

1 **Alzheimer's pathology is associated with dedifferentiation of functional memory networks**  
2 **in aging**

3  
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1 **Abstract**

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3 In presymptomatic Alzheimer's disease (AD), beta-amyloid plaques ( $A\beta$ ) and tau tangles  
4 accumulate in distinct spatiotemporal patterns within the brain, tracking closely with episodic  
5 memory decline. Here, we tested whether age-related changes in the segregation of the brain's  
6 functional episodic memory networks - anterior-temporal (AT) and posterior-medial (PM)  
7 networks - are associated with the accumulation of  $A\beta$ , tau and memory decline using fMRI and  
8 PET. We found that AT and PM networks were less segregated in older than younger adults and  
9 this reduced specialization was associated with more tau and  $A\beta$  in the same regions. The effect  
10 of network dedifferentiation on memory depended on the amount of  $A\beta$  and tau, with low  
11 segregation and pathology associated with better performance at baseline and low segregation and  
12 high pathology related to worse performance over time. This pattern suggests a compensation  
13 phase followed by a degenerative phase in the early, preclinical phase of AD.

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## 1 **Introduction**

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3       The accumulation of beta amyloid (A $\beta$ ) plaques and neurofibrillary tau tangles is  
4 associated with episodic memory loss in both normal and pathological aging<sup>1,2</sup>, but the  
5 mechanisms underlying this association are not understood. Molecular and animal studies  
6 suggest that these pathologies spread through structurally and functionally connected brain  
7 regions<sup>3-6</sup>, with human neuroimaging studies indicating that patterns of tau deposition conform to  
8 large-scale brain networks in older adults (OA)<sup>7-9</sup>. Given that AD pathology starts to deposit in  
9 episodic memory networks, we investigated whether age-related changes in functional  
10 connectivity in these networks were associated with the accumulation of A $\beta$  and tau.

11       Functional connectivity (FC) – the co-activation of brain regions within brain networks –  
12 reflects the brain’s large-scale network architecture. Brain networks specialized for different  
13 cognitive functions become dedifferentiated, or less segregated from each other, with older age<sup>10</sup>.  
14 In task-free functional magnetic resonance imaging (fMRI) studies, this progression is typically  
15 characterized by decreased within- and increased between-network FC at rest<sup>11-15</sup>. This decrease  
16 in network segregation leads to reduced specialization of neural networks and has been linked to  
17 OA’s worse performance relative to younger adults (YA) in several behavioral domains<sup>11,13,16,17</sup>.  
18 In contrast, other studies have found that less segregated networks are associated with *better*  
19 performance, suggesting that dedifferentiation may reflect greater plasticity or compensatory  
20 processes that occur during normal aging and neurodegeneration<sup>18-24</sup>. One potential reason for  
21 this discrepancy may be uncertainty about the molecular and pathological processes that drive  
22 network reconfiguration.

1           During the early stages of neurodegeneration, normal cognitive performance is often  
2 maintained despite neuronal loss, changes in network function, or the accumulation of  
3 neurodegenerative pathologies<sup>25-27</sup>. Such compensation is typically only evident in preclinical or  
4 mild cases of neurodegeneration, diminishing once the neurodegenerative pathology becomes  
5 too severe. There is also evidence that greater FC can be associated with either better or worse  
6 memory performance depending on disease severity. For instance, Van Hooren and colleagues  
7 found that greater FC between the default mode network and the dorsal attention network was  
8 associated with better memory in a cognitively normal group, but with worse memory in an MCI  
9 group<sup>28</sup>. One potential interpretation of these results is that although connectivity between  
10 different networks is beneficial early, it may fail to support compensation as pathology increases.  
11 In addition, it could provide a means for that pathology to spread.

12           Events encoded as episodic memories usually combine information about objects/items  
13 and scenes/context. Processing of these two types of information depends on distinct cortical  
14 pathways in the neocortex and medial temporal lobe (MTL) that converge in the hippocampus<sup>29-</sup>  
15 <sup>31</sup>. Object processing involves an anterior-temporal (AT) system that includes fusiform gyrus  
16 (FuG)/perirhinal cortex, inferior temporal gyrus (ITG), and amygdala. In contrast, scene  
17 processing relies on a posterior-medial system (PM) that includes retrosplenial cortex (RSC),  
18 precuneus, and parahippocampal cortex (PHC).

19           In vivo positron emission tomography (PET) studies have demonstrated that A $\beta$  and tau  
20 accumulate in distinct regions within these two subnetworks in the aging brain<sup>32</sup>. Specifically, tau  
21 initially deposits in the transentorhinal region<sup>33,34</sup> and appears to spread throughout the AT system  
22 in both healthy aging and AD, although it eventually affects the PM system as well. In contrast,  
23 A $\beta$  deposition preferentially affects the PM system<sup>32</sup>. Previous work has shown that the AT and

1 PM functional networks have distinct patterns of resting state FC with entorhinal cortex subregions  
2 in YA, and that such patterns predict the spatial topography and level of cortical tau deposition in  
3 cognitively normal OA<sup>35,36</sup>. However, it remains largely unknown whether these networks change  
4 with age and whether the accumulation of A $\beta$  and tau is associated with changes in their modular  
5 organization and, consequently, memory decline.

6         There were two main goals of this study: first, to investigate the effects of age, A $\beta$  and  
7 tau on the intrinsic functional architecture of the AT and PM memory networks and second, to  
8 examine how relationships between pathology and network segregation affect episodic memory  
9 performance. To that end, we use resting state fMRI (rsfMRI) to measure the segregation of the  
10 AT and PM networks in cognitively healthy YA and OA. After examining the effect of age on  
11 network segregation, we then use PET measures of A $\beta$  and tau deposition in OA to explore the  
12 relationship between these pathologies and segregation in the AT and PM networks. Finally, we  
13 assess the relationship between A $\beta$  and tau, segregation, and episodic memory performance at  
14 baseline as well as change in performance over an average of 6 years in OA. We test three  
15 hypotheses: 1) AT and PM networks will be less segregated in OA compared to YA; 2) Given  
16 their distinct spatial topographies, increased tau in OA will be associated with less segregated AT  
17 networks whereas increased A $\beta$  will be associated with less segregated PM networks, and 3)  
18 Network segregation in OA will interact with A $\beta$  and tau pathology to predict episodic memory  
19 performance at baseline as well as change in performance over time.

20

## 21 **Results**

22

### 23 *Study participants*

1 Fifty-five YA (ages 18-35) and 97 cognitively normal OA (ages 60-93) were included in  
2 this study. All YA and OA participants underwent structural and resting state functional MRI. All  
3 OA additionally underwent tau-PET imaging with  $^{18}\text{F}$ -Flortaucipir (FTP),  $\text{A}\beta$ -PET with  $^{11}\text{C}$ -  
4 Pittsburgh compound-B (PiB), and standard neuropsychological assessments. All OA participants  
5 had a baseline MMSE score of  $\geq 26$  and no history of significant medical illnesses or medications  
6 that affect cognition. Demographic information for each age group is presented in Table 1.

7

8 **Table 1.** Cohort demographics

	<b>YA (n = 55)</b>	<b>OA (n = 97)</b>
Age	24.9 $\pm$ 4.4 (18-35)	76.4 $\pm$ 6.1 (60-93)
Sex (M/F)	28/27	36/61
Education (Yrs)	16.3 $\pm$ 2.0	16.8 $\pm$ 1.9
APOE $\epsilon$ 4 (C/NC)	N/A	28/66 (3 N/A)
Global PiB DVR	N/A	1.17 $\pm$ 0.24 (0.92-1.89)
AT FTP SUVR	N/A	1.28 $\pm$ 0.20 (0.98-2.3)
PM FTP SUVR	N/A	1.18 $\pm$ 0.12 (0.94-1.63)
$\text{A}\beta$ +/-	N/A	42/54 (1 N/A)
Tau +/-	N/A	30/66 (1 N/A)

9

10 ***AT and PM networks are less segregated with older age***

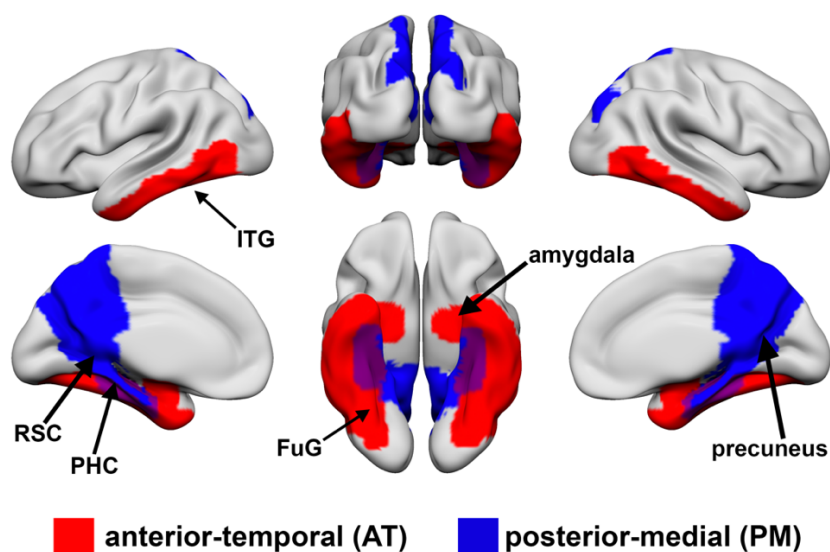
11 Using rsfMRI, we measured functional network segregation in the AT and PM networks  
12 in YA and OA. First-level ROI-to-ROI functional connectivity analysis was performed using the  
13 CONN toolbox<sup>37</sup>. For this analysis, we used 12 unilateral FreeSurfer ROIs that included amygdala,  
14 FuG and ITG as part of the AT network and RSC, PHC, and precuneus as part of the PM network  
15 (Figure 1). Semi-partial correlations were used for these first-level analyses to determine the  
16 unique variance explained by each ROI, controlling for the variance explained by all other ROIs

