

1 **Neural dynamics of semantic categorization in semantic variant of Primary Progressive**
2 **Aphasia**

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4 Running Title:

5 **Brain dynamics of semantic categorization in semantic variant of PPA**

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34

35 **Abstract**

36

37 Awake humans constantly extract conceptual information from a flow of perceptual
38 inputs. Category membership (e.g., *is it an animate or inanimate thing?*) is a critical semantic
39 feature used to determine the appropriate response to a stimulus. Semantic representations
40 are thought to be processed along a posterior-to-anterior gradient reflecting a shift from
41 perceptual (e.g., *it has eight legs*) to conceptual (e.g., *venomous spiders are rare*) information.
42 One critical region is the anterior temporal lobe (ATL): patients with semantic variant primary
43 progressive aphasia (svPPA), a clinical syndrome associated with ATL neurodegeneration,
44 manifest a deep loss of semantic knowledge.

45 Here, we test the hypothesis that svPPA patients, in the absence of an intact ATL,
46 perform semantic tasks by over-recruiting areas implicated in perceptual processing. We
47 acquired MEG recordings of 18 svPPA patients and 18 healthy controls during a semantic
48 categorization task. While behavioral performance did not differ, svPPA patients showed
49 greater activation over bilateral occipital cortices and superior temporal gyrus, and inconsistent
50 engagement of frontal regions.

51 These findings indicate a pervasive reorganization of brain networks in response to ATL
52 neurodegeneration: the loss of this critical hub leads to a dysregulated (semantic) control
53 system, and defective semantic representations are compensated via enhanced perceptual
54 processing.

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56 Introduction

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58 Approaching a greenish, twisted object during a countryside walk, you might have two
59 very different reactions: running away or simply stepping over it. Such a seemingly easy
60 process, i.e., telling a *snake* from a *rope*, requires the interplay of multiple cognitive processes
61 relying on different neural substrates. First, the visual input must be analyzed, collecting
62 information on all possibly relevant motor-perceptual features (e.g., *color*, *sound*, *movement*).
63 Then, the extracted features must be merged into a unitary concept to allow proper
64 identification (e.g., *it's a rope*). Finally, one can select and perform an appropriate response
65 (e.g., *I'll walk by it*). All the neural computations supporting these processes occur within a few
66 seconds. While the earliest perceptual processing takes place in the occipital cortex, the final
67 stages (i.e., motor programming and execution) entail activation of frontal-parietal structures.
68 The critical intermediate steps, involving the transformation from a visual input to a concept
69 (and its semantic categorization as living vs. nonliving, dangerous vs. harmless), have been
70 linked to the coordinated activity of multiple neural areas (Clarke & Tyler, 2015). Functional
71 neuroimaging and neuropsychological research indicate that semantic knowledge is encoded
72 within distributed networks (Huth, Nishimoto, Vu, & Gallant, 2012; Fernandino et al. 2015),
73 with a few key cortical regions acting as critical hubs (Lambon-Ralph, Jefferies, Patterson, &
74 Rogers, 2017). However, many open questions remain as to the nature of neural
75 representations and computations in these different areas, and how they dynamically interact.

76 Prior functional neuroimaging studies suggested that populations of neurons along the
77 ventral occipito-temporal cortex (vOT) tune to ecologically relevant categories leading to a
78 nested representational hierarchy of visual information (Grill-Spector & Weiner, 2014), where
79 specialized cortical regions respond preferentially to faces (Gauthier et al., 2000; Kanwisher,
80 McDermott, & Chun, 1997), places (Epstein & Kanwisher, 1998), bodies and body parts (P. E.
81 Downing, Wiggett, & Peelen, 2007; P. Downing & Kanwisher, 2001), or objects (Lerner, Hendler,
82 Ben-Bashat, Harel, & Malach, 2001). Living stimuli appear to recruit lateral portions of vOT,
83 while nonliving stimuli are highlighted in medial regions (Martin & Chao, 2001). Multiple
84 organizing principles appear to be responsible for the representational organization of these
85 areas, including agency and visual categorizability (Thorat, Proklova, & Peelen, 2019). Overall,

86 semantic representations appear to be processed in a graded fashion along a posterior-to-
87 anterior axis: from perceptual (e.g., *snakes are elongated and legless*) to conceptual
88 information (e.g., *a snake is a carnivorous reptile*) (Borghesani et al., 2016; Peelen & Caramazza,
89 2012). Notwithstanding this overall distributed view, different areas have been linked with
90 specific computational roles: from modality-specific nodes in secondary motor and sensory
91 areas to multimodal convergence hubs in associative cortices (Binder & Desai, 2011).

92 Neuropsychological findings corroborate the idea of a distributed yet specialized
93 organization of semantic processing in the brain, supported by the interaction of a perceptual
94 representational system arising along the occipito-temporal pathway, a semantic
95 representational system confined to the anterior temporal lobe (ATL), and a semantic control
96 system supported by fronto-parietal cortices (Lambon-Ralph et al., 2017). For instance, focal
97 lesions in the occipito-temporal pathway are associated with selective impairment for living
98 items and spared performance on nonliving ones (Blundo, Ricci, & Miller, 2006; Caramazza &
99 Shelton, 1998; Laiacona, Capitani, & Caramazza, 2003; Pietrini et al., 1988; Sartori, Job, Miozzo,
100 Zago, & Marchiori, 1993; Warrington & Shallice, 1984) as well as the opposite pattern (Laiacona
101 & Capitani, 2001; Sacchett & Humphreys, 1992). Moreover, acute brain damage to prefrontal or
102 temporoparietal cortices in the semantic control system has been linked with semantic aphasia,
103 a clinical syndrome characterized by deficits in tasks requiring manipulations of semantic
104 knowledge (Jefferies & Lambon Ralph, 2006).

105 A powerful clinical model to study the organization of the semantic system is offered by
106 the semantic variant primary progressive aphasia (svPPA or semantic dementia, Hodges et al.,
107 1992, Gorno-Tempini et al., 2004). This rare syndrome is associated with ATL
108 neurodegeneration as confirmed by the observation of grey matter atrophy (Collins et al.,
109 2016), white matter alterations (Galantucci et al., 2011), and hypometabolism (Diehl et al.,
110 2004), as well as neuropathological findings (Hodges & Patterson, 2007). Patients with svPPA
111 present with an array of impairments (e.g., single-word comprehension deficits, surface
112 dyslexia, impaired object knowledge) that can be traced back to a generalized loss of semantic
113 knowledge, often affecting all stimuli modalities and all semantic categories (Hodges &
114 Patterson, 2007). Conversely, executive functions and perceptual abilities are relatively

115 preserved. Hence, these patients provide crucial neuropsychological evidence of the role played
116 by the ATL in the storage of semantic representations, and can be leveraged to investigate the
117 breakdown of the semantic system and the resulting compensatory mechanisms.

118 Pivotal steps forward in understanding the neurocognitive systems underlying semantic
119 (as well as any other human) behaviors are enabled by the iterative, systematic combination of
120 behavioral and neuroimaging data from both healthy controls and neurological patients (Price
121 & Friston, 2002). However, task-based imaging in patients is hampered by specific difficulties
122 (e.g., patients' compliance) and limitations (e.g., performance is not matched and error signals
123 can act as confounds) (Price, Crinion, & Friston, 2006; S. Wilson, Yen, & Eriksson, 2018). To date,
124 very few studies have attempted to deploy functional imaging in rare clinical syndromes such as
125 svPPA, thus it is still not fully clear how structural damage and functional alterations relate to
126 the observed cognitive and behavioral profile. Previous findings suggest that residual semantic
127 abilities come from the recruitment of homologous and perilesional temporal regions, as well
128 as increased functional demands on the semantic control system i.e., parietal/frontal regions
129 (Maguire, Kumaran, Hassabis, & Kopelman, 2010; Mummery et al., 1999; Pineault et al., 2019;
130 Viard et al., 2013; S. M. Wilson et al., 2009). Recently, magnetoencephalographic imaging
131 (MEG) has proven useful in detecting syndrome-specific network-level abnormalities
132 (Ranasinghe et al., 2017; Sami et al., 2018) as well as task-related functional alterations (Kielar,
133 Deschamps, Jokel, & Meltzer, 2018) in neurodegenerative patients. Critically, it has been
134 suggested that imperfect behavioral compensation can be achieved via reorganization of the
135 dynamic activity in the brain (Borghesani et al., 2020): owing to their damage to the ventral,
136 lexico-semantic reading route, svPPA patients appear to over-recruit the dorsal,
137 sublexical/phonological pathway to read not only pseudowords, but also irregular ones.

