

Auditory Brainstem Responses in the C57BL/6J Fragile X Syndrome Knockout Mouse Model

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6 **Keywords:** Auditory Brainstem Response (ABR), Fragile X Syndrome, binaural hearing, sex
7 differences, mouse model

8 **Abstract (250 words)**

9 Sensory hypersensitivity, especially in the auditory system, is a common symptom in Fragile X
10 Syndrome (FXS), the most common monogenic form of intellectual disability. However, linking
11 phenotypes across genetic background strains of mouse models has been a challenge and could
12 underly some of the issues with translatability of drug studies to the human condition. This study is
13 the first to characterize the auditory brainstem response (ABR), a minimally invasive physiological
14 readout of early auditory processing that is also used in humans, in a commonly used mouse
15 background strain model of FXS, C57BL/6J. We measured morphological features of pinna and head
16 and used ABR to measure hearing range, monaural and binaural auditory responses in hemizygous
17 males, homozygous females and heterozygous females compared to wildtype mice. Consistent with
18 previous work we showed no difference in morphological parameters across genotypes or sexes.
19 Male FXS mice had increased threshold for high frequency hearing at 64 kHz compared to wildtype
20 males, while females had no difference in hearing range between genotypes. In contrast, female
21 homozygous FXS mice had decreased amplitude of wave IV of the monaural ABR, while there was
22 no difference in males for amplitudes and no change in latency of ABR waveforms across sexes and
23 genotypes. Lastly, FXS males had increased latency of the binaural interaction component (BIC) at 0
24 ITD compared to wildtype males. These findings further clarify auditory brainstem processing in
25 FXS by adding more information across genetic background strains allowing for a better
26 understanding of shared phenotypes.

27 **1 Introduction**

28 Fragile X Syndrome (FXS) is the most common monogenic form of autism spectrum disorder (ASD)
29 and shares many attributes of ASDs including auditory hypersensitivity and other sensory disruptions
30 (Abbeduto and Hagerman, 1997; Chen and Toth, 2001; Hagerman and Hagerman, 2002; Arnett et al.,
31 2014). FXS is a tractable genetic model for ASD with several commercially available models,
32 including rat and mouse (The Dutch-Belgian Fragile X Consortium et al., 1994; Till et al., 2015;
33 Tian et al., 2017). Despite the common use of these models to study FXS, phenotypes are not always
34 shared between species and background strains, particularly for sensory processing. As a result, drug
35 therapies have struggled to rescue the human disorder (Dahlhaus, 2018). One of the most common
36 symptoms described in people with FXS and ASD is auditory hypersensitivity (Ethridge et al., 2017;
37 Stefanelli et al., 2020). The mechanisms that underly auditory alterations are unknown, but likely
38 involve the entirety of the ascending pathway from the periphery to the cortex (reviewed in

39 McCullagh et al., 2020b). A complete characterization of auditory processing from the periphery to
40 cortex across sexes, background strains, and models is needed to fully understand shared phenotypes
41 and circuitry involved in this common symptom.

42 The auditory brainstem is one brain region in the ascending auditory pathway that has shown to have
43 anatomical, physiological, and behavioral alterations in FXS mouse models (Brown et al., 2010;
44 Beebe et al., 2014; Wang et al., 2014, 2015; Rotschafer et al., 2015; Garcia-Pino et al., 2017;
45 McCullagh et al., 2017, 2020a; Rotschafer and Cramer, 2017; Curry et al., 2018; El-Hassar et al.,
46 2019; Lu, 2019). The auditory brainstem is the first site of binaural processing of sound location in
47 the brain using interaural timing and level differences (ITD and ILD respectively) to compute sound
48 source locations (Grothe et al., 2010). This brain area is also involved in separating spatial channels
49 allowing for complex listening environments. Disruptions in this spatial separation and binaural
50 processing could lead to auditory hypersensitivity due to inability to separate sound sources
51 (Bronkhorst, 2015). One measure of auditory brainstem physiology, and binaural hearing, that can be
52 directly translated between animal models and humans is the auditory brainstem response (ABR)
53 (Laumen et al., 2016).

54 The ABR is a minimally invasive physiological measure that allows for simultaneous assessment of
55 sound processing across multiple brainstem nuclei, as each wave of the ABR directly corresponds to
56 distinct areas of the ascending auditory brainstem pathway. These features make the ABR an
57 attractive translational tool. Indeed, recent evidence suggests that ABR measurements are an early
58 indicator for auditory dysfunction in ASD (Santos et al., 2017). ABRs can also be used to assess
59 binaural hearing, which is essential for sound localization and hearing in noisy environments and
60 often impaired in ASD (Visser et al., 2013). Monoaural ABRs can be recorded by stimulating each
61 ear separately and binaural responses can be generated by stimulating both ears simultaneously. The
62 sum of the two monaural (left and right) responses should equal the binaural (both ear) response
63 since the recruited neural activity from each ear should be double when stimulated simultaneously.
64 However, this is not the case, there is a difference that arises when the summed monaural responses
65 are subtracted from the binaural response, called the binaural interaction component (BIC). The BIC
66 is thought to be a direct measure of binaural processing ability in humans and animals that requires
67 the precise balance of excitatory and inhibitory drive in brainstem sound localization circuits
68 (Laumen et al., 2016).

