- 1 **Title:** BOLD cofluctuation 'events' are predicted from static functional connectivity
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15

16 ABSTRACT

- 17 Recent work identified single time points ("events") of high regional cofluctuation in functional
- 18 Magnetic Resonance Imaging (fMRI) which contain more large-scale brain network information
- 19 than other, low cofluctuation time points. This suggested that events might be a discrete,
- 20 temporally sparse signal which drives functional connectivity (FC) over the timeseries. However,
- a different, not yet explored possibility is that network information differences between time
- 22 points are driven by sampling variability on a constant, static, noisy signal. Using a combination
- 23 of real and simulated data, we examined the relationship between cofluctuation and network
- structure and asked if this relationship was unique, or if it could arise from sampling variability
- alone. First, we show that events are not discrete there is a gradually increasing relationship
 between network structure and cofluctuation: ~50% of samples show very strong network
- between network structure and cofluctuation; ~50% of samples show very strong network
 structure. Second, using simulations we show that this relationship is predicted from sampling
- variability on static FC. Finally, we show that randomly selected points can capture network
- 29 structure about as well as events, largely because of their temporal spacing. Together, these
- 30 results suggest that, while events exhibit particularly strong representations of static FC, there is
- 31 little evidence that events are unique timepoints that drive FC structure. Instead, a parsimonious
- 32 explanation for the data is that events arise from a single static, but noisy, FC structure.
- 33 24 KENA

34 KEYWORDS

Resting-state fMRI, cofluctuations, events, simulations, RSFC, networks

37 HIGHLIGHTS

- Past results suggested high cofluctuation BOLD "events" drive fMRI functional
 connectivity, FC
- Here, events were examined in both real fMRI data and a stationary null model to
 test this model
- In real data, >50% of BOLD timepoints show high modularity and similarity to time averaged FC
- Stationary null models identified events with similar behavior to real data
- Events may not be a transient driver of static FC, but rather an expected outcome of it.
- 46

47 **INTRODUCTION**

48 The human brain is organized in large-scale systems, or 'networks,' with coordinated 49 functions such as the visual network, somatomotor network, and default mode network. In 50 humans, these networks can be identified by grouping regions of the brain that have highly 51 correlated spontaneous BOLD fMRI signals - regions with high "functional connectivity (FC)" 52 (Biswal et al., 1995; Power et al., 2011; Yeo et al., 2011). These FC networks have been shown 53 to have a canonical spatial layout (most people have the same networks represented in the 54 same locations), with stable patterns of individual variation (each person's network topography 55 is slightly different from the canonical layout and consistent within themselves across time 56 (Gordon et al., 2017; Gratton et al., 2018; Laumann et al., 2015; Seitzman et al., 2019). At both 57 the individual and group level, functional network topology accurately predicts which regions of 58 the brain will be activated during specific tasks (Braga et al., 2020; Gordon et al., 2017; Smith et 59 al., 2009; Tavor et al., 2016) and variations in network topology are related to individual differences in behavior outside of the scanner (Bijsterbosch et al., 2018; Kong et al., 2019; 60 61 Smith et al., 2015; van den Heuvel et al., 2009)

However, analysis of spontaneous fMRI data is not straightforward. Unlike in task-fMRI, 62 63 there is no predefined temporal structure that can be used to separate relevant signals from 64 artifactual signals. Instead, typical analyses of spontaneous (resting-state) fMRI remove 65 physiological artifacts (motion, respiration, cardiac rhythms, etc.) and assume the residual signal is the neural signal of interest (Power et al., 2020). It is typically presumed that this signal is 66 67 equally present at all moments and FC is calculated using all available data over long periods. 68 However, recent work suggested that rather than being constantly present, FC information 69 might be inordinately present at particular time points called "events" (Esfahlani et al., 2020). 70 Esfahlani and colleagues found that "events," time points with the highest BOLD signal 71 cofluctuation, reproduce static functional connectivity patterns better than the same number of 72 "non-events," time points with the lowest BOLD signal cofluctuation, and require relatively few 73 timepoints to reproduce them well. The authors concluded that rather than functional network 74 structure being present at all timepoints, it is driven by events - a discrete and temporally 75 sparse phenomena (Esfahlani et al., 2020). This idea has deep implications for the field: a 76 thorough analysis of events across brain organizational levels (e.g., from systems to cellular 77 recordings) could reveal information about the physiological mechanisms of FC and new 78 analysis methods focused on events could improve the clinical utility of fMRI (Esfahlani et al., 79 2021; Greenwell et al., 2021).

80 But, there are alternative interpretations of these findings which have not yet been 81 explored. First, it is possible that differences between "events" and "non-events" are driven by 82 contamination in "non-events" (motion, respiration, etc.) rather than by a unique signal present 83 during "events." Second, it has been shown that random sampling variability in BOLD data is 84 high and alone can create the appearance of discrete states in stationary FC simulations (Hlinka 85 & Hadrava, 2015; Laumann et al., 2017). This principle may apply here too - sampling 86 variability could make a subset of single points look extreme, even if they are drawn from a 87 continuous distribution around a static FC matrix (note that if this were the case, events 88 methodology may still be a useful way to rapidly and accurately reproduce static FC structure. 89 but this outcome would suggest that a deep focus on events physiology relative to other 90 timepoints has less utility). In this paper, we ask (1) if events are unique points which drive FC, 91 (2) if non-events are unique points with high contamination, or (3) if events and non-events are 92 an expected consequence of static FC and sampling variability.

To answer these questions, we conduct a series of analyses on real and simulated data. First, we use real data from the Midnight Scan Club dataset to test how unique events and nonevents are by examining whether their properties differ markedly from intermediate timepoints.

96 Second, we create models of simulated static BOLD data to see if sampling variability on a

97 static signal is sufficient to explain event behavior. Finally, we examine why events are able to 98 recreate static FC structure with so few time points.

99

100 MATERIALS AND METHODS

101

102 **Overview and Dataset**

103 The goal of this project was to investigate if high cofluctuation moments in resting state fMRI 104 BOLD signals are discrete events that drive functional connectivity. We used a combination of

- 105 real and simulated data for these analyses.
- 106

107 The publicly available Midnight Scan Club (MSC) dataset was used as our real sample dataset.

108 The MSC dataset contains fMRI data from 10 highly sampled individuals (5 females, ages 24-109 34). The data for each subject was collected across 10 fMRI sessions within 7 weeks. Across

110 these sessions, the MSC dataset includes 5 hours of resting state fMRI; this resting-state data is

- 111 the focus of our analyses. One participant (MSC08) has been excluded from these analyses
- because of head motion and drowsiness during rest. For single session-analysis and
- simulations, sessions with less than 333 usable timepoints (6/90 sessions) were excluded. All
- 114 data collection was approved by the Washington University Internal Review Board and written
- 115 informed consent was received from all participants. The dataset and processing have been
- previously described in detail (Gordon et al., 2017). A summary of relevant details is provided
- 117 below. 118

119 MRI Acquisition

MRI data were acquired on a Siemens 3T Magnetom Tim Trio with a 12-channel head coil. T1weighted (sagittal, 224 slices, 0.8 mm isotropic resolution, TE = 3.74ms, TR = 2.4s, TI = 1.0s,

- 122 flip angle = 8 degrees), T2-weighted (sagittal, 224 slices, 0.8 mm isotropic resolution, TE =
- 123 479ms, TR = 3.2s) and functional (gradient-echo EPI sequence, TE = 27ms, TR = 2.2 s, flip
- angle = 90, voxels = isotropic 4mm³, 36 axial slices) MRI images were collected. Thirty minutes
- 125 of resting-state fMRI were collected at the start of each session.
- 126

127 **Preprocessing**

- 128 Data processing for the MSC dataset is explained in detail elsewhere (Gordon et al., 2017).
- 129 Relevant details for this project are shared below.
- 130

131 <u>Structural MRI Processing:</u> For each participant, T1 images were averaged together and used

- to generate a cortical surface in Freesurfer (Dale et al., 1999). These surfaces were hand-edited
- and registered into fs_LR_32k surface space (Glasser et al., 2013).
- 134
- 135 <u>Functional MRI Processing:</u> Slice time correction, motion correction, and intensity normalization
- to mode 1000 were all completed in the volume. The functional data was then registered to the
- 137 T2 image (which was registered to the T1 image registered to template space), resampled to
- 138 3mm isotropic resolution and distortion corrected (Gordon et al., 2017). All alignments were
- 139 applied in a single step.
- 140
- 141 <u>Functional Connectivity Processing:</u> Described in detail elsewhere (Power et al., 2014),
- 142 preprocessing steps were taken to reduce the effect of artifacts on functional network analysis.
- 143 This included the regression of nuisance signals (white matter, ventricles, global signal, motion
- and derivative and expansion terms), scrubbing of high motion frames (FD > 0.2 mm), and
- bandpass filtering (0.009 Hz to 0.08 Hz). For two subjects (MSC03 and MSC10), motion
- 146 parameters were low pass filtered before censoring to address respiratory activity in the motion

traces (Fair et al., 2020; Gordon et al., 2017). Functional data was then registered to the surface
 and spatially smoothed (FWHM = 6 mm, sigma = 2.55) (Marcus et al., 2011).