1 entered into the same model. For each participant, the mean rsfMRI time series for each ROI was  
2 extracted/computed. Then, the cross-correlation of each ROI's time course with every other ROI's  
3 time course was computed, creating a 12 x 12 correlation matrix for each subject. Correlation  
4 coefficients were converted to z-values using Fisher's r-to-z transformation<sup>38</sup>. The diagonal of the  
5 matrix was removed and negative correlations were set to zero<sup>39</sup>. Network segregation values were  
6 calculated as the difference in mean within-network FC and mean between-network FC divided  
7 by mean within-network FC:

$$8 \quad \text{Network segregation} = \frac{\bar{Z}_w - \bar{Z}_b}{\bar{Z}_w}$$

9 where  $\bar{Z}_w$  is the mean Fisher z-transformed correlation between ROIs within the same network  
10 and  $\bar{Z}_b$  is the mean Fisher z-transformed correlation between ROIs of one network with all ROIs  
11 in the other network<sup>13</sup>. Thus, larger positive values for network segregation indicate that regions  
12 within a network (e.g. AT) have higher connectivity with each other compared to their connectivity  
13 with regions outside of the network (e.g. PM).

14

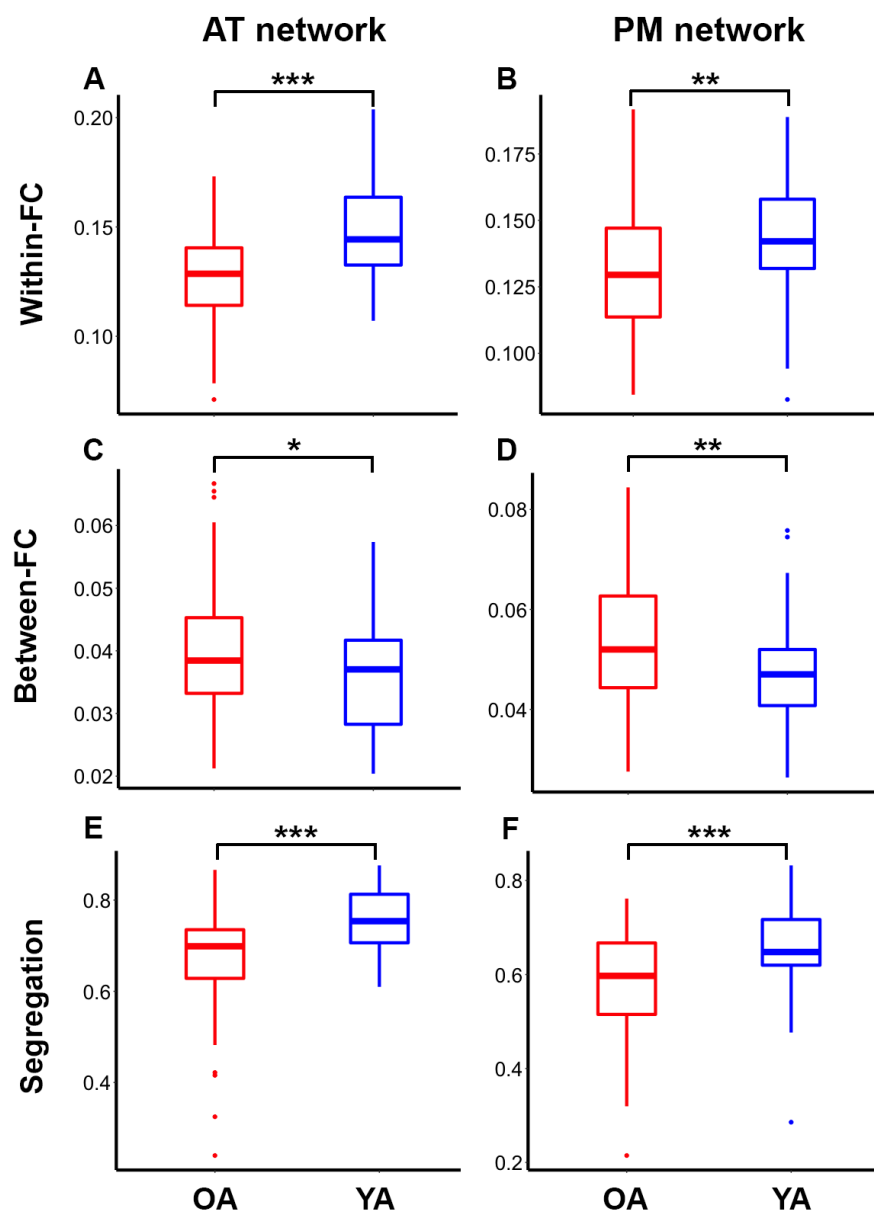


1 **Figure 1. A priori defined regions of interest in anterior-temporal (AT; red) and posterior-**  
2 **medial (PM; blue) networks.** AT regions include bilateral amygdala, fusiform gyrus  
3 (FuG)/perirhinal cortex, and inferior temporal gyrus (ITG). PM regions include bilateral  
4 retrosplenial cortex (RSC), parahippocampal cortex (PHC) and precuneus.

5  
6 As hypothesized, OA exhibited decreased within-network (AT: Fig 2A,  $t = 6.7$ ,  $p < 0.001$ ;  
7 PM: Fig 2B,  $t = 3.1$ ,  $p = 0.002$ ) and increased between-network (AT: Fig 2C,  $t = 2.5$ ,  $p = 0.01$ ;  
8 PM: Fig 2D,  $t = 3$ ,  $p = 0.003$ ) functional connectivity and decreased segregation (AT: Fig 2E,  $t =$   
9  $4.9$ ,  $p < 0.001$ ; PM: Fig 2F,  $t = 4.3$ ,  $p < 0.001$ ) in the AT and PM networks compared to YA. Of  
10 particular importance, the relationship between age group and segregation was assessed across  
11 multiple analysis approaches related to matrix thresholding (i.e., inclusion of positive only vs.  
12 negative correlations), bivariate vs. semi-partial correlations, various network metrics of  
13 intersystem relationships (i.e., segregation, participation coefficient, and modularity), and network  
14 labeling (i.e., the regions included to define AT and PM networks). The age group differences in  
15 segregation were found to be robust in all instances (See Supplemental Figure S1).

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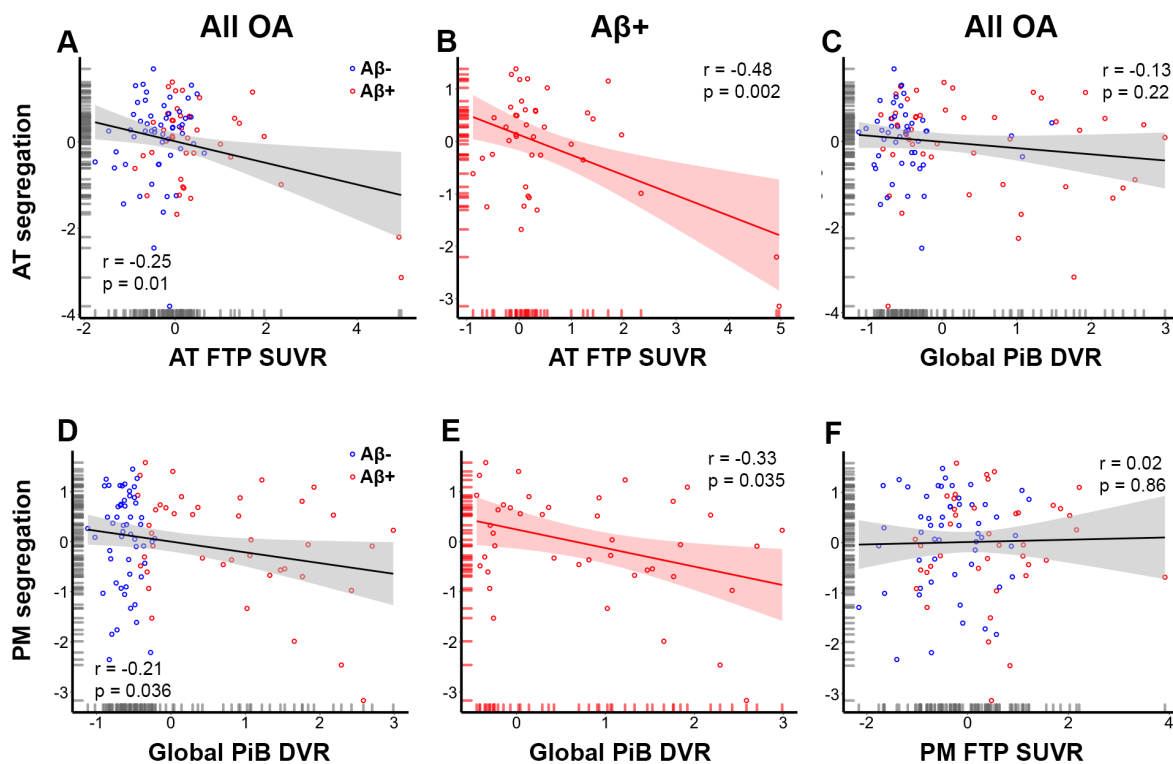
1  
2 **Figure 2. Anterior-temporal (AT; left) and posterior-medial (PM; right) networks are less**  
3 **segregated in older (red) relative to younger (blue) adults. OA show decreased within-network**  
4 **(A and B) and increased between-network (C and D) functional connectivity (FC), and decreased**  
5 **network segregation (E and F) compared to YA. \* $p < 0.05$ , \*\* $p < 0.01$ , and \*\*\* $p < 0.001$ .**  
6  
7 *Tau relates to AT segregation and A $\beta$  relates to PM segregation*