69 In this study we report on the hearing ability, using the ABR and morphological craniofacial and
70 pinna features, of the most common mouse model of FXS, C57BL/6J across the sexes and females
71 heterozygous for the *Fmr1* mutation. We hypothesize that there may be sex differences in ABRs
72 independent of FXS genotype, but that additionally FXS animals are likely to have alterations in peak
73 amplitude or latency of ABRs and impaired high frequency hearing compared to wildtype consistent
74 with work in other FXS mouse strains (Kim et al., 2013; Rotschafer et al., 2015; El-Hassar et al.,
75 2019). Establishing core auditory phenotypes across the sexes and different mouse strains is key to
76 creating a toolbox of techniques that may translate to human FXS.

77 **2 Materials and Methods**

78 All experiments complied with all applicable laws, National Institutes of Health guidelines, and were
79 approved by the Oklahoma State University IACUC.

80 **2.1 Animals**

81 Experiments were conducted in C57BL/6J (stock #000664, B6) wildtype background, hemizygous
82 male, homozygous, or heterozygous female *Fmr1* mutant mice (B6.129P2-*Fmr1*^{tm1Cgr}/J stock
83 #003025, *Fmr1* or *Fmr1* het respectively) obtained from the Jackson Laboratory (Bar Harbor, ME
84 USA)(The Dutch-Belgian Fragile X Consortium et al., 1994). Sex was treated as a biological
85 variable and differences between the sexes, when present, are noted in the results. Numbers of
86 animals for each experiment used are listed in the figure legends and ranged from 6-10 animals per
87 sex and genotype. Animals ranged in age from 62 – 120 days old (average ages per genotype 89 ± 4
88 days old B6, 101 ± 3 days old *Fmr1*, and 97 ± 4 days old *Fmr1* het).

89 **2.2 Morphological Measures**

90 Features of animal's head, pinna, and body mass (weight) were measured for each genotype using 6
91 Inch Stainless Steel Electronic Vernier Calipers (DIGI-Science Accumatic digital caliper Gyros
92 Precision Tools Monsey, NY, USA) and an electronic scale. The distance between the two pinnae
93 (inter pinna distance), distance from the nose to the middle of the pinna (nose to pinna distance) and
94 pinna width and length were measured (Figure 2A). The effective diameter was calculated as the
95 square root of pinna length times pinna width (Anbuhl et al., 2017).

96 **2.3 ABRs**

97 ABR recordings were performed using similar methods to previously published work (Benichoux et
98 al., 2018; McCullagh et al., 2020a; New et al., 2021). Animals were anesthetized using two mixtures
99 of ketamine-xylazine 60mg/kg ketamine and 10mg/kg xylazine for initial induction followed by
100 maintenance doses of 25 mg/kg ketamine and 12 mg/kg xylazine. Once anesthesia was confirmed by
101 lack of a toe-pinch reflex, animals were transferred to a small sound attenuating chamber (Noise
102 Barriers Lake Forest, IL, USA) and body temperature was maintained using a water-pump heating
103 pad. Subdermal needle electrodes were placed under the skin between the ears (apex), directly behind
104 the apex in the nape (reference), and in the back leg for ground. This montage has been shown to be
105 particularly effective in generating the BIC (Levine, 1981; Laumen et al., 2016). Evoked potentials
106 from subdermal needle electrodes were acquired and amplified using a Tucker-Davis Technologies
107 (TDT, Alachua, FL, USA) RA4LI head stage and a TDT RA16PA preamplifier. Further
108 amplification was provided by a TDT Multi I/O processor RZ5 connected to a PC with custom
109 Python software for data recording. Data were averaged across 500-1000 repetitions per condition
110 and processed using a second order 50 - 3000 Hz filter over 12 ms of recording time.

111 Sound stimuli (see below for varying types) were presented to the animal through TDT EC-1
112 electrostatic speakers (frequencies 32 – 64 kHz) or TDT MF-1 multi-field speakers (frequencies 1 –
113 24 kHz and clicks) coupled through custom ear pieces fitted with Etymotic ER-7C probe
114 microphones (Etymotic Research Inc, Elk Grove Village, IL, USA) for in-ear calibration
115 (Beutelmann et al., 2015). Sounds were generated using a TDT RP2.1 Real-Time processor
116 controlled by custom Python code at a sampling rate of 48828.125 Hz. Sounds were presented at an
117 interstimulus interval of 30 ms with a standard deviation of 5 ms (Laumen et al., 2016). An additional
118 rejection threshold was set to eliminate high amplitude heart rate responses from average traces and
119 improve signal to noise ratio.

120 **2.3.1 Audiogram**

121 Hearing range of animals was tested using the threshold for hearing across different frequencies of
122 sound (1, 2, 4, 8, 16, 24, 32, 46, 64 kHz). Threshold was determined using a visual detection method

123 (Brittan-Powell and Dooling, 2004), or the lowest level (dB SPL) a response could be detected
124 (independent of wave) or 2.5 dB SPL below the lowest level that elicited a response. Audiogram
125 stimuli consisted of tone bursts ($2 \text{ ms} \pm 1 \text{ ms}$ on/off ramps) of varying frequency and intensity.