149

150 Network and region definition

- 151 All analyses were done on parcellated timeseries extracted using a group-level map of 333
- 152 cortical parcels (Gordon et al., 2016). These 333 parcels can be split into 12 functional systems:
- 153 somatomotor (SM), somatomotor lateral (SM-lat), visual (Vis), auditory (Aud), cingulo-opercular
- 154 (CO), salience (Sal), frontoparietal (FP), dorsal attention (DAN), ventral attention (VAN), default
- 155 mode (DMN), parietal memory (PMN), and retrosplenial (RSP). These systems are used to
- 156 group parcels in the visualization of FC matrices.
- 157

158 Comparisons between events and static functional connectivity in real data

- 159 Our first goal was to compare the network structure present in events, non-events, and
- 160 intermediate bins. We followed the approach used in Esfahlani et al., 2020, calculating the RSS
- 161 (root-sum-square) cofluctuation for each timepoint and binning timepoints by their RSS
- 162 cofluctuation value. We compared the network structure present in each bin by creating FC
- 163 matrices for each bin and calculating the similarity between bin FC and whole session FC and
- 164 the modularity of bin FC. These measures are defined below.
- 165
- 166 Cofluctuation Time Series and Events: The method for calculating cofluctuation and identifying 167 events has been fully described elsewhere (Esfahlani et al 2020). It was followed exactly and is 168 summarized here. The original fMRI BOLD timeseries was z-scored per parcel. For each edge 169 (a unique pair of parcels), the z-scored values at each timepoint were multiplied, resulting in an 170 edges X timepoints matrix. As described elsewhere, this timeseries (also called the edge-time-171 series), represents the exact contribution of each timepoint to static FC (Esfahlani et al., 2020). 172 For each time point, the RSS (root-sum-square) across parcels was calculated, resulting a 1 X 173 timepoints matrix containing the RSS cofluctuation value at each timepoint. Timepoints were 174 binned based on RSS cofluctuation value in 5% bins, with the 5% of points with highest
- 175 cofluctuation in bin one, the next 5% of points in bin two and so on.
- 176

177 *Functional Connectivity (FC):* For each session and subject, functional connectivity matrices

- 178 were calculated using either the timepoints from the full session ('static' FC matrices) or from
- the timepoints in each bin (cofluctuation bin FC matrices). In all cases, FC was calculated by the product moment correlation between each pair of parcel timeseries, resulting in a 333X333
- 180 product moment correlation between each pair of parcel timesenes, resulting in a 353,555 181 functional network matrix. Parcels were grouped by functional system for visualization. Edges
- 181 inclinational field of the second second second system for visualization. Edges 182 within the diagonal blocks represent within-system correlations, and edges in the off-diagonal
- 183 blocks represent between-system correlations.
- 184
- 185 <u>Similarity:</u> Similarity between each bin's FC and whole-session 'static' FC was calculated by vectorizing both matrices and taking the correlation between them.
- 187
- 188 <u>*Modularity:*</u> Modularity was calculated for each bin as measure of network structure. Modularity maximization is a strategy used to arrange nodes into communities in which there are more
- 190 edges within communities than expected by random chance. Each matrix was thresholded for
- sparseness, keeping only the top 5% of weighted edges (5% edge density). Then, all remaining
- edge weights were set to 1, making the graph unweighted. Newman's spectral optimization was
- 192 used to identify the optimal network structure. This structure was then quantified using
- 194 Newman's modularity statistic, Q, which measures the fraction of within-network edges minus
- 195 the expected value of within-network edges in a network with the same communities but random
- 196 connections (Newman & Girvan, 2004). Larger values of modularity reflect stronger community
- 197 structure than expected by chance.

198

199 Comparisons between events and static functional connectivity in simulated data

200 Our second goal was to test whether the relationship between network structure and

cofluctuation found in real data could be explained by sampling variability in a stationary model.
 To examine this, we created simulated data with the same dimensionality and static covariance
 structure as BOLD data but sampled from a random Gaussian distribution.

203

205 Simulated BOLD Data: For each subject and session, data was sampled from a Gaussian 206 distribution in the dimensionality of the real data from that session. Separately, a static FC 207 matrix was calculated from the full 30 minutes of real data. The random timeseries were 208 projected on to the eigenvectors derived from the static FC matrix, resulting in data matched in 209 dimensionality and covariance structure with real BOLD data but stationary by construction. This 210 strategy is largely adapted from prior simulation work (Laumann et al., 2017). We then did the 211 same analysis in the simulation data as was described above for real data - calculating 212 cofluctuation, binning frames by cofluctuation, and comparing the network structure present in

each bin with two measures (similarity to static FC and modularity).

214

 $\begin{array}{lll} & \underline{Simulated \ Toy \ Model:} \ \mbox{To aid in our second goal, we did a supplementary analysis investigating} \\ & the relationship between network structure and cofluctuation in a very simple non-BOLD-like \\ & data set. The data set comprised of 4 nodes total – 2 anti-correlated networks with two nodes \\ & each. Network A was defined by the simple sine(x) wave, and both network A nodes were given \\ & that signal. Network B was defined by sine(x + \pi/2) and both network B nodes were given that \\ & signal. Normally distributed random noise of half the magnitude as the real signal was added to \\ & all four nodes. Then, cofluctuation was calculated for each timepoint, timepoints were binned by \\ & by the signal was defined by \\ & all four nodes. Then, cofluctuation was calculated for each timepoint, timepoints were binned by \\ & by the signal was defined by \\ & by the signal was added to \\ & all four nodes. Then, cofluctuation was calculated for each timepoint, timepoints were binned by \\ & by the signal was defined by \\ & by the signal was added to \\ & by the si$

222 cofluctuation, and similarity with time-averaged FC calculated for each bin.

223

224 **Temporal Spacing Analysis**

Our third goal was to compare the effects of different sampling methods on the network structure present in the sampled points. We specifically wanted to investigate the effect of temporal spacing on network structure.

228

229 Comparison of Sampling Methods

For each subject and session, we examined the network structure present in four groups of time points: high cofluctuation points (selected as the top 5% of points with highest RSS cofluctuation), low cofluctuation points (selected as the bottom 5% of points with the lowest RSS cofluctuation), consecutive points (5% of points selected consecutively beginning at a random

point of the session and wrapping around when needed), and random points (5% of points

selected randomly from the session). For consecutive samples, 100 iterations were done for

- each session to not bias the result by starting location. We further tested this by varying the
- 237 number of time points selected rather than choosing 5% of time points. The number of time
- 238 points was varied from 1 to 100.
- 239

240 <u>Circular Offset Analysis</u>

241 In a supplemental analysis, we examined the relationship between cofluctuation and network

structure after removing temporal spacing effects. To do this, we binned time points by

cofluctuation and then circularly shifted them by 1-10 points in both directions to maintain the

temporal spacing found in the original binning while varying their cofluctuation values. However,

because we previously scrubbed high motion points from this data set, it was not possible to

select 5% of time points (as in other binned analyses) and shift them without running into

- scrubbed points. To address this issue, we randomly sampled only 5 points per bin and used
- 248 fewer bins (95-100, 85-90, 70-75, 45-50, 20-25, 0-5). This resulted in a smaller number of

- 249 analyzed sessions with lower peak similarities for this analysis. To reduce bias from random
- 250 sampling, we did 100 iterations and averaged the results.
- 251

252 Dataset and Code Availability

- 253 MSC data has been made publicly available
- 254 (https://openneuro.org/datasets/ds000224/versions/1.0.3). The parcellated timeseries used for
- 255 these analyses is available here (https://github.com/GrattonLab/MSC ROI data).The code for
- 256 the analyses in this paper is available at
- 257 (https://github.com/GrattonLab/Ladwig 2022 Events Static FC) which will made public upon 258 publication.
- 259

260 RESULTS

261

262 **Overview:**

263 Previous work showed that moments with high amplitude cofluctuations in BOLD, or "events",

- 264 estimate static functional connectivity patterns better than low cofluctuation moments, and can
- 265 do so with relatively few timepoints (Esfahlani et al., 2020). This suggested that (1) high
- 266 cofluctuation events may be unique, transient phenomena which drive the large-scale network
- 267 organization that we observe over long timeseries (Esfahlani et al., 2020). But there are
- 268 alternate interpretations of this result: (2) differences between low and high cofluctuation could
- 269 be driven by low cofluctuation timepoints exhibiting more BOLD artifacts (e.g., motion or 270
- respiration) that disrupt functional connectivity measures or (3) events may arise as a
- 271 consequence of sampling from a continuous distribution, where some moments will, by chance, 272 exhibit higher cofluctuation than others.
- 273

274 In this work, we test these three hypotheses. We test how network structure changes over a

- 275 range of cofluctuation amplitudes, ask if this relationship is present in stationary simulated data, 276 and analyze why events can recreate static correlation structure with so few time points.
- 277

278 1. Network structure is continuously related to cofluctuation

- 279 First, we examined the relationship between BOLD cofluctuation and network structure across a 280 range of cofluctuation amplitudes. Our hypotheses are visualized in Fig. 1A. If events are 281 specialized discrete timepoints that drive network structure, then they should especially well 282 represent network structure (purple) relative to other points. If low cofluctuation points are 283 discrete timepoints more contaminated by artifacts, they should especially poorly represent 284 network structure (yellow). If BOLD cofluctuations exhibit random variation as would be 285 expected from sampling variation, then there should be a continuous relationship between 286 cofluctuation amplitude and network structure (green).
- 287
- 288 For each participant and resting state session (30 minutes), we calculated BOLD cofluctuation 289 amplitude at each timepoint (after standard preprocessing and denoising to improve alignment 290 and remove artifacts, including those associated with motion, see Methods). In Esfahlani et al., 291 2020, events were defined as the top 5% of timepoints ranked by cofluctuation. We extended 292 this, grouping timepoints in each session into discrete 5% bins based on their cofluctuation (Fig. 293 1B). For each bin, we calculated an FC matrix using Pearson's correlation (Fig. 1C) and
- 294 computed measures of network structure as in Esfahlani et al. 2020. (Fig. 1D-E).
- 295

296 We reproduced both results from Esfahlani et al., 2020 showing that compared to FC from the 297 lowest cofluctuation bin ("non-events"), FC from events is more similar to whole-session FC 298 $(r_{events} = 0.792, r_{lowest} = 0.514, t(89) = 42.2, p = 1.2e-60)$ and more modular $(q_{events} = 0.562, q_{lowest})$ 299 = 0.478, t(89) = 12.3 p = 6.0e-21) (Fig. 1D, E). However, when we examined the relationship

300 across intermediate bins, we found that both metrics increased gradually with cofluctuation, not 301 discretely for events. The increase was especially gradual at high values of cofluctuation. In 302 fact, the top bin (events) was not substantially different than the 70th percentile bin (r_{events} = 303 $0.792 \text{ vs. } r_{70} = 0.797, r_{diff} = -0.005, t(89) = 0.48, p = 0.31; modularity: q_{events} = 0.562 \text{ vs. } q_{70} = 0.792 \text{ vs. } r_{70} = 0.797, r_{diff} = -0.005, t(89) = 0.48, p = 0.31; modularity: q_{events} = 0.562 \text{ vs. } q_{70} = 0.797, r_{diff} = -0.005, t(89) = 0.48, p = 0.31; modularity: q_{events} = 0.562 \text{ vs. } q_{70} = 0.797, r_{diff} = -0.005, t(89) = 0.48, p = 0.31; modularity: q_{events} = 0.562 \text{ vs. } q_{70} = 0.005, t(89) = 0.48, p = 0.31; modularity: q_{events} = 0.562 \text{ vs. } q_{70} = 0.797, r_{diff} = -0.005, t(89) = 0.48, p = 0.31; modularity: q_{events} = 0.562 \text{ vs. } q_{70} = 0.797, r_{diff} = -0.005, t(89) = 0.48, p = 0.31; modularity: q_{events} = 0.562 \text{ vs. } q_{70} = 0.$ 0.561, gdiff=-0.001, t(89) = 0.15, p = 0.45) and only slightly different than the 50th percentile bin 304 $(r_{50} = 0.740, q_{50} = 0.546, r_{diff} = 0.052, q_{diff} = 0.016)$. Low cofluctuation points, while substantially 305 306 different from events, were not obviously discrete when compared with the 10th and 20th 307 percentile bins ($r_{lowest} = 0.514$, $q_{lowest} = 0.478$, $r_{10} = 0.579$, $q_{10} = 0.499$, $r_{20} = 0.637$, $q_{20} = 0.515$). 308 Notably, many sets of points explicitly excluding events still recapitulate network structure well. 309 These relationships were consistent in all 9 subjects (lines in Fig. 1D-E, separated by session in 310 Fig. S1), suggesting that neither high nor low cofluctuation points are discrete, specialized. 311 timepoints that drive network structure (or the lack thereof). Rather, network structure appears to be present in all bins, with variability that is positively correlated with the cofluctuation 312 313 amplitude of a given time point. These results do not suggest that there are a small number of 314 time points which drive functional connectivity.