138 Here, we test the hypothesis that svPPA patients, burdened with ATL damage, thus
139 lacking access to specific conceptual representations, overemphasize perceptual information as
140 well as overtax the semantic control system to maintain accurate performance on a semantic
141 categorization task (living vs. nonliving, see Fig. 1a). Given the shallow semantic nature of the
142 task, we expect comparable performance in patients with svPPA and a group of healthy

143 controls, with the critical differences emerging in neural signatures. Specifically, we expected
144 patients to over-recruit occipital areas, supporting their greater reliance on visual processing.

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147 **Results**

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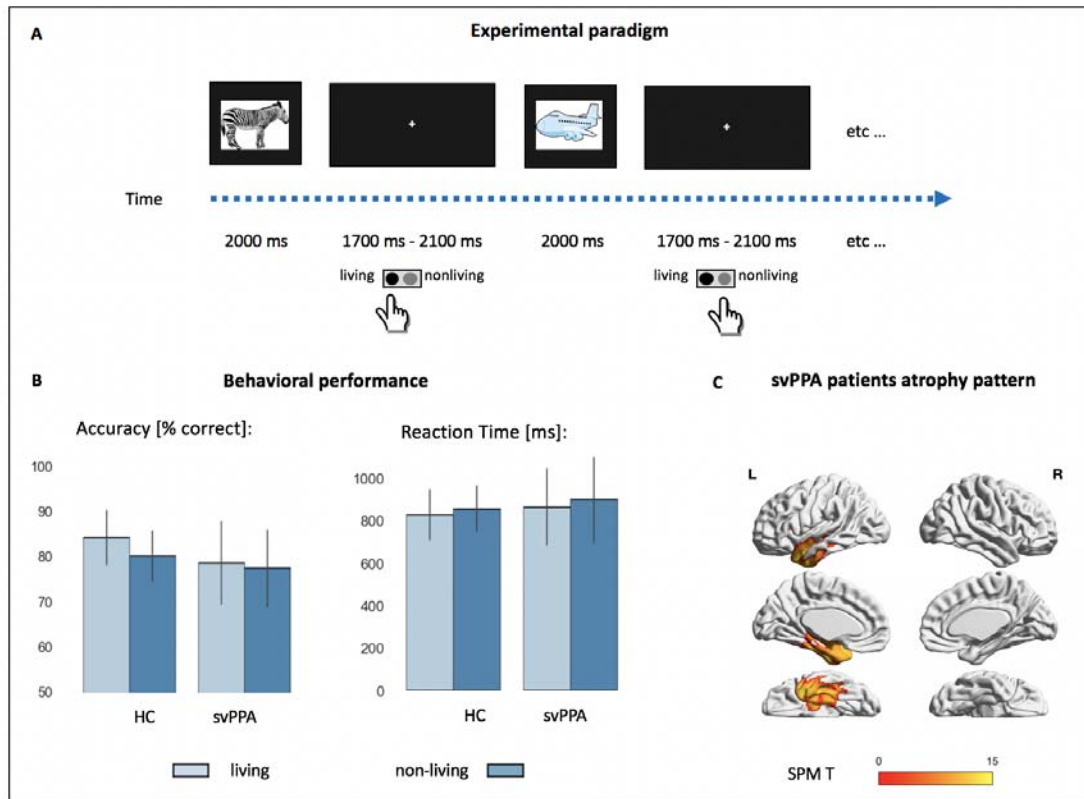
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150 Behavioral data and cortical atrophy

151 Behavioral performance during the MEG scan neither differed between the two cohorts
152 nor between the two stimulus categories. Statistically significant differences were not observed
153 in reaction times (HC: living: 826.3 ± 112.5 , nonliving: 856.9 ± 104.4 ; svPPA: living: 869.8 ± 179.8 ,
154 nonliving: 911.1 ± 194.45), or accuracy (HC: living: 84.5 ± 5.8 , nonliving: 80.4 ± 5.4 ; svPPA: living:
155 80.5 ± 6.2 , nonliving: 79.1 ± 6). Overall, these results indicate that svPPA patients can perform the
156 task as proficiently as healthy elders, an expected finding due to the relatively shallow semantic
157 processing requirements and simple stimuli used in the task (see Fig. 1b).

158 Distribution of cortical atrophy in the svPPA cohort is shown in Figure 1c. Patients
159 present atrophy in the anterior temporal lobe, involving the temporal pole, the inferior and
160 middle temporal gyrus. This pattern of neurodegeneration is consistent with their clinical
161 diagnosis and overall neuropsychological profile (see Table 1).

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163
164 **Fig. 1 Experimental paradigm, behavioral performance, and cortical atrophy.** (A) Cartoon representation of the experimental
165 setting. Colored drawings were presented for 2 seconds, with an inter-stimuli-interval jittered between 1.7 and 2.1 seconds.
166 Subjects responded with a button press with their dominant hand. (B) Percentage accuracy and reaction times during the
167 semantic categorization tasks in controls and svPPA patients, across the two stimuli conditions (living vs. nonliving items). (C)
168 Voxel based morphometry (VBM)-derived atrophy pattern showing significantly reduced grey matter volumes in svPPA
169 patients' anterior temporal lobes, views from top to bottom shown: lateral, medial, ventral (thresholded at $p < 0.001$ with family
170 wise error (FWE) correction).

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173 Time course of neural activity during visual semantic categorization

174 Within-group analyses of brain activity during the semantic categorization task, relative
175 to pre-stimulus baseline activity levels, are presented for both controls and svPPA patients in
176 Supl. Fig. 1. In brief, following presentation of the images both cohorts showed posterior-to-
177 anterior progression of functional activation across all five frequency bands. In the high-gamma
178 band (63-117 Hz), we observed bilateral increases in synchronous power starting in the occipital
179 cortex and progressively extending to temporal, parietal, and frontal regions (see Supl. Fig. 1a).
180 In the low-gamma band (30-55 Hz), subjects show heightened synchronization over bilateral
181 occipital cortices, evident early in the svPPA group and only later in HC. Moreover, both groups
182 showed reductions in activity over frontal cortices starting mid-trial (see Supl. Fig. 1b). A similar

183 progression of alpha (8-12 Hz) and beta (12-30 Hz) band activity revealed significant reductions
184 in synchronous activity for both groups, extending from bilateral occipital cortices to temporal
185 and parietal lobes, and involving progressively larger areas in precentral and superior frontal
186 gyrus. A focus of increased alpha synchrony in anterior cingulate regions, mid-trial, is evident in
187 both groups (see Supl. Fig. 1c-d). Finally, induced theta band (3-7 Hz) activity revealed
188 progressive increases in synchronous activity over bilateral occipital cortices, a similarly
189 progressive pattern of increased synchronization within frontal regions at an onset window
190 after that of occipital regions, and progressively reduced theta activity relative to baseline levels
191 over parietal and temporal lobes (see Supl. Fig. 1e).

192 Taken together, these stimulus-locked task-induced changes indicate, in both cohorts
193 and across all frequency bands, the expected pattern of visual processing followed by motor
194 response preparation. Notwithstanding the overall similarity in spatiotemporal dynamics,
195 specific activation differences were detected between svPPA patients and HC and are reported
196 below.

