

Association versus Prediction: the impact of cortical surface smoothing and parcellation on brain age

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7 **Abstract**

8 Association and prediction studies of the brain target the biological consequences of aging and their
9 impact on brain function. Such studies are conducted using different smoothing levels and parcellations
10 at the preprocessing stage, on which their results are dependent. However, the impact of these
11 parameters on the relationship between association values and prediction accuracy is not established.
12 In this study, we used cortical thickness and its relationship with age to investigate how different
13 smoothing and parcellation levels affect the detection of age-related brain correlates as well as brain
14 age prediction accuracy. Our main measures were resel numbers - resolution elements - and age-related
15 variance explained. Using these common measures enabled us to directly compare parcellation and
16 smoothing effects in both association and prediction studies. In our sample of N=608 participants with
17 age range 18-88, we evaluated age-related cortical thickness changes as well as brain age prediction.
18 We found a negative relationship between prediction performance and correlation values for both
19 parameters. Our results also quantify the relationship between delta age estimates obtained based on
20 different processing parameters. Furthermore, with the direct comparison of the two approaches, we
21 highlight the importance of correct choice of smoothing and parcellation parameters in each task, and
22 how they can affect the results of the analysis in opposite directions.

23 **1 Introduction**

24 From a biological standpoint, aging is defined by the structural and functional alterations in living
25 organisms (López-Otín et al., 2013). Traditionally, brain imaging studies have used neuroimaging data
26 to find associations between age and tissue alterations across brain areas, using chronological age as
27 the ground truth (Booth et al., 2013; Curiati et al., 2009; Hu et al., 2014; Lemaître et al., 2005;
28 Takahashi et al., 2011; Ziegler et al., 2012). However, biological age might vary between individuals
29 with identical chronological age as well as across different tissues within the same person (Horvath,
30 2013). To non-invasively measure the biological age of the brain, neuroimaging data is used to predict
31 age. The difference between predicted age and chronological age is then defined as “delta” or brain
32 age gap estimate i.e. “BrainAGE” to compare the subjects’ chronological age with the predicted brain
33 age in a given reference population (James H. Cole & Franke, 2017; Franke et al., 2012; Franke &
34 Gaser, 2019a; Smith et al., 2019a).

35 Both age related brain alterations and delta age have been studied and used extensively in the
36 neuroimaging literature. Age association studies translate and generalize easily across different

37 datasets. These association studies are applied across brain regions and can distinguish the differential
38 effect of age on different brain areas (Storsve et al., 2014). Furthermore, they directly relate to
39 biological measures and mechanistic changes in the brain (Khundrakpam et al., 2015). More recently,
40 it has been recognized that association studies are prone to overfitting and more studies focus on
41 prediction as the main goal of the study (Bzdok et al., 2020; Yarkoni & Westfall, 2017). Brain age
42 studies (i.e. age prediction studies based on neuroimaging data) rely on modeling and prediction
43 accuracy. This goal is generally achieved by using a feature set that can capture the variability between
44 and within subjects. On the other hand, prediction tasks face a trade-off between a more accurate whole
45 brain model with no regional specificity versus a model with lower accuracy and increased spatial
46 resolution (James H. Cole & Franke, 2017; Franke & Gaser, 2019a). This limitation also results in a
47 more indirect relationship between delta age and other phenotypes without a direct mechanistic and
48 biological model. Nonetheless, the difference between brain age and chronological age is associated
49 with cognitive decline (Gaser et al., 2013), predisposition to neuropsychiatric and neurodegenerative
50 disorders (Kaufmann et al., 2019), and mortality (J. H. Cole et al., 2018). While evidence supports the
51 application of delta age as a valuable measure to study aging in health and disease, it has been criticized
52 due to its reliance on prediction accuracy (i.e. more accurate models result in lower delta values) (James
53 H. Cole & Franke, 2017).

54 The results of both association studies and delta estimation studies are impacted by processing steps
55 such as data normalization, spatial resolution, and parcellation level (i.e. size of the parcels) of the
56 analysis. Most association studies use smoothing to (i) normalize the distributions of cortical thickness
57 across subjects, (ii) minimize registration and anatomical misalignment across subjects, (iii) reduce
58 measurement noise, and (iv) increase statistical power (Lerch et al., 2006; Lerch & Evans, 2005;
59 Worsley et al., 1999; Zhao et al., 2013). These advantages are gained at the cost of losing individual
60 variability and spatial resolution. In fact, smoothing has been studied and optimized for best
61 performance in association studies, using simulation as well as in real datasets. The smoothing level
62 has been proposed as a dimension within the parameter space in the association analysis that needs to
63 be searched for the given statistical contrast (Lerch & Evans, 2005; Zhao et al., 2013).

64 Brain age prediction studies have been conducted with various levels of data smoothing. Moreover,
65 these studies rely on various dimension reduction techniques, brain parcellations, or a combination of
66 the two approaches for feature extraction (Franke & Gaser, 2019b; Smith et al., 2019b). The optimal
67 parcellation for a given task is an open research topic and it can vary between studies (Eickhoff et al.,
68 2018; Gorgolewski et al., 2016; Salehi et al., 2020). While some studies have predicted brain age with
69 multiple parcellation resolutions (Khundrakpam et al., 2015; J. D. Lewis et al., 2019), others have used
70 a predetermined number of parcels. However, the effect of smoothing and parcellation in brain age
71 prediction is not studied systematically. Furthermore, these changes in prediction accuracy also affect
72 the delta estimate (i.e. the variable of interest), and it is not clear whether the delta estimates are robust
73 or sensitive toward these initial choices.

74 In this study, we used cortical thickness as the brain measure of interest and examined the effect of
75 smoothing and parcellation level on both brain associations with age and brain age prediction. Using
76 different levels of parcellation and smoothing, we projected brain measures onto a lower dimension
77 data representation space and investigated how this mapping affects the derived associations and
78 predictions. We further examined the relationship between the two approaches. Finally, we examined
79 how delta age estimates alter based on different smoothing and parcellation levels.

80 **2 Methods**

81 **2.1 Data**

82 Data used in this study included subjects with T1-weighted MRI data available from the second stage
83 of the Cambridge Centre for Ageing and Neuroscience (CamCAN, [https://www.cam-](https://www.cam-can.org/index.php?content=dataset)
84 [can.org/index.php?content=dataset](https://www.cam-can.org/index.php?content=dataset)) dataset, described in more detail in (Shafto et al., 2014; Taylor et
85 al., 2017). Subjects were screened for neurological and psychiatric conditions and those with such
86 underlying disorders were excluded from the study.

87 **2.2 MRI acquisition**

88 T1-weighted MRIs were acquired on a 3T Siemens TIM Trio, with a 32 channel head-coil using a 3D
89 magnetization-prepared rapid gradient echo (MPRAGE) sequence (TR=2250ms, TE=2.99ms,
90 TI=900ms; FA=9 deg; FOV=256x240x192mm; 1mm isotropic; GRAPPA=2; TA=4mins 32s). For
91 detailed acquisition parameters see:

92 https://camcan-archive.mrc-cbu.cam.ac.uk/dataaccess/pdfs/CAMCAN700_MR_params.pdf.

93 **2.3 MRI processing**

94 We used CIVET 2.1.1 (<http://www.bic.mni.mcgill.ca/ServicesSoftware/CIVET>, release December
95 2019), a fully automated structural image analysis pipeline developed at the Montreal Neurological
96 Institute, to perform surface extraction and cortical thickness estimation. Briefly, each subject's T1-
97 weighted MRI is corrected for nonuniformity artifacts using the N3 algorithm (N3 distance = 125 mm)
98 (Sled et al., 1998) and linearly registered to stereotaxic MNI152 space (voxel resolution = 0.5 mm)
99 (Collins et al., 1994). The brain is extracted and undergoes tissue classification into three classes: white
100 matter (WM) tissue, grey matter (GM) tissue, and cerebrospinal fluid (CSF) (Tohka et al., 2004;
101 Zijdenbos et al., 2002). White and grey matter surfaces are extracted using the marching cube algorithm
102 and constrained Laplacian-based automated segmentation with proximities (CLASP) algorithms,
103 respectively (Kabani et al., 2001; Kim et al., 2005; MacDonald et al., 2000). Using the extracted
104 surfaces, cortical thickness is measured as the distance between the white and grey cortical surfaces
105 using the Laplace's equation (Jones et al., 2000). For blurring, a surface-based diffusion smoothing
106 kernel (not to be confused with volumetric kernels) is used, which generalizes Gaussian kernel
107 smoothing and applies it to the curved cortical surfaces (Chung et al., 2002). We applied 6 different
108 smoothing levels with FWHM = 0, 5, 10, 20, 30, and 40 mm. Cortical thickness was measured across
109 the cortical surface for 81924 vertices (40962 vertices per hemisphere). The results underwent visual
110 inspection, specifically subjects with major errors in extracted pial and gray-white surfaces were
111 excluded.