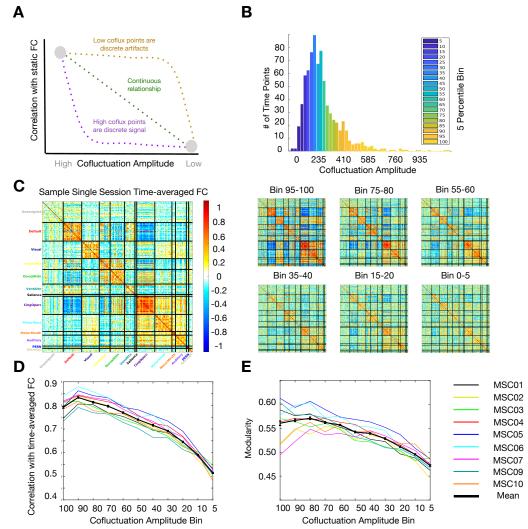


Fig 1: Network structure varies continuously with BOLD cofluctuation. (A) Previous literature showed that high cofluctuation events contain stronger network structure than low cofluctuation points (gray dots). We posited three hypotheses: (1) high cofluctuation points are discrete phenomena which drive network structure (purple), (2) low cofluctuation points are discrete

320 artifacts which do not contain network structure (vellow), or (3) there is a continuous gradual 321 relationship between cofluctuation magnitude and network structure as would be expected from 322 sampling variability (green). (B) To test these hypotheses, we binned time points into 5 323 percentile bins of increasing cofluctuation. See example histogram here from MSC05 session 4. 324 (C) For each bin, we calculated an FC matrix (examples here from MSC02 session 5) and 325 calculated two measures of network structure – similarity to static FC and modularity. (D) 326 Similarity to static FC increased gradually with cofluctuation for all subjects (black line = mean, 327 colored lines = subjects, error bars represent SEM for the group). (E) Modularity increased 328 gradually with cofluctuation as well. These results suggest that neither high nor low cofluctuation 329 time points are discrete, unique entities.

330

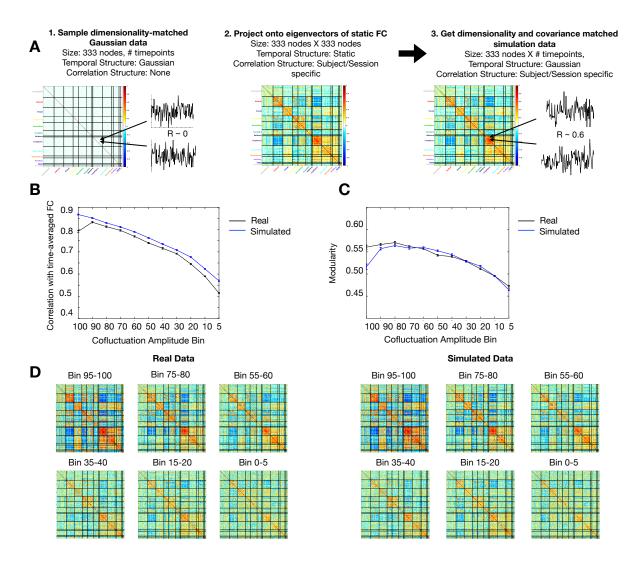
2. Stationary simulations produce similar behavior to BOLD events and non-events

332 Above, we found that there was a consistent and gradual relationship between BOLD 333 cofluctuation amplitude and network structure. Next, we asked, what drives this relationship? 334 One possible explanation is sampling variability: with noisy data, some timepoints will have 335 higher similarity to the session average, while others will have lower similarity, simply by 336 chance. Here, we tested whether sampling variability could account for event behavior by 337 creating and analyzing a simulated BOLD dataset with stationary covariance structure. In this 338 simulated dataset, as in the real data in the previous section, we identified points of high and 339 low cofluctuation and compared their relationship to network structure.

The procedure to generate simulated data is shown in **Fig. 2A**. For each subject and session, data was generated by sampling from a Gaussian distribution in the dimensionality of real data. This data was then projected on to the eigenvectors of the static correlation structure from the real BOLD data for that subject and session, resulting in random Gaussian data with stationary correlation structure matching real data (see *Methods*).

The analysis from **Figure 1** was repeated on the simulated data. We calculated cofluctuation for each time point, binned time points by cofluctuation, computed FC matrices for each bin, and compared the network structure properties across bins.

348 We found that the relationship between network structure and cofluctuation in simulated 349 data was remarkably similar to the one found in real data. Similarity to static FC (Fig. 2B) and 350 modularity (Fig. 2C) both showed gradually increasing relationships with cofluctuation in the 351 simulated data, just as in real data. Visually, the network structure present in each bin was 352 remarkably similar between simulated and real data (Fig. 2D). These results were consistent 353 within individuals and sessions (Fig S2). These results suggest that the difference between high 354 and low cofluctuation moments and their relationship to network structure can be explained by 355 sampling variability alone. Further, we note that even very simple toy models made from 356 correlated sine waves and noise show points of high and low cofluctuation amplitude and a 357 gradually increasing relationship between cofluctuation amplitude and network structure (Fig. 358 **S3**), indicating this property is not specific to BOLD data.



359

360 Fig 2: Sampling variability alone can produce event-like behavior. (A) For each subject and 361 session, we generated a dimensionality-matched timeseries sampled from a Gaussian 362 distribution. This time series was projected onto the eigenvectors of static FC calculated from 363 that session. This yielded a simulated random Gaussian data set with BOLD-matched 364 dimensionality and covariance structure. (B, C) Using the same analysis methods as in Fig 1, 365 we found that the relationship between network structure and cofluctuation in simulated data 366 was remarkably similar to the one found in real data. Both (B) similarity with session FC and (C) 367 modularity increased gradually just as they did in real data. (D) Visually, the FC matrices made 368 from specific cofluctuation bins look similar between simulated and real data. The data shown is 369 an example from a single session: MSC02 Session 5. These results suggest the relationship 370 between network structure and cofluctuation amplitude can be explained by sampling variability 371 and static FC.

372

373 3. Randomly selected timepoints can also reproduce network structure

374 One particularly notable property of events is their ability to recapitulate network structure with a

375 small number of timepoints. As shown in **Fig. 1** and Esfahlani et al., 2020, 5% of time points in a

- 376 30-minute resting state session (approximately 1.5 min. of total data) show high similarity with
- 377 the static FC calculated from the whole session (r = 0.792). In contrast, past work (Gordon et

al., 2017; Laumann et al., 2015; Noble et al., 2017) suggests that large amounts (> 30 min.) of resting state fMRI data collection are required to achieve high reliability. This discrepancy

380 appears to bolster the suggestion that events are discrete transient phenomena which drive

381 static functional connectivity.

382

However, in the previous sections, we showed that events are not unique in their ability to reproduce static FC (**Fig. 1D**). Many other points can recreate static FC. The 70th percentile points were correlated with static FC at r = 0.797 and the 50th percentile points are correlated at r = 0.740. These results raise the question: is the ability for a few points to recreate session FC driven by cofluctuation or something else?

388

We hypothesized that this apparent discrepancy was related to how the events methodology samples time points. One reason that substantial data is required for reliable FC measures is because BOLD data is autocorrelated – each time point shares information with the time points around it. In contrast, the events methodology is not constrained to select temporally adjacent points. Looking at a sample timeseries, it is obvious that events are more spread out than consecutive points (**Fig. 3A**). This is confirmed by looking at the histogram of the distance between events (**Fig. 3B**).

396

397 To test the effect of temporal spacing on network structure, we compared 5% of points (a) 398 sampled consecutively (starting from a random section of the scan). (b) sampled randomly

398 sampled consecutively (starting from a random section of the scan), (b) sampled randomly 399 across the whole scan, (c) sampled from the highest cofluctuation points (events), and (d) 400 sampled from the lowest cofluctuation moments. **Fig. 3C** shows the result: randomly sampled 401 points are similarly correlated with the static session FC structure as events (r_{random} = 0.78, r_{events})

402 = 0.79, t(89) = 1.7, p = 0.045). Random points show substantially higher similarity to static

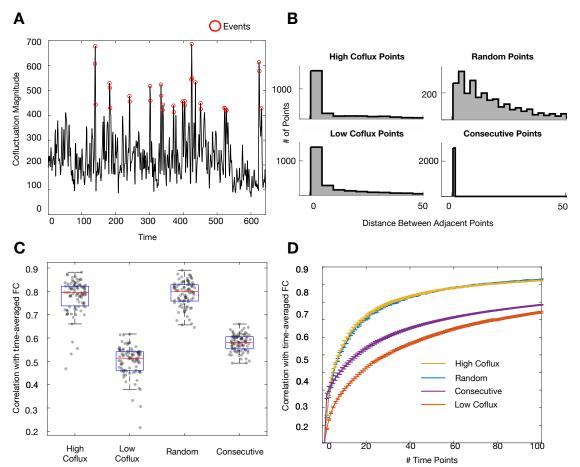
session FC than either low cofluctuation points ($r_{low} = 0.50 t(89) = 43.0 p = 1.3e^{-60}$), or

404 consecutively sampled time points ($r_{consecutive}=0.58$, $t(89) = 35.2 p = 2.42e^{-54}$). These results are 405 consistent over a range of bin sizes (**Fig. 3D**), suggesting that random temporal spacing is

406 sufficient to estimate FC well.

407

408 However, high cofluctuation points are not perfectly matched in spacing to random points 409 (several occur in close succession relative to what would be expected in a random distribution, 410 although they are more distributed than a typical consecutive timepoint FC analysis). To 411 disambiguate the effects of cofluctuation magnitude and temporal spacing, we circularly shifted 412 the cofluctuation-binned time points (see Methods) to keep temporal spacing constant and vary 413 cofluctuation. We found that after accounting for temporal spacing, there remained a graded 414 hierarchy where higher cofluctuation points contained more network structure than lower 415 cofluctuation time points (Fig. S4). The simulation results in the previous section suggest that 416 this is expected and can be parsimoniously explained by sampling variability. Jointly, these 417 findings suggest that the ability to recreate network structure with a few time points is a function 418 of both temporal spacing (as shown here) and sampling variability (as shown in the previous 419 section).