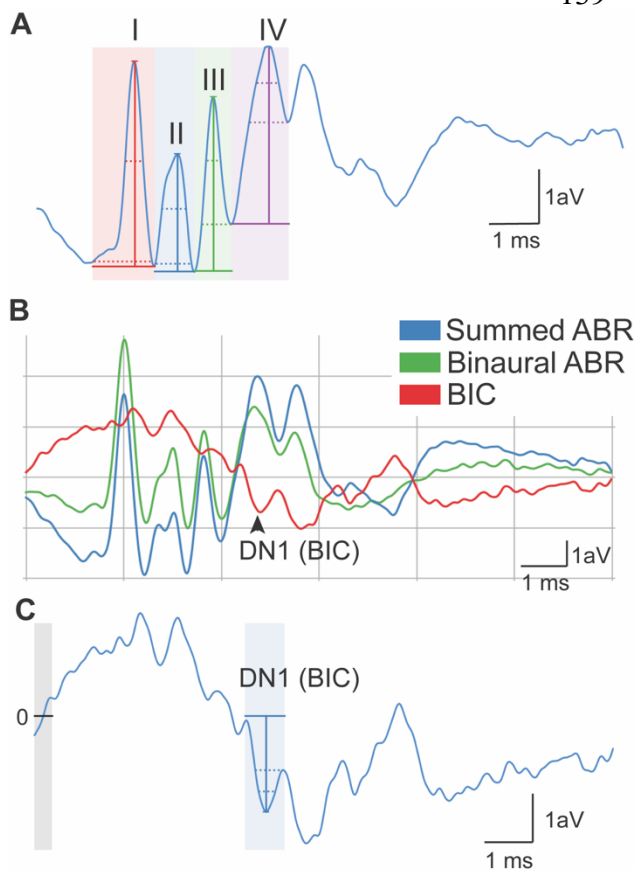
126 2.3.2 Monaural ABRs

127 Click stimuli (0.1 ms transient) were presented to each ear independently to generate monaural
128 evoked potentials. Peak amplitude (voltage from peak to trough) and latency (time to peak amplitude)
129 were measured across the four peaks of the ABR waveform at 90 dB SPL (Figure 1A). The trough
130 was considered the lowest point for that wave. Monaural data from the two ears were averaged to
131 determine monaural amplitude and latency for each animal. Like hearing thresholds across
132 frequency, click threshold was determined for each genotype and sex. Click threshold is determined
133 by decreasing intensity of sound in 5 - 10 dB SPL steps until ABR waveforms disappear.

134 2.3.3 Binaural ABRs

135 Click stimuli at 90 dB SPL were also presented to both ears simultaneously to generate a binaural
136 evoked potential. The binaural interaction component (BIC) of the ABR was calculated by
137 subtracting the sum of the two monaural ABRs from the binaural ABR (Laumen et al., 2016;
138 Benichoux et al., 2018)(Figure 1B and C). BIC amplitude and latency were then measured using

139



custom Python software, with amplitude being relative to the zero baseline of the measurement (Figure 1C, gray area with line). BIC was characterized as the prominent negative DN1 wave corresponding to the fourth wave of the binaural and summed ABR (Figure 1B). To measure interaural timing difference (ITD) computation using the BIC, animals were presented with stimuli that had varying ITDs of $\pm 2 \text{ ms}$ in 0.5 ms steps and corresponding BIC amplitudes and latencies were calculated like above. This ITD range was chosen to be comparable to other studies in small rodents (Benichoux et al., 2018).

Figure 1. Quantification of ABR signals. Monaural ABR amplitudes were quantified for each ear as the voltage between the peak of the ABR and trough of the waveform for waves I-IV (A). Latency was calculated as the time when the height of the peak occurred. DN1 or BIC (red) was calculated as the prominent negative peak corresponding with wave IV of the summed (blue) and binaural (green)(B). BIC is calculated as the summed ABR subtracted from the binaural ABR. The BIC amplitude was calculated as voltage at the peak of the DN1 waveform to the baseline (0, line and gray area) of the measurement (C). Scale represents 1 voltage unit (Y) during 1 ms (X).