112 **2.4 Cortical parcellations**

113 We used the Schaefer functional MRI parcellations (Schaefer et al., 2018), a data-driven atlas based
114 on the widely used seven large-scale functional network parcellations by (Thomas Yeo et al., 2011).
115 We used Schaefer parcellation with 100, 200, 400, and 1000 regions (referred to as parcellation levels).
116 All atlases were registered to the MNI cortical surface template and used in the MNI space (L. B. Lewis
117 et al., 2019). Cortical thickness measurements with different smoothing levels were averaged across
118 these parcellations. These parcellation based measures of cortical thickness were used alongside
119 vertex-wise measurements to examine the interaction between the effect of brain parcellation averaging
120 and smoothing on statistical associations as well as brain age prediction accuracies.

121 **2.5 Cortical resels and effective smoothing**

122 In order to compare the findings between smoothing levels and different parcellations, first all obtained
123 cortical thickness were projected to the brain surface. We used the number of resels (i.e. resolution
124 elements) as the measure of interest, since it takes the statistical dependence of the brain map into
125 consideration and is independent of the analysis resolution (at least from a theoretical standpoint)
126 (Lerch et al., 2006; Worsley, 1996; Worsley et al., 1992, 1999). Using the statistical maps between
127 aging and cortical thickness, we estimated the number of resels for each smoothing and parcellation
128 level and used it to quantify the similarity between these conditions. Resels are the number of resolution
129 elements approximated for a given search space (i.e. $D(S_2)$, $S_2 =$ brain surface) and a given smoothness
130 level FWHM. While the effective FWHM measure varies across brain areas, we defined the overall
131 effective smoothness of the brain map as the square root of the surface search space divided by the
132 number of resels estimated across brain areas (Hayasaka et al., 2004). For the purpose of the current
133 study, the main statistical maps considered are the linear associations between cortical thickness and
134 the chronological age of the participants. All analysis were performed using SurfStat toolbox
135 <https://www.math.mcgill.ca/keith/surfstat/>.

136 **2.6 Statistical methods**

137 To examine the effect of the smoothing and parcellations, mean (μ) and standard deviation (σ) of
138 cortical thickness for each vertex/parcel was calculated across the population. The coefficient of
139 variation (CV), $CV = \sigma/\mu$, was used as the main measure of variability. The CV was averaged across
140 the 7 main cytoarchitectural brain regions (von Economo, CF; Koskinas, 1927) in order to examine the
141 effect of parcellation and smoothing across major cytoarchitectural regions and identify any differential
142 impact on a given brain region. Finally, to measure the association between chronological age and
143 cortical thickness across lifespan, correlation coefficient (r) for each vertex/region was calculated.
144 Variance explained (r^2) was used to visualize the results.

145 **2.7 Brain age prediction**

146 We used principal component analysis (PCA), a singular value decomposition based data factorization
147 method, as the dimensionality reduction approach for our predictive variables (i.e. cortical thickness
148 data) (Smith et al., 2019b). This approach allowed us to use the same number of features across
149 parcellation levels and smoothing kernels and therefore made it possible to compare model
150 performance across these conditions. Our analysis for each condition included 1 to 100 first principal
151 components as features to study different levels of dimensionality reduction. 100 is used as the
152 maximum possible number of independent components for the lowest number of parcels (i.e. Schaefer
153 100). To predict brain age, we used linear regression as the main prediction model, and to ensure
154 generalizability and avoid overfitting, we used 10-fold cross validation. Finally, to increase robustness,
155 results averaged over 100 repetitions are reported. Root-mean-squared error (RMSE) was used as the
156 natural cost function for linear regression models. Mean absolute error (MAE) and correlation between
157 chronological age and predicted age (two other common error metrics in the age prediction literature
158 (Franke & Gaser, 2019b)) are also reported in the supplementary materials.

159 **2.8 The relationship between Brain age prediction and age related brain association**

160 To compare brain age association and age prediction, we used the variance explained between
161 dependent and independent variables as the main measure of interest for each model. This common
162 measure enabled us to quantify the two analyses in relation to each other. Furthermore, we examined
163 how the number of resels affects whole brain associations with age as well as brain age prediction. To
164 translate the age prediction error into variance explained, we used the predictive features in a linear
165 model, calculating the variance explained for age using adjusted R^2 . Finally, the overfitting bias

166 between the variance explained (i.e. adjusted R^2) using this linear model and the cross validated
167 prediction (i.e. r^2 between predicted age and chronological age) is reported.

168 **2.9 Delta age**

169 The main goal of brain age prediction studies is to calculate the deviation from chronological age based
170 on the population norm, also known as delta age. Here, we examined the effect of smoothing and
171 parcellation on delta age estimation:

$$172 \quad Y = X\beta_1 - \delta_1 \longrightarrow \delta_1 = X\beta_1 - Y$$

173 where Y denotes chronological age, X denotes the neuroimaging features, and δ_1 denotes the
174 difference between predicted and chronological age. δ_1 is a measure of brain state/health compared to
175 the population with similar chronological age, and is used to study the predisposition to different brain
176 disorders as well as individual cognitive abilities in neuroimaging literature.

177 δ_1 being residual of the predictive model is by definition: (1) orthogonal to the predictive measures X ,
178 and in the case of linear models (2) correlated with the output Y (i.e. chronological age) (Le et al., 2018;
179 Liang et al., 2019; Smith et al., 2019b). The first feature is unfavorable, since we are interested in brain
180 related discrepancy between chronological and predicted age. The lack of association between δ_1 and
181 brain features predicting age undermines the interpretability of δ_1 in relation to brain measures. The
182 second property is also an adverse feature, since it makes it difficult to distinguish the effect of the
183 chronological age from the additional biological delta age (due to their collinearity). Therefore, in the
184 current study, we followed the recommendation of Smith and colleagues (Smith et al., 2019b) and used
185 δ_2 , the orthogonalized residuals against chronological age:

$$186 \quad \delta_2 = \delta_1 - Y\beta_2$$

187 δ_2 is then used as the main measure of interest for association across conditions. The results for δ_1 is
188 provided in the supplementary materials. Note that δ_2 is also consistently calculated using the same
189 10-fold cross validation with 100 repeats as δ_1 . All statistical and prediction analyses were performed
190 using MATLAB 2018a.

191 **3 Results**

192 **3.1 Cortical thickness aging, resels and practical smoothness**

193 The parcellations have a considerable impact on the number of resels and function as region-based
194 smoothing kernels applied across the brain (Figure 1-A). This change in the number of resels affects
195 the statistical power and the association as well as prediction results. Across parcellation levels from
196 100 to 1000, the effect of the smaller smoothing kernels with FWHM 0-10 mm is negligible, while
197 applying larger kernels reduces the number of resels dramatically. This equivalency plot also suggests
198 that at the vertex level, the smoothing kernels act as a non-specific parcellation (from an anatomical
199 perspective) across the brain.

200 **3.2 Cortical thickness variability**

201 While keeping the mean cortical thickness measure intact, smoothing resulted in underestimation of
202 the cortical thickness in the gyri areas and overestimation in the sulci regions. The results are similar
203 for parcellations in the case of uniformly sized parcels and balanced inclusion of gyri and sulci in each

204 parcel (both criteria are met in Schaefer parcellations). Cortical thickness variability (i.e. CV) reduces
205 significantly both as a result of using greater smoothing and larger parcels (Figure 2-A).

206 The association cortices have the lowest CV across resolutions and parcellations. Both smoothing and
207 parcellation result in the highest decrease in CV in limbic and insular cortices, while primary sensory
208 and motor areas show the lowest change (Figure 2-B). The results are shown for 0 mm smoothing
209 across parcellations. The greatest change occurs with increasing the FWHM value from 10 to 20 mm,
210 as well as decreasing the number of parcels from 400 to 200. The results for different smoothing kernels
211 at vertex level were also similar (Supplementary Figure 1).

212 **3.3 statistical association between cortical thickness and aging**

213 Figure 3-A. shows the association between age and cortical thickness (using variance explained r^2),
214 calculated for each voxel/parcel for all conditions, after Bonferroni correction to account for the
215 multiple comparisons at each level. The correlation increases with greater smoothing and larger
216 parcels. Changing smoothing kernel size results in the highest variability in the correlation distribution
217 across the brain at vertex level resolution (Figure 3-B, top panel), whereas smoothing doesn't change
218 the results within Schaefer 100 parcellations (Figure 3-B, bottom panel). The same pattern is evident
219 between parcellation levels with 0 mm smoothing showing the highest variability, and 40 mm
220 smoothing with lowest variability across parcellations. These findings are further explained with
221 reference to the number of resels and effective smoothing in section 3.5. Finally, while present across
222 all brain areas, the variability between correlation maps is the highest within association cortices,
223 primary motor, and insular cortex.

224 **3.4 brain age prediction based on cortical thickness**

225 For age prediction, vertex-level data outperformed all parcellation-based data using the same (or a
226 smaller) number of principal components as predictive features. The accuracy was also higher for lower
227 smoothing kernel size. However, this effect was more pronounced for FWHMs greater than 10mm,
228 and the results for FWHM values of 0, 5, and 10 mm showed a very similar performance in the vertex-
229 level analysis. A similar pattern was present within each parcellation level. The best performing models
230 (i.e. 0 and 5 mm smoothed vertex-wise), reach their minimum error using the first 20-30 principal
231 components as features in the prediction model (i.e. a sample to feature ratio of 28-18). The pattern
232 was similar for MAE and correlation between predicted age and chronological age (Supplementary
233 Figure 2 and 3).

