

1 **High definition DIC imaging uncovers transient stages of pathogen infection**
2 **cycles on the surface of human adult stem cell-derived intestinal epithelium**

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17

18 **Abstract**

19 Interactions between individual pathogenic microbes and host tissues involve fast
20 and dynamic processes that ultimately impact the outcome of infection. Using live-cell
21 microscopy, these dynamics can be visualized to study e.g. microbe motility, binding
22 and invasion of host cells, and intra-host-cell survival. Such methodology typically
23 employs confocal imaging of fluorescent tags in tumor-derived cell line infections on
24 glass. This allows high-definition imaging, but poorly reflects the host tissue's
25 physiological architecture and may result in artifacts. We developed a method for live-
26 cell imaging of microbial infection dynamics on human adult stem cell-derived intestinal
27 epithelial cell (IEC) layers. These IEC monolayers are grown in alumina membrane
28 chambers, optimized for physiological cell arrangement and fast, but gentle, differential
29 interference contrast (DIC) imaging. This allows sub-second visualization of both
30 microbial and epithelial surface ultrastructure at high resolution without using
31 fluorescent reporters. We employed this technology to probe the behavior of two model
32 pathogens, *Salmonella enterica* Typhimurium (*Salmonella*) and *Giardia intestinalis*
33 (*Giardia*), at the intestinal epithelial surface. Our results reveal pathogen-specific
34 swimming patterns on the epithelium, showing that *Salmonella* adheres to the IEC
35 surface for prolonged periods before host-cell invasion, while *Giardia* uses circular
36 swimming with intermittent attachments to scout for stable adhesion sites. This method
37 even permits tracking of individual *Giardia* flagella, demonstrating that active flagellar
38 beating and attachment to the IEC surface are not mutually exclusive. Thereby, this
39 work describes a powerful, generalizable, and relatively inexpensive approach to study

40 dynamic pathogen interactions with IEC surfaces at high resolution and under near-
41 native conditions.

42

43 **Importance**

44 Knowledge of dynamic niche-specific interactions between single microbes and
45 host cells is essential to understand infectious disease progression. However, advances
46 in this field have been hampered by the inherent conflict between the technical
47 requirements for high resolution live-cell imaging on one hand, and conditions that best
48 mimic physiological infection niche parameters on the other. Towards bridging this
49 divide, we present methodology for differential interference contrast (DIC) imaging of
50 pathogen interactions at the apical surface of enteroid-derived intestinal epithelia,
51 providing both high spatial and temporal resolution. This alleviates the need for
52 fluorescent reporters in live-cell imaging and provides dynamic information about
53 microbe interactions with a non-transformed, confluent, polarized and microvilliated
54 human gut epithelium. Using this methodology, we uncover previously unrecognized
55 stages of *Salmonella* and *Giardia* infection cycles at the epithelial surface.

56

57 **Introduction**

58 Although infectious diseases of the intestine are often caused by large
59 populations of invading pathogens, disease progression and outcome are ultimately
60 dictated by the interactions of individual microbes with the host tissues. To characterize
61 the complex dynamics of these underlying interactions, live cell microscopy has become
62 the method of choice. However, it is intrinsically difficult to study dynamic microbe

63 interactions with internal host tissues such as the intestinal epithelium *in vivo*. The
64 resolution of *ex vivo*-based microscopy techniques often suffers from the complexity
65 and depth of intact tissues, resulting in the need for more phototoxic high-dosage
66 illumination or complex and expensive 2-photon setups. Therefore, researchers have
67 turned to transformed or immortalized cell lines to study intestinal epithelial infections in
68 cultured proxies of the gut epithelium. These cell lines often fail to recapitulate key
69 features of intestinal epithelial cell (IECs) layers, such as a densely-packed polarized
70 morphology, a microvilliated apical surface, and sensitivity to cell-death mechanisms,
71 but have nevertheless uncovered a wealth of information about pathogen infection
72 cycles (1–6). By contrast, the impact of physiologically relevant host cell and tissue
73 parameters on infection dynamics remains understudied.

74 In the past decade, cultured organoid models have been shown to provide a
75 powerful intermediate for this physiological gap between cell lines and intact primary
76 tissues. The central features of the gut epithelium are faithfully recapitulated in both
77 intestinal organoids derived from pluripotent stem cells (PSCs) (7, 8), and in so called
78 enteroids or colonoids derived from adult epithelial stem cells (ASCs) of small intestine
79 or colon, respectively (9, 10). Organoid models can be cultured in a variety of two- and
80 three-dimensional (2D and 3D) settings (11, 12) and retain non-transformed cell
81 behavior over time (13, 14).

82 Despite their potential, organoid models have so far only been sparsely used for
83 live cell imaging of intestinal infection processes (15–17). In our experience, this is a
84 result of the difficulty to adapt current imaging approaches from cell line infections to
85 accommodate the properties of physiologically grown organoid-derived epithelia. First,

86 while cell lines can be grown flat on glass culture ware for optimal working distance and
87 numerical aperture, intestinal organoid-derived IECs only develop into their natural
88 polarized arrangement when cultured within rich extracellular matrices (ECMs), or atop
89 permeable supports. The latter can be accommodated by ECM-coated transwell inserts
90 with permeable membranes of Polyethylene Terephthalate (PET) or similar polymers as
91 a 2D substrate (18, 19). Enteroid/Colonoid-derived IEC layers in such transwell inserts
92 can be efficiently cultured, differentiated, and infected by a variety of gut pathogens
93 (20–28), but are poorly compatible with live cell imaging. Secondly, non-transformed
94 cells are difficult to manipulate genetically, which complicates introduction of fluorescent
95 tags to visualize the host cell and its subcellular architecture by fluorescence microscopy.
96 Finally, in contrast to tumor-derived cell lines, non-transformed cells retain sensitive cell
97 death and stress signaling pathways, which makes them susceptible to phototoxicity
98 and other perturbations and introduces a need for gentle imaging conditions. Taken
99 together, these constraints have limited the applicability of live cell imaging to
100 characterize encounters of pathogens with the apical portion of non-transformed IEC
101 layers at high spatial and temporal resolution.

102 Here, we present a new method to visualize microbial infection cycle dynamics at
103 the apical surface of ASC-derived IEC layers under near-native conditions. To
104 overcome the imaging constraints introduced by PET transwells, we developed a
105 method to grow microvilliated human epithelium layers on ECM-coated alumina
106 membranes in 3D-printed imaging chambers. In addition, we omitted the need for
107 fluorescent tagging and high-dosage illumination by optimizing the conditions for high
108 resolution, live differential interference contrast (DIC) microscopy. The use of DIC rather

109 than more phototoxic fluorescent reporter approaches favors physiologic pathogen and
110 host cell behavior and allows simultaneous visualization of both individual microbes and
111 IEC surface ultrastructure without the need for channel switching. Finally, we used this
112 method to map *Salmonella enterica* Typhimurium (*Salmonella*), and *Giardia intestinalis*
113 (*Giardia*) infection cycles atop the epithelial surface and describe previously
114 unrecognized single-microbe behaviors during IEC attachment. Thereby, we show that
115 this imaging methodology enables detailed, dynamic studies of both microbe and host
116 cell behavior at the interface of gut infection, adaptable even to genetically non-tractable
117 microorganisms.

118

119 **Results**

120 ***An alumina membrane chamber enables high-definition live cell DIC imaging at*** 121 ***the apical border of intestinal epithelial cell layers***

122 We developed a method for live cell imaging of microbe interactions with non-
123 transformed human ASC-derived intestinal epithelial cell layers, aiming to combine i)
124 high structural definition, ii) high temporal resolution, iii) gentle imaging conditions to
125 avoid phototoxicity and the need for fluorescent reporters, and iv) a confluent, polarized
126 IEC arrangement. To achieve this, we sought to improve upon the constraints presented
127 by PET transwell supports to DIC imaging (Fig 1A). Specifically, the PET membrane
128 depolarizes light, the pores in the membranes diffract light, and the plastic membrane
129 holder prevents close approach of the microscope objective to the apical side of the
130 IECs, thereby constraining the working distance and numerical aperture. Therefore, a
131 suitable alternative to PET membranes should not introduce optical interference for

132 imaging within the visual spectrum, but like PET membranes should be permeable to
133 permit efficient epithelial cell polarization. In addition, the membrane holder should allow
134 close proximity of both the objective and condenser to the epithelial surface to optimize
135 the numerical aperture of the system.