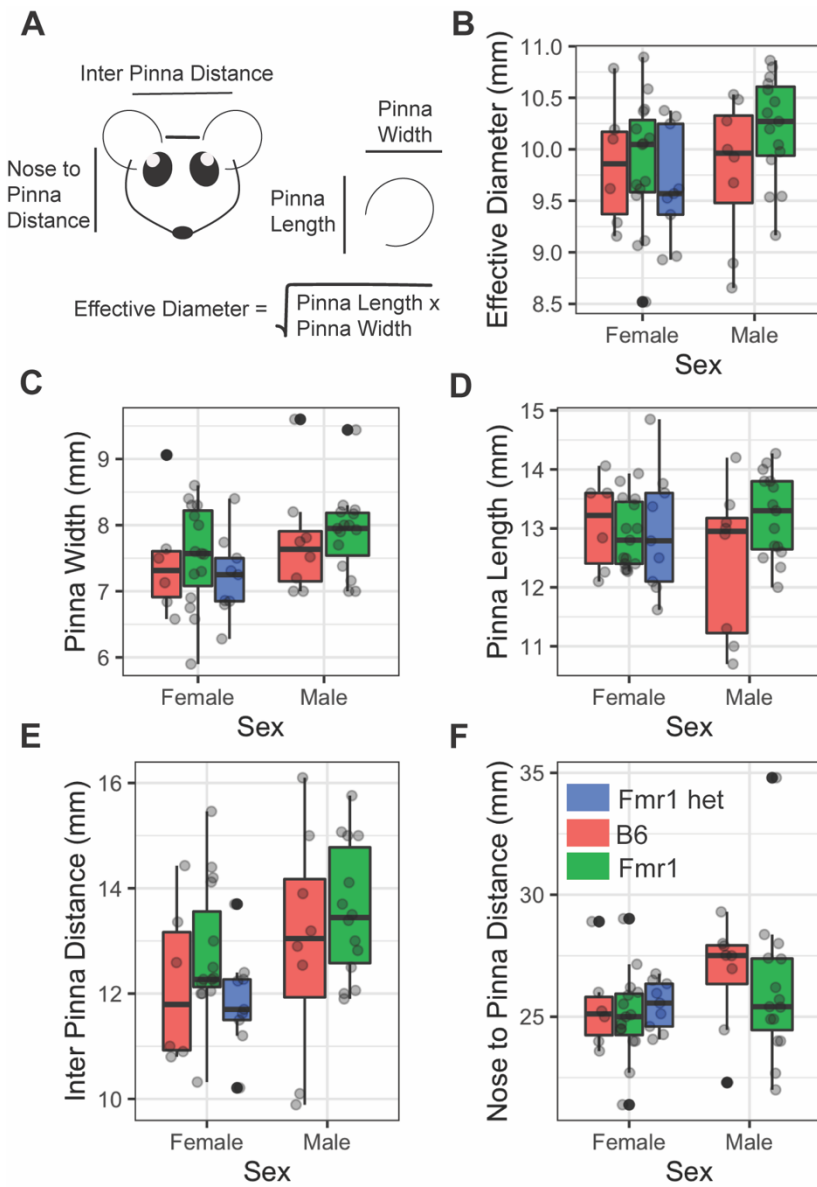
165 2.4 Analysis of ABR waveforms

166 Custom python software was used to analyze evoked potentials for monaural and binaural stimuli
167 (New et al., 2021). To account for fluctuation in the baseline signal of the ABR, raw traces were

168 zeroed to establish a baseline across traces. The software included automatic peak detection with the
 169 capability of manual correction or deselection upon visual confirmation.

170 2.5 Statistical analyses

171 Figures were generated using R Studio (R Core Team, 2013), ggplot2 (Wickham, 2016), and Adobe
 172 Illustrator (Adobe, San Jose, CA USA). Data points on Figures 3, 4, and 5 represent means and error
 173 bars reflect standard error, boxplots in Figure 2 display the median and 25th – 75th percentiles (or 1st
 174 and 3rd quartiles respectively) the whiskers represent +/- 1.5 times the interquartile range. Data that
 175 falls outside the range are plotted as individual points. Multivariate data (monaural peak amplitude
 176 and latency, audiogram, and BIC amplitude and latency across ITD) were analyzed using linear
 177 mixed effects (lme4) models (Bates et al., 2015) with sex, genotype, and condition (ITD, Frequency,



Peak) as fixed effects and animal as a random effect. It was expected that there may be differences between the sexes and genotypes therefore a priori, it was determined that estimated marginal means (emmeans; (Lenth, 2019)) would be used for pairwise comparisons between sexes and genotype. Two-way ANOVAs were performed to compare relationships between morphological features, sex, and genotype with adjusted Tukey posthoc analysis to compare groups. Where values are indicated as statistically significant between the two genotypes, * indicated a p-value of < 0.05, ** = p < 0.01, and *** = p < 0.0001.

Figure 2. Morphological features of FXS mice. Pinna and head features (A) were measured between the sexes (x-axis) and genotypes (purple = B6, teal = Fmr1, yellow = Fmr1 het). There was no difference between the sexes or genotypes for any of the measures (effective diameter B, pinna width C, pinna length D, inter pinna length E, or nose to pinna length F). Data represent 6 B6, 15 Fmr1, 9 Fmr1 het females and 8 B6, 15 Fmr1 males.

4 Results

211 We used both morphological and physiological features to examine hearing differences in a
 212 commonly used mouse model of FXS, C57BL/6J across genotypes and sexes. Hearing measurements

213 included frequency hearing range, monaural hearing ability, and binaural processing using the ABR,
 214 while morphological features included pinna and head measurements.

215 4.1 Morphological features

216 People with FXS have altered craniofacial features, including large ears (Loesch et al., 1988).
 217 Consistent with our previous work (McCullagh et al., 2020a) we see no difference between B6,
 218 Fmr1, or Fmr1 het animals for pinna attributes (Figure 2C pinna width, 2D pinna length, 2B effective
 219 diameter). In addition, pinna characteristics were the same between the sexes ($p = 0.175$ pinna width,
 220 $p = 0.96$ pinna length, $p = 0.267$ effective diameter Figure 2B-D). When genotypes were compared
 221 within the same sex, there were no differences in weight, but sexes were significantly different
 222 independent of genotype ($p = 0.0023$) with females weighing significantly less than males. Similar to
 223 pinna morphology, there was no significant difference in either distance between pinna or distance
 224 from the nose to pinna between the genotypes or sexes (Figure 2E and F). These data suggest that

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mice do not share the same craniofacial changes, at least in the measurements described here, as people with FXS.