234 **3.5 The relationship between prediction and association**

235 As expected, there was a negative relationship between the overall correlation between age and cortical
236 thickness across brain regions (measured by median r^2) and the number of resels within each condition
237 (Figure 5-A). Interestingly, we found a positive association between the number of resels and the
238 overall ability of cortical thickness features to explain the variance of chronological age (as measured
239 by adjusted R^2 of the linear model) shown in Figure 5-B. These results suggest that the higher number
240 of resels results in lower correlation values, but since resels are independent based on their relationship
241 with age, they can explain different modes of chronological age within the population (hence the higher
242 adjusted R^2), whereas, in conditions with lower resel numbers (i.e. higher smoothing and larger
243 parcels) the correlation values are higher but homogenous across the brain and therefore explain a
244 lower proportion of the age variance.

245 Finally, there was a strong linear relationship between (i) the overall variance explained (adjusted R^2)
246 using a linear model with age as dependent variable and PCs as independent variable and (ii) the
247 predictive performance of the linear regression model, with a bias due to overfitting in the linear model
248 (Figure 5-C). Figure 5-D shows the overfitting bias of the adjusted R^2 compared to the cross-validated
249 prediction, as a function of the number of features in the model. Taken together, these results explain
250 the opposing directions between correlation results and prediction accuracy across parcellation and
251 smoothing conditions.

252 **3.6 The effect of smoothing and parcellation on the estimation of brain age delta**

253 In this section, we present δ_2 age prediction accuracy results with 10-fold cross validation. The
254 prediction accuracy based on the modified δ_2 is presented in Figure 6. One of the main assumptions in
255 age prediction studies is that delta age measured in different studies using different processing
256 parameters are similar and can be interpreted as the same measure. We have examined the relationship
257 between the optimal δ_2 across different parcellations and smoothing kernels (Figure 7). These results
258 demonstrate the degree of sensitivity of δ_2 as a function of our choice for parcellation and smoothing
259 kernel. While there is high correlation for large smoothing kernels (20-40 mm) as well as lower number
260 of parcels, these conditions have the lowest prediction accuracies. The correlations between these
261 conditions and higher accuracy conditions (i.e. vertex-wise and 1000 parcels with 0-10 mm smoothing)
262 are lower ($r \sim 0.55$). See the results for δ_1 in the Supplementary Figure 4.

263 **4 Discussion**

264 In this article, we compared the effect of different smoothing and parcellation on associations between
265 cortical thickness and chronological age as well as brain age prediction accuracy. We showed that the
266 optimal choice for association analysis might indeed undermine age prediction accuracy, and vice
267 versa. We further investigated this relationship and demonstrated the underlying differences that lead
268 to this trade-off between the two analyses. Finally, we examined the effect of smoothing and
269 parcellation on delta age estimation and showed that the initial smoothing and parcellation choices can
270 change the delta estimation which in turn will affect any downstream analysis.

271 We used brain association with age and brain age prediction as our target analyses, since age is used
272 as the main variable of interest or at least a confounding variable in most neuroimaging studies. We
273 used cortical thickness as the main measure of interest. Due to the wide availability of T1-weighted
274 MRI in research and clinical settings, cortical thickness is a suitable measure which has been widely
275 used to study brain anatomy in general (Toga, 2015), and more specifically, brain aging and predicting
276 brain age (Groves et al., 2012; Kandel et al., 2013; Liem et al., 2017; Wang & Pham, 2011). Finally,
277 our results are presented based on a sample size of $N \sim 600$ which is a common sample size for publicly
278 available datasets in the field of neuroimaging.

279 Given the limited number of subjects in neuroimaging studies compared to potential features (number
280 of vertices/voxels), most prediction studies apply dimension reduction as an initial step. We used PCA
281 for dimension reduction of the cortical thickness data. Due to its simplicity and interpretability, PCA
282 has been widely used in the brain age prediction literature. Furthermore, we employed linear regression
283 with cross-validation as our prediction model (Smith et al., 2019a). As expected, we observed an initial
284 drop in the prediction error, followed by a plateau/increase in the error as the sample to feature ratio
285 increases (Hastie et al., 2009). At each parcellation level, the accuracy drops with increased smoothing,
286 and for each smoothing level, the accuracy decreases with larger parcels/regions.

287 It is commonplace for neuroimaging studies to use smoothing and parcellation as the first step of their
288 analysis to achieve higher statistical power with reducing the individual variability within the data.
289 Furthermore, with increased availability of public neuroimaging datasets, it is commonplace to release
290 a preprocessed version of the data with a fixed smoothing level and averaged based on a given
291 parcellation. Many research groups in the field use preprocessed and parcellation-based data releases
292 as the starting point for their analyses. In fact, in many cases, the raw data is not publicly distributed,
293 and the preprocessed parcellated data is the only version of data available. For example, some of the
294 most influential public datasets in the field of neuroimaging such as Adolescent Brain Cognitive
295 Development (ABCD, for details see <https://nda.nih.gov/abcd>) Study and UKBiobank (for details see
296 <https://www.ukbiobank.ac.uk>) provide cortical thickness data using Desikan-Killiany-Tourville
297 parcellations (Klein & Tourville, 2012) with 62 regions (smoothing varies across studies) as one of
298 their pre-calculated measures. Our findings can help provide a guide to interpret these available
299 measures and shed light on the effect of these preselected parameters/parcellation when applied in
300 aging studies.

301 Higher correlation values across brain regions (as a result of smoothing) can be explained by increased
302 signal to noise ratio and reduced individual variability (Figure 2). The effect of smoothing on brain
303 related associations has previously been studied (Lerch & Evans, 2005). Indeed, Zhao and colleagues
304 propose smoothing as a scaling dimension which needs optimization for any given target analysis
305 (Zhao et al., 2013). The effect of parcellation on brain association has been addressed in several studies.
306 However, the optimal parcellation level is still an open question dependent on the specific case of
307 interest (Eickhoff et al., 2018). Here, we showed that parcellation level has a similar impact, by
308 reducing variability, using both CV (Figure 2) and number of resels (Figure 1).

309 In neuroimaging, smoothing and parcellations are generally studied separately. In this study, we used
310 a unified metric to directly compare the effect of smoothing and parcellation. Using resel numbers and
311 variance explained in the model, we have calculated common measures for both association and
312 prediction results. Our results show that with increased smoothing and larger parcels (i.e. lower number
313 of resels), cortical thickness variability reduces. This will remove inter-individual differences across
314 brain regions and result in higher associations between cortical thickness and aging (Figure 5-A).
315 However, while this improves the regional correlation with age, most of this general trend can be
316 captured in a few PCs (mainly the first component) and the rest of the PCs do not explain the remaining
317 variance of age. On the other hand, this relationship is reversed in the conditions with higher resel
318 numbers (i.e. lower smoothing and higher spatial resolutions). While in these cases higher regional
319 variability results in lower correlation with age, the age related associations capture different portions
320 of age variance in different PCs and overall they have a higher adjusted R^2 (Figure 5-B). There was a
321 consistent bias in the adjusted R^2 across conditions (Figure 5-C and 5-D), however, the effects
322 remained similar after removing the overfitting with cross-validation. Altogether, these analyses
323 explain the seeming opposite direction of correlation values and prediction accuracies for different
324 smoothing/parcellation levels in section 3.3 and 3.4.

325 Brain age studies investigate the relationship between and other phenotypes, using a given smoothing
326 and vertex/parcellation resolution as their initial step (James H. Cole & Franke, 2017). However, the
327 effect of the preprocessing condition on estimation is not studied. In the current manuscript, we found
328 a range of associations (0.5-1) between δ_2 s obtained in different conditions. These results suggest not
329 only that each study needs to optimize their choice of the smoothing and parcellation level, but also
330 when interpreting results from different studies in the field, these parameters should be considered.

331 One of the main limitations of the current study is the number of subjects (N~600), particularly given
332 that their age spans across 70 years. This leads to overfitting as the number of features increase. In fact,
333 for vertex-wise prediction (with 0 mm smoothing), the first 30 PCs only explain 20 % of the variability
334 in the data. This number is around 40% for 10 mm smoothing. In comparison, the first 30 PCs for 100
335 parcels explain 80 and 90% of the variance of the cortical thickness data for 0 mm and 40 mm
336 smoothing levels, respectively (Supplementary Figure 5). Given the higher performance of the vertex-
337 wise PCs at 0-10 mm smoothing, it is likely that with a larger sample size and increased sample to
338 feature ratio, the accuracy can be further improved. It should be noted that in each case the variance
339 explained corresponds to the total variability for the corresponding smoothing and parcellation
340 condition. Another limitation in the current study is the use of functionally driven Schaefer
341 parcellations. While this does not automatically suggest a disadvantage, multi-resolution anatomically
342 driven parcellations have the theoretical advantage of a more relevant initial feature space for cortical
343 thickness studies. Finally, CamCAN data used in our study is cross-sectional. This potentially
344 decreases the detection power of our study, since we can only estimate the effect of time between
345 subjects with individual variability as part of the measurement, whereas a longitudinal dataset can
346 decrease variability by estimating the effect of aging within subjects.

