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5 **Title:** Medial prefrontal cortex compresses concept representations through learning

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7 **Brief title:** Medial PFC compression during learning

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33 **Keywords:** prefrontal cortex; fMRI; attention; category learning; computational
34 modeling

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Abstract

Prefrontal cortex (PFC) is thought to support the ability to focus on goal-relevant information by filtering out irrelevant information, a process akin to dimensionality reduction. Here, we test this dimensionality reduction hypothesis by combining a data-driven approach to characterizing the complexity of neural representation with a theoretically-supported computational model of learning. We find direct evidence of goal-directed dimensionality reduction within human medial PFC during learning. Importantly, by using model predictions of each participant's attentional strategies during learning, we find that that the degree of neural compression predicts an individual's ability to selectively attend to concept-specific information. These findings suggest a domain-general mechanism of learning through compression in mPFC.

Introduction

Prefrontal cortex (PFC) is sensitive to the complexity of incoming information (Badre, Kayser, & D'Esposito, 2010) and theoretical perspectives suggest that a core function of PFC is to focus representation on goal-relevant features by filtering out irrelevant content (Mante, Sussillo, Shenoy, & Newsome, 2013; Wilson, Takahashi, Schoenbaum, & Niv, 2014). In particular, medial PFC (mPFC) is thought to represent the latent structures of experience (Schlichting, Mumford, & Preston, 2015; Zeithamova, Dominick, & Preston, 2012), coding for causal links (Chan, Niv, & Norman, 2016) and task-related cognitive maps (Schuck et al., 2016). At the heart of these accounts is the hypothesis that during learning, mPFC performs data reduction on incoming information, compressing task-irrelevant features and emphasizing goal-relevant information structures. This compression process is goal-directed and akin to how attention in category learning models dynamically selects features that have proven predictive across recent learning trials (Love & Gureckis, 2007; Love, Medin, & Gureckis, 2004). Although emerging evidence suggests structured representations occur in the rodent homologue of mPFC (Farovik et al., 2015), such coding in human PFC remains poorly understood. Here, we directly assess the data reduction hypothesis by leveraging an information-theoretic approach in human neuroimaging to measure how goal-driven learning is supported by attention updating processes in mPFC.

We focused on concept learning, given the recent findings that mPFC represents conceptual information in an organized fashion (Constantinescu, O'Reilly, & Behrens, 2016). Participants learned to classify the same insect images (Figure 1A), composed of three features that could take on two values (thick/thin legs, thick/thin antennae, pincer/shovel mandible), across three different learning problems (Shepard, Hovland, & Jenkins, 1961). These learning problems were defined by rules that required consideration of different numbers of features to successfully classify (see Table 1): the low category complexity problem was unidimensional (e.g., insects living in warm climates have thick legs, cold climate insects have thin legs), the medium category complexity problem depended on two features (e.g., insects from rural environments have thick antennae and shovel mandible or thin antennae and pincer mandible, urban insects have thick antennae and pincer mandible or thin antennae and shovel mandible), and the high category complexity problem required all three features (i.e., each insect's class was uniquely defined by a combination of features). By using the same stimuli for all three problems, the manipulation of conceptual complexity allowed us to target goal-specific learning processes.

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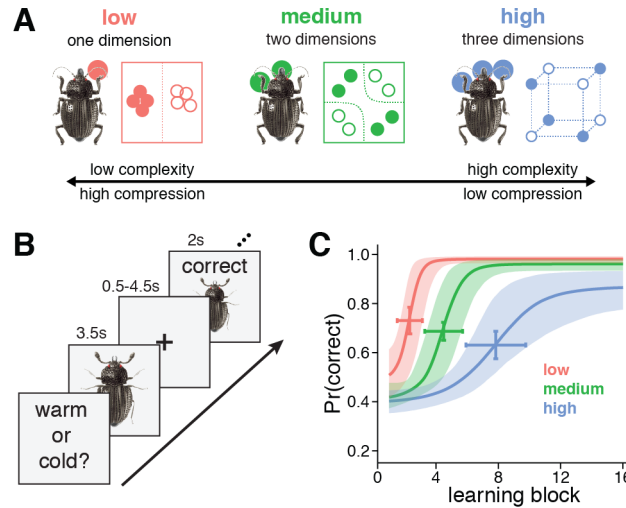
Figure 1: Experimental schematic and behavioral results. **A)** The learning problems differed in rule complexity (see Table S1). The low complexity problem was unidimensional (e.g., antennae size), medium complexity required a conjunction of two features (e.g., leg size and mandible shape), and high complexity required all three features. **B)** Learning blocks consisted of presentation of a stimulus for 3.5s, followed by a fixation cross for 0.5-4.5s, and then a feedback display for 2s that included the stimulus, accuracy of the response, and the correct category. Learning trials were separated by a delay of 2-6s of fixation. **C)** The probability of a correct response increased across learning blocks. The rate of learning differed according to the complexity of the problems.