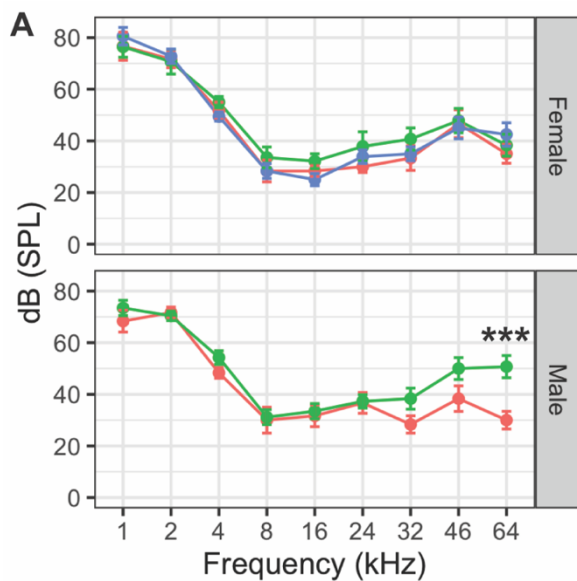
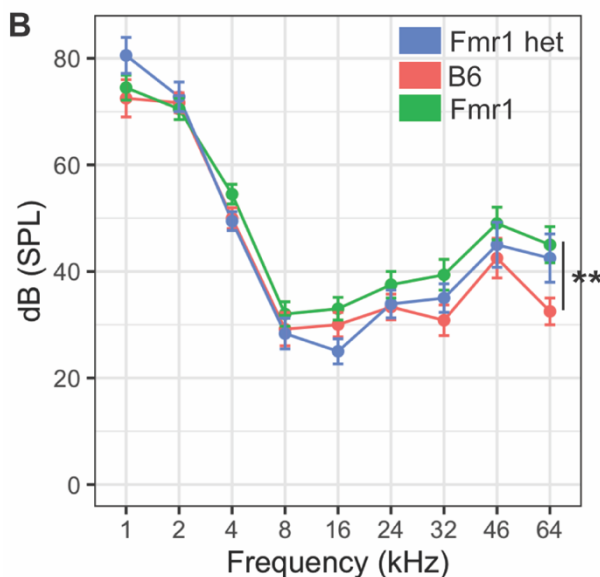


Figure 3. Hearing range of FXS mice. Hearing threshold (dB SPL) was measured across frequencies (1-64 kHz) in male and female mice of all genotypes (A). Fmr1 (green) males (lower panel) had significantly higher threshold hearing at 64 kHz compared to B6 (red) males. There were no differences in hearing range between female Fmr1 (green), B6 (red), and Fmr1 het (blue) mice (top panel A). When sexes were combined, the significant difference in hearing at 64 kHz persisted in Fmr1 animals compared to B6 but was not significant in female Fmr1 het animals (B). ** = $p < 0.01$, *** = $p < 0.001$. Data represent 6 B6, 7 Fmr1, 9 Fmr1 het females and 6 B6, 11 Fmr1 males.

4.2 Hearing range



Our previous work showed that Fmr1 mice have increased thresholds for high frequency hearing compared to B6 at 16 kHz (McCullagh et al., 2020a). However, that work was limited by measuring only three frequencies (4, 8, 16 kHz) and seven mice of each genotype (combined sexes). Mice hear much higher frequencies than humans (Radziwon et al., 2009), therefore we wanted to measure whether this high frequency hearing loss exists across the frequencies in which mice hear in Fmr1 mutants and with a more in-depth sex specific analysis. Interestingly, there were no differences between genotypes across most of the frequencies tested except for an increase in hearing threshold at 64 kHz in Fmr1 mice compared to B6 (Figure 3B).

There were no significant differences in hearing

258 range between the sexes, but Fmr1 males did have significantly higher threshold at 64 kHz than

259 female *Fmr1* mice suggesting that the phenotype is mostly driven by males ($p = 0.0317$) and indeed
 260 both female *Fmr1* and female *Fmr1* het mice were not different than B6 females (Figure 3A). Best
 261 frequencies for both genotypes, as indicated by lower threshold, of mice were between 8 – 64 kHz
 262 consistent with specialized high frequency hearing.