347 Traditionally, neuroimaging studies have targeted brain related associations with a given
348 phenotype/symptom or the statistical differences between different groups for a given brain region,
349 followed up with the association of these differences with a given biological or behavioral variable of
350 interest. More recently, there has been an ongoing conversation in the field towards prediction as an
351 alternative approach. Along the same line, the field of brain aging, has pursued age related associations
352 as well as age prediction. The relationship between the two approaches is often taken for granted (since
353 in ideal settings, i.e. large sample size and low inter-individual variability or noise levels, the results
354 would be equivalent) and ignored in practice. In this study, we have directly addressed both age
355 association and prediction as a function of smoothing and parcellation levels. Within our sample size,
356 we found an inverse relationship between regional age related associations and brain age prediction
357 accuracy as a function of smoothing and parcellation level, highlighting the importance of the
358 parameter selection based on the goal of the study.

359 **5 Conflict of Interest**

360 The authors declare no conflict of interest.

361 **6 Author Contributions**

362 YZ contributed to the study plan, analysed the data, and wrote the manuscript. AE contributed to the
363 study plan and revision of the manuscript.

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377 data analysis and the final manuscript.

378 **9 Data Availability Statement**

379 CamCAN dataset can be accessed after submitting an online application at [https://camcan-](https://camcan-archive.mrc-cbu.cam.ac.uk/dataaccess/datarequest.php)
380 [archive.mrc-cbu.cam.ac.uk/dataaccess/datarequest.php](https://camcan-archive.mrc-cbu.cam.ac.uk/dataaccess/datarequest.php) and accepting the use agreement. Detailed
381 information available at <https://www.cam-can.org> .

382 **10 Reference**

- 383 Booth, T., Starr, J. M., & Deary, I. (2013). Modeling multisystem biological risk in later life:
384 Allostatic load in the lothian birth cohort study 1936. *American Journal of Human Biology*,
385 25(4), 538–543. <https://doi.org/10.1002/ajhb.22406>
- 386 Bzdok, D., Varoquaux, G., & Steyerberg, E. W. (2020). Prediction, not association, paves the road to
387 precision medicine. In *JAMA Psychiatry*. <https://doi.org/10.1001/jamapsychiatry.2020.2549>
- 388 Chung, M., Worsley, K., Paus, T., Robbins, S., Evans, A. C., Taylor, J., Giedd, J. N., & Rapoport, J.
389 L. (2002). Tensor-based surface morphometry. In *University of Wisconsin* (Issue 1049).
390 <http://www.stat.wisc.edu/~mchung>
- 391 Cole, J. H., Ritchie, S. J., Bastin, M. E., Valdés Hernández, M. C., Muñoz Maniega, S., Royle, N.,
392 Corley, J., Pattie, A., Harris, S. E., Zhang, Q., Wray, N. R., Redmond, P., Marioni, R. E., Starr,
393 J. M., Cox, S. R., Wardlaw, J. M., Sharp, D. J., & Deary, I. J. (2018). Brain age predicts
394 mortality. *Molecular Psychiatry*, 23(5), 1385–1392. <https://doi.org/10.1038/mp.2017.62>
- 395 Cole, James H., & Franke, K. (2017). Predicting Age Using Neuroimaging: Innovative Brain Ageing
396 Biomarkers. In *Trends in Neurosciences* (Vol. 40, Issue 12, pp. 681–690). Elsevier Ltd.
397 <https://doi.org/10.1016/j.tins.2017.10.001>
- 398 Collins, D. L., Neelin, P., Peters, T. M., & Evans, A. C. (1994). Automatic 3d intersubject
399 registration of mr volumetric data in standardized talairach space. *Journal of Computer Assisted*
400 *Tomography*, 18(2), 192–205. <https://doi.org/10.1097/00004728-199403000-00005>
- 401 Curiati, P. K., Tamashiro, J. H., Squarzoni, P., Duran, F. L. S., Santos, L. C., Wajngarten, M., Leite,
402 C. C., Vallada, H., Menezes, P. R., Scazufca, M., Busatto, G. F., & Alves, T. C. T. F. (2009).
403 Brain structural variability due to aging and gender in cognitively healthy elders: Results from
404 the São Paulo ageing and health study. *American Journal of Neuroradiology*, 30(10), 1850–
405 1856. <https://doi.org/10.3174/ajnr.A1727>
- 406 Eickhoff, S. B., Yeo, B. T. T., & Genon, S. (2018). Imaging-based parcellations of the human brain.
407 In *Nature Reviews Neuroscience* (Vol. 19, Issue 11, pp. 672–686).
408 <https://doi.org/10.1038/s41583-018-0071-7>

- 409 Franke, K., & Gaser, C. (2019a). Ten years of brainage as a neuroimaging biomarker of brain aging:
410 What insights have we gained? In *Frontiers in Neurology* (Vol. 10, Issue JUL). Frontiers Media
411 S.A. <https://doi.org/10.3389/fneur.2019.00789>
- 412 Franke, K., & Gaser, C. (2019b). Ten years of brainage as a neuroimaging biomarker of brain aging:
413 What insights have we gained? In *Frontiers in Neurology* (Vol. 10, Issue JUL).
414 <https://doi.org/10.3389/fneur.2019.00789>
- 415 Franke, K., Luders, E., May, A., Wilke, M., & Gaser, C. (2012). Brain maturation: Predicting
416 individual BrainAGE in children and adolescents using structural MRI. *NeuroImage*, 63(3),
417 1305–1312. <https://doi.org/10.1016/j.neuroimage.2012.08.001>
- 418 Gaser, C., Franke, K., Klöppel, S., Koutsouleris, N., & Sauer, H. (2013). BrainAGE in Mild
419 Cognitive Impaired Patients: Predicting the Conversion to Alzheimer’s Disease. *PLoS ONE*,
420 8(6). <https://doi.org/10.1371/journal.pone.0067346>
- 421 Gorgolewski, K., Tambini, A., Durnez, J., Sochat, V., Wexler, J., & Poldrack, R. (2016). Evaluation
422 of full brain parcellation schemes using the NeuroVault database of statistical maps.
423 *Organisation for Human Brain Mapping 2016 Annual Meeting*, 2201.
424 <https://54.246.141.91/posters/6-1986>
- 425 Groves, A. R., Smith, S. M., Fjell, A. M., Tamnes, C. K., Walhovd, K. B., Douaud, G., Woolrich, M.
426 W., & Westlye, L. T. (2012). Benefits of multi-modal fusion analysis on a large-scale dataset:
427 Life-span patterns of inter-subject variability in cortical morphometry and white matter
428 microstructure. *NeuroImage*, 63(1), 365–380. <https://doi.org/10.1016/j.neuroimage.2012.06.038>
- 429 Hastie, T., Tibshirani, R., & Friedman, J. (2009). *Springer Series in Statistics The Elements of*
430 *Statistical Learning Data Mining, Inference, and Prediction*.
431 [https://books.google.ca/books?hl=en&lr=&id=tVIjmNS3Ob8C&oi=fnd&pg=PR13&dq=trevor+](https://books.google.ca/books?hl=en&lr=&id=tVIjmNS3Ob8C&oi=fnd&pg=PR13&dq=trevor+hastie++book&ots=EOBcP9J5X5&sig=w9Dod2i1zZD9tkzSKn0TPwDs1UE)
432 [hastie++book&ots=EOBcP9J5X5&sig=w9Dod2i1zZD9tkzSKn0TPwDs1UE](https://books.google.ca/books?hl=en&lr=&id=tVIjmNS3Ob8C&oi=fnd&pg=PR13&dq=trevor+hastie++book&ots=EOBcP9J5X5&sig=w9Dod2i1zZD9tkzSKn0TPwDs1UE)
- 433 Hayasaka, S., Phan, K. L., Liberzon, I., Worsley, K. J., & Nichols, T. E. (2004). Nonstationary
434 cluster-size inference with random field and permutation methods. *NeuroImage*, 22(2), 676–
435 687. <https://doi.org/10.1016/j.neuroimage.2004.01.041>
- 436 Horvath, S. (2013). DNA methylation age of human tissues and cell types. *Genome Biology*, 14(10).
437 <https://doi.org/10.1186/gb-2013-14-10-r115>
- 438 Hu, S., Chao, H. H. A., Zhang, S., Ide, J. S., & Li, C. S. R. (2014). Changes in cerebral morphometry
439 and amplitude of low-frequency fluctuations of BOLD signals during healthy aging: Correlation
440 with inhibitory control. *Brain Structure and Function*, 219(3), 983–994.
441 <https://doi.org/10.1007/s00429-013-0548-0>
- 442 Jones, S. E., Buchbinder, B. R., & Aharon, I. (2000). Three-dimensional mapping of cortical
443 thickness using Laplace’s equation. *Human Brain Mapping*, 11(1), 12–32.
444 [https://doi.org/10.1002/1097-0193\(200009\)11:1<12::AID-HBM20>3.0.CO;2-K](https://doi.org/10.1002/1097-0193(200009)11:1<12::AID-HBM20>3.0.CO;2-K)
- 445 Kabani, N., Le Goualher, G., Macdonald, D., & Evans, A. C. (2001). Measurement of Cortical
446 Thickness Using an Automated 3-D Algorithm: A Validation Study. *Elsevier*.
447 <https://doi.org/10.1006/nimg.2000.0652>