1           Next, we examined the relationship between tau and A $\beta$  pathology and network  
2 segregation in OA. Tau was quantified using the FTP tracer and data acquired at 80-100 minutes  
3 post-injection. The standardized uptake value ratio (SUVR) was calculated, and the weighted mean  
4 SUVRs for FreeSurfer-defined AT and PM ROIs (the same ROIs used for calculating segregation  
5 above) were calculated after partial volume correction (PVC)<sup>40</sup>. A $\beta$  was quantified using the PiB  
6 tracer, and distribution volume ratio (DVR) was calculated. A global measure of PiB DVR was  
7 calculated across cortical FreeSurfer ROIs as described previously<sup>41</sup>, and a threshold of 1.065 was  
8 used to classify participants into A $\beta$ - and A $\beta$ + groups<sup>42</sup>. *APOE* was not related to segregation ( $p$   
9  $> 0.63$ ); therefore, we did not control for *APOE* in these analyses.

10           To assess the relationship between tau and segregation, we first examined the relationship  
11 across all OA. We then split the group into A $\beta$ - and A $\beta$ + subgroups to determine whether this  
12 relationship differed between OA with and without A $\beta$  pathology. Increased FTP SUVR in AT  
13 regions was associated with decreased segregation in the AT network across all OA (Fig 3A,  $r = -$   
14  $0.25$ ,  $p = 0.014$ ). Splitting the group into A $\beta$ - and A $\beta$ + subgroups, we observed the same  
15 relationship in the A $\beta$ + group (Fig 3B,  $r = -0.48$ ,  $p = 0.002$ ), but no significant relationship was  
16 observed in the A $\beta$ - group ( $r = 0.10$ ,  $p = 0.45$ ). We did not find a significant relationship between  
17 global PiB DVR and AT network segregation across all OA (Fig 3C,  $r = -0.13$ ,  $p = 0.23$ ). Because  
18 the relationship between AT-tau and AT segregation appeared to be influenced by a few high-tau  
19 individuals, we performed a follow-up robust regression which is less affected by more extreme  
20 data points<sup>43</sup>. This analysis was performed using the ‘fitlm’ function with the ‘RobustOpts’ name-  
21 value pair in Matlab to create a model that limits the influence of outliers and heteroscedasticity.  
22 The relationship between tau and AT segregation was no longer significant across the whole group  
23 ( $t = 0.95$ ,  $p = 0.34$ ), but remained significant in the A $\beta$ + group ( $t = 3.1$ ,  $p = 0.004$ ).

1 We next examined the relationship between global PiB and network segregation. Increased  
2 global PiB DVR was associated with decreased segregation in the PM network (Fig 3D,  $r = -0.21$ ,  
3  $p = 0.036$ ). Splitting the group into A $\beta$ - and A $\beta$ + subgroups, we observed the same relationship in  
4 the A $\beta$ + group (Fig 3E,  $r = -0.33$ ,  $p = 0.035$ ) but no significant relationship in the A $\beta$ - group ( $r =$   
5  $0.014$ ,  $p = 0.92$ ). We did not observe a significant relationship between FTP SUVR in PM regions  
6 and PM network segregation (Fig 3F,  $r = 0.02$ ,  $p = 0.86$ ).

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8

9 **Figure 3. Tau and beta amyloid (A $\beta$ ) deposition are related to the segregation of anterior-**  
10 **temporal (AT; first row) and posterior-medial (PM; second row) networks, respectively.** Less  
11 segregated AT networks are associated with increased tau in AT regions (A), particularly in A $\beta$  +  
12 OA (B), but are not associated with global A $\beta$  (C). Less segregated PM networks are associated  
13 with increased global A $\beta$  (D), particularly in A $\beta$  + OA (E), but are not associated with tau in PM

1 regions (**F**). All regressions account for age and sex differences; The x and y axes reflect the  
2 residuals from the model.

3

#### 4 ***AD pathology moderates the association between segregation and episodic memory***

5 Cognitive performance was measured as a z-score of standardized neuropsychological tests  
6 in three different domains: episodic memory, executive function, and working memory. We then  
7 examined the relationship between network segregation and cognitive performance at baseline.  
8 Because our episodic memory composite measure included both object- and spatial-related  
9 memory domains, we computed a single segregation measure by averaging the AT and PM  
10 segregation values (follow-up analyses showed essentially the same results for AT and PM  
11 networks; See Supplemental Figure S2).

12 We performed a multiple regression to assess the effects of segregation and A $\beta$ -status on  
13 episodic memory performance in OA, controlling for age, sex, and education. We observed main  
14 effects of segregation ( $t = 2.9, p = 0.005$ ), A $\beta$ -status ( $t = 2.5, p = 0.013$ ), and age ( $t = 2.7, p =$   
15  $0.008$ ) on episodic memory. This analysis also revealed a significant interaction between A $\beta$ -status  
16 and segregation on episodic memory performance ( $t = 2.5, p = 0.014$ ). Specifically, less segregated  
17 networks were associated with better performance in A $\beta$ - OA (Fig 4A,  $r = -0.40, p = 0.004$ )  
18 whereas segregation was not associated with performance in A $\beta$ + OA (Fig 4B,  $r = 0.14, p = 0.40$ ).  
19 Table 2 reports the results of this regression.

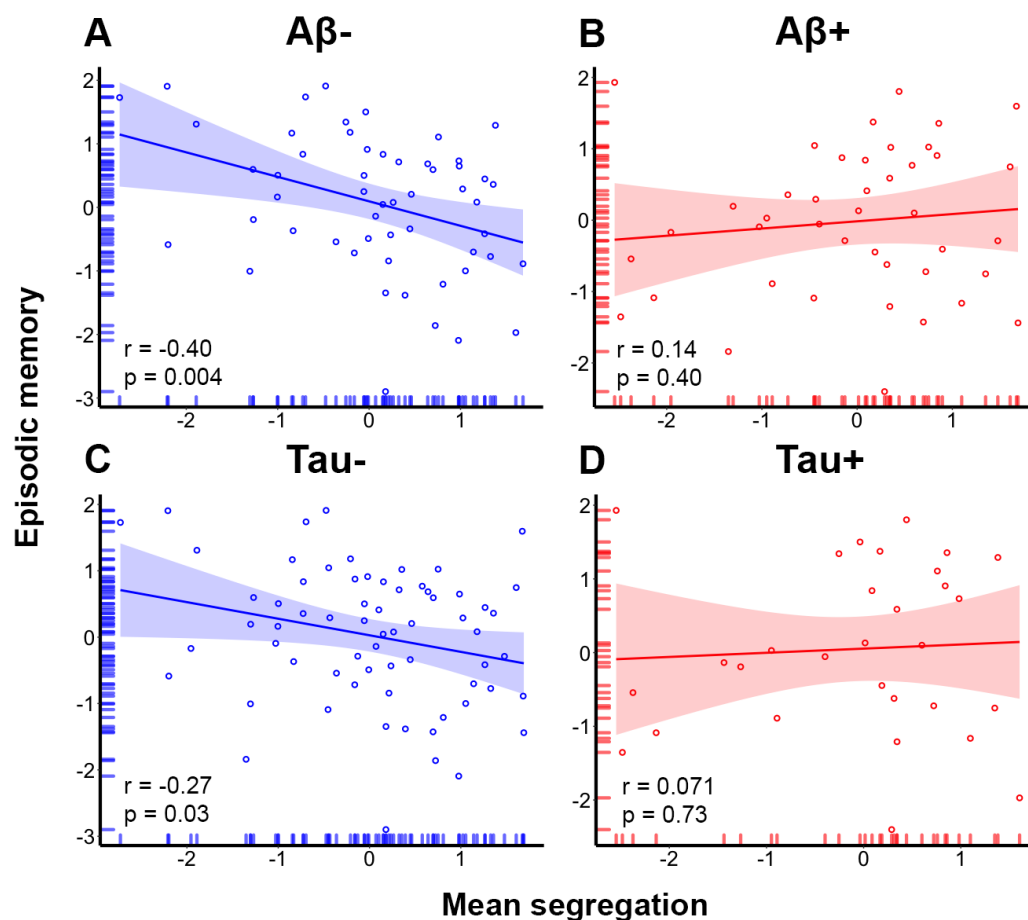
20 To additionally explore the effects of segregation and tau-status on episodic memory  
21 performance, we calculated “tau positivity” as the mean SUVR in a Braak<sub>III-IV</sub> composite ROI (cut-  
22 off of 1.26) that included regions from both AT (amygdala, FuG, and ITG) and PM (PHC and  
23 RSC) systems<sup>32,44</sup> as well as other regions that accumulate tau in the progression from aging to AD.