420

Fig 3: Effects of temporal spacing on estimating FC. (A) Events (red dots) are more temporally spaced than consecutive points, shown here for MSC02 session 6. (B) Histograms of distance between sampled points using consecutive, random, or cofluctuation-based sampling, aggregated over all subjects and sessions. (C) Randomly sampled points are as similar to static session FC as are events; both match static session FC much better than consecutive or low cofluctuation points. (D) These relationships hold over a range of bin sizes. These results

427 suggest that temporal spacing is an important factor in estimating FC well.

428 429 **DISCUSSION**

430

431 In this study, we asked if "events", time points with high BOLD cofluctuation, are discrete, 432 transient events that drive functional connectivity. We found that events are not discrete 433 phenomena driving FC. When they are removed, static FC structure is still present. Further, 434 there is a gradual positive relationship between network structure and cofluctuation amplitude, 435 with relatively similar behavior for the top 50% of timepoints, including events. Next, we asked if 436 this gradual relationship between network structure and cofluctuation could be explained by 437 sampling variability on static FC. We created a simulated data set matched to BOLD in 438 dimensionality and covariance structure. Our model produced the same gradual positive 439 relationship seen in real data, including the existence of extreme points like events, suggesting 440 that event behavior can be explained by sampling variability alone. Finally, we analyzed why 441 events are able to recreate static FC with so few points. We found that small numbers of 442 randomly sampled timepoints are also able reproduce static network structure well, suggesting

that both sampling variability and temporal spacing are important factors in estimating FC.

Taken together, these results support the idea that while events are an especially good

representation of the network structure present in static FC, there is not evidence that they are unique points driving it.

447

448 Should events be used to study the neural underpinnings of functional connectivity?

449 Although there is a large literature linking fMRI BOLD signal to neural activity (Heeger et al., 450 2000; Logothetis et al., 2001), the physiological mechanism of FC itself is incompletely 451 understood. Past work suggests that BOLD FC is constrained by structural connections (Honey 452 et al., 2009; Johnston et al., 2008; Vincent et al., 2007) and is related to correlations in neural 453 activity (Nir et al., 2008; Shmuel & Leopold, 2008; Vincent et al., 2007) but the underlying 454 drivers of these spontaneous activity correlations remain relatively unknown. Because events 455 contain similar functional connectivity patterns to static functional connectivity, it was suggested 456 that these specific moments are responsible for functional connectivity measured over the 457 timeseries (Esfahlani et al., 2020). From a research perspective, this would make them an 458 excellent temporal target for investigating the neural mechanism of FC.

459

In this work, we show that while events do match static FC well, they are not discrete markers for it. When they are discarded, static FC structure is still strongly present in the remaining time points. Further, there is a gradual and increasing relationship between cofluctuation amplitude and FC where many points (at least 50%) have a strong relationship with static FC. These results suggest that events by themselves do not (mechanistically)¹ drive FC and it is unlikely there is a unique physiological event happening at high cofluctuation points which is creating the

466 FC matrix. Given these observations, we consider it unlikely that investigating the unique

temporal physiological activity coincident with events would glean additional new information

about the physiologic origins of FC, beyond what might be seen at other timepoints as well.

However, as events show a very strong relationship to FC structure, it is possible that their

470 study may prove useful for denoising and analysis, to provide a higher signal to noise ratio for

- investigations of simultaneous BOLD and direct neural recordings.
- 472

473 Relationship between events and static vs. dynamic functional connectivity

474 Interpretation of events largely depends on one's perspective about the temporal nature of FC. 475 As has been summarized elsewhere (Lurie et al., 2020), there are two dominant perspectives 476 on this topic. One perspective posits that functional connectivity exhibits meaningful temporal 477 dynamics on a moment to moment basis which could represent differences in neural 478 interactions related to ongoing cognition and task processing (Calhoun et al., 2014; R. M. 479 Hutchison et al., 2013; Lurie et al., 2020). This view is supported by the fact that there are 480 transient BOLD responses to tasks (Bandettini et al., 1992; Kwong et al., 1992; Ogawa et al., 481 1992), that states can be found in resting-state FC data at second and minute time scales using 482 sliding windows or instantaneous coactivation patterns (Allen et al., 2014; Chang & Glover, 483 2010; Petridou et al., 2013; Shakil et al., 2016), and that changes in state properties have been 484 linked to task behavior, ongoing cognition, and arousal (Chang et al., 2016; Gonzalez-Castillo et 485 al., 2015; M. R. Hutchison et al., 2013; Kucyi & Davis, 2014; Kupis et al., 2021; Sadaghiani et 486 al., 2015; Tagliazucchi & Laufs, 2014) as well as more stable measures of cognitive/behavioral 487 traits and psychiatric disease (Damaraju et al., 2014; de Lacy et al., 2017; Liégeois et al., 2019;

Rashid et al., 2016). From this perspective, static FC is less significant than its constituent parts.

489

¹ Events do not appear to drive FC in a unique way but do contribute the most to FC estimates as a mathematical necessity of their definition and relationship with correlation.

490 The second perspective posits FC is temporally stable and primarily reflects a history of co-491 activation between regions (Laumann & Snyder, 2021). This is supported by evidence that 492 functional connectivity patterns are consistent within people over sessions (Gratton et al., 2018; 493 Laumann et al., 2015), only slightly altered during tasks (Cole et al., 2014; Gratton et al., 2016, 494 2018), and present in anesthesia (Mhuircheartaigh et al., 2010) and slow wave sleep (Sämann 495 et al., 2011). This perspective emphasizes that resting state FC patterns are only a weak 496 marker of ongoing cognition, and are instead more related to stable neuroanatomical 497 constraints, homeostatic processes, and learning related adaptations (Laumann & Snyder, 498 2021). This perspective collides with the previous one in that it suggests that the dynamic states 499 found during rest² may be explained by sampling variability, motion artifacts, and arousal (Hindriks et al., 2016; Hlinka & Hadrava, 2015b; Laumann et al., 2017; Liégeois et al., 2017) 500 501 rather than current cognitive content or information processing. From this second perspective, 502 the focus of resting state analysis is on finding a clean and reliable static FC measure that may 503 be informative about brain organization.

504

505 The information held in events, then, largely depends on which perspective one takes. From a 506 dynamic FC states perspective, events help identify states and characterize their properties in a 507 more temporally specific way. Indeed, events have been used to identify states within resting 508 state fMRI (Sporns et al., 2021), states that differentiate people (Jo et al., 2021) and states 509 related to variation in hormone concentrations within individuals across days (Greenwell et al., 510 2021). However, from a static FC perspective, events may instead reflect moments of randomly 511 good representation of the static FC structure. From this view, the previous results could be 512 interpreted as occurring because events are particularly good timepoints for identifying stable 513 differences between people and stable static network structure that is relevant to hormonal 514 neurobiology.

515

516 Consistent with our findings, Novelli and Razi recently showed that many of the results of edge 517 functional connectivity (eFC), including the presence of high amplitude cofluctuations, can be 518 derived from static FC alone (Novelli & Razi, 2021). We showed in this current work that 519 presence of events and the gradual relationship between cofluctuation and static FC is 520 predictable from static FC too. While a more extended discussion of dynamic FC is outside the 521 scope of this work, the results shown suggest that static FC and sampling variability are 522 sufficient to explain the properties of high cofluctuation timepoints during rest reported so far. 523 This work alone does not eliminate the possibility of multiple diverse states within resting state 524 FC. Other modeling work has shown that events arise from biophysical models built on 525 structural connectivity and simulated spontaneous BOLD signal dynamics (Pope et al., 2021). 526 However, the present work provides a parsimonious explanation for how events could arise 527 from a stationary but noisy signal. We echo Novelli and Razi in our interest in future explorations 528 of edge FC features which cannot be explained by static FC (Novelli & Razi, 2021). 529

530 Practical considerations for fMRI functional connectivity analysis

Beyond fundamental neurophysiological concerns related to FC, events could be useful for a range of practical applications in FC analysis. First, we wondered if events could be used to define a filter for data points particularly suited to FC analysis. And second, given that events are good at recapitulating static FC, we wondered if it would be possible to reduce data collection by inducing more event-like time points.

² Significant differences in dynamic FC states are seen with tasks, but they tend to be relatively small (Cole et al., 2014; Gratton et al., 2018; Laumann et al., 2017).

537 Traditionally, resting state FC analyses try to isolate relevant signal by identifying and extracting 538 known artifacts (motion, respiration, etc.) and presuming the residual data is all equally useful 539 (Power et al., 2020). Esfahlani and colleagues' result was particularly exciting because it 540 suggested that, after addressing artifacts, the remaining data varied in utility for defining FC 541 structure, with events providing a means to isolate the particularly useful components (Esfahlani 542 et al., 2020). Although in this paper we showed that events can be explained as a consequence 543 of sampling variability on static FC, this does not rule out that they may be a useful analytical 544 tool. In fact, recent work has shown that ETS (edge-time-series) are better at identifying 545 individuals than static FC (Jo et al., 2021). The strategy of seeking out points with maximal 546 network information as a 'denoising' strategy is a paradigm shift in fMRI FC analysis and could 547 be an exciting avenue of future study.

548

549 The second question is whether the fact that events can recapitulate FC with few timepoints 550 suggests that FC may be effectively measured through much shorter data collection regimes. It 551 has become evident in recent years that it is possible to study functional brain organization at 552 the individual level if enough data is collected (Braga & Buckner, 2017; Gordon et al., 2017; 553 Laumann et al., 2015; Noble et al., 2017), with most papers suggesting more than 30 minutes of 554 high guality resting-state data is needed to measure static cortical FC reliably. This has 555 motivated significant ongoing efforts to collect large amounts of individual 'precision' data 556 (Fedorenko, 2021; Gratton & Braga, 2021; Naselaris et al., 2021; Pritschet et al., 2021) which 557 have led to novel findings, but are costly and time-intensive, and may be difficult to acquire in 558 clinical or pediatric populations. We wondered if, because events contain more network 559 structure information than other time points, one could decrease data collection by increasing 560 the rate of events and focusing analysis solely on those moments. However, the results in this 561 manuscript suggest that event correspondence to static FC can be explained by sampling 562 variability and spaced sampling - suggesting it would be difficult to ensure a high proportion of 563 events in a short amount of data collection time. We are optimistic about new strategies for 564 decreasing data collection needs such as new MRI techniques (Lynch et al., 2020) and efforts 565 to reduce artifacts (Power et al., 2020) to address these continued issues in fMRI data 566 collection.