- 448 Kandel, B. M., Wolk, D. A., Gee, J. C., & Avants, B. (2013). Predicting cognitive data from medical
449 images using sparse linear regression. *Lecture Notes in Computer Science (Including Subseries*
450 *Lecture Notes in Artificial Intelligence and Lecture Notes in Bioinformatics)*, 7917 LNCS, 86–
451 97. https://doi.org/10.1007/978-3-642-38868-2_8
- 452 Kaufmann, T., van der Meer, D., Doan, N. T., Schwarz, E., Lund, M. J., Agartz, I., Alnæs, D., Barch,
453 D. M., Baur-Streubel, R., Bertolino, A., Bettella, F., Beyer, M. K., Bøen, E., Borgwardt, S.,
454 Brandt, C. L., Buitelaar, J., Celius, E. G., Cervenka, S., Conzelmann, A., ... Westlye, L. T.
455 (2019). Common brain disorders are associated with heritable patterns of apparent aging of the
456 brain. *Nature Neuroscience*, 22(10), 1617–1623. <https://doi.org/10.1038/s41593-019-0471-7>
- 457 Khundrakpam, B. S., Tohka, J., Evans, A. C., Ball, W. S., Byars, A. W., Schapiro, M., Bommer, W.,
458 Carr, A., German, A., Dunn, S., Rivkin, M. J., Waber, D., Mulkern, R., Vajapeyam, S.,
459 Chiverton, A., Davis, P., Koo, J., Marmor, J., Mrakotsky, C., ... O'Neill, J. (2015). Prediction of
460 brain maturity based on cortical thickness at different spatial resolutions. *NeuroImage*, 111,
461 350–359. <https://doi.org/10.1016/j.neuroimage.2015.02.046>
- 462 Kim, J., Singh, V., Jun, K. L., Lerch, J., Ad-Dab'bagh, Y., MacDonald, D., Jong, M. L., Kim, S. I., &
463 Evans, A. C. (2005). Automated 3-D extraction and evaluation of the inner and outer cortical
464 surfaces using a Laplacian map and partial volume effect classification. *NeuroImage*, 27(1),
465 210–221. <https://doi.org/10.1016/j.neuroimage.2005.03.036>
- 466 Klein, A., & Tourville, J. (2012). 101 labeled brain images and a consistent human cortical labeling
467 protocol. *Frontiers in Neuroscience, DEC*. <https://doi.org/10.3389/fnins.2012.00171>
- 468 Le, T. T., Kuplicki, R. T., McKinney, B. A., Yeh, H.-W., Thompson, W. K., & Paulus, M. P. (2018).
469 A Nonlinear Simulation Framework Supports Adjusting for Age When Analyzing BrainAGE.
470 *Frontiers in Aging Neuroscience*, 10. <https://doi.org/10.3389/fnagi.2018.00317>
- 471 Lemaître, H., Crivello, F., Grassiot, B., Alperovitch, A., Tzourio, C., & Mazoyer, B. (2005). Age-
472 and sex-related effects on the neuroanatomy of healthy elderly. *NeuroImage*, 26(3), 900–911.
473 <https://doi.org/10.1016/j.neuroimage.2005.02.042>
- 474 Lerch, J. P., & Evans, A. C. (2005). Cortical thickness analysis examined through power analysis and
475 a population simulation. *NeuroImage*, 24(1), 163–173.
476 <https://doi.org/10.1016/j.neuroimage.2004.07.045>
- 477 Lerch, J. P., Worsley, K., Shaw, W. P., Greenstein, D. K., Lenroot, R. K., Giedd, J., & Evans, A. C.
478 (2006). Mapping anatomical correlations across cerebral cortex (MACACC) using cortical
479 thickness from MRI. *NeuroImage*, 31(3), 993–1003.
480 <https://doi.org/10.1016/j.neuroimage.2006.01.042>
- 481 Lewis, J. D., Fonov, V. S., Collins, D. L., Evans, A. C., & Tohka, J. (2019). Cortical and subcortical
482 T1 white/gray contrast, chronological age, and cognitive performance. *NeuroImage*, 196, 276–
483 288. <https://doi.org/10.1016/j.neuroimage.2019.04.022>
- 484 Lewis, L. B., Lepage, C. Y., & Evans, A. C. (2019). An extended MSM surface registration pipeline
485 to bridge atlases across the MNI and the FS/HCP worlds. *Annual Meeting of the Organization*
486 *for Human Brain Mapping*.
487 <https://ww5.aievolution.com/hbm1901/index.cfm?do=abs.viewAbs&abs=1243>

- 488 Liang, H., Zhang, F., & Niu, X. (2019). Investigating systematic bias in brain age estimation with
489 application to post-traumatic stress disorders. *Human Brain Mapping*, *40*(11), 3143–3152.
490 <https://doi.org/10.1002/hbm.24588>
- 491 Liem, F., Varoquaux, G., Kynast, J., Beyer, F., Kharabian Masouleh, S., Huntenburg, J. M., Lampe,
492 L., Rahim, M., Abraham, A., Craddock, R. C., Riedel-Heller, S., Luck, T., Loeffler, M.,
493 Schroeter, M. L., Witte, A. V., Villringer, A., & Margulies, D. S. (2017). Predicting brain-age
494 from multimodal imaging data captures cognitive impairment. *NeuroImage*, *148*, 179–188.
495 <https://doi.org/10.1016/j.neuroimage.2016.11.005>
- 496 López-Otín, C., Blasco, M. A., Partridge, L., Serrano, M., & Kroemer, G. (2013). The hallmarks of
497 aging. In *Cell* (Vol. 153, Issue 6, p. 1194). Cell Press. <https://doi.org/10.1016/j.cell.2013.05.039>
- 498 MacDonald, D., Kabani, N., Avis, D., & Evans, A. C. (2000). Automated 3-D extraction of inner and
499 outer surfaces of cerebral cortex from MRI. *NeuroImage*, *12*(3), 340–356.
500 <https://doi.org/10.1006/nimg.1999.0534>
- 501 Salehi, M., Greene, A. S., Karbasi, A., Shen, X., Scheinost, D., & Constable, R. T. (2020). There is
502 no single functional atlas even for a single individual: Functional parcel definitions change with
503 task. *NeuroImage*, *208*. <https://doi.org/10.1016/j.neuroimage.2019.116366>
- 504 Schaefer, A., Kong, R., Gordon, E. M., Laumann, T. O., Zuo, X.-N., Holmes, A. J., Eickhoff, S. B.,
505 & Yeo, B. T. T. (2018). Local-Global Parcellation of the Human Cerebral Cortex from Intrinsic
506 Functional Connectivity MRI. *Cerebral Cortex*, *28*(9), 3095–3114.
507 <https://doi.org/10.1093/cercor/bhx179>
- 508 Shafto, M. A., Tyler, L. K., Dixon, M., Taylor, J. R., Rowe, J. B., Cusack, R., Calder, A. J., Marslen-
509 Wilson, W. D., Duncan, J., Dalgleish, T., Henson, R. N., Brayne, C., Bullmore, E., Campbell,
510 K., Cheung, T., Davis, S., Geerligs, L., Kievit, R., McCarrey, A., ... Matthews, F. E. (2014).
511 The Cambridge Centre for Ageing and Neuroscience (Cam-CAN) study protocol: A cross-
512 sectional, lifespan, multidisciplinary examination of healthy cognitive ageing. *BMC Neurology*,
513 *14*(1). <https://doi.org/10.1186/s12883-014-0204-1>
- 514 Sled, J. G., Zijdenbos, A. P., & Evans, A. C. (1998). A nonparametric method for automatic
515 correction of intensity nonuniformity in mri data. *IEEE Transactions on Medical Imaging*,
516 *17*(1), 87–97. <https://doi.org/10.1109/42.668698>
- 517 Smith, S. M., Vidaurre, D., Alfaro-Almagro, F., Nichols, T. E., & Miller, K. L. (2019a). Estimation
518 of Brain Age Delta from Brain Imaging. In *bioRxiv*. <https://doi.org/10.1101/560151>
- 519 Smith, S. M., Vidaurre, D., Alfaro-Almagro, F., Nichols, T. E., & Miller, K. L. (2019b). Estimation
520 of brain age delta from brain imaging. *NeuroImage*, *200*, 528–539.
521 <https://doi.org/10.1016/j.neuroimage.2019.06.017>
- 522 Storsve, A. B., Fjell, A. M., Tamnes, C. K., Westlye, L. T., Overbye, K., Aasland, H. W., &
523 Walhovd, K. B. (2014). Differential longitudinal changes in cortical thickness, surface area and
524 volume across the adult life span: Regions of accelerating and decelerating change. *Journal of*
525 *Neuroscience*, *34*(25), 8488–8498. <https://doi.org/10.1523/JNEUROSCI.0391-14.2014>
- 526 Takahashi, R., Ishii, K., Kakigi, T., & Yokoyama, K. (2011). Gender and age differences in normal