1 We again found main effects of segregation ( $t = 2.1$ ,  $p = 0.043$ ) and age ( $t = 2.5$ ,  $p = 0.014$ ), but not  
2 tau-status ( $t = 1.4$ ,  $p = 0.16$ ) on episodic memory. Although there was not a significant interaction  
3 between tau-status and mean segregation on performance, ( $t = 1.5$ ,  $p = 0.14$ ) we did find that less  
4 segregated networks were associated with better performance in tau- OA (Fig 4C,  $r = -0.27$ ,  $p =$   
5  $0.03$ ) whereas segregation was not associated with performance in tau+ OA (Fig 4D,  $r = 0.071$ ,  $p =$   
6  $0.73$ ). Table 3 reports the results of this follow-up regression.

7 As control analyses, we also examined the relationships between segregation, A $\beta$ -status,  
8 and baseline working memory and executive function. We again observed a significant interaction  
9 between A $\beta$ -status and mean segregation on executive function ( $t = 2.21$ ,  $p = 0.03$ ) such that less  
10 segregated networks were associated with better executive function in the A $\beta$ - OA ( $r = -0.35$ ,  $p =$   
11  $0.011$ ) whereas there was no significant association in the A $\beta$ + OA ( $r = 0.08$ ,  $p = 0.63$ ). There  
12 were no significant relationships between segregation and working memory performance, nor was  
13 there an interaction between A $\beta$ -status and segregation on performance ( $ps > .41$ ).

14 Including tau-status in place of A $\beta$ -status, we did not observe a significant interaction  
15 between tau-status and mean segregation on executive function,  $t = 1.5$ ,  $p = 0.13$ . However, we  
16 did find that less segregated networks were associated with better executive function in the tau-  
17 OA ( $r = -0.28$ ,  $p = 0.03$ ) whereas there was no significant association in the tau+ OA ( $r = 0.08$ ,  $p =$   
18  $0.71$ ). There were no significant relationships between segregation and working memory  
19 performance in either group, nor was there an interaction between tau-status and segregation on  
20 performance ( $ps > .67$ ).

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1  
 2 **Figure 4. Alzheimer’s disease pathology moderates the association between mean network**  
 3 **segregation and episodic memory performance. (A)** Less segregated networks are associated  
 4 with better performance in  $A\beta^-$  OA whereas **(B)** segregation is not associated with performance in  
 5  $A\beta^+$  OA. **(C)** Similarly, less segregated networks are associated with better performance in  $\text{Tau}^-$   
 6 OA whereas **(D)** segregation is not associated with performance in  $\text{Tau}^+$  OA.

7  
 8 **Table 2.** Multiple regression results for mean segregation and its interaction with  $A\beta$ -status  
 9 predicting episodic memory at baseline.

Predictor	t	p
Age	-2.7	0.008

A $\beta$ -status	-2.5	0.013
Sex	0.86	0.39
Education	1.3	0.2
Segregation	-2.9	0.005
A $\beta$ -status x Seg	2.5	0.014

1  
2 **Table 3.** Multiple regression results for mean segregation and its interaction with Tau-status  
3 predicting episodic memory at baseline.

<b>Predictor</b>	<b>t</b>	<b>p</b>
Age	-2.5	0.014
Tau-status	-1.4	0.16
Sex	0.75	0.45
Education	1.2	0.22
Segregation	-2.9	0.043
Tau-status x Seg	2.5	0.14

4  
5 ***Baseline segregation predicts longitudinal memory decline***  
6 To examine the effect of segregation and A $\beta$  and tau on change in memory performance  
7 over time, our longitudinal analyses included participants that had at least two neuropsychological  
8 testing sessions (one of which was near the time of the resting state scan). Importantly, all  
9 participants had resting state fMRI, PET, and neuropsychological data at the same time point (i.e.,  
10 “baseline”), which is the time point we used to assess all cross-sectional relationships. Eighty-six  
11 of 97 OA participants had longitudinal cognitive data ( $\geq 2$  testing sessions). These participants had  
12 between 2 and 13 testing sessions (mean,  $6.1 \pm 3.1$ ) over a period of 1 to 13 years (mean,  $6.1 \pm$   
13  $3.5$ ) with an average interval of  $1.3 \pm 0.6$  years between sessions. Sixteen participants had only

1 retrospective data. Figure 5A displays each participant's trajectory in longitudinal episodic  
2 memory performance over time.

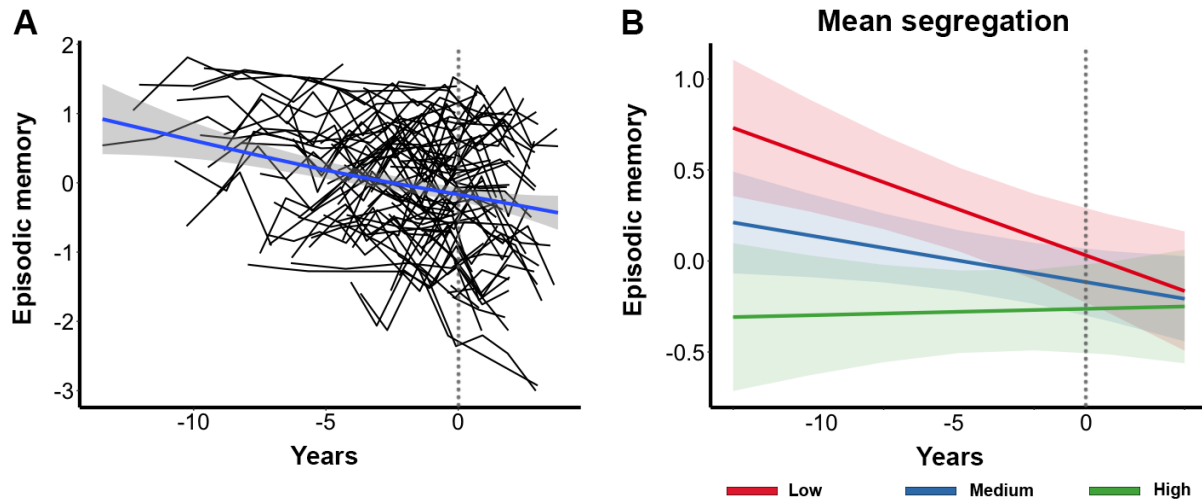
3         Longitudinal cognitive measures were modelled using linear mixed-effects regression with  
4 a random intercept and slope using the lme4 package in R v3.6.3 ([www.r-project.org](http://www.r-project.org)). In order to  
5 examine the relationship between baseline segregation, baseline  $A\beta$  and tau, and change in  
6 cognitive performance in one model, the model included two-way interactions between baseline  
7 segregation and time, global  $A\beta$  and time, and tau and time. We report the results using continuous  
8 measures of global  $A\beta$  and Braak<sub>III-IV</sub> tau as they retain more statistical power in the model. The  
9 results were very similar whether we used Braak<sub>III-IV</sub> tau, AT-tau (Table S1) or PM tau (Table S2)  
10 and whether we used dichotomous (Table S3) or continuous  $A\beta$  and tau in the model. All models  
11 were adjusted for age, sex, and education. Segregation was a continuous variable in the model but  
12 is displayed graphically using tertiles.

13         We found that individuals with lower segregation at baseline showed a steeper decline rate  
14 in episodic memory over time ( $\beta = 0.08$ ,  $SE = 0.03$ ,  $p = 0.02$ ; Figure 5B; Table 3). We also found  
15 that more tau at baseline was associated with a steeper decline rate in memory over time ( $\beta = -$   
16  $0.15$ ,  $SE = 0.04$ ,  $p = 0.002$ ). There was no interaction of  $A\beta$  and time predicting memory change  
17 ( $\beta = -0.003$ ,  $SE = 0.04$ ,  $p = 0.94$ ). To examine whether  $A\beta$  or tau moderated the effect of  
18 segregation on cognitive change, follow-up analyses included the same factors in addition to three-  
19 way interactions between baseline segregation, baseline  $A\beta$  and tau, and time. These analyses did  
20 not show a significant three-way interaction between segregation, tau and time ( $\beta = 0.03$ ,  $SE =$   
21  $0.05$ ,  $p = 0.58$ ) nor between segregation,  $A\beta$ , and time ( $\beta = -0.04$ ,  $SE = 0.04$ ,  $p = 0.34$ ) on memory  
22 change. As a control analysis, we also examined change in working memory and executive  
23 function performance over time using the same model (not including three-way interactions).



1 Baseline segregation was neither associated with longitudinal change in working memory ( $\beta = -$   
2 0.02, SE = 0.04,  $p = 0.57$ ) nor executive function ( $\beta = 0.02$ , SE = 0.03,  $p = 0.66$ ).

3



4

5 **Figure 5. Relationship between network segregation and longitudinal episodic memory**

6 **change.** (A) Individual participant trajectories in longitudinal episodic memory change over time.