136 This led us to evaluate membranes of anodized aluminium oxide (alumina) as a
137 candidate substrate. Alumina forms a dense honeycomb-like structure with parallel,
138 sub-diffraction limit sized pores (Fig S1A), and is optically transparent when wet. Unlike
139 for PET membranes, the pores cannot be distinguished by light microscopy and the
140 alumina does not depolarize transmitted light (Fig S1B). Although alumina membranes
141 poorly support cell adhesion, various adhesion-enhancing surface modifications have
142 been reported for this material (29–31). We found that surface hydroxylation followed by
143 sequential coating with poly-L-lysine and Matrigel enabled efficient attachment and
144 expansion of human ASC-derived IECs atop the alumina membranes (Fig S1C; see
145 methods for details). Furthermore, IECs grown on coated alumina membranes
146 developed into confluent, highly polarized monolayers, reflecting *in vivo* epithelium
147 architecture (Fig S1D). To hold the alumina membrane in place during cell culture, we
148 designed a 3D-printable plastic chamber (Fig 1B). The design of the chamber can easily
149 be adapted to alternative applications, and design files are freely available for download
150 (will be available upon publication). Like a regular transwell, the chamber creates a cell
151 culture area in the middle, but the height of the chamber was kept slim to match the
152 working distance of a water-dipping objective, thereby removing air-liquid interfaces
153 within the light path. In addition, the chamber allows the objective and especially the
154 condenser to be placed in close proximity to the sample, hence maximizing the

155 utilization of the condenser's numerical aperture and thus improving the lateral
156 resolution of DIC imaging.

157 To test if this alumina membrane chamber (AMC) and upright microscope setup
158 indeed improved the quality of live DIC imaging of epithelial infection, we compared this
159 system to the existing PET transwell supports. Human IEC monolayers were grown and
160 differentiated atop PET transwells, or in AMCs, and the apical compartment was
161 infected with wild-type *Salmonella*. The PET transwells were imaged using either a
162 standard inverted DIC microscope and an oil-immersion objective (Fig 1C), or the PET
163 membrane cut out from the holder for imaging with the upright water-dipping objective
164 setup (Fig 1D). Infections in the AMCs were imaged in parallel using the same upright
165 system (Fig 1E). As expected, the contrast and resolution of both the apical IEC surface
166 and the *Salmonella* was poor for PET transwells imaged through the inverted
167 microscope (Fig 1F-G), but markedly improved through the water-dipping upright
168 system (Fig 1H-I). However, residual optical interference from the PET membrane was
169 still evident, resulting in image blurring. Moreover, the need to cut-out the PET
170 membrane prior to imaging complicated sample handling, increased risk of mechanical
171 cell damage, and caused the loose membrane to float with convection currents in the
172 imaging medium, which prevented stable image acquisition over time.

173 The AMC markedly improved on all these imaging issues by providing a stable
174 surface, minimizing the optical interference from membrane pores, and allowing easy
175 handling underneath the water-dipping objective. As such, DIC imaging of live, infected
176 IEC monolayers in AMCs showed distinct contrast of *Salmonella* atop the cell surface
177 (Fig 1J). When focusing on the IEC surface itself, we observed clearly demarcated cell-

178 cell junctions and a remarkable roughness made up of contrasting punctae (Fig 1K),
179 suggestive of a densely microvilliated surface. To correlate the live DIC image with the
180 IEC surface topology, we disassembled non-infected and *Salmonella*-infected AMCs
181 and imaged the epithelial monolayers therein also by scanning electron microscopy
182 (SEM). This provided a powerful, near-correlative setup, as SEM analysis could be
183 done on the same AMC samples used for live DIC. SEM images captured at similar
184 magnification validated the appearance of the apical epithelial surface in live DIC mode,
185 both with respect to the macro-topology of cell junctions, the slight height differences
186 between cells, and the distinctly patterned apical surface (compare figure 1K and L). At
187 higher SEM magnification, we observed a richly microvilliated surface (Fig 1M), with
188 preserved binding of *Salmonella* to the host cells (Fig 1N).

189 In conclusion, the combination of an upright water-dipping objective microscope
190 and the novel AMC provide a system for simultaneous high definition DIC imaging of
191 both microbe- and host cell- features at the apical surface of human intestinal epithelial
192 cell layers. This approach does not require the use of fluorescent dyes or labeled
193 markers, and allows for convenient semi-correlative SEM on samples fixed at the end of
194 live cell imaging.

195

196 ***Resolving sub second-scale microbial motility patterns along the apical surface*** 197 ***of human intestinal epithelium***

198 Pathogenic gut microbes often use flagellar motility to reach and explore the
199 epithelial surface. Motile pathogen behaviors have typically been studied atop artificial
200 surfaces (e.g. plastic or glass) (3, 32), or occasionally under more physiological

201 conditions (e.g. atop tissue explants (33)). However, under the latter conditions the
202 imaging method relies on fluorescent reporters and high-intensity illumination that come
203 at the price of phototoxicity, and may alter the processes under study, or do not permit
204 simultaneous surface structure visualization. The AMC setup presented here should be
205 ideally suited to study authentic pathogen motility patterns at the IEC surface under
206 minimally perturbing conditions. To leverage this possibility, we explored motility of two
207 microbes atop IEC monolayers grown in AMCs: the smaller bacterial pathogen
208 *Salmonella*, and the larger protozoan parasite *Giardia*.

209 Peritrichous flagella-driven *Salmonella* motility physically constrains stretches of
210 the bacterial swim path atop surfaces – a phenomenon called near-surface swimming
211 (NSS) (3). Using DIC imaging alone, we could successfully follow *Salmonella* NSS
212 along the apical surface of the epithelium with high frame rates (up to ~30 frames/sec)
213 at modest light intensity, and with simultaneous visualization of apical epithelial topology
214 (Fig 2A, top row panel). Although bacterial NSS could easily be tracked manually based
215 on the DIC images alone, greyscale images cannot be readily thresholded for
216 automated downstream analysis by particle tracking software, as would be the norm for
217 fluorescence imaging (Fig S2A; (34)). We therefore incorporated a squared temporal
218 median (TM^2) post-processing filter (see methods) to extract bacterial NSS information
219 from the background of the relatively static apical IEC topology. The resulting filtered
220 image stack enabled both segmentation of motile bacteria and automated particle
221 tracking without the use of fluorescent markers (Fig 2A - bottom row panels, movie will
222 be provided upon publication). Automated tracking of *Salmonella* NSS in the TM^2
223 filtered stack showed a variety of curved tracks with a mean speed of 34.7 $\mu\text{m/s}$ (Fig 2B,

224 Fig S2C) and mean turning angle of $\sim 14.68^\circ/15 \mu\text{m}$ clockwise (Fig S2E), corresponding
225 to its flagella's counterclockwise spin (35, 36). Reassessment of this pattern by
226 fluorescence imaging resulted in broadly similar tracks (Fig S2A,C), but importantly did
227 not allow simultaneous visualization of epithelial surface topology. These observations
228 validate and extend previous studies of *Salmonella* motility (3, 33, 36–38), by mapping
229 *Salmonella* NSS parameters atop a physiologically arranged epithelial surface and
230 under minimally perturbing conditions.

231 *Giardia* trophozoites feature four pairs of flagella, and use motility to swiftly
232 approach the intestinal epithelium, followed by stable attachment using a ventral disk
233 (39, 40). *Giardia* free-swimming motility in medium involves flexion of the caudal portion
234 of the parasite body (32). On flat surfaces (i.e. glass), *Giardia* adapt the swimming
235 mode to planar motility, largely driven by the flagella. Planar motility in this context is
236 defined by a swimming pattern with the ventral disk continuously in the same plane as
237 the attachment surface (32, 41). As these *Giardia* motility characteristics remain inferred
238 from more simplistic experimental conditions (40), we performed live DIC imaging of
239 early *Giardia* motility atop IEC monolayers within AMCs. Again, we could
240 simultaneously visualize the IEC surface and individual *Giardia* trophozoites, and follow
241 parasite movements at a variety of frame rates (Fig 2C, top row panels). The lower
242 contrast and less predictable swim paths noted for these bigger protozoans, as
243 compared to *Salmonella*, were not well suited for automated particle tracking. However,
244 an unsquared temporal median filtering (TM) step aided robust manual segmentation
245 and tracking of *Giardia* motility (Fig 2C - bottom row panels, movie will be provided upon
246 publication). This revealed epithelium-proximal swimming in curved or circular tracks

247 with a mean speed of 38.6 $\mu\text{m/s}$ (Fig 2D, Fig S2D) and an almost straight mean turning
248 angle of $0.41^\circ/15 \mu\text{m}$, but with a large standard deviation in both the clockwise and
249 counterclockwise direction (Fig S2F). We validated these findings also by fluorescence
250 imaging of mNeonGreen-labelled *Giardia* and automated particle tracking (Fig S2B,D).
251 The speed values aligned well with the maximal speeds measured for *Giardia* during
252 free-swimming in media (up to $\sim 40 \mu\text{m/s}$; (32)). This indicates that when first
253 approaching a polarized microvilliated epithelium, *Giardia* sustains maximal swim speed
254 for a significant period after switching to planar 2D motility.