567 568 Limitations

569 We will close by noting some limitations in this work and opportunities for future research. First. 570 we used a dataset collected from a small number of individuals. However, we showed that the 571 results were very similar across each participant and sessions within participants (Fig. S1). 572 suggesting robustness in these results. Second, when simulating BOLD data, we used a very 573 simple model which accounted only for spatial correlation and included no BOLD-like temporal 574 features (e.g., autocorrelation, matched spectral structure) (Cordes et al., 2001; He et al., 2010; 575 Liégeois et al., 2021; Zarahn et al., 1997). However, this simple model still was able to produce 576 event-like behavior, as was an even simpler toy model from sine-waves (Fig. S4). That even 577 such simple models showed event-like behavior suggests that events arise based on simple 578 properties of the BOLD timeseries. Third, we focused on resting-state fMRI data in this 579 manuscript, rather than data from task sessions. We are curious about the effects of tasks on 580 BOLD cofluctuation: given that arousal and tasks can create real non-stationarities in BOLD 581 data, we consider it possible that tasks and imposed states could change the prevalence and 582 structure of events (Betzel et al., 2020; Cole et al., 2014; Gratton et al., 2016, 2018; Laumann et 583 al., 2017; Tagliazucchi & Laufs, 2014). Future work will be needed to fully explore this issue. 584

585 Conclusions

586 In this work, we investigated high cofluctuation BOLD events and found evidence suggesting

587 that, rather than events behaving as unique discrete timepoints that drive functional

- 588 connectivity, events may arise as an expected byproduct of a static functional network structure.
- 589 Event recapitulation of network structure was not unique, but varied continuously across
- 590 timepoints in real data, and was present in data from which events had been excluded.
- 591 Simulations demonstrated similar responses from stationary signals. Finally, one of the primary
- 592 interesting properties of events that they can recreate static FC with a few points is not
- 593 unique and is driven in part by sampling rate. These results suggest that events are
- 594 parsimoniously explained as a consequence of a highly correlated, modular, noisy signal
- 595 (BOLD) and therefore might be better suited as methods for identifying good representations of
- 596 static network structure than as a tool to investigate the mechanistic sources of functional 597 connectivity.
- 598

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- 606 Technology.
- 607

608 DECLARATIONS OF COMPETING INTERESTS

609 None 610

611 CITATION DIVERSITY STATEMENT

612 Recent work in several fields of science has identified a bias in citation practices such that 613 papers from women and other minority scholars are under-cited relative to the number of such 614 papers in the field (Bertolero et al., 2020; Caplar et al., 2017; Chatterjee & Werner, 2021; Dion 615 et al., 2018; Dworkin et al., 2020; Fulvio et al., 2021; Maliniak et al., 2013; Mitchell et al., 2013; 616 Wang et al., 2021). Here we sought to proactively consider choosing references that reflect the 617 diversity of the field in thought, form of contribution, gender, race, ethnicity, and other factors. 618 First, we obtained the predicted gender of the first and last author of each reference by using 619 databases that store the probability of a first name being carried by a woman (Dworkin et al., 620 2020; Zhou et al., 2020).By this measure (and excluding self-citations to the first and last 621 authors of our current paper), our references contain 7.04% woman(first)/woman(last), 11.27% 622 man/woman, 19.72% woman/man, and 61.97% man/man. This method is limited in that a) 623 names, pronouns, and social media profiles used to construct the databases may not, in every 624 case, be indicative of gender identity and b) it cannot account for intersex, non-binary, or 625 transgender people. Second, we obtained predicted racial/ethnic category of the first and last 626 author of each reference by databases that store the probability of a first and last name being 627 carried by an author of color (Ambekar et al., 2009; Sood & Laohaprapanon, 2018). By this 628 measure (and excluding self-citations), our references contain 8.93% author of color 629 (first)/author of color(last), 12.55% white author/author of color, 28.74% author of color/white 630 author, and 49.78% white author/white author. This method is limited in that a) names and 631 Florida Voter Data to make the predictions may not be indicative of racial/ethnic identity, and b) 632 it cannot account for Indigenous and mixed-race authors, or those who may face differential 633 biases due to the ambiguous racialization or ethnicization of their names. We look forward to 634 future work that could help us to better understand how to support equitable practices in

- 635 science.
- 636
- 637 **REFERENCES**

- Allen, E. A., Damaraju, E., Plis, S. M., Erhardt, E. B., Eichele, T., & Calhoun, V. D. (2014).
 Tracking whole-brain connectivity dynamics in the resting state. *Cerebral Cortex (New York, N.Y.: 1991)*, 24(3), 663–676. https://doi.org/10.1093/cercor/bhs352
- Ambekar, A., Ward, C., Mohammed, J., Male, S., & Skiena, S. (2009). Name-ethnicity
 classification from open sources. *Proceedings of the 15th ACM SIGKDD International Conference on Knowledge Discovery and Data Mining*, 49–58.
 https://doi.org/10.1145/1557019.1557032
- Bandettini, P. A., Wong, E. C., Hinks, R. S., Tikofsky, R. S., & Hyde, J. S. (1992). Time course
 EPI of human brain function during task activation. *Magnetic Resonance in Medicine*,
 25(2), 390–397. https://doi.org/10.1002/mrm.1910250220
- Bertolero, M., Dworkin, J., David, S., Lloreda, C. L., Srivastava, P., Stiso, J., Zhou, D., Dzirasa,
 K., Fair, D., Kaczkurkin, A., Marlin, B. J., Shohamy, D., Uddin, L., Zurn, P., & Bassett, D.
 (2020). Racial and ethnic imbalance in neuroscience reference lists and intersections
 with gende. https://doi.org/10.1101/2020.10.12.336230
- Betzel, R. F., Byrge, L., Esfahlani, F. Z., & Kennedy, D. P. (2020). Temporal fluctuations in the
 brain's modular architecture during movie-watching. *NeuroImage*, *213*, 116687.
 https://doi.org/10.1016/j.neuroimage.2020.116687
- Bijsterbosch, J. D., Woolrich, M. W., Glasser, M. F., Robinson, E. C., Beckmann, C. F., Van
 Essen, D. C., Harrison, S. J., & Smith, S. M. (2018). The relationship between spatial
 configuration and functional connectivity of brain regions. *ELife*, 7, e32992.
 https://doi.org/10.7554/eLife.32992
- Biswal, B., Yetkin, F. Z., Haughton, V. M., & Hyde, J. S. (1995). Functional connectivity in the
 motor cortex of resting human brain using echo-planar MRI. *Magnetic Resonance in Medicine*, *34*(4), 537–541. https://doi.org/10.1002/mrm.1910340409
- Braga, R. M., & Buckner, R. L. (2017). Parallel Interdigitated Distributed Networks within the
 Individual Estimated by Intrinsic Functional Connectivity. *Neuron*, *95*(2), 457-471.e5.
 https://doi.org/10.1016/j.neuron.2017.06.038
- Braga, R. M., DiNicola, L. M., Becker, H. C., & Buckner, R. L. (2020). Situating the leftlateralized language network in the broader organization of multiple specialized largescale distributed networks. *Journal of Neurophysiology*, *124*(5), 1415–1448.
 https://doi.org/10.1152/jn.00753.2019
- Calhoun, V. D., Miller, R., Pearlson, G., & Adalı, T. (2014). The chronnectome: Time-varying
 connectivity networks as the next frontier in fMRI data discovery. *Neuron*, *84*(2), 262–
 274. https://doi.org/10.1016/j.neuron.2014.10.015
- 672 Caplar, N., Tacchella, S., & Birrer, S. (2017). Quantitative evaluation of gender bias in
 673 astronomical publications from citation counts. *Nature Astronomy*, 1(6), 0141.
 674 https://doi.org/10.1038/s41550-017-0141
- 675 Chang, C., & Glover, G. H. (2010). Time–frequency dynamics of resting-state brain connectivity
 676 measured with fMRI. *NeuroImage*, *50*(1), 81–98.
 677 https://doi.org/10.1016/j.neuroimage.2009.12.011
- Chang, C., Leopold, D. A., Schölvinck, M. L., Mandelkow, H., Picchioni, D., Liu, X., Ye, F. Q.,
 Turchi, J. N., & Duyn, J. H. (2016). Tracking brain arousal fluctuations with fMRI. *Proceedings of the National Academy of Sciences*, *113*(16), 4518–4523.
 https://doi.org/10.1073/pnas.1520613113
- Chatterjee, P., & Werner, R. M. (2021). Gender Disparity in Citations in High-Impact Journal
 Articles. JAMA Network Open, 4(7), e2114509.
- 684 https://doi.org/10.1001/jamanetworkopen.2021.14509
- Cole, M. W., Bassett, D. S., Power, J. D., Braver, T. S., & Petersen, S. E. (2014). Intrinsic and
 task-evoked network architectures of the human brain. *Neuron*, *83*(1), 238–251.
 https://doi.org/10.1016/j.neuron.2014.05.014