7 Each black line represents one participant. The blue trendline reflects the participant average

8 change in memory over time. The dotted gray line (at X = 0) represents the “baseline” time point

9 in each plot. (B) Plot of estimated curves for three groups with different baseline network

10 segregation (low, medium, and high) and episodic memory outcomes over time. Note that

11 segregation was modeled as a continuous variable but is shown as a categorical variable for

12 illustration purposes only. Lower baseline segregation was associated with a steeper decline rate

13 in episodic memory over time.

14

15 **Table 3.** Linear mixed model results for segregation and pathology predicting longitudinal

16 episodic memory change.

<b>Predictor</b>	<b>Estimate</b>	<b>p</b>
Age	-0.19	0.03
Sex	-0.01	0.93
Education	0.13	0.13
Segregation	-0.20	0.02
Time	-0.07	0.06
Tau	-0.13	0.17
A $\beta$	0.03	0.8
Tau x Time	-0.15	0.002
A $\beta$ x Time	-0.003	0.94
Segregation x Time	0.08	0.02

1  
2 **Discussion**  
3  
4       The goal of this study was to investigate the effects of A $\beta$  and tau on the intrinsic functional  
5 architecture of episodic memory networks and episodic memory ability in cognitively normal OA.  
6 OA showed reduced segregation of AT and PM networks compared to YA. This effect was driven  
7 by reduced within-network FC and increased between-network FC between the two systems.  
8 Increased tau in AT regions was associated with a less segregated AT network, whereas increased  
9 global A $\beta$  was associated with a less segregated PM network, demonstrating a regional  
10 dissociation of these AD pathologies to the large-scale organization of the AT and PM systems.  
11 Finally, less segregated networks were associated with better memory ability at baseline in OA  
12 with low levels of AD pathology but with a steeper decline in memory performance over time,  
13 independent of baseline pathology. These findings suggest there may be different phases in the  
14 association of brain network integrity and memory ability that depend on the degree of AD  
15 pathology.

1           We interpreted our findings based on a model that includes both age- and AD pathology-  
2 related effects. We found that age was associated with changes in the functional segregation of the  
3 AT and PM resting state networks. This finding is consistent with studies of age-related neural  
4 dedifferentiation demonstrating that older age is associated with less distinct neural activation  
5 patterns<sup>10,11,45-48</sup> and, more recently, with less distinct large-scale resting state networks<sup>11-15,49,50</sup>.  
6 While a majority of these prior studies explored the organization of the brain's canonical resting  
7 state networks (e.g., the default mode, fronto-parietal and cingulo-opercular networks), we  
8 demonstrated a robust age effect in two neural networks that are associated with episodic memory  
9 and AD pathology. Recent work from our laboratory also showed that less differentiated activation  
10 in AT and PM regions during an object/scene discrimination task was associated with more tau  
11 deposition<sup>32</sup>. These findings, in conjunction with the present results, suggest a neuropathological  
12 correlate of dedifferentiation in the episodic memory system.

13           We found that the modular organization of the AT and PM brain networks was selectively  
14 vulnerable to tau and A $\beta$  deposition. Specifically, increased tau in AT regions was associated with  
15 less segregated AT networks, but was not associated with PM network segregation. In contrast,  
16 increased cortical A $\beta$  was associated with less segregated PM networks, but was not associated  
17 with AT network segregation. Since between-network FC was the same in the AT and PM  
18 networks, these results indicate that this relationship was driven by within-network FC. This is  
19 consistent with previous investigations that have demonstrated relationships between within-  
20 network FC and AD pathology<sup>8,35,51</sup>. The findings of a double dissociation between AD pathology  
21 and network segregation are in accordance with previous work from our lab demonstrating  
22 differential selective vulnerability to these two networks participating in episodic memory  
23 function. Specifically, Maass et al. (2019) showed that tau deposits mainly in AT regions, resulting

1 in object discrimination deficits, whereas A $\beta$  deposits preferentially in PM regions, resulting in  
2 impaired scene discrimination<sup>32</sup>.

3         There is no agreement on a precise region where A $\beta$  deposition begins, and existing data  
4 suggest that this pathology appears multifocally and quickly accumulates throughout most of  
5 association cortex<sup>52-55</sup>. For example, while we used a global measure of cortical A $\beta$  to define  
6 positivity, A $\beta$  in the PM network is highly correlated with this measure as are most regions  
7 throughout the brain<sup>56</sup>. In contrast, tau initially deposits in the entorhinal cortex and then progresses  
8 in a distinct spatiotemporal pattern first to anterior temporal and limbic regions and then  
9 throughout association cortex<sup>52,57,58</sup>. Cellular and molecular data reveal that tau can spread trans-  
10 synaptically and in relation to neural activity<sup>5,6,59,60</sup>, suggesting that this specific AD pathology  
11 accumulates through the brain along neural connections. The idea that large-scale brain network  
12 connectivity may underlie the spatiotemporal patterns of AD pathology has support from other  
13 laboratories. For instance, Franzmeier et al. found that canonical network regions with higher FC  
14 showed higher covariance of tau deposition<sup>7</sup>. In addition, Jacobs et al. found that A $\beta$  facilitated the  
15 spread of tau from the hippocampus to the posterior cingulate via structural connectivity<sup>61</sup>, and  
16 Adams et al. reported that FC of the entorhinal cortex was related to A $\beta$ -facilitated neocortical tau  
17 deposition<sup>31</sup>. Previous data suggesting preferential involvement of the AT network by tau<sup>32</sup>, along  
18 with these results showing dedifferentiation, raise the possibility that tau may spread from the AT  
19 to the PM network as these networks become less segregated.

20         Our results revealed complex interactions between segregation, A $\beta$  and tau pathology, and  
21 memory performance. Our cross-sectional data showed that AD pathology moderated the  
22 relationship between segregation and baseline performance. Specifically, less segregated networks  
23 were associated with better performance in OA with low levels of pathology but not in those with

1 high levels of pathology. Additionally, our longitudinal results revealed that less segregated  
2 networks and more tau at baseline independently predicted a steeper decline in memory  
3 performance over time. These findings are consistent with previous studies demonstrating that  
4 neurodegenerative pathology interacts with FC to influence performance<sup>28,62</sup>. For instance, Lin et  
5 al. (2020) showed an interactive effect of A $\beta$  deposition and FC on cognition such that increased  
6 FC between left middle frontal gyrus and a memory encoding network was associated with better  
7 attention/processing speed and executive function in those with low levels of A $\beta$  but with worse  
8 function in those with high levels of A $\beta$ <sup>62</sup>.

9 Overall, our findings may suggest different phases in the long-term interaction of network  
10 segregation and AD pathology on episodic memory ability. OA with low pathology may  
11 compensate, either for normal aging processes or for the start of AD pathology, by increasing  
12 communication between AT and PM networks. As functionality in one system declines, recruiting  
13 the other system may help performance. Over time, however, this increased between-network FC  
14 in the context of increasing pathology could become detrimental, as well as providing a route for  
15 AD disease pathology to spread from one network to the other, leading to more decline in memory  
16 ability. Based on this model, it is likely that AT and PM networks continue to de-differentiate over  
17 time, especially in the transition phase from cognitively normal to cognitively impaired. This  
18 would further the spread of AD pathology, eventually resulting in the hallmark episodic memory  
19 impairments observed in MCI and AD. Future studies that include patient data as well as  
20 longitudinal measures of FC, AD pathology, and memory function are crucial in testing this  
21 hypothesis.

22 The cross-sectional PET and MRI data limit our interpretations of causality as well as long-  
23 term changes in this study. Although it is possible that A $\beta$  and tau spread lead to disruptions in

1 large-scale network FC (rather than the reverse), several studies suggest that A $\beta$  and tau  
2 propagation is a multifactorial process that depends on both neural connectivity and regional  
3 vulnerability<sup>6,8,60</sup>. Hence, the relationship between A $\beta$  and tau and FC is likely bidirectional such  
4 that age-related disruptions in network FC guide pathology spread and this, in turn, leads to further  
5 changes in the network architecture. Longitudinal designs are critical in determining the order of  
6 age-related changes as well as elucidating the sequence of neural events leading to episodic  
7 memory decline. Another limitation of this study was that the longitudinal cognitive data included  
8 different numbers of timepoints before and after the “baseline” timepoint for different participants.  
9 This design feature complicates our interpretation of the longitudinal effects of segregation and  
10 A $\beta$  and tau on performance because our analyses were both retrospective and prospective.  
11 However, this design feature allowed us to examine memory change over a longer period of time  
12 (average of ~6 years) compared to many previous studies<sup>63–65</sup>. Furthermore, we were able to include  
13 more participants from our sample with longitudinal data using this design. Longitudinal studies  
14 are often unable to observe any significant change in cognition in OA given the relatively short  
15 time periods of observation<sup>66,67</sup>. We believe that having a greater number of timepoints for more  
16 participants outweighs the disadvantage of this design feature.

17 Taken together, our data support a model whereby network dedifferentiation performs a  
18 neural compensatory function which fails over time as AD pathology accumulates. The effect of  
19 network dedifferentiation on episodic memory ability is helpful to performance when pathology  
20 levels are low but is harmful to performance over time as pathology presumably spreads. This  
21 research provides an important step in elucidating the neural mechanisms associated with episodic  
22 memory decline in healthy and pathological aging. By studying this episodic memory system in  
23 healthy OA, we can advance our understanding of healthy aging and its similarities to and

1 differences from pathological aging, which could serve as a crucial building block for the early  
2 detection of AD.

