Jia, Y., Rafal Jozefowicz, Lukasz Kaiser,  
639 Manjunath Kudlur, ... Xiaoqiang Zheng. (2015). *TensorFlow: Large-Scale Machine Learning on*  
640 *Heterogeneous Systems*. <https://www.tensorflow.org/>
- 641 Martin, S., Iturrate, I., Millán, J. del R., Knight, R. T., & Pasley, B. N. (2018). Decoding Inner Speech  
642 Using Electrocorticography: Progress and Challenges Toward a Speech Prosthesis. *Frontiers in*  
643 *Neuroscience*, 12, 422. <https://doi.org/10.3389/fnins.2018.00422>
- 644 Matchin, W., & Hickok, G. (2020). The Cortical Organization of Syntax. *Cerebral Cortex (New York,*  
645 *N.Y. : 1991)*, 30(3), 1481–1498. <https://doi.org/10.1093/cercor/bhz180>
- 646 Matsui, T., Tamura, K., Koyano, K. W., Takeuchi, D., Adachi, Y., Osada, T., & Miyashita, Y. (2011).  
647 Direct comparison of spontaneous functional connectivity and effective connectivity measured  
648 by intracortical microstimulation: An fMRI study in macaque monkeys. *Cerebral Cortex*.  
649 <https://doi.org/10.1093/cercor/bhr019>
- 650 Matsumoto, R., & Kunieda, T. (2019). Cortico-cortical evoked potentials mapping. In S. Lhatoo, P.  
651 Kahane, & H. Lüders (Eds.), *Invasive Studies of the Human Epileptic Brain—Principles and Practice*  
652 (First, pp. 431–452). Oxford University Press.
- 653 Matsumoto, R., Kunieda, T., & Nair, D. (2017). Single pulse electrical stimulation to probe functional  
654 and pathological connectivity in epilepsy. *25th Anniversary Issue*, 44, 27–36.  
655 <https://doi.org/10.1016/j.seizure.2016.11.003>

- 656 Matsumoto, R., Nair, D. R., LaPresto, E., Najm, I., Bingaman, W., Shibasaki, H., & Lüders, H. O.  
657 (2004). Functional connectivity in the human language system: A cortico-cortical evoked  
658 potential study. *Brain*. <https://doi.org/10.1093/brain/awh246>
- 659 Milde, T., Leistriz, L., Astolfi, L., Miltner, W. H. R., Weiss, T., Babiloni, F., & Witte, H. (2010). A new  
660 Kalman filter approach for the estimation of high-dimensional time-variant multivariate AR  
661 models and its application in analysis of laser-evoked brain potentials. *NeuroImage*.  
662 <https://doi.org/10.1016/j.neuroimage.2009.12.110>
- 663 Moro, A. (2014a). On the similarity between syntax and actions. *Trends in Cognitive Sciences*, 18(3), 109–  
664 110.
- 665 Moro, A. (2014b). Response to Pulvermüller: The syntax of actions and other metaphors. *Trends in*  
666 *Cognitive Sciences*, 18(5), 221.
- 667 Moro, A. (2016). *Impossible languages*. MIT Press.  
668 <https://doi.org/10.7551/mitpress/9780262034890.001.0001>
- 669 Munari, C., Hoffmann, D., Francione, S., Kahane, P., Tassi, L., Lo Russo, G., & Benabid, A. L. (1994).  
670 Stereo-electroencephalography methodology: Advantages and limits. *Acta Neurologica*  
671 *Scandinavica. Supplementum*, 152, 56–67, discussion 68-9. [https://doi.org/10.1111/j.1600-](https://doi.org/10.1111/j.1600-0404.1994.tb05188.x)  
672 [0404.1994.tb05188.x](https://doi.org/10.1111/j.1600-0404.1994.tb05188.x)
- 673 N. T. Duc & B. Lee. (2020). Decoding Brain Dynamics in Speech Perception Based on EEG  
674 Microstates Decomposed by Multivariate Gaussian Hidden Markov Model. *IEEE Access*, 8,  
675 146770–146784. <https://doi.org/10.1109/ACCESS.2020.3015292>
- 676 Neuhäuser, M. (2011). Wilcoxon–Mann–Whitney Test. In M. Lovric (Ed.), *International Encyclopedia of*  
677 *Statistical Science* (pp. 1656–1658). Springer. [https://doi.org/10.1007/978-3-642-04898-2\\_615](https://doi.org/10.1007/978-3-642-04898-2_615)
- 678 Nichols, T. E., & Holmes, A. P. (2002). Nonparametric permutation tests for functional neuroimaging:  
679 A primer with examples. *Human Brain Mapping*. <https://doi.org/10.1002/hbm.1058>
- 680 Nordin, A. D., Hairston, W. D., & Ferris, D. P. (2019). Human electrocortical dynamics while stepping  
681 over obstacles. *Scientific Reports*, 9(1), 4693. <https://doi.org/10.1038/s41598-019-41131-2>