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TABLE 3. Results of MEG contrasts				
t-test svPPA vs HC	Time Window	Local Maxima		
	ms	MNI [x,y,z]	p-value	t-value
<i>Theta Band [3-7 Hz]</i>				
left lingual gyrus	0 - 212	-10.0 -100.0 -10.0	0.005	3.7
left lingual gyrus	412 - 612	-8.5 -100.0 -8.1	0.005	3.1
right precentral gyrus	62 - 187	41.9 -13.6 66.2	0.005	3.4
right medial and superior frontal gyrus	187 - 412	21.8 64.0 -8.1	0.001	-3.2
<i>Alpha Band [8-12 Hz]</i>				
right precentral gyrus	212 - 612	45.0 -15.0 40.0	0.001	3.4
left middle temporal gyrus	237 - 362	-59.8 -41.6 -1.0	0.005	2.8
left anterior cingulate	462 - 612	-4.7 35.5 -9.7	0.005	3.1
left parahippocampal gyrus	512 - 612	-22.5 -49.3 -8.9	0.005	2.9
<i>Beta Band [12-30 Hz]</i>				
left cingulate cortex	0 - 62	-6.2 -30.3 43.3	0.005	2.9
left lingual gyrus	87 - 112	-9.3 -100.5 -13.6	0.005	2.9
right superior frontal gyrus	62 - 137	30.3 36.2 47.8	0.005	3
right medial frontal gyrus	137 - 262	7.8 56.8 11.7	0.001	3.6
left middle temporal gyrus	237 - 362	-65.0 -20.0 -5.0	0.001	-3.4
left superior frontal gyrus	562 - 612	-21.8 46.7 45.7	0.005	-3.1
<i>Low Gamma Band [30-55 Hz]</i>				
left lingual gyrus	62 - 612	-10.1 -98.4 -8.9	0.001	4.2
left inferior occipital gyrus	362 - 612	-34.8 -93.9 2.7	0.001	4.1
right lingual gyrus	212 - 437	18.2 -89.1 8.3	0.005	3.4
right medial frontal gyrus	212 - 412	9.3 63.0 2.2	0.001	3.7
left superior frontal gyrus	262 - 462	-3.8 62.8 14.0	0.005	3.6
<i>High Gamma Band [63-117 Hz]</i>				
left superior frontal gyrus	62 - 137	-36.5 26.6 48.8	0.001	3.4
left superior temporal gyrus	62 - 287	-48.2 -22.3 13.3	0.005	3
left parahippocampal gyrus	212 - 312	-15.5 -27.1 -6.5	0.001	3.3
right medial frontal gyrus	287 - 337	13.2 70.7 0.6	0.005	3.2
left superior frontal gyrus	287 - 612	-22 68.4 14	0.001	3.6
right superior frontal gyrus	462 - 612	43.9 54.7 17.2	0.001	3.9

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Table 3. Local maxima in MNI coordinates. Time window, MNI coordinates, p- and t-value of the local maxima of the different MEG whole-brain contrasts performed. The spatiotemporal distribution of these clusters at 4 exemplar time points can be appreciated in Figure 2.

Neural dynamics of semantic categorization in a faulty semantic system

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We investigated when, where, and at which frequency svPPA patients differ from healthy controls during semantic categorization of visual stimuli. While the overall pattern of activation across frequencies and time is similar, crucial differences between the two cohorts emerged in the between-group analyses performed in each frequency band. Table 3 summarizes the temporal windows, peaks of local maxima, and t-values of all clusters isolated by the direct comparison of the two cohorts. Figure 2 allows appreciation of the spatiotemporal distribution of these clusters at 4 exemplar time points.

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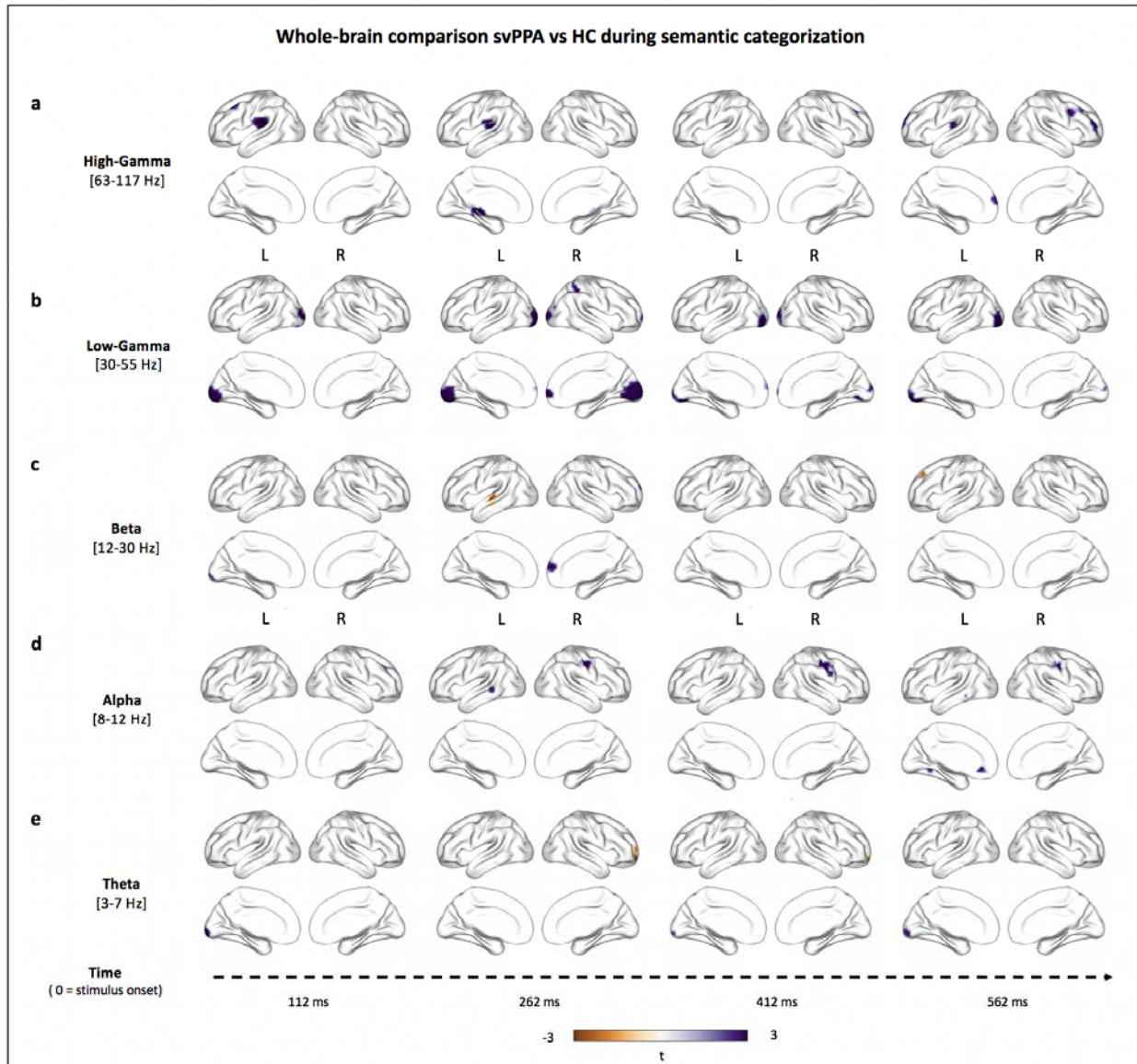
215 In the high-gamma band, we detected significantly higher synchronization in svPPA
216 patients, relative to controls, over left superior temporal (at both early and late time points)
217 and right frontal (at late time points) cortices (see Fig. 2a). In the low-gamma band, we
218 observed an extensive spatio-temporal cluster over bilateral occipital cortices with significantly
219 higher synchronized activity in svPPA patients relative to controls. Similarly, small clusters of
220 gamma activity, relatively more desynchronized in HC than svPPA, resulted in an increased
221 gamma synchrony in medial frontal cortices at ~300 ms for the svPPA group (see Fig. 2b).
222 Overall, the results at high frequencies (30-117 Hz) suggest thus higher activity in svPPA over
223 bilateral occipital and left superior temporal cortices throughout the trial, and right frontal
224 cortices at late time points.

225 Between-group contrast in beta-band revealed, in svPPA patients, more
226 desynchronization (i.e., more beta suppression) over the left superior temporal gyrus at ~300
227 ms, while simultaneously displaying less desynchronization in a right middle-frontal cluster (see
228 Fig. 2c). In the alpha-band, svPPA patients showed less desynchronization over left middle
229 temporal gyrus at ~300 ms as well as in later clusters in the right precentral gyrus, left anterior
230 cingulate, and left parahippocampal gyrus (see Fig. 2d). Finally, in the theta band significant
231 differences over the left occipital cortex occurred at both early (~100 ms) and late (~500 ms)
232 time points indicating higher synchronization in svPPA patients compared to HC, while the
233 opposite pattern (i.e., higher activity for HC) is observed in a right frontal cluster at ~300ms (see
234 Fig. 2e). Overall, the results at low frequencies (3-30 Hz) suggest thus higher activity in svPPA
235 over bilateral occipital and left superior temporal cortices, while indicating less activity in left
236 middle-temporal and right frontal regions.