3

#### 4 **Methods**

5

##### 6 *Participants*

7 Fifty-five YA (age 18-35) and 97 cognitively normal OA (age 60+) enrolled in the  
8 Berkeley Aging Cohort Study (BACS) were included in this study. All YA and OA participants  
9 underwent structural and resting state functional MRI. All OA additionally underwent tau-PET  
10 imaging with <sup>18</sup>F-Flortaucipir (FTP), A $\beta$ -PET with C-Pittsburgh <sup>11</sup>Compound-B (PiB), and a  
11 standard neuropsychological assessment. Eligibility requirements included that all participants had  
12 a baseline MMSE score of  $\geq 26$ . We also excluded any participants with a history of significant  
13 neurological disease (e.g., stroke, seizure, loss of consciousness  $\geq 10$  minutes), or any medical  
14 illness that could affect cognition, history of substance abuse, depression, or contraindications to  
15 MRI or PET. All study procedures were reviewed and approved by the Institutional Review Boards  
16 of the University of California Berkeley and Lawrence Berkeley National Laboratory (LBNL). All  
17 participants provided written informed consent for their involvement in this study.

18

##### 19 *Neuropsychological assessment*

20 All OA participants in the BACS undergo neuropsychological testing to measure cognitive  
21 performance related to verbal and visual memory, working memory, processing speed, executive  
22 function, language, and attention. In this study, composite scores were calculated to measure three  
23 specific cognitive domains: episodic memory, working memory, and executive functioning. The

1 tests for episodic memory included the California Verbal Learning Test (CVLT) immediate and  
2 long delay free recall totals as well as the Visual Reproduction (VR) immediate and delay recall  
3 totals. Working memory was assessed with the Digit Span total score. Tests for executive function  
4 included Trail Making test B minus A, Stroop number correct in 1 min, and Digit Symbol total.  
5 For episodic memory and executive function, the composite scores were produced by calculating  
6 the average z-score of the tests included in each domain. Please refer to Harrison et al. (2019) for  
7 more details of the procedure<sup>44</sup>.

8 To examine change in memory performance over time, our longitudinal analyses included  
9 participants (from the 97 OA sample) that had (1) at least one resting state fMRI scan, (2) at least  
10 one A $\beta$  and one tau PET scan (both near the time of the resting state scan), and (3) at least two  
11 neuropsychological testing sessions (one of which was near the time of the resting state scan).  
12 Critically, all participants had resting state fMRI, PET, and neuropsychological data at the same  
13 time point, which is the time point we used to assess all cross-sectional relationships (i.e.,  
14 “baseline” time point). The additional neuropsychological session(s) could be either before or after  
15 the baseline time point (or both), depending on the participant. Eighty-six of 97 OA participants  
16 had longitudinal cognitive data ( $\geq 2$  testing sessions). These participants had between 2 and 13  
17 testing sessions (mean,  $6.1 \pm 3.1$ ) over a period of 1 to 13 years (mean,  $6.1 \pm 3.5$ ) with an average  
18 delay of  $1.3 \pm 0.6$  years between sessions.

19

## 20 ***MRI data acquisition***

21 All YA and OA participants underwent structural and functional MRI acquired on a 3T  
22 TIM/Trio scanner (Siemens Medical System, software version B17A) using a 32-channel head  
23 coil. First, a whole-brain high resolution T1-weighted volumetric magnetization prepared rapid



1 gradient echo image (MPRAGE) structural MRI scan was acquired with the following parameters:  
2 voxel size = 1 mm isotropic, TR = 2300 ms, TE = 2.98 ms, matrix = 256 x 240 x 160, FOV = 256  
3 x 240 x 160 mm<sup>3</sup>, sagittal plane, 160 slices, 5 minute acquisition time. This was followed by a  
4 rsfMRI scan that was acquired using T2\*-weighted echo planar imaging (EPI) with the following  
5 parameters: voxel size = 2.6 mm isotropic, TR = 1067 ms, TE = 31.2 ms, FA = 45, matrix = 80 x  
6 80, FOV = 210 mm, sagittal plane, 300 volumes, anterior to posterior phase encoding, ascending  
7 acquisition, 5 minute acquisition time. A multiband acceleration factor of 4 was used to acquire  
8 whole-brain coverage at high spatial resolution by acquiring 4 slices at the same time<sup>68,69</sup>. During  
9 the rsfMRI scan, participants were instructed to remain awake with their eyes open and focused  
10 on the screen, which displayed a white asterisk on a black background.

11 As part of the standard PET processing pipeline, a whole-brain high resolution T1-  
12 weighted volumetric MPRAGE scan was acquired for each participant on a Siemens Magnetom  
13 Avanto scanner at LBNL with the following parameters: voxel size = 1 mm isotropic, TR = 2110  
14 ms, TE = 3.58 ms, flip angle = 15°, sagittal slice orientation. These data were used for PET  
15 coregistration and to parcellate the brain for PET data analysis.

### 17 ***PET data acquisition***

18 All OA participants underwent PET scanning at LBNL using a Biograph PET/CT  
19 Truepoint 6 scanner (Siemens, Inc.) with CT scans performed for attenuation correction prior to  
20 each emission acquisition and radiotracers synthesized at the LBNL Biomedical Isotope Facility.  
21 Tau deposition was measured using <sup>18</sup>F-Flortacipir (FTP) with data binned into 4 x 5 minute frames  
22 from 80-100 minute post-injection<sup>35,44,70</sup>. A $\beta$  was measured using <sup>11</sup>C-Pittsburgh Compound B  
23 (PiB), with data acquired across 35 dynamic frames for 90 minutes post-injection (4 x 15, 8 x 30,

1 9 x 60, 2 x 180, 10 x 300, and 2 x 600 seconds). All PET images were reconstructed using an  
2 ordered subset expectation maximization algorithm, with attenuation correction, scatter correction,  
3 and smoothing using a Gaussian kernel of 4 mm.

4

### 5 ***MRI processing***

6 Structural scans (3T) were processed with FreeSurfer to derive regions of interest (ROIs)  
7 in each subject's native space using the Desikan-Killany atlas. The structural images were also  
8 segmented into gray matter (GM), white matter (WM), and cerebrospinal fluid (CSF) using  
9 Statistical Parametric Mapping software (SPM12; Wellcome Trust Centre for Neuroimaging,  
10 London, UK) (default parameters). RsfMRI data were preprocessed using SPM12 and FreeSurfer  
11 (v5.3.0). Preprocessing included slice time correction, realignment, coregistration to the T1 image,  
12 and outlier volume detection. All functional images were first corrected for differences in slice  
13 time acquisition using SPM12. Functional images were then realigned to the first volume, and  
14 coregistered to the T1 image. Outliers in average intensity and/or scan-to-scan motion were  
15 identified using the artifact detection toolbox (ART; [http://www.nitrc.org/projects/artifact\\_detect](http://www.nitrc.org/projects/artifact_detect))  
16 using a conservative movement threshold of >0.5 mm/TR and a global intensity z-score of 3.  
17 Outlier volumes were flagged and included as spike regressors during the denoising procedure<sup>71,72</sup>.

18 Additional denoising on the rsfMRI data was performed using the CONN toolbox (v18a:  
19 [www.nitrc.org/projects/conn](http://www.nitrc.org/projects/conn)). Temporal and confounding factors were regressed from each voxel  
20 BOLD timeseries and the resulting residual timeseries were filtered using a temporal band-pass  
21 filter of 0.008-0.09 Hz to examine the frequency band of interest and to exclude higher frequency  
22 sources of noise such as heart rate and respiration. For noise reduction, we used the anatomical  
23 component-based noise correction method aCompCor, which models the influence of noise as a

1 voxel-specific linear combination of multiple empirically estimated noise sources by deriving  
2 principal components from noise regions of interest and including them as nuisance regressors in  
3 the first level general linear model (GLM)<sup>73</sup>. Residual head movement parameters (three rotations,  
4 three translations, and six parameters representing their first-order temporal derivatives) and  
5 signals from WM and CSF, and spike regressors from motion detection were regressed out during  
6 the computation of functional connectivity maps.

7 First-level ROI-to-ROI functional connectivity analysis was performed using the CONN  
8 toolbox. For this analysis, we used 12 FreeSurfer ROIs that included unilateral amygdala, fusiform  
9 gyrus/perirhinal cortex, and inferior temporal gyrus as part of the AT network and retrosplenial  
10 cortex, parahippocampal cortex, and precuneus as part of the PM network (Figure 1). Semi-partial  
11 correlations were used for these first-level analyses to determine the unique variance of each  
12 (unilateral) seed, controlling for the variance of all other seed regions entered into the same model.  
13 For each participant, the rsfMRI time series within each of the ROIs was extracted and the mean  
14 time series was computed. Then, the cross-correlation of each ROI's time course with every other  
15 ROI's time course was computed, creating a 12 x 12 correlation matrix for each subject.  
16 Correlation coefficients (i.e., graph edges) were converted to z-values using Fisher's r-to-z  
17 transformation<sup>38</sup>. As in previous studies<sup>11-13</sup>, the diagonal of the matrix was removed and negative  
18 correlations were set to zero as we were mainly interested in positive connections<sup>39</sup>. We also  
19 performed the same analyses with inclusion of both positive and negative correlations and  
20 observed similar results. Finally, AT and PM network segregation were calculated as the difference  
21 in mean within-network FC and mean between-network FC divided by the mean within-network  
22 FC<sup>13</sup>.