255 Taken together, we demonstrate that DIC imaging in AMCs provides a powerful
256 solution for resolving microbial motility patterns atop a human intestinal epithelial cell
257 layer. Specifically, this methodology simultaneously captures both apical IEC layer
258 topology and single microbe behaviors at high frame rates, does not require fluorescent
259 labelling, and as such avoids both potential problems with reporter toxicity/phototoxicity,
260 as well as the temporal delays that come with switching between multiple imaging
261 channels. Moreover, the AMC imaging technology will allow in-depth analysis of how
262 microbial motility on the epithelial surface is impacted by physiologically relevant
263 surface features (e.g. crevices formed at cell-cell junctions, extruding IECs etc.).

264

265 ***Longer-term imaging reveals a previously unrecognized Salmonella Typhimurium***
266 ***infection cycle stage atop the epithelial surface***

267 Following NSS, *Salmonella* can adhere to the epithelial surface through a
268 combination of transient interactions via dedicated adhesins and/or flagella, and stable
269 docking to the plasma membrane via type-III-secretion system-1 (TTSS-1) (42–45).

270 Docking of the TTSS-1 tip subsequently permits the translocation of bacterial effector
271 proteins into the host cell cytoplasm (1). A rich body of work in epithelial cell line models
272 has shown that this leads to the near-instantaneous induction of large actin-dependent
273 membrane ruffles and swift *Salmonella* invasion of the targeted cell (1). However,
274 recent work has also shown that the induced invasion structure phenotype is dependent
275 on the context of the host cell, and suggests a relation between invasion phenotype and
276 host cell polarization status (46). It therefore remains less well understood how the
277 physiological properties of intact non-transformed epithelia may impact *Salmonella*
278 infection cycle stage(s) at the host cell surface.

279 To survey the longer-term fate(s) of *Salmonella* on IECs, we performed one-hour
280 infections of AMC chamber-grown IEC monolayers. In the resulting movies, we
281 observed an abundance of non-motile bacteria on the surface of the IEC monolayer (Fig
282 3A). The accumulation of bacteria on the cell surface occurred in a time-dependent
283 manner, and they most often remained attached for the duration of the experiment. On
284 occasion a bacterium was seen to clearly detach, indicating that not all bacteria
285 successfully formed stable docking interactions with the epithelial surface. Surprisingly,
286 stable immobilization of the bacteria only rarely led to successful invasion of the
287 monolayer (Fig 3A). Instead, this analysis uncovered prolonged lingering of *Salmonella*
288 atop the epithelial surface as the predominant behavior, even enabling bacterial division
289 of attached bacteria upon the apical surface (Fig S3). This contrasts sharply to similar
290 experiments in non-polarized epithelial cell line models, where ruffle-dependent
291 *Salmonella* entry begins within seconds to minutes post-attachment (example movie will
292 be provided upon publication) (3, 46). Nevertheless, IEC invasion could still be detected

293 in the AMC-grown IEC monolayers, albeit at lower-than-expected frequency. Some
294 bacteria disappeared from the focal plane without obvious morphological changes to the
295 IEC surface (Fig 3B, top row panels). We could for this category not unequivocally
296 distinguish between sudden detachment or IEC invasion in the absence of overt surface
297 perturbation. In other cases, we observed unambiguous *Salmonella* invasion through a
298 small digitated IEC surface rim transiently formed around the bacterium (Fig 3B - middle
299 row panels, movie will be provided upon publication), or through somewhat more
300 pronounced donut-like ruffles which begun resembling those elicited in *Salmonella*-
301 infected polarized MDCK cells (Fig 3B, bottom row panels) (46–48).

302 Successful entry of the bacterium was occasionally followed by prompt neighbor-
303 coordinated extrusion of the targeted IEC from the monolayer (Fig 3C). The extrusion
304 phenotype and timeframe corresponded well with the extrusions we previously reported
305 in *Salmonella*-infected 3D enteroids (15), and which have also been observed *in vivo*
306 (49–51). Again, using DIC imaging alone, the morphological changes in both the
307 extruding IEC and the neighboring cells could be traced over time (Fig 3C).

308 In conclusion, our results show that imaging of epithelial infection within AMCs
309 opens up new avenues for the microscope-aided study of bacterial behavior at the
310 apical border of a human IEC layer, compatible with both short (sub-second) and long
311 (hours or more) time scales. By employing this technology, we find that *Salmonella* do
312 not invade a physiologically arranged human IEC layer as easily as what has been
313 described for tumor-derived cell line infection models. Instead, stable and prolonged
314 bacterial colonization of the IEC surface constitutes a significant infection cycle stage,
315 which only for a fraction of the bacteria converts into productive IEC invasion. The

316 molecular and physiological basis for these observations constitutes an intriguing area
317 for future research.

318

319 ***Giardia alternates between rapid swimming and intermittent attachment during***
320 ***local surface exploration***

321 Earlier reports of *Giardia* behavior on glass have described the trophozoites' pre-
322 attachment swimming pattern as circular movements, largely driven by beating of the
323 anterior and ventral flagella and steered by lateral bending of the caudal region (32, 41).
324 Although the eventual attachment of *Giardia* has been validated in numerous reports
325 (40, 52), and also in epithelial cell line cultures (5, 53), exploratory trophozoite behavior
326 that leads to successful stable attachment has not yet been studied atop an intact
327 epithelial surface.

328 Therefore, we homed in on individual *Giardia* swim tracks in IEC layer regions
329 that harbored both moving and stably adhered trophozoites (Fig 4A, attached *Giardia*
330 indicated by arrows in top panel). The subset of motile *Giardia* was observed to swim in
331 circular tracks which gradually shifted their position on top of the monolayer (Fig 4B).
332 From these tracks, the link speed was calculated as the displacement divided by the
333 time interval between two subsequent frames. Unlike for the patterns described on
334 glass (32, 41), we observed a remarkably high link speed variation for this pre-
335 attachment swimming, with an average of 31.98 $\mu\text{m/s}$ ranging up to $\sim 155 \mu\text{m/s}$ (Fig S4).
336 Over time, these tracks scanned repeatedly over a local region of the epithelium (Fig
337 4A, track).

338 To study how this swimming behavior relates to IEC attachment, we carefully
339 followed the link speed variation over each full track. This revealed that trophozoites in
340 planar swimming mode occasionally slowed down to a full stop on certain areas of the
341 monolayer (Fig 4B, black arrows). Interestingly, we also found that trophozoites often
342 repeatedly visited a certain location, coming to a brief stop with each pass across that
343 particular stretch of surface (Fig 4B, white arrow). This suggests that some areas of the
344 IEC monolayer may possess properties more favorable to attachment than others. It
345 seems plausible that the highly repetitive circular pre-attachment swim patterns we
346 observe will maximize the parasite's ability to find such ideal attachment sites within a
347 given epithelial region.

348 With four pairs of flagella and an adhesive ventral disk, *Giardia* behavior at a
349 surface is the result a complicated interplay of propulsion and adhesive forces. Aside
350 from their role in propulsion, flagellar movement has been described to influence correct
351 positioning of the adhesive disk on the attachment surface, although the exact
352 mechanism of that process remains a topic of discussion (32, 52). To test if our AMC
353 imaging setup would allow studies of individual flagella movements within the context of
354 epithelial infection, we imaged individual *Giardia* atop the IEC monolayer at high frame
355 rate. We found that DIC imaging alone was indeed sufficient to distinguish the
356 movement of individual flagella on intermittently attached trophozoites (Fig 4C, top
357 panel). Application of the TM filter further facilitated manual segmentation of individual
358 flagella (Fig 4C - middle panel, movie will be provided upon publication), and the
359 imaging resolution was sufficient to indicate the movement of all four pairs of flagella
360 over time (Fig 4C, middle and bottom panel). This allowed us to determine that all of the

361 anterior, posterolateral, and ventral flagella exhibit continued movement also in
362 intermittently attached *Giardia* on IEC monolayers. Consequently, intermittent *Giardia*
363 pausing at the IEC surface is not caused by the temporary cessation of flagellar beating.
364 This finding also illustrates the power of the AMC imaging technology to resolve
365 dynamic host-pathogen interactions under near-native conditions even with subcellular
366 resolution.

367

368 **Discussion**

369 Recent work has shown that intestinal organoid-derived monolayers grown on
370 permeable supports provide a physiologically relevant culture model for host-pathogen
371 interaction, applicable to both bacteria (21–26, 28), parasites (27), and viruses (20). In
372 this context, organoids bridge the gap between the complexity and polarized nature of
373 the epithelium encountered *in vivo* and the convenient (yet sometimes
374 misrepresentative) properties of continuous cultured cell lines. Furthermore, 2D
375 organoid cultures offer an attractive alternative to 3D culture specifically for studies of
376 microbe interactions with the apical cell surface. The latter can be microinjected (15, 54,
377 55), fragmented (56), or inverted (57), but because of the 3D-topology these structures
378 are better suited for population-scale dynamics than single-microbe behavior in a stable
379 apical plane. While live-cell imaging of microbe dynamics has been published on
380 monolayers of continuous cell lines (3, 47, 58) and to an extent in microinjected 3D
381 enteroids (15), dynamic behaviors of microbes at the surface of a physiologically
382 arranged human intestinal epithelium remain poorly investigated. We show that this
383 short-coming can be explained by the inherent conflict between the technical

384 prerequisites for high-definition light microscopy (e.g. a short working distance, a thin
385 specimen, and an optically inert substrate) and the current best practices for
386 establishment of polarized IEC layer cultures.