This design allows us to ask the central question of whether compression in neural representation corresponds with the complexity of the problem-specific conceptual structure throughout learning. Complexity and compression have an inverse relationship; the lower the complexity of a conceptual space, the higher the degree of compression. For instance, in learning the unidimensional problem, variance along the two irrelevant feature dimensions can be compressed resulting in a lower complexity conceptual space. In contrast, learning the high complexity problem requires less compression because all three feature dimensions must be represented, resulting in a relatively more complex conceptual space. Differences in complexity across the three learning problems thus provide a means for testing how learning shapes the dimensionality of neural concept representations. Namely, brain regions involved in goal-directed data compression should *learn* to represent less complex problems with fewer dimensions.

Results

To test this prediction, we recorded functional magnetic resonance imaging (fMRI) data while participants learned the three problems and measured the degree that multivoxel activation patterns were compressed through learning using principal component

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116 analysis (PCA; Figure 2A), a method for low-rank approximation of multidimensional
117 data (Eckart & Young, 1936). Specifically, trial-level neural representations (Mumford,
118 Turner, Ashby, & Poldrack, 2012) for each insect image were submitted to PCA, and the
119 number of principal components (PC) that were necessary to explain 90% of the
120 variance across trials within a learning block was used to calculate an index of neural
121 compression (i.e., fewer PCs reflects more neural compression). This measure of neural
122 compression was calculated across the whole brain with searchlight methods
123 (Kriegeskorte, Goebel, & Bandettini, 2006) for each learning block in each problem. We
124 then identified brain regions that reduce dimensionality with learning (i.e., learn to
125 represent the less complex problems with fewer dimensions) by conducting a voxel-
126 wise linear mixed effects regression on the searchlight compression maps. Specifically,
127 at each voxel, we assessed how neural compression changed as a function of learning
128 block and problem complexity and their interaction.

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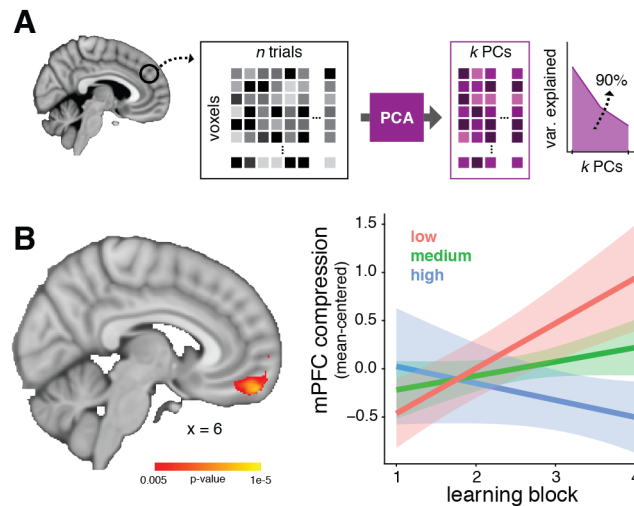
132 **Figure 2:** Neural compression analysis schematic and results. **A)** Principal component analysis (PCA)
133 was performed on neural patterns evoked for each of n trial within a learning block. The number of
134 principal components (PC) required to explain 90% of the variance (k) was used to calculate a neural
135 compression score (1-k/n). We quantified neural compression as a function of problem complexity and
136 learning block; the interaction of these factors reflects changes in the complexity of neural representations
137 that emerge with learning. **B)** A whole brain voxel-wise linear mixed effects regression revealed an mPFC
138 region that showed a significant interaction between learning block and problem complexity. The nature of
139 the interaction in the mPFC region is depicted in the interaction plot on the left. Shaded regions
140 representing 95% confidence bands.

141

142 Throughout the entire brain, only a region within mPFC showed an interaction of
143 problem complexity and learning block (peak coordinates [4, 54, -18]; 653 voxels; voxel-
144 wise threshold = 0.001, cluster extent threshold = 0.05; Figure 2B). The nature of the
145 interaction within this cluster showed that mPFC compression corresponded with

146 problem complexity and emerged over learning blocks ($F_{1,253.8}$ = 19.02, p = 1.9×10^{-5}).
147 Importantly, the interaction effect was independent of individual differences in learning
148 performance (see Materials and Methods for details about the voxel-wise regression
149 modeling). Because the stimuli were identical across the three problems, this finding
150 demonstrates that learning-related compression is goal-specific, with mPFC requiring
151 fewer dimensions for less complex goals.