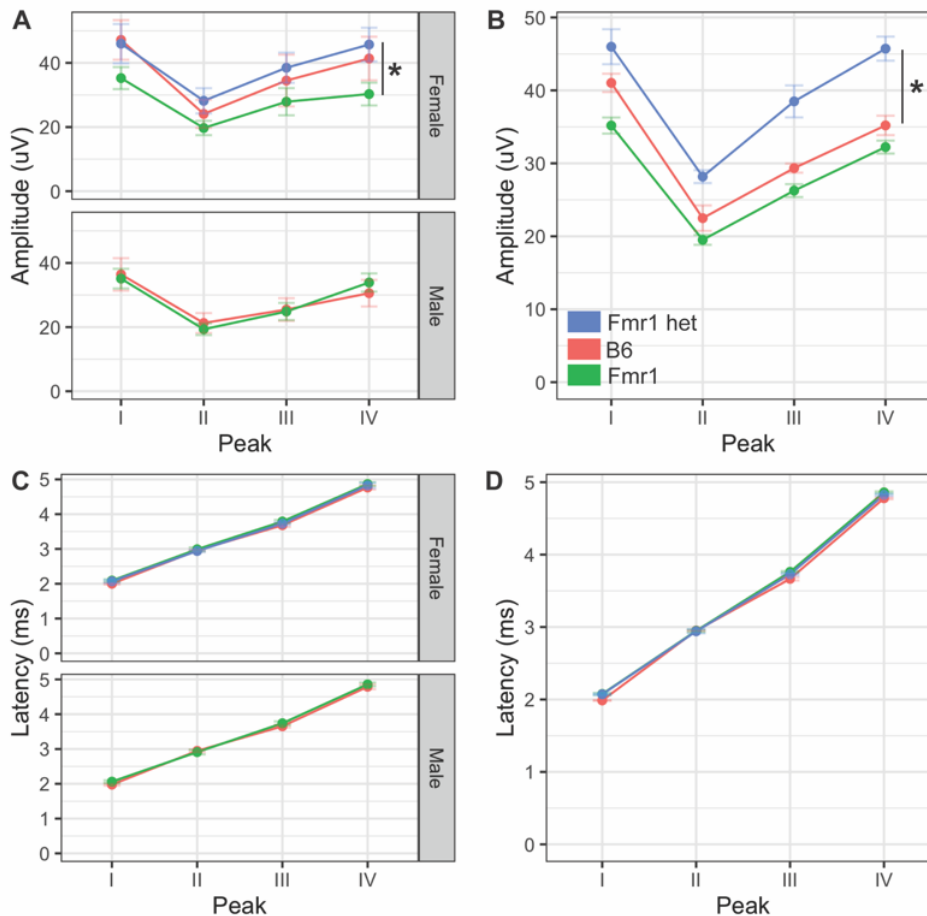


Figure 4. Monaural hearing in FXS mice. Monaural amplitudes and latencies for peaks I-IV of the ABR were recorded for *Fmr1*, *Fmr1* het, and B6 animals. Peak IV amplitude was significantly lower in *Fmr1* mice females compared to *Fmr1* het females (A upper), There were no significant differences in amplitudes for males (A, lower). When combined, there was a significant difference in *Fmr1* het animals compared to *Fmr1* (B). There was no difference in latency of peaks I-IV between sexes (C) or genotypes (D). * = $p < 0.05$. Data represent 6 B6, 12 *Fmr1*, 9 *Fmr1* het females and 8 B6, 14 *Fmr1* males.

4.3 Monaural hearing

Amplitude and latency of

291 monaural ABRs correspond with neural activity across the ascending auditory pathway, with each
 292 wave representing different brain areas involved in auditory processing (Alvarado et al., 2012). Other
 293 studies have shown both latency and amplitude alterations in the FVB mouse strain of *Fmr1* mutation
 294 (Kim et al., 2013; Rotschafer et al., 2015; El-Hassar et al., 2019). We measured ABR responses of
 295 *Fmr1* mutants to monaural click stimuli compared to B6 mutant mice to determine if they have a
 296 similar ABR phenotype to the FVB strain. We saw no differences in overall click threshold for either
 297 genotype or sex ($p = 0.102$ genotype and $p = 0.47$ for sex). Amplitude of monaural responses was
 298 significantly lower for wave IV of the ABR in *Fmr1* females compared to *Fmr1* het females (Figure
 299 4A upper). Indeed, *Fmr1* het female amplitudes were closer to B6 than *Fmr1* females, though *Fmr1*
 300 females were not significantly different from B6. In contrast, *Fmr1* male amplitudes for waves I-IV
 301 were not different from B6 (Figure 4A lower). When sexes were combined, *Fmr1* het females had
 302 significantly higher amplitudes than B6, and were close to being significantly higher than *Fmr1* mice
 303 ($p = 0.0593$). Consistent with sex driving the differences in genotype, peak amplitudes varied
 304 between the sexes. Female B6 mice had significantly higher amplitude peaks I and IV compared to
 305 B6 males ($p = 0.0295$ peak I and $p = 0.0289$ peak IV). In contrast, there were no sex differences
 306 between male and female *Fmr1* mice suggesting a more male-like phenotype (independent of
 307 genotype) in homozygous *Fmr1* females. There were no differences between the sexes or genotypes
 308 in latency of monaural peaks (Figure 4C and D).

309

310 4.4 Binaural hearing

311 While the monaural ABR provides information about binaural areas of the brainstem (potentially
 312 peaks III and IV), since they are elicited by either sound played directly to one ear (closed field) or
 313 equally to both ears (open field), little information can be gained about binaural integration of sound
 314 information. We used the BIC of the ABR to measure binaural processing ability of the brainstem as
 315 the BIC varies with ITDs played to both ears. We saw no differences in amplitude of the BIC at any
 316 ITD between the two genotypes ($p = 0.809$) or with sex ($p = 0.6904$, Figure 5A, B), though there was
 317 a significant difference between Fmr1 male and female mouse BIC amplitudes at 1.5 ms ITD.
 318 Latency of the BIC was significantly slower in male Fmr1 compared to B6 (Figure 5C, lower panel)
 319 only at 0 ITD, with no difference in genotype for female mice (Figure 5C, upper panel). When data
 320 were combined for sexes across genotype, there was no significant difference in latency of the BIC at
 321 any ITD (Figure 5D). There were differences in latency of the BIC between B6 (-1.5 ms) and Fmr1
 322 (1 ms) males and females though there was no overall main effect of sex ($p = 0.3367$).