387 Therefore, we here developed a custom imaging chamber based on a coated
388 alumina membrane substrate. This AMC is compatible with water-dipping objective
389 imaging to maximize optical resolution, while the alumina membrane has optical
390 properties superior to permeable plastic cell culture supports. With these improvements
391 to the ASC-derived IEC monolayer culture system, we present an optimized method for
392 high-definition imaging of host - microbe interactions at the apical surface of a confluent,
393 polarized, non-transformed, human gut epithelium. Finally, we used this technique to
394 uncover previously unknown behaviors of both *Salmonella* and *Giardia* on IEC
395 monolayers.

396 Our AMC imaging model allows tracing of the behavior of individual *Salmonella*
397 cells over time from the moment they come in proximity to the apical cell surface.
398 Previous work using continuous cell lines and *in vivo* infection models have shown that
399 flagella-dependent *Salmonella* motility drives the approach towards host cells (37, 59)
400 and initiates subsequent NSS-behavior in search of suitable entry sites (3, 33). Our
401 findings regarding *Salmonella*'s curved NSS atop IEC monolayers (Fig 2A,B; Fig
402 S2A,C,E) agree with this model of approach. However, in contrast to observations in
403 e.g. HeLa cells, we found that successful binding to the IEC monolayer does not
404 necessarily lead to prompt ruffle-mediated invasion (Fig 3A). Rather, we observed that
405 the bacteria often remain attached without invading within an hour post-infection. From
406 our current observations, it is not clear if this binding is reversible and adhesin-

407 dependent, or rather comprises irreversible TTSS-1-mediated docking (42). The
408 molecular obstacle(s) that make polarized non-transformed IECs more challenging to
409 invade than typical cell lines constitutes an intriguing area for further enquiry. The
410 prolonged bacterial attachment also suggests an additional biologically relevant
411 epithelial colonization stage in the infection cycle of *Salmonella*, in apparent analogy to
412 attaching-effacing enteropathogens that use the epithelial surface as a primary
413 colonization niche (60).

414 Nevertheless, we still observed *Salmonella* invasion of IECs (Fig 3B), albeit at
415 lower-than-expected frequency and often through entry structures that were smaller and
416 more transient than previously noted for infections of flat-growing cell lines (example
417 movie will be provided upon publication; (46)). This is in line with the more ‘discreet’
418 mode of *Salmonella* TTSS-1-dependent IEC invasion described in the intact mouse
419 intestine (46). In agreement with literature (17, 49–51, 61–64), we also observed that
420 successful invasion of the monolayer can lead to immediate extrusion of the infected
421 IEC (Fig 3C). When combined with tools for targeted epithelial cell differentiation,
422 bacterial and mammalian genetics, we expect the AMC imaging technology to provide a
423 framework for deciphering bacterial IEC invasion mechanics and the IEC extrusion
424 response in a near-native epithelial context.

425 Previous studies of *Giardia* infections have shown that the motile trophozoites
426 can attach to both inert substrates like glass (40) and to microvilliated cell surfaces *in*
427 *vivo* (65) and in culture (5). Research on interaction dynamics of *Giardia* with inert
428 substrates have shown that flagellar motility is essential for motility, cell division, and
429 selection of suitable attachment sites (32, 41, 52, 66, 67), although this behavior has not

430 yet been studied in real time on live cells. We here report the first study of *Giardia*
431 swimming on top of cultured cells, and on polarized IEC monolayers at that. In general
432 agreement with earlier studies on glass (32), we found that *Giardia* exhibits circular,
433 planar swimming above the attachment surface. Specifically, we found that *Giardia*
434 planar swimming speeds average around 30-40 $\mu\text{m/s}$ with short bursts of up to 155
435 $\mu\text{m/s}$ (Fig S4). These speeds are much higher than pre-attachment swimming that has
436 been characterized before on glass (32, 41, 67–69). Furthermore, we see circular
437 swimming interceded by short stretches of straight swimming (Fig 4A). Finally, we show
438 that trophozoite planar swimming along the epithelial surface leads to intermittent,
439 transient, attachments to the host cells (Fig 4B). Some of these attachments were seen
440 to repeatedly occur in the same location on the epithelial surface. Therefore, our results
441 suggest that *Giardia* planar swimming is geared towards a local surface-scanning
442 pattern, optimized to select a suitable attachment site within a given region. The circular
443 swimming pattern could aid in this process by repeatedly visiting promising sites of
444 adhesion, until an unknown threshold of stable adhesion is reached. Earlier work on
445 glass has elegantly shown that flagellar beating is instrumental to the planar swimming
446 behavior of *Giardia*, although the respective contribution of the anterior, posterolateral,
447 and ventral pair is still a matter of debate (32, 41). Strikingly, temporal median filtering in
448 our study resolved the continued movements of both anterior, posterolateral, and
449 ventral flagella in intermittently surface-attached *Giardia* (Fig 4C). Although we cannot
450 directly measure attachment force, this suggests that the transient *Giardia* pauses
451 during surface search can be explained by ventral disk or ventrolateral flange (65, 70)
452 engagement with the surface, rather than by an on-off behavior of flagellar propulsion.

453 As the AMC imaging method can be used to study both the overall swim patterns and
454 the movement of individual flagella, this technique is ideally suited to characterize the
455 complete spectrum of *Giardia* (and other parasite) behaviors atop intestinal epithelia.

456 Finally, the AMC imaging method can be adapted to accommodate a variety of
457 different host cell types and microbes. As we have shown that the coated alumina
458 membrane supports the growth of ASC-derived human enteroid monolayers, the current
459 system can likely be used to grow a variety of embryonic stem cell-, iPSC- and ASC-
460 derived epithelia. This would allow for high-definition imaging of microbial interactions
461 with any stem cell-derived human epithelium culture (e.g. airway, mammary gland,
462 stomach, or bladder epithelium, see (12) for a comprehensive overview). As ASC-
463 derived organoids retain the locational and functional identity (71) from the donor
464 material, this methodology could also be used to study the impact of congenital
465 disorders of the epithelium (like some forms of Very Early Onset Inflammatory Bowel
466 Disease) on microbial infection. Lastly, recent studies have reported an adapted
467 chamber for ASC-derived intestinal organoid monolayer co-culture with gut anaerobes
468 (26). Innovations like this open the door to even better modeling of both resident and
469 pathogenic microbes under even more physiologically accurate conditions. However, it
470 remains difficult to study dynamic interactions with the host epithelium in this context, as
471 most gut microbiota strains cannot yet be genetically modified to incorporate fluorescent
472 markers. Our AMC approach to image microbe interactions with the intestinal epithelium
473 without fluorescence could here provide a stepping stone for dynamic analysis of host
474 epithelium - microbiota interactions in the coming years.

475

476 **Materials & methods**

477 ***Ethics statement***

478 Human jejunal ASC-derived enteroids were generated from resected tissue
479 acquired from routine bariatric surgery, following prior informed consent. All personal
480 information was pseudonymized, and the patients' identities were unknown to
481 researchers working with the tissue samples. These procedures were approved by the
482 local governing body (Etikprövningsmyndigheten, Uppsala, Sweden) under license
483 number 2010-157 with addendums 2010-157-1 (2018-06-13) and 2020-05754 (2020-
484 10-26)

485

486 ***Alumina Membrane Chambers***

487 The Alumina Membrane Chambers (AMCs) for 13 mm alumina Whatman
488 Anodisc membranes with 0.2 μm pores (GE Healthcare, Little Chalfont, UK) were
489 designed in-house using FreeCAD v0.19 (<https://www.freecadweb.org>). The chamber
490 comprises a bottom holder and top cover, which fit together using a friction press fit to
491 hold the alumina membrane in place, with culture medium compartments generated on
492 each side of the membrane. The top cover contains a groove to hold a silicone gasket
493 (product number 527-9790, RS Components Ltd. Corby, UK) with inner diameter of 7.65
494 millimeter in place. AMC design files are available for non-commercial use and will be
495 provided upon publication. The AMC designs were printed using an Original Prusa
496 MINI+ (Prusa Research, Prague, Czech Republic) 3D printer with a 0.4 mm nozzle and
497 a layer height of 0.2 mm. The AMCs were printed in 1.75 mm, clear, natural PLA
498 filament (prod. number 832-0210, RS Components Ltd.).