- Cordes, D., Haughton, V. M., Arfanakis, K., Carew, J. D., Turski, P. A., Moritz, C. H., Quigley,
 M. A., & Meyerand, E. (2001). Frequencies contributing to functional connectivity in the
 cerebral cortex in "resting-state" data. *AJNR. American Journal of Neuroradiology*, 22(7),
 1326–1333.
- Dale, A. M., Fischl, B., & Sereno, M. I. (1999). Cortical Surface-Based Analysis: I. Segmentation
 and Surface Reconstruction. *NeuroImage*, 9(2), 179–194.
 https://doi.org/10.1006/nimg.1998.0395
- Damaraju, E., Allen, E. A., Belger, A., Ford, J. M., McEwen, S., Mathalon, D. H., Mueller, B. A.,
 Pearlson, G. D., Potkin, S. G., Preda, A., Turner, J. A., Vaidya, J. G., van Erp, T. G., &
 Calhoun, V. D. (2014). Dynamic functional connectivity analysis reveals transient states
 of dysconnectivity in schizophrenia. *NeuroImage: Clinical*, *5*, 298–308.
 https://doi.org/10.1016/j.nicl.2014.07.003
- de Lacy, N., Doherty, D., King, B. H., Rachakonda, S., & Calhoun, V. D. (2017). Disruption to
 control network function correlates with altered dynamic connectivity in the wider autism
 spectrum. *NeuroImage. Clinical*, *15*, 513–524. https://doi.org/10.1016/j.nicl.2017.05.024
- Dion, M. L., Sumner, J. L., & Mitchell, S. M. L. (2018). Gendered Citation Patterns across
 Political Science and Social Science Methodology Fields. *Political Analysis*, 26(3), 312– 327. https://doi.org/10.1017/pan.2018.12
- Dworkin, J. D., Linn, K. A., Teich, E. G., Zurn, P., Shinohara, R. T., & Bassett, D. S. (2020). The
 extent and drivers of gender imbalance in neuroscience reference lists. *Nature Neuroscience*. 23(8). 918–926. https://doi.org/10.1038/s41593-020-0658-v
- Esfahlani, F. Z., Byrge, L., Tanner, J., Sporns, O., Kennedy, D. P., & Betzel, R. F. (2021). Edge *centric analysis of time-varying functional brain networks with applications in autism spectrum disorder* (p. 2021.07.01.450812). https://doi.org/10.1101/2021.07.01.450812
- Esfahlani, F. Z., Jo, Y., Faskowitz, J., Byrge, L., Kennedy, D. P., Sporns, O., & Betzel, R. F.
 (2020). High-amplitude cofluctuations in cortical activity drive functional connectivity. *Proceedings of the National Academy of Sciences of the United States of America*,
 117(45), 28393–28401. https://doi.org/10.1073/pnas.2005531117
- Fair, D. A., Miranda-Dominguez, O., Snyder, A. Z., Perrone, A., Earl, E. A., Van, A. N., Koller, J.
 M., Feczko, E., Tisdall, M. D., van der Kouwe, A., Klein, R. L., Mirro, A. E., Hampton, J.
 M., Adeyemo, B., Laumann, T. O., Gratton, C., Greene, D. J., Schlaggar, B. L., Hagler,
 D. J., ... Dosenbach, N. U. F. (2020). Correction of respiratory artifacts in MRI head
 motion estimates. *NeuroImage*, *208*, 116400.
- 721 https://doi.org/10.1016/j.neuroimage.2019.116400
- Fedorenko, E. (2021). The early origins and the growing popularity of the individual-subject
 analytic approach in human neuroscience. *Current Opinion in Behavioral Sciences*, 40,
 105–112. https://doi.org/10.1016/j.cobeha.2021.02.023
- Fulvio, J. M., Akinnola, I., & Postle, B. R. (2021). Gender (Im)balance in Citation Practices in
 Cognitive Neuroscience. *Journal of Cognitive Neuroscience*, *33*(1), 3–7.
 https://doi.org/10.1162/jocn a 01643
- Glasser, M. F., Sotiropoulos, S. N., Wilson, J. A., Coalson, T. S., Fischl, B., Andersson, J. L.,
 Xu, J., Jbabdi, S., Webster, M., Polimeni, J. R., Van Essen, D. C., & Jenkinson, M.
 (2013). The minimal preprocessing pipelines for the Human Connectome Project. *NeuroImage*, 80, 105–124. https://doi.org/10.1016/j.neuroimage.2013.04.127
- Gonzalez-Castillo, J., Hoy, C. W., Handwerker, D. A., Robinson, M. E., Buchanan, L. C., Saad,
 Z. S., & Bandettini, P. A. (2015). Tracking ongoing cognition in individuals using brief,
 whole-brain functional connectivity patterns. *Proceedings of the National Academy of Sciences*, *112*(28), 8762–8767. https://doi.org/10.1073/pnas.1501242112
- Gordon, E. M., Laumann, T. O., Adeyemo, B., Huckins, J. F., Kelley, W. M., & Petersen, S. E.
 (2016). Generation and Evaluation of a Cortical Area Parcellation from Resting-State

738 Correlations. Cerebral Cortex (New York, N.Y.: 1991), 26(1), 288-303. 739 https://doi.org/10.1093/cercor/bhu239 740 Gordon, E. M., Laumann, T. O., Gilmore, A. W., Newbold, D. J., Greene, D. J., Berg, J. J., 741 Ortega, M., Hoyt-Drazen, C., Gratton, C., Sun, H., Hampton, J. M., Coalson, R. S., 742 Nguyen, A. L., McDermott, K. B., Shimony, J. S., Snyder, A. Z., Schlaggar, B. L., 743 Petersen, S. E., Nelson, S. M., & Dosenbach, N. U. F. (2017). Precision Functional 744 Mapping of Individual Human Brains. Neuron, 95(4), 791-807.e7. 745 https://doi.org/10.1016/j.neuron.2017.07.011 746 Gratton, C., & Braga, R. M. (2021). Editorial overview: Deep imaging of the individual brain: 747 past, practice, and promise. Current Opinion in Behavioral Sciences, 40, iii-vi. 748 https://doi.org/10.1016/i.cobeha.2021.06.011 749 Gratton, C., Laumann, T. O., Gordon, E. M., Adeyemo, B., & Petersen, S. E. (2016). Evidence 750 for Two Independent Factors that Modify Brain Networks to Meet Task Goals. Cell 751 Reports, 17(5), 1276–1288. https://doi.org/10.1016/j.celrep.2016.10.002 752 Gratton, C., Laumann, T. O., Nielsen, A. N., Greene, D. J., Gordon, E. M., Gilmore, A. W., 753 Nelson, S. M., Coalson, R. S., Snyder, A. Z., Schlaggar, B. L., Dosenbach, N. U. F., & 754 Petersen, S. E. (2018). Functional Brain Networks Are Dominated by Stable Group and 755 Individual Factors, Not Cognitive or Daily Variation. Neuron, 98(2), 439-452.e5. 756 https://doi.org/10.1016/j.neuron.2018.03.035 757 Greenwell, S., Faskowitz, J., Pritschet, L., Santander, T., Jacobs, E. G., & Betzel, R. F. (2021a). 758 High-amplitude network co-fluctuations linked to variation in hormone concentrations 759 over menstrual cycle (p. 2021.07.29.453892). https://doi.org/10.1101/2021.07.29.453892 760 Greenwell, S., Faskowitz, J., Pritschet, L., Santander, T., Jacobs, E. G., & Betzel, R. F. (2021b). 761 High-amplitude network co-fluctuations linked to variation in hormone concentrations 762 over menstrual cycle (p. 2021.07.29.453892). https://doi.org/10.1101/2021.07.29.453892 763 He, B. J., Zempel, J. M., Snyder, A. Z., & Raichle, M. E. (2010). The temporal structures and 764 functional significance of scale-free brain activity. Neuron, 66(3), 353-369. 765 https://doi.org/10.1016/j.neuron.2010.04.020 Heeger, D. J., Huk, A. C., Geisler, W. S., & Albrecht, D. G. (2000). Spikes versus BOLD: What 766 767 does neuroimaging tell us about neuronal activity? Nature Neuroscience, 3(7), 631-633. 768 https://doi.org/10.1038/76572 769 Hindriks, R., Adhikari, M. H., Murayama, Y., Ganzetti, M., Mantini, D., Logothetis, N. K., & Deco, 770 G. (2016). Can sliding-window correlations reveal dynamic functional connectivity in 771 resting-state fMRI? NeuroImage, 127, 242-256. 772 https://doi.org/10.1016/i.neuroimage.2015.11.055 773 Hlinka, J., & Hadrava, M. (2015a). On the danger of detecting network states in white noise. 774 Frontiers in Computational Neuroscience, 9, 11. 775 https://doi.org/10.3389/fncom.2015.00011 776 Hlinka, J., & Hadrava, M. (2015b). On the danger of detecting network states in white noise. 777 Frontiers in Computational Neuroscience, 9, 11. 778 https://doi.org/10.3389/fncom.2015.00011 779 Honey, C. J., Sporns, O., Cammoun, L., Gigandet, X., Thiran, J. P., Meuli, R., & Hagmann, P. 780 (2009). Predicting human resting-state functional connectivity from structural 781 connectivity. Proceedings of the National Academy of Sciences, 106(6), 2035-2040. 782 https://doi.org/10.1073/pnas.0811168106 783 Hutchison, M. R., Womelsdorf, T., Gati, J. S., Everling, S., & Menon, R. S. (2013). Resting-state 784 networks show dynamic functional connectivity in awake humans and anesthetized 785 macagues. Human Brain Mapping, 34(9), 2154–2177. 786 https://doi.org/10.1002/hbm.22058 787 Hutchison, R. M., Womelsdorf, T., Allen, E. A., Bandettini, P. A., Calhoun, V. D., Corbetta, M., 788 Della Penna, S., Duyn, J. H., Glover, G. H., Gonzalez-Castillo, J., Handwerker, D. A.,