237 Taken together, these findings suggest that svPPA patients performed the semantic
238 categorization tasks by over-recruiting bilateral occipital cortices and left superior temporal
239 gyrus, while showing less reliance on left middle-temporal regions and inconsistent
240 engagement of frontal ones.

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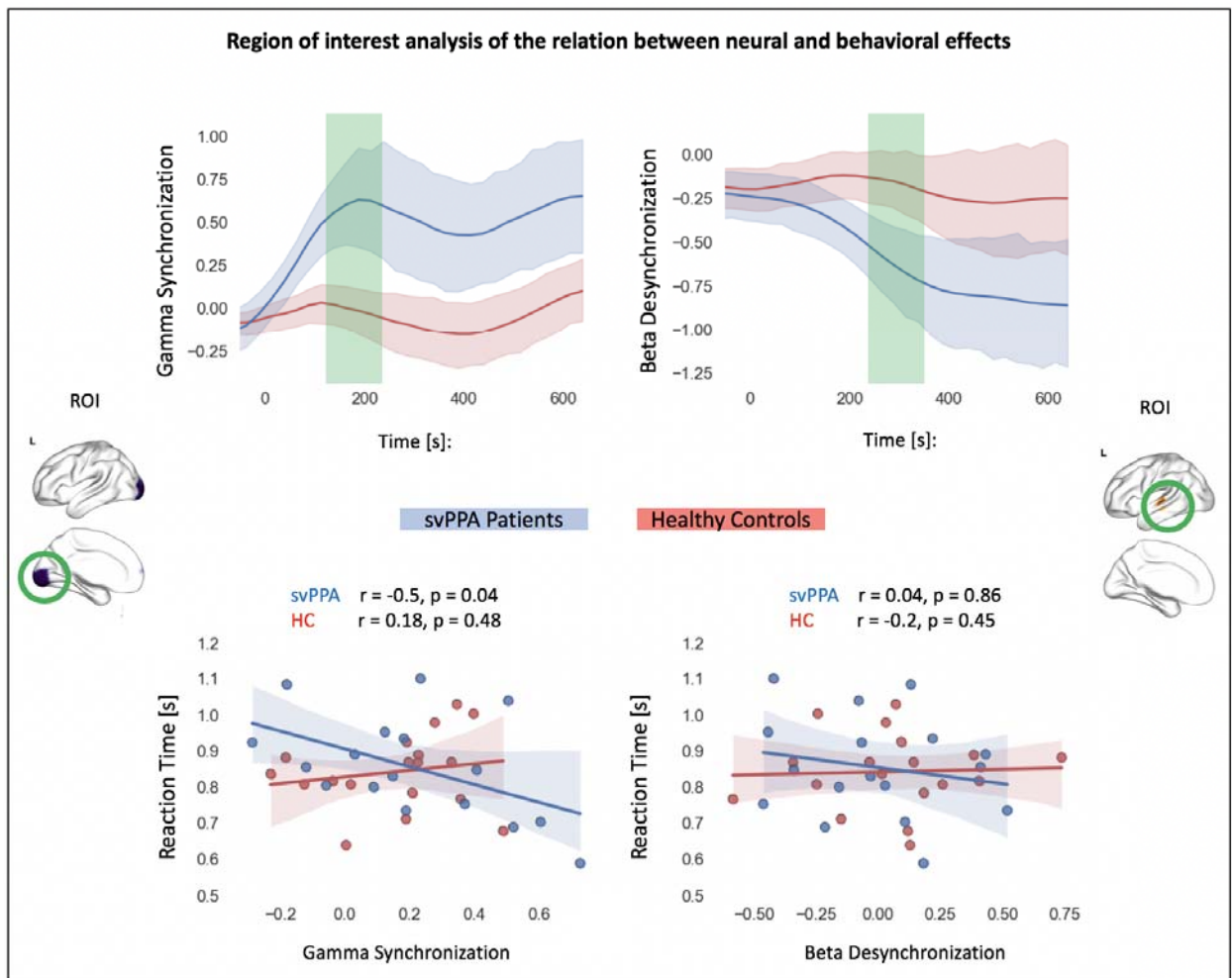
243 **Figure 2. Stimulus-locked (0 ms = stimulus onset) between-group analyses of changes in oscillatory power.** Rendering of the
244 results in the high-gamma (a), low-gamma (b), beta (c), alpha (d) and theta (e) bands. Purple color = more synchronization in
245 svPPA (vs. HC). Brown color = less synchronization in svPPA (vs. HC). Table 3 summarizes the temporal windows, peaks of local
246 maxima, and t-values of all clusters isolated by the direct comparison of the two cohorts.

247

248 Occipital gamma synchronization correlates with reaction times in svPPA

249 As illustrated in Fig. 3, our region-of-interest (ROI) post-hoc analysis suggests a linear
250 relation between occipital gamma synchronization and RTs in svPPA patients ($r = -0.5$, $p = 0.04$),
251 an effect not seen in healthy controls ($r = 0.18$, $p = 0.48$). Neither of the cohorts show a

252 significant correlation between STG beta suppression and RTs (svPPA: $r = 0.04$, $p = 0.86$, HC: $r =$
253 -0.2 , $p = 0.45$).



254
255 **Figure 3. Results of the region of interest post-hoc analysis correlating reaction times and beta/gamma activity.** Two ROIs
256 were centered on the main clusters resulting from the contrast svPPA patients vs. healthy controls in the gamma band (left) and
257 in the beta band (right) in the 100ms window surrounding the peak effect.

258 259 Discussion

260
261 This is the first study investigating the spatiotemporal dynamics of semantic
262 categorization of visual stimuli in a cohort of svPPA patients. We provide compelling evidence
263 that, burdened with ATL damage, svPPA patients recruit additional perilesional and distal
264 cortical regions to achieve normal performance on a shallow semantic task. As compared to
265 healthy age-matched controls, svPPA patients showed greater activation over bilateral occipital
266 cortices and superior temporal gyrus, indicating over-reliance on perceptual processing and

267 spared dorsal language networks. Conversely, they showed inconsistent engagement of frontal
268 regions, suggesting less efficient control responses.

269 These findings have important implications both for current neurocognitive models of
270 the language systems, and on the utility of MEG imaging in clinical populations. First, the
271 detection of over-recruitment of occipital and superior-temporal regions paired with
272 incongruous engagement of frontal ones, speaks to the distributed and dynamic organization of
273 the semantic system, where semantic representations are supported by occipito-temporal
274 cortices and semantic control by fronto-parietal ones. Second, the observation that normal
275 performance can be achieved via altered neural dynamics elucidates the neurocognitive
276 mechanisms that support compensation in neurological patients. Specifically, we contribute to
277 the body of literature illustrating how network-driven neurodegeneration leads to the
278 reorganization of the interplay of various cortical regions.

279

280 Faulty semantic representations: compensating conceptual loss with perceptual information

281 Our key finding is that svPPA patients can achieve normal performance in a shallow
282 semantic task by over-relying on perilesional language-related regions (STG), as well as on distal
283 visual (occipital) and executive (frontal) networks. At frequencies spanning low and high gamma
284 bands, svPPA patients show increased activity in occipital and superior temporal cortices
285 relative to their healthy counterparts. Gamma oscillations have been associated with local
286 computations (Donner & Siegel, 2011), promoting unification and binding processes (Hagoort et
287 al. 2004), including merging of multimodal semantic information (van Ackeren et al., 2014).
288 Similarly, results at lower frequencies indicate greater neural activity in svPPA over bilateral
289 occipital and left superior temporal cortices. Theta oscillations have been associated with
290 operations over distributed networks, such as those required for lexico-semantic retrieval
291 (Bastiaansen et al., 2005; Bastiaansen et al., 2008; Kiehl et al., 2015) and integration of
292 unimodal semantic features (van Ackeren et al., 2014). This data also suggests that more
293 engagement of occipital areas (via increased gamma band activity) is related to better
294 performance (faster RTs). In our patients, compensation for faulty semantic representations

295 seems thus to rely primarily on local and distributed computations in networks associated with
296 perceptual processing.