23

## 1 *PET data processing*

2           As part of our standard PET preprocessing procedure, 1.5T structural MRI data were  
3       preprocessed with FreeSurfer to derive ROIs in subject native space. These ROIs were then used  
4       for the calculation of PiB-PET global distribution volume ratio (DVR) and region-specific, partial  
5       volume corrected (PVC<sup>40</sup>) FTP standardized uptake value ratio (SUVR) measures. FTP images  
6       were processed with SPM12. Images were realigned, averaged, and coregistered to each  
7       participant's 1.5T structural MRI scan. SUVR images were calculated by averaging the mean  
8       tracer uptake over the 80-100 minute data and normalized by an inferior cerebellar gray reference  
9       region<sup>74</sup>. The mean SUVR of each (FreeSurfer segmented) ROI was extracted from the native  
10      space images. This data was then partial volume corrected using a modified Geometric Transfer  
11      Matrix approach<sup>75</sup> as previously described<sup>40</sup>. The weighted mean (by region size), partial volume  
12      corrected FTP SUVR of all AT (amygdala, FuG/perirhinal cortex, ITG) and PM (RSC, PHC, and  
13      precuneus) ROIs were used in subsequent analyses. Tau positivity was defined as the mean SUVR  
14      in a Braak<sub>III-IV</sub> composite ROI (cut-off 1.26) that included regions from both AT (amygdala, FuG,  
15      and ITG) and PM (PHC, RSC) systems. *APOE* was not related to segregation ( $p > 0.63$ );  
16      therefore, we did not control for *APOE* in these analyses.

17           PiB images were also processed with SPM12. Images were realigned, averaged across  
18      frames from the first 20 minutes of acquisition, and coregistered to each participant's 1.5T  
19      structural MRI image. DVR values for PiB-PET images were calculated with Logan graphical  
20      analysis over 35-90 minute data and normalized by a cerebellar gray matter reference region<sup>76,77</sup>.  
21      Global PiB was calculated across cortical FreeSurfer ROIs as previously described<sup>41</sup>, and a  
22      threshold of 1.065 was used to classify participants into A $\beta$ - and A $\beta$ + groups<sup>42</sup>. One participant

1 was missing PiB DVR data, and therefore was excluded from all analyses involving measures of  
2 A $\beta$ .

3

#### 4 *Statistical analyses*

5 Statistical analyses were conducted using R (<http://www.R-project.org/>) and SPSS (SPSS  
6 Inc., Chicago IL) software. Independent sample t-tests were used to test for age group differences  
7 in within- and between-network FC and segregation. Pearson correlations and multiple regression  
8 models were used to assess the relationship between segregation, A $\beta$  and tau, and cognitive  
9 performance. To assess the relationship between tau and segregation, we first examined the  
10 relationship across all OA, regardless of A $\beta$  or tau status. We then split the group into A $\beta$ - and  
11 A $\beta$ + subgroups to determine whether there was an interaction of A $\beta$  pathology and tau on  
12 segregation. We used the same procedure to assess the relationship between A $\beta$  and network  
13 segregation. Similarly, to assess the relationship between segregation and cognition, we first  
14 examined this relationship across all OA, regardless of A $\beta$  or tau status. We then split the group  
15 into A $\beta$ - and A $\beta$ + subgroups to determine whether there was an interaction of A $\beta$  pathology and  
16 segregation on cognitive performance. As a follow-up analysis, we also split the groups into tau-  
17 and tau+ groups to confirm that the results remained the same. As the results did not change  
18 depending on whether we split the groups by A $\beta$  or tau status, we report the results in the present  
19 study by splitting the group by A $\beta$  status.

20 Longitudinal cognitive measures were modelled using linear mixed-effects regression with  
21 a random intercept and slope using the lme4 package in R v3.6.3 ([www.r-project.org](http://www.r-project.org)). In order to  
22 examine the relationship between baseline segregation, A $\beta$  and tau, and change in cognitive  
23 performance, the models included two-way interactions between baseline segregation and time,

1 baseline A $\beta$  and time as well as tau and time. We were specifically interested in the segregation x  
2 time interaction to determine whether baseline segregation was associated with longitudinal  
3 episodic memory decline. As a control analysis, we also examined change in working memory and  
4 executive function performance over time using the same model.

5 All predictor variables were standardized before entered into the model. All models were  
6 adjusted for age and sex, and years education (for models including cognitive measures). All  
7 statistical analyses used a two-tailed level of 0.05 for determining statistical significance. Reported  
8 *p*-values were not corrected for multiple comparisons.

9

## 10 **Author Contributions**

11

12 Conceptualization, K.C. and W.J.J.; Methodology & Software: K.E.C., J.N.A., X.C., A.M.,  
13 T.M.H., S.L., and S.B.; Formal Analysis: K.E.C., J.N.A., X.C., A.M., T.M.H., and S.B.; Writing  
14 – Original Draft, K.C. and W.J.J.; Writing – Review & Editing, all authors.

15

## 16 **Competing Interests Statement**

17 Dr. Jagust has served as a consultant to Genentech, Biogen, Bioclinica, Grifols, and CuraSen

18

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23  
24

1 Supplemental Material

2

3 **Alzheimer's pathology is associated with dedifferentiation of functional memory networks**  
4 **in aging**

5

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21

## 1 *AT and PM networks are less segregated with older age regardless of analysis approaches*

2           The relationship between age group and segregation was assessed across multiple analysis  
3 approaches related to matrix thresholding, bivariate vs. semi-partial correlations, various network  
4 metrics of intersystem relationships, and network labeling.

5           To assess the influence of matrix thresholding on age group differences in network  
6 segregation, this supplementary analysis was identical to the original analysis (in the main text)  
7 except we retained both positive and negative correlations in each subject's z-matrix (Figure S1A).  
8 Similarly, to assess the influence of type of correlation analysis on age group differences in  
9 network segregation, this supplementary analysis was identical to the original one except we  
10 calculated bivariate correlations instead of semi-partial correlations (Figure S1B).

11           To examine the influence of network labeling on age group differences in network  
12 segregation, we used two different labeling schemes (in addition to our original one). First, we  
13 used the Brainnetome Atlas<sup>1</sup>, using all ROIs from amygdala (4 ROIs), FuG (6 ROIs), ITG (14  
14 ROIs), PHC (12 ROIs), RSC (4 ROIs), and precuneus (8 ROIs). To create these ROIs, we produced  
15 4mm-radius spheres centered around each MNI coordinate from the literature (Figure S1C). To  
16 create AT and PM networks based on the same AT and PM regions used in one of the seminal  
17 papers defining AT and PM systems<sup>2</sup>, we added 4 FreeSurfer ROIs each to our original AT and  
18 PM networks. These additional FreeSurfer regions included bilateral lateral orbitofrontal cortex  
19 and temporal pole for the AT network and medial orbitofrontal and posterior cingulate cortices for  
20 the PM network, creating a total of 10 ROIs for each network (Figure S1D).

21           To assess the influence of various network metrics of intersystem relationships, we used  
22 the Brain Connectivity Toolbox in Matlab to calculate participation coefficient and modularity  
23 values for each subject. The participation coefficient of a given ROI measures to what extent an



1 ROI interacts with ROIs in other networks in relation to the total number of connections it contains  
2 in its own network. Each subject's participation coefficient value was calculated from their  
3 respective z-matrix. Participation coefficients for each ROI were computed based on the following  
4 formula:

$$5 \quad P(i) = 1 - \sum_{m=1}^M \left[ \frac{k_i(m)}{k_i} \right]^2$$

6  
7 where  $k_i(m)$  is the weighted connections of ROI  $i$  with nodes in network  $m$  and  $k_i$  is the  
8 total weighted connections ROI  $i$  exhibits. Thus, higher participation coefficient values indicate  
9 proportionally greater communication with ROIs in other networks (Figure S1E).