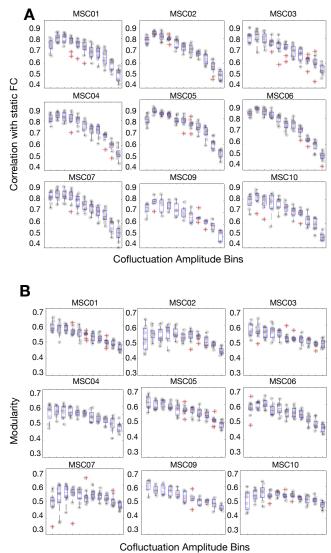
789 Keilholz, S., Kiviniemi, V., Leopold, D. A., de Pasquale, F., Sporns, O., Walter, M., & 790 Chang, C. (2013). Dynamic functional connectivity: Promise, issues, and interpretations. 791 NeuroImage, 80, 360-378. https://doi.org/10.1016/j.neuroimage.2013.05.079 792 Jo, Y., Faskowitz, J., Esfahlani, F. Z., Sporns, O., & Betzel, R. F. (2021). Subject identification 793 using edge-centric functional connectivity. NeuroImage, 238, 118204. 794 https://doi.org/10.1016/j.neuroimage.2021.118204 795 Johnston, J. M., Vaishnavi, S. N., Smyth, M. D., Zhang, D., He, B. J., Zempel, J. M., Shimony, J. 796 S., Snyder, A. Z., & Raichle, M. E. (2008). Loss of Resting Interhemispheric Functional 797 Connectivity after Complete Section of the Corpus Callosum. Journal of Neuroscience, 798 28(25), 6453-6458. https://doi.org/10.1523/JNEUROSCI.0573-08.2008 799 Kong, R., Li, J., Orban, C., Sabuncu, M. R., Liu, H., Schaefer, A., Sun, N., Zuo, X.-N., Holmes, 800 A. J., Eickhoff, S. B., & Yeo, B. T. T. (2019). Spatial Topography of Individual-Specific 801 Cortical Networks Predicts Human Cognition, Personality, and Emotion. Cerebral Cortex 802 (New York, N.Y.: 1991), 29(6), 2533–2551. https://doi.org/10.1093/cercor/bhy123 803 Kucyi, A., & Davis, K. D. (2014). Dynamic functional connectivity of the default mode network 804 tracks daydreaming. NeuroImage, 100, 471-480. 805 https://doi.org/10.1016/j.neuroimage.2014.06.044 Kupis, L., Goodman, Z. T., Kornfeld, S., Hoang, S., Romero, C., Dirks, B., Dehoney, J., Chang, 806 807 C., Spreng, R. N., Nomi, J. S., & Uddin, L. Q. (2021). Brain Dynamics Underlying 808 Cognitive Flexibility Across the Lifespan. Cerebral Cortex, 31(11), 5263-5274. 809 https://doi.org/10.1093/cercor/bhab156 810 Kwong, K. K., Belliveau, J. W., Chesler, D. A., Goldberg, I. E., Weisskoff, R. M., Poncelet, B. P., 811 Kennedy, D. N., Hoppel, B. E., Cohen, M. S., & Turner, R. (1992). Dynamic magnetic 812 resonance imaging of human brain activity during primary sensory stimulation. 813 Proceedings of the National Academy of Sciences, 89(12), 5675–5679. 814 https://doi.org/10.1073/pnas.89.12.5675 815 Laumann, T. O., Gordon, E. M., Adeyemo, B., Snyder, A. Z., Joo, S. J., Chen, M.-Y., Gilmore, 816 A. W., McDermott, K. B., Nelson, S. M., Dosenbach, N. U. F., Schlaggar, B. L., Mumford, J. A., Poldrack, R. A., & Petersen, S. E. (2015). Functional System and Areal 817 818 Organization of a Highly Sampled Individual Human Brain. Neuron, 87(3), 657–670. 819 https://doi.org/10.1016/j.neuron.2015.06.037 820 Laumann, T. O., & Snyder, A. Z. (2021). Brain activity is not only for thinking. Current Opinion in 821 Behavioral Sciences, 40, 130-136. https://doi.org/10.1016/j.cobeha.2021.04.002 822 Laumann, T. O., Snyder, A. Z., Mitra, A., Gordon, E. M., Gratton, C., Adeyemo, B., Gilmore, A. 823 W., Nelson, S. M., Berg, J. J., Greene, D. J., McCarthy, J. E., Tagliazucchi, E., Laufs, H., 824 Schlaggar, B. L., Dosenbach, N. U. F., & Petersen, S. E. (2017). On the Stability of 825 BOLD fMRI Correlations. Cerebral Cortex (New York, N.Y.: 1991), 27(10), 4719–4732. 826 https://doi.org/10.1093/cercor/bhw265 827 Liégeois, R., Laumann, T. O., Snyder, A. Z., Zhou, J., & Yeo, B. T. T. (2017). Interpreting 828 temporal fluctuations in resting-state functional connectivity MRI. NeuroImage, 163, 829 437–455. https://doi.org/10.1016/j.neuroimage.2017.09.012 830 Liégeois, R., Li, J., Kong, R., Orban, C., Van De Ville, D., Ge, T., Sabuncu, M. R., & Yeo, B. T. 831 T. (2019). Resting brain dynamics at different timescales capture distinct aspects of 832 human behavior. Nature Communications, 10(1), 2317. https://doi.org/10.1038/s41467-833 019-10317-7 834 Liégeois, R., Yeo, B. T. T., & Van De Ville, D. (2021). Interpreting null models of resting-state 835 functional MRI dynamics: Not throwing the model out with the hypothesis. *NeuroImage*, 836 243, 118518. https://doi.org/10.1016/j.neuroimage.2021.118518 837 Logothetis, N. K., Pauls, J., Augath, M., Trinath, T., & Oeltermann, A. (2001). 838 Neurophysiological investigation of the basis of the fMRI signal. Nature, 412(6843), 150-839 157. https://doi.org/10.1038/35084005

- Lurie, D. J., Kessler, D., Bassett, D. S., Betzel, R. F., Breakspear, M., Kheilholz, S., Kucyi, A.,
 Liégeois, R., Lindquist, M. A., McIntosh, A. R., Poldrack, R. A., Shine, J. M., Thompson,
 W. H., Bielczyk, N. Z., Douw, L., Kraft, D., Miller, R. L., Muthuraman, M., Pasquini, L., ...
 Calhoun, V. D. (2020). Questions and controversies in the study of time-varying
 functional connectivity in resting fMRI. *Network Neuroscience (Cambridge, Mass.)*, 4(1),
 30–69. https://doi.org/10.1162/netn a 00116
- Lynch, C. J., Power, J. D., Scult, M. A., Dubin, M., Gunning, F. M., & Liston, C. (2020). Rapid
 Precision Functional Mapping of Individuals Using Multi-Echo fMRI. *Cell Reports*, 33(12),
 108540. https://doi.org/10.1016/j.celrep.2020.108540
- Maliniak, D., Powers, R., & Walter, B. F. (2013). The Gender Citation Gap in International
 Relations. *International Organization*, 67(4), 889–922.
 https://doi.org/10.1017/S0020818313000209
- Marcus, D. S., Harwell, J., Olsen, T., Hodge, M., Glasser, M. F., Prior, F., Jenkinson, M.,
 Laumann, T., Curtiss, S. W., & Van Essen, D. C. (2011). Informatics and data mining
 tools and strategies for the human connectome project. *Frontiers in Neuroinformatics*, 5.
 Scopus. https://doi.org/10.3389/fninf.2011.00004
- Mhuircheartaigh, R. N., Rosenorn-Lanng, D., Wise, R., Jbabdi, S., Rogers, R., & Tracey, I.
 (2010). Cortical and subcortical connectivity changes during decreasing levels of
 consciousness in humans: A functional magnetic resonance imaging study using
 propofol. *The Journal of Neuroscience: The Official Journal of the Society for Neuroscience*, 30(27), 9095–9102, https://doi.org/10.1523/JNEUROSCI.5516-09.2010
- Mitchell, S. M., Lange, S., & Brus, H. (2013). Gendered Citation Patterns in International
 Relations Journals. *International Studies Perspectives*, *14*(4), 485–492.
 https://doi.org/10.1111/insp.12026
- Naselaris, T., Allen, E., & Kay, K. (2021). Extensive sampling for complete models of individual
 brains. *Current Opinion in Behavioral Sciences*, 40, 45–51.
 https://doi.org/10.1016/j.cobeha.2020.12.008
- Newman, M., & Girvan, M. (2004). Finding and evaluating community structure in networks.
 Physical Review E, 69(2), 026113. https://doi.org/10.1103/PhysRevE.69.026113
- Nir, Y., Mukamel, R., Dinstein, I., Privman, E., Harel, M., Fisch, L., Gelbard-Sagiv, H.,
 Kipervasser, S., Andelman, F., Neufeld, M. Y., Kramer, U., Arieli, A., Fried, I., & Malach,
 R. (2008). Interhemispheric correlations of slow spontaneous neuronal fluctuations
 revealed in human sensory cortex. *Nature Neuroscience*, *11*(9), 1100–1108.
 https://doi.org/10.1038/nn.2177
- Noble, S., Spann, M. N., Tokoglu, F., Shen, X., Constable, R. T., & Scheinost, D. (2017).
 Influences on the Test-Retest Reliability of Functional Connectivity MRI and its
 Relationship with Behavioral Utility. *Cerebral Cortex (New York, N.Y.: 1991)*, 27(11),
 5415–5429. https://doi.org/10.1093/cercor/bhx230
- Novelli, L., & Razi, A. (2021). A mathematical perspective on edge-centric functional
 connectivity. *ArXiv:2106.10631 [Physics, q-Bio]*. http://arxiv.org/abs/2106.10631
- Ogawa, S., Tank, D. W., Menon, R., Ellermann, J. M., Kim, S. G., Merkle, H., & Ugurbil, K.
 (1992). Intrinsic signal changes accompanying sensory stimulation: Functional brain
 mapping with magnetic resonance imaging. *Proceedings of the National Academy of Sciences*, 89(13), 5951–5955. https://doi.org/10.1073/pnas.89.13.5951
- Petridou, N., Gaudes, C. C., Dryden, I. L., Francis, S. T., & Gowland, P. A. (2013). Periods of
 rest in fMRI contain individual spontaneous events which are related to slowly fluctuating
 spontaneous activity. *Human Brain Mapping*, *34*(6), 1319–1329.
 https://doi.org/10.1002/hbm.21513
- Pope, M., Fukushima, M., Betzel, R. F., & Sporns, O. (2021). *Modular origins of high-amplitude co-fluctuations in fine-scale functional connectivity dynamics* [Preprint]. Neuroscience.
 https://doi.org/10.1101/2021.05.16.444357