- 527 adult human brain: Voxel-based morphometric study. *Human Brain Mapping*, 32(7), 1050–
528 1058. <https://doi.org/10.1002/hbm.21088>
- 529 Taylor, J. R., Williams, N., Cusack, R., Auer, T., Shafto, M. A., Dixon, M., Tyler, L. K., Cam-CAN,
530 & Henson, R. N. (2017). The Cambridge Centre for Ageing and Neuroscience (Cam-CAN) data
531 repository: Structural and functional MRI, MEG, and cognitive data from a cross-sectional adult
532 lifespan sample. *NeuroImage*, 144, 262–269. <https://doi.org/10.1016/j.neuroimage.2015.09.018>
- 533 Thomas Yeo, B. T., Krienen, F. M., Sepulcre, J., Sabuncu, M. R., Lashkari, D., Hollinshead, M.,
534 Roffman, J. L., Smoller, J. W., Zöllei, L., Polimeni, J. R., Fisch, B., Liu, H., & Buckner, R. L.
535 (2011). The organization of the human cerebral cortex estimated by intrinsic functional
536 connectivity. *Journal of Neurophysiology*, 106(3), 1125–1165.
537 <https://doi.org/10.1152/jn.00338.2011>
- 538 Toga, A. W. (2015). Brain Mapping: An Encyclopedic Reference. In *Brain Mapping: An*
539 *Encyclopedic Reference* (Vols. 1–3). <https://doi.org/10.1016/C2011-1-07037-6>
- 540 Tohka, J., Zijdenbos, A., & Evans, A. (2004). Fast and robust parameter estimation for statistical
541 partial volume models in brain MRI. *NeuroImage*, 23(1), 84–97.
542 <https://doi.org/10.1016/j.neuroimage.2004.05.007>
- 543 von Economo, CF; Koskinas, G. (1927). Die Cytoarchitektonik der Hirnrinde des erwachsenen
544 Menschen. *Journal of Anatomy*, 61, 264–266.
545 [https://scholar.google.com/scholar?q=Von+Economo+C%2C+Koskinas+G.+Die+Cytoarchitekt
546 onik+der+Hirnrinde+des+erwachsenen+Menschen.+Berlin%3A+Springer%3B+1925.](https://scholar.google.com/scholar?q=Von+Economo+C%2C+Koskinas+G.+Die+Cytoarchitekt+onik+der+Hirnrinde+des+erwachsenen+Menschen.+Berlin%3A+Springer%3B+1925.)
- 547 Wang, B., & Pham, T. D. (2011). MRI-based age prediction using hidden Markov models. *Journal of*
548 *Neuroscience Methods*, 199(1), 140–145. <https://doi.org/10.1016/j.jneumeth.2011.04.022>
- 549 Worsley, K. J. (1996). An unbiased estimator for the roughness of a multivariate Gaussian random
550 eld 1 Model. *Pdfs.Semanticscholar.Org*, 1–5.
551 <https://pdfs.semanticscholar.org/4159/a64da50863a945c8af38c42f8b09487a985b.pdf>
- 552 Worsley, K. J., Andermann, M., Koulis, T., MacDonald, D., & Evans, A. C. (1999). Detecting
553 changes in nonisotropic images. *Human Brain Mapping*, 8(2–3), 98–101.
554 [https://doi.org/10.1002/\(SICI\)1097-0193\(1999\)8:2/3<98::AID-HBM5>3.0.CO;2-F](https://doi.org/10.1002/(SICI)1097-0193(1999)8:2/3<98::AID-HBM5>3.0.CO;2-F)
- 555 Worsley, K. J., Evans, A. C., Marrett, S., & Neelin, P. (1992). A three-dimensional statistical
556 analysis for CBF activation studies in human brain. *Journal of Cerebral Blood Flow and*
557 *Metabolism*, 12(6), 900–918. <https://doi.org/10.1038/jcbfm.1992.127>
- 558 Yarkoni, T., & Westfall, J. (2017). Choosing Prediction Over Explanation in Psychology: Lessons
559 From Machine Learning. *Perspectives on Psychological Science*, 12(6), 1100–1122.
560 <https://doi.org/10.1177/1745691617693393>
- 561 Zhao, L., Boucher, M., Rosa-Neto, P., & Evans, A. C. (2013). Impact of scale space search on age-
562 and gender-related changes in MRI-based cortical morphometry. *Human Brain Mapping*, 34(9),
563 2113–2128. <https://doi.org/10.1002/hbm.22050>
- 564 Ziegler, G., Dahnke, R., Jäncke, L., Yotter, R. A., May, A., & Gaser, C. (2012). Brain structural

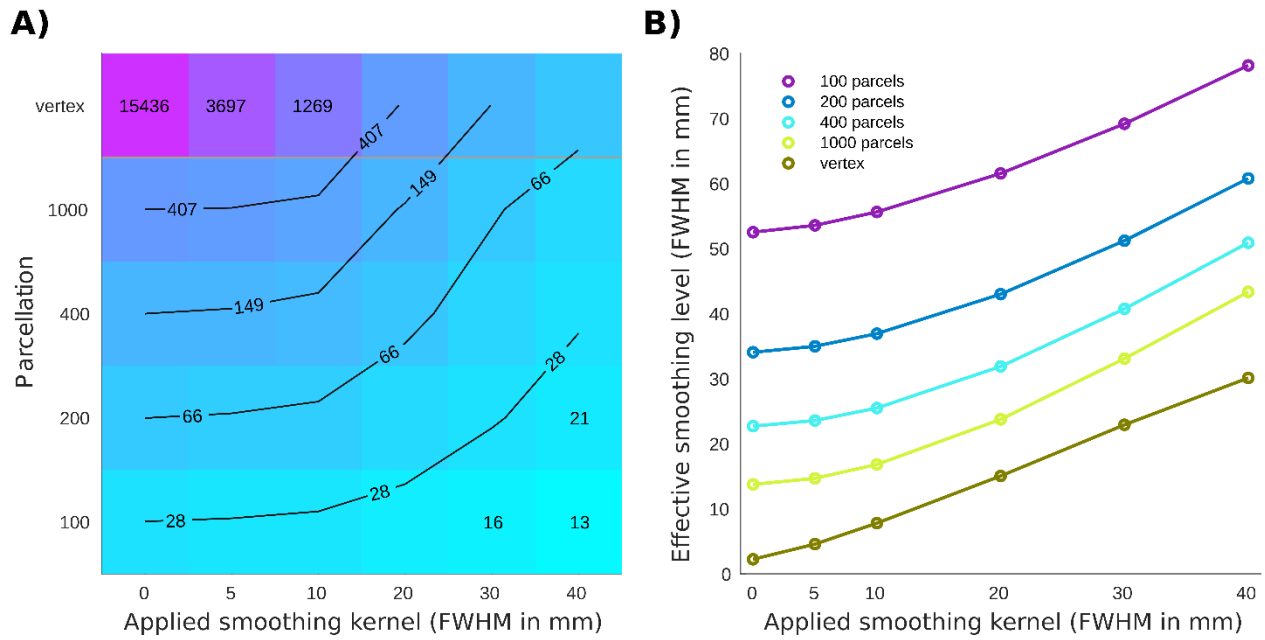
565 trajectories over the adult lifespan. *Human Brain Mapping*, 33(10), 2377–2389.
566 <https://doi.org/10.1002/hbm.21374>

567 Zijdenbos, A. P., Forghani, R., & Evans, A. C. (2002). Automatic “pipeline” analysis of 3-D MRI
568 data for clinical trials: Application to multiple sclerosis. *IEEE Transactions on Medical*
569 *Imaging*, 21(10), 1280–1291. <https://doi.org/10.1109/TMI.2002.806283>