297 In principle, the semantic task employed in the current study (i.e., identifying a visually
298 presented object as either a living or nonliving) can be performed by focusing on a few key,
299 distinctive, motor-perceptual features: *if it has eyes and teeth, it is a living being*. Further
300 processing steps, such as would be required for an object-identification and naming (i.e.,
301 accessing the appropriate lexical label), require the integration of multiple motor-perceptual as
302 well as conceptual features (Borghesani & Piazza, 2017): *a python is a nonvenomous snake that*
303 *kills by constriction*. Combining the behavioral data collected during the recordings and outside
304 and the scanner, it appears clear that HC can recognize (and likely inevitably mentally name)
305 each item, while svPPA patients can only provide the categorical label. Patient data is thus
306 critical in characterizing the division of labor between the distributed set of cortical regions
307 involved in semantic processing. Our findings strongly suggest that ATL damage hampers
308 operation of the semantic representation system, by shattering their conceptual components
309 and thus forcing over-reliance on perceptual features coded in posterior cortices. This is
310 consistent with a growing body of research. For instance, it has been shown that the ability to
311 merge perceptual features into semantic concepts relies on the integrity of the ATL (Hoffman,
312 Evans, & Lambon Ralph, 2014), and that ATL damage promotes reliance on perceptual
313 similarities over conceptual ones (Lambon-Ralph, Sage, Jones, & Mayberry, 2010). Moreover, it
314 appears that the more motor-perceptual information is associated with a given concept, the
315 more resilient it is to damage, an advantage that is lost once the disease progresses from ATL to
316 posterior ventral temporal regions (Hoffman, Jones, & Ralph, 2012).

317

318 Faulty semantic representations: overtaxing the semantic control network

319 Compared to healthy controls, svPPA patients appear to have less activation in the left
320 middle-temporal gyrus and to inconsistently engage frontal regions, suggesting that increased
321 demands to the semantic control systems are met by inefficient responses in prefrontal and
322 superior frontal cortices. Comparing the two cohorts across frequency bands, it appears that an
323 enhanced late high frequency (local neural) response occurs in svPPA, versus an earlier and

324 lower frequency (long range connection) response in controls. One speculation for this pattern
325 is that in svPPA an initial inefficient response in the (semantic) cognitive control network
326 centered on frontal areas leads to a later higher reliance on local activity for (semantic)
327 cognitive control and decision-making processes.

328 Previous studies demonstrated that object recognition in visual areas is facilitated by
329 prior knowledge (Bannert & Bartels, 2013) received via feedback projections from both frontal
330 (Bar et al., 2006) and anterior temporal (Coutanche & Thompson-Schill, 2015) cortices.
331 Moreover, it has been observed that higher demands for feature integration entail more
332 recurrent activity between fusiform and ATL (Clarke, Taylor, & Tyler, 2011). Our study provides
333 a direct contrast between subjects in which both frontal and ATL feedback inputs are preserved
334 (HC), and those in which ATL neurodegeneration forces reliance exclusively on frontal inputs.

335 Interestingly, the observed temporal dynamics (with the detection of early frontal
336 involvement) are not compatible with a strictly feedforward model of visual stimuli processing.
337 This is in line with recent evidence that recurrent neural models are needed to explain the
338 representational transformations supporting visual information processing (Gwilliams & King,
339 2019; Kietzmann, Spoerer, Sörensen, Cichy, & Hauk, 2019).

340 Thus, taken together, our findings corroborate the idea that the conversion from
341 percept to concept is supported by recurrent loops over fronto-parietal and occipito-temporal
342 regions which have been implicated in, respectively, semantic control and semantic
343 representations (Chiou, Humphreys, Jung, & Lambon Ralph, 2018).

344 345 Clinical implications

346 Our findings corroborate the idea that neurodegeneration leads to the dynamic
347 reorganization of distributed networks (Agosta et al., 2014; Guo et al., 2013), and that task-
348 based MEG imaging can be instrumental in deepening our understanding of the resulting
349 alterations (Borghesani et al., 2020). Ultimately, these efforts will pave the way towards
350 treatment options, as well as better early diagnostic markers as functional changes are known
351 to precede structural ones (Bonakdarpour et al., 2017). For instance, our results support
352 previous neuropsychological evidence suggesting that the origin of svPPA patients' difficulties
353 during semantic categorization tasks are linked to degraded feature knowledge rather than, as

354 it happens in other FTDs, to a deficit of the executive processes involved (Koenig, Smith, &
355 Grossman, 2006).

356 Our results are in line with prior studies relating svPPA patients' performance on
357 semantic tasks with respect to not only the expected hypoactivation of the left ATL and
358 functionally connected left posterior inferior temporal lobe (Mummery et al., 1999), but also
359 based on the patterns of hyperactivations observed in the current study. Heightened activity
360 has been reported in peritrophic left anterior superior temporal gyrus as well as more distant
361 left premotor cortex, and right anterior temporal lobe (Mummery et al., 1999; Pineault et al.,
362 2019). Individual subject analyses have indicated that patients might attempt different
363 compensatory strategies, which may vary in terms of efficiency and, crucially, would rely on the
364 recruitment of different cortical networks (Viard et al., 2013, 2014). For instance, studies on
365 reading have associated svPPA patients' imperfect compensation of the semantic deficit
366 (leading to regularization errors) with over-reliance on parietal regions subserving sub-lexical
367 processes (Wilson et al., 2009). Consistently, task-free studies of intrinsic functional networks
368 suggest that the downregulation of damaged neurocognitive systems can be associated with
369 the upregulation of spared ones. In svPPA patients, recent fMRI evidence shows coupling of
370 decreased connectivity in the ventral semantic network with increased connectivity in the
371 dorsal articulatory-phonological one (Battistella et al., 2019; Montembeault et al., 2019).
372 Additionally, svPPA has been linked with specific spatiotemporal patterns of neuronal
373 synchrony alterations: alpha and beta hyposynchrony in the left posterior superior temporal
374 and adjacent parietal cortices, and delta-theta hyposynchrony in left posterior
375 temporal/occipital cortices (Ranasinghe et al., 2017). Our findings also align with the recent
376 observation that, during reading, svPPA patients can (imperfectly) compensate for their
377 damage to the ventral route by over-recruiting the dorsal one (Borghesani et al., 2020). The
378 present findings corroborate thus the idea that neurodegeneration forces the reorganization of
379 the interplay between ventral and dorsal language networks.

380 Critically, the present functional neuroimaging results and their interpretation rest on
381 the fact that the task allowed engagement of semantic processing in patients in which the
382 semantic system is, by definition, compromised. Contrary to a more challenging task such as

383 naming, patients with svPPA were able to perform the semantic categorization as accurately
384 and fast as healthy controls. Hence, probing the semantic system at the proper level of
385 difficulty (Wilson et al., 2018), we avoided the challenging interpretation of activation maps
386 associated with failure to perform a task (Price et al., 2006). Our findings thus call for caution
387 when evaluating studies comparing clinical cohorts based solely on behavioral data: failing to
388 detect a difference in performance does not necessarily correspond to similar underlying
389 neurocognitive resources.

390

391 Limitations and future perspectives

392 The nature of the clinical model we adopted constrains our sample. First, even if ours is
393 the to-date largest cohort of svPPA patients assessed with task-based functional neuroimaging,
394 our sample size is relatively small, owing to the rareness of the disease. We thus have limited
395 statistical power, preventing us from, for instance, further exploring brain-behavior
396 correlations. Second, our subjects (both healthy controls and patients) are older than those
397 reported in previous studies on semantic categorization, cautioning against direct comparisons.
398 While it has been shown that the neural dynamics of visual processing are affected by aging,
399 the reduced and delayed activity observed does not necessarily relate to poorer performance,
400 but rather may be mediated by task difficulty (Bruffaerts et al., 2019). Moreover, previous
401 evidence suggests that even if semantic processing remains intact during aging, its
402 neurofunctional organization undergoes changes. For instance, (Lacombe, Jolicoeur, Grimault,
403 Pineault, & Joubert, 2015) found that, during a verbal semantic categorization task, older adults
404 exhibited behavioral performance equivalent to that of young adults, but showed less
405 activation of the left inferior parietal cortex and more activation of bilateral temporal cortex.
406 Finally, our task design does not allow further investigation of potential categorical effects.
407 Future studies wishing to investigate representations of living and nonliving items separately
408 will require more trials and stimuli carefully controlled for psycholinguistic variables such as
409 prototypicality and familiarity. Contrary to patients with damage to the ventral occipito-
410 temporal cortex due to stroke or herpes simplex encephalitis, svPPA patients usually do not
411 present categorical dissociations (Moss, Rodd, Stamatakis, Bright, & Tyler, 2005). However,
412 deeper investigations of time-resolved neural activity in svPPA could shed light onto the debate

413 on the nature of ATL representations: category-specific deficits might arise from lacunar (rather
414 than generalized) impairment of graded representations (Lambon Ralph, Lowe, & Rogers,
415 2007).