499

500 ***Enteroid culture***

501 Human jejunal enteroids were established and cultured as described previously
502 (15, 17). Briefly, pieces of intestinal resections were washed thoroughly in ice-cold PBS
503 and epithelial crypts were subsequently dissociated using Gentle Cell Dissociation
504 Reagent (STEMCELL Technologies, Vancouver, BC, Canada) by nutating at 4°C for 30
505 minutes followed by trituration. The resulting epithelial fragments were filtered through a
506 70 µm cell strainer and crypt-enriched fractions suspended in 50 µl Matrigel (Corning,
507 Corning, NY, USA) domes in a 24 well plate. The embedded crypts were cultured in
508 OGM (IntestiCult Organoid Growth Medium (Human), STEMCELL Technologies) with
509 100 U/ml penicillin/streptomycin (Thermo Fisher (Gibco), Waltham, MA, USA) at 37°C
510 and 5% CO₂. Growth medium was refreshed every 2-3 days.

511 For maintenance of human enteroids, the structures were passaged weekly at a
512 ratio of circa 1:8 by mechanical dissociation. The Matrigel domes were manually broken
513 up by pipetting with Gentle Dissociation Reagent and then washed once with
514 DMEM/F12/1.25% BSA. The resulting suspended enteroids were disrupted by triturating
515 15-20 times with a 200ul pipet tip. Following disruption, enteroid fragments were again
516 suspended in 50 µl Matrigel:Intesticult at the ratio 3:1, divided over 3 domes per well in
517 a 24 well plate, and cultured at 37°C and 5% CO₂.

518

519 ***Enteroid-derived IEC monolayer culture***

520 Human IEC monolayers were cultured on either 24-well transparent polyethylene
521 terephthalate (PET) tissue culture inserts with 0.4 µm pores (Sarstedt, Nümbrecht,

522 Germany) or 13 mm diameter alumina Whatman Anodisc membranes. The PET
523 transwell inserts were coated with 40× diluted Matrigel in PBS for one hour at room
524 temperature prior to use. After this time, the coating was completely removed and the
525 cell suspension was immediately added to the transwell inserts. The alumina
526 membranes were coated with extracellular matrix as well, but required more extensive
527 pretreatment. First, the alumina membranes were soaked in 30% H₂O₂ for 1 hour at
528 room temperature to add negatively charged hydroxyl groups to the surface (30) and
529 allow protein binding. Then, the alumina membranes were washed in sterile dH₂O and
530 incubated in 0.1 mg/ml poly-L-lysine (Sigma-Aldrich, Stockholm, Sweden) in dH₂O for 5
531 minutes to prepare the surface for Matrigel coating. After poly-L-lysine coating, the
532 membranes were air-dried in a laminar flow cabinet for ~2 hours or overnight. Finally,
533 the alumina membranes were soaked in 40× diluted Matrigel in dH₂O for 1 hour, and
534 air-dried again. After coating, the membranes were mounted within AMCs.

535 Human enteroids were dissociated into single cell suspensions as described
536 before (17). Briefly, circa one well of enteroids per membrane was dissociated into
537 single cells at day 7 after passaging. The enteroids were first taken up from the Matrigel
538 in Gentle Dissociation Reagent, then washed in PBS/1.25% BSA, and dissociated into
539 single cells using TrypLE Express (Thermo Fisher (Gibco)) for 5-10 minutes at 37°C.
540 Cells were then spun down at 300 rcf for 5 minutes and resuspended in OGM+Y (Rho
541 kinase inhibitor Y-27632 (10 μM), Sigma). Finally, the cells were counted manually and
542 3.0×10^5 cells were seeded into the apical compartment of PET transwells in 150 μl
543 (600 μl medium in bottom compartment, 24-well plate wells), or into the apical
544 compartment of AMCs in 75 μl (600 μl medium in the bottom compartment, 12 well plate

545 wells). The monolayers typically grew confluent in 2-4 days, whereafter the cells were
546 differentiated towards an enterocyte phenotype by deprivation of Wnt-signalling for 4-5
547 days. The medium for differentiation consisted of DMEM/F12 supplemented with 5% R-
548 Spondin1 conditioned medium (home made from Cultrex 293T R-spondin1-expressing
549 cells, R&D Systems, MN, USA), 10% Noggin conditioned medium (home made with
550 HEK293-mNoggin-Fc cells, kindly provided by Prof. Hans Clevers, Utrecht University),
551 50 ng/ml mouse recombinant EGF (Sigma-Aldrich), 1X B27 supplement (Gibco), 1.25
552 mM N-acetyl cysteine, and 100 U/ml penicillin/streptomycin (9, 10).

553

554 ***Salmonella Typhimurium strain, plasmid, culture, and infection***

555 All *Salmonella* infections in this study were performed with *Salmonella enterica*
556 serovar Typhimurium, SL1344 (SB300) (72). For validation by standard fluorescence
557 microscopy, the strain carried a pFPV-mCherry (rpsM-mCherry; Addgene plasmid
558 number 20956) plasmid directing constitutive mCherry expression (73). As reported
559 previously, expression of this mCherry construct did not influence motility or invasive
560 behavior of *Salmonella* SL1344. For IEC monolayer infections, *Salmonella* inoculi were
561 grown in LB/0.3 M NaCl (Sigma-Aldrich) for 12 h overnight with 50 µg/ml ampicillin. The
562 following day, a 1:20 dilution was subcultured in LB/0.3 M NaCl without antibiotics for 4
563 h. For subsequent infection of monolayer cultures, the 4h inoculum was diluted to
564 1.0×10^8 CFU/ml in DMEM/F12 (Thermo Fisher (Gibco)) without antibiotics of which 10
565 µl was used for each infection, resulting in 1.0×10^6 CFU per monolayer.

566

567 ***Giardia intestinalis* culture and infection**

568 *Giardia intestinalis* isolate WB, clone C6 (ATCC 30957) was used in this study.
569 For validation by standard fluorescence microscopy, a modified *Giardia* line
570 constitutively expressing mNeonGreen was generated (see below). *Giardia* trophozoites
571 were grown at 37°C in 10 ml flat plastic tubes (Thermo Fisher Nunc, MA, USA) or 50ml
572 tubes (Sarstedt, Germany) filled with TYDK medium (also known as modified TYI-S-33
573 or Keister's medium) (74), supplemented with 10% heat-inactivated bovine serum
574 (Gibco, Thermo Fisher MA, United States). All materials used in the TYDK medium
575 were purchased from Sigma-Aldrich (MO, USA) unless otherwise stated. For IEC
576 monolayer infections, *Giardia* trophozoites were grown until approximately 70%
577 confluence and washed once with TYDK to remove dead cells. Further, trophozoites
578 were incubated on ice (12 min), counted and pelleted by centrifugation (800 x g, 10 min,
579 4°C). Cells were washed once in 1 ml DMEM/F12 (Thermo Fisher (Gibco)), centrifuged
580 and diluted to 2×10^7 or 4×10^7 trophozoites/ml using DMEM/F12 of which 10 μ l were
581 used for infection, resulting in 2×10^5 - 4×10^5 trophozoites per monolayer.

582

583 ***mNeonGreen* plasmid construction and *Giardia* trophozoite transfection**

584 To visualize *Giardia* trophozoites on IEC monolayers also by fluorescence
585 microscopy, we created a trophozoite strain constitutively expressing mNeonGreen
586 under the control of the beta-giardin promoter. The mNeonGreen gene was PCR-
587 amplified from the pNCS-mNeonGreen plasmid (Allele Biotechnology, CA, USA) and
588 the beta-giardin 5'UTR and 3'UTR regions were amplified from genomic DNA of the WB
589 isolate (see Table S1). The PCR fragments were fused by overlap extension PCR and

590 cloned into the integration vector pPacV-Integ-HA-C (75) using XbaI/PacI restriction
591 sites. *Giardia* trophozoites were electroporated as previously described (76). Transgenic
592 parasites that had the mNeonGreen expression cassette integrated on the chromosome
593 were selected by adding puromycin (50µg/ml) to the culture medium approximately 16 h
594 after transfection. To ensure homogeneous mNeonGreen expression in the culture, we
595 created a clonal trophozoite population from the original mNeonGreen stable
596 transfectant population using serial dilution. Briefly, the original trophozoite culture was
597 diluted in TYDK and seeded as single cells into the wells of a 96-well plate. Wells
598 reaching 70–80% confluence were selected and grown in 10 ml tubes containing TYDK.
599 After the establishment of the clonal mNeonGreen strains the trophozoites were grown
600 without antibiotics.

601

602 ***Fixed IEC monolayer imaging***

603 Differentiated IEC monolayers grown in AMCs were fixed in 4% PFA for 30 min
604 and permeabilized with 0.1% Triton X-100 for 10 minutes. Then, the cells were stained
605 with phalloidin-AF488 (Thermo Fisher) and 4',6-Diamidino-2-phenylindole
606 dihydrochloride (DAPI, Sigma-Aldrich) counterstain for 30 min in PBS. Subsequently,
607 the alumina membrane with cells was removed from the plastic membrane holder,
608 washed, and mounted under a 0.17 µm coverslip in Mowiol 4-88 (Sigma-Aldrich). The
609 samples were imaged on a Zeiss LSM700 inverted point-scanning microscope system
610 with a 63X/1.4 NA oil immersion objective using a voxel size of 70.6 nm (x,y) and 0.54
611 µm (z-sections).