153 To assess whether mPFC compression tracked changes in attentional allocation, we
154 characterized the participant-specific attentional weights given to each stimulus feature
155 across the three problems using a computational learning model (Love et al., 2004).
156 Attention weight entropy indexed changes in attentional allocation; high entropy
157 indicates equivalent weighting to all three features, whereas low entropy indicates
158 attention directed to only one feature. We found that across the learning problems,
159 attention weight entropy increased with conceptual complexity (β = 0.121, SE = 0.0176,
160 t = 6.90, p = 1.43×10^{-8}; Figure 3B). Importantly, the increase in attention weight entropy
161 mirrored the decrease in mPFC neural compression (β = -0.021, SE = 0.005, t = -4.30, p
162 = 9.02×10^{-5}; Figure 3A), suggesting a link between the behavioral and neural signatures
163 of dimensionality reduction.
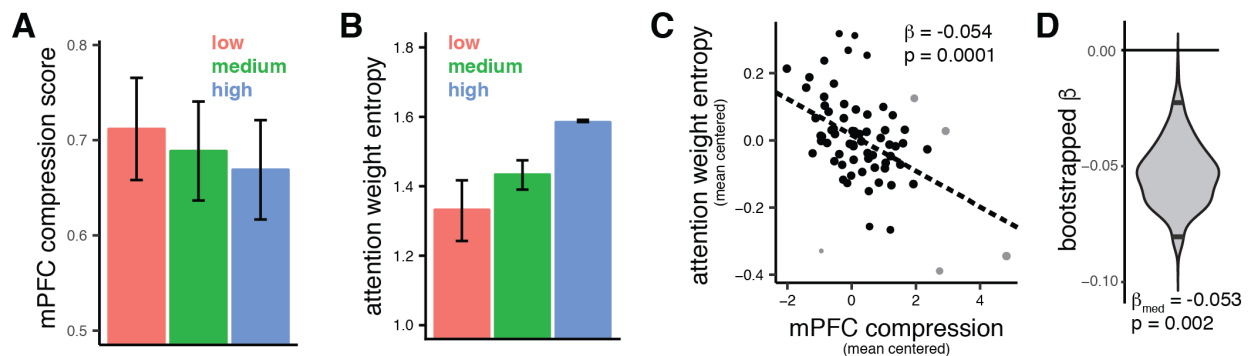
Figure 3: Relationship between mPFC compression and model-based attention weighting in the final learning block. **A)** mPFC neural compression decreased across problems, consistent with their complexity demands. **B)** Attention weight entropy (i.e., dispersion in attention weights) mirrored neural compression, showing attentional strategies consistent with the feature relevancy across the problems (error bars represent 95% CI of the means). **C)** mPFC compression predicted the degree of problem-specific attention weighting (indexed as attention weight entropy). The size of the scatterplot points depicts the weighting from a robust regression analysis; grey-colored points signify observations identified as outliers; the dashed line depicts the best-fitting regression line. **D)** The violin plot depicts a bootstrapped distribution of regression coefficients relating neural compression and attention entropy. Black lines within the distribution mark 95% confidence bounds.

To directly assess this relationship, we evaluated whether entropy of participants' attention weights was predicted by mPFC neural compression at the individual participant level. Specifically, if the ability to compress neural representations in a problem-appropriate fashion is related to participants' ability to attend to problem-relevant features, the prediction follows that participants with more neural compression for a given problem will also show more selective attention, thus lower entropy values. A regression analysis confirmed this hypothesis (β=-0.0536, *SE*=0.0132, *t* = -4.065, *p* = 0.0001; see Figure 3C).

To assess the reliability of this finding and evaluate the influence of potential outliers, we performed three additional analyses. First, we analyzed the relationship between neural compression and attention entropy with robust regression using a logistic weighting function. Robust regression accounts for potential outlier observations by down weighting observations that individually influence the estimation of a linear regression model between two variables. Consistent with the correlation results, the robust regression results showed evidence of a linear relationship between neural compression and attention weight entropy (β = -0.0532, *SE* = 0.0122, *t* = -4.358, *p* < 0.0001). The weighting of each observation estimated in the robust regression analysis is depicted in Figure 3C as the relative size of the data points. Second, we identified and removed potential outliers by evaluating the standardized difference in fit statistic (DFFITS) for each observation. Using the standard DFFITS threshold (Aguinis, Gottfredson, & Joo, 2013), five observations were identified as outliers (noted as grey data points in Figure 3C). Even with these potential outlier observations removed a strong relationship remained (β = -0.056, *SE* = 0.0122, *t* = -3.691, *p* = 0.0005). Third, a nonparametric bootstrap analysis of the linear relationship between neural compression and attention entropy showed a robust effect (see Figure 3D; median β = -0.053, *p* = *0.002, 95% CI* [-0.0785, -0.0201]). Collectively, these findings suggest that the degree of problem-specific neural compression in mPFC predicted participants' attentional strategies.