570

571

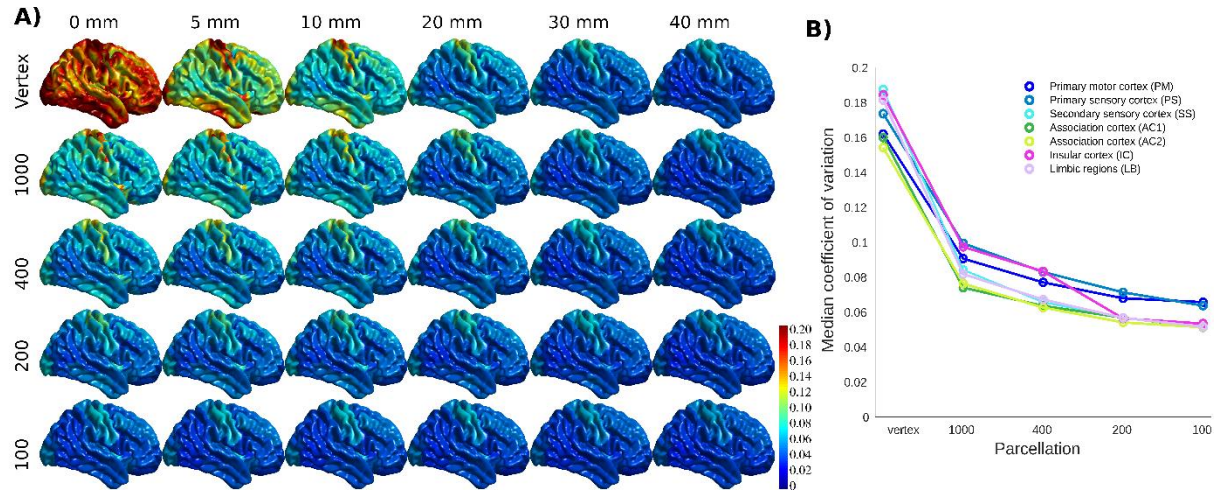
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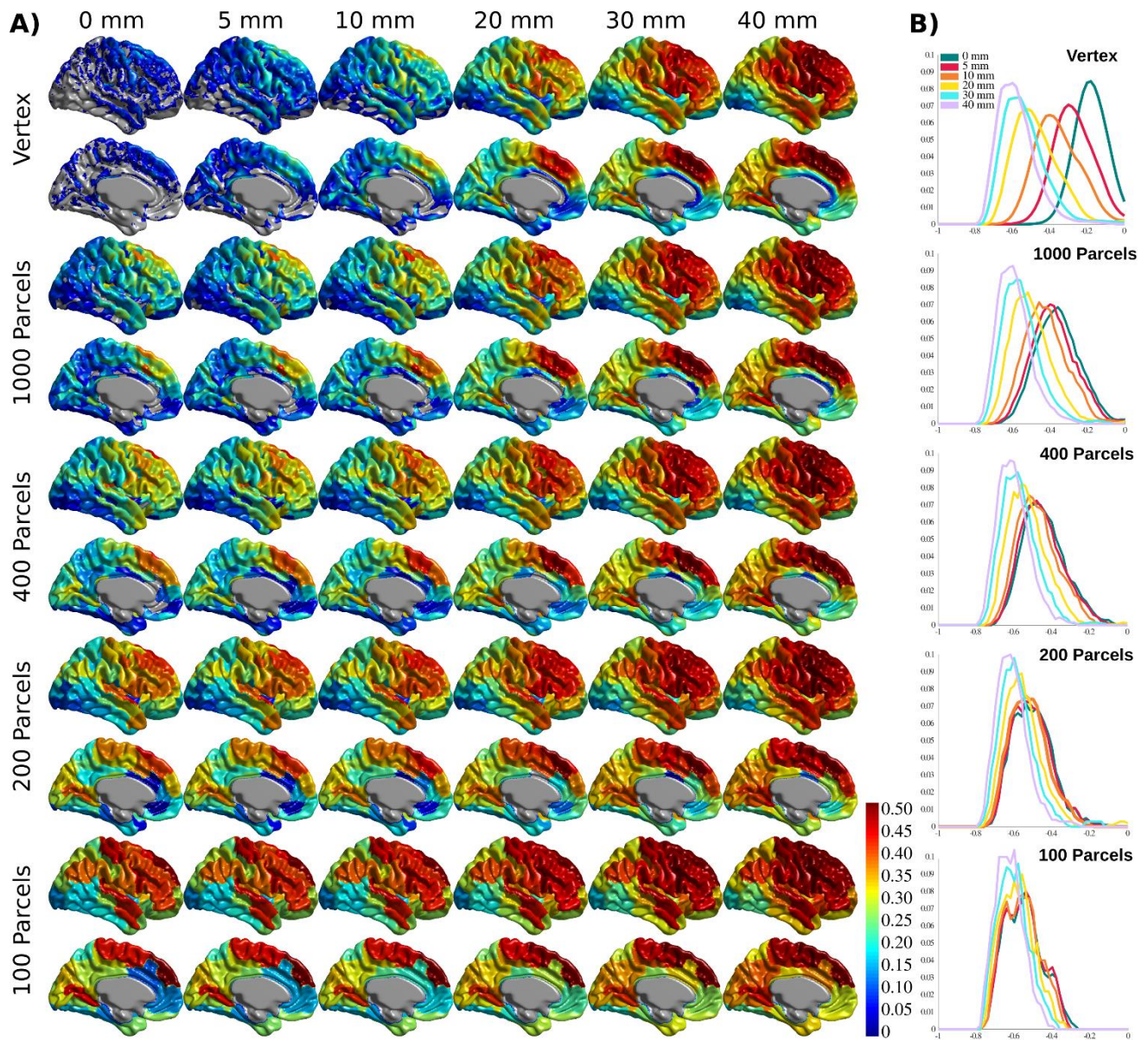
574 **Figure 1** | Number of resels and affective smoothing for cortical thickness association with age. **A)**
575 Number of resels estimated for different parcellations/smoothing pairs. The lines show the interpolated
576 iso-response values. **B)** Effective smoothing based on the number of resels for each condition. The
577 results show the initial effective smoothing as a result of parcellation with additional smoothing with
578 applied smoothing kernels.

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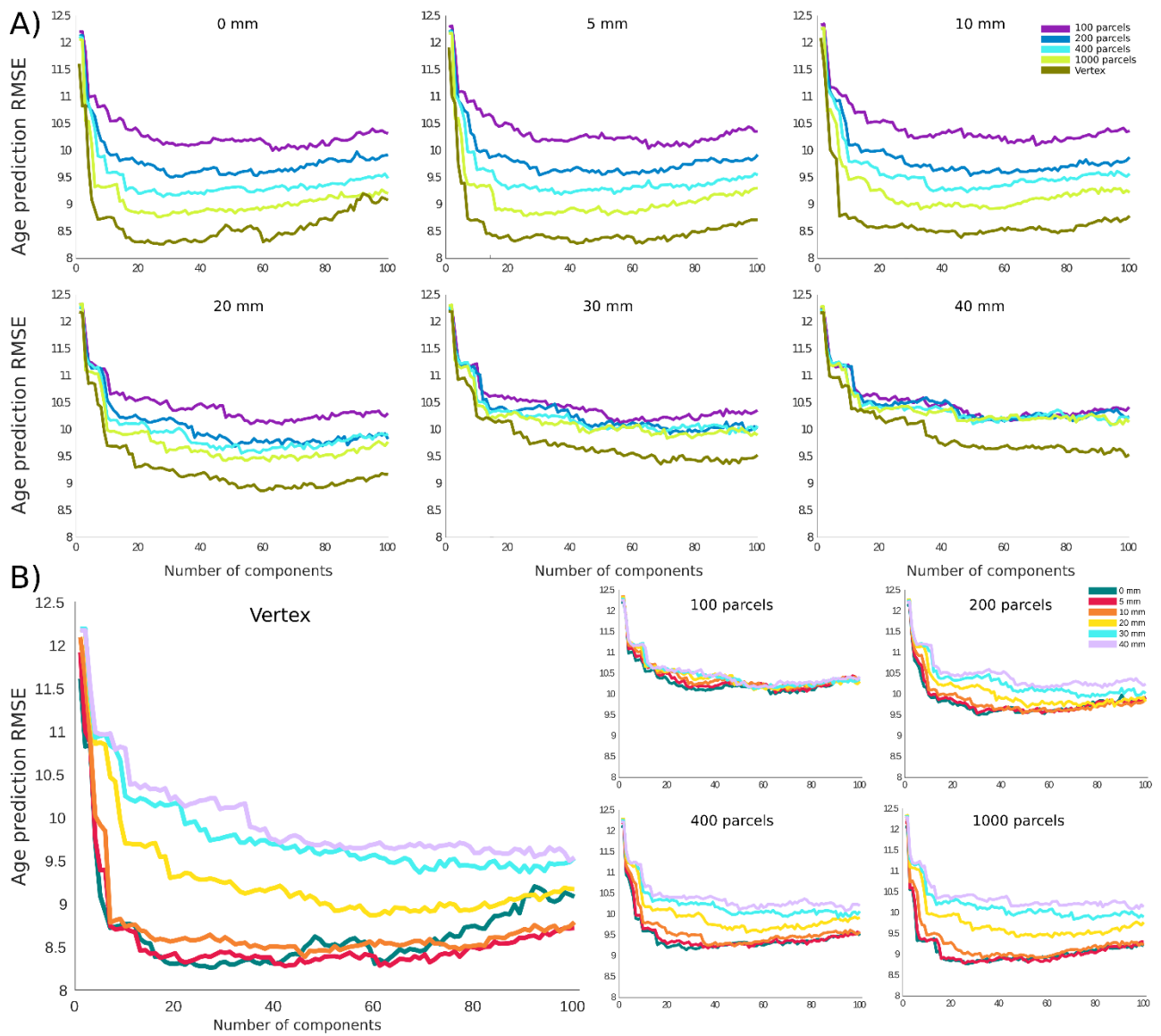
580

581 **Figure 2** | The coefficient of variation (CV) of cortical thickness across population. **A)** CV projected
582 across brain vertices for each parcellations/smoothing pair. **B)** CV shown at 0 mm smoothing level for
583 each cytoarchitectural region across parcellation resolutions.