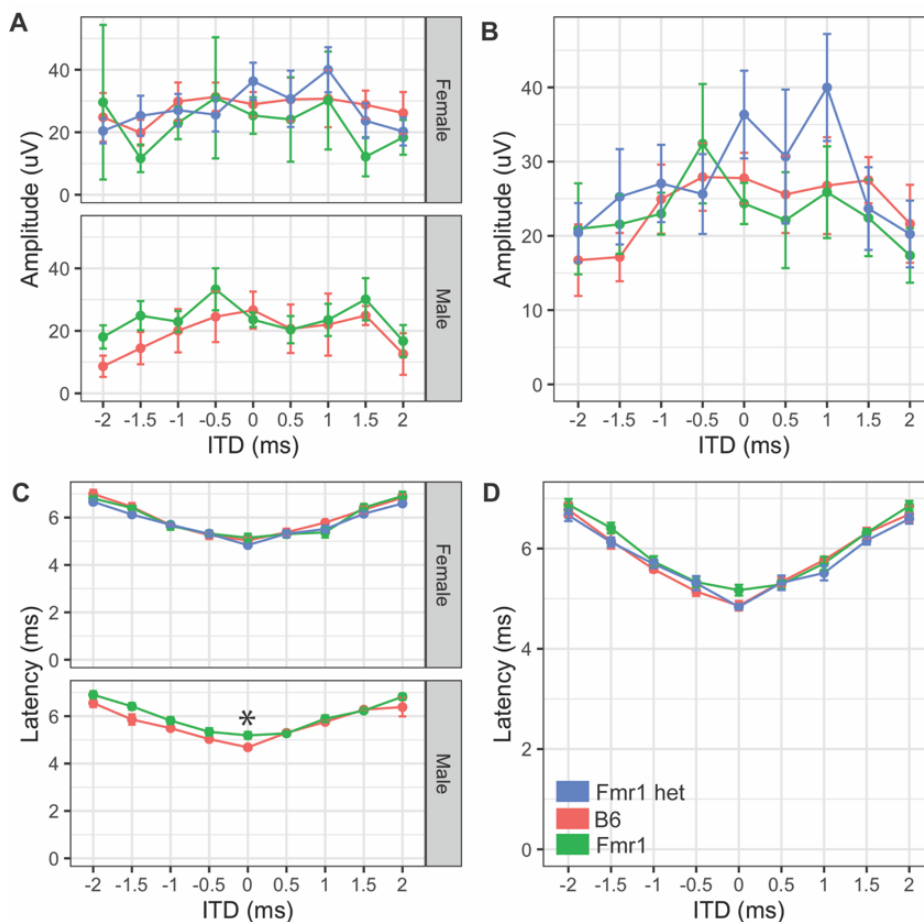


Figure 5. Binaural hearing in FXS mice. Binaural amplitudes and latencies for the BIC at ITDs between -2 to +2 ms in 0.5 ms steps were recorded for Fmr1 (green), Fmr1 het (blue), and B6 (red) animals. No differences in amplitude of the BIC with ITD for females (A upper), or males (A lower). When sexes were combined, there was no significant difference in amplitude of the BIC with ITD (B). Fmr1 males had significantly longer latency of the BIC at 0 ITD compared to B6 males (C, lower), while there was no difference in latency of female responses (C, upper). When sexes were combined, there was no difference in the BIC latency across ITDs between the genotypes (D). * = $p < 0.05$. Data represent 6 B6, 7 Fmr1, 9 Fmr1 het females and 6 B6, 9 Fmr1 males.

352

353 5 Discussion

354 This is the first study to characterize the ABR in the C57BL/6J Fmr1 mutant mouse, and in particular
 355 highlights morphological characteristics, hearing range, monaural ABRs, and binaural integration
 356 across sexes and in heterozygote females. Consistent with previous work, we see an increase in

357 hearing threshold at high frequencies in Fmr1 mice, though this phenotype is male specific, and no
358 change in morphology (pinna or facial characteristics)(McCullagh et al., 2020a). Female Fmr1 mice
359 have reduced wave IV amplitudes of the monaural ABR, and wildtype females have increased wave I
360 and IV amplitudes compared to B6 males, suggesting that female Fmr1 mice have a more male-like
361 phenotype for monaural ABR amplitude. Lastly, we showed that male Fmr1 mice have increased
362 latency of the BIC at 0 ITD, but not other ITDs or changes in amplitude of the BIC across ITD
363 compared to B6 animals suggesting changes in timing of the processing of binaural information that
364 does not change overall ITD following ability.

365 Pinnae size and shape are the first feature available to determine sound localization ability in animals
366 with external ears (Butler, 1975; Musicant and Butler, 1984). Craniofacial alterations including
367 prominent ears and elongated face are hallmark features of humans with FXS (Loesch et al., 1988;
368 Heulens et al., 2013) and indeed may be a factor in auditory hypersensitivity that has been
369 underexplored. Consistent with our previous work, we see no alterations in pinna or facial
370 characteristics in the C57BL/6J mouse model of FXS (McCullagh et al., 2020a) using calipers as a
371 measurement tool. Others have explored morphological skull differences in FXS mice using different
372 tools such as CT/MRI (Ellegood et al., 2010) and micro-CT (Heulens et al., 2013) with mixed results.
373 Heulens et al., 2013 showed alterations in skull and jaw characteristics that had not been
374 characterized previously with a similar technique (Ellegood et al., 2010) though differences may be
375 due to how features were measured. We also see no difference in weight of Fmr1 animals compared
376 to wildtype which is in contrast to our previous work where we noted that Fmr1 animals weighed less
377 than wildtype (McCullagh et al., 2020a) and others that showed an increase in male Fmr1 mouse
378 weight compared to wildtype (Leboucher et al., 2019). Differences in weight may be due to inclusion
379 of female animals (McCullagh et al., 2020a) and older animals (Leboucher et al., 2019). Overall
380 changes in pinna morphology may still be an important factor in sound localization ability in Fmr1
381 animals and should be explored with more detailed techniques to determine if increased pinna
382 measures in both humans and animal models may underly some aspect of auditory hypersensitivity
383 symptomology.