Discussion

By focusing on a mechanism by which mPFC forms and represents concepts through goal-sensitive dimensionality reduction, we show that neural representations in mPFC are shaped by experience. And, this shaping is adaptive, promoting efficient representation of information that focuses on encoding features that are most predictive of positive outcomes for a given goal. Importantly, by evaluating behavior through the lens of a theoretically-oriented computational model, we demonstrate that the process of learning to compress in mPFC is consistent with the mechanisms of SUSTAIN (Love

217 & Gureckis, 2007; Love et al., 2004). These findings provide a quantitative account of
218 mPFC's role in the coding of schematic models or cognitive maps (Constantinescu et
219 al., 2016; Schuck et al., 2016; Wikenheiser & Schoenbaum, 2016), specifically in the
220 conceptual domain.

221

222 Successfully learning new concepts requires attending to goal-diagnostic features and
223 ignoring irrelevant information to build abstracted representations that capture the
224 structure defining a concept (Love et al., 2004). Viewed in these terms, concept learning
225 has many parallels to schema formation, a mPFC-related function born out of lesion
226 studies in the memory literature (Gilboa & Marlatte, 2017). Schemas are defined as
227 structured memory networks that represent associative relationships among prior
228 experiences and provide predictions for new experiences (Schlichting et al., 2015; Tse
229 et al., 2011; van Kesteren, Fernández, Norris, & Hermans, 2010; Zeithamova et al.,
230 2012). Schema-related memory behaviors are significantly impacted by mPFC lesions.
231 For example, mPFC lesion patients exhibit a reduced influence of prior knowledge
232 during recognition of items presented in schematically congruent contexts compared
233 with healthy controls (Spalding, Jones, Duff, Tranel, & Warren, 2015). Moreover, mPFC
234 lesions have been associated with a marked inability to differentiate schema-related
235 concepts from concepts inappropriate for a given schema (Ghosh, Moscovitch, Melo
236 Colella, & Gilboa, 2014). From this work, it is clear that mPFC is necessary for retrieving
237 generalized representations built from prior events that are relevant to current
238 experience. Such guided retrieval of relevant learned representations is key to building
239 new concepts.

240

241 A key proposal of the SUSTAIN computational model we leveraged is that concept
242 learning is decidedly goal-based, with concept representations adaptively formed to
243 reflect the task at hand (Love et al., 2004). Recent rodent and human work support this
244 proposal with findings that latent mPFC representations are goal-specific in nature, at
245 least at the end of learning. Specifically, neural ensembles in the rodent homologue of
246 mPFC have been demonstrated to represent higher order goal states that relate stimuli
247 to behaviorally-relevant value (Farovik et al., 2015; Lopatina et al., 2017). Similarly, one
248 human neuroimaging study recently localized latent representations of a complex task
249 space relating 16 different goal states to mPFC activation patterns (Schuck et al., 2016).
250 Importantly, these mPFC representations of goal states predicted participants'
251 behavioral performance, supporting the notion that mPFC organizes knowledge based
252 on goals to promote flexible behaviors.

253

254 Our findings provide important evidence for the role of mPFC during the *formation* of
255 conceptual maps of experience. Although theoretical perspectives highlight the

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256 important of mPFC in cognitive map formation (Wikenheiser & Schoenbaum, 2016;
257 Wilson et al., 2014), empirical work has failed to directly examine the computations of
258 mPFC contributions during encoding. Instead, evidence is limited to representations that
259 are established after long periods of training (Constantinescu et al., 2016; Schuck et al.,
260 2016). Relatedly, most current models of mPFC function in memory focus on its role in
261 biasing reactivation of relevant prior experiences via the hippocampus (e.g., Miller &
262 Cohen, 2001). Few directly address mPFC's impact at encoding, despite the fact that
263 there is neuroimaging evidence for interactions between mPFC and memory centers
264 during encoding (Mack, Love, & Preston, 2016; Schlichting & Preston, 2016; van
265 Kesteren et al., 2010; Zeithamova et al., 2012). Our findings provide novel evidence for
266 mPFC's important role in encoding processes that build goal-specific mental models. By
267 linking mPFC coding to the learning mechanisms defined in SUSTAIN, our results
268 suggest that mPFC influences encoding through dimensionality reduction wherein
269 selective attention highlights goal-specific information and discards irrelevant
270 dimensions. That mPFC was the only region identified in our analysis suggests that this
271 influence is direct: inputs to mPFC are directly weighted to select goal-related
272 information and discard irrelevant features. These weightings may then be fed back to
273 memory centers (i.e., hippocampus) to impact neural coding of learning experiences
274 (Mack et al., 2016).