612

613 ***Live cell infection imaging***

614 Live cell imaging was performed on an inverted Nikon Ti-eclipse microscope
615 (Nikon Corporation, Tokyo, Japan) with a 60X/1.4 NA Nikon PLAN APO objective (0.19
616 mm WD), Nikon condenser (0.52 NA, LWD), and Andor Zyla sCMOS camera
617 (Abingdon, Oxfordshire, England) with pixel size of 108 nm for Fig 1C,D,F-I and a
618 custom upright microscope for all other experiments. The upright microscope is a
619 custom-build, largely based on the Thorlabs Cerna upright microscopy system (Newton,
620 NJ, USA) with a heated 60X/1.0 NA Nikon CFI APO NIR objective (2.8 mm WD) and a
621 Nikon D-CUO DIC Oil Condenser (1.4 NA) controlled by Micro-Manager 2.0-gamma
622 (77). Images were acquired with an ORCA-Fusion camera (model number C14440-
623 20UP, Hamamatsu photonics, Hamamatsu City, Japan), with a final pixel size of 109
624 nm. Transmitted light was supplied by a 530 nm Thorlabs LED (M530L3) to minimize
625 phototoxicity and chromatic aberrations. The microscope chamber was maintained at
626 37°C in a moisturized 5% CO₂ atmosphere and an objective heater was used
627 additionally. Samples in AMCs were mounted in 35 mm glass-bottom dishes (Cellvis,
628 Mountain View, CA, USA) in 3 ml DMEM/F12 without antibiotics in the microscope's
629 light path, and allowed to equilibrate for 30 minutes. Then, *Salmonella* or *Giardia* were
630 added in pre-made dilutions directly underneath the objective, and imaging was started
631 immediately with <20 ms exposure times for DIC imaging and <50 ms for fluorescence
632 imaging.

633

634 **SEM imaging**

635 For SEM analysis of AMC-grown monolayers, *Salmonella* infected IEC
636 monolayers were fixed at 40 minutes post-infection and compared with uninfected
637 controls. To fix the samples, the monolayers were gently washed once with PBS and
638 fixed at 4°C overnight with 2.5% glutaraldehyde (Sigma) in 0.1M PHEM buffer (60mM
639 PIPES, 25mM HEPES, 10mM EGTA, and 4mM MgSO₄·7H₂O, pH 6.9). Prior to SEM
640 imaging, the samples were dehydrated in series of graded ethanol, critical point dried
641 (Leica EM CPD300) and coated with 5 nm platinum (Quorum Q150T-ES sputter coater).
642 The sample morphology was examined by field-emission scanning electron microscope
643 (FESEM; Carl Zeiss Merlin) using in-lens and in-chamber secondary electron detectors
644 at accelerating voltage of 4 kV and probe current of 100 pA.

645

646 **Image processing**

647 The acquired microscopy images were processed with Fiji (78). DIC images in
648 figures 2, 3, 4, and S3 were filtered to acquire an even field of illumination by
649 subtracting a (30-pixel sigma) gaussian blurred projection from the original. Where
650 indicated, a temporal median (TM) filter was used to extract quickly moving structures
651 (e.g. motile *Salmonella*, *Giardia*, and moving flagella) by subtracting the median
652 projection of the time stack from each individual frame. To enable automated particle
653 tracking of moving *Salmonella* in DIC time series, pixel values of the signed 32-bit TM
654 filtered stacks were squared to convert both 'dark' and 'light' bacteria in the TM-filtered
655 image to positive values. These TM²-filtered images were used for automated particle

656 tracking. Both automated and manual particle tracking was performed with Trackmate
657 for ImageJ v6.0.1 (34).

658

659 ***Tracking analysis and statistics***

660 Data analysis was performed with R (79) and RStudio (80) and packages
661 available from the Comprehensive R Archive Network (CRAN, [https://cran.r-](https://cran.r-project.org/)
662 [project.org/](https://cran.r-project.org/)). Tracking statistics were exported from Trackmate, and actual frame
663 intervals were obtained from the image metadata using the Cellocity python package
664 (81) to correct for variations between frames which would be reflected in inaccurate link
665 speeds. Subsequently, the track data was formatted and plotted in R with the 'tidyverse'
666 (82) package. Tracks with a mean speed of $>100 \mu\text{m/s}$ were manually confirmed to be
667 false positives of automated tracking, and therefore excluded from analysis. Track angle
668 changes for DIC-tracked swimming paths were calculated using functions based on the
669 'trajr' package (83) with an interval of three links. For the *Salmonella* swimming tracks,
670 only tracks with a mean speed of $>5 \mu\text{m/s}$ were included in the analysis to filter away
671 most non-motile bacteria. The three-link angle change was divided by the distance
672 travelled from the reference link to calculate the angle change per micron. To aid
673 interpretation of this parameter, the angle change / micron was normalized to angle
674 change / 15 micron, the average distance travelled in 3 links. Other supporting
675 packages for R include 'ggpubr', 'rstatix', 'ggbeeswarm', 'viridis', 'ggribes', and 'scales'.
676

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693 DLW, PMH, SGS, MES; Supervision: SGS, MES; Project administration: MS, DLW,
694 PMH, SGS, MES; Funding acquisition: SGS, PMH, MES; Visualization: JMvR, JG;
695 Writing - Original Draft: JMvR, MES; Writing - Reviewing & Editing: all authors.

696
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698

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- 970

971 **Figure legends**

972 **Figure 1. High-definition live cell DIC imaging of IEC monolayer infections in a**
973 **novel alumina membrane chamber.** Schematic comparison of assemblies for IEC
974 monolayer culture highlight that PET transwell membrane holders have a large plastic
975 support (A), which has been omitted in the novel AMCs (B). Both structures were placed
976 in a 35 mm glass bottom dish for imaging. The lower height of AMCs allows for closer
977 proximity, and thus greater numerical aperture, of the microscope's objective and
978 condenser. The optical interference caused by the large plastic transwell support and
979 resulting larger working distances of both objective and condenser is illustrated by live
980 cell imaging of infections in intact PET transwells in an inverted microscope (C,F,G)
981 versus cut-out PET membranes using an upright water-dipping microscope (D,H,I). This
982 change in microscope setup improved the lateral resolution of bacteria (*Salmonella*) on
983 the cell surface (F,H) and the apical surface topology of IECs (G,I). Either bacteria or
984 surface topology could be emphasized by slightly changing the focal plane, as indicated
985 on the right. Replacing the PET membrane with an alumina membrane held within the
986 custom-designed AMC (E) further improved the imaging resolution and minimized
987 optical interference (J,K). AMCs allow for sequential imaging of the same sample with
988 DIC and SEM (L-N). The latter confirmed that differentiated IECs grown in AMCs exhibit
989 a highly interconnected epithelium with a densely microvilliated surface. Bacteria are
990 indicated with yellow arrow heads. Overlaid dashed lines indicate cell-cell junctions.
991 White and yellow scale bars: 10 and 1 μm , respectively.

992

993 **Figure 2. Tracking of microbes on IEC monolayers using DIC imaging resolve**
994 ***Salmonella* and *Giardia* motility patterns.** Confluent, differentiated IEC monolayers in
995 AMCs were infected with *Salmonella-mCherry* (A-B) or *Giardia-mNeonGreen* (C-D).
996 The figure shows tracking from DIC time-lapse movies. Tracking using the respective
997 fluorescent markers (for validation purposes) is shown in Fig S2. DIC movies were
998 processed using a gaussian filter (DIC-GF) to remove uneven background illumination
999 and achieve optimal contrast for *Salmonella* (A, top panel) and *Giardia* (C, top panel).
1000 Subsequently, the total DIC-GF stack temporal median projection was subtracted from
1001 every frame to specifically emphasize moving structures (TM), and pixel values were
1002 squared (TM^2) to yield positive (white) pixels on a zero (black) background. The TM^2
1003 filtered time series was used to track all visible *Salmonella* using automated particle
1004 tracking (A, bottom panel). For *Giardia*, the TM filtered images were used for manual
1005 tracking of swimming trophozoites (C, bottom panel). A random sample of tracks within
1006 the field of view (FOV) was used to visualize *Salmonella* motility (B), while all manually
1007 tracked paths are shown for *Giardia* (D). The population mean and standard deviation
1008 for the track speeds were calculated based on all available tracks (Fig S2C,D). In A and
1009 C, a representation of the focal plane (red) is indicated on the right. Tracked microbes
1010 are indicated by magenta circles, tracks by continuous colored lines. Overlaid dashed
1011 lines indicate cell-cell junctions. Scale bars: 10 μ m.