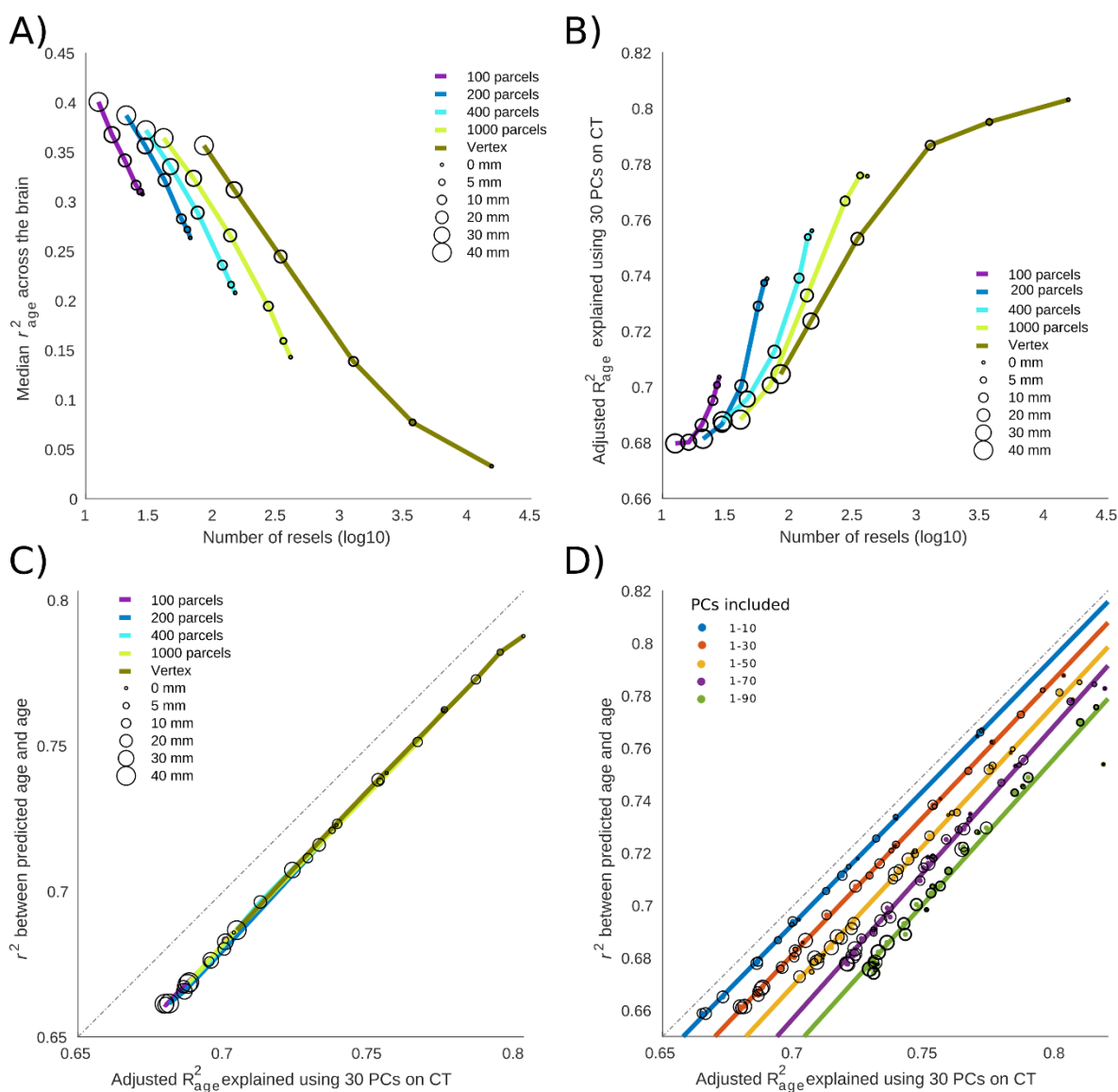
584

585 **Figure 3** | Cortical thickness variance explained by age (r^2). **A)** Cortical thickness variance explained
586 by age (r^2) for each vertex/parcel across smoothing/parcellation conditions. **B)** Histograms for
587 correlation values ρ for each parcellation conditions, grouped by smoothing level.



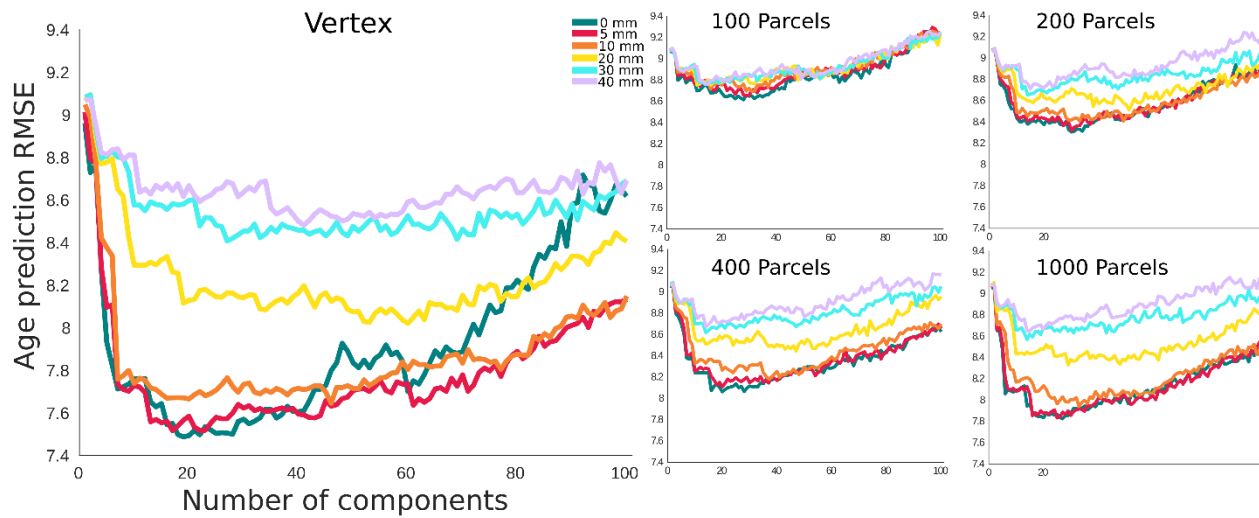
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589 **Figure 4** | Root mean square error (RMSE) for age prediction as a function of number of principal
590 components included as features in the predictive model. **A)** Results grouped together based on the
591 smoothing level. **B)** Results grouped together based on the parcellation resolution.



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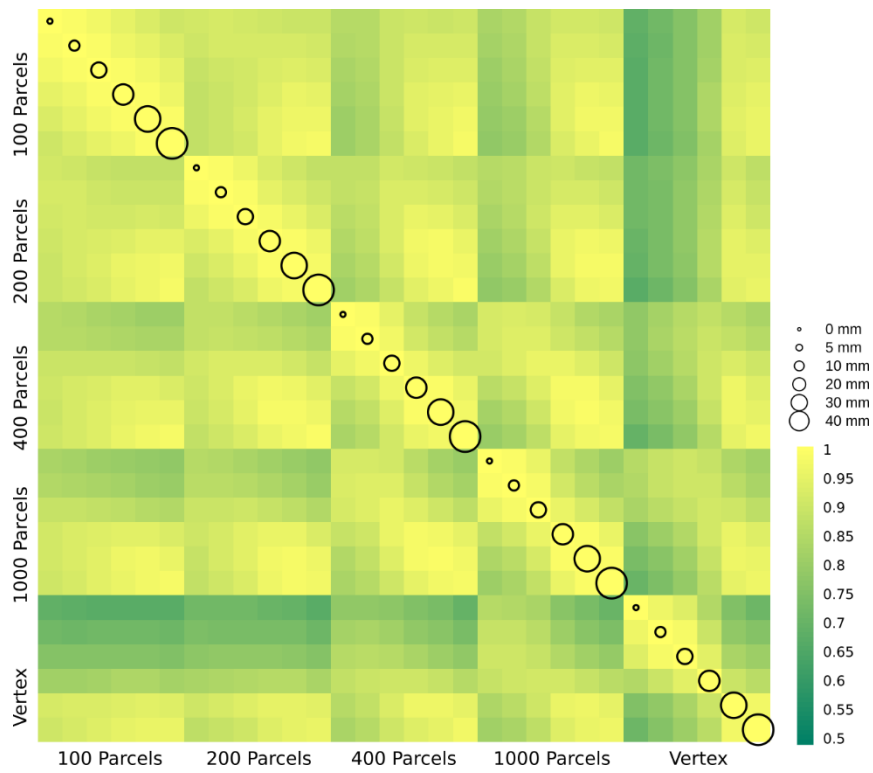
593 **Figure 5** | The relationship between cortical thickness association with age versus brain age prediction.
 594 **A)** Median variance explained of cortical thickness across the brain. The results are grouped based on
 595 the parcellation. Circles represent the something level within each parcellation. **B)** Total variance
 596 explained of age by the first 30 principal components (PCs) of cortical thickness as independent
 597 variables. **C)** The relationship between age prediction accuracy and total variance explained of age. In
 598 the case of prediction, the first PCs are used as predictive features alongside cross validation to prevent
 599 overfitting. The total variance explained of age is the same as depicted in **B**. **D)** The overfitting bias of
 600 linear model compared to the same model used with cross validation. As expected, a higher number of
 601 predictive features results in higher level of overfitting bias.



602

603

604 **Figure 6** | Root mean square error (RMSE) for Age prediction with δ_2 as the error term. The x axis
605 shows the number of principal components included as features. The results are grouped based on the
606 parcellation resolution.



607

608 **Figure 7** | δ_2 age prediction error. The correlation between delta age (as measured by δ_2) across
609 parcellation resolutions (x and y axis labels) and smoothing kernels (represented by circle size).