275

276 Our hypothesized view of mPFC function is based on SUSTAIN's formalism of highly
277 interactive mechanisms of selective attention and learning (Love et al., 2004), functions
278 theoretically mapped onto interactions between PFC and the hippocampus (Love &
279 Gureckis, 2007; Mack et al., 2016). Support for this view is found in recent patient work
280 that has demonstrated a causal link between attentional processes and mPFC function
281 in decision making (Noonan, Chau, Rushworth, & Fellows, 2017; Vaidya & Fellows,
282 2015, 2016). These studies have shown that lesions to ventral mPFC disrupt attentional
283 guidance based on prior experience with cue-reward associations (Vaidya & Fellows,
284 2015), learning the value of task-diagnostic features during probabilistic learning
285 (Vaidya & Fellows, 2016), and value comparison during reinforcement learning (Noonan
286 et al., 2017). Relatedly, recent rodent work demonstrates the bidirectional flow of
287 information between mPFC and hippocampus during context-guided memory encoding
288 and retrieval (Place, Farovik, Brockmann, & Eichenbaum, 2016). Coupled with the
289 recent demonstration of hippocampal-mPFC functional coupling during concept learning
290 (Mack et al., 2016), the current findings align well with the view that mPFC is critical for
291 evaluating and representing information in learning and decision making.

292

293 In summary, we show that learning can be viewed as a process of goal-directed
294 dimensionality reduction and that such a mechanism is apparent in mPFC neural

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295   representations throughout learning. Thus, mPFC plays a critical role not only in
296   representing conceptual content, but in the process of *learning* concepts. Notably,
297   dimensionality reduction through selective attention offers a reconciling account of many
298   processes associated with mPFC including schema representation (Van Kesteren,
299   Ruiter, Fernández, & Henson, 2012), latent casual models (Schuck et al., 2016), grid-
300   like conceptual maps (Constantinescu et al., 2016), and value coding (Clithero &
301   Rangel, 2013; Grueschow, Polania, Hare, & Ruff, 2015).
302
303
304   **Materials and Methods**
305
306   *Participants*
307
308   Twenty-three volunteers (11 females, mean age 22.3 years old, ranging from 18 to 31
309   years) participated in the experiment. All subjects were right handed, had normal or
310   corrected-to-normal vision, and were compensated $75 for participating. One participant
311   did not perform above chance in one of the learning problems, thus was excluded from
312   analysis.
313
314   *Stimuli*
315
316   Eight color images of insects were used in the experiment (Figure 1A). The insect
317   images consisted of one body with different combinations of three features: legs, mouth,
318   and antennae. There were two versions of each feature (pointy or rounded tail, thick or
319   thin legs, and shovel or pincer mandible). The eight insect images included all possible
320   combinations of the three features. The stimuli were sized to 300 x 300 pixels.
321
322   *Procedures for the learning problems*
323
324   After an initial screening and consent in accordance with the University of Texas
325   Institutional Review Board, participants were instructed on the classification learning
326   problems. Participants then performed the problems in the MRI scanner by viewing
327   visual stimuli back-projected onto a screen through a mirror attached onto the head coil.
328   Foam pads were used to minimize head motion. Stimulus presentation and timing was
329   performed using custom scripts written in Matlab (Mathworks) and Psychtoolbox
330   (www.psychtoolbox.org) on an Apple Mac Pro computer running OS X 10.7.
331
332   Participants were instructed to learn to classify the insects based on the combination of
333   the insects' features using the feedback displayed on each trial. As part of the initial

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334 instructions, participants were made aware of the three features and the two different
335 values of each feature. Before beginning each classification problem, additional
336 instructions that described the cover story for the current problem and which buttons to
337 press for the two insect classes were presented to the participants. One example of this
338 instruction text is as follows: "Each insect prefers either Warm or Cold temperatures.
339 The temperature that each insect prefers depends on one or more of its features. On
340 each trial, you will be shown an insect and you will make a response as to that insect's
341 preferred temperature. Press the 1 button under your index finger for Warm
342 temperatures or the 2 button under your middle finger for Cold temperatures." The other
343 two cover stories involved classifying insects into those that live in the Eastern vs.
344 Western hemisphere and those that live in an Urban vs. Rural environment. The cover
345 stories were randomly paired with the three learning problems for each participant. After
346 the instruction screen, the four fMRI scanning runs (described below) for that problem
347 commenced, with no further problem instructions. After the four scanning runs for a
348 problem finished, the next problem began with the corresponding cover story
349 description. Importantly, the rules that defined the classification problems were not
350 included in any of the instructions; rather, participants had to learn these rules through
351 trial and error.

352

353 The three problems the participants learned were structured such that perfect
354 performance required attending to a distinct set of feature attributes (Figure 1A). For the
355 low complexity problem, class associations were defined by a rule depending on the
356 value of one feature attribute. For the medium complexity problem, class associations
357 were defined by an XOR logical rule that depended on the value of the two feature
358 attributes that were not relevant in the low complexity problem. For the high complexity
359 problem, class associations were defined such that all feature attributes had to be
360 attended to respond correctly. As such, different features were relevant for the three
361 problems and successful learning required a shift in attending to and representing those
362 feature attributes most relevant for the current problem. Critically, by varying the number
363 of diagnostic feature attributes across the three problems, the representational space
364 for each problem had a distinct informational complexity.