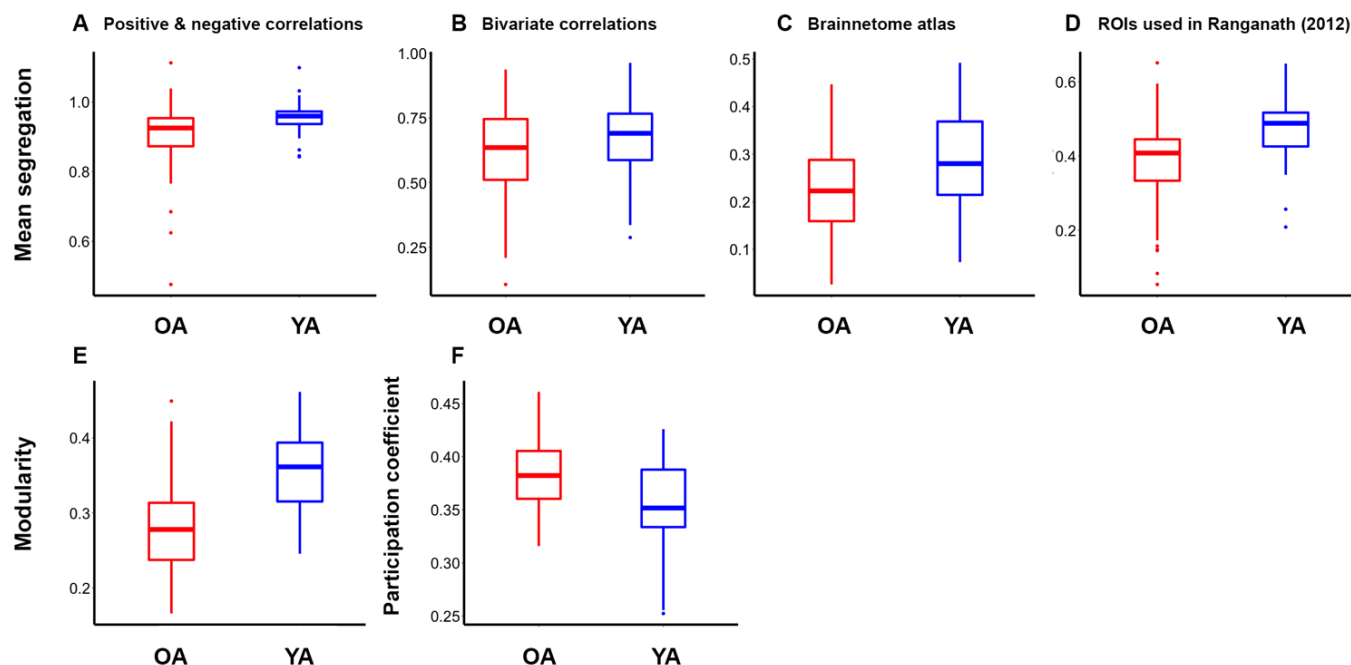
10 Similar to network segregation, modularity assesses the strength of module (i.e., network)  
11 segregation. Specifically, the modularity index ( $Q$ ) compares the observed intra-module functional  
12 connectivity with that which is expected by chance. Thus, higher modularity values reflect stronger  
13 separation of the system's modules. The modularity index is formally defined as:

$$14 \quad Q = \frac{1}{2E} \sum_{ij} [A_{ij} - \gamma e_{ij}] \delta(m_i, m_j)$$

15  
16  
17 Where  $E$  is the number of graph connections (i.e., edges),  $A$  is the adjacency matrix,  $\gamma$  is the  
18 resolution parameter,  $e$  is the null model, and  $\delta$  is an indicator that equals 1 if ROIs  $i$  and  $j$  belong  
19 to the same module and 0 otherwise (Figure S1F).

20

21



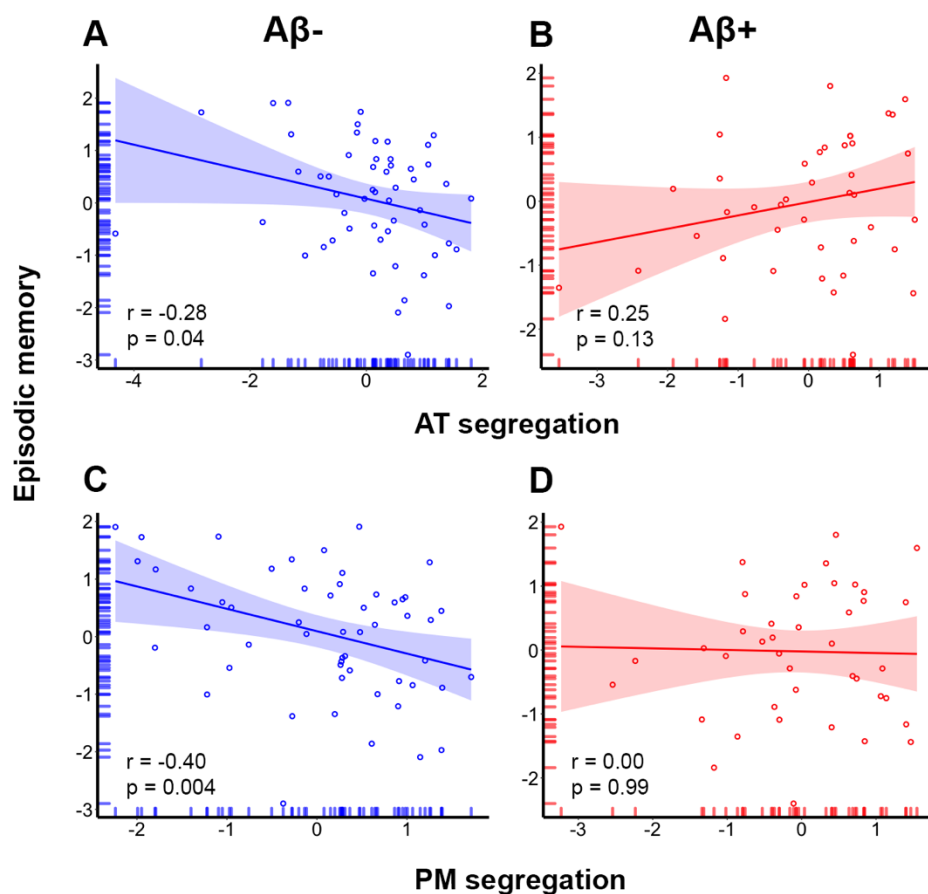
1  
2 **Figure S1.** Older adults show significantly less segregated networks compared to younger adults  
3 across multiple analysis approaches related to A) matrix thresholding: inclusion of positive and  
4 negative correlations ( $t = 2.8, p = 0.006$ ), B) bivariate correlations ( $t = 2.4, p = 0.019$ ), network  
5 labeling: C) Brainnetome Atlas ( $t = 3.4, p = 0.001$ ) and D) inclusion of 20 FreeSurfer ROIs used  
6 in Ranganath et al. 2012. ( $t = 5.7, p < 0.001$ ), and various network metrics of intersystem  
7 relationships: E) participation coefficient ( $t = 4.7, p < 0.001$ ), and F) modularity ( $t = 7.9, p <$   
8  $0.001$ ).

9  
10 ***AD pathology moderates the association between segregation and episodic memory in AT and***  
11 ***PM networks***

12 To examine the association between network segregation and episodic memory in the main  
13 text, we computed a single segregation measure by averaging the AT and PM segregation values  
14 because our episodic memory composite measure included both object- and spatial-related

1 memory domains. Figure S2 below shows that the results were essentially the same in both the AT  
2 and PM networks separately.

3



4

5 **Figure S2. Alzheimer's disease pathology moderates the association between network**

6 **segregation and episodic memory performance in AT and PM systems. (A)** Less segregated

7 AT networks are associated with better performance in Aβ- older adults whereas **(B)** AT

8 segregation is not associated with performance in Aβ+ older adults. **(C)** Similarly, less segregated

9 PM networks are associated with better performance in Aβ- older adults whereas **(D)** PM

10 segregation is not associated with performance in Aβ+ older adults.

11

12 *Baseline segregation predicts longitudinal memory decline using various measures of pathology*

1  
2 In order to examine the relationship between baseline segregation, baseline A $\beta$  and tau,  
3 and change in cognitive performance, we used a linear mixed model that included two-way  
4 interactions between baseline segregation and time, global A $\beta$  and time, and tau and time. In the  
5 main text, we report the results using continuous measures of global A $\beta$  and Braak<sub>III-IV</sub> tau as they  
6 retain more statistical power in the model. The results were very similar whether we used Braak<sub>III-</sub>  
7 <sub>IV</sub> tau (Table 3 in main text), AT-tau (Table S1) or PM tau (Table S2) and whether we used  
8 dichotomous (Table S3) or continuous A $\beta$  and tau (Table 3 in main text) in the model. All models  
9 were adjusted for age, sex, and education.

10  
11 **Table S1.** Linear mixed model results for segregation and pathology (including AT-tau) predicting  
12 longitudinal episodic memory change.

Predictor	Estimate	p
Age	-0.20	0.02
Sex	-0.003	0.97
Education	0.13	0.12
Segregation	-0.23	0.007
Time	-0.07	0.051
AT-tau	-0.11	0.4
A $\beta$	0.03	0.79
AT-tau x Time	-0.19	<0.001
A $\beta$ x Time	0.007	0.87
Segregation x Time	0.07	0.049

13

14

1 **Table S2.** Linear mixed model results for segregation and pathology (including PM-tau) predicting  
2 longitudinal episodic memory change.

<b>Predictor</b>	<b>Estimate</b>	<b>p</b>
Age	-0.20	0.03
Sex	0.02	0.84
Education	0.13	0.13
Segregation	-0.18	0.036
Time	-0.07	0.071
PM-tau	-0.11	0.29
A $\beta$	0.03	0.79
PM-tau x Time	-0.08	0.073
A $\beta$ x Time	-0.05	0.25
Segregation x Time	0.07	0.05

3  
4 **Table S3.** Linear mixed model results for segregation and (dichotomous) pathology predicting  
5 longitudinal episodic memory change.

<b>Predictor</b>	<b>Estimate</b>	<b>p</b>
Age	-0.20	0.02
Sex	0.007	0.94
Education	0.13	0.15
Segregation	-0.18	0.032
Time	-0.06	0.09
Tau-status	0.009	0.93
A $\beta$ -status	0.03	0.78
Tau-status x Time	-0.09	0.03
A $\beta$ -status x Time	-0.01	0.78
Segregation x Time	0.07	0.05

6  
7 **References**

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