- 682 Ossmy, O., Fried, I., & Mukamel, R. (2015). Decoding speech perception from single cell activity in  
683 humans. *NeuroImage*, *117*, 151–159. <https://doi.org/10.1016/j.neuroimage.2015.05.001>
- 684 Panachakel, J. T., & Ramakrishnan, A. G. (2021). Decoding Covert Speech From EEG-A  
685 Comprehensive Review. *Frontiers in Neuroscience*, *15*, 392.  
686 <https://doi.org/10.3389/fnins.2021.642251>
- 687 Pedregosa, F., Varoquaux, G., Gramfort, A., Michel, V., Thirion, B., Grisel, O., Blondel, M.,  
688 Prettenhofer, P., Weiss, R., Dubourg, V., Vanderplas, J., Passos, A., Cournapeau, D., Brucher,  
689 M., Perrot, M., & Duchesnay, É. (2011). Scikit-learn: Machine Learning in Python. *Journal of*  
690 *Machine Learning Research*, *12*(85), 2825–2830.
- 691 Penny, W. D., Stephan, K. E., Mechelli, A., & Friston, K. J. (2004). Modelling functional integration: A  
692 comparison of structural equation and dynamic causal models. *NeuroImage*.  
693 <https://doi.org/10.1016/j.neuroimage.2004.07.041>
- 694 Poeppel, D., Idsardi, W. J., & van Wassenhove, V. (2008). Speech perception at the interface of  
695 neurobiology and linguistics. *Philosophical Transactions of the Royal Society of London. Series B,*  
696 *Biological Sciences*, *363*(1493), 1071–1086. PubMed. <https://doi.org/10.1098/rstb.2007.2160>
- 697 Proix, T., Delgado Saa, J., Christen, A., Martin, S., Pasley, B. N., Knight, R. T., Tian, X., Poeppel, D.,  
698 Doyle, W. K., Devinsky, O., Arnal, L. H., Mégevand, P., & Giraud, A.-L. (2022). Imagined  
699 speech can be decoded from low- and cross-frequency intracranial EEG features. *Nature*  
700 *Communications*, *13*(1), 48. <https://doi.org/10.1038/s41467-021-27725-3>
- 701 Radovic, M., Ghalwash, M., Filipovic, N., & Obradovic, Z. (2017). Minimum redundancy maximum  
702 relevance feature selection approach for temporal gene expression data. *BMC Bioinformatics*,  
703 *18*(1), 9. <https://doi.org/10.1186/s12859-016-1423-9>
- 704 Russo, S., Pigorini, A., Mikulan, E., Sarasso, S., Rubino, A., Zauli, F. M., Parmigiani, S., d’Orto, P.,  
705 Cattani, A., Francione, S., Tassi, L., Bassetti, C. L. A., Lo Russo, G., Nobili, L., Sartori, I., &  
706 Massimini, M. (2021). Focal lesions induce large-scale percolation of sleep-like intracerebral

- 707 activity in awake humans. *NeuroImage*, 234, 117964.  
708 <https://doi.org/10.1016/j.neuroimage.2021.117964>
- 709 Salmelin, R., & Kujala, J. (2006). Neural representation of language: Activation versus long-range  
710 connectivity. *Trends in Cognitive Sciences*, 10(11), 519–525.  
711 <https://doi.org/10.1016/j.tics.2006.09.007>
- 712 Schwarz, G. (1978). Estimating the Dimension of a Model. *The Annals of Statistics*.  
713 <https://doi.org/10.1214/aos/1176344136>
- 714 Shapiro, S. S., & Wilk, M. B. (1965). An Analysis of Variance Test for Normality (Complete Samples).  
715 *Biometrika*, 52(3/4), 591–611. <https://doi.org/10.2307/2333709>
- 716 Shmuel, A., & Leopold, D. A. (2008). Neuronal correlates of spontaneous fluctuations in fMRI signals  
717 in monkey visual cortex: Implications for functional connectivity at rest. *Human Brain Mapping*.  
718 <https://doi.org/10.1002/hbm.20580>
- 719 Trebault, L., Deman, P., Tuyisenge, V., Jedynak, M., Hugues, E., Rudrauf, D., Bhattacharjee, M., Tadel,  
720 F., Chanteloup-Foret, B., Saubat, C., Reyes Mejia, G. C., Adam, C., Nica, A., Pail, M., Dubeau,  
721 F., Rheims, S., Trébuchon, A., Wang, H., Liu, S., ... David, O. (2018). Probabilistic functional  
722 tractography of the human cortex revisited. *NeuroImage*, 181, 414–429.  
723 <https://doi.org/10.1016/j.neuroimage.2018.07.039>
- 724 Tzourio-Mazoyer, N., Perrone-Bertolotti, M., Jobard, G., Mazoyer, B., & Baciú, M. (2017). Multi-  
725 factorial modulation of hemispheric specialization and plasticity for language in healthy and  
726 pathological conditions: A review. *Cortex; a Journal Devoted to the Study of the Nervous System and*  
727 *Behavior*, 86, 314–339. <https://doi.org/10.1016/j.cortex.2016.05.013>
- 728 Van Essen, D. C., Ugurbil, K., Auerbach, E., Barch, D., Behrens, T. E. J., Bucholz, R., Chang, A.,  
729 Chen, L., Corbetta, M., Curtiss, S. W., Della Penna, S., Feinberg, D., Glasser, M. F., Harel, N.,  
730 Heath, A. C., Larson-Prior, L., Marcus, D., Michalareas, G., Moeller, S., ... WU-Minn HCP  
731 Consortium. (2012). The Human Connectome Project: A data acquisition perspective.  
732 *NeuroImage*, 62(4), 2222–2231. PubMed. <https://doi.org/10.1016/j.neuroimage.2012.02.018>