365

366 The binary values of the eight insect stimuli along with the class association for the
367 three learning problems are depicted in Table 1. The stimulus features were randomly
368 mapped onto the attributes for each participant. These feature-to-attribute mappings
369 were fixed across the different classification learning problems within a participant. After
370 the high complexity problem, participants learned the low and medium problems in
371 sequential order. The learning order of the low and medium problems was

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counterbalanced across participants. This problem order was used for purposes described in a prior analysis of this data (Mack et al., 2016).

stimulus	feature attribute			problem complexity		
	1	2	3	low	medium	High
1	0	0	0	A	A	B
2	0	0	1	A	B	A
3	0	1	0	A	B	A
4	0	1	1	A	A	B
5	1	0	0	B	A	A
6	1	0	1	B	B	B
7	1	1	0	B	B	B
8	1	1	1	B	A	A

Table 1: Stimulus features and class associations for the three learning problems. Each of the eight stimuli are represented by the binary values of the three feature attributes. The stimuli are assigned to different classes (A or B) across the low, medium, and high complexity learning problems according to rules that depend on one, two, or three of the feature attributes, respectively.

The classification problems consisted of learning trials (Figure 1a) during which an insect image was presented for 3.5s. During stimulus presentation, participants were instructed to respond to the insect's class by pressing one of two buttons on an fMRI-compatible button box. Insect images subtended 7.3° × 7.3° of visual space. The stimulus presentation period was followed by a 0.5-4.5s fixation. A feedback screen consisting of the insect image, text of whether the response was correct or incorrect, and the correct class was shown for 2s followed by a 4-8s fixation. The timing of the stimulus and feedback phases of the learning trials was jittered to optimize general linear modeling estimation of the fMRI data. Within one functional run, each of the eight insect images was presented in four learning trials. The order of the learning trials was pseudo randomized in blocks of sixteen trials such that the eight stimuli were each presented twice. One functional run was 194s in duration. Each of the learning problems included four functional runs for a total of sixteen repetitions for each insect stimulus. The entire experiment lasted approximately 65 minutes.

Behavioral analysis

Participant-specific learning curves were extracted for each problem by calculating the average accuracy across blocks of sixteen learning trials. These learning curves were used for the computational learning model analysis.

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Computational learning modeling

Participant behavior was modeled with an established mathematical learning model, SUSTAIN (Love et al., 2004). SUSTAIN is a network-based learning model that classifies incoming stimuli by comparing them to memory-based knowledge representations of previously experienced stimuli. Sensory stimuli are encoded by SUSTAIN into perceptual representations based on the value of the stimulus features. The values of these features are biased according to attention weights operationalized as receptive fields on each feature attribute. During learning, these attention weight receptive fields are tuned to give more weight to diagnostic features. SUSTAIN represents knowledge as clusters of stimulus features and class associations that are built and tuned over the course of learning. New clusters are recruited and existing clusters updated according to the current learning goals. A full mathematical formulization of SUSTAIN is provided in its introductory publication (Love et al., 2004).

To characterize the attention weights participants formed during learning, we fit SUSTAIN to each participant's learning performance. First, SUSTAIN was initialized with no clusters and equivalent attention weights across the stimulus feature attributes. Then, stimuli were presented to SUSTAIN in the same order as a participant's experience, and model parameters were optimized to predict each participant's learning performance (mean accuracy averaged over blocks of 16 trials) in the three learning problems through a maximum likelihood genetic algorithm optimization method (Storn & Price, 1997). In the fitting procedure, the model state at the end of the first learning problem was used as the initial state for the second learning problem. In doing so, parameters were optimized to account for learning with the assumption that attention weights, and knowledge clusters learned from the first problem carried over to influence learning in the second problem. Similarly, model state from the second problem carried over and influenced early learning in the third problem. Thus, problem order effects are considered a natural consequence of our model fitting approach. The optimized parameters were then used to extract measures of feature attribute attention weights during the second half of learning in the three problems. Specifically, for each participant, the model parameters were fixed to the optimized values and the model was presented with the trial order experienced by the participant. After the model was presented with the first 96 of trials, the values of the feature attribute attention weights were extracted for each participant. This was repeated for each of the three learning problems. The average value and 95% confidence intervals of the SUSTAIN's five free parameters were: $\gamma = 3.286 \pm 2.064$, $\beta = 4.626 \pm 0.220$, $\eta = 0.308 \pm 0.145$, $d = 20.293 \pm 5.724$, $\tau_h = 0.112 \pm 0.039$.

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MRI data acquisition

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Whole-brain imaging data were acquired on a 3.0T Siemens Skyra system at the University of Texas at Austin Imaging Research Center. A high-resolution T1-weighted MPRAGE structural volume (TR = 1.9s, TE = 2.43ms, flip angle = 9°, FOV = 256mm, matrix = 256x256, voxel dimensions = 1mm isotropic) was acquired for coregistration and parcellation. Two oblique coronal T2-weighted structural images were acquired perpendicular to the main axis of the hippocampus (TR = 13,150ms, TE = 82ms, matrix = 384x384, 0.4x0.4mm in-plane resolution, 1.5mm thru-plane resolution, 60 slices, no gap). High-resolution functional images were acquired using a T2*-weighted multiband accelerated EPI pulse sequence (TR = 2s, TE = 31ms, flip angle = 73°, FOV = 220mm, matrix = 128x128, slice thickness = 1.7mm, number of slices = 72, multiband factor = 3) allowing for whole brain coverage with 1.7mm isotropic voxels.