1012

1013 **Figure 3. *Salmonella* infection cycle stages at the apical IEC surface.** Differentiated
1014 IEC monolayers were infected with *Salmonella* and imaged every 15 s. *Salmonella* was
1015 most commonly observed to attach to the apical surface for the duration of the

1016 experiment (A). A fraction of bacteria was unsuccessful in establishing a lasting
1017 adhesion, seen as a short attachment and sudden disappearance (A, asterisk). In other
1018 cases, *Salmonella* disappeared from the surface after prolonged attachment either in
1019 the absence of visible IEC surface perturbation (B, top row panels), or concomitant with
1020 the induction of phenotypically small and discreet (B, middle row panels), or larger
1021 donut-shaped (B, bottom row panels) host cell invasion structures. *Salmonella* invasion
1022 elicited prompt extrusion of some targeted IECs (C, top panel), which involved an
1023 inward movement of the surrounding IECs, evident from an overlaid drawing of the cell-
1024 cell junctions (C, bottom panel). Throughout, a representation of the focal plane (red) is
1025 indicated on the right. Bacteria are indicated with yellow, and invasion structures with
1026 red arrow heads. Yellow asterisks indicate disappearing bacteria (detachment or
1027 invasion). Overlaid dashed lines indicate cell-cell junctions. Scale bars: 10 μm .

1028

1029 **Figure 4. *Giardia* trophozoite exploration of the IEC surface.** The link speeds of
1030 *Giardia* tracks from Fig 2C,D was analyzed (see also Fig S4) and a representative track
1031 showing the common circular pattern was plotted on the DIC (A, top panel) and TM
1032 filtered (A, bottom panel and enlarged crop) images. Upon inspection of link speeds, the
1033 trophozoite was found to swim with highly variable speeds within a single track (B). The
1034 mean, minimum, and maximum speed for this track are indicated (B). During planar
1035 swimming, the trophozoite intermittently paused upon sections of the epithelium (B,
1036 black arrows), in one location each of the four times the trophozoite visited that
1037 particular area (B, white arrow). Upon closer inspection of a single, attached trophozoite
1038 (C), the TM filtered time stack showed movement of individual flagellar pairs, which

1039 could be manually segmented to follow their shape and position over time (C, middle-
1040 and bottom panel to the right, respectively). In A, a representation of the focal plane
1041 (red) is indicated on the right. Tracked microbes are indicated by magenta circles,
1042 tracks by continuous yellow lines. Yellow- and red arrow heads indicate continuously
1043 attached and temporarily attached *Giardia* respectively. The enlarged trophozoite is
1044 indicated with a yellow square. Scale bars: 10 μ m.

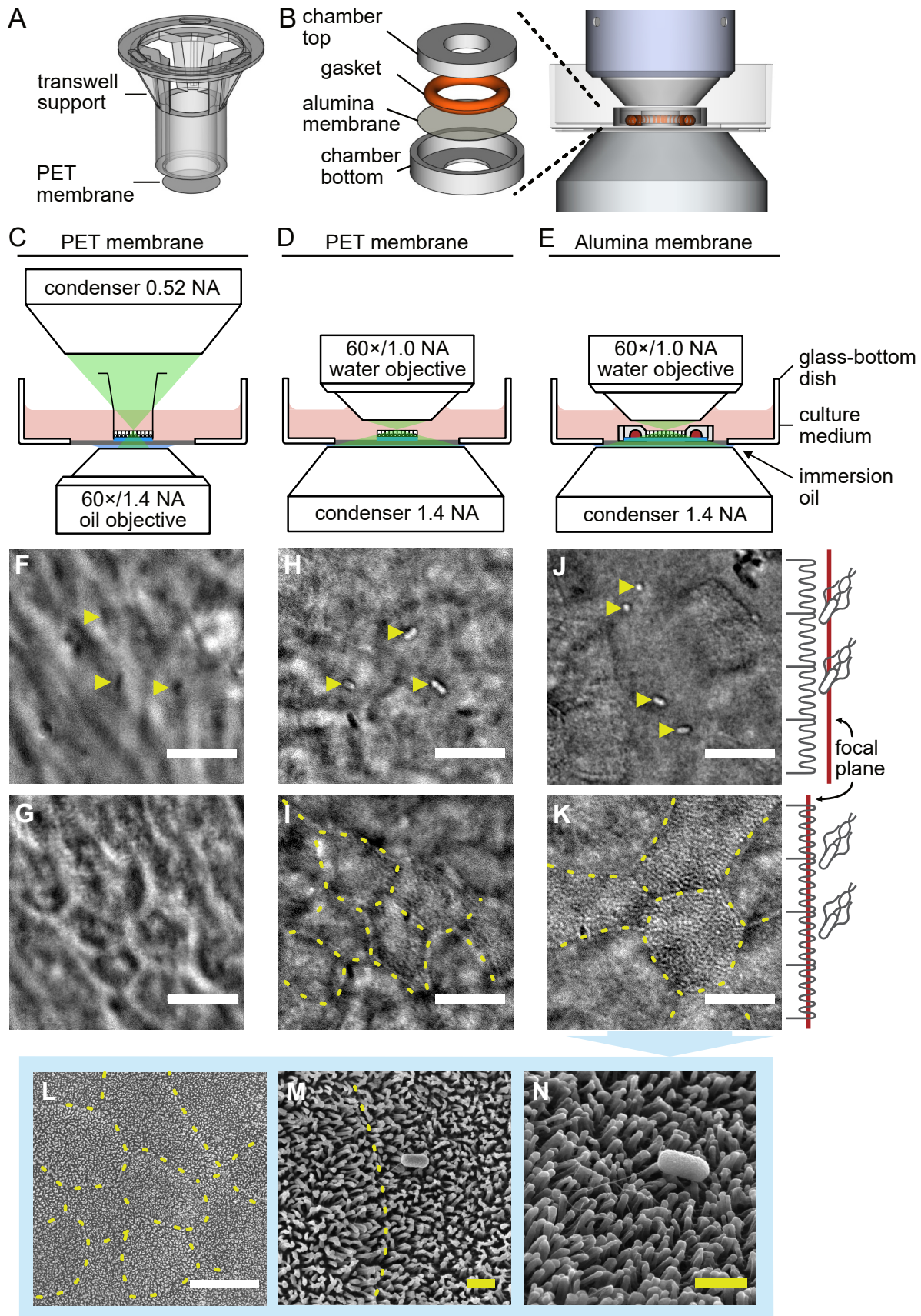


Figure 1. High-definition live cell DIC imaging of IEC monolayer infections in a novel alumina membrane chamber.

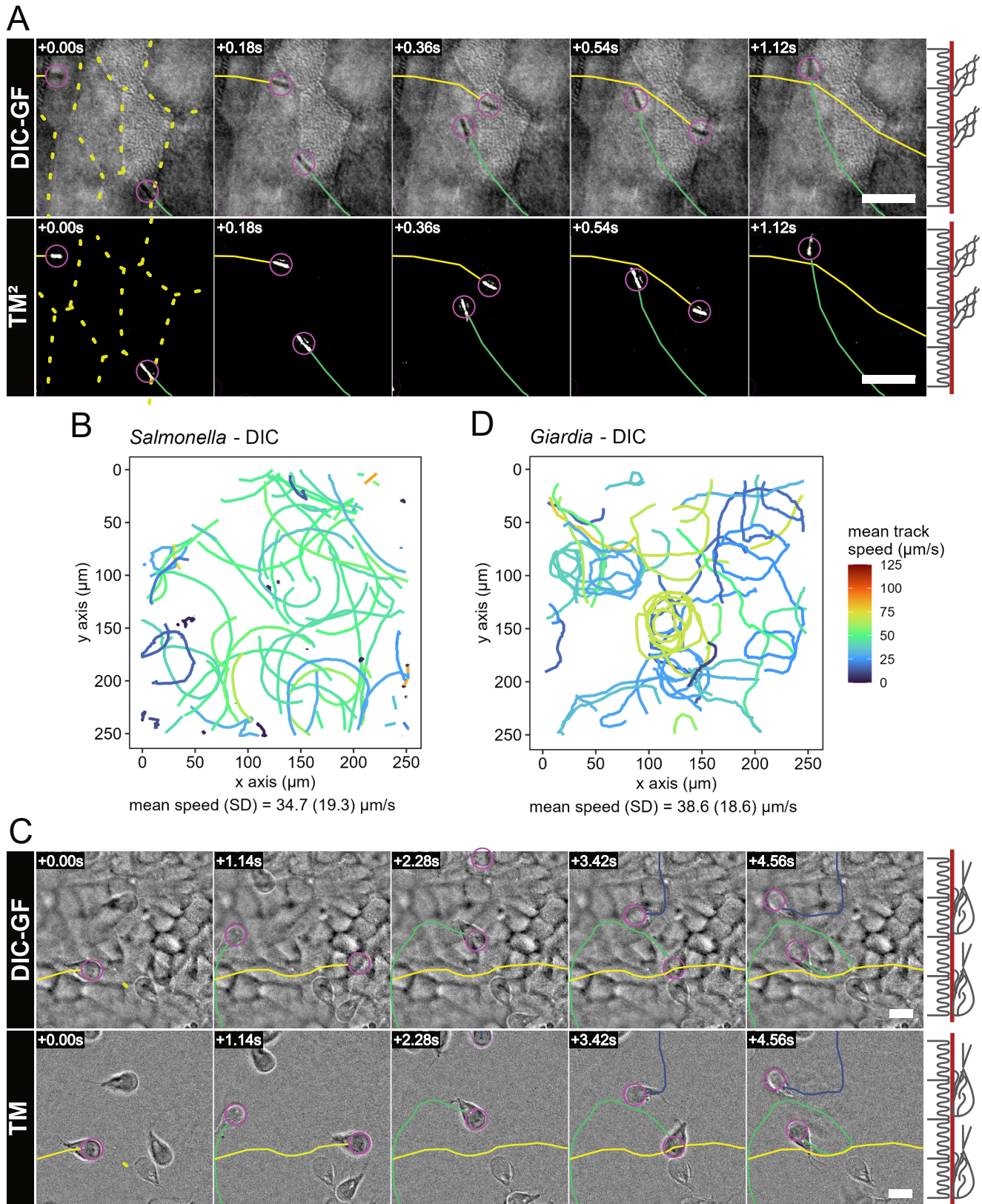


Figure 2. Tracking of microbes on IEC monolayers using DIC imaging resolve *Salmonella* and *Giardia* motility patterns.