416 417 Conclusions

418 Combining task-based MEG imaging and a neuropsychological model, we provide novel
419 evidence that faulty semantic representations following ATL damage can be partially
420 circumvented by additional processing in relatively spared occipital and dorsal stream regions.
421 Our results thus inform current neurocognitive models of the semantics system by
422 corroborating the idea that it relies on the dynamic interplay of distributed functional neural
423 networks. Moreover, we highlight how MEG imaging can be leveraged in clinical populations to
424 study compensation mechanisms such as the recruitment of perilesional and distal cortical
425 regions.

426 427 **Materials and methods**

428 429 Subjects

430 Eighteen svPPA patients (13 female, 66.9 ± 6.9 years old) and 18 healthy age-matched
431 controls (11 female, 71.3 ± 6.1 years old) were recruited through the University of California
432 San Francisco (UCSF) Memory and Aging Center (MAC). All subjects were native speakers, and
433 had no contraindications to MEG. Patients met currently published criteria as determined by a
434 team of clinicians based on a detailed medical history, comprehensive neurological and
435 standardized neuropsychological and language evaluations (Gorno-Tempini et al., 2011).
436 Besides being diagnosed with svPPA, patients were required to score at least 15 out of 30 on
437 the Mini-Mental Status Exam (MMSE; Folstein, Folstein, & McHugh, 1975) and be otherwise
438 sufficiently functional to be scanned. Healthy controls were recruited from the University of
439 California San Francisco Memory and Aging Center (UCSF MAC) healthy aging cohort, a
440 collection of subjects with normal cognitive and neurological exam and MRI scans without
441 clinically evident strokes. Inclusion criteria required the absence of any psychiatric symptoms or
442 cognitive deficits (i.e., Clinical Dementia Rating - CDR = 0, and MMSE $\geq 28/30$). Demographic

443 information and neuropsychological data are shown in Table 1. The study was approved by the
444 UCSF Committee on Human Research and all subjects provided written informed consent.
445

446 **Table 1 Demographics and neuropsychological profiles.** Healthy controls and semantic variant of Primary Progressive Aphasia
 447 (svPPA) patients, native English speakers, were matched for age, gender and education. Scores shown are mean (standard
 448 deviation). * indicate values significantly different from controls (P<0.05). MMSE = Mini-Mental State Exam; CDR = Clinical
 449 Dementia Rating; PPVT = Picture Vocabulary Test; WAB = Western Aphasia Battery; VOSP = Visual Object and Space Perception
 450 Battery.

TABLE 1. Demographics and neuropsychological profiles		
	<i>Controls</i>	<i>svPPA</i>
<i>Demographic</i>		
<i>N</i>	18	18
Age, mean (SD)	70.7 ± 6.5	67.1 ± 6.2
Education, mean (SD)	17.5 ± 1.8	17.9 ± 3.2
Gender, <i>n</i> female	12	9
Handedness, <i>n</i> right	15	15
MMSE (max 30)	29.0 ± 1.6	24.5 ± 3.8*
CDR score	0.03 ± 0.1	0.7 ± 0.4*
CDR Box score	0.3 ± 1.2	4.0 ± 2.6*
<i>Language Production</i>		
Boston (object) naming test (15)	14.7 ± 0.6	5.4 ± 3.7*
Phonemic (D-letter) fluency	15.7 ± 5.8	9.1 ± 4.3*
Semantic (animal) fluency	23.4 ± 3.9	9.3 ± 4.1*
<i>Language Comprehension</i>		
PPVT (max 16)	---	9.4 ± 3.2
WAB Auditory Word Recognition (60)	---	56.5 ± 4.2
WAB Sequential Command (100)	---	70.7 ± 14.3
Digit Span forwards	7.1 ± 1.1	6.4 ± 1.2
<i>Reading</i>		
Arizona Reading Total (max 36)	35.6 ± 0.5	30.5 ± 3.7*
Regular High Frequency Words (9)	9 ± 0.0	8.8 ± 0.4
Regular Low Frequency Words (9)	8.9 ± 0.2	8.3 ± 1.2
Irregular High Frequency Words (9)	8.9 ± 0.3	7.7 ± 0.6
Irregular Low Frequency Words (9)	8.8 ± 0.4	5.7 ± 2.3
PseudoWords (18)	15.8 ± 2.7	15.2 ± 2.2
<i>Spelling</i>		
Arizona Spelling Total (max 20)	18.1 ± 1.6	13.1 ± 4.0*
Regular High Frequency Words (5)	5 ± 0.0	4.4 ± 0.9
Regular Low Frequency Words (5)	4.5 ± 0.6	4.1 ± 0.8
Irregular High Frequency Words (5)	4.1 ± 0.9	2.1 ± 1.6
Irregular Low Frequency Words (5)	4.5 ± 0.5	2.6 ± 1.6
PseudoWords (10)	8.8 ± 1.3	8.1 ± 2.6
Famous Faces- Spontaneous Naming (max 16)	12.4 ± 3.4	2.9 ± 2.4*
Famous Faces- Face Recognition (max 20)	18.4 ± 2.0	12.8 ± 6.5*
Famous Faces Short Triplets, Pictures (max 10)	8.9 ± 1.0	6.6 ± 2.4
Famous Faces Short Triplets, Words (max 10)	9.7 ± 0.6	7.0 ± 2.0
<i>Working Memory/Executive functions</i>		
Digit Span backwards	5.4 ± 1.1	4.5 ± 1.6*
Modified Trials (total time)	25.3 ± 13.6	41.9 ± 23.1*
Modified Trials (# of correct lines)	13.2 ± 3.2	13.2 ± 3.3
Design Fluency (# of correct designs)	11.7 ± 3.0	7.1 ± 3.4*
<i>Visuospatial function</i>		
Benson figure copy (17)	15.7 ± 0.7	15.3 ± 1.0
VOSP Number Location (30)	9.3 ± 0.9	9.0 ± 1.5
<i>Visual memory</i>		
Benson figure recall (17)	12.1 ± 2.4	7.1 ± 4.9*

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457 Stimuli and Experimental Design

458 All subjects performed a semantic judgment task on visually presented stimuli (Figure
459 1a). Stimuli consisted of 70 colored drawings: 36 belonging to the semantic category of living
460 items (e.g., animals, plants), and 34 belonging to the semantic category of nonliving items (e.g.,
461 tools, furniture).

462 To validate the set of stimuli, a behavioral study was conducted on a separate group of
463 54 age-matched healthy subjects (31 women; 47 right-handed; age = 74.21 years \pm 8.63;
464 education = 15 years \pm 2.02). First, subjects had to report the most common name for each
465 drawing (i.e., *"Identify the item in the image: what is the first name that comes to mind?"*). They
466 were given the possibility of providing a second term if needed (i.e., *"If appropriate, write the
467 second name that came to mind."*). They were then asked to rate how familiar they are with the
468 item on a 7-point scale from *"not at all familiar"* to *"very familiar"*. Finally, they were asked
469 whether the item belongs to the category of living or nonliving items, and to rate how
470 prototypical for that category the item is (i.e., *"How good is this picture as example of an item
471 of that category?"*) on a 7-point scale from *"bad example"* to *"good example"*. Data were
472 collected with Qualtrics software (Qualtrics, Provo, UT, USA. <https://www.qualtrics.com>) and
473 subjects recruited from the broad pool of subjects enrolled in the above described UCSF MAC
474 healthy aging cohort. For each stimulus, we calculated the percentage of agreement with our
475 pre-set categorization, average familiarity, average prototypicality, and then compared the
476 living and nonliving categories. For living items, the average percentage of agreement with the
477 assigned category was 96.86% \pm 4.07, the lowest score was 75.93% for the item *"dinosaur"*. For
478 non-living items, the average percentage of agreement was 99.18% \pm 1.20, the lowest score
479 was 96.30% for the items *"pizza"* and *"hamburger"*. A two-tailed t-test revealed that the
480 difference between the two categories was significant ($p=0.002$): the rate of agreement was
481 higher for nonliving items than for living ones. The average prototypicality of living items was
482 6.24 \pm 0.52 (range 6.74 to 4), while for nonliving items 6.47 \pm 0.32 (range 6.85 to 5.19) for
483 nonliving items. Again, a two-tails t-test revealed a significant difference between the two
484 categories ($p=0.032$): nonliving items were judged more prototypical of their category than
485 living ones. As for familiarity, the average for living items was 6.15 \pm 0.32 (range 6.8 to 4.81),

486 while for nonliving items was 6.67 ± 0.21 (range 6.91 to 6.02). Even in this case the difference
487 between the two categories was significant (two-tails t-test, $p < 0.001$): nonliving items were
488 judged more familiar.