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MRI data preprocessing and statistical analysis

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MRI data were preprocessed and analyzed using FSL 6.0 (Jenkinson, Beckmann, Behrens, Woolrich, & Smith, 2012) and custom Python routines. Functional images were realigned to the first volume of the seventh functional run to correct for motion, spatially smoothed using a 3mm full-width-half-maximum Gaussian kernel, high-pass filtered (128s), and detrended to remove linear trends within each run. Functional images were registered to the MPRAGE structural volume using Advanced Normalization Tools, version 1.9 (Avants et al., 2011).

464

Neural compression analysis

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The goal of the neural compression analysis was to assess the informational complexity of the neural representations formed during the different learning problems. To index representational complexity, we measured the extent that neural activation patterns could be compressed into a smaller dimensional space according to principal component analyses (PCA). The compression analyses were implemented using PyMVPA (Hanke et al., 2009) and custom Python routines and were conducted on preprocessed and spatially smoothed functional data. First, whole brain activation patterns for each stimulus within each run were estimated using an event-specific univariate general linear model (GLM) approach (Mumford et al., 2012). This approach allowed us to model stable estimates of neural patterns for the eight insect stimuli across the trials in each learning problem. For each classification problem run, a GLM with separate regressors for stimulus presentation on each trial, modeled as 3.5s

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479 boxcar convolved with a canonical hemodynamic response function (HRF), was
480 conducted to extract voxel-wise parameter estimates for each trial. Additionally, trial-
481 specific regressors for the feedback period of the learning trials (2s boxcar) and
482 responses (impulse function at the time of response), as well as six motion parameters
483 were included in the GLM. This procedure resulted in, for each participant, whole brain
484 activation patterns for each trial in the three learning problems.

485

486 We assessed the representational complexity of the neural measures of stimulus
487 representation during learning with a searchlight method (Kriegeskorte et al., 2006).
488 Using a searchlight sphere with a radius of 4 voxels (voxels per sphere: 242 mean, 257
489 mode, 76 minimum, 257 maximum), we extracted a vector of activation values across
490 all voxels within a searchlight sphere for all 32 trials within a problem run. These
491 activation vectors were then submitted to PCA to assess the degree of correlation in
492 voxel activation across the different trials. PCA was performed using the singular value
493 decomposition method as implemented in the decomposition.PCA function of the scikit-
494 learn (version 0.17.1) Python library. To characterize the amount of dimensional
495 reduction possible in the neural representation, we calculated the number of principal
496 components that were necessary to explain 90% of the variance (k) in the activation
497 vectors. We scaled this number into a compression score that ranged from 0 to 1,

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499
$$compression = 1 - \frac{k}{n},$$

500

501 where n is equal to 32, the total number of activation patterns submitted to PCA. By
502 definition, 32 PCs will account for 100% of the variance, but no compression. With this
503 definition of neural compression, larger compression scores indicated fewer principal
504 components were needed to explain the variance across trials in the neural data (i.e.,
505 neural representations with lower dimensional complexity). In contrast, smaller
506 compression scores indicated more principal components were required to explain the
507 variance (i.e., neural representations with higher dimensional complexity). This neural
508 compression searchlight was performed across the whole brain separately for each
509 participant and each run of the three learning problems in native space.

510

511 Group-level analyses were performed on the neural compression maps calculated with
512 the searchlight procedure. Each participant's compression maps were normalized to
513 MNI space using ANTs (Avants et al., 2011) and combined into a group dataset. To
514 identify brain regions that demonstrated neural compression that was consistent with
515 the representational complexity of the learning problems, we performed a voxel-wise
516 linear mixed effects regression analysis. The mixed effects model included factors of

517 problem complexity and learning block as fixed effects as well as participants as a
518 random effect to predict neural compression. The interaction of problem complexity and
519 learning block was the central effect of interest. We also included each participant's
520 accuracy for the three problems within each learning block as a covariate. This
521 regression model was evaluated at each voxel. A statistical map was constructed by
522 saving the *t*-statistic of the interaction between complexity and learning block. The
523 resulting statistical map was voxel-wise corrected at $p = 0.001$ and cluster corrected at p
524 $= 0.05$ which corresponded to a cluster extent threshold of greater than 259 voxels. The
525 cluster extent threshold was determined with AFNI (Cox, 1996) 3dClustStim (version
526 16.3.12) using the *acf* option, second-nearest neighbor clustering, and 2-sided
527 thresholding. The 3dClustSim software used was downloaded and compiled on
528 November 21, 2016 and included fixes for the recently discovered errors of improperly
529 accounting for edge effects in simulations of small regions and spatial autocorrelation in
530 smoothness estimates (Eklund, Nichols, & Knutsson, 2016).