- 733 Vigliocco, G., Vinson, D. P., Druks, J., Barber, H., & Cappa, S. F. (2011). Nouns and verbs in the  
734 brain: A review of behavioural, electrophysiological, neuropsychological and imaging studies.  
735 *Neuroscience and Biobehavioral Reviews*, *35*(3), 407–426.  
736 <https://doi.org/10.1016/j.neubiorev.2010.04.007>
- 737 Vincent, J. L., Patel, G. H., Fox, M. D., Snyder, A. Z., Baker, J. T., Van Essen, D. C., Zempel, J. M.,  
738 Snyder, L. H., Corbetta, M., & Raichle, M. E. (2007). Intrinsic functional architecture in the  
739 anaesthetized monkey brain. *Nature*. <https://doi.org/10.1038/nature05758>
- 740 Virtanen, P., Gommers, R., Oliphant, T. E., Haberland, M., Reddy, T., Cournapeau, D., Burovski, E.,  
741 Peterson, P., Weckesser, W., Bright, J., van der Walt, S. J., Brett, M., Wilson, J., Millman, K. J.,  
742 Mayorov, N., Nelson, A. R. J., Jones, E., Kern, R., Larson, E., ... van Mulbregt, P. (2020). SciPy  
743 1.0: Fundamental algorithms for scientific computing in Python. *Nature Methods*, *17*(3), 261–272.  
744 <https://doi.org/10.1038/s41592-019-0686-2>
- 745 Vorontsova, D., Menshikov, I., Zubov, A., Orlov, K., Rikunov, P., Zvereva, E., Flitman, L., Lanikin,  
746 A., Sokolova, A., Markov, S., & Bernadotte, A. (2021). Silent EEG-Speech Recognition Using  
747 Convolutional and Recurrent Neural Network with 85% Accuracy of 9 Words Classification.  
748 *Sensors*, *21*(20), 6744. <https://doi.org/10.3390/s21206744>
- 749 Wilson, G. H., Stavisky, S. D., Willett, F. R., Avansino, D. T., Kelemen, J. N., Hochberg, L. R.,  
750 Henderson, J. M., Druckmann, S., & Shenoy, K. V. (2020). Decoding spoken English from  
751 intracortical electrode arrays in dorsal precentral gyrus. *Journal of Neural Engineering*, *17*(6),  
752 066007. <https://doi.org/10.1088/1741-2552/abbfef>
- 753 Wu, J., Ngo, G. H., Greve, D., Li, J., He, T., Fischl, B., Eickhoff, S. B., & Yeo, B. T. T. (2018).  
754 Accurate nonlinear mapping between MNI volumetric and FreeSurfer surface coordinate  
755 systems. *Human Brain Mapping*, *39*(9), 3793–3808. <https://doi.org/10.1002/hbm.24213>
- 756 Xia, M., Wang, J., & He, Y. (2013). BrainNet Viewer: A Network Visualization Tool for Human Brain  
757 Connectomics. *PLOS ONE*, *8*(7), e68910. <https://doi.org/10.1371/journal.pone.0068910>

- 758 Y. Ho & S. Wookey. (2020). The Real-World-Weight Cross-Entropy Loss Function: Modeling the  
759 Costs of Mislabeling. *IEEE Access*, 8, 4806–4813.  
760 <https://doi.org/10.1109/ACCESS.2019.2962617>
- 761 Zhang, D., Gong, E., Wu, W., Lin, J., Zhou, W., & Hong, B. (2012). Spoken sentences decoding based  
762 on intracranial high gamma response using dynamic time warping. *Proceedings of the Annual*  
763 *International Conference of the IEEE Engineering in Medicine and Biology Society, EMBS*, 3292–3295.  
764 <https://doi.org/10.1109/EMBC.2012.6346668>
- 765