489 Images of the two categories were also compared in terms of visual complexity
490 (calculated as Shannon entropy via the python package Scikit-Image, <https://scikit-image.org/>).
491 No significant difference between living (3.04 ± 0.84) and nonliving (3.13 ± 0.96) items
492 emerged. Finally, we compared stimuli in terms of the length (number of letter), imaginability,
493 concreteness, and familiarity of their most common lexical label as extracted from the Medical
494 Research Council (MRC, http://websites.psychology.uwa.edu.au/school/MRCDatabase/uwa_mrc.htm) Psycholinguistic
495 Database, and word frequency was extracted from the Corpus of Contemporary American
496 English (COCA, <https://www.wordfrequency.info/>). Consistent with our online questionnaire,
497 the only statistically significant differences between the two categories were imaginability
498 (living: 613.19 ± 19.62 , nonliving: $596.43.15 \pm 28.08$, $p = 0.03$) and familiarity (living: $498.26 \pm$
499 69.32 , nonliving: 547.96 ± 45.82 , $p < 0.001$). All the psycholinguistic variables characterizing the
500 stimuli are shown in Table 2.
501

502 Visual stimuli were projected into the magnetically shielded MEG scanner room via a
503 system of mirrors mounted within the scanner room for this purpose, with the final mirror
504 positioned roughly 24" from the subject's face. Subjects were instructed to classify the pictures
505 as living or nonliving by pressing one of two response buttons with their dominant hand. Stimuli
506 were displayed for 2 seconds, with an inter-stimulus interval jittered between 1.7 and 2.1
507 seconds. A total of 170 trials were presented: each individual stimulus was repeated 2.5 times
508 in a random order. E-Prime (<https://pstnet.com/products/e-prime/>) was used to present the
509 stimuli; events from ePrime and the response pad were automatically routed into the imaging
510 acquisition software and integrated with magnetoencephalographic traces in real time.

511
512

	<i>Living Items</i>	<i>Nonliving Items</i>
N	36	34
Examples	<i>fish, flower</i>	<i>scissors, train</i>
Frequency (log)	3.69 (0.54)	3.96 (0.65)
Length (# of letters)	5.29 (1.58)	5.61 (1.84)
Immaginability	613.19 (19.62)	596.43 (28.08) *
Familiarity (norm)	498.26 (69.32)	547.96 (45.82) *
Familiarity (quest)	6.15 (0.32)	6.67 (0.21) *
Concreteness	608.27 (16.26)	599.10 (25.94)
Cat. Agreement	96.86 (4.07)	99.18 (1.20) *
Cat. Prototypicality	6.24 (0.52)	6.47 (0.32) *
Visual Complexity	3.04 (0.84)	3.13 (0.96)

513

514 **Table 2. Psycholinguistic characteristics of the stimuli.** Stimuli consisted of 70 colored drawings illustrating living items (n=36)
515 or nonliving items (34). Length, Imaginability, Concreteness, and Familiarity (norm) were extracted from the Medical Research
516 Council (MRC) Psycholinguistic Database searching for the most common label for each item. Similarly, Frequency was
517 extracted from the Corpus of Contemporary American English (COCA). Category Agreement, Category prototypicality, and
518 Familiarity (quest.) were assessed with a behavioral study on separate age-matched healthy controls. As a proxy for Visual
519 Complexity, we used Shannon entropy as computed with Scikit-Image. Values shown are mean (standard deviation). * indicate
520 values significantly different between the two categories (two-tailed t-test, $p < 0.05$).

521

522 Behavioral analyses

523 Subject performance, i.e. reaction times (RTs) and accuracy, was analyzed using an
524 analysis of variance (ANOVA) based on the two stimuli categories (living vs. nonliving) and two
525 cohorts (controls vs. svPPA patients) using the Python statistical library (statsmodels -
526 www.statsmodels.org). Data from one outlier in the svPPA cohort were excluded from the
527 behavioral analyses (average reaction times were 1.35 s versus 0.8 ms in the whole cohort).

528

529 MRI protocol and analyses

530 Structural T1-weighted images were acquired on a 3T Siemens system (Siemens,
531 Erlangen, Germany) installed at the UCSF Neuroscience Imaging Center, equipped with a
532 standard quadrature head coil with sequences previously described (Mandelli et al., 2014). MRI
533 scans were acquired within 1 year of the MEG data acquisition.

534

535 To identify regions of atrophy, svPPA patients were compared to a separate set of 25
536 healthy controls collected using the same protocol (14 females, mean age 66.2 ± 8.5) via voxel-
537 based morphometry (VBM). Image processing and statistical analyses were performed using
538 the VBM8 Toolbox implemented in Statistical Parametric Mapping (SPM8, Wellcome Trust
Center for Neuroimaging, London, UK, <http://www.fil.ion.ucl.ac.uk/spm>) running under Matlab

539 R2013a (MathWorks). The images were segmented into grey matter, white matter, and CSF,
540 bias corrected, and then registered to the Montreal Neurological Institute (MNI). Grey matter
541 value in each voxel was multiplied by the Jacobian determinant derived from the spatial
542 normalization to preserve the total amount of grey matter from the original images. Finally, to
543 ensure the data are normally distributed and compensate for inexact spatial normalization, the
544 modulated grey matter images were smoothed with a full-width at half-maximum (FWHM)
545 Gaussian kernel filter of 8x8x8 mm. A general linear model (GLM) was then fit at each voxel,
546 with one variable of interest (group), and three confounds of no interest: gender, age,
547 education, and total intracranial volume (calculated by summing across the grey matter, white
548 matter and CSF images). The resulting statistical parametric map (SPM) was thresholded at
549 $p < 0.001$, with family wise error (FWE) correction, and a cluster extent threshold of 100 voxels.
550 This SPM was additionally used as a binarized image of atrophy to act as an exclusive mask for
551 the MEG source reconstruction results visualization (see below).

552

553 MEG protocol and analyses

554 Neuromagnetic recordings were conducted using a whole-head 275 axial gradiometer
555 MEG system (Omega 2000, CTF, Coquitlam, BC, Canada) at a sampling rate of 1200 Hz, under a
556 bandpass filter of 0.001 to 300 Hz, while subjects performed the task. Subjects were lying
557 supine, with their head supported near the center of the sensor array. Head position was
558 recorded before and after each scan using three fiducial coils (nasion, left/right preauricular)
559 placed on the subject. All subjects included in the current study reported movement under 5
560 mm during the experimental run. Twenty-nine reference sensors were used to correct distant
561 magnetic field disturbance by calculating a synthetic 3rd order gradiometer (Weinburg et al.,
562 1984; Vrba and Robinson, 2001), which was applied to signal post-acquisition. Datasets were
563 epoched with respect to stimulus presentation onset (stimulus-locked trials from -0.5 to 1.0
564 sec) and artifacts rejected using a semi-automated process outlined as follows: noisy channels
565 were identified as having more than 20 trials exceeding 1.5pT amplitude under a temporary
566 bandpass filter of 3 to 50 Hz, with no more than 5 channels in the sensor array removed.
567 Epochs were then flagged and removed for any remaining artifacts exceeding the 1.5pT
568 threshold. Mean number of trials included in analyses for the two groups did not significantly

569 differ (svPPA mean = 155 trials [std dev = 20, range 121-170], control mean = 162 [std dev = 16,
570 range 103-172], 2-tailed $t[34]=1.059$, $p=.297$).

571 Alignment of structural and functional images was performed using 3 prominent
572 anatomical points (nasion and preauricular points), marked in the individuals' MR images and
573 localized in the MEG sensor array using the 3 fiducial coils attached to these points during the
574 MEG scan. A 3D grid of voxels with 5mm spatial resolution covering the entire brain was
575 created for each subject and recording, based on a multisphere head model of the coregistered
576 structural 3D T1-weighted MR scan. Reconstruction of whole brain oscillatory activity within
577 these voxels was performed via the Neurodynamic Utility Toolbox for MEG (NUTMEG;
578 <http://nutmeg.berkeley.edu>), which implements a time–frequency optimized adaptive spatial
579 filtering technique to estimate the spatiotemporal estimate of neural sources. The tomographic
580 volume of source locations was computed using a 5 mm lead field that weights each cortical
581 location relative to the signal of the MEG sensors (Dalal et al., 2008).