531

532 We assessed the nature of the interaction in the mPFC cluster by extracting each
533 participant's average neural compression score within the cluster for each problem
534 across the four learning runs. The same linear mixed effects model described above
535 was run on the extracted compression values. It is important to note that this analysis
536 was conducted to characterize the interaction underlying the mPFC cluster and,
537 therefore, does not represent a set of independent findings. The results of this model
538 are shown in Table 2.

539

	estimate	SE	df	*t*	*p*
intercept	-2.260	0.632	218.4	-3.58	4.3×10^{-4}
block	0.789	0.164	219.1	4.82	2.7×10^{-6}
complexity	0.566	0.252	140.6	2.24	0.0266
accuracy	0.945	0.461	221.2	2.05	0.0415
block:complexity	-0.321	0.074	253.8	-4.36	1.9×10^{-5}

540

541 **Table 2:** Results of the linear mixed effects regression model predicting average neural compression
542 within the mPFC region depicted in Figure 2B. The estimated values, standard errors (SE), Satterthwaite
543 approximations of degrees of freedom (df), *t*-statistics, and *p* values are reported for each fixed effect.

544

545 *Relating neural compression to behavioral signatures of selective attention*

546

547 To evaluate the relationship between neural compression and model-based estimates
548 of attention weighting, we first extracted individual participant-based measures of each.
549 Because we were interested in the outcome of learning, we focused on the final learning

550   block. The participant-specific average neural compression within the mPFC cluster was
551   extracted for each learning problem. We used the SUSTAIN parameter estimates of
552   stimulus dimension attention weights to calculate a signature of selective attention.
553   Specifically, the attention weight estimates for the three stimulus dimensions in each
554   problem were transformed to sum to 1, thus creating a probability distribution
555   representing the likelihood of attention to the three features. For example, given the
556   attention weights [0.1, 0.1, 0.8], there is a probability of 0.8 that attention will be directed
557   to the third stimulus dimension on any one trial. We then calculated entropy (Davis,
558   Love, & Preston, 2012) across the attention weights for each problem separately:

559
560
$$entropy = -\sum_{i=1}^{3} a_i \log_2 a_i,$$

561

562   such that a_i is the attention weight for stimulus dimension *i*. This entropy measure
563   indexed the dispersion of attention across the stimulus dimensions. For example, high
564   attention weight entropy means that attention is unselective with all three stimulus
565   dimensions equally weighted. On the other hand, low entropy means that attention is
566   highly predictive with the majority of weight on a single dimension. As such, the
567   attention weight entropy index offers a unique signature for optimal attentional strategy
568   across the three learning problems: the lowest entropy should be seen in the low
569   complexity problem, an intermediate entropy for the medium complexity problem, and
570   the highest entropy for the high complexity problem. The effect of problem complexity
571   on both mPFC neural compression and attention weight entropy was assessed with
572   linear mixed effects regression (see Figure 3A and 3B).

573

574   We next evaluated the relationship between mPFC neural compression and attention
575   weight entropy on an individual participant basis with linear regression and several
576   follow up analysis. We first mean centered both measures within participant and entered
577   the resulting measures into a regression model with neural compression as a predictor
578   of attention weight entropy (Figure 3C). We performed three additional analyses to
579   assess the reliability of the regression results and to evaluate the influence of potential
580   outliers. First, we reran the regression analysis with robust regression using a logistic
581   weighting function. Robust regression accounts for potential outlier observations by
582   down weighting observations that individually influence the estimation of a linear
583   regression model between two variables. The weighting of each observation estimated
584   in the robust regression analysis is depicted in Figure 2C as the relative size of the data
585   points. Second, we identified and removed potential outliers by evaluating the
586   standardized difference in fit statistic (DFFITS) for each observation. The standard
587   DFFITS threshold of $\pm 2\sqrt{(k+1)/n}$ (Aguinis et al., 2013) identified five observations as
588   potential outliers (noted as a grey data point in Figure 3C). These observations were

589 excluded and the linear regression analysis was performed again. Third, we performed
590 a nonparametric bootstrap analysis to assess the robustness of the regression findings.
591 We randomly sampled participants' data with replacement from the compression and
592 entropy observations 5000 times, calculating and storing the regression coefficient on
593 each iteration. The 95% confidence interval of the resulting distribution of correlation
594 coefficients was then compared to 0 to determine the robustness of the mPFC
595 compression and attention weight entropy relationship (Figure 3D).

596
597

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Author Contributions

607

608 All authors designed the experiment and wrote the paper. M.L.M. conducted the
609 research and data analysis.

610

Competing Interests

612

613 The authors declare no competing interests.

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