891 Power, J. D., Cohen, A. L., Nelson, S. M., Wig, G. S., Barnes, K. A., Church, J. A., Vogel, A. C., 892 Laumann, T. O., Miezin, F. M., Schlaggar, B. L., & Petersen, S. E. (2011). Functional 893 network organization of the human brain. Neuron, 72(4), 665–678. 894 https://doi.org/10.1016/j.neuron.2011.09.006 895 Power, J. D., Lynch, C. J., Adeyemo, B., & Petersen, S. E. (2020). A Critical, Event-Related 896 Appraisal of Denoising in Resting-State fMRI Studies. Cerebral Cortex (New York, N.Y.: 897 1991), 30(10), 5544-5559. https://doi.org/10.1093/cercor/bhaa139 898 Power, J. D., Mitra, A., Laumann, T. O., Snyder, A. Z., Schlaggar, B. L., & Petersen, S. E. 899 (2014). Methods to detect, characterize, and remove motion artifact in resting state fMRI. 900 NeuroImage, 84, 320-341. https://doi.org/10.1016/j.neuroimage.2013.08.048 901 Pritschet, L., Taylor, C. M., Santander, T., & Jacobs, E. G. (2021). Applying dense-sampling 902 methods to reveal dynamic endocrine modulation of the nervous system. Current 903 Opinion in Behavioral Sciences, 40, 72–78. https://doi.org/10.1016/j.cobeha.2021.01.012 904 Rashid, B., Arbabshirani, M. R., Damaraju, E., Cetin, M. S., Miller, R., Pearlson, G. D., & 905 Calhoun, V. D. (2016). Classification of schizophrenia and bipolar patients using static 906 and dynamic resting-state fMRI brain connectivity. NeuroImage, 134, 645-657. 907 https://doi.org/10.1016/j.neuroimage.2016.04.051 908 Sadaghiani, S., Poline, J.-B., Kleinschmidt, A., & D'Esposito, M. (2015). Ongoing dynamics in 909 large-scale functional connectivity predict perception. Proceedings of the National 910 Academy of Sciences, 112(27), 8463–8468. https://doi.org/10.1073/pnas.1420687112 Sämann, P. G., Wehrle, R., Hoehn, D., Spoormaker, V. I., Peters, H., Tully, C., Holsboer, F., & 911 912 Czisch, M. (2011). Development of the brain's default mode network from wakefulness 913 to slow wave sleep. Cerebral Cortex (New York, N.Y.: 1991), 21(9), 2082-2093. 914 https://doi.org/10.1093/cercor/bhg295 915 Seitzman, B. A., Gratton, C., Laumann, T. O., Gordon, E. M., Adevemo, B., Dworetsky, A., 916 Kraus, B. T., Gilmore, A. W., Berg, J. J., Ortega, M., Nguyen, A., Greene, D. J., 917 McDermott, K. B., Nelson, S. M., Lessov-Schlaggar, C. N., Schlaggar, B. L., Dosenbach, 918 N. U. F., & Petersen, S. E. (2019). Trait-like variants in human functional brain networks. 919 Proceedings of the National Academy of Sciences, 116(45), 22851–22861. 920 https://doi.org/10.1073/pnas.1902932116 921 Shakil, S., Lee, C.-H., & Keilholz, S. D. (2016). Evaluation of sliding window correlation 922 performance for characterizing dynamic functional connectivity and brain states. 923 NeuroImage, 133, 111-128. https://doi.org/10.1016/j.neuroimage.2016.02.074 924 Shmuel, A., & Leopold, D. A. (2008). Neuronal correlates of spontaneous fluctuations in fMRI 925 signals in monkey visual cortex: Implications for functional connectivity at rest. Human 926 Brain Mapping, 29(7), 751–761. https://doi.org/10.1002/hbm.20580 927 Smith, S. M., Fox, P. T., Miller, K. L., Glahn, D. C., Fox, P. M., Mackay, C. E., Filippini, N., 928 Watkins, K. E., Toro, R., Laird, A. R., & Beckmann, C. F. (2009). Correspondence of the 929 brain's functional architecture during activation and rest. Proceedings of the National 930 Academy of Sciences, 106(31), 13040–13045. https://doi.org/10.1073/pnas.0905267106 931 Smith, S. M., Nichols, T. E., Vidaurre, D., Winkler, A. M., Behrens, T. E. J., Glasser, M. F., 932 Ugurbil, K., Barch, D. M., Van Essen, D. C., & Miller, K. L. (2015). A positive-negative 933 mode of population covariation links brain connectivity, demographics and behavior. 934 Nature Neuroscience, 18(11), 1565–1567. https://doi.org/10.1038/nn.4125 935 Sood, G., & Laohaprapanon, S. (2018). Predicting Race and Ethnicity From the Sequence of 936 Characters in a Name. ArXiv:1805.02109 [Stat]. http://arxiv.org/abs/1805.02109 937 Sporns, O., Faskowitz, J., Teixeira, A. S., Cutts, S. A., & Betzel, R. F. (2021). Dynamic 938 expression of brain functional systems disclosed by fine-scale analysis of edge time 939 series. Network Neuroscience (Cambridge, Mass.), 5(2), 405–433. 940 https://doi.org/10.1162/netn a 00182

- Tagliazucchi, E., & Laufs, H. (2014). Decoding wakefulness levels from typical fMRI resting state data reveals reliable drifts between wakefulness and sleep. *Neuron*, *82*(3), 695–
 708. https://doi.org/10.1016/j.neuron.2014.03.020
- Tavor, I., Jones, O. P., Mars, R. B., Smith, S. M., Behrens, T. E., & Jbabdi, S. (2016). Task-free
 MRI predicts individual differences in brain activity during task performance. *Science*,
 352(6282), 216–220. https://doi.org/10.1126/science.aad8127
- van den Heuvel, M. P., Stam, C. J., Kahn, R. S., & Hulshoff Pol, H. E. (2009). Efficiency of
 functional brain networks and intellectual performance. *The Journal of Neuroscience: The Official Journal of the Society for Neuroscience*, 29(23), 7619–7624.
 https://doi.org/10.1523/JNEUROSCI.1443-09.2009
- Vincent, J.-L., Patel, G. H., Fox, M. D., Snyder, A. Z., Baker, J. T., Van Essen, D. C., Zempel, J.
 M., Snyder, L. H., Corbetta, M., & Raichle, M. E. (2007). Intrinsic functional architecture
 in the anaesthetized monkey brain. *Nature*, *447*(7140), 83–86.
 https://doi.org/10.1038/nature05758
- Wang, X., Dworkin, J. D., Zhou, D., Stiso, J., Falk, E. B., Bassett, D. S., Zurn, P., & LydonStaley, D. M. (2021). Gendered citation practices in the field of communication. *Annals*of the International Communication Association, 45(2), 134–153.
 https://doi.org/10.1080/23808985.2021.1960180
- Yeo, B. T., Krienen, F. M., Sepulcre, J., Sabuncu, M. R., Lashkari, D., Hollinshead, M., Roffman,
 J. L., Smoller, J. W., Zöllei, L., Polimeni, J. R., Fischl, B., Liu, H., & Buckner, R. L.
 (2011). The organization of the human cerebral cortex estimated by intrinsic functional
 connectivity. *Journal of Neurophysiology*, *106*(3), 1125–1165.
 https://doi.org/10.1152/jn.00338.2011
- Zarahn, E., Aguirre, G. K., & D'Esposito, M. (1997). Empirical analyses of BOLD fMRI statistics.
 I. Spatially unsmoothed data collected under null-hypothesis conditions. *NeuroImage*, 5(3), 179–197. https://doi.org/10.1006/nimg.1997.0263
- 267 Zhou, D., Cornblath, E. J., Stiso, J., Teich, E. G., Dworkin, J. D., Blevins, A. S., & Bassett, D. S.
 268 (2020). *Gender Diversity Statement and Code Notebook v1.0*. Zenodo.
- 969 https://doi.org/10.5281/zenodo.3672110

970 SUPPLEMENTAL INFORMATION

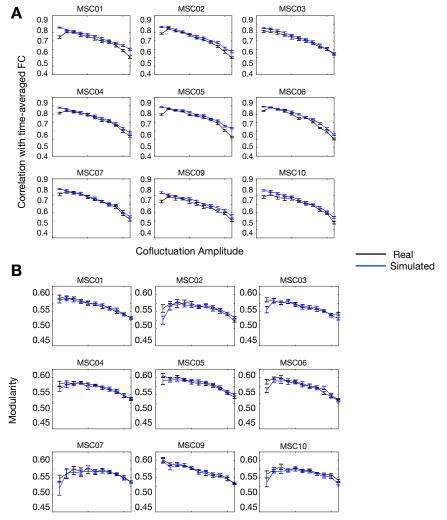


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Fig S1, related to Fig 1: Individual subject results for Fig 1 analyses. In all subjects and
 sessions, the relationships present between cofluctuation and correlation with time-averaged FC
 (A) and modularity (B) are continuous, positive, and gradual. It suggests that in all cases,

975 neither high or low cofluctuation time points are discrete. Boxplots show the median, 25th and

976 75th percentile values per subject calculated across sessions.



977

Cofluctuation Amplitude

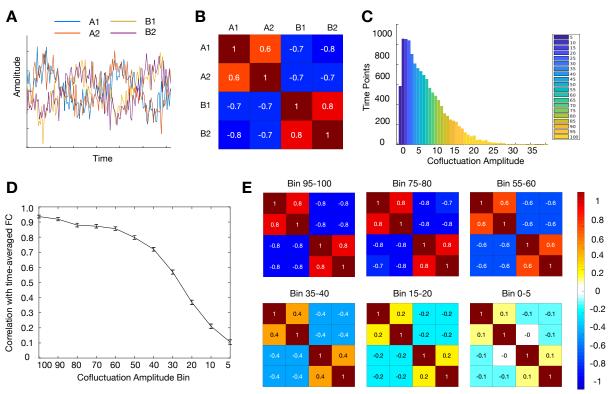
978 **Fig S2, related to Fig 2:** Individual subject results for simulation analysis. In all subjects, the

979 relationships present between cofluctuation amplitude and correlation with time-averaged FC
 980 (A) and modularity (B) are continuous, positive, and extremely similar to the relationships

980 (A) and modularity (B) are continuous, positive, and extremely similar to the relationships
 981 present in real data. This suggests sampling variability in static FC is sufficient to explain the

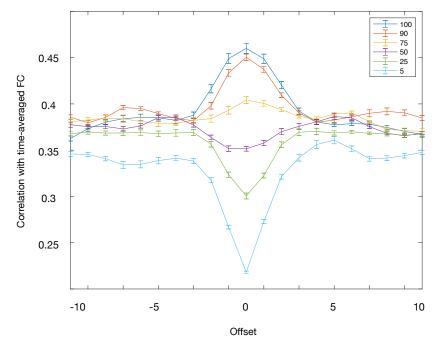
982 presence of high and low cofluctuation points in real data.

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983

984 Figure S3. Related to Fig 2: The relationship between network structure and cofluctuation is 985 present in extremely simple non-BOLD-like models. We created a 2 network, 4 node model from 986 sine waves and tested the relationship between network structure and cofluctuation. (A) 987 Network A is made of two nodes, each with the sine(t) wave. Network B is made of two nodes, 988 each with sine($t+\pi/2$) wave. Random noise was added to all four nodes. (B) Over the time 989 course, there is moderately high magnitude (r = 0.7) correlation between in-network nodes. (C) 990 As in real data, there were points of high and low cofluctuation so it was possible to bin time 991 points the same way as was done in real and BOLD-simulated data. (D) A similar relationship 992 exists between cofluctuation and network structure where higher cofluctuation bins are better 993 able to reproduce network structure from the overall time course. Error bars here represent 994 SEM over 1000 iterations of the model. (E) This relationship is visually obvious in correlation 995 matrices. In high cofluctuation bins, the two antagonistic networks are strongly present, and in 996 low bins there is little or no relationship between nodes.



997

998 Figure S4. Related to Fig 3: After accounting for spacing, there remains a graded hierarchy of 999 network structure with cofluctuation. We completed a circular shifting analysis (see Methods) 1000 where time points are binned by cofluctuation and then circularly offset. Due to scrubbing, it was 1001 not possible to select as many time points per bin (typically all time points, 5% of total time 1002 points) without running into scrubbed points while circularly shifting the values. To address this 1003 issue, we randomly sampled only 5 eligible points per bin and used fewer bins (95-100, 85-90, 1004 70-75, 45-50, 20-25, 0-5). This resulted in a smaller number of sessions (53/90) which 1005 contained full data for all bin and shift combinations. Because we used only five points, 1006 correlation values (maximum = 0.45 in group data) were much lower than when we calculate 1007 similarity with session FC using 5% of available points. We completed 100 iterations of this 1008 analysis and averaged the results to reduce single trial bias of the random selection of 5 eligible 1009 points. Higher cofluctuation bins have stronger correlation with time averaged FC compared to 1010 their offset counterparts and lower cofluctuation bins have weaker correlation. This suggests 1011 that while temporal spacing does in part drive the similarity of events to static network structure, 1012 there is a relationship between cofluctuation and network structure. Fig 2 suggests this is 1013 parsimoniously explained by sampling variability.