582 We sought to investigate both evoked and induced changes in brain activity, i.e. to study
583 modulations of ongoing oscillatory processes that are not necessarily phased-locked (Makeig et
584 al., 2004). Moreover, we wished to explore both high and low frequency ranges as they bear
585 different functional interpretations, in particular their association with different spatial scales:
586 high-frequency and low-frequency oscillations are associated with local and distributed
587 computations, respectively (Donner & Siegel, 2011). Thus, we examined task-related
588 modulations of ongoing oscillatory processes in 5 frequency bands: theta (3-7 Hz), alpha (8-12
589 Hz), beta (12-30 Hz), low-gamma (30-55 Hz) and high-gamma (63-117 Hz) (FIR filter having
590 widths of 300 ms for theta/alpha, 200 ms for beta, 150 ms for low-gamma, and 100 ms for high-
591 gamma; sliding over 25 ms time windows). Source power for each voxel location in a specific
592 time window and frequency band was derived through a noise-corrected pseudo-F statistic
593 expressed in logarithmic units (decibels; dB), describing signal magnitude during an “active”
594 experimental time window relative to an equivalently-sized, static pre-stimulus baseline
595 “control” window (Robinson & Vrba, 1999). Single subject beamformer reconstructions were
596 spatially normalized by applying each subject's T1-weighted transformation matrix to their
597 statistical map.

598 Group analyses were performed on normalized reconstructions using statistical
599 nonparametric mapping (SnPM, Singh et al, 2003), both within-group and between-groups.
600 Three-dimensional average and variance maps across subjects were calculated at each time
601 point and smoothed with a $20 \times 20 \times 20\text{mm}^3$ Gaussian kernel (Dalal et al., 2008). From this map,
602 pseudo-t statistics evaluated the magnitude of the contrast obtained at each voxel and time.
603 Voxel labels were permuted to create a T-distribution map for within- and between- group
604 contrasts (2^N permutations, where N = number of subjects, up to 10,000 permutations). Each
605 voxel's t-value was evaluated using 2^N degrees of freedom to determine the corresponding p-
606 value associated with each voxel's pseudo-F value (Singh, Barnes, & Hillebrand, 2003). For
607 uncorrected p-values attaining a threshold of $p < .005$, a cluster correction was applied,
608 whereby cortical significance maps were thresholded, voxel-wise, under an additional
609 requirement to have 26 adjacent significant voxels. To remove potential artifacts due to
610 neurodegeneration or eye movement (lacking electrooculograms), we masked statistical maps
611 using patients' ATL atrophy maps (see section MRI protocol and analyses), as well as a
612 ventromedial frontal mask [MNI coordinates: -70 70; 5 75; -60 -10]. We utilized these to
613 examine the pattern of activation during semantic categorization separately for controls and
614 svPPA patients (SnPM one-sample t-test against baseline) and directly compare svPPA patients
615 and controls to highlight spatiotemporal clusters of differential activity between the two
616 cohorts (SnPM two-sample t-test).

617 Finally, we conducted a region-of-interest (ROI) post-hoc analysis aimed at investigating
618 the relation between subjects' behavioral performance and neural activity. Two ROIs were
619 centered on the main clusters resulting from the contrast svPPA patients vs. healthy controls in
620 the gamma band (occipital lobe, coordinates: [-15 -5], [-105 -95], [-15 -5]) and in the beta band
621 (temporal lobe, coordinates: [-70 -60], [-25 -15], [-10 0]). Single subjects' values were extracted
622 in both ROIs in the 100ms window surrounding the peak effect (gamma-band peak: 112-212
623 ms, beta-band peak: 237-337 ms) and correlated with the reaction times.

624

625 Data Availability

626 The clinical and neuroimaging data used in the current paper are available from the
627 corresponding author, upon reasonable request. The sensitive nature of patients' data and our
628 current ethics protocol do not permit open data sharing at this stage.

629

630

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635

636

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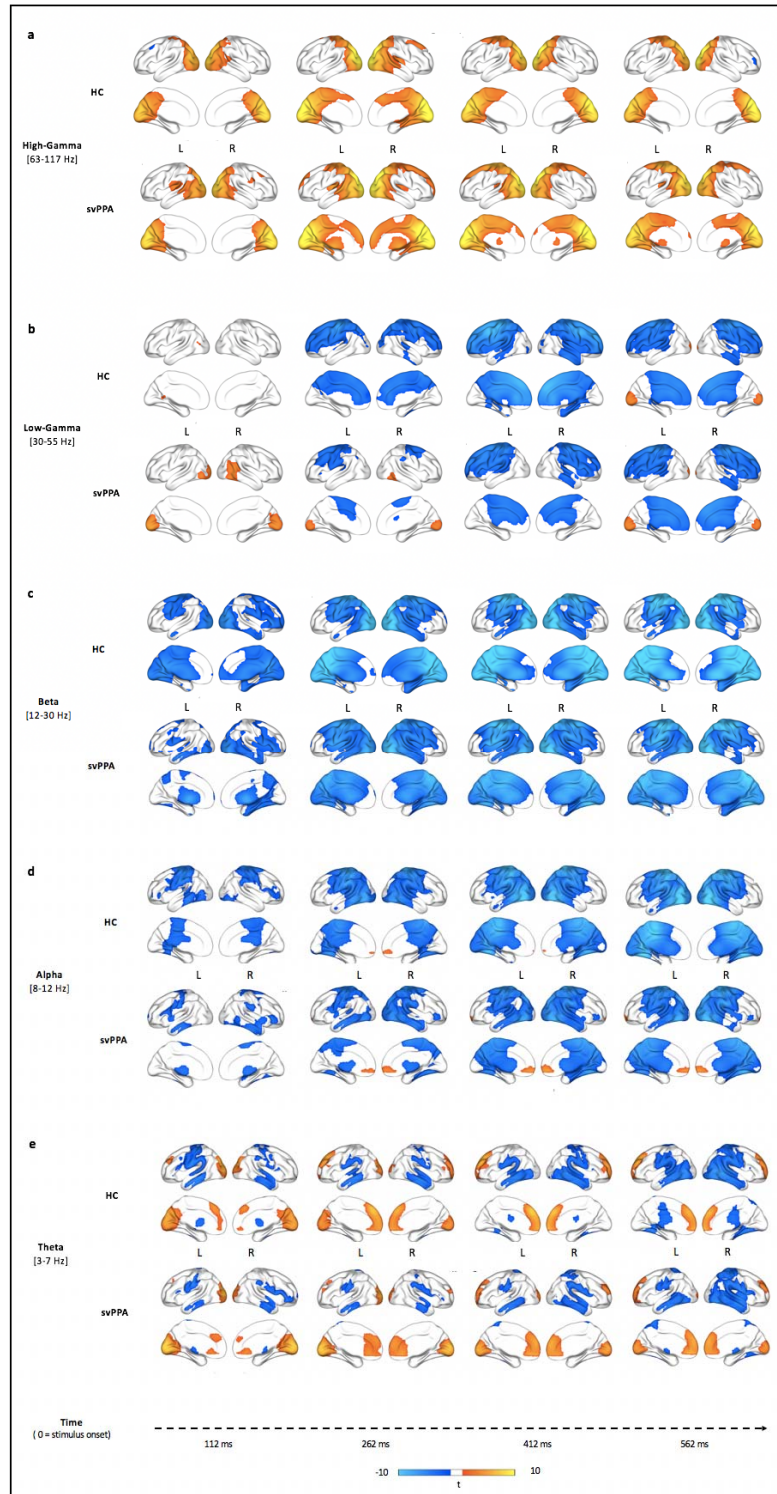
647 **Competing interests**

648 The authors declare no competing interests.

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Supl. Fig. 1. Stimulus-locked (0 ms = stimulus onset) within-group analyses of task-related changes in oscillatory power. a) Rendering of the results in the high-gamma band for both controls (HC, upper row) and patients (svPPA, lower row). Cold color = more desynchronization (vs. baseline). Warm color = more synchronization (vs. baseline). c-d) Same as in (a) but for the low-gamma, beta, alpha, and theta band respectively. For details, please see text.

660

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