384 Our previous results showed increased ABR measured hearing thresholds at high frequencies (16
385 kHz) in the C57BL/6J Fmr1 strain with data combined for the sexes (McCullagh et al., 2020a). In the
386 current study, we do not see increased thresholds at 16 kHz but do see similar increased thresholds at
387 64 kHz in male Fmr1 mice specifically. These data are consistent with the increased thresholds
388 across frequencies seen in adult male FVB Fmr1 mice (Rotschafer et al., 2015), though note that
389 there was no change in threshold across frequencies in males of the same FVB strain at younger ages
390 (Kim et al., 2013; El-Hassar et al., 2019). These data suggest that there may be age-related changes in
391 high frequency hearing in adult male mice with FXS mutations across strains. This is particularly
392 interesting since FVB mice are largely protected from early onset age-related hearing loss that the
393 C57BL/6J background strain is particularly known for (Ison et al., 2007; Ho et al., 2014) suggesting
394 that high frequency hearing deficits in males is a potentially conserved trait in FXS independent of
395 background strain. Additional studies should examine hearing range across development and sexes in
396 both strains to further show whether loss of high frequency hearing is a conserved feature in FXS.

397 Previous studies in the FVB Fmr1 mouse line show a robust wave I amplitude decrease in males
398 across ages (Rotschafer et al., 2015; El-Hassar et al., 2019), though see (Kim et al., 2013). We do not
399 see any change in wave I amplitude in the C57BL/6J Fmr1 line in adult animals of either sex. These
400 conflicting results may be in part due to the earlier onset age-related hearing loss, which can be seen
401 as decreases in early waves of the ABR, that occurs in the B6 background (Hunter and Willott,
402 1987). Changes in wave I amplitude specific to FXS may be masked by overall decreases in wave I

403 amplitude across genotypes in this background. Interestingly, data in male FVB Fmr1 mice show no
404 differences (adults, Kim et al., 2013; Rotschafer et al., 2015), or increased amplitudes in wave IV of
405 the ABR (young, El-Hassar et al., 2019) whereas our data show decreased wave IV amplitude in
406 Fmr1 females on the B6 background. These differences again may be due to differences in sexes and
407 ages of animals tested. Lastly, our finding of no difference in latency of monaural waves is consistent
408 with the majority of the work in FVB mice (Rotschafer et al., 2015; El-Hassar et al., 2019), though
409 note that Kim et al., 2013 showed shorter latency for wave I. Our data further adds to the knowledge
410 of ABR phenotypes that might be consistent across genotypes.

411 While ours is the first study to characterize the BIC in a FXS mutant mouse strain, our data are
412 consistent with the BIC as it varies with ITD in mice (Benichoux et al., 2018). Namely, mice have a
413 small range of ITD cues available due to their small head size and therefore the BIC amplitude
414 decreases with increasing ITD between the ears, but this overall amplitude change is smaller than
415 animals with more dominant ITD hearing ability (such as chinchilla or cats)(Benichoux et al., 2018).
416 Additionally, consistent with previous work, the BIC latency gets longer with increasing ITD (Ferber
417 et al., 2016; Laumen et al., 2016; Benichoux et al., 2018). Interestingly our work in FXS mice is
418 consistent with increased latency of the BIC seen in a study in autistic people (ElMoazen et al.,
419 2019), though they also see a decrease in amplitude of the BIC. Our findings that the BIC latency is
420 only significant in males at 0 ITD potentially suggests that there is overall slowing of binaural
421 processing in the brainstem, but that it is not dependent on ITD, which would be consistent with mice
422 that do not rely as predominantly on ITD cues compared to other species.

423 The subject of sex differences in animal models is important for fully understanding the complexities
424 of disorders such as autism spectrum disorder or FXS which seem to impact females differently than
425 males (Werling and Geschwind, 2013; Nolan et al., 2017). In FXS, due to it being an X-linked
426 disorder, there is a higher prevalence in males than females, which can undergo X-inactivation on the
427 effected X chromosome (genetic mosaicism)(Kirchgessner et al., 1995). However, mice offer a
428 unique opportunity to measure both heterozygote and homozygous females giving insight into
429 potential sex differences related to loss of Fmr1 on one or both X chromosomes. Our data suggest
430 that there are indeed differences in auditory phenotypes between heterozygous and homozygous
431 females (wave IV amplitude) in addition to differences between males and females. These and future
432 data comparing female Fmr1 subtypes may give insight into the role of X-inactivation in auditory
433 brainstem processing phenotypes.

434 In conclusion, this study offers important insight into auditory phenotypes that may be shared or
435 differ between background strains of FXS mice. Additionally, while subtle, we show sex-specific and
436 full or heterozygote mutation-specific differences in auditory brainstem function for both monaural
437 and binaural hearing in B6 mice. Further studies measuring auditory phenotypes for B6 mice in
438 earlier ages across the sexes would be useful to further characterize potential similarities with the
439 FVB Fmr1 strain. In addition, characterizing the BIC in the FVB strain would be useful to elucidate
440 if latency phenotypes are consistent across backgrounds.

441 **6 Conflict of Interest**

442 *The authors declare that the research was conducted in the absence of any commercial or financial*
443 *relationships that could be construed as a potential conflict of interest.*

444 **7 Author Contributions**

445 All authors helped write and revise the manuscript. EAM developed the ideas and methods. EAM
446 and AC collected the data for the manuscript. EAM performed the statistical analyses and created the
447 figures for the manuscript.

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