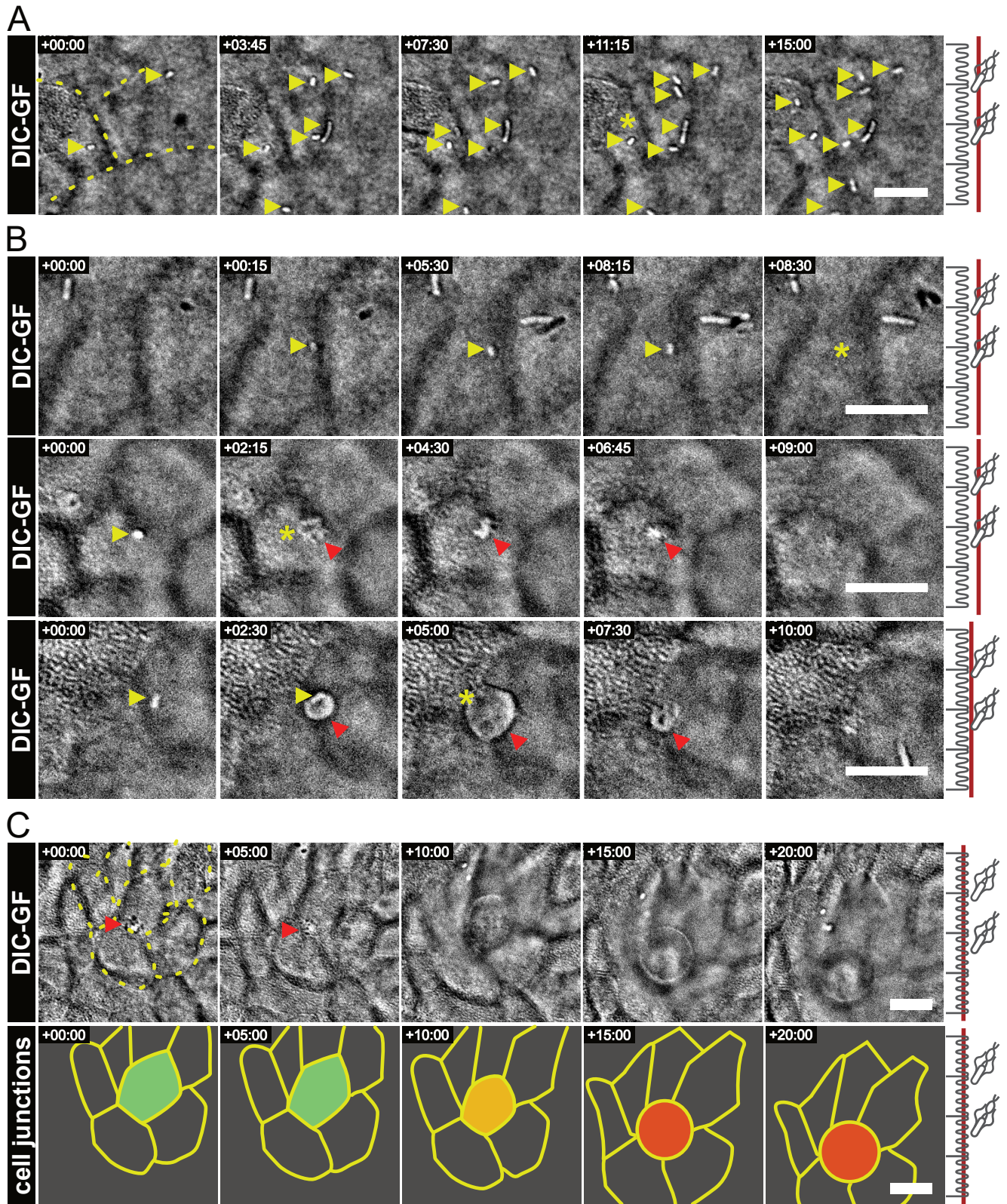


Figure 3. Salmonella infection cycle stages at the apical IEC surface.

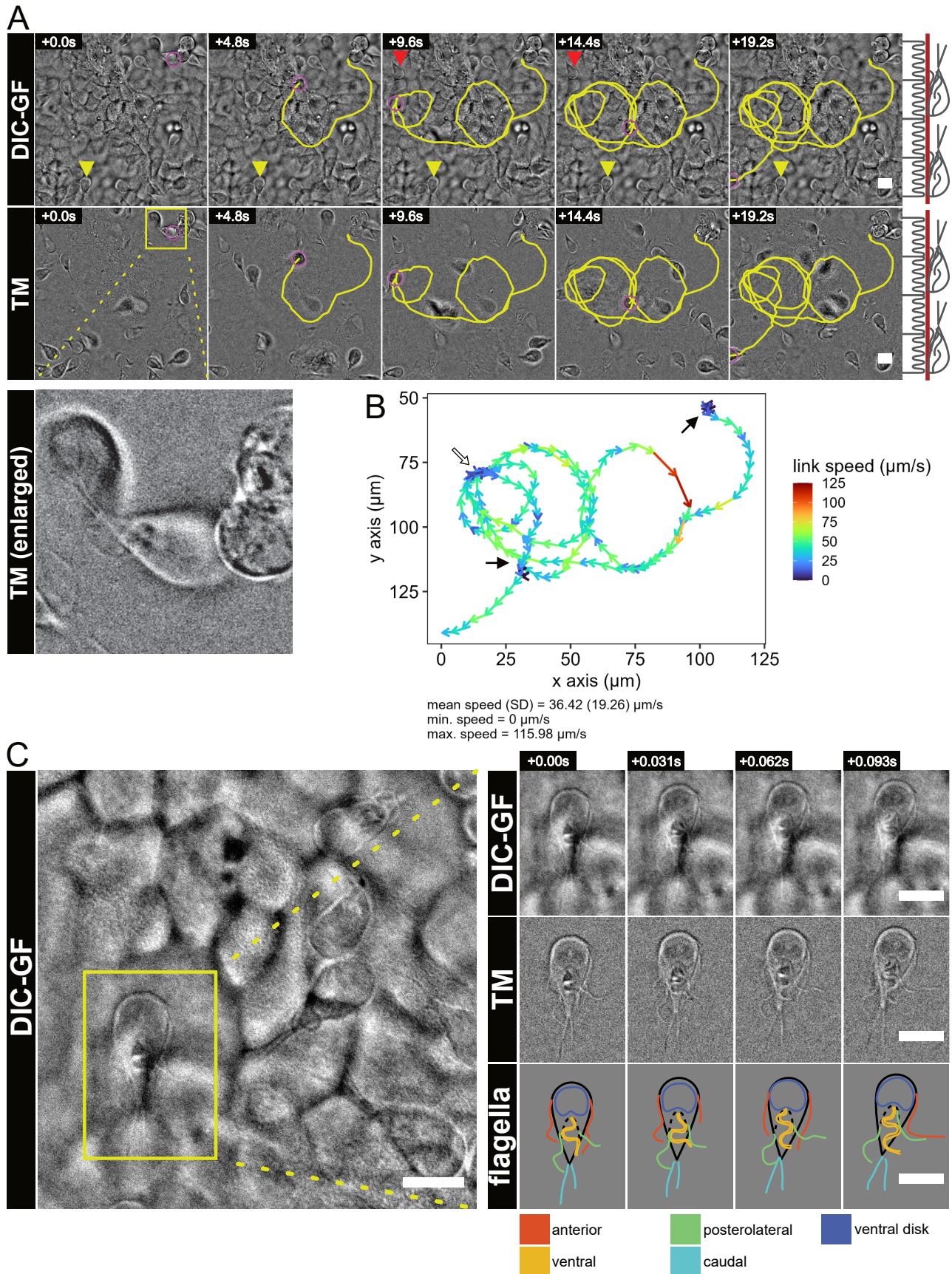


Figure 4. Giardia trophozoite exploration of the IEC surface.